

# Monte Carlo Study on Dose Distributions Around $^{192}\text{Ir}$ , $^{169}\text{Yb}$ , and $^{125}\text{I}$ Brachytherapy Sources Using EGSnrc-based `egs_brachy` User-code

Subhalaxmi Mishra<sup>1</sup>, Bibekananda Mishra<sup>2</sup>, T. Palani Selvam<sup>1,3</sup>, Sudesh Deshpande<sup>4</sup>, Munir Shabbir Pathan<sup>1</sup>, Rajesh Kumar<sup>1</sup>

<sup>1</sup>Division of Radiological Physics and Advisory, Health Safety and Environment Group, Bhabha Atomic Research Centre, <sup>2</sup>Division of Radiological Safety, Atomic Energy Regulatory Board, <sup>3</sup>Homi Bhabha National Institute, <sup>4</sup>Department of Radiation Oncology, P. D. Hinduja National Hospital and MRC, Mumbai, Maharashtra, India

## Abstract

**Introduction:** As per the recommendations of the American Association of Physicists in Medicine Task Group 43, Monte Carlo (MC) investigators should reproduce previously published dose distributions whenever new features of the code are explored. The purpose of the present study is to benchmark the TG-43 dosimetric parameters calculated using the new MC user-code `egs_brachy` of EGSnrc code system for three different radionuclides  $^{192}\text{Ir}$ ,  $^{169}\text{Yb}$ , and  $^{125}\text{I}$  which represent high-, intermediate-, and low-energy sources, respectively. **Materials and Methods:** Brachytherapy sources investigated in this study are high-dose rate (HDR)  $^{192}\text{Ir}$  VariSource (Model VS2000),  $^{169}\text{Yb}$  HDR (Model 4140), and  $^{125}\text{I}$  -low-dose-rate (LDR) (Model OcuProsta). The TG-43 dosimetric parameters such as air-kerma strength,  $S_k$ , dose rate constant,  $\Lambda$ , radial dose function,  $g(r)$  and anisotropy function,  $F(r;\theta)$  and two-dimensional (2D) absorbed dose rate data (along-away table) are calculated in a cylindrical water phantom of mass density  $0.998\text{ g/cm}^3$  using the MC code `egs_brachy`. Dimensions of phantom considered for  $^{192}\text{Ir}$  VS2000 and  $^{169}\text{Yb}$  sources are 80 cm diameter  $\times$  80 cm height, whereas for  $^{125}\text{I}$  OcuProsta source, 30 cm diameter  $\times$  30 cm height cylindrical water phantom is considered for MC calculations. **Results:** The dosimetric parameters calculated using `egs_brachy` are compared against the values published in the literature. The calculated values of dose rate constants from this study agree with the published values within statistical uncertainties for all investigated sources. Good agreement is found between the `egs_brachy` calculated radial dose functions,  $g(r)$ , anisotropy functions, and 2D dose rate data with the published values (within 2%) for the same phantom dimensions. For  $^{192}\text{Ir}$  VS2000 source, difference of about 28% is observed in  $g(r)$  value at 18 cm from the source which is due to differences in the phantom dimensions. **Conclusion:** The study validates TG-43 dose parameters calculated using `egs_brachy` for  $^{192}\text{Ir}$ ,  $^{169}\text{Yb}$ , and  $^{125}\text{I}$  brachytherapy sources with the values published in the literature.

**Keywords:** Brachytherapy, `egs_brachy`, EGSnrc code system, Monte Carlo, TG-43 dosimetry

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## INTRODUCTION

As per the American Association of Physicists in Medicine (AAPM) Task Group 43 (TG-43) recommendations, Monte Carlo (MC) investigators should reproduce previously published dose distributions for at least one widely used brachytherapy source model whenever new features of the code are explored.<sup>[1,2]</sup> `egs_brachy`<sup>[3,4]</sup> is a new user-code of EGSnrc code system<sup>[5]</sup> designed especially for brachytherapy applications. To the best of our knowledge, TG-43 dosimetry parameters are investigated for two high-dose rate (HDR)

sources  $^{192}\text{Ir}$  MicroSelectron V2 and BEBIG  $^{60}\text{Co}$  (model Co0. A86) using `egs_brachy` code.<sup>[3,6]</sup> Recently, TG-43 parameters are calculated by Safigholi *et al.*<sup>[7]</sup> for low-energy ( $\leq 50\text{ keV}$ ) photon-emitting low-dose rate (LDR) brachytherapy

**Address for correspondence:** Dr. Subhalaxmi Mishra, Division of Radiological Physics and Advisory, Health Safety and Environment Group, Bhabha Atomic Research Centre, Mumbai - 400 094, Maharashtra, India.  
E-mail: b.subwu@gmail.com

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sources (40 numbers) using `egs_brachy` to update the Carleton Laboratory for Radiotherapy Physics TG-43 dosimetry database. TG-43 parameters vary significantly with different source designs and encapsulation materials due to the existence of high-dose gradient region around it. Hence, it is important to benchmark the dosimetry dataset of a given brachytherapy source model before carrying out further studies using a new MC code.

The purpose of the present study is to benchmark the TG-43 dosimetric parameters calculated using the new user-code `egs_brachy`<sup>[3,4]</sup> for three different radionuclides <sup>192</sup>Ir, <sup>169</sup>Yb, and <sup>125</sup>I which represent high-, intermediate-, and low-energy sources, respectively. The brachytherapy sources for which TG-43 parameters are not available using `egs_brachy`<sup>[3,4]</sup> MC code are chosen for benchmarking and the sources considered for the investigation are HDR <sup>192</sup>Ir (Model VS2000),<sup>[8]</sup> HDR <sup>169</sup>Yb (Model 4140)<sup>[9]</sup> and LDR <sup>125</sup>I (Model OcuProsta).<sup>[10]</sup> Thus, this study covers a range of photon energies relevant in brachytherapy.

