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Catalytically active gold clusters with atomic precision for noninvasive early intervention of neurotrauma

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Abstract

Background: Neurotrauma is a worldwide public health problem which can be divided into primary and secondary damage. The primary damage is caused by external forces and triggers the overproduction of peroxides and superoxides, leading to long-lasting secondary damage including oxidative stress, wound infection and immunological reactions. The emerging catalysts have shown great potential in the treatment of brain injury and neurogenic inflammation, but are limited to biosafety issues and delivery efficiency.

Results: Herein, we proposed the noninvasive delivery route to brain trauma by employing highly active gold clusters with enzyme-like activity to achieve the early intervention. The decomposition rate to H₂O₂ of the ultrasmall gold clusters is 10 times that of glassy carbon (GC) electrodes, indicating excellent catalytic activity. The gold clusters can relieve the oxidative stress and decrease the excessive O₂^{·-} and H₂O₂ both in vitro and in vivo. Besides, gold clusters can accelerate the wound healing of brain trauma and alleviate inflammation via inhibiting the activation of astrocytes and microglia through noninvasive administration. decrease the peroxide and superoxide of brain tissue.

Conclusions: Present work shows noninvasive treatment is a promising route for early intervention of brain trauma.

Keywords: Gold clusters, Catalytic activity, Traumatic brain injury, Noninvasive administration

Background

Traumatic brain injury (TBI) has led to globally death and disability with high mobility [1–3] and caused heavily economic burden as a serious public health issue [4–6]. The primary brain damage can trigger a cascade of molecular and biochemical events, leading to long-lasting secondary damage including oxidative stress, wound

infection and chronic neurodegenerative diseases [1, 7–9]. Reactive oxygen species (ROS) and reactive nitrogen species (RNS) can oxidatively impair biomacromolecules in vivo and play a crucial role in the pathophysiology of TBI including hydroxyl radical (OH·), superoxide anion radicals (O₂^{·-}), hydrogen peroxide (H₂O₂), nitric oxide radicals (NO·) and peroxynitrite (ONOO⁻) [1, 7, 8, 10, 11]. Previous studies have confirmed that TBI can be improved via balancing oxidation reduction by elimination of reactive oxygen and nitrogen species (RONS). Thus, antioxidative biocatalysts with catalase-like (CAT-like), superoxide dismutase-like (SOD-like), peroxidase (POD-like) and glutathione peroxidase-like (GPx-like) activities and good stability show great potential in the treatment and diagnosis of TBI through catalytically scavenging the RONS [12–20].

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Earlier studies have shed light on the enzyme-like activities of nanozymes. Carbogenic and gold-based nanozymes exhibited exceeding activity against oxidative stress and neuroinflammation [11, 13, 19, 21, 22]. Nanozymes composed of metals, metallic oxide and alloys like Pt, Pd, Cr, V and Ce possess high enzymatic activities, beneficial for TBI treatment [12, 14, 15, 18, 23, 24]. Especially, the ceria nanozymes showed excellent SOD-like and CAT-like catalytic activities on scavenging RONS via redox cycle between Ce^{4+} and Ce^{3+} [12, 18, 25]. Compared with traditional nanozymes, the gold clusters show controllable modulation in catalytic activity and selectivity, which can be improved by increasing the atomic utilization efficiency at atomic levels as well as atomic engineering via atom manipulation [26]. Unlike traditional nanozyme, bioactive gold clusters exhibit the high efficient renal clearance and negligible toxicity even at very high injected dose (500 mg/kg) [24, 25, 27]. Moreover, due to ultrasmall size, the gold clusters can enter cell or injury site easily, resulting in high efficient treatment [26, 28]. Gold clusters possess activities like SOD, CAT and GPx enzymes, performing significant antioxidant effects in TBI treatment [26, 28–31]. Though nanotechnologies for TBI diagnosis and monitoring were employed to promote the activity and utilization of nanozymatic biocatalysts like atom engineering, surface modification, and size modulation [32–34], it remains painless and challenged for clinical translation [12, 15, 29–31, 35–45]. Different from the intravenous injection, the noninvasive diagnosis and stimulation for TBI can achieve rapid and painless treatment, worthy of considering to promote recovery and minimize disability. However, the noninvasive methods for TBI treatment are still highly challenged.

Herein, we investigated a noninvasive administration to treat brain trauma at the early stage with gold clusters of well-defined structure and high catalytic selectivity. Electrochemical assay unraveled their high catalytic activities toward hydrogen evolution reaction (HER) and oxygen evolution reaction (OER), and further revealed their excellent activity toward the reduction of O_2 and H_2O_2 . Furthermore, noninvasive administration of the gold clusters distinctly improved the wound healing on TBI mice and Morris water maze tests further confirmed significant recovery on learning ability and spatial memory with $Au_{24}Cu_1$ and $Au_{24}Cd_1$ treatment. *Ex vivo* assay further proved the ability of gold clusters on mitigating oxidative stress and inhibiting neuroinflammation. Together with the results of acceptable biocompatibility, gold clusters showed promising potential as noninvasive therapeutics against TBI.

