

Chinese Pharmaceutical Association Institute of Materia Medica, Chinese Academy of Medical Sciences

Acta Pharmaceutica Sinica B

www.elsevier.com/locate/apsb www.sciencedirect.com



ORIGINAL ARTICLE

In situ monitoring of the structural change of microemulsions in simulated gastrointestinal conditions by SAXS and FRET



Xia Lv^{a,b,†}, Shuguang Zhang^{c,†}, Huipeng Ma^{d,†}, Peipei Dong^a, Xiaodong Ma^a, Ming Xu^a, Yan Tian^a, Zeyao Tang^a, Jinyong Peng^a, Haibo Chen^a, Jianbin Zhang^{a,*}

^aCollege of Pharmacy, Dalian Medical University, Dalian 116044, China ^bCollege of Life Science, Dalian Minzu University, Dalian 116600, China ^cXinglin College, Liaoning University of Traditional Chinese Medicine, Shenyang 110167, China ^dCollege of Medical Laboratory, Dalian Medical University, Dalian 116044, China

Received 1 February 2018; received in revised form 17 March 2018; accepted 26 April 2018

KEY WORDS

Microemulsions; SAXS; FRET; Lipolysis; Mucus; Liquid crystalline phase **Abstract** Microemulsions are promising drug delivery systems for the oral administration of poorly watersoluble drugs. However, the evolution of microemulsions in the gastrointestinal tract is still poorly characterized, especially the structural change of microemulsions under the effect of lipase and mucus. To better understand the fate of microemulsions in the gastrointestinal tract, we applied small-angle X-ray scattering (SAXS) and fluorescence resonance energy transfer (FRET) to monitor the structural change of microemulsions under the effect of lipolysis and mucus. First, the effect of lipolysis on microemulsions was studied by SAXS, which found the generation of liquid crystalline phases. Meanwhile, FRET spectra indicated micelles with smaller particle sizes were generated during lipolysis, which could be affected by CaCl₂, bile salts and lecithin. Then, the effect of mucus on the structural change of lipolysed microemulsions was studied. The results of SAXS and FRET indicated that the liquid crystalline phases disappeared, and more micelles were generated. In summary, we studied the structural change of microemulsions in simulated gastrointestinal conditions by SAXS and FRET, and successfully monitored the appearance and disappearance of the liquid crystalline phases and micelles.

© 2018 Chinese Pharmaceutical Association and Institute of Materia Medica, Chinese Academy of Medical Sciences. Production and hosting by Elsevier B.V. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/).

*Corresponding author.

https://doi.org/10.1016/j.apsb.2018.05.008

2211-3835 © 2018 Chinese Pharmaceutical Association and Institute of Materia Medica, Chinese Academy of Medical Sciences. Production and hosting by Elsevier B.V. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/).

E-mail address: zhangjb@dmu.edu.cn (Jianbin Zhang).

[†]These authors made equal contributions to this work.

Peer review under responsibility of Institute of Materia Medica, Chinese Academy of Medical Sciences and Chinese Pharmaceutical Association.

1. Introduction

In the past several decades, many new formulations have been developed to improve the oral bioavailability of drugs¹. Among those formulations, microemulsions and self-microemulsifying drug delivery systems (SMEDDS) have been proven to be promising drug delivery systems for the oral administration of poorly water-soluble drugs^{2,3}. Microemulsions are single optically isotropic and thermodynamically stable liquid solutions composed of water, oil, surfactants and co-surfactants. SMEDDS is a preconcentrate of microemulsions that forms stable microemulsions in the gastrointestinal (GI) tract under gentle digestive motility⁴. Microemulsions and SMEDDS can significantly promote the oral bioavailability of poorly water-soluble drugs by improving the solubility and the dissolution rate, increasing the intestinal epithelial permeability, inhibiting the P-glycoprotein drug efflux and promoting lymphatic transport^{5,6}. Several products have been successfully commercialized in the last two decades, including Neoral[®] (cyclosporine A), Norvir[®] (ritonavir), Fortovase^{\mathbb{R}} (saquinavir), and Agenerase^{\mathbb{R}} (amprenavir)⁷.

Despite the benefits, the development of microemulsion formulations still encounters some problems, e.g., the toxicity of surfactant and drug precipitation⁸. The primary problem is the poor correlation between the microemulsion characteristics in vitro and the drug bioavailability in vivo^{9,10}. Microemulsion characteristics such as particle size, chain length of triglyceride as well as surfactant/oil ratio are considered the main factors of influencing the bioavailability of drugs. However, the effect of those characteristics was always controversial as reported by previous research¹¹⁻¹³. Hence predicting the drug bioavailability of microemulsions in vivo is extremely difficult. The main reason is microemulsions undergo various structural changes in the GI tract, which is quite difficult to monitor; therefore, leading the fate of microemulsions in the GI tract is still poorly characterized¹⁴. Before being absorbed by the intestine epithelium, microemulsions encounter the lipolysis of lipase and the hindrance of the mucus barrier, where complicated structural changes occur.

Lipase is considered one of the main barriers affecting the fate of microemulsions in the GI tract. As the oil phases are digested by lipases (especially the pancreatic lipase), microemulsions suffer complicated structural changes in the GI tract¹⁵. The study of microemulsion digestion is commonly carried out by the in vitro lipolysis model¹⁶. Fatouros et al. reported the formation of the unilamellar spherical vesicle, the bilamellar vesicle and micelles during SMEDDS digestion observed by the cryogenic transmission electron microscopy (cryo-TEM)¹⁷. Interestingly, Tran et al.¹⁸ also found multivesicular and unilamellar vesicles in the human intestinal contents with cryo-TEM. Moreover, small-angle X-ray scattering (SAXS) and small-angle neutron scattering (SANS) have been applied to monitor the structure of digested microemulsions, founding the formation of micelles, lamellar liquid crystalline and hexagonal liquid crystalline phases¹⁹⁻²². The physicochemical properties (including the particle sizes, particle geometry, zeta potentials, and solubilizing capabilities) of the generated intermediate phases (micelles, vesicles as well as liquid crystals) are obviously different from that of microemulsions. Theoretically, the performance of the intermediate phases in the GI tract should be varied from microemulsions; therefore, the loaded drugs might suffer different fates in the GI tract. It has been reported that the generation of the intermediate phases is highly associated with the lipolysis of the microemulsions. The type and amount of each intermediate phase is highly associated with the types of surfactant and oil, the surfactant/

oil ratio, as well as the physicochemical properties of microemulsions during digestion²³. In our previous work, we found the dissolution rate of drug from microemulsions was affected by lipolysis, which was related to the extent of the digested oil phase²⁴.