<sup>192</sup>Ir HDR VS2000<sup>[8]</sup> source is widely in use for clinical applications and differs significantly from other commercially available <sup>192</sup>Ir HDR brachytherapy sources in their dimensions such as active length, active diameter, and the encapsulation materials. It consists of two active sources of 2.5 mm each, as compared to the single source of typical active length of about 3.5 mm; the active diameter of VS2000 sources is 0.35 mm as compared to the typical active diameter of 0.6 mm. Alloy of Nickel and Titanium is used as the encapsulation material in VS2000 whereas stainless steel is used in other brachytherapy sources. For VS2000<sup>[8]</sup> source, Angelopoulos *et al.*<sup>[8]</sup> calculated TG-43 dosimetric parameters in a 30 cm diameter spherical water phantom using an `egs_brachy` analytical MC code.<sup>[11-13]</sup> In another study, Taylors and Rogers<sup>[14]</sup> calculated the TG-43 dosimetric parameters in a rectilinear water phantom of dimensions of 80 cm × 80 cm × 80 cm for <sup>192</sup>Ir VS2000<sup>[8]</sup> and <sup>169</sup>Yb 4140<sup>[9]</sup> sources using the MC code BrachyDose.<sup>[15,16]</sup> Medich *et al.*<sup>[9]</sup> calculated TG-43 dosimetric parameters in a 40 cm diameter spherical water phantom for <sup>169</sup>Yb (model 4140) source using MCNP5 MC code.<sup>[17]</sup>

OcuProsta is an indigenous model of <sup>125</sup>I brachytherapy source designed and fabricated by Radiopharmaceuticals Division of Bhabha Atomic Research Centre for brachytherapy applications.<sup>[10,18-20]</sup> This source is clinically used in permanent prostate implant.<sup>[20]</sup> It consists of 0.5 mm diameter and 3.0 mm long silver rod coated with palladium on which <sup>125</sup>I is adsorbed and encapsulated in a hollow cylindrical 0.05 mm thick titanium tube. The external dimensions of the seed are 0.8 mm diameter and 4.75 mm length. Sharma *et al.*<sup>[10]</sup> calculated TG-43 parameters in a 30 cm diameter spherical water phantom for this source using MCNP Version 3.1<sup>[21]</sup> MC code. The authors have calculated radial dose functions up to a distance of 5 cm and anisotropy function at  $r = 1, 2,$

3, and 5 cm for polar angles from 0° to 90° at 10° interval. In another study, Sahoo *et al.*<sup>[22]</sup> reported dose rate constant and radial dose functions (up to a distance of 10 cm) for this source using DORZnrc user-code<sup>[23]</sup> of EGSnrc code system.<sup>[5]</sup>

In the present study, TG-43 dosimetric parameters such as air-kerma strength,  $S_k$ , dose rate constant,  $\Lambda$ , radial dose function,  $g(r)$  and anisotropy function,  $F(r; \theta)$  and two-dimensional (2D) absorbed dose rate data (along-away table) are calculated for <sup>192</sup>Ir HDR VariSource VS2000,<sup>[8]</sup> <sup>169</sup>Yb HDR 4140<sup>[9]</sup>, and <sup>125</sup>I LDR OcuProsta<sup>[10]</sup> brachytherapy sources using the new user-code `egs_brachy`<sup>[3,4]</sup> of the EGSnrc code system.<sup>[5]</sup> Statdose<sup>[24]</sup> and 3ddose\_tools<sup>[25]</sup> user-codes of EGSnrc code system are used for analyzing the dose distributions obtained from the `egs_brachy` MC code. The TG-43 parameters calculated using `egs_brachy` are compared with the published data.<sup>[10,14,22]</sup> For OcuProsta source,  $F(r; \theta)$  are calculated for additional radial distances  $r = 0.25, 0.5, 7.5,$  and 10 cm for polar angles 0°–90° at an interval of 2°–5°. 2D-dose rate data (along-away table) is also calculated in this study which is not available for this source.

## MATERIALS AND METHODS

### Egs\_brachy Monte Carlo code

MC-based EGSnrc code system<sup>[5]</sup> consists of several user-codes<sup>[23]</sup> dedicated to address specific applications. `egs_brachy`<sup>[3,4]</sup> is a fast and versatile new user-code of EGSnrc code system designed especially for brachytherapy applications. `egs_brachy` is a modern EGSnrc application which employs C++ class library (`egs++`)<sup>[26]</sup> for modeling geometries and particle sources.

### Brachytherapy sources

Brachytherapy sources investigated in this study were HDR <sup>192</sup>Ir VariSource (Model VS2000),<sup>[8]</sup> <sup>169</sup>Yb HDR (Model 4140)<sup>[9]</sup> and <sup>125</sup>I LDR (Model OcuProsta).<sup>[10]</sup> The geometry, dimensions, and material details of the above sources were taken from the published studies.<sup>[8-10]</sup> The photon energy spectra of <sup>192</sup>Ir and <sup>169</sup>Yb needed for the MC calculations were taken from literature.<sup>[9,27]</sup> For <sup>125</sup>I source, the photon spectrum was taken from AAPM TG-43U1.<sup>[2]</sup>

### Monte Carlo calculations

In the MC calculations of absorbed dose to water, the brachytherapy source was positioned at the center of the water phantom of mass density 0.998 g/cm<sup>3</sup>. For <sup>192</sup>Ir VS2000<sup>[8]</sup> and <sup>169</sup>Yb 4140<sup>[9]</sup> sources, a cylindrical water phantom of dimensions 80 cm diameter and 80 cm height was simulated which was consistent with the recommendation of AAPM and ESTRO Report for photon-emitting brachytherapy sources with an average energy higher than 50 keV.<sup>[28,29]</sup> For OcuProsta<sup>[10]</sup> source, a cylindrical water phantom of dimensions 30 cm diameter

and 30 cm height was considered which was consistent with the AAPM TG-43U1 recommendations.<sup>[2]</sup> The geometric center of the active part of the source was taken as the origin. The water phantom was divided into a number of cylindrical voxels with different sizes. For high-dose gradients regions, small voxel sizes were adapted. Absorbed dose was scored in voxels of dimensions 0.1 mm × 0.1 mm for distance  $r \leq 1$  cm, 0.5 mm × 0.5 mm voxels for  $1 < r \leq 5$  cm, 1 mm × 1 mm voxels for  $5 < r \leq 10$  cm, and 2 mm × 2 mm voxels for  $10 < r \leq 20$  cm. For  $S_k$  calculations, the source was immersed at the center of a 50 cm diameter vacuum sphere. Air-kerma per history was calculated in a voxel of dimension 0.1 cm × 0.1 cm × 0.05 cm filled with air (40% humidity, as recommended by TG-43U1<sup>[2]</sup>) located at a distance of 10 cm from the transverse axis of the source.

The PEGS4 dataset needed for MC calculations is based on the XCOM<sup>[30]</sup> compilations. For the investigated sources, charged particle equilibrium was assumed and collision-kerma was considered as absorbed dose since the range of secondary electrons is short.<sup>[4]</sup> The photon fluence spectrum scored using track length estimator was converted to collision-kerma to water by using the mass energy-absorption coefficients of water. Up to  $8 \times 10^9$  photon histories were simulated. Uncertainties were calculated with the default history-by-history method

used in EGSnrc code system.<sup>[31]</sup> As per the recommendations of AAPM TG-268,<sup>[32]</sup> Table 1 summarizes the parameters used in the MC calculations.

## RESULTS AND DISCUSSION

### Air-kerma strength, $S_k$

The MC-calculated air-kerma per history obtained at 10 cm was corrected to give the air-kerma per history at a point of 1 m. The values of  $S_k$  calculated for <sup>192</sup>Ir VS2000, <sup>169</sup>Yb 4140, and <sup>125</sup>I OcuProsta sources are  $1.202 \pm 0.0014 \times 10^{-13}$ ,  $2.184 \pm 0.0019 \times 10^{-14}$ , and  $4.138 \pm 0.0017 \times 10^{-14}$  Gy cm<sup>2</sup>/history, respectively.

