



# Assessment of Osteoporosis in Lumbar Spine: *In Vivo* Quantitative MR Imaging of Collagen Bound Water in Trabecular Bone

## **OPEN ACCESS**

#### Edited by:

Bing Wu, GE Healthcare, China

#### Reviewed by:

Liheng Ma, The First Affiliated Hospital of Guangdong Pharmaceutical University, China Yunfei Zha, Renmin Hospital of Wuhan University, China

#### \*Correspondence:

Shao-Lin Li lishaolin1963@126.com

<sup>†</sup>These authors have contributed equally to this work and share first authorship

<sup>‡</sup>These authors have contributed equally to this work and share last authorship

#### Specialty section:

This article was submitted to Bone Research, a section of the journal Frontiers in Endocrinology

Received: 26 October 2021 Accepted: 21 January 2022 Published: 16 February 2022

#### Citation:

Liu J, Liao J-W, Li W, Chen X-J, Feng J-X, Yao L, Huang P-H, Su Z-H, Lu H, Liao Y-T, Li S-L and Ma Y-J (2022) Assessment of Osteoporosis in Lumbar Spine: In Vivo Quantitative MR Imaging of Collagen Bound Water in Trabecular Bone. Front. Endocrinol. 13:801930. doi: 10.3389/fendo.2022.801930 Jin Liu<sup>1†</sup>, Jian-Wei Liao<sup>1†</sup>, Wei Li<sup>1</sup>, Xiao-Jun Chen<sup>1</sup>, Jia-Xin Feng<sup>1</sup>, Lin Yao<sup>1</sup>, Pan-Hui Huang<sup>1</sup>, Zhi-Hai Su<sup>2</sup>, Hai Lu<sup>2</sup>, Yu-Ting Liao<sup>3</sup>, Shao-Lin Li<sup>1\*‡</sup> and Ya-Jun Ma<sup>4‡</sup>

<sup>1</sup> Department of Radiology, The Fifth Affiliated Hospital of Sun Yat-Sen University, Zhuhai, China, <sup>2</sup> Department of Spinal Surgery, The Fifth Affiliated Hospital of Sun Yat-Sen University, Zhuhai, China, <sup>3</sup> MR Research, GE Healthcare, Guangzhou, China, <sup>4</sup> Department of Radiology, University of California San Diego, La Jolla, CA, United States

**Aim:** Bone collagen matrix makes a crucial contribution to the mechanical properties of bone by imparting tensile strength and elasticity. The collagen content of bone is accessible *via* quantification of collagen bound water (CBW) indirectly. We prospectively study the performance of the CBW proton density (CBWPD) measured by a 3D short repetition time adiabatic inversion recovery prepared ultrashort echo time (STAIR-UTE) magnetic resonance imaging (MRI) sequence in the diagnosis of osteoporosis in human lumbar spine.

**Methods:** A total of 189 participants with a mean age of 56 (ranged from 50 to 86) years old were underwent MRI, quantitative computed tomography (QCT), and dual-energy X-ray absorptiometry (DXA) in lumbar spine. Major fracture risk was also evaluated for all participants using Fracture Risk Assessment Tool (FRAX). Lumbar CBWPD, bone marrow fat fraction (BMFF), bone mineral density (BMD) and T score values were calculated in three vertebrae (L2–L4) for each subject. Both the CBWPD and BMFF were correlated with BMD, T score, and FRAX score for comparison. The abilities of the CBWPD and BMFF to discriminate between three different cohorts, which included normal subjects, patients with osteopenia, and patients with osteoporosis, were also evaluated and compared using receiver operator characteristic (ROC) analysis.

**Results:** The CBWPD showed strong correlation with standard BMD ( $R^2 = 0.75$ , P < 0.001) and T score ( $R^2 = 0.59$ , P < 0.001), as well as a moderate correlation with FRAX score ( $R^2 = 0.48$ , P < 0.001). High area under the curve (AUC) values ( $\ge 0.84$  using QCT as reference;  $\ge 0.76$  using DXA as reference) obtained from ROC analysis demonstrated that the CBWPD was capable of well differentiating between the three different subject cohorts. Moreover, the CBWPD had better correlations with BMD, T score, and FRAX score than BMFF, and also performed better in cohort discrimination.

1

**Conclusion:** The STAIR-UTE-measured CBWPD is a promising biomarker in the assessment of bone quality and fracture risk.

Keywords: osteoporosis, ultrashort echo time, collagen bound water proton density, bone mineral density, bone marrow fat fraction

## INTRODUCTION

Osteoporosis (OP) has become a major public health burden as the population continues to age (1, 2). Each year, about 200 million people worldwide suffer from OP, with approximately 89 million fractures occurring on an annual basis (3). OP is characterized by a decrease in bone strength combined with an increased risk of fracture as a result of low bone mass and microarchitectural deterioration of bone tissue (4).

Bone mineral density (BMD) plays a major role in bone strength and its measurement of trabecular bone in the spine and/or hip using dual-energy x-ray absorptiometry (DXA) is the clinical standard for assessments of both OP and fracture risk (5–7). Quantitative computed tomography (QCT) utilizes 3D volumetric imaging and quantification to further improve the accuracy of these BMD measurements but with increased ionizing radiation.

The organic matrix, another important bone component, provides tensile strength and elasticity, also contributing significantly to the mechanical properties of bone (8). Because changes in the collagen density and integrity within the bone's organic matrix affect overall bone quality (9), quantitative evaluation of the collagen matrix is likely to provide valuable information on an individual's bone strength (10–12).

Unfortunately, both DXA and QCT are limited in their abilities to assess changes in the collagen matrix due to their low soft tissue contrast. Magnetic resonance imaging (MRI) is a superior method in that it offers high-contrast soft tissue imaging. However, collagen cannot be directly imaged by MRI due to its extremely short T2 relaxation time (about 10 µs) (13-15). Alternatively, indirect evaluation of the collagen matrix can be performed by quantification of the water molecules which are tightly bound to the collagen matrix (i.e., collagen bound water (CBW)) and are highly correlated with the matrix collagen's density and integrity (16). Like collagen itself, the CBW also has a relatively short T<sub>2</sub> relaxation time—around 300 µs. While CBW is not accessible to clinical sequences with long echo times (TEs) (i.e., several to hundreds of milliseconds) such as gradient recalled echo (GRE) and fast spin echo (FSE) (17, 18), a specialized MRI technique known as the ultrashort echo time (UTE) sequence has been developed with a TE less than 100 µs to specifically target tissues with short T<sub>2</sub> relaxation times. This UTE MRI approach can be used to image and quantify the CBW (19).