The mucus layer, a selective viscoelastic hydrogel on the surface of epithelial cells, is considered another barrier affecting the fate of drugs in the GI tract²⁵. The mucus layer retards the diffusion of drugs and carriers, not only by the size exclusion effect of the hydrogel but also by the interactions between mucin and drugs (or carriers). Mucoadhesive nanoparticles and mucuspenetrating nanoparticles have been designed to overcome the mucus barrier²⁶. Microemulsions coated with a dense PEG shell significantly avoid the hindrance of mucus, and several mucuspenetrating microemulsions have been reported²⁷⁻²⁹. Moreover, some reports demonstrated that partially intact lipid-based nanoparticles diffuse through the mucus layer, including the intestinal epithelium^{30,31}. However, it worth noting that the intermediate phases will be inevitably affected by the mucus layer when passing through mucus, and the performance should be dependent on their physicochemical properties. Up to now, some research has reported the diffusion of microemulsions through the mucus laver: however, the fate of digested microemulsions in mucus has never been reported.

Hence, to accurately predict the drug bioavailability of microemulsions *in vivo*, it is necessary to demonstrate the structural change pathway of microemulsions in the GI tract, especially the effect of lipase and mucus. In this work, we monitored the structural change of microemulsions on lipolysis as well as the further structural change of digested microemulsions in the mucus layer by small-angle X-ray scattering (SAXS) and fluorescence resonance energy transfer (FRET).

2. Materials and methods

2.1. Materials

MCT (medium chain triglyceride) was provided by Qiandao Fine Chemical Industry Co., Ltd. (Hangzhou, China). Cremophor RH40 was purchased from Puruixing Fine Chemicals Co., Ltd. (Shenyang, China). Ethyl oleate (EO) and tributyrin were obtained from Aladdin Chemistry Co., Ltd. (Shanghai, China). 1,2-Propanediol and castor oil were purchased from Damao Chemical Reagent Factory (Tianjin, China). Taurocholic acid sodium salt (NaTC) was purchased from Bio Basic Inc. (Markham, Ontario, Canada). Lecithin (PC) was purchased from Sangon Biotech Co., Ltd. (Shanghai, China). Porcine pancreatin ($8 \times USP$ specifications activity) and mucin from porcine stomach (type II) were purchased from Sigma Chemical Co. (St. Louis, MO, USA). 4-Bromophenylboronic acid (4-BPB) was purchased from Alfa Aesar (Tianjin, China). HPLC grade Methanol was supplied by J&K Chemical Ltd. (Shanghai, China). All other chemicals and reagents were of analytical grade and used without further purification.

2.2. Preparation of SMEDDS and the characterization of microemulsions

SMEDDS formulations were prepared following the method in our previous report²⁴. Briefly, MCT, ethyl oleate and castor oil were selected as the oil phase, while Cremophor RH40 and 1,2-propanediol were selected as the surfactant and co-surfactant. Each component was accurately weighed according to the ratios

|--|

Compositions (w/w)	SMEDDS formulations			
	SME-1	SME-2	SME-3	SME-4
MCT	60%	40%		
Ethyl oleate			40%	
Castor oil				40%
Cremophor RH40	27%	40%	40%	40%
1,2-Propanediol	13%	20%	20%	20%

shown in Table 1. They were added into sealed glass vials and stirred on a magnetic stirrer overnight to obtain the SMEDDS formulations. Microemulsions were obtained by adding moderate amount of deionized water to 1 g SMEDDS formulation and stirred 1 h on a magnetic stirrer.

The particle size, polydispersity index and zeta potential of SME 1–4 microemulsions with 100-fold dilution were measured by Malvern ZS90 zetasizer (Malvern Instruments Corp, Malvern, UK). Briefly, microemulsions were diluted 100 times by deionized water, and 1 mL of microemulsions were put into the cell to measure the particle size, polydispersity index and zeta potential. For each group, three parallel samples were measured.

2.3. Influence of lipolysis on the structure of microemulsions

2.3.1. In vitro lipolysis study

One gram of SMEDDS formulation was separately mixed with 18 mL Sorensen's phosphate buffer solution (0.067 mmol/L, pH 7.0) to form microemulsions in a sealed glass vial, and kept at 37 °C for 30 min. Then, 1 mL pancreatin extract was added to begin the lipolysis experiment. After 6 h, 100 μ L 4-BPB solution (a lipolysis inhibitor, 0.5 mol/L) was added into the mixture to stop further lipolysis. Finally, 1 mL the mixture was taken for particle size distribution analysis, while the remaining mixture was placed for 2 h for further observation.

Pancreatin extract was prepared by adding 1 g porcine pancreatin (containing pancreatic lipase and co-lipase) to 5 mL digestion buffer (50 mmol/L Trizma maleate, 150 mmol/L NaCl, 5 mmol/L CaCl₂ · 2H₂O, pH 7.5) containing 5 mmol/L NaTC and 1.25 mmol/L PC. The mixture was stirred for 15 min followed by centrifugation at $1600 \times g$ and 5 °C for 15 min. The supernatant was collected and stored on ice. Pancreatin extracts were freshly prepared for each experiment. The lipase activity of pancreatin extract was measured according to the previously reported method^{32,33}. Briefly, 6 mL tributyrin was added into 10 mL digestion buffer at pH 7.5 and 37 °C. Then, 1 mL pancreatin extract was added to start the measurement. The pH-Stat automatic titration unit (848 Titrino plus, Metrohm AG, Herisau, Switzerland) was used to maintain the pH at 7.50 \pm 0.05 by titrating with 0.1 mol/L NaOH to neutralize the generated fatty acids. The lipase activity of pancreatin extract was expressed in terms of tributyrin units (TBU), where 1 TBU is the amount of enzyme that can liberate 1 µmol of titratable fatty acids from tributyrin per min. In this work, the lipase activity of 1 mL pancreatin extract was measured to be 2803 TBU.