### Dose rate constant, $\Lambda$

The dose rate constant ( $\Lambda$ ) was calculated by dividing the absorbed dose to water per history at reference position (1 cm, 90°) in the water phantom to the  $S_k$  per history. The values of  $\Lambda$  for <sup>192</sup>Ir VS2000, <sup>169</sup>Yb 4140 and <sup>125</sup>I OcuProsta sources are  $1.099 \pm 0.003$ ,  $1.186 \pm 0.003$ , and  $0.962 \pm 0.003$  cGyh<sup>-1</sup>U<sup>-1</sup>, respectively. The egs\_brachy-calculated values of dose rate constants are in excellent agreement with the published values<sup>[8-10,14,22]</sup> within statistical uncertainties for all investigated sources.

**Table 1: Summary of parameters used for Monte Carlo calculations as per the recommendations of American Association of Physicists in Medicine task group-286**

Item name	Descriptions	References
Code, version/release date	egs_brachy, 2017 version/September 15, 2017	[3,4]
Validation	Validated for <sup>192</sup> Ir MicroSelectron V2, BEBIG <sup>60</sup> Co and about 40 numbers of LDR brachytherapy sources	[3,6,7]
Timing	About 7680 total CPU hours on Intel (R) Xeon (R) 32 CPUs with clock speeds of 2.6 GHz	
Source description	<sup>192</sup> Ir HDR (Model VS2000): It consists of two active sources made of iridium ( $\rho=22.42$ g/cm <sup>3</sup> ) of 2.5 mm long and 0.35 mm diameter each. The uniformly distributed radioactive iridium core is encapsulated in a nickel and titanium alloy ( $\rho=6.95$ g/cm <sup>3</sup> ). Photons are uniformly distributed in the active iridium core and the photon emission is isotropic <sup>169</sup> Yb HDR (Model 4140): It consists of a 0.73 mm diameter and 3.6 mm long ytterbium oxide rod ( $\rho=6.9$ g/cm <sup>3</sup> ) enclosed in a stainless steel capsule ( $\rho=7.8$ g/cm <sup>3</sup> ). Photons are uniformly distributed in the active core and the photon emission is isotropic <sup>125</sup> I LDR (Model OcuProsta): It consists of 0.5 mm diameter and 3 mm long silver rod ( $\rho=10.5$ g/cm <sup>3</sup> ) coated with palladium on which <sup>125</sup> I is adsorbed and encapsulated in a hollow cylindrical 0.05 mm thick titanium tube. Photons are uniformly distributed in 0.003 cm thick layer of NaI ( $\rho=3.67$ g/cm <sup>3</sup> ) which is coated on the surface of <sup>103</sup> Pd core and the photon emission is isotropic	[8-10]
Cross-sections	Photon cross-sections and mass-energy absorption coefficients are calculated using XCOM database	[30]
Transport parameters	Rayleigh scattering, bound Compton scattering, photoelectric absorption, and fluorescent emission of characteristic X-rays processes are simulated in all the calculations For <sup>192</sup> Ir VS2000 and <sup>169</sup> Yb HDR 4140 sources, PCUT=10 keV and ECUT=1.5 MeV used in all calculations For <sup>125</sup> I OcuProsta source, PCUT=1 keV and ECUT=1 MeV in all calculations, except $S_k$ calculations for which PCUT=5 keV	
VRT and AIET	No variance reduction technique is used in this study	
Scored quantities	Dose to medium is scored using track length estimator	
Number of histories/statistical uncertainties	Up to $8 \times 10^9$ photon histories are simulated/ $1\sigma$ statistical uncertainties on the calculated values are <1% for $r < 10$ cm, <2% for $r=10-15$ cm and <3% for $r=10-20$ cm	
Statistical methods	Uncertainties are calculated with the default history-by-history method used in EGSnrc	[31]
Postprocessing	TG-43 parameters are calculated using the TG-43 formalism and the results are reported without using any kind of filtrations	[1,2]

LDR: Low-dose rate, CPU: Central processing unit, TG-43: Task group 43, PCUT: Photon cutoff energy, ECUT: Electron cutoff energy

**Table 2: Radial dose function,  $g(r)$ , of  $^{192}\text{Ir}$  VS2000 and  $^{169}\text{Yb}$  4140 high-dose-rate brachytherapy sources**

Distance $r$ (cm)	$^{192}\text{Ir}$ VS2000			$^{169}\text{Yb}$ 4140		
	This study	Published <sup>[14]</sup>	Difference (%)	This study	Published <sup>[14]</sup>	Difference (%)
0.25	0.990	0.991	-0.10	0.932	0.927	0.54
0.3	0.990	0.993	-0.30	0.940	0.934	0.64
0.4	0.995	0.995	0.00	0.949	0.945	0.42
0.5	0.999	0.997	0.20	0.958	0.955	0.31
0.6	0.999	0.997	0.20	0.967	0.966	0.10
0.7	1.000	0.997	0.30	0.977	0.975	0.21
0.75	1.000	0.999	0.10	0.979	0.978	0.10
0.8	1.000	1.000	0.00	0.986	0.982	0.41
0.9	1.000	0.998	0.20	0.993	0.993	0.00
1	1.000	1.000	0.00	1.000	1.000	0.00
1.25	1.006	1.004	0.20	1.020	1.021	-0.10
1.5	1.006	1.005	0.10	1.041	1.040	0.10
1.75	1.007	1.007	0.00	1.061	1.057	0.38
2	1.011	1.010	0.10	1.077	1.074	0.28
2.5	1.012	1.011	0.10	1.107	1.101	0.54
3	1.014	1.012	0.20	1.130	1.119	0.98
3.5	1.011	1.014	-0.30	1.143	1.137	0.53
4	1.011	1.013	-0.20	1.152	1.147	0.44
4.5	1.010	1.013	-0.30	1.168	1.157	0.95
5	1.008	1.011	-0.30	1.160	1.161	-0.09
6	1.001	1.003	-0.20	1.165	1.158	0.60
7	0.992	0.994	-0.20	1.151	1.140	0.96
8	0.979	0.982	-0.31	1.120	1.111	0.81
9	0.963	0.966	-0.31	1.076	1.084	-0.74
10	0.947	0.949	-0.21	1.053	1.047	0.57
11	0.926	0.930	-0.43	1.017	1.004	1.29
12	0.906	0.908	-0.22	0.972	0.960	1.25
13	0.886	0.884	0.23	0.928	0.913	1.64
14	0.859	0.858	0.12	0.882	0.867	1.73
15	0.832	0.834	-0.24	0.806	0.820	-1.71
16	0.797	0.805	-0.99	0.790	0.776	1.80
17	0.768	0.777	-1.16	0.719	0.732	-1.78
18	0.758	0.749	1.20	0.696	0.686	1.46
19	0.720	0.721	-0.14	0.652	0.644	1.24
20	0.688	0.694	-0.86	0.610	0.599	1.84

