Special Convolutional Neural Network for Identification and Positioning of Interstitial Lung Disease Patterns in Computed Tomography Images

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Abstract—In this paper, automated detection of interstitial lung disease patterns in high resolution computed tomography images is achieved by developing a faster region-based convolutional network based detector with GoogLeNet as a backbone. GoogLeNet is simplified by removing few inception models and used as the backbone of the detector network. The proposed framework is developed to detect several interstitial lung disease patterns without doing lung field segmentation. The proposed method is able to detect the five most prevalent interstitial lung disease patterns: fibrosis, emphysema, consolidation, micronodules and ground-glass opacity, as well as normal. Five-fold cross-validation has been used to avoid bias and reduce over-fitting. The proposed framework performance is measured in terms of F-score on the publicly available MedGIFT database. It outperforms state-of-the-art techniques. The detection is performed at slice level and could be used for screening and differential diagnosis of interstitial lung disease patterns using high resolution computed tomography images.

Keywords: Convolutional Neural Networks, detection of interstitial lung disease patterns, high-resolution computed tomography, faster region-based convolutional network based object detection and F-score **DOI:** 10.1134/S1054661821040027

INTRODUCTION

A group of nearly 200 different pulmonary diseases is combined together to form a common group known as interstitial lung disease (ILD) [32]. The radio-histopathological finding of the majority of diseases from this group suggests the progressive scarring of lung tissues, which would cause increased breathlessness in the patient. It also disturbs the flow of oxygen into the bloodstream. The group shows similar clinical properties among them. It makes difficult to distinguish among them. It makes higher intra and inter variability of the observers. Even experienced medical experts find it difficult for differential diagnoses. Earlier diagnosis improves the chance of cure and recovery with less time. High-resolution computed tomography (HRCT) images are identified as ideal imaging tools for studying patterns of ILD as it provides higher resolution as compared to CT images. The most prevalent ILD patterns can be broadly classified into five major groups: fibrosis, emphysema, consolidation, micronodules, groundglass opacity (GGO), and normal. All these patterns are shown in Fig. 1.

Different imaging modalities exist in the medical domain, such as X-ray, CT, magnetic resonance imaging (MRI), positron emission tomography (PET). Image analysis plays an essential role in the identification of different abnormalities. Hence, intelligence is applied to analysis imaging technique that reduced human intervention to make clinical and research decisions in the medical domain [19]. The deep learning approach recently shows an impressive perfor-

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Fig. 1. Different ILD patterns are: (a) fibrosis, (b) emphysema, (c) consolidation, (d) micronodule, (e) GGO, and (f) normal lung.

mance in different fields: object detection, classification, and segmentation. Sarvamangala et al. [23] have explained the importance of CNN for analyzing the images. The primary advantage of CNN architecture is extracting features from an image without human intervention. This is the main reason researchers have applied CNN based techniques in the different medical domains like detection of ILD patterns [1, 16], classification of ILD [22, 30], lung cancer classification [20], segmentation, prediction, and staging of COVID-19 [4, 31].

Bermejo-Peláez et al. [22] have used a deep learning approach for the classification of ILD patterns. They have developed a CNN architecture that comprises three different architectures such as 2D, 2.5D, and 3D for the classification of ILD abnormalities. To calculate the network's performance, they have extracted radiographic tissue of 37424 from 208 CT images for eight classes. The result is reported in terms of sensitivity and specificity, i.e., 91.41 and 98.18%, respectively. Detection of ILD patterns is a significant prevalence to measure the severity of COVID-19 in this pandemic situation. Chassagnonn et al. [4] proposed a method for finding the stage of patients affected by COVID-19 pneumonia. The authors have compared three network architectures as: CovidENet, CovidE2D, and CovidE3D. The results are evaluated in terms of dice coefficient and dice Hausdorff distance. The CovidENet has been given the best result. The mean dice coefficient and Hausdorff distance are 0.70 and 8.9, respectively, for CovidENet. Wang et al. [31] have used the hybrid encoder technique for better segmentation of lesion features for COVID-19. Those features are help to distinguish between general lung lesions with infected lung lesions. The performance is reported in NSD, mean DSC, F1-score, MCC, sensitivity, and accuracy with the value of 0.704, 0.735, 0.682, 0.707, 0.994, and 0.716, respectively. Therefore, in this paper, we have applied a deep learning approach for the identification of ILD patterns. The state-of-the-art works on detecting ILD patterns are broadly divided into two categories: patch-based methods and slice-based methods.