2.3.2. SAXS monitoring the structural change of microemulsions during lipolysis

First, 1 g SMEDDS formulation was weighed and dissolved in 18 mL simulated fasted intestinal fluid (50 mmol/L Trizma maleate, 150 mmol/L NaCl, 5 mmol/L CaCl₂ · 2H₂O, 5 mmol/L NaTC, 1.25 mmol/L PC, pH 7.5). The pH was then adjusted to 7.5 with 0.1 mol/L NaOH. Then, 1 mL pancreatin extract was added to the mixture to initiate the lipolysis experiment at 37 °C. Meanwhile, a pH-Stat automatic titration unit (848 Titrino plus, Metrohm AG, Herisau, Switzerland) was used to maintain the pH at 7.50 \pm 0.05 by titrating with 0.1 mol/L NaOH. At the lipolysis time of 0, 10, 20, 30, 40, 50 and 60 min, 0.5 mL sample was withdrawn and added into the sample cell through a syringe for SAXS analysis. The front and back of the sample cell was covered by two pieces of polyamide membrane.

SAXS measurements were performed in a beamline (BL16B1) of the Shanghai Synchrotron Radiation Facility (SSRF) with an X-ray energy of 10 keV (corresponding to a wavelength (λ) of 1.24 Å). The sample-to-detector distance was 1.87 m, and the exposure time was set to 300 s. After the data acquisition, the obtained 2D images were integrated into 1D scattering curves (I(q) vs q) by means of the Fit2D software, according to Eq. (1).

$$q = \frac{4\pi}{\lambda} \sin\theta \tag{1}$$

where q is the scattering vector, $\lambda = 1.24$ Å is the X-ray wavelength and 2θ is the scatting angle.

2.3.3. FRET monitoring the structural change of microemulsions during lipolysis

The fluorescent probes RhB-MP and FITC-ODA were synthesized as a FRET pair according to our previously reported method³⁴. RhB-MP was synthesized by forming an ester between the carboxyl group of rhodamine B (RhB) and the hydroxyl group of α -monopalmitin (MP). The FITC-ODA was synthesized by the reaction between the isothiocyanate group of FITC and the amino group of octadecylamine (ODA) (see Scheme 1).

The FRET experiment was carried out using a Perkin-Elmer LS 55 luminescence spectrometer (Perkin-Elmer Ltd, Beaconsfield, England). Briefly, SMEDDS containing RhB-MP (0, 2.5, 5, 10, 15 mg/g) and FITC-ODA (5 mg/g) were prepared in the dark and diluted 20 times with deionized water. One millilitre of the formed microemulsions was put into a quartz cell and measured by the luminescence spectrometer. The excitation wavelength was set to 491 nm and the emission wavelength ranged from 500 to 650 nm. The slit widths of the excitation and emission were both 10 nm and the emission filter was set to 1% T attenuator. Similarly, RhB-MP and FITC-ODA in aqueous solution with different concentration ratios were prepared by maintaining the concentration of FITC-ODA constant and altering the amount of RhB-MP. The fluorescence spectrometer with the same conditions.

To monitor the structural change of microemulsions during lipolysis, 1 g SME-3 SMEDDS formulation containing 5 mg RhB-MP and 5 mg FITC-ODA was dissolved into 18 mL Sorensen's phosphate buffer solution (containing 5 mmol/L CaCl₂ or 5 mmol/L NaTDC/1.25 mmol/L PC). Then, 1 mL pancreatin extract was added to the mixture to initiate the lipolysis experiment. At different lipolysis times, the emission spectra of the lipolysed microemulsions were recorded ranging from 500 to 650 nm.



Scheme 1 Synthesis of fluorescent probes RhB-MP (A) and FITC-ODA (B).

Moreover, the ratios of fluorescence intensity at 580 nm/520 nm were calculated and compared, at different lipolysis times.

the mixtures (0.5 mL) were added into the sample cell through a syringe for SAXS analysis.

2.4. Influence of mucus on the structure of microemulsions

2.4.1. Preparation of mucin solution

Mucin solution with the concentration of 5% (*w/v*) was prepared as simulated mucus. Briefly, porcine gastric mucin was added into a sealed glass vial containing the desired amount of Sorensen's phosphate buffer solution. Then, the mixtures were gently stirred for 2 h on ice to obtain the mucin solution. For all experiments, the mucin solution was freshly prepared and equilibrated to room temperature before use.

2.4.2. Diffusion in of microemulsions in mucus

The diffusion of microemulsions in mucus was measured by multiple particle tracking (MPT), according to previously reported method^{35,36}. Briefly, FITC-ODA labeled SME 1–4 were added to simulated mucus (0.2%, *w/w*) or water, with the concentration of 20 µg/mL. The samples were equilibrated for 30 min at 37 °C, and then transferred to microwells. The Brownian movement was observed by an inverted epifluorescence microscope equipped with a 100 × oil-immersion objective and a CCD camera. Movies was captured for 20 s and analyzed with Image-Pro Plus 6.0 software to extract the *x* and *y* positions of microemulsions centroids over time. For each trajectory, the time-averaged mean squared displacement (MSD) was calculated as a function of time scale. The ensemble-averaged MSD (*<*MSD*>*) for all microemulsions in mucus was calculated by taking the geometric mean of the individual microemulsions' time-averaged MSD.

2.4.3. SAXS monitoring the structural change of lipolysed microemulsions in mucus

After the lipolysis study mentioned in Section 2.3.1, the lipolysed microemulsions were obtained by adding 100 μ L 4-BPB solution to stop the lipolysis reaction, at the lipolysis time of 60 min. The lipolysed microemulsions were then mixed with simulated mucus at the volume ratios of 1:1, 1:2 and 2:1. After stirring for 30 min,

2.4.4. FRET monitoring the structural change of lipolysed microemulsions in mucus

SME-3 SMEDDS formulation containing RhB-MP (5 mg/g) and FITC-ODA (5 mg/g) was prepared and lipolysed following the method mentioned in Section 2.3.1. After 6 h, the lipolysed microemulsions were obtained by adding 100 μ L 4-BPB solution. The lipolysed microemulsions were mixed with simulated mucus at the volume ratio of 1:1, and gently stirred on a magnetic stirrer in dark. At predetermined time intervals, the emission spectrum of the mixture was recorded.

