RESEARCH ARTICLE

Cortical Responsiveness to Nociceptive Stimuli in Patients with Chronic Disorders of Consciousness: Do C-Fiber Laser Evoked Potentials Have a Role?

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Abstract

It has been shown that the presence of Aδ-fiber laser evoked potentials (Aδ-LEP) in patients suffering from chronic disorders of consciousness (DOC), such as vegetative state (VS) and minimally conscious state (MCS), may be the expression of a residual cortical pain arousal. Interestingly, the study of C-fiber LEP (C-LEP) could be useful in the assessment of cortical pain arousal in the DOC individuals who lack of Aδ-LEP. To this end, we enrolled 38 DOC patients following post-anoxic or post-traumatic brain injury, who met the international criteria for VS and MCS diagnosis. Each subject was clinically evaluated, through the coma recovery scale-revised (CRS-R) and the nociceptive coma scale-revised (NCS-R), and electrophysiologically tested by means of a solid-state laser for Aδ-LEP and C-LEP. VS individuals showed increased latencies and reduced amplitudes of both the $A\delta$ -LEP and C-LEP components in comparison to MCS patients. Although nearly all of the patients had both the LEP components, some VS individuals showed only the C-LEP ones. Notably, such patients had a similar NCS-R score to those having both the LEP components. Hence, we could hypothesize that C-LEP generators may be rearranged or partially spared in order to still guarantee cortical pain arousal when Aδ-LEP generators are damaged. Therefore, the residual presence of C-LEP should be assessed when A δ -LEP are missing, since a potential pain experience should be still present in some patients, so to properly initiate, or adapt, the most appropriate pain treatment.

Introduction

In contrast to comatose patients, who lack of both wakefulness and awareness, individuals suffering from Vegetative State (VS) are awake but unaware of the environment and cannot purposefully respond to stimuli, whilst patients affected by Minimally Conscious State (MCS) are awake but limitedly aware and may show some purposeful behaviors [1-2].



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Pain perception in chronic disorder of consciousness (DOC) represents a controversial issue, since there is growing evidence concerning the presence of residual pain experience even in some VS individuals [3–6]. Taking into account that such patients have a strongly limited repertoire of communication, and that the inability to communicate could not exclude a possible pain experience, the issues of nociception and pain in such individuals are of ethic and clinical importance, especially concerning a proper diagnosis and an adequate pain treatment.

Laser evoked potentials (LEP) are extensively used in pain study, since the laser stimulation can selectively activate the nociceptive pathways [7]. Laser stimulation typically evokes several LEP components, reflecting the activity of multiple cortical assemblies within different cortical areas (including primary and secondary somatosensory cortices, insula, and anterior cingulate cortex) that process either nociceptive or non-nociceptive inputs [8–9]. The N1P1 complex reflects an early stage of sensory processing at unaware level, whereas the N2P2 wave is related to the stimulus saliency, independently from the nociceptive nature of the incoming stimulus [8,10–12].

Although the A δ -fiber LEP (A δ -LEP) amplitudes and latencies have been put in relation with the intensity of nociceptive pain [12], it has been shown that LEP depend on non-specific neural pathways within the so-called pain-matrix, so that LEP characteristics cannot be considered as a marker of pain-related cognitive processes [8,13–14], but only a sign of a relevant-stimulus dependent arousal [8–15].

Interestingly, recent LEP studies have shown reliable cortical responses following nociceptive stimuli in VS and MCS individuals [10-11], regardless of the preservation of non-nociceptive somatosensory evoked potentials. Such issues may suggest that "the cortical awareness toward pain stimulus may be a basal function for survival in state of vegetative autonomy, despite the absence of evident motor reaction to nociceptive inputs". Therefore, nociceptive stimuli may be processed even in severe DOC patients [10-11].

Nevertheless, whereas A δ -LEP have been studied in DOC patients [10–11], the assessment of C-fiber LEP (C-LEP) has not been yet performed in DOC individuals. C-LEP have been shown to be generated by C-fiber activation through laser stimuli with specific characteristics, but they probably share common cortical generators with A δ -LEP [16–18].

We hypothesized that the VS patients who lack of $A\delta$ -LEP could show a cortical pain arousal, as demonstrated by C-LEP preservation, and they therefore might experience pain. Therefore, we tested this hypothesis by assessing the presence and the characteristics of C-LEP elicited by means of a solid-state laser device in a sample of DOC patients lacking of $A\delta$ -LEP.

