

RESEARCH

Open Access



Magnetic resonance spectroscopy associations with clinicopathologic features of estrogen-dependent endometrial cancer

Jie Zhang¹, Qingwei Liu¹, Jie Li², Zhiling Liu¹, Ximing Wang¹, Na Li³, Zhaoqin Huang^{1*} and Han Xu^{1*}

Abstract

Background: We studied the magnetic resonance spectroscopy (MRS) associations with clinicopathologic features of estrogen-dependent endometrial cancer (type I EC).

Methods: Totally 45 patients with type I EC who underwent preoperative multi-voxel MRS at 3.0 T were enrolled. The mean ratio of the Cho peak integral to the unsuppressed water peak integral (Cho/water) of the tumor was calculated. The Cho/water and apparent diffusion coefficient (ADC) of type I EC with and without local invasion, as well as with different levels of Ki-67 staining index (SI) ($\leq 40\%$ and $> 40\%$), were compared. Correlation test was used to examine the relationship of Cho/water, as well as mean ADC, with Ki-67 SI, tumor stage, and tumor grade.

Results: The mean Cho/water of EC with Ki-67 SI $\leq 40\%$ (2.28 ± 0.93) $\times 10^{-3}$ was lower than that with Ki-67 SI $> 40\%$ (4.08 ± 1.00) $\times 10^{-3}$ ($P < 0.001$). The mean Cho/water of EC with deep and superficial myometrial invasion was (3.41 ± 1.26) $\times 10^{-3}$ and (2.43 ± 1.11) $\times 10^{-3}$, respectively ($P = 0.011$). There was no significant difference in Cho/water between type I EC with and without cervical invasion ($[2.68 \pm 1.00] \times 10^{-3}$ and $[2.77 \pm 1.28] \times 10^{-3}$, $P = 0.866$). The mean Cho/water of type I EC with and without lymph node metastasis was (4.02 ± 1.90) $\times 10^{-3}$ and (2.60 ± 1.06) $\times 10^{-3}$, respectively ($P = 0.014$). The Cho/water was positively correlated with the Ki-67 SI ($r = 0.701$, $P < 0.001$). There were no significant differences in ADC among groups (all $P > 0.05$).

Conclusion: MRS is helpful for preoperative assessment of clinicopathological features of type I EC.

Keywords: Type I endometrial cancer, Ki-67, Local invasiveness, Magnetic resonance spectroscopy

Background

Endometrial cancer (EC) is one of the most common female genital tract cancers, which could be divided into the estrogen-dependent (type I) and non-estrogen-dependent (type II) EC types. Type I EC only contains endometrioid adenocarcinoma, which is the most common pathological type. Type I EC occurs in about 80%

of the EC cases. Type II EC is more rarely seen, which generally contains multiple subtypes of EC, and is closely related to lymphatic metastasis and poor prognosis. Type II EC accounts for the remaining 20% of all the EC cases [1].

Precise assessment of EC aggressiveness before treatment may contribute to personalized treatment and prognosis prediction. Tumor proliferation activity is also an indicator to evaluate the EC aggressiveness, in addition to tumor pathological type, grade, stage and size [2]. Ki-67, a proliferation-related nuclear antigen, is expressed in all cycling cells, except for the resting cells in the G0 phase. Ki-67 staining index (SI) reflects the tissue

*Correspondence: devin813@sina.com; xuhantsh@163.com

¹ Department of Radiology, Shandong Provincial Hospital Affiliated to Shandong First Medical University, No. 324, Jingwu Road, Jinan 250021, Shandong, China

Full list of author information is available at the end of the article



proliferation activity. It has been suggested that the Ki-67 level in the type I EC tissue has been shown to be higher than that in the endometrial polyps [3]. High expression level of Ki-67 has been correlated with relatively higher incidence of distant recurrence [4].

As a non-invasive examination, magnetic resonance spectroscopy (MRS) is a method to obtain biochemical information from tissues. It is reported that MRS can differentiate between malignant and benign lesions of the uterus [5]. In our previous studies, MRS helped to differentiate EC from benign lesions in endometria or in submucosa, and also differentiated the type II from type I EC [6, 7]. Choline-containing compounds (Cho) are marker of active tumors, which is increased in actively proliferating tissues. The ratio of Cho peak integral and water peak integral (Cho/water) represents the concentration of Cho to a certain extent. Preoperative diagnostic curettage pathology is the main method for the diagnosis of EC. However, the specimens are limited and cannot reflect the overall pathological characteristics of the tumor. Although MRS only plays an auxiliary role, multi-voxel MRS can cover the whole tumor and reflect the metabolic characteristics of the whole tumor.

In this study, the relationship between Cho/Water and clinicopathologic features, including Ki-67 SI, of type I EC was investigated. Our findings may help to preoperatively understand the clinicopathologic features of EC to some extent.

Methods

Study subjects

This is a retrospective analysis. Patients with type I EC, who received hysterectomy from March 2012 to May 2014, were included in this study. The time interval between MR imaging and surgery was 1–10 days (Median, 4 days). These patients underwent total hysterectomy with bilateral salpingo-oophorectomy and pelvic lymph node dissection. The International Federation of Gynecology and Obstetrics (FIGO) stage, local invasion (myometrial invasion, cervical invasion and lymph node

metastasis), grade, and size (maximum diameter) were determined by an experienced pathologist. The tumor stage was determined according to the FIGO revised staging criteria in 2014 [8].

Inclusion criteria were as follows: 1) patients with type I EC confirmed by surgical pathology (estrogen receptor, positive); 2) patients who underwent the MRS; and 3) patients with complete information, including tumor FIGO stage, grade, size and Ki-67 SI. Exclusion criteria: Subjects who had no satisfactory MRS voxel in lesions were excluded. Informed consent was waived by the ethics review board of Shandong Provincial Hospital Affiliated to Shandong First Medical University because this is a retrospective analysis. All methods were performed in accordance with the Declaration of Helsinki and the study was approved by the ethics review board of Shandong Provincial Hospital Affiliated to Shandong First Medical University (Approval No.: SWYX2020-051).

MR imaging

MR examination was performed with a 3.0-T system (Magnetom Verio, Siemens, Germany), equipped with an eight-channel pelvic phased-array surface coil and integrated spine coils. Before MR imaging, patients were fasted for 4 h. Raceanisodamine hydrochloride injection (Minsheng Pharma., Hangzhou, China) was administered before image acquisition to reduce bowel motion. The bladder was partially filled.

MR imaging included the 3D multi-voxel 1H MRS besides the routine sequences, i.e., the T2-weighted (T2W) imaging, diffusion-weighted (DW) imaging (DWI), and dynamic contrast enhanced (DCE) imaging. Conventional MR imaging parameters were shown in Table 1. MRS (with the parameters of TR, 750 ms; TE, 145 ms; flip angle, 90°; vector size, 512; and bandwidth, 1250 Hz) was performed with 3D chemical shift imaging techniques based on point-resolved spectroscopic sequence. A weighted elliptical K-Space acquisition mode was used to save the scan time, and a Hamming filter with a width of 100% (relative to the dimension

Table 1 Parameters of conventional magnetic resonance imaging sequences

Sequences	TR (ms)	TE (ms)	ST (mm)	Average	FOV (cm ²)	Matrix
Axial T2W	3110	101	3–4.5	2	20 × 20	320 × 256
Coronal T2W	3350	97	3–4	2	20 × 20	320 × 256
Sagittal T2W	2950	101	3–4	2	20 × 20	320 × 310
DWI ^a	6200	63	3–4.5	6	20 × 20	160 × 120
T1W-DCE (VIBE)	5.21	1.8	3–4	1	26 × 26	224 × 161

TR Repetition time, TE Echo time, ST Slice thickness, FOV Field of view, DCE Dynamic contrast enhancement imaging, VIBE Volume interpolated body examination, DWI Diffusion-weighted imaging