In the last decade, UTE MRI imaging of CBW has been studied by several groups as a possible surrogate measure for the bone's collagen matrix (18, 20–23). It was found that the UTE measurements scale to an almost linear degree with collagen matrix density (22, 24, 25), and highly correlated with yield, peak stress, and elastic toughness (25, 26). However, most of the previous studies were focused on CBW measurement in cortical bone. CBW evaluation in trabecular bone has the potential to be even more valuable a measurement because not only do most osteoporotic fractures occur in trabecular bone, but trabecular bone is also highly responsive to metabolic stimuli (27–30). However, quantification of CBW in trabecular bone is more technically challenging than in cortical bone due to trabecular bone's much lower CBW content and higher concentration of tissue components with long T<sub>2</sub> relaxation times, such as marrow fat (31).

Most recently, a new 3D short repetition time adiabatic inversion recovery prepared UTE (3D STAIR-UTE) Cones sequence was developed which could volumetrically quantify CBW proton density (CBWPD) of trabecular bone *in vivo* for the first time (17). The STAIR-UTE sequence can generate high contrast imaging of CBW with sufficient suppression of all the long  $T_2$  signals.

The purpose of our study was to investigate the STAIR-UTEmeasured CBWPD in the classification of patients as normal, osteopenic and osteoporotic in the lumbar spine with golden standard QCT-measured BMD and DXA-measured T score as reference. The CBWPD was also correlated with fracture risk score which was characterized by Fracture Risk Assessment Tool (FRAX). Moreover, vertebral bone marrow fat fraction (BMFF) —another quantitative imaging biomarker that has been studied extensively in OP assessment—was also employed for comparison against CBWPD.

#### MATERIALS AND METHODS

#### Subject Recruitment

This study was conducted under Institutional Review Board approval; written informed consent was obtained from all participants. Between June 2020 and January 2021, 189 participants with a mean age of 56 (ranged from 50 to 86) years old were recruited to participate in this prospective study. MRI, QCT, and DXA examinations of the lumbar spine for each participant were performed in the same week. Subjects were excluded if they had known preexisting bone diseases (e.g., lumbar fracture, tumor, metastases, dysplasia, or metabolic disorders), a history of lumbar surgery, or a history of drug therapy targeted at BMD. We also excluded any subjects who had a history of osteoarthritis, inflammatory arthritis, cancer, Paget disease, endocrinologic or gastrointestinal disorder, glucocorticoid use, selective serotonin uptake inhibitor use, or anticonvulsant use.

#### QCT and DXA Examinations

QCT examinations of the lumbar region were performed on a 128-channel multi-detector CT scanner (uCT 760, United

Imaging Healthcare). All CT parameters were set in accordance with the "China Health Quantitative CT Big Data Project Research Program" (32) as follows: collimation: 0.625 mm, tube voltage: 120 kVp, tube current: automatic. All CT images were reconstructed to 512×512 matrices using iterative reconstruction algorithms available from the vendor's CT scanners. The reconstruction intervals were 1.0 mm. Our QCT post-processing can only quantify three vertebral bodies at a time, so the center three vertebral elements of the lumbar spine (i.e., L2-L4) were chosen for the quantification.

Standard DXA scan (Osteocore, Medilink 90kv and 2mA) was performed according to WHO guidelines (33) to acquire T score in the lumbar spine. Images of the lumbar spine were obtained in posterior-anterior projection.

#### **MR** Imaging

All 189 participants underwent spine MR imaging on a 3T clinical scanner (Pioneer, GE Healthcare Technologies, Milwaukee, WI) with a spine-array surface coil for signal reception. Clinical sagittal T<sub>1</sub>-weighted FSE (repetition time (TR): 540 ms, TE: 8 ms, flip angle (FA): 80°, field-of-view (FOV):  $32\times32$  cm<sup>2</sup>, pixel size:  $1.0\times1.4$  mm<sup>2</sup>, number of slices: 13, slice thickness: 4 mm, scan time: 1 min) and T<sub>2</sub>-weighted FSE (TR: 2291 ms, TE: 90 ms, FA: 90°, FOV:  $32\times32$  cm<sup>2</sup>, pixel size:  $1.0\times1.4$  mm<sup>2</sup>, number of slices: 13, slice thickness: 4 mm, scan time: 1 min) and T<sub>2</sub>-weighted FSE (TR: 2291 ms, TE: 90 ms, FA: 90°, FOV:  $32\times32$  cm<sup>2</sup>, pixel size:  $1.0\times1.4$  mm<sup>2</sup>, number of slices: 13, slice thickness: 4 mm, scan time: 2 min) scans of the lumbar spine were included. A product sequence, IDEAL-IQ (Iterative decomposition of water and fat with echo asymmetry and least squares estimation) (34), was used to quantify BMFF (TR: 7.3 ms; TEs: 1.2, 2.1, 3.1, 4.1, 5.0, and 6.0 ms; FA: 4°; FOV:  $32\times32$  cm<sup>2</sup>; pixel size:  $2.0\times2.0$  mm<sup>2</sup>; number of slices: 12; slice thickness: 8 mm; and scan time: 16 sec).

The 3D STAIR-UTE Cones sequence was performed in the sagittal plane for the CBW imaging (17) (TR: 150 ms, TE: 0.032 ms, inversion time (TI): 64 ms, FA: 18°, number of spokes per-TR: 5, spoke interval: 5.5 ms, FOV: 30 cm×30 cm, pixel size: 2.1×2.1mm<sup>2</sup>, number of slices: 16, slice thickness: 4.5 mm, oversampling factor: 2, scan time: 10 min). In order to acquire a spine coil sensitivity profile for correction of the STAIR-UTE imaging inhomogeneity, the 3D UTE Cones sequence was applied twice without STAIR preparation, using spine and body coils for signal reception, respectively (17) (TR: 6 ms, TE: 0.032 ms, FA: 2°, FOV: 30 cm×30 cm; pixel size, 2.1×2.1 mm<sup>2</sup>, number of slices: 16, slice thickness: 4.5 mm, and scan time: 1 min. A rubber band with a T2\* of 0.34 ms and a premeasured proton density of 18 mol/L was placed between the spine coil and participants during scanning to serve as a reference standard. The CBWPD of trabecular bone was calculated using Equation [9] in Ref (17).. Ten healthy volunteers were recruited to study the reproducibility of the STAIR-UTE Cones sequence. Each volunteer was scanned three times over three consecutive days.

#### **Fracture Risk Characterization**

The major fracture risk (i.e., 10-year probability of osteoporotic fracture) of each participant was characterized using FRAX (https://www.sheffield.ac.uk/FRAX) with 11 clinical variables taken into consideration (i.e., age, sex, weight, height, previous fracture, parental hip fracture, current smoking status,

glucocorticoid use, rheumatoid arthritis, secondary OP, and alcohol use of three or more units per day).