Materials and Methods

The study was conducted in accordance with the Declaration of Helsinki and was approved by Ethic Committee of IRCCS Centro Neurolesi "Bonino-Pulejo" all the HC subjects and the legal guardian of the DOC patients gave written informed consent before any study-related procedures were performed. Moreover, the families of the patients gave written informed consent to publish the potentially identifying case details.

Subjects

We enrolled 38 DOC subjects affected by anoxic or traumatic brain injury, who met the international criteria for VS and MCS diagnosis [1-2]. The exclusion criteria were: cutaneous or systemic disease contraindicating LEP execution; critical conditions (e.g. mechanical ventilation, hemodynamic instability); peripheral nervous system damage; brainstem lesions. As control group, we enrolled 15 healthy age-matched individuals (HC). We summarized the detailed clinic and demographic characteristics of DOC patients in <u>Table 1</u>. All of the patients and the

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age	den	B	242	52						AO-LEP																	
					N1(ms)	ß	~	N1(µV)		SD	N2(ms)		SD	N2(µV)		SD	N1(ms)		SD	N1(µV)	S	SD	N2(ms)	0	SD	N2(µV)	SD
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64	LL.	14	17			130±12 2	1±0.5				172±22 17	170±12	2 11	11±1 1	12±1 0	0.7 213	213±27 22	222±16		3.3±0.5 3.4±	3.4±0.5 0.0	0.03 306:	306±40 314	314±49	5 6.6±1	:1 6±1	0.4
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62		30					~́						2 7.3												4 3.3±0.5		
61		18			131±17 135:	135±13 3	1±0.5	.5 1.1±0.5		0.003 2	200±26 20	201±15	1	17±1 1	14±1	2 209	209±27 22	220±17	8 4.4:	4.4±0.5 4.4	4.4±0.5 0.0	0.04 241±31		244±19	1 1.4±0.5	0.5 3.2±0.5	5 1.3
75		24			114±15 118:		1±0.5	.5 1.2±0.5		0.05 1	159±21 15	152±15 8	5 6.4	6.4±1 6.	6.4±1 0.1	0.001 276	276±36 27	275±17 0	0.5 3.2:	3.2±0.5 3.24	3.2±0.5 0.0	0.02 312±40		302±15	8 4±0.5	5 4±1	0.03
60		32	16				2.2±0.5	0.5 2±0.5			131±17 13	134±19 2	2 7.6	7.6±1 7.	7.7±1 0	0.1 315	315±41 30	309±25	4 3.4:	3.4±0.5 3.45	3.4±0.5 0.0	0.01 275±36		225±15 0	0.5 5.3±1	:1 5.5±1	0.1
57		33			133±17 132:	132±18 1	4.4±0.5	0.5 4.1±0.5		0.1 1	179±23 18	180±13	14	14±2 1	13±1 0	0.7 218	218±28 20	207±17	7 5.8	5.8±0.5 5.7±	5.7±0.5 0.	0.1 347±45		346±20	2 2.2±0.5	0.5 2±0.5	0.1
68		15	16		116±15 119-	119±14 3	2.1±0.5	0.5 2.2±0.5		0.04 1	185±24 18	185±14 0	0.5 10	10±2 1	10±1 0	0.2 227	227±28 23	237±12	7 3.2	3.2±0.5 3.04	3.0±0.5 0.	0.1 278±36		286±49	5 5.3±0.5	0.5 5.1±0.5	5 0.1
59		17			113±15 115:						149±19 14	145±12 (3 4.1				218±28 20	208±12	7 6±	6±0.5 5.4	5.4±0.5 0.	0.5 237±31		227±21	7 3±0.5	5 3.1±0.5	5 0.1
99		29	15		109±14 106:	106±19 2	3.3±0.5		3.1±0.5	0.1 1	185±24 19	191±16 4	4 10	10±1 1	10±1 0	0.4 250	253±33 25	253±14 0	0.5 5.9:	5.9±0.5 5.8±	5.8±0.5 0.0	0.02 255:	255±33 262	262±42	4 2.1±0.5	0.5 2.1±0.5	5 0.1
