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Data Article

EEG/EOG/EMG data from a cross sectional study on psychophysiological insomnia and normal sleep subjects



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ABSTRACT

The data presented here had been originally collected for a research project entitled 'Sleep EEG spectral analysis in psychophysiological insomnia and normal sleep subjects'. This article describes the data of 11 subjects, referred to Sleep Disorders Research Center (SDRC) in Kermanshah, Iran. The data includes 14 EEG, 6 EOG, and 3 EMG channels, with a sampling ratio of 256 Hz. It includes power spectral features in segments of 30 s for each channel, and nonlinear analysis parameter. Also, the complete demographic and polysomnography specifications are attached.

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Specifications Table

Subject area	Neuroscience, Neurobiology
More specific sub-	Psychiatry, sleep, psychophysiological insomnia
ject area	
Type of data	Table, text file, m-file, mat file,
How data was	Polysomnography, Matlab software
acquired	
Data format	Filtered, analyzed,

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Experimental	Sleep questionnaire were used for subjective features. Age, gender, height,
factors	weight, education, marriage, and body mass index were used as covariates.
Experimental	Power spectrum includes delta, theta, alpha and beta bands. Parameters from
features	nonlinear analysis (Poincare's map and standard descriptors).
Data source	Samples were collected in the Sleep Disorders Research Center in Kermanshah
location	University of Medical Science.
Data accessibility	The dataset is freely available at [1] for any academic, educational, and research
	purposes.
	http://dx.doi.org/10.17632/3hx58k232n.4

Value of the data

- The raw data could be processed using algorithms and other procedures during future researches.
- The data represents 8 h of sleep signals (EEG, EOG, and EMG) from 22 subjects; including 11 psychophysiological insomniacs and 11 normal subjects.
- Psychophysiological insomnia is a more prevalent sleep disorder, which leads to clinically significant impairment in social, occupational, and cognitive functions.
- The data can also be used to assess the EEG Sleep Pattern in psychophysiological insomnia patients as well as good sleepers.
- The diagnosis was performed by a sleep clinician, based on subjective and objective sleep features.

1. Experimental design, materials and methods

1.1. Participant

A total of 22 subjects that includes 8 males (36.36%) and 14 females (63.64%) aged between 18 and 63 years (43.2 ± 14.2) were recruited for participation. Out of the participators, 11 patients were suffering from psychophysiological insomnia (18.18% male; age: 44 ± 13.2 years; Body Mass Index (BMI): 26.6 ± 3.7 kg m⁻²) and 11 subjects had normal sleep pattern (54.5% male; age: 42.4 ± 15.4 years; BMI: 27.53 ± 4.24 kg m⁻²).

The patients were selected from people referred to SDRC, due to insomnia complaints. Normal sleep subjects were recruited from the general population. A detailed written consent was obtained from all participants. Both patients and normal subjects completed their demographic and medical history checklists, including substance and alcohol check as well as psychiatric disorders. For selection of normal subjects, candidates had to first complete the Pittsburgh questionnaire. Preliminary selection was done based on these results. Then, they were further tested using Polysomnography. Finally, subjects who cleared the PSG test round, were selected.

1.2. Procedure

All subjects underwent a one-night polysomnography (PSG) test with the help of SOMNOscreen device called SOMNOscreen[™] plus PSG produced by SOMNOmedics GmbH, Germany. The duration of the test was 8 h (23:00–07:00 h), as per standard protocol at SDRC of KUMS, Iran. A day before appointment, the subjects were invited to sleep in the laboratory of SDRC. They were advised against consuming any tea, coffee, heavy diet or cigarette. Sleeping during the day was also prohibited. Upon arriving at the laboratory, the height and weight of the subject was measured by an experienced personnel. Next, the subjects and participants completed the Pittsburgh questionnaire followed by a detailed briefing on PSG procedures. The measurement of PSG was based on the American Academy of Sleep Medicine guidelines. The polysomnography room was cleaned from artefacts like auditory and visual noises, based on standards [1].

24 recording electrodes were prepared, including 14 electroencephalogram channels (C4A1, C3A2, F3, F4, C3, C4, A1, A2, O1, O2, F3A2, F4A1, O1A2, O2A1), 6 electrooculogram channels (EOG1, EOG2,



Fig. 1. Electrode montage corresponding to the international 10–20: Sites included frontal (F3, F4), central (C3, C4), and occipital (01, 02) placements of the International 10–20 System.

EOG1A1, EOG2A1, EOG1A2, EOG2A2), 3 electromyogram channels (EMG, EMG1, EMG2), and ECG channel. All the recordings were sampled at the rate of 256 Hz. EEG was recorded using Ag/AgCl electrodes, as per the International 10–20 System of Electrode Placement, as shown in Fig. 1. Recorded EEG signals is also shown in Fig. 2.

Both psychophysiological insomnia and normal sleep were determined after clinical interview and careful study of the data obtained from PSG test by an experienced psychiatrist, trained in sleep medicine and PSG. Subjective information was obtained from clinical interview using Pittsburgh Sleep Quality Index (PQSL) [2,3].

All raw datasets were stored in the European Data Format (EDF) format, one file per subject. For example, the file 'Normal_Subject_xx', contains the raw data from normal subject number 'xx'. Similarly, for a patient suffering from psychophysiological insomnia, the file would be 'Raw_-Signal_Psychophysiological_ Insomnia_xx'. Description of all participants were recorded in 'PSG_Psycho_Normal.xlsx'. The outputs from polysomnography were collected at 'PSG_Outputs.rar'. Data file names and their descriptions are listed in Table 1.