^a b value = 0, 100, 400, and 800 s/mm²

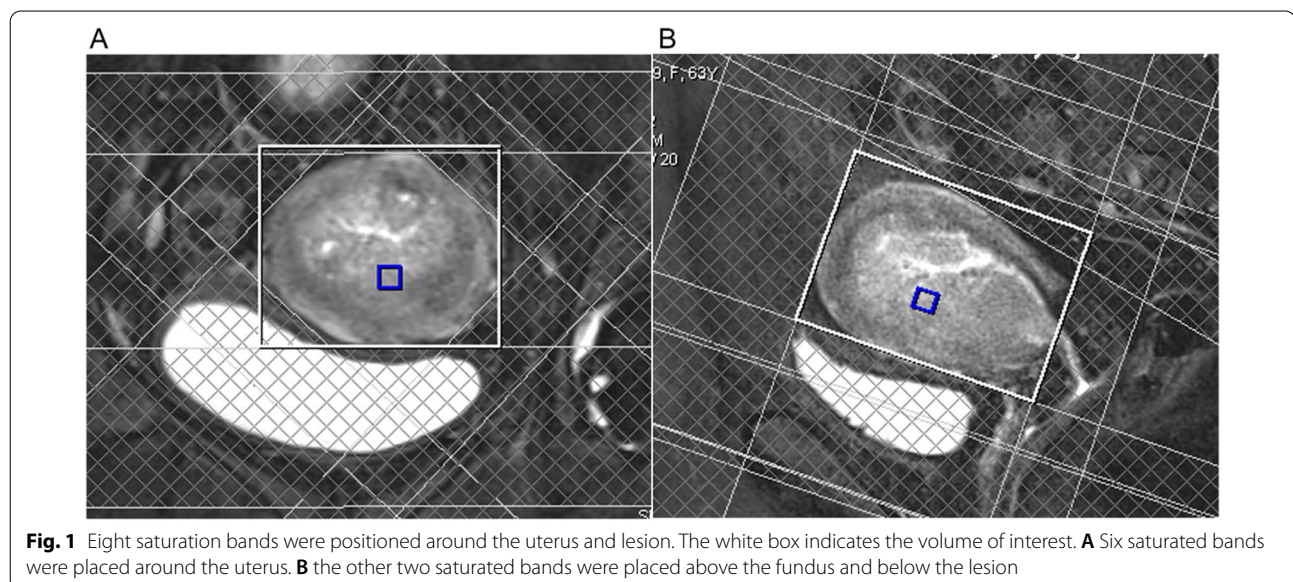
of the K-Space) was applied to the K-Space data to suppress the contamination from the adjacent voxel due to the point-spread function. For Choline acquisition, fat and water were simultaneously suppressed by using the MEGA pulses [9], while for water signal acquisition, MEGA pulses with only fat suppression were applied. Unsuppressed and suppressed water MRS shared identical imaging parameters except the average number of acquisitions, which were 6 for water suppression spectra and 2 for unsuppressed water spectra. Eight saturation bands were positioned around the uterus and lesion, to suppress the signal contamination from the extrauterine lipids or the bladder (Fig. 1). The field of view (FOV) was 84 mm × 84 mm. The matrix was 12 × 12. The voxel size was 7 mm × 7 mm × 7 mm. MRS data were overlaid on the corresponding axial, sagittal and coronal T2W images. The acquisition of MRS data took about 16 min. Anatomy images, including axial, sagittal and coronal T2W images and DCE images, were used as reference images to select the voxels of interest in the solid part of lesions, avoiding cystic or necrotic areas. Therefore, although the FOV covered the lesion, the effective voxels were selected in the solid part of the tumor.

MRS data analysis

MRS processing was performed with the jMRUI v.5.2 software (<http://sermn02.uab.es/mrui>). The Cho and water peaks were quantified. On the spectrum of suppressed water, the Cho peak was detected at 3.2 ppm. On the spectrum of unsuppressed water, the water peak was detected at 4.7 ppm. The spectra needed to be pre-processed before Cho peak quantification, as follows:

filtering with “Lorentzian” 5 Hz, further water suppression and Fourier transformation. If there was phase offset for the Cho peak, the phase correction was performed. The same preprocessing was performed for the water peak, except for further water suppression. The time domain fitting algorithm AMARES (Advanced Method for Accurate, Robust and Efficient Spectral fitting) was used to quantify the water peak and Cho peak. The amplitude standard deviation (i.e., the Cramér-Rao standard deviation [CRSD]) of the metabolites could be obtained from the AMARES fitting algorithm. The CRSD could be used to measure the accuracy of metabolite peak fitting, which reflected the signal-to-noise ratio (SNR). The relative CRSD of metabolite was calculated by the CRSD/amplitude, which was inversely related to SNR. The availability of the spectrum was determined by a radiologist and a spectroscopist in consensus (both blinded to the patients’ clinical information), according to the correct positions of the Cho and water peaks, relatively stable baseline and absence of large lipid signals. Any spectrum with a relative metabolite CRSD greater than 20% or full width at half maximum (FWHM) greater than 15 Hz was excluded. There were a total of 2364 voxels of type I EC (median, 32; range, 1–273 per patient) included. The radiologist also interpreted the conventional MR images.

The Cho/water was the statistical unit herein (Eq. 1). In Eq. 1, Cho_i was the i^{th} voxel from suppressed water; $water_i$ was the i^{th} voxel from unsuppressed water; n was the total number of included voxels for a patient. The Cho/water reflected the Cho concentration in tissues.



$$\text{Cho/water} = \left(\sum_{i=1}^n \text{Cho}_i/\text{water}_i \right) / n \quad (1)$$

DWI data analysis

ADC maps were automatically generated from DW images ($b=0, 100, 400$ and 800 s/mm^2). The regions of interest (ROI) were placed on ADC map in the tumor by two radiologists independently, according to lesion

morphology, avoiding cystic and necrotic areas, and with DW images, T2W images and DCE images as reference images (Fig. 2).

The mean ADC value of the tumor was calculated by averaging the ADC values of all voxels in all ROIs (Eq. 2). Because the areas of ROIs often differed greatly, the area S_i was the weight of the ADC_i . The Eq. 2 could provide the mean ADC accurately. The mean ADC measured by two radiologists was defined as the final mean ADC (ADC_m).

