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Original Article

The impact of walking speed on interlimb coordination in individuals with Parkinson's disease

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Abstract. [Purpose] Interlimb coordination can be affected by the symptoms associated with Parkinson's disease and may result in an increased risk of falls. The purpose of the current study was to compare changes in interlimb coordination in individuals with Parkinson's disease to healthy older adults while systematically manipulating walking speed. [Subjects and Methods] Participants walked on a treadmill while systematically increasing and decreasing the walking speed between 0.22 and 1.30 m/s. Kinematic data were collected by means of a three dimensional motion capture system. Dependent variables included the phase relation between arm and leg movements as well as between pelvic and thoracic rotation. [Results] Compared to healthy controls, an increased variability in relative phase between left and right arm swing, and smaller amplitude with arm, leg as well as less variability for the phase relation between thoracic and pelvic rotations were shown in individuals with Parkinson's disease. [Conclusion] The increased variability of phase relation between left and right arm swing may be related to the reduced out-of-phase forcing of the arm movements at the shoulders as a result of axial rigidity in Parkinson's disease. It deserves further investigation whether the improvement of the coordination between arms could result in the normalization of parkinsonian gait.

Key words: Coordination, Variability, Parkinson's disease

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INTRODUCTION

Limitations in walking ability can be observed in individuals with advanced Parkinson's disease (PD), and can eventually lead to serious consequences such as falls, fear of falling, and loss of independence^{1,2)}. Individuals with PD display a reduced range of phase relations between transverse pelvic and thoracic rotations accompanied by a smaller standard deviation of the relative phase compared to healthy subjects, indicating reduced flexibility and variability in trunk coordination^{3,4)}. These coordination changes have been shown to be associated with the presence of axial rigidity demonstrating a relationship between neurological symptoms and coordination patterns during gait³⁻⁵).

Interlimb coordination is essential for stable, smooth and economical walking⁶⁻⁹⁾. Studies examining the impact of PD on coordination of walking have found that the coordination between limb movements may be disrupted^{10–13}). Although the underlying mechanism remains unclear, the impaired interlimb coordination during walking was found to correlate with clinical symptoms (i.e. rigidity and bradykinesia), lower subscores in posture and gait on the United Parkinson's Disease Rating Scale, and also the severity of the degeneration of the dopaminergic system^{12, 13}. However, a key limitation of previous studies on parkinsonian gait is that subjects were instructed to walk at their comfortable walking speed which is known to

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be slower compared to healthy older adults. Walking speed has been shown to significantly alter movement kinematics and the coordination of trunk and limb movements—in the absence of any disease condition^{9, 14, 15)}. It is possible that the slower comfortable walking speed may account for the changes of interlimb coordination observed in PD.

The purpose of the current study is to compare changes of interlimb coordination in individuals with PD and in healthy older adults while systematically manipulating walking speed to determine the impact of PD symptoms on interlimb coordination while controlling for the effects of walking velocity.

SUBJECTS AND METHODS

Twenty-four PD and 26 healthy control subjects (HC) participated in the present study. The mean age and the ratio of number of females and males are significantly lower in PD than HC (Table 1). Individuals diagnosed with typical, idiopathic PD were recruited from the Department of Neurology at Boston Medical Center and from local support groups in the Boston area. Individuals with PD were part of a randomized clinical study¹⁶, and the inclusion criteria were: (1) stable medication usage; (2) early to moderate stage of the disease (Hoehn and Yahr stage II or III (Table 2)); (3) a rigidity score of at least 1 point for one of the extremity sub-items of the Unified Parkinson's Disease Rating Scale (UPDRS); (4) ability to walk independently; (5) age 35 to 75 years; (6) no severe cognitive impairments (Mini-Mental State Examination score \geq 24); and (7) no other severe neurologic, cardiopulmonary or orthopedic disorders. HC were screened via a medical history questionnaire and free from any significant history of cardiopulmonary, musculoskeletal, somatosensory, or neurological disorders. The study was approved by the Institutional Review Board at Boston University, and all participants provided written informed consent.

Participants were instructed to walk comfortably on a treadmill with computer-controlled speed, without holding the handrails. Standby supervision was provided to ensure safety. During the experiment, the speed of the belt was gradually increased from 0.22 m/s to 1.30 m/s, in increments of 0.22 m/s, and then decreased in similar steps to 0.22 m/s. Each speed condition was maintained for about 1 minute, and movements of body segments were recorded for 30 seconds.