#### **Data Analysis**

The CBWPD calculation was performed in MATLAB (The MathWorks, Natick, MA). Regions of interest (ROIs) were manually drawn in the trabecular bone region—avoiding the subchondral bone region—to measure BMD, CBWPD, and BMFF in L2–L4. Mean lumbar BMD, CBWPD, and BMFF values were computed by averaging them across these three vertebrae for each subject. ROIs were independently drawn by two radiologists with 10 (W.L.) and 8 (J.L.) years of respective experience to assess inter-observer agreement of ROIs. To assess intra-observer agreement of ROI drawing, this procedure was repeated by the radiologist with 10 years of experience two months after the initial ROI drawing.

For the DXA experiment, T score was used to assess osteoporosis since all the participants were over 50 years old according to WHO guidelines (35). The scanned subjects were grouped into three cohorts (normal, osteopenia, and OP). A BMD (measured by QCT) greater than 120 mg/cm<sup>3</sup> (equivalent to a DXA T score > -1.0 standard deviation (SD)) indicates normal, a BMD value between 80 mg/cm<sup>3</sup> and 120 mg/cm<sup>3</sup> (equivalent to a DXA T score < -1.0 SD and > -2.5 SD) indicates osteopenia, and a BMD less than 80 mg/cm<sup>3</sup> (equivalent to a DXA T score of < -2.5 SD) indicates OP.

#### **Statistical Analysis**

Statistical analysis was performed using Statistical Package for Social Sciences (SPSS) software (version 23.0). P < 0.05 was considered statistically significant. Linear regression and Bland-Altman analysis were performed to assess the reproducibility of the STAIR-UTE Cones sequence. Intra- and interclass correlation coefficients (ICC) were calculated to assess both the interobserver and intra-observer reproducibility of CBWPD and BMFF measurements. The differences in age, body mass index (BMI), BMD, T score, CBWPD, BMFF, and FRAX score among all three cohorts (normal, osteopenia, and OP) were determined using the Kruskal-Wallis test. The differences in sex among all three cohorts were determined using the Chi-square test. Linear regression was performed to correlate the CBWPD and BMFF with BMD and T score, respectively. Non-linear regression using an exponential function was performed to correlate the CBWPD and BMFF with FRAX score. To evaluate the performances of the CBWPD and BMFF in discriminating between the three cohorts, receiver operating characteristic (ROC) analysis was performed and the area under the curve (AUC) with 95% confidence interval (CI) was computed using Medcalc software (version 20.0.3). The DeLong test was used to compare the ROC curves (i.e., AUCs) between CBWPD and BMFF.

## RESULTS

Data analysis was performed on 162 of the recruited 189 participants, with the 27 exclusions made due to bone disease (n = 17) and poor MR image quality caused by motion during the

scan (n = 10). Participant characteristics are described in **Table 1**. Age, BMD, T score, CBWPD, BMFF, and FRAX score all showed significant differences among the three cohorts, with QCT and DXA used as the respective reference standards.

**Figure 1** shows representative BMD, T score, CBWPD, and BMFF maps of the lumbar spines of three subjects: one from each cohort (normal, osteopenia, and OP). Lower CBWPD, BMD, and T score, as well as higher BMFF, were found in more osteoporotic subjects.

#### Reproducibility

The results of linear regression and Bland–Altman analysis of the STAIR-UTE measured CBWPDs for the three repeated volunteer scans are shown in **Figure 2**. Strong correlations and high agreements of the CBWPD measurements were found between the first and the second scans with a  $R^2 = 0.96$  (P < 0.001) and a mean bias of -0.02 mol/L (± 1.96 SD: range -0.30 to 0.27 mol/L) (**Figure 2A**) respectively, between the first and the third scans with a  $R^2 = 0.90$  (P < 0.001) and a mean bias of -0.003 mol/L (± 1.96 SD: range -0.42 to 0.41 mol/L) (**Figure 2B**) respectively, and between the second and the third scans with a  $R^2 = 0.91$  (P < 0.001) and a mean bias of 0.01 mol/L (± 1.96 SD: range -0.37 to 0.40 mol/L) (**Figure 2C**) respectively. These results demonstrate an excellent reproducibility for the STAIR-UTE Cones scans.

The interobserver ICCs for the CBWPD and BMFF measurements between the two radiologists were 0.93 and 0.92, respectively. The intra-observer ICCs for the CBWPD and BMFF quantification were 0.95 and 0.93, respectively. These high ICC values demonstrate excellent reproducibility for both interobserver and intra-observer measurements.

## Correlations

The CBWPD showed a positive correlation with BMD ( $R^2 = 0.75$ , P < 0.001) (**Figure 3A**), a positive correlation with T score

 $(R^2 = 0.59, P < 0.001)$  (**Figure 3B**), and a negative correlation with FRAX score ( $R^2 = 0.48, P < 0.001$ ) (**Figure 3C**).

The BMFF showed a negative correlation with BMD ( $R^2 = 0.45$ , P < 0.001) (**Figure 3D**), a negative correlation with T score ( $R^2 = 0.23$ , P < 0.001) (**Figure 3E**), and a positive correlation with FRAX score ( $R^2 = 0.20$ , P < 0.001) (**Figure 3F**).

As demonstrated by these results, the CBWPD correlates better with BMD, T score, and FRAX score than the BMFF does.

## **ROC Analysis**

**Figures 4A–C** show the ROC curves of CBWPD<sup>QCT</sup> and BMFF<sup>QCT</sup> (with QCT as reference standard) in differentiating normal subjects, patients with osteopenia, and patients with OP. **Table 2** summarizes all the criteria that were used to evaluate the diagnostic performance of CBWPD<sup>QCT</sup> and BMFF<sup>QCT</sup>. The AUC values of CBWPD<sup>QCT</sup> and BMFF<sup>QCT</sup> were 0.84 and 0.70 (P < 0.001) for normal vs. osteopenia, 0.98 and 0.89 (P < 0.001) for normal vs. OP, and 0.90 and 0.79 (P < 0.001) for osteopenia vs. OP, respectively. The AUC values of CBWPD<sup>QCT</sup> were consistently higher than the corresponding AUC values of BMFF<sup>QCT</sup>.

**Figures 4D-F** show the ROC curves of CBWPD<sup>DXA</sup> and BMFF<sup>DXA</sup> (with DXA as reference standard) in differentiating normal subjects, patients with osteopenia, and patients with OP. **Table 3** summarizes all the criteria that were used to evaluate the diagnostic performance of CBWPD<sup>DXA</sup> and BMFF<sup>DXA</sup>. The AUC values of CBWPD<sup>DXA</sup> and BMFF<sup>DXA</sup> were 0.83 and 0.68 (P < 0.001) for normal vs. osteopenia, 0.93 and 0.82 (P < 0.001) for normal vs. OP, and 0.76 and 0.65 (P = 0.005) for osteopenia vs. OP, respectively. The AUC values of CBWPD<sup>DXA</sup> were consistently higher than the corresponding AUC values of BMFF<sup>DXA</sup>.