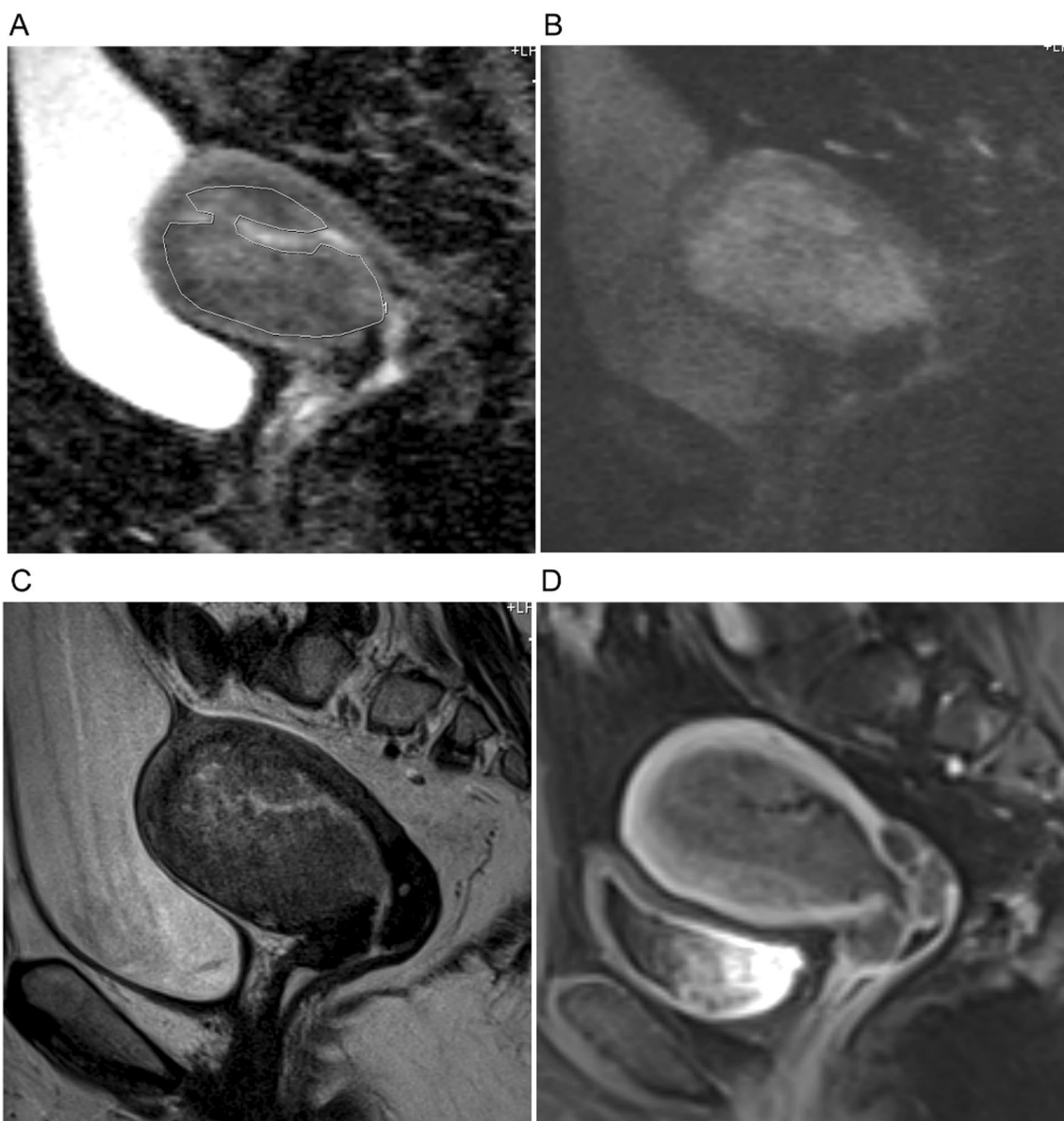


Fig. 2 The regions of interest (ROI) were placed on ADC map (A) in the tumor, avoiding cystic and necrotic areas with DW image ($b=800 \text{ s/mm}^2$) (B), T2W images (C) and DCE image (D) as reference images

$$\text{mean ADC} = \left(\sum_{i=1}^n \text{ADC}_i * S_i \right) / \sum_{i=1}^n S_i \quad (2)$$

Immunohistochemical analysis of Ki-67

For the immunohistochemical staining, the Ki-67 mouse monoclonal antibody (MIB-1; ZSGBBIO, Beijing, China) was used. Briefly, the paraffin Sects. (4 μm) were kept in an oven (60 $^{\circ}\text{C}$) overnight. The sections were dewaxed in xylene (three cylinders for 10 min each), incubated with graded alcohol and then washed in distilled water for 3 times (2 min each time). The sections were repaired with citric acid antigen repairing solution, followed by immersing in 0.3% H_2O_2 in methanol at room temperature for 15 min. Then, the slides were washed by phosphate-buffered saline for three times (3 min each). For antigen retrieval, slides were heated in 0.01 M citrate buffer (pH 6) in an autoclave. Then, the slides were cooled to room temperature and rinsed with PBS. After nonspecific protein blockage, the slides were incubated with the primary antibody at 37 $^{\circ}\text{C}$ for 90 min. Then, the slides were incubated with corresponding secondary antibody for 20 min. Then the slides were counterstained with hematoxylin.

Ki-67 was considered positive when the cell nuclei were stained brown. The Ki-67 SI was defined as the percentage of positive nuclei out of totally 1000 cells counted according to the eyepiece grid, which was performed by a pathologist in a blinded manner.

Statistical analysis

Statistical analysis was performed with SPSS for Windows, version 17.0 (SPSS, Chicago, Illinois). $P < 0.05$ was considered as statistically significant. Kolmogorov–smirnov test was used to detect whether the data were normally distributed. The Cho/water of type I EC was dichotomized for the analysis as Ki-67 SI $\leq 40\%$ versus $> 40\%$ [2]. Five-year cancer-specific survival rates were 58% for those tumors with high Ki-67 expression ($> 40\%$), compared with 88% for those with tumors with low Ki-67 expression [2]. Reliability analysis was used to test the consistency of the mean ADC between two radiologists. Comparisons of Cho/water, as well as ADC_m , among different FIGO stages or different grades of EC were performed using one-way analysis of variance (ANOVA). The Cho/water and the ADC_m of type I EC with different expression levels of Ki-67 SI, with deep and superficial myometrial invasion, with and without cervical invasion, and with and without lymph node metastasis were compared with the independent-sample t-test. The receiver operating characteristic (ROC) curve analyses was used to determine an optimal Cho/water threshold to distinguish between these two groups. The

Pearson correlation test was used to analyze the correlations between the Cho/water and Ki-67 SI, between the Cho/water and tumor size, and, between the Ki-67 SI and tumor size as well as between the ADC_m and Ki-67 SI, and between the ADC_m and tumor size. The Spearman correlation test was performed to analyze the correlations between Cho/water and number of included voxels, the Ki-67 and FIGO stage, between the Ki-67 and tumor grade, between the Cho/water and FIGO stage, and, between the Cho/water and tumor grade, as well as between ADC_m and FIGO stage, and between the ADC_m and tumor grade.

Results

Basic clinical data

Initially, 50 cases were eligible for inclusion. Among them, 5 cases had no satisfactory MRS voxel, mainly due to the unstable baseline and FWHM greater than 15 Hz. Finally, 45 cases were enrolled. Their mean age was 56.4 ± 6.8 years old. The basic clinical data of patients were shown in Table 2. The Cho peak was observed for all 45 patients with type I EC. Our results showed that the Cho/water ($P = 0.843$), Ki-67 SI ($P = 0.638$) and tumor size ($P = 0.889$) were normally distributed.

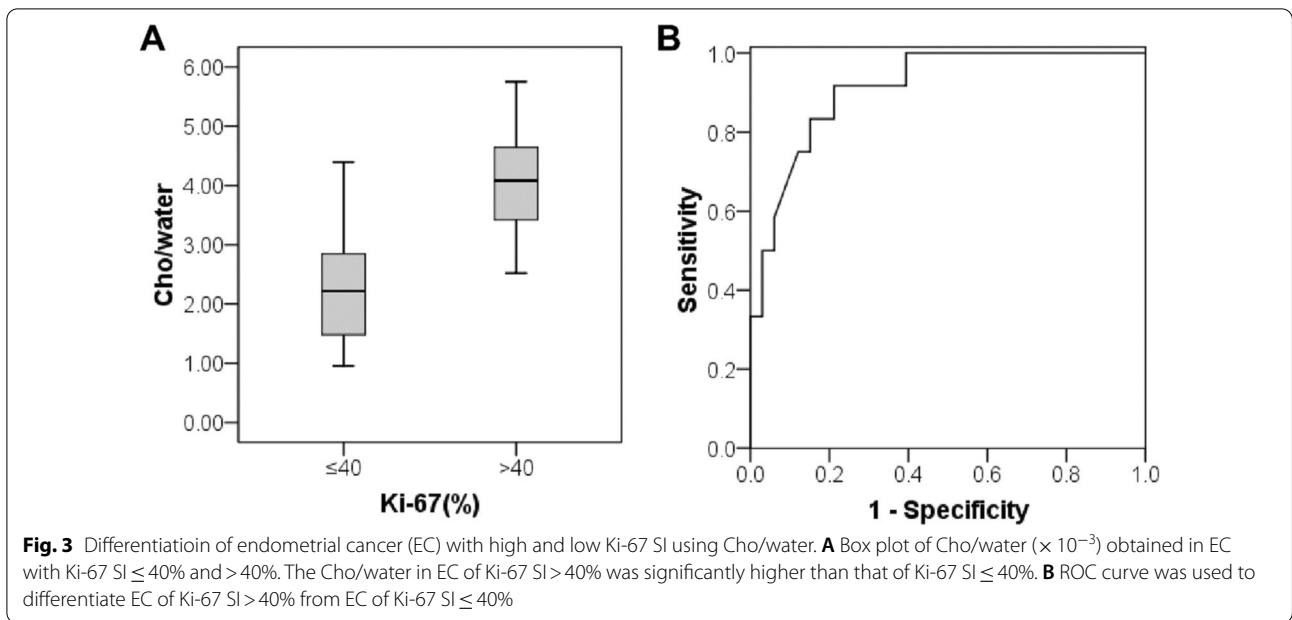
Cho/water of EC with high and low Ki-67 SI