1.1. Patch-Based Classification

Most of the reported works concentrated on the patch-based classification of ILD patterns, where patches are extracted manually by expert radiologists [5, 7, 26, 33]. Informative features are extracted from several ILD patches with the help of different feature extraction techniques for the classification of ILD patterns. They have been used in [10] to produce multiscale filters and the generated responses were saved as corresponding features. The selection of an appropriate classifier is very important. A plethora of techniques and methods can be found in the literature for this topic. Some of the methods of prominence are k-nearest neighbors [9, 15, 18, 21], artificial neural network [14], and support vector machines [3, 5, 14, 21, 28, 29, 34, 35]. Depeursinge et al. [5] have developed a near-affine-invariant texture-based feature descriptor based on wavelet transformation. This method was evaluated for the classification of five HRCT patterns (healthy, emphysema, GGO, fibrosis, and micronodules) and achieved a classification accuracy of 76.9%. Song et al. [26] used texture and gradient features for patch-based classification of five HRCT patterns, as mentioned earlier. Rotation-invariant Gabor-local binary patterns texture descriptor and gradient

descriptor of multicoordinate histogram of oriented gradients have been used to represent HRCT patterns. The accuracy of classification using support vector machine reported in terms of F-score for each pattern. F-scores for healthy, emphysema, GGO, fibrosis, and micronodules are 84, 75.3, 78.2, 84.1, and 85.7%. To handle intraclass variation and interclass ambiguity in HRCT patterns, Song et al. [27] developed a large margin local estimate classification model and improved classification accuracy. The majority of these techniques have used handcrafted features, and the method fails for a new data or pattern which is not adaptive. Learning features are extracted using the restricted Boltzmann machine (RBM) to cope up with the above issue. RBM is a generative stochastic artificial neural network that can be trained either in unsupervised or supervised ways.

Huang et al. [14] have compared two different network architectures for the classification of ILD patterns. One is based on deep CNN architecture that comprises six different convolutional layers followed by batch normalization layers and ends with a fully connected layer. The network takes input as patches of size 32×32 that is extracted from ILD images. Each layer having a kernel size of 2×2 , and the number of kernels adds in increasing order from 32 up to 192. In this architecture, ReLU is used as an activation function. Another architecture is based on a deep convolution autoencoder (DCAE). To train. these network architecture, authors have been used ADAM optimizer and cross-entropy loss function. The learning rate of 0.0008 is used, which is decreased by 10% after every 20 epochs. The main contribution of authors they have been used twostage transfer learning. The results are evaluated in terms of F1-score. The authors achieved the best results using two-stage transfer learning in both network architectures. The F1-scores are 0.9791 and 0.9810 for CNN and DCAE, respectively. The limitation of this method used patch-based instead of slice-based input images.

Deep learning based image processing techniques using convolutional neural networks (CNNs) have registered their strong presence and effectiveness while dealing with natural color images. Anthimopoulos et al. [2] have developed a CNN for the classification of ILD patterns in HRCT images. LeakyReLU was used as an activation function. The cross-entropy loss is used to optimize ADAM. The network is evaluated for seven HRCT patterns: healthy, micronodules, GGO, consolidation, honeycombing, reticulation, and combination of GGO/reticulation, and achieved a classification accuracy of 85%. The shallow design of this network restricts it from utilizing the adequate advantage from the ability of deep CNN layers. However, patch-based classification is clinically less desirable as it cannot be used for screening of HRCT patterns at slice level.

1.2. Slice-Based Classification

Gao et al. [11] used pretrained AlexNet to classify HRCT slices depending on the presence of pathology. Input images are rescaled to fit AlexNet architectural design, as to exploit the advantages of colored images, they have used different Hounsfield unit (HU) windows to artificially create the three channels. The accuracy of classification is better for emphysema, but the poor classification is observed for micronodules and healthy patterns due to change of contrast. Shin et al. [24] improved the slice level classification accuracy of HRCT slices using GoogLeNet. The main objective of the slice test is to classify the slice based on the presence of five ILD patterns. Anthimopoulos et al. [1] have proposed a CNN network with dilated filters to segmentation ILD patterns. This network input images are any arbitrary size of lung CT and outputs generated by this network are label maps. This network consists of eight convolutional layers having different dilation rates that increase exponentially. This helps to increase the receptive field and also linearly grown number of parameters. The result is evaluated on 172 HRCT slices collected from two hospitals such as Geneva University Hospital and Bern University Hospital. This network achieves an accuracy of 81.8%. The network was trained by minimizing the categorical cross-entropy using the ADAM optimizer with a learning rate of 0.0001.