As demonstrated by these results, the CBWPD shows high capability to classify patients as normal, osteopenic and

TABLE 1 | Characteristics of patients in three cohorts of normal subjects, patients with osteopenia, and patients with osteoporosis.

	All subjects (n=162)	QCT as reference standard				DXA as reference standard			
		Normal (n = 86)	Osteopenia (n = 41)	Osteoporosis (n = 35)	<b>PValue</b>	Normal (n = 88)	Osteopenia (n = 46)	Osteoporosis (n = 28)	<i>P</i> Value
Sex					0.198				0.148
male	65 (40%)	35 (41%)	20 (49%)	10 (29%)		36 (41%)	22 (48%)	7 (25%)	
female	97 (60%)	51 (59%)	21 (51%)	25 (71%)		52 (59%)	24 (52%)	21 (75%)	
Age (years)	58 (9)	53 (5)	60 (8)	68 (9)	< 0.001	55 (6)	60 (9)	66 (10)	<0.001
BMI (kg/m <sup>2</sup> )	23.4 (21.3-25.4)	23.4 (21.5-25.5)	23.8 (21.1-26.8)	22.9 (20.5-	0.517	23.7 (21.7-26.0)	23.9 (21.3-	21.68 (20.1-	0.004
				25.0)			26.1)	23.6)	
BMD (mg/cm <sup>3</sup> )	119.8 (83.6-	155.6 (132.5-	100.7 (90.0-	54.1 (43.9-	< 0.001	148.9 (125.5-	99.8 (80.2-	60.9 (47.9-	<0.001
	154.7)	175.7)	111.1)	67.9)		174.7)	120.6)	71.1)	
T score	0.5 (-2.1 to	0.8 (-0.3 to 2.0)	-1.3 (-2.0 to	-2.7 (-3.4 to	< 0.001	1.0 (0.0 to 2.0)	-1.7 (-2.1 to	-3.1 (-3.5 to	<0.001
	-0.6)		-0.3)	-2.3)			-1.3)	-2.6)	
CBWPD (mol/L)	2.5 (1.9-2.9)	2.9 (2.5-3.3)	2.3 (2.1-2.5)	1.6 (1.3-1.8)	< 0.001	2.9 (2.4-3.2)	2.2 (1.8-2.4)	1.7 (1.4-1.9)	< 0.001
BMFF (%)	54.2 (44.4-63.3)	48.0 (41.2-55.2)	55.8 (48.2-62.8)	67.5 (60.0- 73.4)	<0.001	49.2 (42.0-56.5)	57.1 (46.7- 67.9)	65.0 (58.1- 72.7)	<0.001
FRAX score (%)	3.7 (1.5-4.7)	1.9 (1.2-2.0)	3.80 (1.9-5.0)	7.8 (4.6-9.5)	< 0.001	1.7 (1.2-1.9)	3.9 (2.3-4.8)	9.3 (6.2-10.0)	<0.001

Data are presented as n (%), mean (SD), or median (IQR). All comparisons between the three cohorts were significant (P < 0.001) except for sex (P = 0.198, taking QCT as reference standard; P = 0.148, taking DXA as reference standard) and BMI (P = 0.517, taking QCT as reference standard; P = 0.004, taking DXA as reference standard). BMI, body mass index; CBWPD, collagen bound water proton density; QCT, quantitative computed tomography; BMD, bone mineral density; DXA, dual-energy X-ray absorptiometry; BMFF, bone marrow fat fraction; FRAX, Fracture Risk Assessment Tool; IQR, interquartile range.





osteoporotic. It also performs better than the BMFF in discrimination of the three cohorts whether using QCT or DXA as the reference standard.

# DISCUSSION

In this prospective study, we presented a noninvasive and nondestructive MRI technique to measure CBWPD in the human lumbar spine for assessment of trabecular bone quality using QCT and DXA as the reference standard. To the best of our knowledge, this is the first study of trabecular CBWPD in the diagnosis of OP *in vivo*. The CBWPD showed strong correlations with standard BMD ( $\mathbb{R}^2 = 0.75$ ) and T score ( $\mathbb{R}^2 = 0.59$ ), as well as a moderate correlation with FRAX score ( $\mathbb{R}^2 = 0.48$ ). High AUC values ( $\geq 0.84$  using QCT as reference,  $\geq 0.76$  using DXA as reference) obtained from ROC analysis demonstrated that the CBWPD was capable of discriminating between the three subject cohorts which included normal subjects, patients with osteopenia, and patients with OP. Moreover, the CBWPD had stronger correlations with BMD, T score, and FRAX score than BMFF did, and also performed better in cohort discrimination. This study demonstrates that the STAIR-



measured CBWPDs between the first and the second scans (A), between the first and the third scans (B), and between the second and the third scans (C). Dotted lines in the Bland–Altman difference plots (right column) demarcate 1.96 standard deviations of the mean difference.

UTE-measured CBWPD is a promising biomarker to be used in clinical practice for assessment of bone quality and fracture risk.

The STAIR-UTE sequence used in this study is able to efficiently suppress all the long T<sub>2</sub> components in trabecular bone, including marrow fat and free water, and selectively image CBW. As can be seen in Ref. 17, numerical simulation results showed that, when a sufficiently short TR was used, the STAIR-UTE sequence achieved efficient signal suppression for long  $T_2$ tissues with a wide range of  $T_{1s}$ . When a minimal TR (i.e., TR = 150 ms, restricted by SAR limitation) was used in the STAIR-UTE sequence on a clinical 3T scanner, only short T<sub>2</sub> signals were detected in the *in vivo* vertebral bone with a  $T_2^*$  of 0.31 ms, clearly demonstrating the technical feasibility of the STAIR-UTE sequence in sufficient suppression of all the long T<sub>2</sub> signals. At the long T<sub>2</sub> signal null point (TI<sub>null</sub>), signal from the short T<sub>2</sub> component (i.e., the CBW) can be efficiently detected by the 3D UTE Cones sequence with a minimal TE of 32 µs. In addition, the relatively low STAIR-UTE resolution used in this study was able to increase the SNR of short T<sub>2</sub> imaging and thereby improve the accuracy of CBW quantification.

Approximately 40-50% of women and 13-22% of men are at risk of osteoporotic fracture after the age of 50, and major osteoporotic fractures result in substantial morbidity and mortality (2, 36). Early assessment of bone quality and fracture risk is crucial for effective intervention or treatment. The collagen matrix makes a crucial contribution to the mechanical properties of bone by imparting tensile strength and elasticity (37). However, changes in the organic matrix are inaccessible to DXA, QCT, and even clinical MRI due to the technical limitations of these imaging modalities (14, 15).