57					128±17 131:	131±11 2		0.5 2±0.5		0.1 1	188±24 18	188±14 0	0.5 8.2	8.2±1 7.	7.5±1 0	0.5 237	237±31 22	224±19	9 4.3	4.3±0.5 4.3	4.3±0.5 0.0	0.04 324:	324±42 328	328±60	4 4.4±1	:1 4.4±0.5	5 0.02
6709			16±1 7		130±19 131:	131±17 2±	1 2.9±1.8	1.8 2.8±1.8		0.03±0.05 1	178±25 17	179±27 2:	2±2 7.6:	7.6±4.1 7.4	7.4±3.7 0	0.1 235	235±34 23	233±35 4	4±3 4.6:	4.6±1.2 4.5±	4.5±1.2 0.	0.1 290±36		291±40 4	4±2 3±1	1 4±1	0.2±0.
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64		25			170±31 165:	165±11 3	4.1±1	E1 4.1±1			215±39 21	216±10	6	9±2 13	13±0.5	3 314	314±57 31	316±41	2 1±	1±0.5 2.1	2.1±0.5 0.	0.8 410±75		405±44	4 3±1	3.5±0.5	5 0.4
62		19			129±24 125:	125±19 3	2±0.5	.5 4±0.5	0.5	+	179±33 18	189±11	7 6:	6±1 8:	8±0.5	1 44	442±81 34	344±35	2	1±0.5 1.1±	1.1±0.5 0.	0.1 596±109		592±56	3 7±1	1 3±0.5	33
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48		13			156±26 160:	160±10 3	4	4		0.04	NA	NA N	NA N	NA			448±82 44	447±70	1 3		3.2±0.5 0.	0.1 333±61		348±21 1	10 5±1	I 5.4±0.5	5 0.3
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61	Σ			136	136±13 138:	138±10 1		1 12±1	±1	3	165±15 16	166±13	9.	9±1 11	11±0.5	1 234	234±21 23	238±11	5 6:	6±1 5±	5±0.5 1	1 266±21		270±11	3 19±2	2 10±0.5	9
55	Σ			156		159±15 1			Ħ.	-	187±17 28	288±13	12	12±1 11	11±0.5	1 18	182±16 19	191±10	7 6.	6±1 8±	8±0.5 1	1 291±27			2 18±2	2 16±0.5	1
61	Σ			122					R		126±12 12	128±14	14		9±0.5	4 25		254±15	4 4±	4±0.5 6±1	6±0.5 1	1 304±28		309±12	3 12±1	1 19±0.5	5
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	SD	9	4	9	4	e	-	N	-	3±2
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	N2(µV)	16±0.5	11±0.5	8±0.5	6±0.5	15±0.5	10±0.5	11±0.5	11±0.5	13±4
	Ż	8±1	6±1	16±1	11±1	11±1	12±1	8±1	13±1	13±4
	ß	-	-	4	ო	-	-	5	-	2±1
	us)	352±28	355±28	250±14	351±16	252±49	218±12	313±17	252±10	258±85
C-LEP	N2(ms)	350±32	354±32	245±22	355±32	253±20	217±29	317±23	253±23	276±65
Ċ	S	-	0.1	-	4	-	2	-	-	2±4
	\$	5±0.5	9±0.5	7±0.5	9±0.5	6±0.5	3±0.5	4±0.5	6±0.5	7±5
	(VI) HN	7±1	8±1	6±1	3±0.5	4±0.5	6±1	6±1	4±0.6	6±2
	ß	5	-	2	2	9	-	4	9	£±5
	us)	208±10	159±17	168±15	150±17	167±11	181±17	229±17	178±13	177±34
	N1(ms)	201±18	162±15	171±15	147±13	158±14	183±17	227±21	169±15	182±30
	ß	-	0	7	4	4	Ħ	7	15	4±4
	ŗ)	12±0.5	9±0.5	28±0.5	13±0.5	19±0.5	28±0.5	21±0.5	33±0.5	16±8
	N2(μV)	30±3	12±1	18±2	29±3	23±2	33±3	11±1	21±2	17±8
	ß	e	-	4	0	4	e	4	0.5	3±2
	ls)	168±17	177±13	163±17	205±16	159±17	210±15	181±17	167±17	176±35
۵.	N2(ms)	164±15	176±16	168±15	202±18	152±14	206±19	187±17	167±15	178±30
Að-LEP	ß	-	÷	-	÷	0	÷	ю	÷	2±1
	ľ,	8±1	10±1	10±1	8±1	9±1	9±1	6±1	10±1	9±2
	VI) IN	10±1	8±1	9±1	9±1	6±1	10±1	10±1	9±1	9±2
	8	-	e	7	0.5	0.5	-	0.5	-	5±5
	(su	150±12 152±15	126±15	119±17	132±17	119±16	160±17	143±12	133±17	137±14
	N1(ms)	150±12	130±15	110±10	131±12	119±10	162±15	143±13	134±12	132±16
NCS										
CRS										
pp										
gen		L	ш	ш	ш	Σ	ш	Σ	ш	
age		63	55	56	65	56	59	55	65	60±4
et										