There were 33 patients with the Ki-67 SI $\leq 40\%$ and 12 patients with the Ki-67 SI $> 40\%$. The mean Cho/water of the former (2.28 ± 0.93) $\times 10^{-3}$ was significantly lower than the latter (4.08 ± 1.00) $\times 10^{-3}$ ($P < 0.001$) (Fig. 3A). The area under the curve (AUC) was 0.912. The Cho/water threshold was 2.89×10^{-3} , with the sensitivity and specificity of 0.917 and 0.788, respectively (Fig. 3B). Immunohistochemical images of EC with low and high

Table 2 The basic clinical data of patients

Items	Number
Total	45
Ki-67 SI	
$\leq 40\%$	33
$> 40\%$	12
Myometrial invasion	
Superficial	30
Deep	15
Cervical invasion	
Yes	6
No	39
Lymph node metastasis	
Yes	5
No	40

SI Staining index

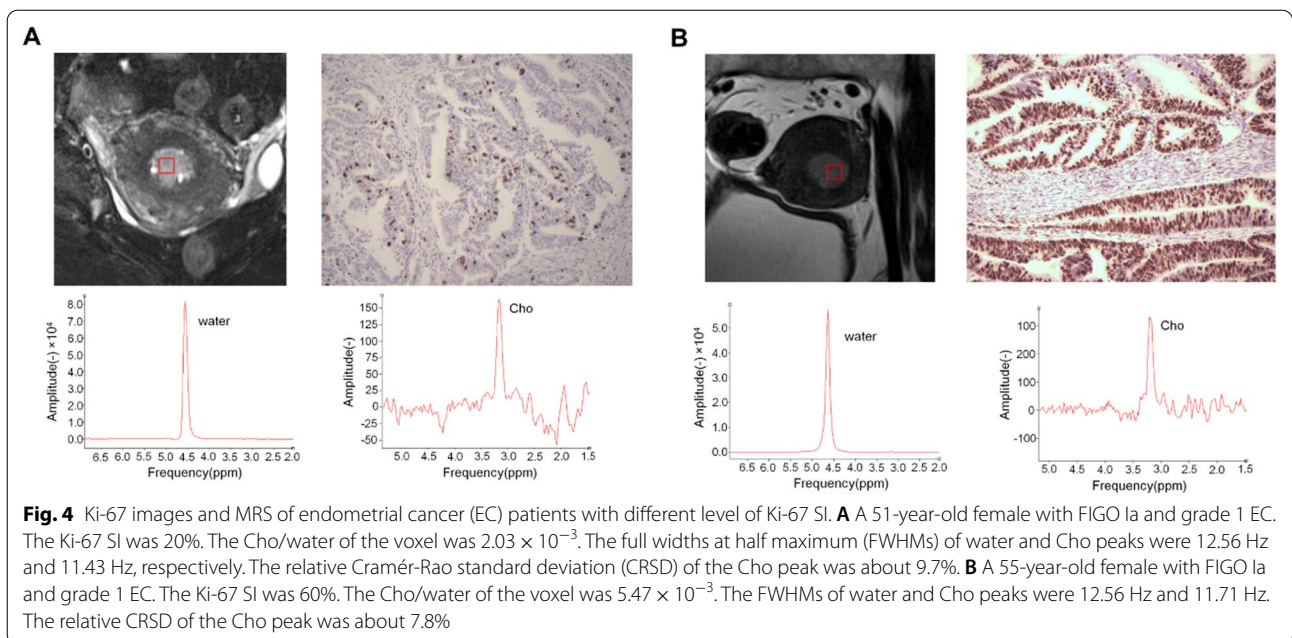


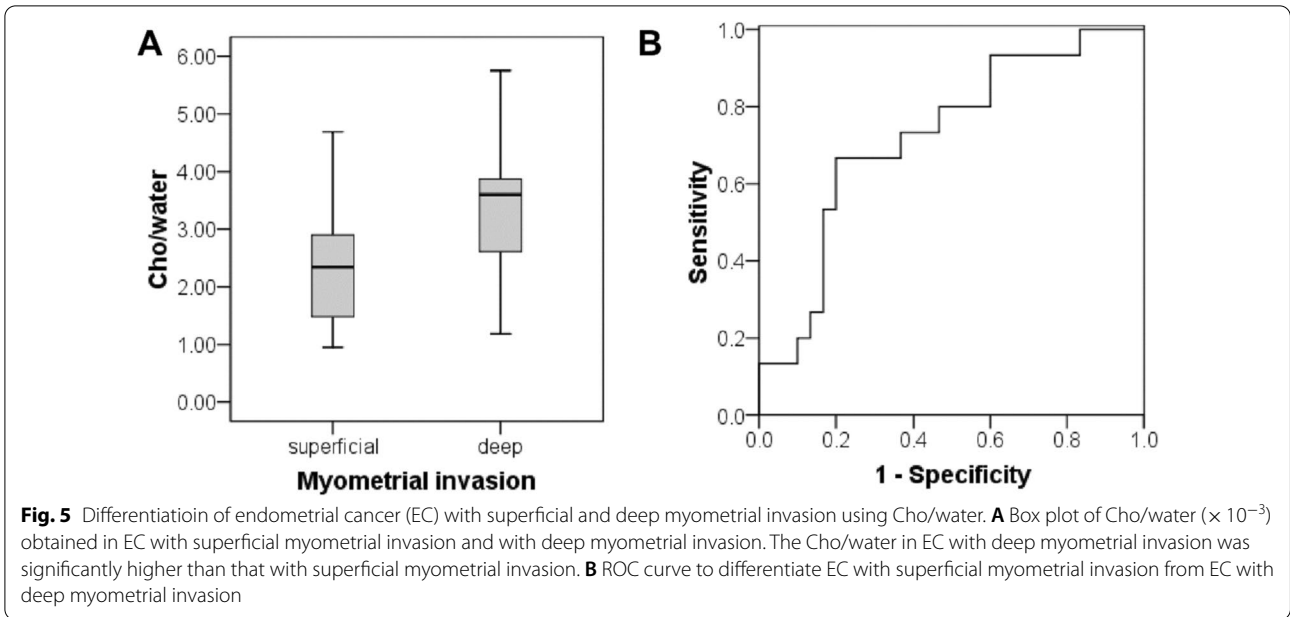
Ki-67 SI and the corresponding Cho and water peaks were shown in Fig. 4A, B.