Furthermore, Cremophor RH40, 1,2-propanediol, ethyl oleate and oleic acid were mixed with the ratio of 40:20:24:16 (*w/w*), to simulate the lipolysed SME-3 microemulsions (40% oil phase lipolysed). In the FRET study, the simulated lipolysed microemulsions containing RhB-MP (5 mg/g) and FITC-ODA (5 mg/g) was also mixed with simulated mucus and the emission spectra at predetermined time intervals were recorded.

3. Results and discussion

3.1. Influence of lipolysis on the structure of microemulsions

3.1.1. Characteristics of microemulsions before and after lipolysis

As listed in Table 1, four SMEDDS formulations (SME 1-4) have been previously prepared, with Cremophor RH40/1,2-propanediol (2:1, *w/w*) serving as the surfactant/co-surfactant and different lipids (MCT, ethyl oleate and castor oil) serving as the oil phase ²⁴. Fig. 1 shows the visual appearance of SME 1-4 microemulsions diluted 20-fold, 100-fold, 200-fold, 500-fold and 1000-fold with deionized water. Table 2 listed the particle size, polydispersity index and zeta potential of microemulsions with 100-fold dilution. We found the appearance of microemulsions was closely related to the dilution times. They could form homogenous microemulsions



Figure 1 Visual appearance of SME-1 (A), SME-2 (B), SME-3 (C) and SME-4 (D) with different dilution times. From left to right, the microemulsions were diluted 20-fold, 100-fold, 200-fold, 500-fold and 1000-fold.

with light blue opalescence, after being diluted more than 100 times. SME-2 and SME-3 had similar particle sizes of 66.7 ± 1.2 nm and 63.5 ± 0.5 nm, and they seemed more clear and transparent. SME-1 and SME-4 appeared to be opaque milky emulsion at low dilution rates; however, their particle sizes $(153.5 \pm 4.6$ nm and 205.8 ± 10.8) were still in the range of microemulsions at 100-fold dilution.

It is worth noting that, the increased or decreased particle sizes of digested microemulsions were partly dependent on their compositions. Joseph Chamieh et al.³⁷ applied a Taylor dispersion analysis to study the particle sizes of SEDDS during lipolysis. They found the particle sizes of a Labrasol[®]-based formulation exponentially decreased, and that of a Gelucire[®] 44/14-based formulation sigmoïdally increased. In this work, the four microemulsions were lipolysed for 6 h under the present of pancreatin extract. The visual appearance and particle size distribution of microemulsions before and after lipolysis were recorded (Figs. 2 and 3). As seen in Fig. 2, lipase had completely destroyed the structure of SME-1 microemulsions, leading to the disappearance of the milk white colour. SME-1 microemulsions were composed of MCT/Cremophor RH40/1,2-propanediol (60:27:13, *w/w*), and MCT

was digested into caprylic/capric acids, diglycerides and 2monoglycerides. In our previous study, we found up to 100% of MCT was digested for SME-1 in 1 h lipolysis²⁴. The generated products were excessive and formed unstable structures, which finally separated from the aqueous phase. As seen in Fig. 3A, the particle sizes of SME-1 microemulsions were also obviously altered under the effect of lipolysis. The micron-sized structures were appeared in the lipolysed SME-1 microemulsions, which should be the unstable structures formed by the lipolysis products. Apart from the micron-sized structures, the particle sizes of digested SME-1 microemulsions were even smaller than undigested microemulsions. This could be attributed to the loss of MCT leading microemulsions shrinking. Compared to SME-1 microemulsions, SME 2-4 microemulsions contained higher amounts of surfactant and co-surfactant (60%, w/w), which stayed at the interface and could inhibit lipase hydrolysing the oil phase. Moreover, ethyl oleate and castor oil were more stable than MCT under digestion, which led the degree of lipid digested to be much lower than for the SME-1 microemulsions¹². In our previous work, the degrees of digested oil phases were found to be less than 40% for SME-2 microemulsions and less than 8.5% for SME 3-4 microemulsions²⁴. As shown in Fig. 2 and 3B-D, the lipolysed SME 2-4 microemulsions were still homogeneous in appearance, and the change of particle size distributions was negligible.

3.1.2. SAXS monitoring the structural change of microemulsions during lipolysis

In SAXS experiments, the elastic scattering of X-rays by samples (with different electron density) was recorded at very low angles (typically $0.1-10^{\circ}$). This angular range contains information about the shape and size of macromolecules, characteristic distances of partially ordered materials, pore sizes, and other data. Hence, SAXS is commonly used to determine the priorities of biological materials, polymers, colloids, chemicals, nanocomposites, metals, minerals, food and pharmaceuticals^{38,39}. Researchers have studied the intermediate phases of digested microemulsions using SAXS, and they identified the structure of unilamellar vesicles, bilamellar vesicles, micelles, lamellar and hexagonal liquid crystals^{17,20}. Moreover, they found the formation of the intermediate phases was highly related to the digestion time and the compositions²⁰. To identify the structure of the intermediate phases during the digestion of the four formulations, we applied SAXS to monitor the microemulsions with different digestion times. As seen in Fig. 4, the SAXS data recoded the curve of intensity versus the wave vector (q). No Bragg peak was found in the SAXS spectra of four microemulsions before digestion. However, the Bragg peaks appeared in SME-1 ($q = 1.9 \text{ nm}^{-1}$), SME-3 ($q = 1.3 \text{ nm}^{-1}$) and SME-4 ($q = 1.3 \text{ nm}^{-1}$) microemulsions after the lipolysis started, and the intensity of the Bragg peak gradually increased with lipolysis time. The appearance of the Bragg peaks means some liquid crystalline phases formed^{40,41}. The higher Bragg peak intensity indicated more liquid crystalline intermediate phases were generated.

Table 2 Mean particle size, polydispersity index and zeta potential of diluted microemulsions (Mean \pm SD, n = 3).

	Mean particle size (nm)	Polydispersity index	Zeta potential (mV)
SME-1	153.5 ± 4.6	0.513 ± 0.011	-9.70 ± 0.83
SME-2	667 + 12	0.213 + 0.005	-7.18 + 0.71
SME-3	63.5 ± 0.5	$\begin{array}{r} 0.183 \pm 0.008 \\ 0.183 \pm 0.008 \\ 0.536 \pm 0.049 \end{array}$	-8.22 ± 1.54
SME-4	205.8 ± 10.8		-9.24 ± 0.61



Figure 2 The visual appearance of microemulsions before (left) and after (right) lipolysis.