The calculated data are based on a cylindrical liquid water phantom of dimensions 80 cm diameter×80 cm height

### Radial dose function, $g(r)$

Radial dose function,  $g(r)$ , calculated for  $^{192}\text{Ir}$  VS2000 and  $^{169}\text{Yb}$  4140 sources for distances  $r = 0.25$ –20 cm were presented in Table 2 along with the corresponding published values.<sup>[14]</sup> For  $^{125}\text{I}$  OcuProsta source,  $g(r)$  values are calculated up to a distance of 10 cm and are presented in Figure 1 along with the corresponding published values.<sup>[10,22]</sup>  $g(r)$  values for  $^{192}\text{Ir}$  VS2000 source were found to be in good agreement with the published values<sup>[14]</sup> with a maximum deviation of about 1.2% at a distance  $r = 18$  cm. However, significant differences in  $g(r)$  values were observed beyond  $r = 8$  cm which increases gradually with  $r$  when compared with the  $g(r)$  values (a maximum difference of about 28% at  $r = 18$  cm) calculated by Angelopoulos *et al.*<sup>[8]</sup> This

is due to the fact that Angelopoulos *et al.*<sup>[8]</sup> considered spherical water phantom of 40 cm diameter in their study whereas in the present study a cylindrical phantom of 80 cm diameter ×80 cm height is considered. The phantom dimensions significantly affect  $g(r)$  values only near the phantom boundaries. This effect is due to the reduction of scatter contribution to overall dose at the edges of the phantom.

For  $^{169}\text{Yb}$  4140 and  $^{125}\text{I}$  OcuProsta sources, excellent agreement is found between the  $g(r)$  values calculated using egs\_brachy and the published values.<sup>[14,22]</sup> A maximum deviations of about 1.8% at a distance  $r = 20$  cm and 0.68% at a distance  $r = 10$  cm are observed for  $^{169}\text{Yb}$  4140 and  $^{125}\text{I}$  OcuProsta sources, respectively.

**Table 3: Anisotropy function,  $F(r,\theta)$ , of  $^{192}\text{Ir}$  VS2000 high-dose-rate brachytherapy source**

$\theta$ (deg)	distance $r$ (cm)										
	0.25	0.5	1	2	3	4	5	7.5	10	12.5	15
0	-	-	0.524	0.536	0.577	0.605	0.638	0.670	0.741	0.791	0.767
1	-	-	0.530	0.536	0.571	0.612	0.639	0.692	0.741	0.791	0.769
2	-	-	0.541	0.558	0.584	0.624	0.672	0.709	0.752	0.805	0.814
3	-	-	0.571	0.584	0.624	0.663	0.695	0.712	0.767	0.809	0.824
5	-	-	0.643	0.657	0.667	0.716	0.722	0.780	0.783	0.842	0.843
7	-	-	0.705	0.715	0.712	0.775	0.795	0.810	0.813	0.858	0.842
10	-	-	0.780	0.784	0.808	0.818	0.826	0.834	0.837	0.889	0.875
12	-	-	0.805	0.809	0.822	0.838	0.854	0.870	0.875	0.926	0.868
15	-	-	0.840	0.847	0.856	0.890	0.896	0.896	0.903	0.839	0.913
20	-	-	0.892	0.883	0.886	0.898	0.909	0.927	0.947	0.959	0.924
25	-	0.941	0.914	0.916	0.918	0.925	0.952	0.940	0.957	0.967	0.916
30	-	0.955	0.937	0.931	0.944	0.957	0.967	0.942	0.966	0.985	0.931
35	-	0.950	0.960	0.946	0.957	0.959	0.973	0.959	0.969	0.993	0.935
40	-	0.980	0.972	0.963	0.971	0.978	0.994	0.979	0.980	0.994	0.943
45	-	0.996	0.973	0.978	0.975	0.964	0.987	0.981	0.989	1.011	0.953
50	-	0.997	0.984	0.978	0.970	0.994	0.999	0.981	0.996	1.015	0.962
55	0.996	0.997	0.994	0.984	0.988	0.991	0.996	0.983	0.993	1.015	0.947
60	0.997	1.004	0.986	0.996	0.988	0.991	1.012	0.979	0.985	1.016	0.968
65	0.997	1.006	0.995	0.996	0.989	0.993	1.010	0.976	0.994	1.013	0.949
70	0.998	0.996	1.006	0.987	0.984	1.000	1.003	0.987	1.006	1.005	0.949
75	0.998	1.010	1.002	0.999	0.990	0.998	0.999	1.003	1.000	1.009	0.969
80	0.999	1.009	1.001	0.994	1.014	0.997	0.998	1.000	0.999	1.012	0.975
85	0.999	0.991	1.000	1.006	1.003	1.001	1.000	1.016	0.999	1.013	0.981
90	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
95	0.999	0.996	1.000	1.012	0.990	1.006	1.002	1.000	1.000	1.003	0.996
100	0.999	1.008	1.002	1.000	1.004	1.008	1.000	0.994	0.992	1.004	0.968
105	0.999	1.006	1.000	0.990	0.989	1.003	1.000	1.006	1.021	0.996	0.968
110	0.999	1.001	1.003	0.999	0.988	0.997	0.998	1.012	1.014	0.998	0.954
115	0.998	1.008	0.991	0.990	0.980	0.995	0.996	1.015	1.004	0.998	0.968
120	0.997	1.000	0.993	0.987	0.991	0.999	0.994	0.983	0.995	0.994	0.978
125	0.995	0.980	0.994	0.978	0.980	0.997	0.992	0.993	1.004	0.989	0.959
130	-	1.006	0.979	0.972	0.975	0.994	0.985	0.980	0.991	0.987	0.943
135	-	1.008	0.973	0.980	0.971	0.968	0.975	0.973	0.991	0.986	0.949
140	-	0.995	0.971	0.961	0.963	0.972	0.987	0.961	0.974	0.981	0.935
145	-	0.969	0.964	0.950	0.950	0.951	0.969	0.980	0.983	0.979	0.933
150	-	0.982	0.933	0.940	0.930	0.951	0.964	0.967	0.969	0.981	0.912
155	-	0.989	0.921	0.906	0.912	0.926	0.951	0.938	0.934	0.966	0.919
160	-	-	0.895	0.894	0.891	0.902	0.919	0.890	0.919	0.957	0.906
165	-	-	0.835	0.840	0.843	0.865	0.867	0.870	0.908	0.907	0.866
168	-	-	0.808	0.804	0.833	0.853	0.859	0.850	0.891	0.903	0.856
170	-	-	-	0.762	0.801	0.809	0.838	0.843	0.886	0.894	0.877
173	-	-	-	0.724	0.731	0.739	0.752	0.819	0.840	0.865	0.827
175	-	-	-	-	0.644	0.702	0.718	0.756	0.775	0.802	0.788
177	-	-	-	-	-	0.634	0.673	0.708	0.740	0.794	0.793
178	-	-	-	-	-	-	-	0.662	0.719	0.781	0.755
179	-	-	-	-	-	-	-	0.608	0.682	0.685	0.740
180	-	-	-	-	-	-	-	0.546	0.621	0.644	0.686