Legend: A: post-anoxic brain-injury; age in years; CRS-R: coma recovery scale-revised; dd: disease duration in months; et: etiology; gen: gender; MCS: minimally conscious state; NCS-R: nociception coma scale-revised; sd: standard deviation; T: post-traumatic brain-injury; VS: vegetative state.

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HC had previously performed an A δ -LEP study, according to the standard procedures of Cruccu and coworkers [19–20].

Clinical assessment

DOC individuals (23 VS and 15 MCS) were clinically evaluated by two neurologists, skilled in DOC diagnosis, through the JFK Coma Recovery Scale-Revised (CRS-R). This scale is a reliable and standardized tool, which integrates neuropsychological and clinical assessment, and includes the current diagnostic criteria for coma, VS and MCS, allowing the clinician to assign the patient to the most appropriate diagnostic category. Thus, the CRS-R is considered as an appropriate measure for characterizing level of consciousness and for monitoring neurobehavioral function recovery [21].

Pain perception was specifically evaluated by means of the Nociception Coma Scale-Revised (NCS-R) [22] that has been developed for assessing pain in severely brain-injured patients, and allows a better specification of the conscious behavioral patterns linked to pain experience in MCS and VS. This tool consists in the observation of motor, verbal, and facial responses to painful stimulation. The total score ranges from zero to 9. A cut-off of 4 has been proposed to suggest an aware pain perception.

Laser stimulation set-up

LEP were recorded at bed and over a reclining armchair in a quiet and mild-lighted room in DOC patients and HC individuals, respectively. All measures concerning laser-safety were observed (protective goggles, earplugs). Aδ-LEP were previously recorded in either HC or DOC patients. We used a Neodymium:Yttrium-Aluminium-Perovskite laser (Nd:YAP) (wavelength 1.34µm, pulse duration 2-20ms, maximum energy 7J, 4mm beam diameter) with fiberoptic guidance (Electronic Engineering, Florence, Italy). A red helium-neon (He-Ne) laser, confocal with the infrared beam, was used to visually indicate the irradiated skin area of the right trigeminal maxillary branch region, close to the nasus-genius sulcus. In each individual, we employed a laser stimulation intensity of 60-80mJ/mm² that induced a Visual Analogic Score of at least 4/10 in the HC. Such intensity produced clear and stable evoked components in all of the HC individuals, and was therefore used throughout the entire experimental procedure. The mean stimulation intensity employed in HC individuals was used to evoke LEP in the DOC sample. We delivered two trains of 30 laser pulses, with a 5-minute inter-train interval. In order to avoid habituation phenomena and skin overheating and damage, the delivery frequency was 0.1±0.025Hz and the stimulator, whose handle was held perpendicularly to skin surface, was slightly shifted over the skin. During the stimulation, HC did not perform any mental task (neutral condition) [16], whereas DOC patients practiced the CRS-R arousal protocol [23] before the LEP session.

In order to record C-LEP, the laser stimulation was carried out according to Bragard and co-workers protocol [24] that obtained the direct isolation of C-LEP from tiny cutaneous surfaces by means of a CO_2 laser. The laser stimuli (wavelength 1.34µm, pulse duration 10ms, 4mm beam diameter) were directed to the skin area of the right trigeminal maxillary branch region, close to the nasus-genius sulcus, but a thin aluminium disk, drilled with calibrated holes (~0.15mm²) was interposed just above the skin surface [24]. Stimulus intensity was individually adapted in the HC individuals, so that sensations reported ranged from "barely detectable" to "slight pain". Such intensity produced clear and stable evoked components in all of the HC individuals, and was, therefore, used throughout the entire experimental procedure. The mean stimulation intensity applied in HC individuals was employed to evoke C-LEP in the DOC sample.