Figure 3 The particle size distribution of microemulsions before and after lipolysis. (A) SME-1, (B) SME-2, (C) SME-3, (D) SME-4.

3.1.3. FRET monitoring the structural change of microemulsions during lipolysis

FRET was also applied to monitor the structural change of microemulsions during digestion in this study. FRET is commonly used to determine molecular interaction in a myriad of biological processes, as well as the stability of nanoparticles^{42,43}. FRET is distance-dependent and occurs only when the distance between the donor and acceptor less than 10 nm⁴⁴. Pan et al.⁴⁵ previously applied FRET to analyse the dynamics of emulsion interfaces during digestion, and they found changes in the donor/acceptor ratio in FRET reflect the release of fatty acids. In this study, we applied the synthesized fluorescent probes FITC-ODA and RhB-MP as the FRET donor/acceptor pair (see Scheme 1). Both FITC-ODA and RhB-MP were hydrophobic due to the introduction of octadecylamine and α -monopalmitin, which ensured they were embedded in the core of microemulsions. There was an overlap between the emission spectrum of FITC-ODA and the excitation spectrum of RhB-MP (see Fig. 5A), indicating the possibility of energy transfer from FITC-ODA to RhB-MP. Then, RhB-MP and FITC-ODA were co-loaded in microemulsions, where the concentration of FITC-ODA was held constant and the amount of RhB-MP was altered. As seen in Fig. 5B, the fluorescence intensity of FITC-ODA gradually decreased with the increase of RhB-MP, despite the unchanged concentration of FITC-ODA. This demonstrated that the energy transfer occurred from FITC-ODA to RhB-MP, after they were co-loaded in microemulsions. Furthermore, we measured the fluorescence spectra of RhB-MP/ FITC-ODA in aqueous solution, under the same condition. The results showed that the increase of RhB-MP slightly decreased the intensity of FITC-ODA (see Fig. 5C). The decrease of FITC-ODA intensity in aqueous solution was negligible compared to that of microemulsions, at the RhB-MP/FITC-ODA ratio of 1:1. Hence, the FRET was negligible in aqueous solution, where FITC-ODA and RhB-MP were homogeneously distributed, and the distance was generally more than 10 nm. However, when FITC-ODA and RhB-MP were co-loaded in microemulsions with particle sizes smaller than 200 nm, plenty of FRET pair had a distance less than 10 nm, meaning that FRET obviously occurred inside of the microemulsions.

Based on the FRET microemulsions, we studied the fluorescence emission spectra of microemulsions during lipolysis. In this work, we fixed the RhB-MP/FITC-ODA ratio at 1:1 (w/w), and the structural change of microemulsions could be reflected by the change of the fluorescence spectra. Generally, the FRET efficiency (or the acceptor/ donor ratio) is dependent on the distance of the FRET pair, where the closer distance results in higher FRET efficiency. Hence, we considered that the formation of intermediate phases with larger particle sizes separates the FRET pair farther and the FRET efficiency decreases. Similarly, the formation of smaller intermediate phases will lead to the FRET efficiency increasing. SME-3 microemulsions were selected as the model, which generated oleic acid and ethanol after lipolysis. As seen in Fig. 6, the fluorescence spectra of FRET microemulsions were changed at different digestion times, with the intensity of FITC-ODA at 520 nm gradually decreased. Similarly, the decrease of fluorescence intensity at 520 nm was observed in microemulsions containing CaCl2 or NaTDC/PC. The fluorescence intensity of RhB-MP at 580 nm was also altered at different digestion times. To further compare difference of the fluorescence spectra, we calculated



Figure 4 SAXS spectra recorded for the four microemulsion formulations during digestion at 0, 10, 20, 30, 40, 50 and 60 min. The intensity is plotted *versus* the wave vector. (A) SME-1, (B) SME-2, (C) SME-3, (D) SME-4.



Figure 5 (A) The excitation spectra (ex) and emission spectra (em) of FITC-ODA and RhB-MP. (B) The fluorescence emission spectra of FRET probes loaded microemulsions with different RhB-MP/FITC-ODA ratios. (C) The fluorescence emission spectra of FRET probes in aqueous solution with different RhB-MP/FITC-ODA ratios.

the intensity ratios of RhB-MP at 580 nm (I₅₈₀) and FITC-ODA at 520 nm (I_{520}) and normalized the I_{580}/I_{520} ratio to the microemulsions before digestion. The normalized I_{580}/I_{520} ratio reflects the extent of energy transferred from FITC-ODA to RhB-MP. From Fig. 6D, we found the ratio of I_{580}/I_{520} gradually increased with the digestion time, and the presence of CaCl2 and NaTDC/PC accelerates the increase of I_{580}/I_{520} ratio. The results indicated that more energy was transferred from FITC-ODA to RhB-MP during the lipolysis of microemulsions, meaning that intermediate phases with smaller particle sizes were generated. We inferred that the smaller intermediate phases should be the mixed micelles. Because various studies have demonstrated that the mixed micelles, with small particle sizes of approximately 10 nm, were one of the main intermediate phases of digested lipid based formulations¹⁷. In the GI tract they were formed in the present of fatty acids, monoglycerides, bile salts and lecithin. It was reported that the generated fatty acids could inhibit the binding of lipase to the oil phase by staying at the interface of microemulsions. However, CaCl₂ and NaTDC/PC could remove fatty acids from the interface by forming calcium soaps and mixed micelles^{15,46}. Hence, the addition of CaCl₂ or NaTDC/PC accelerates the formation of micelles. Interestingly, the liquid crystalline phases observed by SAXS have much larger particle sizes and should decrease the I_{580}/I_{520} values decreased. This seemed contradictory to the FRET results. In fact, the liquid crystalline phases and micelles are always coexisted in the digested lipid based drug delivery systems, as reported by many researchers 17,20,21,38 . In this experiment, the number of micelles should be far greater than the liquid crystalline phases, increasing the I_{580}/I_{520} values increased. In the work of Pan at al.⁴⁵, the acceptor/donor ratio was also increased during lipid-based formulation digestion in the present of bile salts.