The STAIR-UTE MRI technique is capable of indirectly accessing properties in the collagen matrix by performing measurements of the CBWPD in trabecular bone (17). The CBW provides important information regarding the collagen density and hydration state of the organic matrix to which it is bound. In this way, CBW quantification could act as a possible surrogate for assessment of the collagen matrix.

It is known that mineral crystals are scattered in the gaps between continuous collagen fibers (38), suggesting that the quantity of collagen fibers may be related to the BMD. In our



FIGURE 3 | Correlation curves and scatter plots for the measurements between (A) collagen bound water proton density (CBWPD) and bone mineral density (BMD), (B) CBWPD and T score, (C) CBWPD and Fracture Risk Assessment Tool (FRAX) score, (D) bone marrow fat fraction (BMFF) and BMD, (E) BMFF and T score, and (F) BMFF and FRAX score.

trabecular bone study, the strong positive correlation between CBWPD and BMD was in line with the findings in previous cortical bone studies as it demonstrated that both the bone mineral and organic matrix were decreased in OP (39–41).

A moderate correlation between the CBWPD and FRAX score demonstrated that the STAIR-UTE-measured CBWPD has the potential to be useful in assessing fracture risk or could even be combined into the FRAX score calculation for further improved risk assessment. Another advantage of the STAIR-UTE MRI technique is the absence of ionizing radiation which may make it a preferable technique for regular examinations (an important approach for early detection of bone loss) or longitudinal studies that monitor patient response to treatment.

Many studies have shown increased marrow fat during OP (42–47). In our study, it was clear that CBWPD was more sensitive to the changes in bone than BMFF, evidenced by the CBWPD's improved correlations with BMD, T score, and FRAX score over BMFF, as well as its superior performance in terms of cohort discrimination. CBWPD's increased sensitivity to bone changes is not surprising because BMFF does not reveal true bone loss: some patients with normal BMFF have been reported to have bone loss or abnormal bone mineralization (48).



TABLE 2 | Performance of the CBWPD<sup>QCT</sup> and BMFF<sup>QCT</sup> in discrimination between three cohorts of normal subjects, patients with osteopenia, and patients with osteopenias, with QCT as reference standard.

	CBWPD <sup>QCT</sup>			BMFF <sup>QCT</sup>			
	Normal vs. osteopenia	Normal vs. osteoporosis	Osteopenia vs. osteoporosis	Normal vs. osteopenia	Normal vs. osteoporosis	Osteopenia vs. osteoporosis	
AUC (95%Cl)	0.839 (0.799, 0.879)	0.978 (0.963, 0.992)	0.902 (0.861, 0.944)	0.704 (0.649, 0.759)	0.894 (0.854, 0.933)	0.786 (0.728, 0.845)	
Sensitivity (95%Cl)	0.705 (0.649, 0.762)	0.968 (0.946, 0.990)	0.872 (0.813, 0.931)	0.840 (0.776, 0.904)	0.882 (0.821, 0.942)	0.636 (0.546, 0.726)	
Specificity (95%Cl)	0.808 (0.739, 0.877)	0.918 (0.867, 0.969)	0.845 (0.778, 0.913)	0.490 (0.428, 0.552)	0.821 (0.773, 0.868)	0.808 (0.739, 0.877)	
ACC (95%CI)	0.739 (0.738, 0.740)	0.953 (0.953, 0.953)	0.860 (0.859, 0.861)	0.606 (0.605, 0.608)	0.839 (0.839, 0.840)	0.728 (0.726, 0.729)	
PPV (95%Cl)	0.881 (0.836, 0.925)	0.964 (0.941, 0.987)	0.865 (0.805, 0.925)	0.451 (0.387, 0.515)	0.683 (0.607, 0.760)	0.745 (0.657, 0.833)	
NPV (95%Cl)	0.577 (0.504, 0.650)	0.927 (0.878, 0.976)	0.853 (0.787, 0.920)	0.860 (0.803, 0.917)	0.941 (0.909, 0.972)	0.716 (0.642, 0.791)	

CBWPD, collagen bound water proton density; BMFF, bone marrow fat fraction; QCT, quantitative computed tomography; AUC, area under curve; ACC, Accuracy; PPV, Positive Predictive Value; NPV, Negative Predictive Value; CI, Confidence Interval.

There are several limitations in this study. First, the scan time of the CBWPD measurement protocol was relatively long (around 12 min in total) compared to clinical sequences. Advanced image reconstruction methods such as compressed sensing or deep learning could be incorporated to accelerate the scan with comparable image quality (49, 50) in the future. Second, we did not follow up on the fracture rate of these patients for 5-10 years, though such a long-term study will be completed in future work. The longitudinal study would be valuable in further validating the proposed technique and in TABLE 3 | Performance of the CBWPD<sup>DXA</sup> and BMFF<sup>DXA</sup> in discrimination between three cohorts of normal subjects, patients with osteopenia, and patients with osteopenia, with DXA as reference standard.