Cho/water of EC with superficial and deep myometrial invasion

There were 30 patients with superficial myometrial invasion and 15 patients with deep myometrial invasion. The mean Cho/water of patients with superficial myometrial

invasion $(2.43 \pm 1.11) \times 10^{-3}$ was significantly lower than the patients with deep myometrial invasion $(3.41 \pm 1.26) \times 10^{-3}$ ($P=0.011$) (Fig. 5A). The AUC value was 0.722. The Cho/water threshold was 3.07×10^{-3} , with the sensitivity and specificity of 0.667 and 0.800, respectively (Fig. 5B).



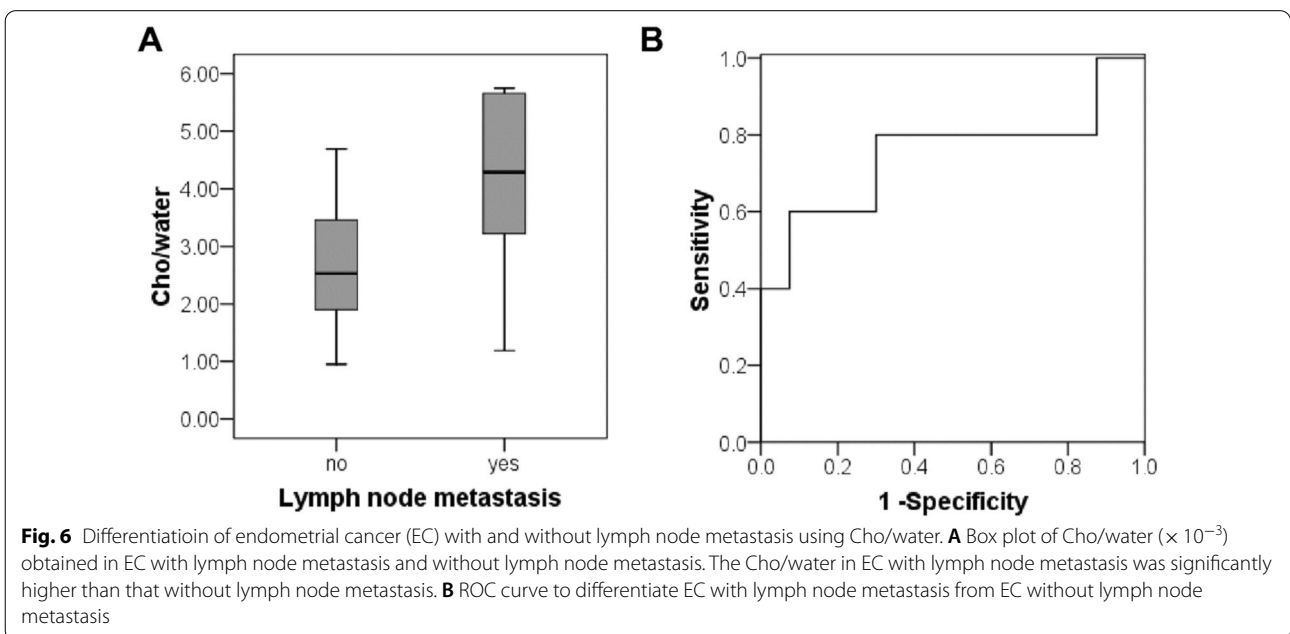


Cho/water of EC with and without cervical invasion

There were 6 patients with cervical invasion (mean Cho/water, $[2.68 \pm 1.00] \times 10^{-3}$) and 39 patients without cervical invasion (mean Cho/water, $[2.77 \pm 1.28] \times 10^{-3}$). There was no significant difference in the Cho/water between patients with and without cervical invasion ($P=0.866$).

Cho/water of EC with and without lymph node metastasis

There were 5 patients with lymph node metastasis and 40 patients without lymph node metastasis. The mean Cho/water for patients with lymph node metastasis $(4.02 \pm 1.90) \times 10^{-3}$ was significantly higher than the patients without lymph node metastasis $(2.60 \pm 1.06) \times 10^{-3}$ ($P=0.014$) (Fig. 6A). The AUC value was 0.750. The Cho/water threshold was



3.07×10^{-3} , with the sensitivity and specificity of 0.800 and 0.700, respectively (Fig. 6B).

Correlations between Cho/water and Ki-67, between Cho/water and size, and between Ki-67 and size of EC

In addition, our results showed that there was significant correlation between the Cho/water and Ki-67 SI for EC ($r=0.701$, $P<0.001$) (Fig. 7A), between Cho/water and tumor size ($r=0.538$, $P<0.001$) (Fig. 7B), between Cho/water and number of voxel ($r=0.500$, $P<0.001$) (Fig. 7C), and between Ki-67 SI and tumor size ($r=0.609$, $P<0.001$) (Fig. 7D).

Correlations between the Ki-67 and FIGO stage, between the Ki-67 and tumor grade, between the Cho/water and FIGO stage, and between the Cho/water and tumor grade

The Ki-67 SI and Cho/water for EC cases of different FIGO stages and grades were shown in Table 3. Our results showed that there were no significant difference in the Ki-67 SI among different FIGO stages ($P=0.308$). There were significant differences in the Cho/water among different FIGO stages ($P=0.025$), but the difference only existed between FIGO Ia and III EC ($P=0.015$). There were significant differences in the Ki-67 SI among