3.2. Influence of mucus on the structure of microemulsions

3.2.1. Diffusion in of microemulsions in mucus

We compared the diffusion in of microemulsions in mucus and water by multiple particle tracking (MPT). As seen in Fig. 7A, the representative trajectories of microemulsions in water and mucus showed that the movement distance of microemulsions in mucus was much lower than that in water. Furthermore, the ensemble-averaged MSD (<MSD>) for microemulsions in mucus and water was calculated and shown in Fig. 7B. The result showed that <MSD> of microemulsions in water was much higher than that in mucus. It was obvious that the diffusion of microemulsions was severely hindered by mucus, which might be caused by the interactions between mucin and microemulsions, as well as the mesh of mucus. Hence, it is essential to study the fate of microemulsions in mucus and find the solution to overcome the mucus barrier. It worth noting that, SME-2 and SME-3 with



Figure 6 The fluorescence emission spectra of FRET microemulsions during lipolysis, (A) microemulsions in PBS, (B) microemulsions in PBS with 5 mmol/L CaCl₂, (C) microemulsions in PBS with 5 mmol/L NaTDC/1.25 mmol/L PC. (D) The normalized intensity ratios of I_{580}/I_{520} of microemulsions during digestion.



Figure 7 Transport of SME 1–4 in water and mucus. (A) Representative trajectories of SME 1–4 in water and mucus during 20 s movies. (B) Ensemble-averaged geometric mean square displacement ($\langle MSD \rangle$) of SME 1–4 in water and mucus.

smaller particle sizes exhibited much higher <MSD> than SME-1 and SME-4 (see Fig. 7B), meaning the particle sizes played an important role on the diffusion of microemulsions in mucus.

3.2.2. SAXS monitoring the structural change of lipolysed microemulsions in mucus

After being digested by lipase, microemulsions as well as the intermediate phases must diffuse through the mucus layer before reaching the epithelial cells. In mucus, mucin or lipids might interact with the microemulsions and the intermediate phases, resulting in further structural change. In our previous report, we found part of the microemulsions aggregated into larger emulsions in mucus³⁴. Here we applied SAXS and FRET to monitor the further structural change of lipolysed microemulsions in mucus. The lipolysed microemulsions were mixed with mucus for 30 min. As seen in Fig. 8, the Bragg peaks disappeared in the SAXS spectra of SME-1, SME-3 and SME-4, at the microemulsions/ mucus ratios of 1:1 and 1:2. This indicated the liquid crystalline phases were damaged in mucus. In the structure of mucin proteins, there are many naked hydrophobic cysteine-rich domains, which could absorb significant lipids by forming numerous low-affinity



Figure 8 SAXS spectra recorded for the lipolysed microemulsions in mucus. The intensity is plotted *versus* the wave vector. (A) SME-1, (B) SME-2, (C) SME-3, (D) SME-4.



Figure 9 The fluorescence emission spectra of lipolysed SME-3 microemulsions (A) and the simulated lipolysed SME-3 microemulsions (B).

bonds⁴⁷. The damage to the liquid crystalline phases might be attributed to the hydrophobic interaction and the hydrogen bonds, between mucin and liquid crystals.

3.2.3. FRET monitoring the structural change of lipolysed microemulsions in mucus

In the FRET study, we used FRET probes to label the lipolyzed SME-3 microemulsions and mixed the microemulsions with mucus for different times. From Fig. 9A, we found the fluorescence intensity of RhB-MP at 580 nm was slightly decreased after mixed for more than 15 min, despite the change was not obvious. As previously reported, the percentage of lipolysed SME-3 microemulsions was less than 8.5%, we thought that higher degree of lipolysis might make the change to the SAXS data more obvious. Therefore, we prepared the formulation containing oleic acid (16%, w/w) to simulate the lipolysed microemulsions with 40% of oil phase digested. After the simulated lipolysed SME-3 microemulsions were mixed with mucus, the fluorescence spectra were significantly changed; the fluorescence intensity decreased at 520 nm and increased at 580 nm (Fig. 9B). These results demonstrated that more energy was transferred from the donor to the

acceptor, meaning the particle sizes of the lipolysed microemulsions decreased and the distance between the probes shortened. Here, we inferred that the liquid crystalline phases transformed into smaller micelles in mucus, as they could interact with mucin or lipids. In fact, the lyotropic liquid crystals generated from lipolysed microemulsions were unstable and transformed into other structures depending on the concentrations and components. Lyotropic liquid crystals applied for drug carriers have been widely studied. Especially, cubic and hexagonal mesophases are good candidates for mucosal drug delivery systems due to their mucoadhesive properties. The interaction of liquid crystalline phases with mucin would inevitably inhibit their diffusion through the mucus layer. However, they transformed into smaller micelles in mucus. We thought that this might be beneficial for lipolysed microemulsions to rapidly diffuse through the mucus layer.

Based on the results above, we found the microemulsions suffered complicated structural changes under the effect of lipase and mucus (see Fig. 9). Microemulsions were first digested by lipase to form several intermediate phases. SAXS identified the formation of liquid crystalline phases during digestion. FRET



Figure 10 Schematic illustrations showing the possible structural change of microemulsions under the effect of lipase and mucus.

found that the intermediate phases with smaller particle sizes were formed, which was mainly micelles. In mucus, the structure of the intermediate phases was further altered, with the Bragg peaks of liquid crystalline phases disappearing in the SAXS spectra. FRET results indicated that the liquid crystals transformed into smaller micelles in mucus. In addition, some microemulsions were aggregated into larger emulsions in mucus due to the microemulsion-mucin interaction. In this work, part of the structural change of microemulsions under the effect of lipase and mucus was revealed. However, there are still many questions to be solved, such as the mechanism of those structures absorbed by the intestinal epithelium, how to control the formation of the intermediate phases, which kind of structure can make drug to reach the highest bioavailability, how to monitor the structural change in vivo. Hence, far more work should be carried out to resolve those questions. Apart from FRET and SAXS, other techniques have been used or might be used to study the fate of nanoparticles in the GI tract, such as cryo-TEM, near-infrared fluorescent dye, the water-quenching environment-responsive fluorescent probes, quantum dot and aggregation-induced emission (AIE)^{18,31} (Fig. 10).