CBWPD <sup>DXA</sup>			BMFF <sup>DXA</sup>			
Normal vs. osteopenia	Normal vs. osteoporosis	Osteopenia vs. osteoporosis	Normal vs. osteopenia	Normal vs. osteoporosis	Osteopenia vs. osteoporosis	
0.832 (0.792, 0.873)	0.930 (0.897, 0.963)	0.761 (0.690, 0.831)	0.676 (0.619, 0.732)	0.816 (0.760, 0.872)	0.655 (0.580, 0.729)	
0.882 (0.843, 0.921)	0.958 (0.934, 0.982)	0.917 (0.872, 0.962)	0.479 (0.398, 0.561)	0.750 (0.655, 0.845)	0.800 (0.712, 0.888)	
0.625 (0.546, 0.704)	0.788 (0.698, 0.877)	0.550 (0.441, 0.659)	0.809 (0.762, 0.857)	0.763 (0.712, 0.815)	0.458 (0.377, 0.540)	
0.791 (0.790, 0.791)	0.918 (0.918, 0.919)	0.786 (0.784, 0.787)	0.692 (0.691, 0.693)	0.760 (0.759, 0.761)	0.580 (0.578, 0.582)	
0.811 (0.765, 0.856) 0.744 (0.666, 0.822)	0.937 (0.907, 0.966) 0.851 (0.770, 0.932)	0.786 (0.724, 0.848) 0.786 (0.678, 0.893)	0.580 (0.491, 0.669) 0.739 (0.688, 0.790)	0.492 (0.403, 0.581) 0.909 (0.871, 0.947)	0.451 (0.369, 0.533) 0.805 (0.719, 0.891)	
	Normal vs. osteopenia   0.832 (0.792, 0.873) 0.882 (0.843, 0.921)   0.625 (0.546, 0.704)   0.791 (0.790, 0.791)   0.811 (0.765, 0.856)   0.744 (0.666, 0.822)	CBWPD <sup>DXA</sup> Normal vs. osteopenia Normal vs. osteoporosis   0.832 (0.792, 0.873) 0.930 (0.897, 0.963)   0.882 (0.843, 0.921) 0.958 (0.934, 0.982)   0.625 (0.546, 0.704) 0.788 (0.698, 0.877)   0.791 (0.790, 0.791) 0.918 (0.918, 0.919)   0.811 (0.765, 0.856) 0.937 (0.907, 0.966)   0.744 (0.666, 0.822) 0.851 (0.770, 0.932)	Normal vs. osteopenia Normal vs. osteoporosis Osteopenia vs. osteoporosis   0.832 (0.792, 0.873) 0.930 (0.897, 0.963) 0.761 (0.690, 0.831)   0.882 (0.843, 0.921) 0.958 (0.934, 0.982) 0.917 (0.872, 0.962)   0.625 (0.546, 0.704) 0.788 (0.698, 0.877) 0.550 (0.441, 0.659)   0.791 (0.790, 0.791) 0.918 (0.918, 0.919) 0.786 (0.784, 0.787)   0.811 (0.765, 0.856) 0.937 (0.907, 0.966) 0.786 (0.724, 0.848)   0.744 (0.666, 0.822) 0.851 (0.770, 0.932) 0.786 (0.678, 0.893)	CBWPD <sup>DXA</sup> Normal vs. osteopenia Normal vs. osteopenia Normal vs. osteopenia Normal vs. osteopenia Normal vs. osteopenia Normal vs. osteopenia   0.832 (0.792, 0.873) 0.930 (0.897, 0.963) 0.761 (0.690, 0.831) 0.676 (0.619, 0.732) 0.479 (0.398, 0.561)   0.625 (0.546, 0.704) 0.788 (0.698, 0.877) 0.550 (0.441, 0.659) 0.809 (0.762, 0.857)   0.791 (0.790, 0.791) 0.918 (0.918, 0.919) 0.786 (0.784, 0.787) 0.692 (0.691, 0.693)   0.744 (0.666, 0.822) 0.851 (0.770, 0.932) 0.786 (0.678, 0.893) 0.739 (0.688, 0.790)	CBWPD <sup>DXA</sup> BMFF <sup>DXA</sup> Normal vs. osteopenia Normal vs. osteoporosis Osteopenia vs. osteoporosis Normal vs. osteopenia Normal vs. osteoporosis   0.832 (0.792, 0.873) 0.882 (0.843, 0.921) 0.930 (0.897, 0.963) 0.958 (0.934, 0.982) 0.761 (0.690, 0.831) 0.917 (0.872, 0.962) 0.676 (0.619, 0.732) 0.479 (0.398, 0.561) 0.816 (0.760, 0.872) 0.750 (0.655, 0.845)   0.625 (0.546, 0.704) 0.788 (0.698, 0.877) 0.550 (0.441, 0.659) 0.809 (0.762, 0.857) 0.763 (0.712, 0.815)   0.791 (0.790, 0.791) 0.811 (0.765, 0.856) 0.937 (0.907, 0.966) 0.937 (0.907, 0.966) 0.786 (0.724, 0.848) 0.786 (0.678, 0.893) 0.692 (0.691, 0.693) 0.580 (0.491, 0.669) 0.492 (0.403, 0.581) 0.492 (0.403, 0.581)   0.744 (0.666, 0.822) 0.851 (0.770, 0.932) 0.786 (0.678, 0.893) 0.739 (0.688, 0.790) 0.909 (0.871, 0.947)	

CBWPD, collagen bound water proton density; BMFF, bone marrow fat fraction; DXA, dual-energy X-ray absorptiometry; AUC, area under curve; ACC, Accuracy; PPV, Positive Predictive Value; NPV, Negative Predictive Value; CI, Confidence Interval.

providing information about collagen matrix changes that accompany aging.

In conclusion, the STAIR-UTE-measured CBWPD is a promising biomarker for evaluation of the bone changes in OP and of osteoporotic fracture risk.

# DATA AVAILABILITY STATEMENT

The original contributions presented in the study are included in the article/supplementary material. Further inquiries can be directed to the corresponding author.

# ETHICS STATEMENT

The studies involving human participants were reviewed and approved by ethical approval from the institutional review board

## REFERENCES

- Khosla S, Hofbauer LC. Osteoporosis Treatment: Recent Developments and Ongoing Challenges. *Lancet Diabetes Endocrinol* (2017) 5(11):898–907. doi: 10.1016/S2213-8587(17)30188-2
- 2. Roux C, Briot K. The Crisis of Inadequate Treatment in Osteoporosis. *Lancet Rheumatol* (2020) 2(2):e110–9. doi: 10.1016/S2665-9913(19)30136-5
- Pisani P, Renna MD, Conversano F, Casciaro E, Di Paola M, Quarta E, et al. Major Osteoporotic Fragility Fractures: Risk Factor Updates and Societal Impact. World J Orthop (2016) 7(3):171–81. doi: 10.5312/wjo. v7.i3.171
- Hennemann A. Osteoporosis Prevention, Diagnosis, and Therapy. Jama (2001) 285(6):785–95. doi: 10.1001/jama.285.6.785
- Bandirali M, Lanza E, Messina C, Sconfienza LM, Brambilla R, Maurizio R, et al. Dose Absorption in Lumbar and Femoral Dual Energy X-Ray Absorptiometry Examinations Using Three Different Scan Modalities: An Anthropomorphic Phantom Study. J Clin Densitom (2013) 16(3):279–82. doi: 10.1016/j.jocd.2013.02.005
- Blake GM, Fogelman I. The Role of DXA Bone Density Scans in the Diagnosis and Treatment of Osteoporosis. *Postgrad Med J* (2007) 83(982):509–17. doi: 10.1136/pgmj.2007.057505
- Wehrli FW, Saha PK, Gomberg BR, Song HK, Snyder PJ, Benito M, et al. Role of Magnetic Resonance for Assessing Structure and Function of Trabecular Bone. *Top Magn Reson Imaging* (2002) 13(5):335–55. doi: 10.1097/00002142-200210000-00005

of The Fifth Affiliated Hospital of Sun Yat-Sen University. The patients/participants provided their written informed consent to participate in this study.

# **AUTHOR CONTRIBUTIONS**

JL, S-LL, and Y-JM conceived the study. WL, X-JC, J-XF, LY, P-HH, Z-HS, and HL collected the data. JL, Y-JM, and Y-TL analyzed the data. All the authors collaborated in interpretation of the results and drafting and revision of the report. All authors contributed to the article and approved the submitted version.