Three dimensional (3D) kinematic data were collected using an Optotrak 3020 system (Northern Digital Inc., Waterloo, ON, Canada). Infrared light emitting diodes (IREDs) were placed bilaterally on the following bony landmarks: foot (fifth metatarsal head), heel (calcaneus), ankle (lateral malleolus), knee (lateral femoral condyle), hip (greater trochanter), thigh (one third of the distance between knee and hip IRED), wrist (radial styloid process), elbow (lateral epicondyle), shoulder (acromion process), and head (zygomatic arch). Additionally, four IREDs were attached to the ends of two T-bars, which were mounted on harnesses and fixated around the hip and thorax to record pelvic and thoracic rotations in the transverse plane. The instantaneous positions of each IRED were sampled at a rate of 100 Hz, and were stored on a PC for further off-line processing.

Leg swing angle in the sagittal plane was determined by the orientation angle between the projection of line of gravity and long axis of the leg defined by the hip and ankle marker. Arm swing in the sagittal plane was determined in a similar manner as leg swing mentioned above. The long axis of arm was defined by the shoulder and wrist marker. Transverse thoracic and pelvic rotation was obtained by calculating the orientation angle between the line of two markers fixed on the thoracic and pelvic T-bar and the axis of absolute Cartesian coordinate signifying mediolateral direction, respectively.

Point estimate of relative phase (PERP) between body segments was calculated by using the moment (t_{limbx} and t_{limby}) at which the positive maxima were reached for the angle of each body segment with the following equation¹⁷):

$$\theta(i) = \frac{\text{tlimby}(i) - \text{tlimbx}(i)}{\text{tlimbx}(i+1) - \text{tlimbx}(i)}$$

where t_{limby} and t_{limbx} represent (1) right arm and left arm (Θ RALA), (2) left leg and left arm (Θ LALL), (3) right leg and right arm (Θ RARL), (4) right leg and left leg (Θ RLLL), and (5) pelvis and thorax (Θ PT). The mean and SD of PERP were calculated by means of circular statistics¹⁸.

All statistical analyses were carried out with version 15.0 of SPSS statistical software package (SPSS, Inc. Chicago, IL, USA). The difference in age and gender between groups was examined by means of a Mann-Whitney U test and a χ^2 test, respectively. An ANOVA with repeated measures was performed for all dependent variables. If a significant interaction was found, post-hoc t-tests were performed. Due to significant differences in age and gender between PD and HC, both factors were included in the analyses of variance as covariates. The level of significance was set at 0.05.

RESULTS

Table 2 presents the outcomes and statistics (F- and p-values) for all dependent variables.

A significant main effect of Age for mean Θ_{LALL} , F(1,45)=8.95, p<0.01, indicates that older participants had larger mean Θ_{LALL} than younger participants. An interaction between Group and Speed was obtained for SD of Θ_{RALA} . The variability of Θ_{RALA} decreased with the increasing speed, and was larger in PD than HC at all speeds with the exception of the slowest speed (p<0.05) (Table 3). A significant main effect of Gender for SD of Θ_{RLLL} , F(1,45)=4.55, p=0.04, indicates that SD of

	PD	НС
Number	24	26
Age (years, range)*	$62.2 \pm 9.7 (37 - 75)$	$72.3 \pm 5.6 \ (63 - 84)$
Gender (male/female)*	20/4	14/12
Hoehn and Yahr score		
2	16	NA
2.5	2	NA
3	6	NA
* .0.07		

Table 1. General characteristics of the individuals with Parkinson's disease (PD) and healthy controls subjects (HC)

*p<	0	05	
‴n<		115	

Table 3. Standard deviation (SD) for relative phase (RP)		
between left and right arm swing (degree) with		
increasing speed (meter per second) in individu-		
als with Parkinson's disease (PD) and healthy		
control subjects (HC)		

Speed (m/s)	PD	HC
1	32.9 ± 17.9	41.9 ± 22.9
2	$29.0\pm17.4*$	19.6 ± 14.0
3	$26.5 \pm 15.3*$	17.2 ± 14.7
4	$21.9\pm16.0*$	10.2 ± 7.7
5	$19.7 \pm 12.1*$	8.6 ± 6.7
6	$13.9\pm10.6^{*}$	6.0 ± 2.5
*p<0.05.		