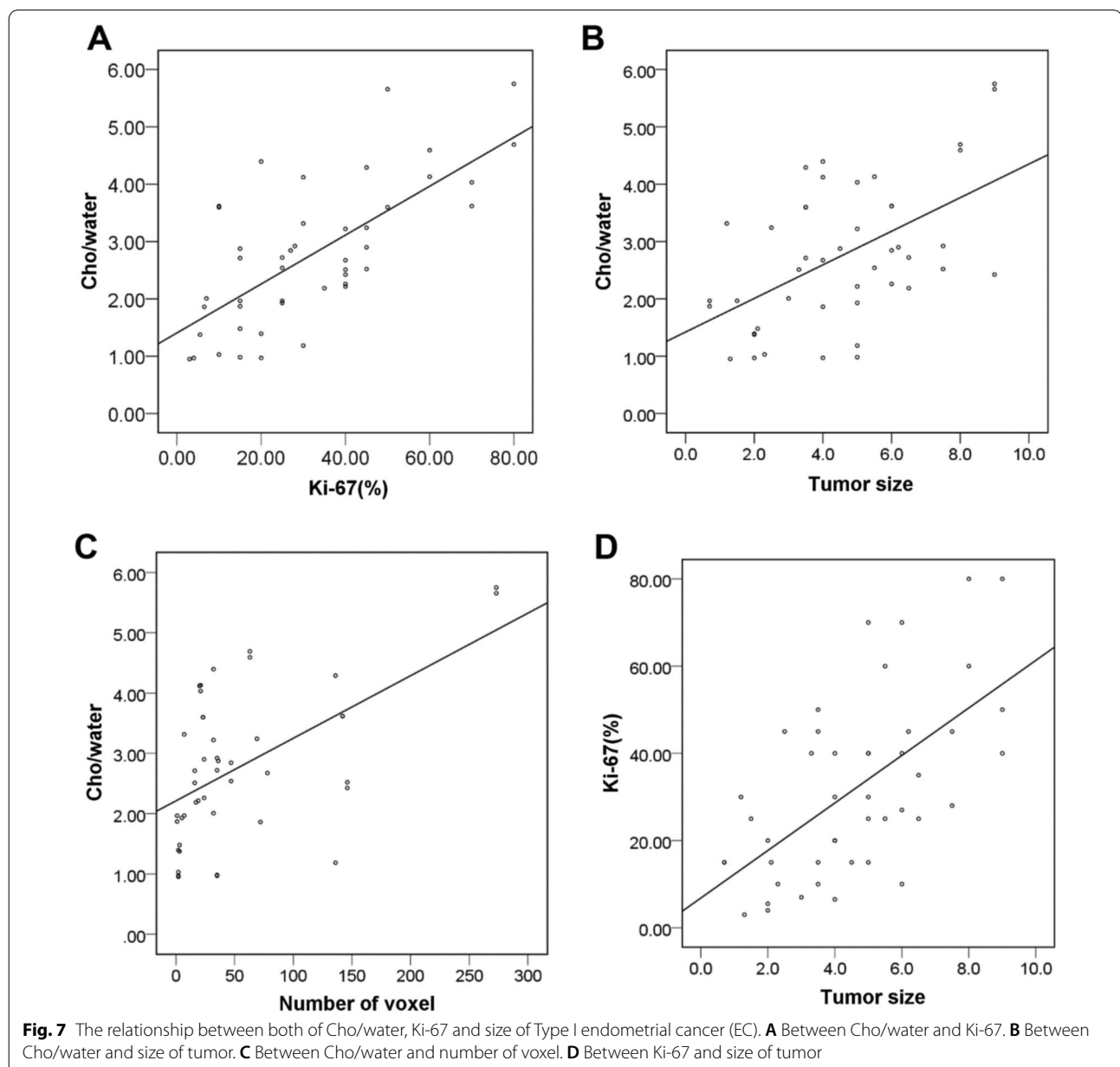


Table 3 The Ki-67 SI and Cho/water of different FIGO stages and grades of type I EC

Variable	No. of cases	Ki-67 expression (%) (Mean ± SD)		Cho/water × 10 ⁻³ (Mean ± SD)	
<i>FIGO stage</i>					
Ia	26	28.5 ± 20.8	^a P=0.308	2.40 ± 1.19	^b P=0.025
Ib	9	30.2 ± 22.1		2.98 ± 0.70	
II	4	34.5 ± 9.54		2.65 ± 0.22	
III	6	45.8 ± 18.6		4.04 ± 1.70	
Spearman correlation		^e ρ=0.295, P=0.049		^f ρ=0.376, P=0.011	
<i>Histologic grade</i>					
Grade 1	16	18.8 ± 13.6	^c P=0.001	1.95 ± 0.99	^d P=0.003
Grade 2	21	35.5 ± 19.1		3.23 ± 0.97	
Grade 3	8	47.5 ± 21.2		3.15 ± 1.58	
Spearman correlation		^g ρ=0.541, P<0.001		^h ρ=0.443, P=0.002	

^a differences in the Ki-67 SI among different FIGO stages; ^b differences in the Cho/water among different FIGO stages; ^c differences in the Ki-67 SI among different grades; ^d differences in the Cho/water among different grades; ^e the correlation coefficient between Ki-67 and FIGO stage; ^f the correlation coefficient between Cho/water and FIGO stage; ^g the correlation coefficient between Ki-67 and grade; ^h the correlation coefficient between Cho/water and grade

different EC grades (P=0.001). The statistical differences in Ki-67 SI existed between any two grades of EC, except between G2 and G3 EC (G1 vs. G2, P=0.018; G1 vs. G3, P=0.002; and G2 vs. G3, P=0.248, respectively). There were significant differences in the Cho/water among different EC grades (P=0.003). The statistical differences in Cho/water existed between any two grades of EC, except between G2 and G3 EC (G1 vs. G2, P=0.003; G1 vs. G3, P=0.040; G2 vs. G3, P=0.986, respectively). The Ki-67 SI and Cho/water were positively correlated with the FIGO stage and grade (Table 3).

The relationship between ADC_m and invasiveness of type I EC

The intraclass correlation coefficient of ADC was 0.956 (P<0.001) (95% confidence interval 0.922, 0.976). There were no significant differences in the tumor ADC_m between different levels of Ki-67 SI, between deep and superficial myometrial invasion, between with and without cervical invasion, and between with and without lymph node metastasis (Table 4). There was no significant correlation between ADC_m and FIGO stage (ρ=-0.001, P=0.996), as well as between ADC_m and grade (ρ=-0.237, P=0.118). There was no significant correlation between ADC_m and Ki-67 SI (r=-0.218, P=0.151), as well as between ADC_m and size (r=-0.178, P=0.242).

Discussion

In this study, only type I EC patients were included and investigated. The type II EC cases have multiple histopathological subtypes, such as serous carcinoma and clear cell carcinoma. Type II EC is clinically treated as a high grade of malignancy and is no longer graded in

Table 4 Comparisons of ADC_m among different groups

Invasiveness	ADC _m (× 10 ⁻³ mm ² /s)	P value
<i>Ki-67 SI</i>		
≤ 40%	0.873 ± 0.146	0.171
> 40%	0.810 ± 0.095	
<i>Myometrial invasion</i>		
Superficial	0.866 ± 0.153	0.531
Deep	0.838 ± 0.097	
<i>Cervical invasion</i>		
No	0.855 ± 0.146	0.843
Yes	0.867 ± 0.030	
<i>Lymph node metastasis</i>		
No	0.867 ± 0.139	0.155
Yes	0.775 ± 0.079	
<i>FIGO stage</i>		
Ia	0.864 ± 0.164	0.841
Ib	0.857 ± 0.088	
II	0.876 ± 0.033	
III	0.810 ± 0.111	
<i>Grade</i>		
G1	0.864 ± 0.126	0.065
G2	0.889 ± 0.149	
G3	0.758 ± 0.072	

pathology. In previous studies, we differentiated the type II EC from type I EC with MRS [6, 7]. Therefore, the type II EC cases were not studied herein.

No Ki-67 expression was detected during the G0 and early G1 phase in the cell cycle. Ki-67 expression would be detected in the late G1 phase, which gradually increases in the S and G2 phases, and then rapidly degrades after peaking in the M phase [10]. Ki-67 is a key

factor in ribosome synthesis, is crucial for cell proliferation and closely related to cell anabolism [11]. Cho is a marker for cell proliferation, which is often elevated in cancer and associated with tumor progression [12]. High expression of Ki-67 has been associated with reduced EC-specific survival [13]. To the best of our knowledge, there has been no reports studying the EC proliferation using MRS.

In this study, the Cho peak was observed in all type I EC cases. The Cho/water of EC with high Ki-67 SI was higher than with low Ki-67 SI. The Cho/water and Ki-67 SI were positively correlated. The Ki-67 expression reflects the proliferative activity of tumor, and Cho is a marker for cell proliferation [12]. Cell proliferation per unit volume may result in a high cell density and relative reduction of extracellular free water [14], which may result in a decrease in the water peak. This may explain the positive correlation between Cho/water and Ki-67 SI of EC. There are few studies on EC proliferation using MRS. However, there are relevant studies on proliferation of glioma and prostate cancer. These results showed that the level of Cho was positively correlated with the proliferative activity [15, 16]. The Cho/water for EC patients with deep myometrial invasion, as well as with lymph node metastasis, was significantly higher than that with superficial myometrial invasion, as well as without lymph node metastasis. This is different from previous study [17], which has shown that the differences are not statistically significant. There was no significant difference in the Cho/water between patients with and without cervical invasion, which was in line with the previous study [17]. The heterogeneity of MRS Cho/water within solid part of EC was studied in our previous study [6], which showed that the Cho/water heterogeneity of Ib and III EC was significantly greater than that of Ia EC; and the Cho/water heterogeneity of EC was increased with the increased tumor stage and size.