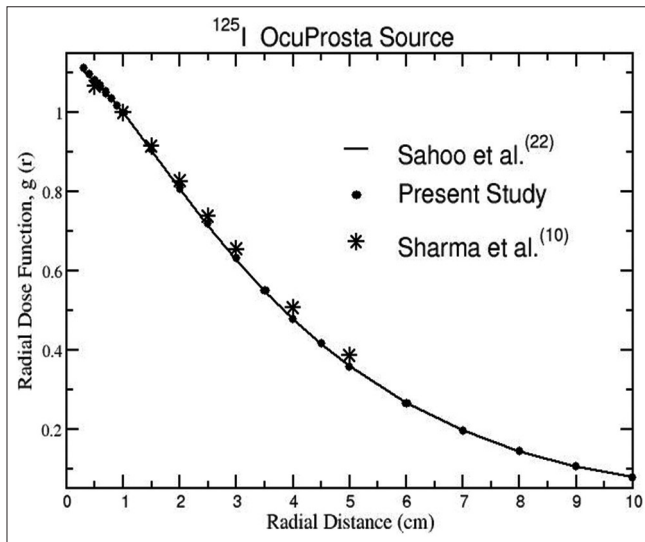
The calculated data are based on a cylindrical liquid water phantom of dimensions 80 cm diameter  $\times$  80 cm height

### Anisotropy function, $F(r,\theta)$

For  $^{192}\text{Ir}$  VS2000,  $^{169}\text{Yb}$  4140 sources,  $F(r;\theta)$  were calculated at radii of 0.25, 0.5, 0.75, 1, 2, 3, 4, 5, 7.5, 10, 12.5, and

15 cm for polar angles from  $0^\circ$  to  $180^\circ$  with varying intervals.

For  $^{125}\text{I}$  OcuProsta source,  $F(r;\theta)$  were calculated for polar angles  $0^\circ$  to  $90^\circ$  at radii of 0.25, 0.5, 0.75, 1, 2, 3, 4, 5, 7.5,



**Figure 1:** Radial dose function,  $g(r)$ , of  $^{125}\text{I}$  LDR OcuProsta brachytherapy source for radial distances 0.25–10 cm. The calculated data are based on a cylindrical liquid water phantom of dimensions 30 cm diameter  $\times$  30 cm height

and 10 cm because of the symmetry of the source. Tables 3–5 present the  $F(r;\theta)$  values for  $^{192}\text{Ir}$  VS2000,  $^{169}\text{Yb}$  4140, and  $^{125}\text{I}$  OcuProsta sources, respectively. For  $^{192}\text{Ir}$  VS2000 and  $^{169}\text{Yb}$  4140 sources, values of  $F(r;\theta)$  are in good agreement with the published values<sup>[14]</sup>

For  $^{125}\text{I}$  OcuProsta source, the values of  $F(r;\theta)$  are in good agreement with the published values.<sup>[10]</sup> Figure 2a and b presents the values of  $F(r;\theta)$  at different polar angles along with the corresponding published values<sup>[10]</sup> at radial distances  $r = 1$  and 5 cm, respectively.

### Along and away two-dimensional dose rate distribution

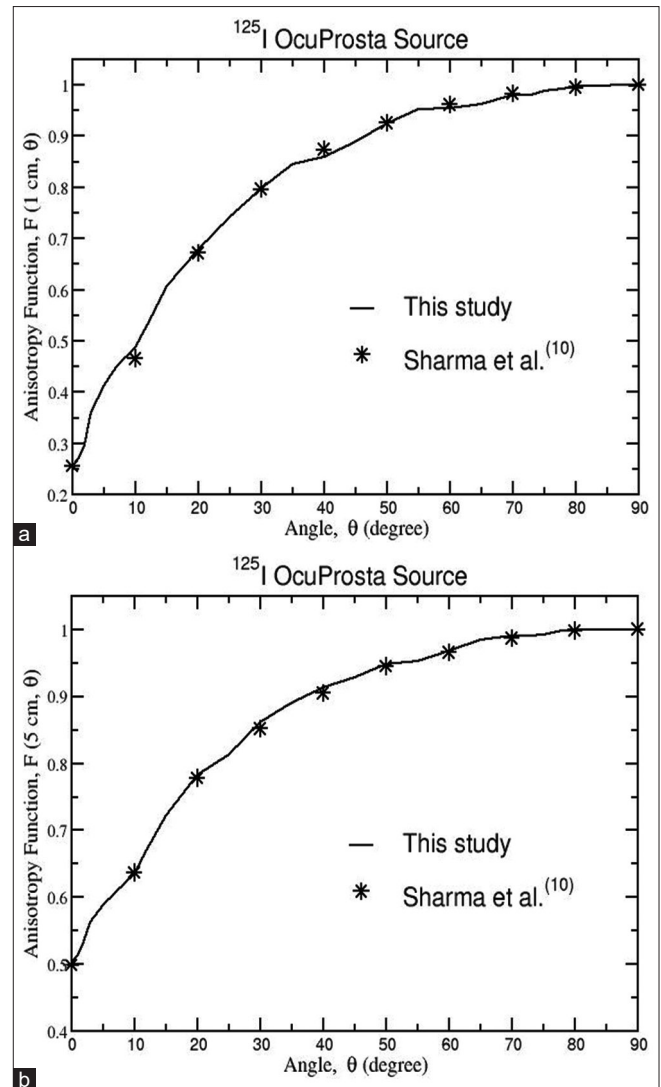
For  $^{125}\text{I}$  OcuProsta source absorbed dose per unit air-kerma strength was calculated up to a distance of 10 cm and presented in Table 6. The 2D-dose rate values for  $^{192}\text{Ir}$  VS 2000 and  $^{169}\text{Yb}$  4140 sources agree well with the published data<sup>[14]</sup> within 2%. It may be noted that, for  $^{125}\text{I}$  OcuProsta source, 2D along-away table is not available for comparison.

### Uncertainties

The uncertainties associated with the estimated quantities are only statistical. It does not include Type B uncertainty related to cross-section, source geometry, source material, and size of the voxel. However, to minimize the uncertainty that may arise due to dimensions of voxel, distance-specific voxel dimensions were chosen as recommended by Taylor *et al.*<sup>[15]</sup> In this study,  $1\sigma$  statistical uncertainties on the calculated dosimetry values are  $<1\%$  at distances  $r < 10$  cm,  $<2\%$  at distances  $r = 10$ –15 cm, and  $<3\%$  at distances  $r = 10$ –20 cm.