# **FUNDING**

This work was supported by the National Natural Science Foundation of China (Grant Nos. 82172053).

- Mehta SS, Oz OK, Antich PP. Bone Elasticity and Ultrasound Velocity Are Affected by Subtle Changes in the Organic Matrix. J Bone Miner Res (1998) 13 (1):114–21. doi: 10.1359/jbmr.1998.13.1.114
- Paschalis EP, Mendelsohn R, Boskey AL. Infrared Assessment of Bone Quality: A Review. *Clin Orthop Relat Res* (2011) 469(8):2170-8. doi: 10.1007/s11999-010-1751-4
- Nyman JS, Gorochow LE, Adam Horch R, Uppuganti S, Zein-Sabatto A, Manhard MK, et al. Partial Removal of Pore and Loosely Bound Water by Low-Energy Drying Decreases Cortical Bone Toughness in Young and Old Donors. J Mech Behav BioMed Mater (2013) 22:136–45. doi: 10.1016/ j.jmbbm.2012.08.013
- Unal M, Yang S, Akkus O. Molecular Spectroscopic Identification of the Water Compartments in Bone. *Bone* (2014) 67:228–36. doi: 10.1016/ j.bone.2014.07.021
- Samuel J, Sinha D, Zhao JC, Wang X. Water Residing in Small Ultrastructural Spaces Plays a Critical Role in the Mechanical Behavior of Bone. *Bone* (2014) 59:199–206. doi: 10.1016/j.bone.2013.11.018
- Ma YJ, Tadros A, Du J, Chang EY. Quantitative Two-Dimensional Ultrashort Echo Time Magnetization Transfer (2D UTE-MT) Imaging of Cortical Bone. *Magn Reson Med* (2018) 79(4):1941–9. doi: 10.1002/mrm.26846
- Hodgson RJ, Evans R, Wright P, Grainger AJ, O'Connor PJ, Helliwell P, et al. Quantitative Magnetization Transfer Ultrashort Echo Time Imaging of the Achilles Tendon. *Magn Reson Med* (2011) 65(5):1372–6. doi: 10.1002/mrm.22715
- 15. Ma YJ, Chang EY, Bydder GM, Du J. Can Ultrashort-TE (UTE) MRI Sequences on a 3-T Clinical Scanner Detect Signal Directly From Collagen

Protons: Freeze-Dry and D2 O Exchange Studies of Cortical Bone and Achilles Tendon Specimens. *NMR BioMed* (2016) 29(7):912-7. doi: 10.1002/nbm.3547

- Loegering IF, Denning SC, Johnson KM, Liu F, Lee KS, Thelen DG. Ultrashort Echo Time (UTE) Imaging Reveals a Shift in Bound Water That Is Sensitive to Sub-Clinical Tendinopathy in Older Adults. *Skeletal Radiol* (2021) 50(1):107– 13. doi: 10.1007/s00256-020-03538-1
- Ma YJ, Chen Y, Li L, Cai Z, Wei Z, Jerban S, et al. Trabecular Bone Imaging Using a 3D Adiabatic Inversion Recovery Prepared Ultrashort TE Cones Sequence at 3T. *Magn Reson Med* (2020) 83(5):1640–51. doi: 10.1002/mrm.28027
- Du J, Diaz E, Carl M, Bae W, Chung CB, Bydder GM. Ultrashort Echo Time Imaging With Bicomponent Analysis. *Magn Reson Med* (2012) 67(3):645–9. doi: 10.1002/mrm.23047
- Du J, Carl M, Bydder M, Takahashi A, Chung CB, Bydder GM. Qualitative and Quantitative Ultrashort Echo Time (UTE) Imaging of Cortical Bone. J Magn Reson (2010) 207(2):304–11. doi: 10.1016/j.jmr.2010.09.013
- Diaz E, Chung CB, Bae WC, Statum S, Znamirowski R, Bydder GM, et al. Ultrashort Echo Time Spectroscopic Imaging (UTESI): An Efficient Method for Quantifying Bound and Free Water. *NMR BioMed* (2012) 25(1):161–8. doi: 10.1002/nbm.1728
- Biswas R, Bae W, Diaz E, Masuda K, Chung CB, Bydder GM, et al. Ultrashort Echo Time (UTE) Imaging With Bi-Component Analysis: Bound and Free Water Evaluation of Bovine Cortical Bone Subject to Sequential Drying. *Bone* (2012) 50(3):749–55. doi: 10.1016/j.bone.2011.11.029
- Horch RA, Gochberg DF, Nyman JS, Does MD. Clinically Compatible MRI Strategies for Discriminating Bound and Pore Water in Cortical Bone. *Magn Reson Med* (2012) 68(6):1774–84. doi: 10.1002/mrm.24186
- Manhard MK, Horch RA, Harkins KD, Gochberg DF, Nyman JS, Does MD. Validation of Quantitative Bound- and Pore-Water Imaging in Cortical Bone. *Magn Reson Med* (2014) 71(6):2166–71. doi: 10.1002/mrm.24870
- Horch RA, Nyman JS, Gochberg DF, Dortch RD, Does MD. Characterization of 1H NMR Signal in Human Cortical Bone for Magnetic Resonance Imaging. *Magn Reson Med* (2010) 64(3):680–7. doi: 10.1002/mrm.22459
- Horch RA, Gochberg DF, Nyman JS, Does MD. Non-Invasive Predictors of Human Cortical Bone Mechanical Properties: T(2)-Discriminated H NMR Compared With High Resolution X-Ray. *PloS One* (2011) 6(1):e16359. doi: 10.1371/journal.pone.0016359
- Nyman JS, Ni Q, Nicolella DP, Wang X. Measurements of Mobile and Bound Water by Nuclear Magnetic Resonance Correlate With Mechanical Properties of Bone. *Bone* (2008) 42(1):193–9. doi: 10.1016/j.bone.2007.09.049
- Majumdar S. Magnetic Resonance Imaging of Trabecular Bone Structure. Top Magn Reson Imaging (2002) 13(5):323–34. doi: 10.1097/00002142-200210000-00004
- Amstrup AK, Jakobsen NF, Moser E, Sikjaer T, Mosekilde L, Rejnmark L. Association Between Bone Indices Assessed by DXA, HR-pQCT and QCT Scans in Post-Menopausal Women. *J Bone Miner Metab* (2016) 34(6):638–45. doi: 10.1007/s00774-015-0708-9
- Bergot C, Laval-Jeantet AM, Hutchinson K, Dautraix I, Caulin F, Genant HK. A Comparison of Spinal Quantitative Computed Tomography With Dual Energy X-Ray Absorptiometry in European Women With Vertebral and Nonvertebral Fractures. *Calcif Tissue Int* (2001) 68(2):74–82. doi: 10.1007/ bf02678144
- Wehrli FW, Song HK, Saha PK, Wright AC. Quantitative MRI for the Assessment of Bone Structure and Function. NMR BioMed (2006) 19 (7):731-64. doi: 10.1002/nbm.1066
- Marcon M, Keller D, Wurnig MC, Eberhardt C, Weiger M, Eberli D, et al. Separation of Collagen-Bound and Porous Bone Water Transverse Relaxation in Mice: Proposal of a Multi-Step Approach. *NMR BioMed* (2016) 29(7):866– 72. doi: 10.1002/nbm.3533
- Wu Y, Guo Z, Fu X, Wu J, Gao J, Zeng Q, et al. The Study Protocol for the China Health Big Data (China Biobank) Project. *Quant Imaging Med Surg* (2019) 9(6):1095–102. doi: 10.21037/qims.2019.06.16
- Kanis JA. Assessment of Fracture Risk and Its Application to Screening for Postmenopausal Osteoporosis: Synopsis of a WHO Report. WHO Study Group. Osteoporos Int (1994) 4(6):368–81. doi: 10.1007/bf01622200
- Yu H, McKenzie CA, Shimakawa A, Vu AT, Brau AC, Beatty PJ, et al. Multiecho Reconstruction for Simultaneous Water-Fat Decomposition and T2\* Estimation. *J Magn Reson Imaging* (2007) 26(4):1153–61. doi: 10.1002/jmri.21090