Results and discussion

The Au_{25} cluster is composed of 13 gold atoms as the core and 6 $Au_2(SG)_3$ as the outer shell. The catalytically active sites of the cluster are mainly located on the surface. Single atom Cu or Cd replaces the Au in one of the S-Au-S, indicative of synthesizing $Au_{24}Cu_1$ and $Au_{24}Cd_1$, respectively. After single atom Cu and Cd substitution, the valence electron structure of the cluster is altered, thereby changing the catalytic performance of the cluster [23]. Figure 1a illustrated the effects of MPA-protected Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ clusters in brain trauma via catalytic systems. TEM images illustrated the homogeneous distribution of the clusters at about 2 nm (Fig. 1b, c), similar with L-NIBC-coated gold clusters [46]. The hydrodynamic sizes determined by dynamic light scattering (DLS) were 1.98, 1.92 and 2.58 nm for Au_{25} , $Au_{24}Cd_1$ and $Au_{24}Cu_1$, respectively, a little larger than the statistical diameter of TEM. After incubation in water for 24 and 48 h, the size of clusters changed negligibly, revealing the favorable stability (Fig. 1d, e). In addition, the zeta potentials of all clusters were around -35 mV (Fig. 1f), consistent with our previous work [26, 47]. The concentration Cd and Cu elements in $Au_{24}Cd_1$ and $Au_{24}Cu_1$ clusters account for 3% and 5% of the total metal as determined by an accurate inductively coupled plasma mass spectrometry (ICP-MS), respectively, further confirming the single-atom substitution in Au_{25} clusters (Additional file 1: Fig. S1). X-ray photoelectron spectroscopy (XPS) confirmed that the dominant state of Au in the clusters is the Au (0) state, and the peaks of Cu $2p_{3/2}$ (931.8 eV) and Cd $3d_{5/2}$ (404.8 eV) are on the reducing side of Cu (0) (id. =932.2 eV) and Cd (0) (id. =405.3 eV), respectively, indicating the successful single-atom substitution in Au_{25} clusters (Additional file 1: Fig. S2). These results display the ultrasmall size and good colloid stability of clusters, manifesting the potential in biological applications.

To evaluate the electrocatalytic activities of the Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ clusters, a standard three-electrode system were employed to conduct the electrocatalytic activities toward HER and OER [48–50]. Figure 2a shows cyclic voltammetry (CV) curves of glassy carbon (GC) electrodes modified with as prepared Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ clusters. Compared with a blank GC electrode, clusters achieve larger negative current density toward HER (Fig. 2a), which were further verified by linear sweep voltammetry (LSV) measurement (Fig. 2b). As shown in Fig. 2c, $Au_{24}Cu_1$ clusters demonstrated a higher efficiency at the potential of -0.4585 V in catalysis, significantly better than $Au_{25}(SC_{12}H_{25})_{18}$ [8] and PtCo cluster [10]. OER exhibits similar results with HER that all clusters improved the performance of the electrochemical reaction (Fig. 2d, f). $Au_{24}Cd_1$ shows the lowest current onset on CV curves at 1.3 V, followed by $Au_{24}Cu_1$