LEP recording

LEP were recorded from three Ag-AgCl scalp-surface electrodes (put on Fp2, Cz, and T3). The reference electrode was put on the nose and the ground on Fpz. Eye movements and blinks were monitored by an electrode above the right eyebrow. Electrode impedance was kept $\leq 5 k \Omega$. The time-analysis was set at 2s, with a pre-analysis period of 100ms. Signals were filtered at 0.3-70Hz, sampled at 250Hz through a Synergy-Medelec System (Tecnomed, Pescara, Italy), and stored on a PC for off-line analysis. Trials contaminated by ocular or muscle artifacts were automatically excluded from the analysis through an artifact-rejection system that excluded all runs containing transient signals exceeding ±65µV in any recording channel (including the electrooculogram) from the average. In the HC group, we identified three LEP components, defined in terms of estimated topography and latency values, i.e the N2P2 (Cz-nose), the N1 (T3-nose), and the P1 (Fp2-nose). The time-windows were determined after having analyzed the grandaverage of all the LEP, and then applied in each individual analysis. Thus, we measured the baseline-peak amplitude (μ V) of N1 and N2 waves, and the latency (ms) of N2 and N1 (in addition, we calculated the N1P1 by computing an offline bipolar montage T3-Fp2, where phase reversal is evident) [17,25], in either the single runs or the average of the two runs. Latencies were determined by using a modified box-plot method known as the median rule [26].

Statistical analysis

Latencies and amplitudes of the LEP components were analyzed at their scalp sites through a one-way analysis of variance (ANOVA), with *group* (three levels: HC, VS, and MCS) as between-subject factor. Cases without LEP were labeled as missing data. The Greenhouse-Geisser method was used if necessary to correct the degrees of freedom [27]. A p-value <0.05 after correction was accepted as statistically significant. Conditional on a significant F-value, *posthoc* analysis (Tukey's honestly significant difference -THSD) was performed to explore the strength of the main effects and the patterns of interaction between experimental factors. All data are given as means± standard deviation (SD). We also calculated a two-tailed bivariate Pearson's correlation coefficient between the clinical (CRS-R and NCS-R) and electrophysiological parameters (latencies and amplitudes of A δ -LEP and C-LEP components).

Results

We did not report any side effects during and after the stimulation protocol. In Table 1, we summarize the single-subject values of LEP latencies and amplitudes in the two runs of laser stimulation, the standard deviation of LEP amplitude and latencies between the two laser stimulation runs for each subject, the group values of LEP latencies and amplitudes, and the clinical and demographic characteristics of HC and DOC patients. In Fig 1, we reported the two averaged waveforms at each electrode in the two groups of DOC patients, concerning either A δ -LEP or C-LEP.

The A δ -LEP stimulation set up induced both the N1P1 and N2P2 components, as well as the C-LEP paradigm produced the ultra-late LEP waves. Either the HC or the DOC patients showed reliable evoked responses, since the LEP waveforms were track-by-track stable within each laser stimulation run, and the two consecutive averaged waveforms were almost superimposable at either individual or group level (Fig 1). Similarly, the individual LEP values showed a run-by-run low variability (i.e. no more than 3 times the mean run-by-run SD) (Table 1).

All of the participants showed the N1P1 component of both A δ -LEP and C-LEP. All of the HC and the MCS patients showed the A δ -LEP N2P2 component, whereas this was missing in 13 VS individuals (Table 1). Interestingly, six out of these patients showed the C-LEP N2P2 component. Hence, the VS individuals showed three distinct N2P2 LEP patterns: i) both the



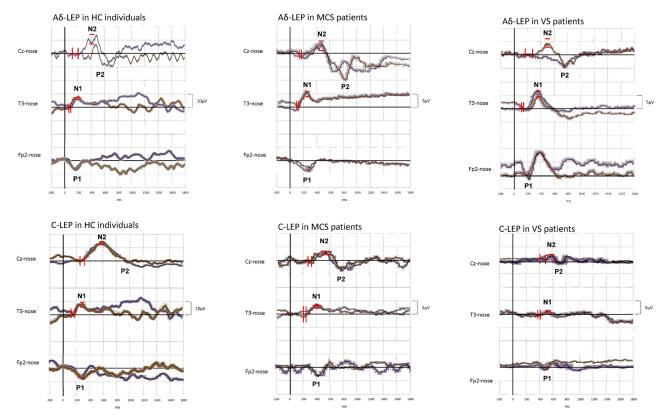


Fig 1. Shows the grand averages in the time-domain (the two thick waveforms represent the two pulse-train–runs, the shady areas express the inter-subject variability) of A δ -LEP and C-LEP at electrode Cz (N2P2), T3 (N1) and Fp2 (P1). Amplitude negative values are plotted up. The vertical and horizontal black lines indicate the time point of the laser stimulation and the zero line, respectively. The vertical and horizontal red bars refer to the standard deviation concerning LEP latency and amplitude, respectively.