- 35. Engelke K, Adams JE, Armbrecht G, Augat P, Bogado CE, Bouxsein ML, et al. Clinical Use of Quantitative Computed Tomography and Peripheral Quantitative Computed Tomography in the Management of Osteoporosis in Adults: The 2007 ISCD Official Positions. J Clin Densitom (2008) 11 (1):123–62. doi: 10.1016/j.jocd.2007.12.010
- 36. Pickhardt PJ, Lee LJ, del Rio AM, Lauder T, Bruce RJ, Summers RM, et al. Simultaneous Screening for Osteoporosis at CT Colonography: Bone Mineral Density Assessment Using MDCT Attenuation Techniques Compared With the DXA Reference Standard. J Bone Miner Res (2011) 26(9):2194–203. doi: 10.1002/jbmr.428
- 37. Seifert AC, Li C, Rajapakse CS, Bashoor-Zadeh M, Bhagat YA, Wright AC, et al. Bone Mineral (31)P and Matrix-Bound Water Densities Measured by Solid-State (31)P and (1)H MRI. NMR BioMed (2014) 27(7):739–48. doi: 10.1002/nbm.3107
- Ritchie RO, Buehler MJ, Hansma P. Plasticity and Toughness in Bone. *Phys Today* (2009) 62(6):41–7. doi: 10.1063/1.3156332
- Jerban S, Lu X, Dorthe EW, Alenezi S, Ma Y, Kakos L, et al. Correlations of Cortical Bone Microstructural and Mechanical Properties With Water Proton Fractions Obtained From Ultrashort Echo Time (UTE) MRI Tricomponent T2\* Model. NMR BioMed (2020) 33(3):e4233. doi: 10.1002/nbm.4233
- Seifert AC, Li C, Wehrli SL, Wehrli FW. A Surrogate Measure of Cortical Bone Matrix Density by Long T2 -Suppressed MRI. J Bone Miner Res (2015) 30 (12):2229–38. doi: 10.1002/jbmr.2580
- Ong HH, Wright AC, Wehrli FW. Deuterium Nuclear Magnetic Resonance Unambiguously Quantifies Pore and Collagen-Bound Water in Cortical Bone. *J Bone Miner Res* (2012) 27(12):2573–81. doi: 10.1002/jbmr.1709
- He J, Fang H, Li X. Vertebral Bone Marrow Fat Content in Normal Adults With Varying Bone Densities at 3T Magnetic Resonance Imaging. *Acta Radiol* (2019) 60(4):509–15. doi: 10.1177/0284185118786073
- Li CJ, Cheng P, Liang MK, Chen YS, Lu Q, Wang JY, et al. MicroRNA-188 Regulates Age-Related Switch Between Osteoblast and Adipocyte Differentiation. J Clin Invest (2015) 125(4):1509–22. doi: 10.1172/jci77716
- Griffith JF, Yeung DK, Tsang PH, Choi KC, Kwok TC, Ahuja AT, et al. Compromised Bone Marrow Perfusion in Osteoporosis. J Bone Miner Res (2008) 23(7):1068–75. doi: 10.1359/jbmr.080233
- 45. Kim H, Taksali SE, Dufour S, Befroy D, Goodman TR, Petersen KF, et al. Comparative MR Study of Hepatic Fat Quantification Using Single-Voxel Proton Spectroscopy, Two-Point Dixon and Three-Point IDEAL. *Magn Reson Med* (2008) 59(3):521–7. doi: 10.1002/mrm.21561
- 46. Aoki T, Yamaguchi S, Kinoshita S, Hayashida Y, Korogi Y. Quantification of Bone Marrow Fat Content Using Iterative Decomposition of Water and Fat With Echo Asymmetry and Least-Squares Estimation (IDEAL): Reproducibility, Site Variation and Correlation With Age and Menopause. Br J Radiol (2016) 89(1065):20150538. doi: 10.1259/bjr.20150538
- Kanis JA, Johnell O, Oden A, Johansson H, McCloskey E. FRAX and the Assessment of Fracture Probability in Men and Women From the UK. Osteoporos Int (2008) 19(4):385–97. doi: 10.1007/s00198-007-0543-5
- Griffith JF, Yeung DK, Antonio GE, Lee FK, Hong AW, Wong SY, et al. Vertebral Bone Mineral Density, Marrow Perfusion, and Fat Content in Healthy Men and Men With Osteoporosis: Dynamic Contrast-Enhanced MR Imaging and MR Spectroscopy. *Radiology* (2005) 236(3):945–51. doi: 10.1148/ radiol.2363041425
- Lustig M, Donoho D, Pauly JM. Sparse MRI: The Application of Compressed Sensing for Rapid MR Imaging. *Magn Reson Med* (2007) 58(6):1182–95. doi: 10.1002/mrm.21391
- Zhu B, Liu JZ, Cauley SF, Rosen BR, Rosen MS. Image Reconstruction by Domain-Transform Manifold Learning. *Nature* (2018) 555(7697):487–92. doi: 10.1038/nature25988

Conflict of Interest: Author Y-TL was employed by GE Healthcare.

The remaining authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

**Publisher's Note:** All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

Copyright © 2022 Liu, Liao, Li, Chen, Feng, Yao, Huang, Su, Lu, Liao, Li and Ma. This is an open-access article distributed under the terms of the Creative Commons

Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.