### CONCLUSION

In this study, TG-43 dosimetric parameters were calculated for  $^{192}\text{Ir}$  VS2000,  $^{169}\text{Yb}$  4140, and  $^{125}\text{I}$  OcuProsta brachytherapy



**Figure 2:** (a) Anisotropy function,  $F(r,\theta)$ , of  $^{125}\text{I}$  LDR OcuProsta brachytherapy source at a radial distance of 1 cm. The calculated data are based on a cylindrical liquid water phantom of dimensions 30 cm diameter  $\times$  30 cm height. (b) Anisotropy Function,  $F(r,\theta)$ , of  $^{125}\text{I}$  LDR OcuProsta brachytherapy source at a radial distance of 5 cm. The calculated data are based on a cylindrical liquid water phantom of dimensions 30 cm diameter  $\times$  30 cm height

sources using the new `egs_brachy` user-code of the EGSnrc code system. The calculated dosimetric parameters are in good agreement with the published data. The present study validates the new user-code `egs_brachy` with the published dose distributions. This study thus demonstrates the ability of `egs_brachy` MC code to handle the transport of photons and electrons accurately at brachytherapy photon energies such as  $^{192}\text{Ir}$ ,  $^{169}\text{Yb}$ , and  $^{125}\text{I}$ . The study also demonstrates the capability of the `egs_brachy` to model the complex geometry of sources accurately. For example, the simulation of VS2000 which consists of two cylindrical sources having spherical caps at both ends, which is not possible using user-code such as DOSRZnrc due to the limitations associated with it.

**Table 4: Anisotropy function,  $F(r,\theta)$ , of  $^{169}\text{Yb}$  4140 high-dose rate brachytherapy source**

$\theta$ (°)	Distance $r$ (cm)										
	0.25	0.50	1.00	2.00	3.00	4.00	5.00	7.50	10.00	12.50	15.00
0	-	0.555	0.558	0.609	0.660	0.696	0.726	0.774	0.802	0.833	0.850
1	-	0.556	0.558	0.609	0.657	0.696	0.725	0.774	0.814	0.832	0.850
2	-	0.555	0.558	0.612	0.662	0.698	0.726	0.780	0.813	0.833	0.850
3	-	0.556	0.559	0.616	0.666	0.703	0.731	0.783	0.813	0.835	0.851
5	-	0.560	0.571	0.628	0.676	0.712	0.737	0.791	0.812	0.838	0.855
7	-	0.571	0.589	0.644	0.690	0.724	0.749	0.801	0.825	0.846	0.860
10	-	0.598	0.620	0.671	0.715	0.746	0.768	0.812	0.832	0.854	0.869
12	-	0.621	0.642	0.691	0.731	0.758	0.779	0.824	0.843	0.862	0.878
15	-	0.658	0.676	0.719	0.754	0.783	0.798	0.837	0.852	0.871	0.883
20	-	0.716	0.728	0.764	0.795	0.816	0.829	0.859	0.876	0.889	0.898
25	-	0.769	0.777	0.804	0.828	0.844	0.855	0.886	0.892	0.905	0.912
30	-	0.814	0.819	0.839	0.857	0.872	0.880	0.901	0.912	0.921	0.927
35	-	0.851	0.849	0.868	0.885	0.894	0.900	0.922	0.926	0.935	0.938
40	-	0.883	0.884	0.895	0.908	0.915	0.917	0.935	0.939	0.945	0.951
45	-	0.909	0.909	0.916	0.930	0.937	0.940	0.956	0.952	0.958	0.960
50	-	0.931	0.931	0.937	0.946	0.951	0.953	0.963	0.965	0.968	0.972
55	0.963	0.951	0.950	0.952	0.959	0.962	0.964	0.973	0.971	0.976	0.979
60	0.973	0.963	0.960	0.967	0.974	0.976	0.976	0.984	0.983	0.982	0.984
65	0.981	0.976	0.979	0.978	0.984	0.984	0.985	0.994	0.989	0.990	0.990
70	0.988	0.985	0.986	0.986	0.991	0.992	0.994	1.002	0.995	0.995	0.994
75	0.994	0.991	0.991	0.993	0.997	0.997	0.998	1.004	0.996	0.998	0.999
80	0.997	0.998	0.997	0.997	1.000	1.000	1.000	1.004	1.002	1.003	1.002
85	0.998	1.000	1.000	0.997	1.003	1.004	1.000	1.004	0.995	1.001	1.001
90	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000
95	0.998	0.999	1.002	0.998	1.001	1.002	1.001	1.003	0.999	1.002	1.000
100	0.997	0.997	0.995	0.994	0.999	1.001	0.999	1.001	1.000	1.001	0.996
105	0.993	0.990	0.992	0.990	0.994	0.994	0.991	0.996	0.993	0.996	0.998
110	0.989	0.984	0.985	0.983	0.988	0.992	0.991	0.995	0.989	0.994	0.992
115	0.981	0.975	0.974	0.975	0.980	0.981	0.978	0.989	0.988	0.988	0.988
120	0.973	0.960	0.964	0.966	0.971	0.973	0.969	0.979	0.974	0.981	0.981
125	0.963	0.946	0.947	0.949	0.957	0.961	0.959	0.970	0.967	0.971	0.975
130	-	0.928	0.927	0.932	0.942	0.947	0.950	0.960	0.959	0.963	0.967
135	-	0.904	0.902	0.911	0.923	0.929	0.933	0.943	0.946	0.952	0.955
140	-	0.877	0.880	0.888	0.902	0.910	0.915	0.929	0.932	0.940	0.946
145	-	0.843	0.843	0.859	0.878	0.888	0.894	0.912	0.918	0.926	0.931
150	-	0.805	0.805	0.827	0.847	0.861	0.871	0.894	0.903	0.910	0.919
155	-	0.754	0.760	0.789	0.816	0.832	0.845	0.872	0.881	0.895	0.902
160	-	-	0.708	0.744	0.775	0.798	0.813	0.847	0.860	0.877	0.888
165	-	-	0.644	0.690	0.730	0.755	0.776	0.818	0.837	0.856	0.872
168	-	-	0.596	0.652	0.698	0.731	0.752	0.801	0.821	0.845	0.859
170	-	-	0.560	0.625	0.673	0.710	0.736	0.787	0.808	0.835	0.850
173	-	-	0.505	0.583	0.639	0.679	0.711	0.763	0.797	0.823	0.840
175	-	-	0.472	0.557	0.618	0.661	0.693	0.759	0.786	0.815	0.835
177	-	-	0.457	0.537	0.599	0.644	0.677	0.742	0.778	0.808	0.827
178	-	-	0.455	0.532	0.594	0.639	0.672	0.740	0.777	0.805	0.825
179	-	-	0.451	0.528	0.590	0.636	0.671	0.736	0.772	0.803	0.821
180	-	-	0.454	0.527	0.589	0.633	0.665	0.733	0.774	0.802	0.819