Two files, namely PSD_Normal_Subjects and PSD_Psycophysiological_Insomnia, contain the power spectral density analyses for all subjects. In these files, the data is arranged in the form of cell arrays, where each row represents a channel and each column represents a 30 s epoch. Also, each cell contains a two-column matrix; the first column represents frequency and the second, power. The



Fig. 2. 6 EEG channels sampled at 256 Hz using SOMNOscreen PSG (SOMNOscreen TM plus PSG+, SOMNOmedics GmbH, Germany). This shows the voltage in microvolts on each channel referenced to the left or right earlobe (A1, A2) over a 4 s window.

Table 1				
Data file	names	and	their	descriptions.

Name	Description
Arousal.txt	Time of arousal events
REM.txt	Time of REM events
Sleep Profile Reliability.txt	Reliability of the sleep profile
Sleep Profile.txt	Time of events including Stage 4, Stage 3, Stage 2, Stage 1,Rem,Wake,Movement.
Spindle K.txt	Time of events sleep spindle and K_Complex.

power spectrum analysis is commonly used in the study of biological signals, to calculate the frequency power [4]. Power spectrum analysis was conducted using Fast Fourier transform (FFT) in the range of 0.1–35 Hz, continually [5]. This transform is defined as follows:

$$Y(k) = \sum_{j=1}^{n} X(j) \tilde{n} W_n^{(j-1)(k-1)}$$
(1)

In this data collection project, frequency resolution in power spectrum analysis was 0.5 Hz, which is defined as Fs/N in FFT [6]. As polysomnography analysis is separated by 30 s time intervals, the band's power was also extracted from these 30 s epochs.

The EEG data was filtered using the band pass method between 0.1 Hz and 35 Hz. It should be noted that signal filtering was done by SOMNOscreen[™] plus instrument and the filtered data was exported only, and not completely raw data. In the next step, large artefacts due to electromyography activity, horizontal eye movement or ECG artefact were removed using independent component analysis (ICA). This method was considered in the past decade. Independent signal extraction from mixed signals is one of its applications. The ICA literature is divided into two major categories: practical algorithms and theoretical analyses. ICA could separate activities stemming from the most favourable parts of the brain by using their independent components [7].

With further spectral features, the present data has some important benefits to sleep clinicians and researchers, who are unaware of spectral analysis. They would have considerable findings by download and statistical analysis of spectral features.

1.3. Poincare map

The Poincare's map, as a nonlinear analysis, is valuable, as it could reveal the nonlinear aspects of the data collection [8]. Therefore, the challenge lies in recording temporal information of the plot

quantitatively. The standard descriptors used for quantifying the Poincare's map, measure the impure variability of the time series data. Standard deviations across the line of identification (SD_2) and perpendicular to the line of identification (SD_1), represent the magnitude of the major and minor axes of the ellipse, respectively. SD_1 represents the SD of the instantaneous short term variability. SD_2 represents the SD of long-term variability. SD_1 and SD_2 support the potent data and also, the proportion of SD_1 to SD_2 has been suggested as strongly indicator [9]. Descriptors SD_1 and SD_2 can be defined as:

$$SD_1 = \frac{\sqrt{2}}{2}\tilde{n}SD(x_n - x_{n+1})$$
(2)

$$SD_2 = \sqrt{2\tilde{n}SD(x_n)^2 - \frac{1}{2}\tilde{n}SD(x_n - x_{n+1})^2}$$
(3)

where SD is a standard deviation of the time series.

To plot the Poincare's map — summation, maximum, and standard deviation of the band's power in each epoch was calculated and saved, as time series data. Then, the standard descriptors were calculated and the Poincare plots were extracted from the statics result of the band's power. Each Poincare plot was constructed with the *X*-axis illustrating the statics result, at a specific epoch (x(k)), and the *Y*-axis illustrating the statics result after a specified epoch delay (x(k+1)).

We calculated the *SD* of statics result dispersion along with the diametric line and the *SD* of the power dissipation perpendicular to the diametric line, to present more quantitative data on the repartition of statics result in the Poincare plots (Fig. 3). The *SD* perpendicular to the diametric line was defined as SD_1 and the *SD* along the diametric line was defined as SD_2 . SD_1 is the level of instantaneous variability and demonstrates the variability from one epoch to the next. In contrast, SD_2 demonstrates the power variability across all the epochs. We then defined the SD_1/SD_2 ratio that is a potent candidate, reflecting the psychophysiological disorder depth, which has been used to specify the clarity and linearity of the scatter pattern.



Fig. 3. A typical Poincare plot. The horizontal axes demonstrate the illustrating the statics result at a specific epoch (x(k)) and the vertical axis illustrating the statics result after a specified epoch delay (x(k+1)). An ellipse is fitted to the data points and the Poincare plot descriptors are measured by estimating the *SD* perpendicular to the diametric line was defined as *SD*₁, and the *SD* along the diametric line was defined as *SD*₂ and ratio of the *SD*₁/*SD*₂ of the fitted ellipse.

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Transparency document. Supplementary material

Transparency document associated with this article can be found in the online version at doi:10. 1016/j.dib.2017.09.033.

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