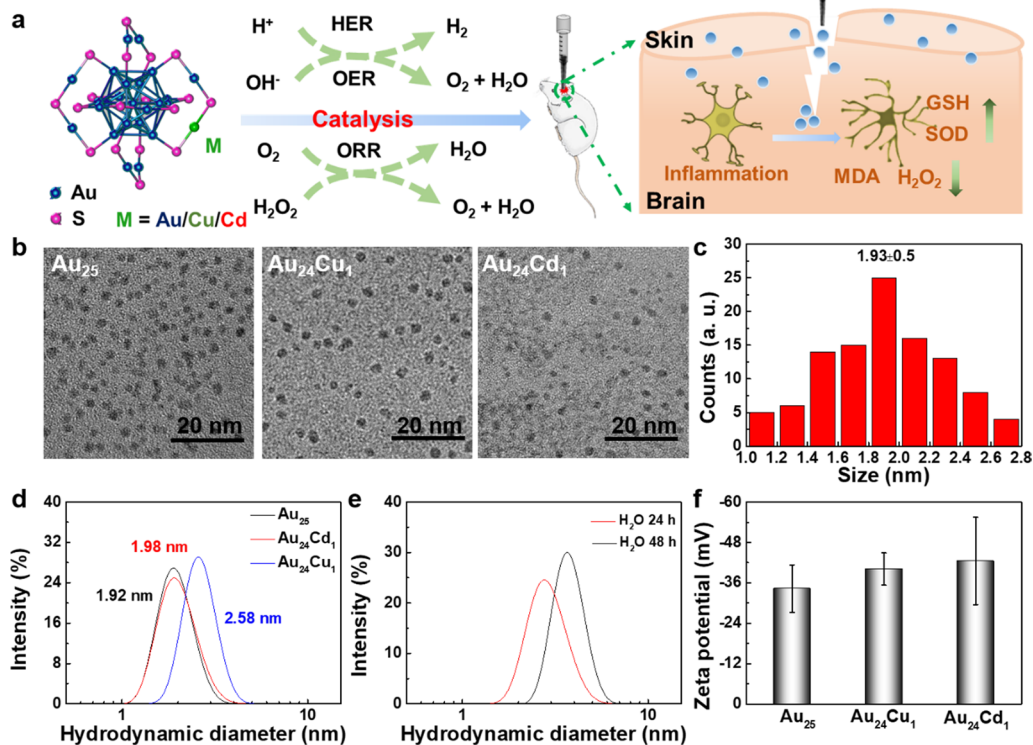


Fig. 1 Structural characterization of Au_{25} clusters. **a** Schematic illustration of noninvasive TBI treatment with gold clusters *via* a catalytic system. **b** TEM image of MPA-protected Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ clusters. Scale bar: 20 nm. **c** Size distribution of MPA-protected Au_{25} nanocluster measured by analyzing 100 nanodots from TEM images. **d** Hydrodynamic diameters of MPA-protected Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ in PBS buffer, and the mean sizes of Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ were 1.98, 1.92 and 2.58 nm respectively. **e** Stability of Au_{25} nanocluster in H_2O after 24 and 48 h at room temperature, and the slightly increase of hydrodynamic diameter revealed satisfying stability. Additionally, the zeta potentials of the clusters **f** were around -35 mV, indicative of good colloid stability ($n=3$ independent experiments, data are presented as mean \pm SD)

and Au_{25} , which is a little different from the results of HER. Besides, $Au_{24}Cd_1$ can reach 0.023 mA/cm^2 at a potential of 1.3254 V, while that of NiFe clusters is less than 0.01 mA/cm^2 , indicating better superiority to NiFe cluster [11]. The results of HER and OER further demonstrated that the catalytic performance were altered by the valence electron structure change via different single-atom substitution [23].

We also evaluated the *in vitro* catalytic activities of Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ clusters in H_2O_2 reduction and oxygen reduction reaction (ORR) [51, 52]. As shown in Fig. 3a, the current density of the GC electrode modified by $Au_{24}Cu_1$ clusters can reach -1.48 mA/cm^2 at a potential of -0.8 V, a little higher than Pt_{12} clusters [18]. The results were further verified by LSV measurement (Fig. 3b), demonstrating that all clusters can enhance the electrocatalytic activity and $Au_{24}Cu_1$ clusters exhibit the best activity for ORR among all clusters. For the reduction of H_2O_2 , only imperceptible reduction current was observed in the presence of H_2O_2 on the GC electrode,

consistent with previous works [51]. Compared with the GC electrode at -0.8 V, $Au_{24}Cu_1$ clusters show the current density of -1.74 mA/cm^2 , and $Au_{24}Cd_1$ clusters exhibit that of -1.56 mA/cm^2 (Fig. 3d, e), slightly better than noble metal (Ag, Pd, Au, Pt) on Graphene/ZnO multi-hybrid nanoarchitectures [19]. Figure 3c, f quantitatively demonstrate the improvement of all clusters on O_2 and H_2O_2 reduction, indicating excellent catalytic activities. $Au_{24}Cu_1$ presented the predominance toward both reactions, and $Au_{24}Cd_1$ and Au_{25} followed toward H_2O_2 and O_2 reduction, respectively.

Since the remarkable catalytic activities inspired us to investigate their biological responses in cells and brain-injured mice, we conducted biological inspections to evaluate their activities *in vitro* and *in vivo*. Combined with our previous work [26], $Au_{24}Cd_1$ and $Au_{24}Cu_1$ clusters conferred catalytic selectivity and enzyme-like activities, beneficial to reduce the oxidative stress induced by brain injury (Fig. 4a). Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ exhibit good biocompatibility at the concentration of $50 \mu\text{g/}$