The calculated data are based on a cylindrical liquid water phantom of dimensions 80 cm diameter×80 cm height

**Table 5: Anisotropy function,  $F(r,\theta)$ , of  $^{125}\text{I}$  OcuProsta low-dose rate brachytherapy source**

Theta (deg)	Distance (r)									
	0.25	0.5	0.75	1	2	3	4	5	7.5	10
0	0.199	0.209	0.233	0.256	0.370	0.437	0.501	0.504	0.634	0.696
1	0.226	0.251	0.268	0.272	0.395	0.450	0.509	0.514	0.655	0.723
2	0.245	0.270	0.288	0.298	0.411	0.509	0.515	0.534	0.671	0.728
3	0.285	0.337	0.347	0.361	0.454	0.470	0.522	0.563	0.687	0.723
5	0.320	0.352	0.409	0.412	0.486	0.495	0.561	0.589	0.706	0.730
7	0.349	0.391	0.434	0.448	0.507	0.523	0.605	0.607	0.721	0.747
10	0.381	0.443	0.468	0.469	0.557	0.592	0.685	0.635	0.739	0.767
12	0.424	0.456	0.522	0.522	0.593	0.634	0.710	0.671	0.755	0.781
15	0.475	0.511	0.586	0.607	0.679	0.672	0.751	0.723	0.775	0.809
20	0.585	0.629	0.667	0.678	0.734	0.740	0.794	0.782	0.824	0.838
25	0.665	0.715	0.736	0.742	0.781	0.786	0.828	0.813	0.870	0.859
30	0.727	0.782	0.782	0.798	0.828	0.825	0.868	0.862	0.889	0.890
35	0.769	0.827	0.837	0.846	0.863	0.862	0.901	0.890	0.910	0.904
40	0.804	0.847	0.851	0.860	0.900	0.894	0.921	0.912	0.931	0.933
45	0.836	0.870	0.879	0.888	0.924	0.913	0.941	0.929	0.946	0.944
50	0.864	0.893	0.916	0.924	0.941	0.938	0.966	0.949	0.961	0.962
55	0.871	0.937	0.947	0.952	0.942	0.945	0.971	0.952	0.972	0.962
60	0.889	0.935	0.952	0.954	0.970	0.960	0.981	0.968	0.981	0.987
65	0.909	0.945	0.959	0.962	0.987	0.981	0.989	0.985	0.989	0.986
70	0.933	0.960	0.979	0.980	0.991	0.994	0.997	0.990	0.990	0.989
73	0.956	0.968	0.981	0.985	0.993	1.000	0.999	0.990	0.990	0.990
75	0.972	0.976	0.985	0.987	0.997	1.000	1.000	0.992	0.990	0.990
78	0.979	0.984	0.995	0.992	0.998	1.000	0.999	0.997	0.992	0.991
80	0.982	0.987	0.999	0.997	0.995	1.000	1.000	0.999	0.993	0.996
82	0.987	0.990	1.000	0.999	0.993	1.000	0.999	1.000	0.994	0.997
84	0.990	0.990	0.999	0.999	0.996	1.000	0.997	0.999	0.999	0.992
85	0.992	0.992	1.000	0.999	0.999	1.000	1.000	1.000	1.000	1.000
86	0.998	0.999	1.001	0.999	0.998	1.000	1.000	1.000	1.000	0.999
87	0.999	0.999	0.999	0.999	0.998	0.999	1.000	1.000	1.000	0.999
88	0.999	0.992	0.999	1.000	0.999	1.000	1.000	1.000	0.999	1.001
89	1.000	0.996	0.998	0.997	0.999	1.000	1.000	1.000	1.000	1.000
90	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000	1.000

The calculated data are based on a cylindrical liquid water phantom of dimensions 30 cm diameter × 30 cm height

**Table 6: Dose rate (2D along away) data per unit air-kerma strength ( $\text{cGyh}^{-1} \text{U}^{-1}$ ) for  $^{125}\text{I}$  OcuProsta low-dose-rate brachytherapy source**

Along (cm)	Away (cm)										
	0.25	0.5	0.75	1	1.5	2	3	4	5	7.5	10
0	13.477	4.075	1.799	0.962	0.389	0.196	0.068	0.029	0.014	0.003	0.001
0.25	7.332	3.203	1.544	0.903	0.378	0.192	0.068	0.029	0.014	0.003	0.001
0.5	2.668	1.861	1.143	0.738	0.341	0.181	0.065	0.028	0.014	0.003	0.001
0.75	1.069	1.008	0.770	0.558	0.294	0.165	0.062	0.027	0.014	0.003	0.001
1	0.564	0.600	0.518	0.410	0.243	0.145	0.058	0.026	0.013	0.003	0.001
1.5	0.215	0.246	0.244	0.219	0.157	0.106	0.048	0.023	0.012	0.003	0.001
2	0.108	0.122	0.127	0.122	0.099	0.074	0.039	0.020	0.011	0.002	0.001
3	0.040	0.042	0.044	0.045	0.041	0.035	0.023	0.013	0.008	0.002	0.001
4	0.019	0.018	0.019	0.019	0.019	0.017	0.013	0.009	0.005	0.002	0.001
5	0.009	0.009	0.009	0.009	0.009	0.009	0.007	0.005	0.004	0.001	---
7.5	0.002	0.002	0.002	0.002	0.002	0.002	0.002	0.001	0.001	0.001	---
10	0.001	0.001	0.001	0.001	0.001	0.001	---	---	---	---	---

The calculated data are based on a cylindrical liquid water phantom of dimensions 30 cm diameter × 30 cm height. “---”Negligible dose rate values



## Ethical approval

This article does not contain any studies with human participants or animals performed.

## Informed consent

Informed consent was obtained from all individual participants included in this study.

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Nil.

## Conflicts of interest

There are no conflicts of interest.