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A δ -LEP N2P2 and C-LEP (10 individuals); ii) only the C-LEP N2P2 (6 individuals); and iii) neither the A δ -LEP N2P2 nor the C-LEP N2P2 (7 individuals). Notably, none of the patients showed the A δ -LEP N2P2 without the C-LEP N2P2.

We found higher LEP amplitudes and less delayed LEP latencies in HC than DOC patients. On the other hand, LEP latencies were significantly higher in VS than MCS individuals, whereas LEP amplitudes were almost superimposable. The statistically significant inter-group differences are summarized in <u>Table 2</u>. The other parameters (age, disease duration, etiology, and gender) were not significantly different among the three groups, and the LEP parameters did not correlate with the clinical scale scores.

Discussion

To the best of our knowledge, this is the first study investigating C-LEP in DOC patients. Our findings agree with previous reports showing an increased latency of A δ -LEP in DOC patients (more in VS than MCS individuals) without any significant amplitude inter-group difference [10–11]. The preservation of N2P2 A δ -LEP may suggest a residual nociceptive cortical processing in severe brain-injured patients, even when other sensory evoked potentials are missing [10–11]. Therefore, a potential pain experience should be taken into account in such patients.

It is worthy to note that it is not so easy to record C-LEP, as reported by the international guidelines $[\underline{28}-\underline{29}]$. Therefore, a first critical question is whether the evoked responses we obtained may or not reliably represent C-LEP. Indeed, there are two main problems in C-LEP

	one-way	ANOVA		post-hoc THSD	
	F _(2,100)	р	HC/MCS	HC/VS	MCS/VS
		Aδ-L	EP		
N1 latency	4.9	0.01	NS	0.02	0.01
N1 amplitude	75	<0.001	<0.001	<0.001	NS
N2 latency	3.9	0.03	NS	0.02	0.01
N2 amplitude	11	<0.001	<0.001	0.003	NS
		C-LI	EP		
N1 latency	67	<0.001	0.01	<0.001	<0.001
N1 amplitude	19	<0.001	0.001	<0.001	0.002
N2 latency	29	<0.001	NS	<0.001	<0.001
N2 amplitude	42	<0.001	<0.001	<0.001	NS

Table 2. Resumes the one-way ANOVA findings (group effect) and the post-hoc THSD data concerning LEP parameters. NS stands for non-significant.

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recording: i) the preceding A δ -LEP may hinder the following C-LEP; and ii) the extremely low range of conduction speed of the unmyelinated fibers limits the necessary synchronization of the input to produce a clear signal from the scalp (in fact, C-LEP have been mainly investigated in facial territories). There are two main methods to record C-LEP: i) Bragard et al. [24] and Opsommer et al. [30] employed a laser beam passing through a grid with micro-spots, without any substantial A δ -LEP interference; and ii) Iannetti et al. [13] and Cruccu et al. [31] used very large and low-energy laser beams, directly focused on skin, thus stimulating warmth receptors of the skin overlying the spine.

We used the Bragard's approach (i.e. the micro-spot technique) [24], since mechano/heatsensitive A-fiber nociceptors (AMHs) are less numerous than mechano/heat-sensitive C-fiber nociceptors (CMHs), and therefore the micro-spot technique reduces the probability of activating AMHs. Instead, the large-beam and low-intensity method [13,31] allows a selective activation of the warmth C-fiber receptors, which have a lower threshold than AMHs and CMHs. Nevertheless, AMHs are more sparse on face but have larger receptive fields than CMHs and warmth C-fiber receptors. Hence, the probability of activating AMHs could be the same with or without the spatial restriction provided by the grid [32]. However, in the present study we used a solid-state laser, which has well-known different properties in comparison to the gas one, with the former showing a shorter wavelength and a deeper penetration power [14,33]. Instead, gas laser has a greater energy dissipation [34–35] when has to activate the deep nociceptors (i.e. at the dermo-epidermal junction, approximately 100–500µm). Moreover, the short pulse duration of solid-state laser reduces the time for CMHs activation and generates a more synchronous afferent volley [36], leading to more synchronized brain evoked potentials [37]. In addition, AMHs in glabrous skin respond with a long latency of several seconds to sustained heat stimulus and can be sensitized dramatically, whereas CMHs innervating glabrous skin do not share these properties [38-39]. Hence, there is a bulk of data attesting to the suitability of solid-state lasers in activating CMHs [31,40].