In this study, we found that the Cho/water was positively correlated with the tumor grade. There were statistical differences in Cho/water between any two grades of EC, except between G2 and G3 EC. This is different from the previous study, which reported that there were no significant differences among different grades of EC and no correlation between Cho/water and tumor grades [6]. The reason may be that 1) only type I EC was included in this study; 2) the number of patients with EC included in this study was more than that of the previous study. But the results were similar to those in a previous study [17]. The relationship between Cho/water or signal to noise ratio of Cho and FIGO stage was in line with the previous studies [6, 7]. In a study with large series, tumor size was demonstrated as an independent prognostic factor of local recurrence in women with low-risk EC and could

be a valuable additional criterion to personalize the treatment approach to these patients [18]. In our study, the number of included voxels per patient reflected the size of tumor. Cho/water was found to be positively correlated with the number of included voxels. Ki-67 and Cho/water were positively correlated with tumor size, which is partly similar to previous studies [6, 7, 17]. Tumor tCho/Creatine ratio is reported to be positively correlated to MRI-measured tumor volume [17]. This may be also explained that both of Ki-67 and Cho/water can reflect the proliferative activity of tumor cells.

In patients with EC, endometrium without tumor proliferation would be difficult to display. The voxel size of MRS was 7 mm × 7 mm × 7 mm. Therefore, the adjacent endometrium was too small to obtain the accurate metabolites from MRS. Therefore, Cho/water of EC was not compared with that of the adjacent endometrium. In some patients, the lesions invaded the whole myometrium, and there was almost no normal myometrium, or the normal myometrium was very thin. Thus, the MRS of the normal myometrium was not studied.

In previous studies, other MR parameters or MR image texture parameters were generally used to study the correlation with Ki-67 and other invasive indicators [14, 19–24]. The relationship between Ki-67 and ADC is controversial in patients with EC. A study has shown that Ki-67 and ADC are negatively correlated [14], while another study has indicated that there is no correlation between them [22]. In this study, we also found that there was no significant correlation between ADC_m and Ki-67 SI. Both the DWI and DKI parameters provide valuable imaging biomarkers for EC diagnosis and the assessment of risk stratification in EC [19–22]. However, in this study, we found no significant difference in ADC_m among different grades of EC, as well as different FIGO stages of EC. The APT (amide proton transfer) imaging signal intensity is reported to be positively correlated with the histologic grades of endometrioid EC, but the mean and minimum ADCs shows no significant differences among the three histologic grades [23]. The combination of tumor volume ratio and ADC can be used for predicting the tumor grade, lymphovascular invasion, and depth of myometrial invasion, but there is no significant difference in the ADCs between grades 1 and 2 tumors [24]. MRI-derived tumor texture parameters could independently predict the deep myometrial invasion, high-risk histological subtype, lymphovascular space invasion, high-grade tumor and reduced survival in EC [25, 26]. Ktrans and Ve values are significantly higher in low grade but no significant correlations are found between quantitative perfusion parameters and histological type, lympho-vascular invasion, or FIGO stage [27]. Low tumor blood flow and low rate constant for contrast agent intravasation are

associated with high-risk histological subtype; but the derived DCE parameters of tumor are not significantly different in patients with more advanced stage, i.e., the deep myometrial invasion, cervical stroma invasion or lymph node metastases [28]. Haldorsen et al. [29] have reported that tumor blood flow and capillary transit time had significant impacts on recurrence-/progression-free survival; but there were no significant differences in the tumour perfusion parameters among tumour grades, stage, tumour type, tumours, with or without lymph node metastases or among tumours with or without deep myometrial invasion. Therefore, there are many studies on DWI to assess the aggressiveness of EC, but the relationship between ADC and Ki-67, as well as the relationship between ADC and tumor grade, are controversial. The role of DCE parameters in EC invasiveness varies in different studies. The relationship between the Cho/water obtained from MRS and Ki-67 SI of type I EC has been rarely studied. Herein, we found that Cho/water and Ki-67 had good correlation.

There were some limitations for this study. First, this was a retrospective study. Second, the number of patients was small, especially the patients with cervical invasion and with lymph node metastasis. Third, this was a single center study. Further in-depth studies are still needed to address these issues in the future.

Conclusions

In conclusion, the Cho/water of type I EC was positively correlated with proliferative activity. High levels of Cho/water were associated with deep myometrial invasion, lymph node metastasis, high grade of EC, high FIGO stage of EC, and big size of tumor, but not cervical invasion. Therefore, MRS is helpful for pre-operative assessment of clinicopathological features of type I EC.

Abbreviations

MRS: Magnetic resonance spectroscopy; EC: Endometrial cancer; SI: Staining index; Cho: Choline-containing compounds; T2W: T2-weighted; DWI: Diffusion-weighted imaging; DCE: Dynamic contrast enhanced; SNR: Signal-to-noise ratio.

Acknowledgements

Not applicable.

Author contributions

Study design: JZ, ZH, HX; Study conception: JZ, HX, ZH; Data analysis: JZ, HX, ZL, QL; Case collection: JZ, JL, NL, ZL, XW; Statistical analysis: JZ, XW; Image capture: HX; JL; Manuscript preparation: JZ, HX, QL; Manuscript revision: QL, XW. All authors read and approved the final manuscript.

Funding

The study was funded by the Primary Research & Development Plan of Shandong Province (No. 2016GSF201095) and the Academic Promotion Program of Shandong First Medical University (No. 2019QL023).

Availability of data and materials

The datasets generated and/or analysed during the current study are not publicly available due to local ownership of the data but are available from the corresponding author on reasonable request.

Declarations

Ethics approval and consent to participate

Informed consent was waived by the ethics review board of Shandong Provincial Hospital Affiliated to Shandong First Medical University because this is a retrospective analysis. All methods were performed in accordance with the Declaration of Helsinki and the study was approved by the ethics review board of Shandong Provincial Hospital Affiliated to Shandong First Medical University (Approval No.: SWYX2020-051).

Consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

Author details

¹Department of Radiology, Shandong Provincial Hospital Affiliated to Shandong First Medical University, No. 324, Jingwu Road, Jinan 250021, Shandong, China. ²Special Inspection Department, Taian City Central Hospital Branch, No. 336, Wanguan Road, Taian 271000, Shandong, China. ³Department of Gynecology, Shandong Provincial Hospital Affiliated to Shandong First Medical University, No. 324, Jingwu Road, Jinan 250021, Shandong, China.

Received: 21 March 2022 Accepted: 8 July 2022

Published online: 18 July 2022

References

- Lax SF, Kurman RJ. A dualistic model for endometrial carcinogenesis based on immunohistochemical and molecular genetic analyses. *Verh Dtsch Ges Pathol.* 1997;81:228–32.
- Kitsos S, Sivalingam VN, Bolton J, McVey R, Nickkho-Amiry M, Powell ME, Leary A, Nijman HW, Nout RA, Bosse T, et al. Ki-67 in endometrial cancer: scoring optimization and prognostic relevance for window studies. *Mod Pathol Off J U S Can Acad Pathol Inc.* 2017;30(3):459–68.
- Peres GF, Spadoto-Dias D, Bueloni-Dias FN, Leite NJ, Elias LV, Domingues MAC, Padovani CR, Dias R. Immunohistochemical expression of hormone receptors, Ki-67, endoglin (CD105), claudins 3 and 4, MMP-2 and -9 in endometrial polyps and endometrial cancer type I. *Onco Targets Ther.* 2018;11:3949–58.
- Di Donato V, Iacobelli V, Schiavi MC, Colagiovanni V, Pecorella I, Palaia I, Perniola G, Marchetti C, Musella A, Tomao F, et al. Impact of hormone receptor status and Ki-67 expression on disease-free survival in patients affected by high-risk endometrial cancer. *Int J Gynecol Cancer Off J Int Gynecol Cancer Soc.* 2018;28(3):505–13.
- Takeuchi M, Matsuzaki K, Harada M. Differentiation of benign and malignant uterine corpus tumors by using proton MR spectroscopy at 3T: preliminary study. *Eur Radiol.* 2011;21(4):850–6.
- Zhang J, Cai S, Li C, Sun X, Han X, Yang C, Fu C, Liu Q, Xin Y, Zong Y. Can magnetic resonance spectroscopy differentiate endometrial cancer? *Eur Radiol.* 2014;24(10):2552–60.
- Han X, Kang J, Zhang J, Xiu J, Huang Z, Yang C, Sun X, Fu C, Liu Q. Can the signal-to-noise ratio of choline in magnetic resonance spectroscopy reflect the aggressiveness of endometrial cancer? *Acad Radiol.* 2015;22(4):453–9.
- Oncology FCoG. FIGO staging for carcinoma of the vulva, cervix, and corpus uteri. *Int J Gynaecol Obstet Off Organ Int Fed Gynaecol Obstet.* 2014;125(2):97–8.
- Mescher M, Merkle H, Kirsch J, Garwood M, Gruetter R. Simultaneous in vivo spectral editing and water suppression. *NMR Biomed.* 1998;11(6):266–72.
- Denkert C, Loibl S, Müller BM, Eidtmann H, Schmitt WD, Eiermann W, Gerber B, Tesch H, Hilfrich J, Huober J, et al. Ki67 levels as predictive and