## REFERENCES

- Nath R, Anderson LL, Luxton G, Weaver KA, Williamson JF, Meigooni AS. Dosimetry of interstitial brachytherapy sources: Recommendations of the AAPM Radiation Therapy Committee Task Group No. 43. American Association of Physicists in Medicine. Med Phys 1995;22:209-34.
- Rivard MJ, Coursey BM, DeWerd LA, Hanson WF, Huq MS, Ibbott GS, *et al.* Update of AAPM Task Group No. 43 Report: A revised AAPM protocol for brachytherapy dose calculations. Med Phys 2004;31:633-74.
- Chamberland MJ, Taylor RE, Rogers DW, Thomson RM. egs\_brachy: A versatile and fast Monte Carlo code for brachytherapy. Phys Med Biol 2016;61:8214-31.
- Thomson RM, Taylor RE, Chamberland MJ, Rogers DW. User Manual for egs\_brachy a Versatile and Fast EGSnrc Application for Brachytherapy. Report CLRP-17-02. Carleton University, Ottawa, Canada; 2017.
- Kawrakow I, Seuntjens JP, Rogers DWO, Tessier F, Walters BRB. The EGSnrc Code System: Monte Carlo Simulation of Electron and Photon Transport, NRCC Report No. PIRS-701. Ottawa, Canada: National Research Council of Canada; 2013.
- Reddy BR, Chamberland MJ, Ravikumar M, Varatharaj C. Measurements and Monte Carlo calculation of radial dose and anisotropy functions of BEBIG <sup>60</sup>Co high-dose-rate brachytherapy source in a bounded water phantom. J Contemp Brachytherapy 2019;11:563-72.
- Safigholi H, Chamberland MJ, Taylor RE, Allen CH, Martinov MP, Rogers DW, *et al.* Update of the CLRP TG-43 parameter database for low-energy brachytherapy sources. Med Phys 2020;47:4656-69.
- Angelopoulos A, Baras P, Sakelliou L, Karaiskos P, Sandilos P. Monte Carlo dosimetry of a new <sup>192</sup>Ir high dose rate brachytherapy source. Med Phys 2000;27:2521-7.
- Medich DC, Tries MA, Munro JJ 2<sup>nd</sup>. Monte Carlo characterization of an ytterbium-169 high dose rate brachytherapy source with analysis of statistical uncertainty. Med Phys 2006;33:163-72.
- Sharma SD, Basu M, Shanta A, Selvam TP, Tripathi UB, Bhatt BC. Dosimetry parameters of BARC OcuProsta I-125 seed source. Australas Phys Eng Sci Med 2005;28:14-20.
- Angelopoulos A, Perris A, Sakellariou K, Sakelliou L, Sarigiannis K, Zarris G. Accurate Monte Carlo calculations of the combined attenuation and build-up factors, for energies (20-1500 keV) and distances (0-10 cm) relevant in brachytherapy. Phys Med Biol 1991;36:763-78.
- Karaiskos P, Angelopoulos A, Sakelliou L, Sandilos P, Antypas C, Vlachos L, *et al.* Monte Carlo and TLD dosimetry of an <sup>192</sup>Ir high dose-rate brachytherapy source. Med Phys 1998;25:1975-84.
- Sakelliou L, Sakellariou K, Sarigiannis K, Angelopoulos A, Perris A, Zarris G. Dose rate distributions around <sup>60</sup>Co, <sup>137</sup>Cs, <sup>198</sup>Au, <sup>192</sup>Ir, <sup>241</sup>Am, <sup>125</sup>I (models 6702 and 6711) brachytherapy sources and the nuclide <sup>99</sup>Tcm. Phys Med Biol 1992;37:1859-72.
- Taylor RE, Rogers DW. EGSnrc Monte Carlo calculated dosimetry parameters for <sup>192</sup>Ir and <sup>169</sup>Yb brachytherapy sources. Med Phys 2008;35:4933-44.
- Taylor RE, Yegin G, Rogers DW. Benchmarking brachydose: Voxel based EGSnrc Monte Carlo calculations of TG-43 dosimetry parameters. Med Phys 2007;34:445-57.
- Thomson RM, Yegin G, Taylor R, Sutherland J, Rogers DWO. Fast Monte Carlo dose calculations for brachytherapy with Brachy Dose. Med Phys 2010;37:3910-1.
- Brown FB. MCNP-A General Monte Carlo N-Particle Transport Code, Version 5. Los Alamos National Laboratory, Oak Ridge, TN; 2003.
- Mathew C, Majali MA, Balakrishnan SA. A novel approach for the adsorption of iodine-125 on silver wire as matrix for brachytherapy source for the treatment of eye and prostate cancer. Appl Radiat Isot 2002;57:359-67.
- Manolkar RB, Sane SU, Pillai KT, Majali MA. Comparison of methods for preparation of <sup>125</sup>I brachytherapy source cores for the treatment of eye cancer. Appl Radiat Isot 2003;59:145-50.
- Palled SR, Saminathan S, Pasha T, Naveen T, Ganesh KM, Lokesh V. Prostate permanent implant brachytherapy with BARC I-125 Ocu-Prosta seeds. J Cancer Res Ther 2021;17:340-7.
- Los Alamos Monte Carlo Group, MCNP – A General Monte Carlo Code for Neutron and Photon Transport (version 3.1); 1983.
- Sahoo S, Selvam TP. An EGSnrc investigation of the air-kerma strength, dose rate constant, and radial dose function of <sup>125</sup>I brachytherapy sources. Radiol Phys Technol 2009;2:198-204.
- Rogers DWO, Kawrakow I, Seuntjens JP, Walters BRB, Mainegra-Hing E. NRC User Codes for EGSnrc, NRC Technical Report No. PIRS-702. Ottawa, Canada: National Research Council of Canada; 2006.
- McGowan HCE, Faddegon BE and Ma CM. STATDOSE for 3D Dose Distributions. NRCC Report No. PIRS-509. Ottawa, Canada: National Research Council of Canada; 2020.
- Martinov MP, Thomson RM. User Guide for 3ddose\_Tools. CLRP Report No. 13-01. Ottawa, Canada: Carleton Laboratory for Radiation Physics; 2016.
- Kawrakow I, Mainegra-Hing E, Tessier F, Walters BRB. The EGSnrc C++ class library, Technical Report PIRS-898 (rev A), National Research Council Canada, Ottawa, Canada; 2009.
- Shirley VS. Nuclear Data Sheets for A=192. Berkeley, CA: Lawrence Berkeley Laboratory; 1991.
- Perez-Calatayud J, Ballester F, Das RK, Dewerd LA, Ibbott GS, Meigooni AS, *et al.* Dose calculation for photon-emitting brachytherapy sources with average energy higher than 50 keV: Report of the AAPM and ESTRO. Med Phys 2012;39:2904-29.
- Beaulieu L, Carlsson Tedgren A, Carrier JF, Davis SD, Mourtada F, Rivard MJ, *et al.* Report of the Task Group 186 on model-based dose calculation methods in brachytherapy beyond the TG-43 formalism: Current status and recommendations for clinical implementation. Med Phys 2012;39:6208-36.
- Berger MJ, Hubbell JH. XCOM, Photon Cross Sections on a Personal Computer. Report No. NBSIR87-3597. Gaithersburg, MD: NIST; 1987.
- Walters BR, Kawrakow I, Rogers DW. History by history statistical estimators in the BEAM code system. Med Phys 2002;29:2745-52.
- Sechopoulos I, Rogers DW, Bazalova-Carter M, Bolch WE, Heath EC, McNitt-Gray MF, *et al.* RECORDS: Improved reporting of monte Carlo RaDiation transport studies: Report of the AAPM Research Committee Task Group 268. Med Phys 2018;45:e1-5.