4. Conclusion

To demonstrate the fate of microemulsions in the GI tract, we applied SAXS and FRET to monitor the structural change of four microemulsions (SME 1-4) in simulated gastrointestinal conditions, especially the effect of lipase and mucus. During the lipolysis of microemulsions, the liquid crystalline phases were observed by SAXS. Meanwhile, FRET spectra indicated micelles with smaller particle sizes were generated during lipolysis, and the presence of CaCl₂, bile salts and lecithin accelerated the formation of micelles. We further investigated the structural change of digested microemulsions in the mucus layer. The SAXS spectra showed that the peaks from the liquid crystals disappeared, and the FRET spectra showed that structures with smaller particles sizes appeared. These results indicated that the liquid crystalline phases were transformed into micelles due to their interaction with mucus. The structural change of microemulsions in the GI tract would inevitably affect the delivery of drugs, including drug release, drug adsorption and drug distribution. This work helps researchers to better understand the fate of microemulsions in the GI tract and the drug performance in vivo. In this work, part of the structural change of microemulsions was revealed. However, there are still many questions to be solved and far more work should be carried out. In future work, the combination of SAXS and FRET with some other methods can provide deeper insight into the whole pathway of microemulsions in the GI tract, such as cryo-TEM.

Acknowledgement

This work was supported by the National Natural Science Foundation of China (Grant No. 81703606), the Educational Committee Foundation of Liaoning Province (Grant No. L2016026), and the Fundamental Research Funds for the Central Universities (Grant no. wd01185). The authors thank the staff at the beamline BL16B1 of Shanghai Synchrotron Radiation Facility (SSRF) for SAXS tests.

References

- Shekhawat PB, Pokharkar VB. Understanding peroral absorption: regulatory aspects and contemporary approaches to tackling solubility and permeability hurdles. *Acta Pharm Sin B* 2017;7:260–80.
- He CX, He ZG, Gao JQ. Microemulsions as drug delivery systems to improve the solubility and the bioavailability of poorly water-soluble drugs. *Expert Opin Drug Deliv* 2010;7:445–60.
- Lv X, Liu T, Ma H, Tian Y, Li L, Li Z, et al. Preparation of essential oil-based microemulsions for improving the solubility, pH stability, photostability, and skin permeation of quercetin. *AAPS PharmSciTech* 2017;18:3097–104.
- Li F, Hu R, Wang B, Gui Y, Cheng G, Gao S, et al. Self-microemulsifying drug delivery system for improving the bioavailability of huperzine A by lymphatic uptake. *Acta Pharm Sin B* 2017;7:353–60.
- Martins S, Sarmento B, Ferreira DC, Souto EB. Lipid-based colloidal carriers for peptide and protein delivery — liposomes versus lipid nanoparticles. Int J Nanomed 2007;2:595–607.
- 6. Trevaskis NL, Charman WN, Porter CJH. Lipid-based delivery systems and intestinal lymphatic drug transport: a mechanistic update. *Adv Drug Deliv Rev* 2008;60:702–16.
- Porter CJ, Pouton CW, Cuine JF, Charman WN. Enhancing intestinal drug solubilisation using lipid-based delivery systems. *Adv Drug Deliv Rev* 2008;60:673–91.
- Dokania S, Joshi AK. Self-microemulsifying drug delivery system (SMEDDS) - challenges and road ahead. *Drug Deliv* 2015;22:675–90.
- **9.** Han SF, Yao TT, Zhang XX, Gan L, Zhu CL, Yu HZ, et al. Lipidbased formulations to enhance oral bioavailability of the poorly watersoluble drug anethol trithione: effects of lipid composition and formulation. *Int J Pharm* 2009;**379**:18–24.
- Narang AS, Delmarre D, Gao D. Stable drug encapsulation in micelles and microemulsions. *Int J Pharm* 2007;345:9–25.
- 11. Porter CJH, Kaukonen AM, Boyd BJ, Edwards GA, Charman WN. Susceptibility to lipase-mediated digestion reduces the oral bioavailability of danazol after administration as a medium-chain lipid-based microemulsion formulation. *Pharm Res* 2004;**21**: 1405–12.
- 12. Dahan A, Hoffman A. Use of a dynamic *in vitro* lipolysis model to rationalize oral formulation development for poor water soluble drugs: correlation with *in vivo* data and the relationship to intra-enterocyte processes in rats. *Pharm Res* 2006;23:2165–74.
- 13. Dahan A, Hoffman A. The effect of different lipid based formulations on the oral absorption of lipophilic drugs: the ability of *in vitro* lipolysis and consecutive *ex vivo* intestinal permeability data to predict *in vivo* bioavailability in rats. *Eur J Pharm Biopharm* 2007;**67**:96–105.
- 14. O'Driscoll CM. Lipid-based formulations for intestinal lymphatic delivery. *Eur J Pharm Sci* 2002;15:405–15.
- Golding M, Wooster TJ. The influence of emulsion structure and stability on lipid digestion. *Curr Opin Colloid Interface Sci* 2010;15:90–101.
- Porter CJ, Trevaskis NL, Charman WN. Lipids and lipid-based formulations: optimizing the oral delivery of lipophilic drugs. *Nat Rev Drug Discov* 2007;6:231–48.