- prognostic parameters in pretherapeutic breast cancer core biopsies: a translational investigation in the neoadjuvant GeparTrio trial. *Ann Oncol Off J Eur Soc Med Oncol*. 2013;24(11):2786–93.
11. Yoshioka T, Hosoda M, Yamamoto M, Taguchi K, Hatanaka KC, Takakuwa E, Hatanaka Y, Matsuno Y, Yamashita H. Prognostic significance of pathologic complete response and Ki67 expression after neoadjuvant chemotherapy in breast cancer. *Breast Cancer*. 2015;22(2):185–91.
 12. Julia-Sape M, Candiota AP, Arus C. Cancer metabolism in a snapshot: MRS(I). *NMR Biomed*. 2019;32(10):e4054.
 13. Sivalingam VN, Latif A, Kitson S, McVey R, Finegan KG, Marshall K, Lisanti MP, Sotgia F, Stratford IJ, Crosbie EJ. Hypoxia and hyperglycaemia determine why some endometrial tumours fail to respond to metformin. *Br J Cancer*. 2020;122(1):62–71.
 14. Jiang JX, Zhao JL, Zhang Q, Qing JF, Zhang SQ, Zhang YM, Wu XH. Endometrial carcinoma: diffusion-weighted imaging diagnostic accuracy and correlation with Ki-67 expression. *Clin Radiol*. 2018;73(4):413 e411–413 e416.
 15. Gao W, Wang X, Li F, Shi W, Li H, Zeng Q. Cho/Cr ratio at MR spectroscopy as a biomarker for cellular proliferation activity and prognosis in glioma: correlation with the expression of minichromosome maintenance protein 2. *Acta Radiol (Stockholm, Sweden: 1987)*. 2019;60(1):106–12.
 16. Lima AR, Pinto J, Bastos ML, Carvalho M, Guedes de Pinho P. NMR-based metabolomics studies of human prostate cancer tissue. *Metabol Off J Metabol Soc*. 2018;14(7):88.
 17. Ytre-Hauge S, Esmaili M, Sjobakk TE, Gruner R, Woie K, Werner HM, Krakstad C, Bjorge L, Salvesen OO, Stefansson IM, et al. In vivo MR spectroscopy predicts high tumor grade in endometrial cancer. *Acta Radiol (Stockholm, Sweden: 1987)*. 2018;59(4):497–505.
 18. Sozzi G, Uccella S, Berretta R, Petrillo M, Fanfani F, Monterossi G, Ghizzoni V, Frusca T, Ghezzi F, Chiantera V, et al. Tumor size, an additional risk factor of local recurrence in low-risk endometrial cancer: a large multicentric retrospective study. *Int J Gynecol Cancer Off J Int Gynecol Cancer Soc*. 2018;28(4):684–91.
 19. Yue W, Meng N, Wang J, Liu W, Wang X, Yan M, Han D, Cheng J. Comparative analysis of the value of diffusion kurtosis imaging and diffusion-weighted imaging in evaluating the histological features of endometrial cancer. *Cancer Imaging Off Publ Int Cancer Imaging Soc*. 2019;19(1):9.
 20. Zhang Q, Yu X, Lin M, Xie L, Zhang M, Ouyang H, Zhao X. Multi-b-value diffusion weighted imaging for preoperative evaluation of risk stratification in early-stage endometrial cancer. *Eur J Radiol*. 2019;119:108637.
 21. Liu J, Yuan F, Wang S, Chen X, Ma F, Zhang G, Tian X. The ability of ADC measurements in the assessment of patients with stage I endometrial carcinoma based on three risk categories. *Acta radiologica (Stockholm, Sweden: 1987)*. 2019;60(1):120–8.
 22. Yan B, Liang X, Zhao T, Ding C, Zhang M. Is the standard deviation of the apparent diffusion coefficient a potential tool for the preoperative prediction of tumor grade in endometrial cancer? *Acta Radiol*. 2020;61(12):1724–32.
 23. Takayama Y, Nishie A, Togao O, Asayama Y, Ishigami K, Ushijima Y, Okamoto D, Fujita N, Sonoda K, Hida T, et al. Amide proton transfer MR imaging of endometrioid endometrial adenocarcinoma: association with histologic grade. *Radiology*. 2018;286(3):909–17.
 24. Nougaret S, Reinhold C, Alsharif SS, Addley H, Arceneau J, Molinari N, Guiu B, Sala E. Endometrial cancer: combined MR volumetry and diffusion-weighted imaging for assessment of myometrial and lymphovascular invasion and tumor grade. *Radiology*. 2015;276(3):797–808.
 25. Ytre-Hauge S, Dybvik JA, Lundervold A, Salvesen OO, Krakstad C, Fasmer KE, Werner HM, Ganeshan B, Hoivik E, Bjorge L, et al. Preoperative tumor texture analysis on MRI predicts high-risk disease and reduced survival in endometrial cancer. *J Magn Reson Imaging JMRI*. 2018;48(6):1637–47.
 26. Ueno Y, Forghani B, Forghani R, Dohan A, Zeng XZ, Chamming's F, Arsenneau J, Fu L, Gilbert L, Gallix B, et al. Endometrial carcinoma: MR imaging-based texture model for preoperative risk stratification-A preliminary analysis. *Radiology*. 2017;284(3):748–57.
 27. Satta S, Dolciami M, Celli V, Di Stadio F, Perniola G, Palaia I, Pernazza A, Della Rocca C, Rizzo S, Catalano C, et al. Quantitative diffusion and perfusion MRI in the evaluation of endometrial cancer: validation with histopathological parameters. *Br J Radiol*. 2021;94(1125):20210054.
 28. Fasmer KE, Bjornerud A, Ytre-Hauge S, Gruner R, Tangen IL, Werner HM, Bjorge L, Salvesen OO, Trovik J, Krakstad C, et al. Preoperative quantitative dynamic contrast-enhanced MRI and diffusion-weighted imaging predict aggressive disease in endometrial cancer. *Acta Radiol*. 2018;59(8):1010–7.
 29. Haldorsen IS, Gruner R, Husby JA, Magnussen IJ, Werner HM, Salvesen OO, Bjorge L, Stefansson I, Akslen LA, Trovik J, et al. Dynamic contrast-enhanced MRI in endometrial carcinoma identifies patients at increased risk of recurrence. *Eur Radiol*. 2013;23(10):2916–25.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Ready to submit your research? Choose BMC and benefit from:

- fast, convenient online submission
- thorough peer review by experienced researchers in your field
- rapid publication on acceptance
- support for research data, including large and complex data types
- gold Open Access which fosters wider collaboration and increased citations
- maximum visibility for your research: over 100M website views per year

At BMC, research is always in progress.

Learn more biomedcentral.com/submissions