In our study, we at first registered C-LEP in HC individuals, identifying clear and stable LEP components, with a significantly low intra-subject and inter-subject variability. In addition, the two averaged trains of stimuli were overimposable. In DOC patients, the evoked responses were more delayed in latency and smaller in amplitude in comparison to HC, but they still showed a low intra-subject variability, and a similar inter-train superimposability. Therefore, taking into account the aforementioned methodological discussion, we believe that

the responses we obtained reliably expressed the C-LEP. Moreover, although several hundred stimuli were necessary in order to record C-LEP in a previous study [24], we could use a smaller number of laser stimuli because of differences in our methodology, including the laser type employed (solid-state vs. gas) and the site of stimulation (face vs. hand).

Notably, 13 VS patients did not show any A δ -LEP N2P2 response, whereas previous studies reported a high-level of A δ -LEP preservation [10–11]. Such discrepancy between our findings and de Tommaso's data [10–11] may depend on either the larger sample we studied, or the aforementioned methodological issues.

By a quantitative point of view, C-LEP latencies were significantly higher in the VS than the MCS individuals, whereas there were no significant inter-group differences concerning C-LEP N2P2 amplitude. Nonetheless, our LEP patterns did not significantly correlate with the clinical assessment, without any relation between pain arousal and the awareness level, according to previous works [10–11]. Moreover, some VS patients showed very small LEP amplitude, even for the C-LEP amplitude range. This may depend on the variability of P2 waveforms we observed, which could have somehow influenced the baseline-peak amplitude values of N2 waves.

Interestingly, six out of the 13 VS patients lacking of Aδ-LEP N2P2 component showed clear C-LEP N2P2 waves. Moreover, such patients had a clinical picture, NCS-R and CRS-R score, similar to the VS patients showing both the A δ -LEP and C-LEP N2P2 components. Hence, we may argue that the cortical arousal towards nociceptive stimuli could be guaranteed in those patients lacking of $A\delta$ -LEP by a reshuffle or a residual preservation of cortical C-LEP generators. In our opinion, such findings raise an important question concerning the functional role of the C-LEP generators, since we did not observe any patients showing only Aδ-LEP N2P2 without C-LEP N2P2 waves. Although previous source analysis studies have shown that Aδ-LEP and C-LEP cortical generators may share similar circuits (even if related to different A δ /C-fiber activation) [9], they independently process (either in series or in parallel) [31] some features of the afferent inputs (e.g. abrupt vs. slow-changing stimuli) [41]. Taking into account the functional differentiation of LEP generators, a substitute role of C-LEP N2P2 generators could be due to an over-activation of the slow-conducting medial pain-system (that oversees the nociceptive-related reflexive and affective responses) [41-42], which in turn depends on a brain injury-induced limbic and subcortical hyperconnectivity [43]. In addition, a selective modulation of the regional cortical excitability, an enlargement of the receptive fields, and the effects of cortical deafferentation could be taken into account in an attempt to explain a C-LEP generator preservation or reorganization [44-47]. Moreover, we could speculate about a strong C-LEP network stability in reason of an older phylogenetic origin [48], and a functional switch to a fixed "in-parallel" or "in-series" processing of nociceptive inputs [49].

The main limitations in our study are to be considered the small number of EEG channels we employed (since we were not able to use a full-EEG cap), and the non-homogeneous gender and age matching of our sample.

In conclusion, our work suggests that DOC patients may somehow show a residual cortical responsiveness to nociceptive stimuli. Indeed, C-LEP preservation could indicate the presence of a residual pain arousal even in the VS patients who do not show A δ -LEP. Therefore, a possible pain experience should be carefully assessed in each VS patient so to properly initiate, or adapt, the most appropriate treatment.

Author Contributions

Conceived and designed the experiments: AN MR RSC. Performed the experiments: AN MR AL CR PP. Analyzed the data: AN. Contributed reagents/materials/analysis tools: CR PP AL PB. Wrote the paper: AN RSC PB.

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