- Tran T, Fatouros DG, Vertzoni M, Reppas C, Mullertz A. Mapping the intermediate digestion phases of human healthy intestinal contents from distal ileum and caecum at fasted and fed state conditions. J Pharm Pharmacol 2017;69:265–73.
- Salentinig S, Sagalowicz L, Leser ME, Tedeschi C, Glatter O. Transitions in the internal structure of lipid droplets during fat digestion. *Soft Matter* 2011;7:650–61.
- 20. Fatouros DG, Deen GR, Arleth L, Bergenstahl B, Nielsen FS, Pedersen JS, et al. Structural development of self nano emulsifying drug delivery systems (SNEDDS) during *in vitro* lipid digestion monitored by small-angle X-ray scattering. *Pharm Res* 2007;24:1844–53.
- Warren DB, Anby MU, Hawley A, Boyd BJ. Real time evolution of liquid crystalline nanostructure during the digestion of formulation lipids using synchrotron small-angle X-ray scattering. *Langmuir* 2011;27:9528–34.
- Rezhdo O, Di Maio S, Le P, Littrell KC, Carrier RL, Chen SH. Characterization of colloidal structures during intestinal lipolysis using small-angle neutron scattering. *J Colloid Interface Sci* 2017;499:189–201.
- 23. Thomas N, Mullertz A, Graf A, Rades T. Influence of lipid composition and drug load on the *in vitro* performance of self-nanoemulsifying drug delivery systems. *J Pharm Sci* 2012;**101**:1721–31.
- 24. Zhang JB, Lv Y, Zhao S, Wang B, Tan MQ, Xie HG, et al. Effect of lipolysis on drug release from self-microemulsifying drug delivery systems (SMEDDS) with different core/shell drug location. AAPS PharmSciTech 2014;15:731–40.
- 25. Boegh M, Nielsen HM. Mucus as a barrier to drug delivery understanding and mimicking the barrier properties. *Basic Clin Pharm Toxicol* 2015;**116**:179–86.
- 26. Ci L, Huang Z, Liu Y, Liu Z, Wei G, Lu W. Amino-functionalized poloxamer 407 with both mucoadhesive and thermosensitive properties: preparation, characterization and application in a vaginal drug delivery system. *Acta Pharm Sin B* 2017;7:593–602.
- Karamanidou T, Karidi K, Bourganis V, Kontonikola K, Kammona O, Kiparissides C. Effective incorporation of insulin in mucus permeating self-nanoemulsifying drug delivery systems. *Eur J Pharm Biopharm* 2015;97:223–9.
- 28. Li X, Chen D, Le C, Zhu C, Gan Y, Hovgaard L, et al. Novel mucuspenetrating liposomes as a potential oral drug delivery system: preparation, *in vitro* characterization, and enhanced cellular uptake. *Int J Nanomed* 2011;6:3151–62.
- 29. Griesser J, Burtscher S, Kollner S, Nardin I, Prufert F, Bernkop-Schnurch A. Zeta potential changing self-emulsifying drug delivery systems containing phosphorylated polysaccharides. *Eur J Pharm Biopharm* 2017;119:264–70.
- **30.** Roger E, Gimel J-C, Bensley C, Klymchenko AS, Benoit J-P. Lipid nanocapsules maintain full integrity after crossing a human intestinal epithelium model. *J Control Release* 2017;**253**:11–8.
- Xia F, Fan W, Jiang S, Ma Y, Lu Y, Qi J, et al. Size-dependent translocation of nanoemulsions via oral delivery. ACS Appl Mater Interfaces 2017;9:21660–72.

- 32. Sek L, Porter CJ, Kaukonen AM, Charman WN. Evaluation of the *invitro* digestion profiles of long and medium chain glycerides and the phase behaviour of their lipolytic products. *J Pharm Pharmacol* 2002;54:29–41.
- 33. Sek L, Porter CJ, Charman WN. Characterisation and quantification of medium chain and long chain triglycerides and their *in vitro* digestion products, by HPTLC coupled with *in situ* densitometric analysis. *J Pharm Biomed Anal* 2001;25:651–61.
- 34. Zhang JB, Lv Y, Wang B, Zhao S, Tan MQ, Lv GJ, et al. Influence of microemulsion–mucin interaction on the fate of microemulsions diffusing through pig gastric mucin solutions. *Mol Pharm* 2015;12:695–705.
- 35. Shan W, Zhu X, Liu M, Li L, Zhong J, Sun W, et al. Overcoming the diffusion barrier of mucus and absorption barrier of epithelium by selfassembled nanoparticles for oral delivery of insulin. ACS Nano 2015;9:2345–56.
- Schuster BS, Suk JS, Woodworth GF, Hanes J. Nanoparticle diffusion in respiratory mucus from humans without lung disease. *Biomaterials* 2013;34:3439–46.
- 37. Chamieh J, Merdassi H, Rossi J-C, Jannin V, Demarne F, Cottet H. Size characterization of lipid-based self-emulsifying pharmaceutical excipients during lipolysis using Taylor dispersion analysis with fluorescence detection. *Int J Pharm* 2018;537:94–101.
- Reinke SK, Roth SV, Santoro G, Vieira J, Heinrich S, Palzer S. Tracking structural changes in lipid-based multicomponent food materials due to oil migration by microfocus small-angle X-ray scattering. Acs Appl Mater Interfaces 2015;7:9929–36.
- Mouri A, Diat O, El Ghzaoui A, Bauer C, Maurel JC, Devoisselle J-M, et al. Phase behavior of reverse microemulsions based on Peceol (R). *J Colloid Interface Sci* 2014;416:139–46.
- 40. Khan J, Hawley A, Rades T, Boyd B. *In situ* lipolysis and synchrotron Small-Angle X-ray Scattering for the direct determination of the precipitation and solid-state form of a poorly water-soluble drug during digestion of a lipid-based formulation. *J Pharm Sci* 2016;105:2631–9.
- Phan S, Salentinig S, Gilbert E, Darwish TA, Hawley A, Nixon-Luke R, et al. Disposition and crystallization of saturated fatty acid in mixed micelles of relevance to lipid digestion. *J Colloid Interface Sci* 2015;449:160–6.
- 42. Shi JY, Tian F, Lyu J, Yang M. Nanoparticle based fluorescence resonance energy transfer (FRET) for biosensing applications. *J Mater Chem B* 2015;3:6989–7005.
- Lu J, Owen SC, Shoichet MS. Stability of self-assembled polymeric micelles in serum. *Macromolecules* 2011;44:6002–8.
- 44. Ray PC, Fan Z, Crouch RA, Sinha SS, Pramanik A. Nanoscopic optical rulers beyond the FRET distance limit: fundamentals and applications. *Chem Soc Rev* 2014;43:6370–404.
- 45. Pan Y, Nitin N. Real-time measurements to characterize dynamics of emulsion interface during simulated intestinal digestion. *Colloids Surfaces B: Biointerfaces* 2016;141:233–41.
- 46. Chakraborty S, Shukla D, Mishra B, Singh S. Lipid an emerging platform for oral delivery of drugs with poor bioavailability. *Eur J Pharm Biopharm* 2009;73:1–15.
- Cone RA. Barrier properties of mucus. Adv Drug Deliv Rev 2009;61:75–85.