 Table 2. Main and interaction effects of Speed (S), and

 Group (G) for the means and standard deviation

 (SD) of arm and leg swing and trunk rotation

	Speed (S)	Group (G)	S*G
	F	F	F
$\Theta_{RALA*\S}$	26.27	6.60	0.35
$\mathrm{SD}\Theta_{RALA^*\S}$	47.68	12.26	1.44
⊖ _{RLLL*§}	13.34	11.34	0.91
$SD\Theta_{RLLL^* \mathbb{Q}}$	53.41	0.34	3.75
⊖ _{LALL*§} ♀	29.56	4.58	2.83
$\mathrm{SD}\Theta_{\mathrm{LALL}^*}$	16.26	0.74	0.97
Θ_{RARL^*}	20.31	0.45	2.14
$\mathrm{SD}\Theta_{RARL^*}$	23.61	2.11	0.86
$\Theta_{PT^*\S^{\bigcirc}_{+}}$	54.08	29.70	6.03
$SD \Theta_{PT^*\S^{\bigcirc}}$	3.38	5.42	3.0
F 1 1 1	1 1 1	1 0.1	1 0 .

F and p indicate the F and p values of the analyses of variance. RALA: right arm and left arm; RLLL: right leg and left leg; LALL: left arm and left leg; RARL: right arm and right leg; PT: pelvis and thorax. *Significant main effect of Speed, §Significant main effect of Group, ♀Significant interaction effect between Speed and Group.

 Θ_{RLLL} was larger in males than females.

An interaction between Group and Speed was observed for mean ΘP_T . The mean ΘP_T increased with speed for both groups with larger values in HC than PD at all speeds (p<0.03), and the difference between groups increased with speed.

A significant main effect of Age for SD of Θ_{PT} , F(1,43)=9.26, p<0.01, indicates that SD of Θ_{PT} was larger in elderly participants than younger participants.

DISCUSSION

Walking speed is an important control parameter for coordination of walking and can be used as a basis for the evaluation of normal and pathological gait. The main purpose of the present study was to control the effects of walking speed to examine the impact of PD on the flexibility and stability of the coordination of arm and leg movements in persons with PD.

Our study extends the previous findings by showing that the variability of coordination between arms was significantly larger in PD compared to healthy adults while controlling for the walking speed. This suggests that PD symptoms, and not slow walking velocity, contributes to the impaired interlimb coordination between the arms. On the other hand, the lack of group difference for the coordination between left and right leg movements and between ipsilateral arm and leg movements may be due the pacing or cueing effect of the treadmill¹⁹.

The increased variability in relative phase between left and right arm movements in individuals with PD compared to the healthy subjects indicates that right and left arm in PD reached their peak rotation angles at variable moments in the stride cycle. This finding also suggests that not only the coordination of the individual arm swings but also the coordination between left and right arm swing is affected. The increased variability in the coordination of left and right arm movements during walking may be explained by the smaller transverse thoracic rotation, which reduces the out-of-phase forcing of the arm movements at the shoulder joints²⁰. It is hypothesized that the reduced out-of-phase forcing at the shoulder joints will result in a weaker out-of-phase coupling between the left and right arm movements during walking has been demonstrated from the studies investigating the effect of restricting arm swing during walking in which decreased joint angle, stride length and walking speed and increased stride frequency and energy expenditure were reported while walking without arm swing^{21, 22)}. The increased variability of gait parameters such as stride and swing time has been associated with an increased risk of fall in individuals with PD^{11, 23)}. Hence, our findings of an increased variability of coordination between arms suggest that the normalization of coordination between arms should be incorporated into the rehabilitation plan to improve the parkinsonian gait.

The present study has several limitations. As mentioned above, the cueing effect of treadmill may contribute to the reduced group differences in interlimb coordination²⁴. Moreover, all participants in the present study were able to walk at the highest walking speed, and therefore had a high functional status. The generalizability of the results in the present study to individuals with PD with more severe neurological symptoms and lower functional status as well as with different dominant symptoms may be limited²⁵.

The results of present study reveals altered coordination dynamics during walking in PD at a variety of walking velocities. The application of force driven pendulum models combined with EMG recordings may provide us with more accurate estimation of stiffness and interlimb coupling strength in parkinsonian gait²⁶. In addition, future study should include individuals with PD at different disease stages to obtain a better understanding of the progress of the disease and its effects on the gait dynamics. In summary, individuals with PD display an increased variability in relative phase between arm movements in comparison to older adults which coincides with decreased amplitude in arm and leg movements, and transverse thoracic, pelvic, and trunk rotations.

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Conflict of interest

None of the authors reports a conflict of interest.

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