1.3. Contribution

Localization of ILD patterns in HRCT image slices is clinically more desirable than patch level classification for screening of ILD. The present work focuses on the localization of several ILD patterns in a HRCT slice using a faster region-based convolutional network (R-CNN) based object detection network. GoogLeNet architecture is modified for reduction of complexity and used as a feature extractor of faster R-CNN object detector in the proposed framework. Feature map is obtained from GoogLeNet and fed to region proposal network (RPN) to serve as detection network. The number of the bounding box enclosing ILD patterns in a slice would help in pathology quantification. This framework is fast, accurate, and could be used in the screening of ILD using HRCT image slices. The proposed work reveals that the deep learning based techniques could eliminate the lung field extraction step for the identification of ILD patterns.

2. METHODS

2.1. Database

Publicly available MedGIFT database [8] is used for this study. The database has 108 annotated image series of HRCT. It consists of 17 different patterns of ILD with sizes 512×512 . Total 1946 ROIs were provided from

 Table 1. Total number of image slice with respect to different type of patterns and there corresponding total number of region of interest (ROI) present for that specific patterns are acquired from MedGIFT database

ILD patterns	Total number of image slice	Total number of ROIs
Consolidation	116	194
Emphysema	71	108
Fibrosis	293	479
GGO	241	415
Healthy	69	98
Micronodule	154	277
Total	944	1571

Table 2. Average number of images used in each pattern for training and testing purpose

ILD patterns	Training images before augmentation	Training data after augmentation	Testing images
Consolidation	93	557	23
Emphysema	57	341	14
Fibrosis	234	1406	59
GG0	193	1157	48
Healthy	55	331	14
Micronodule	123	739	31

108 image series of HRCT. In this work, the five most prevalent ILD patterns and healthy patterns are considered. The database is multipattern in nature, which means there is a probability of more than one pattern in the same slice. Statistical detail has been provided in Table 1 for an aforementioned pattern.

2.2. State-of-the-Art CNN Architectures

Several networks like VGGNet, GoogLeNet, and ResNet have been used for the natural image classification task. VGGNet [25] uses only 3×3 convolutional layers, those are stacked on top of each other. The networks have varying depths ranging from 11 to 19. The architectural design of GoogLeNet [6] is different as the depth of the network is increased vertically as well as horizontally with the help of inception modules. This was the naive idea of an inception module, where three convolution networks with filter size 1×1 , 3×3 , and 5×5 are used in parallel together with a 3×3 max-pooling layer. In this network, a 1×1 convolutional layer is introduced before the 3×3 and 5×5 layers. The 1×1 layer acts as an instrument for the reduction of computational complexity. The final module comprises network in the network layer, large and medium size convolution filter, and pooling operation. This network layer is capable of extracting information at a fine level. The 5×5 filter provides a wider receptive field, and the pooling operation reduces the spatial sizes and also looks after overfitting. ResNets [13] are the deepest networks with a maximum of 152 layers. The deeper networks face a degradation problem when they start to converge. In this network concept of residual learning is introduced to address the degradation problem. The residual block is an ensemble of conv-relu-conv series.

2.3. Faster R-CNN Based Object Detector with GoogLeNet as Backbone

In the proposed framework (Fig. 2), GoogLeNet architecture with a reduced inception module is used to extract features for finding region proposals. Instead of nine, five inception modules are used in GoogLeNet in order to reduce network parameters. The fifth inception block provides features, which is used for finding region proposal. The region proposal network (RPN) has two outputs such as RPN classification head and RPN regression head. The RPN classification output layer predicts an anchor box that is an object or background. The RPN regression output layer predicts box offsets (left corner coordinates, width, and height). The feature map is also connected to ROI max-pooling layer to pool features for classifying the pooled regions. Classification and bounding box regression head are attached with the ROI pooling layer. After detection of region proposals for an object, the class score is calculated for every region. The proposed network is trained from scratch with a learning rate of 0.00001. The training was performed up to 35 epochs. ADAM [17] issued to optimize the crossentropy based loss function.

3. EXPERIMENTAL RESULTS

3.1. Dataset for Training and Testing

Table 1 shows that the average number of training and testing images for each pattern is very less. Unlike classical techniques, where the feature is manually defined and calculated, in deep learning, the feature is extracted with the help of a training image. The true potential of CNNs can only be realized if the training data is large enough to effectively train the network so that it captures all the relevant features. There is always a shortage of annotated quality data in the medical domain. Therefore, data augmentation techniques (flip, rotation, change of contrast, and addition of Gaussian noise) have been used to increase the available data. With an increased number of existing training data, the chances of overfitting also get reduced.



Fig. 2. Faster R-CNN based object detector.

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The number of testing and training images for all ILD patterns after applying data augmentation techniques is shown in Table 2.

3.2. Quantitative Results of Slice Test

The proposed framework performance is compared with Shin et al. [24] method in terms of Fscore. It assigns a score based on precision and recall values [12]. Precision is the ratio of true-positive detection to all detections, whereas recall is the ratio of true-positive detection to ground-truth instances. An overlap greater than 0.1 between the ground truth bounding box and the object's detected bounding box is considered true positive. F-score is simply the harmonic mean of precision and recall. The value of the F-score varies between (0, 1), where 1 is the best case

and 0 is the worst case. Here,
$$\beta$$
 is a positive real factor, while putting $\beta = 1$ in Eq. (3), we got F_1 -score

<u>.</u>

$$Precision = \frac{x_{\rm tp}}{x_{\rm tp} + x_{\rm fp}},$$
(1)

$$Recall = \frac{x_{\rm tp}}{x_{\rm tp} + x_{\rm fn}},\tag{2}$$

$$F_{\beta}$$
-Score

$$= (1 + \beta^2) \left(\frac{Precision.Recall}{(Precision \times \beta^2) + Recall} \right),$$
(3)

$$F_1 - Score = 2\left(\frac{Precision.Recall}{Precision + Recall}\right),\tag{4}$$

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Fig. 3 Results of detection of the proposed framework for (a) consolidation (b) GGO, (c) emphysema, (d) micronodules, (e) fibrosis, and (f) normal lung field, respectively. The ground truth and output bounding box is represented by red and yellow color respectively.

where x_{tp} , x_{fn} , and x_{fp} are number of true positives, false negative, and false positives, respectively.

The performance of the proposed framework is calculated in terms of F-score (Eq. (4)) using five-fold crossvalidation. Table 3 shows the comparison of the F-score of the proposed framework with Shin et al. [24]. The proposed method outperforms the competing techniques for all patterns except fibrosis. In the MedGIFT database, all the ROIs with particular pathology in HRCT slices were not annotated by radiologists. The lack of annotations is a major bottleneck of improvement of the performance of detection. In the case of Fig. 3d, the GGO is not annotated by radiologists in the right lung and treated as a false positive. Therefore, detection is affected by incomplete annotations. Shin et al. converted the grayscale HRCT images to color images, where each channel indicates a grayscale image with a particular contrast. This type of forced

Table 3. Comparison of the proposed framework with competing technique

ILD patterns	F-score of Shin et al.	F-score of the proposed method
Consolidation	0.16	0.70
Emphysema	0.35	0.55
Fibrosis	0.75	0.68
GGO	0.56	0.58
Healthy	0.22	0.70
Micronodule	0.71	0.86

conversion may limit the proper transfer of contextual information between the two image types. We have avoided the conversion of grayscale images to RGB. Moreover, the method of Shin et al. is able to find the absence or presence of pathology in an HRCT slice. Their method is unable to tell the location of ILD patterns within the slice. The proposed method has true potential to detect the ILD patterns in a lung HRCT slice effectively.

3.3. Qualitative Results

Figure 3 shows the qualitative results of the proposed framework for the detection of ILD patterns using without lung field segmentation. In this figure, the ground truth and output bounding box are represented by red and yellow colors, respectively. The results show the effectiveness of the proposed framework in the detection of ILD patterns (Figs. 3a–3f). Figure 3b having two ROIs of GGO, but only one ROI was detected by the proposed framework, marked yellow.

CONCLUSIONS

In this paper, automated detection of different ILD patterns in lung HRCT images is performed using faster R-CNN based detector network. The proposed framework is able to detect ILD patterns in lung HRCT slices using only five inception blocks in GoogLeNet. The proposed framework performance is competent with research work by Shin et al. The proposed method avoids the hassles of lung field segmentation. The result shows that the conversion of grayscale biomedical images to color images is not mandatory for the detector network. This detector framework could be used in the screening of ILD.

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COMPLIANCE WITH ETHICAL STANDARDS

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Conflict of Interest

The process of writing and the content of the article does not give grounds for raising the issue of a conflict of interest.

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