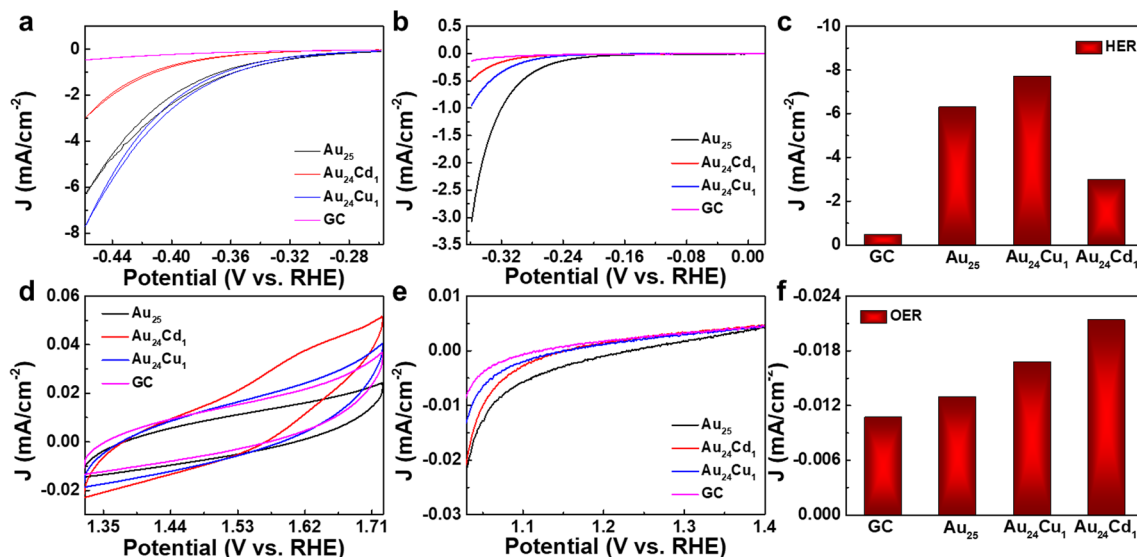


Fig. 2 Catalytic performance for overall water splitting. **a** CVs of GC electrode modified with as-prepared Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters in 0.5 M H_2SO_4 . Scanning rate: 0.010 V s^{-1} . **b** Linear sweep HER voltammograms for Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters. Scanning rate: 0.001 V s^{-1} . **c** Current density of different clusters at the potential of -0.4585 V toward the activity of HER. **d** CVs of GC electrode modified with as-prepared Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters in 1 M KOH. Scanning rate: 0.10 V s^{-1} . **e** Linear sweep OER voltammograms for Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters. Scanning rate: 0.005 V s^{-1} . **f** Current density of different clusters at the potential of 1.3244 V toward the activity of OER

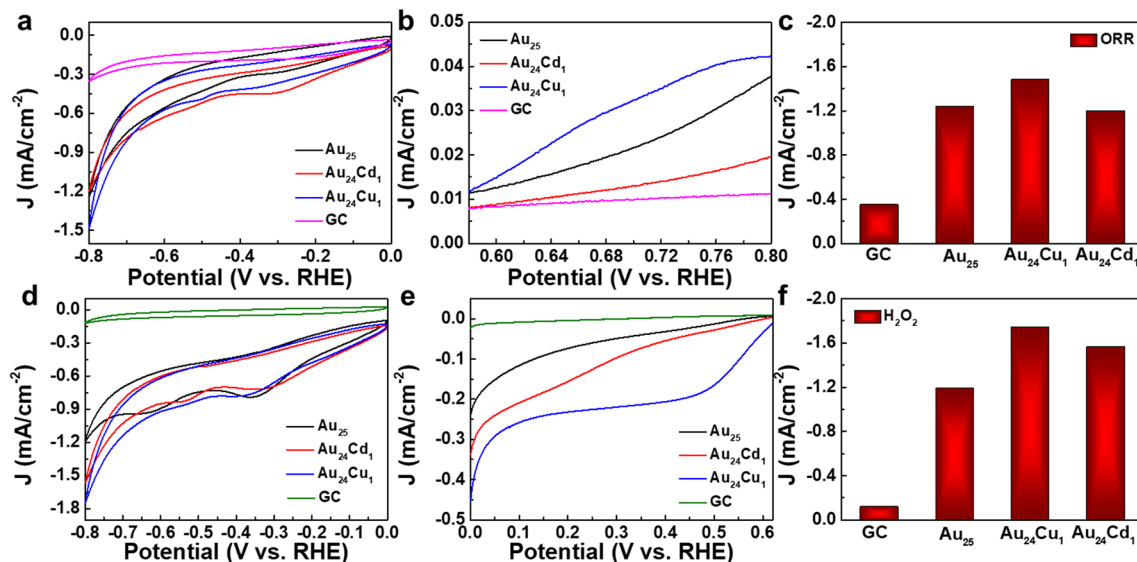
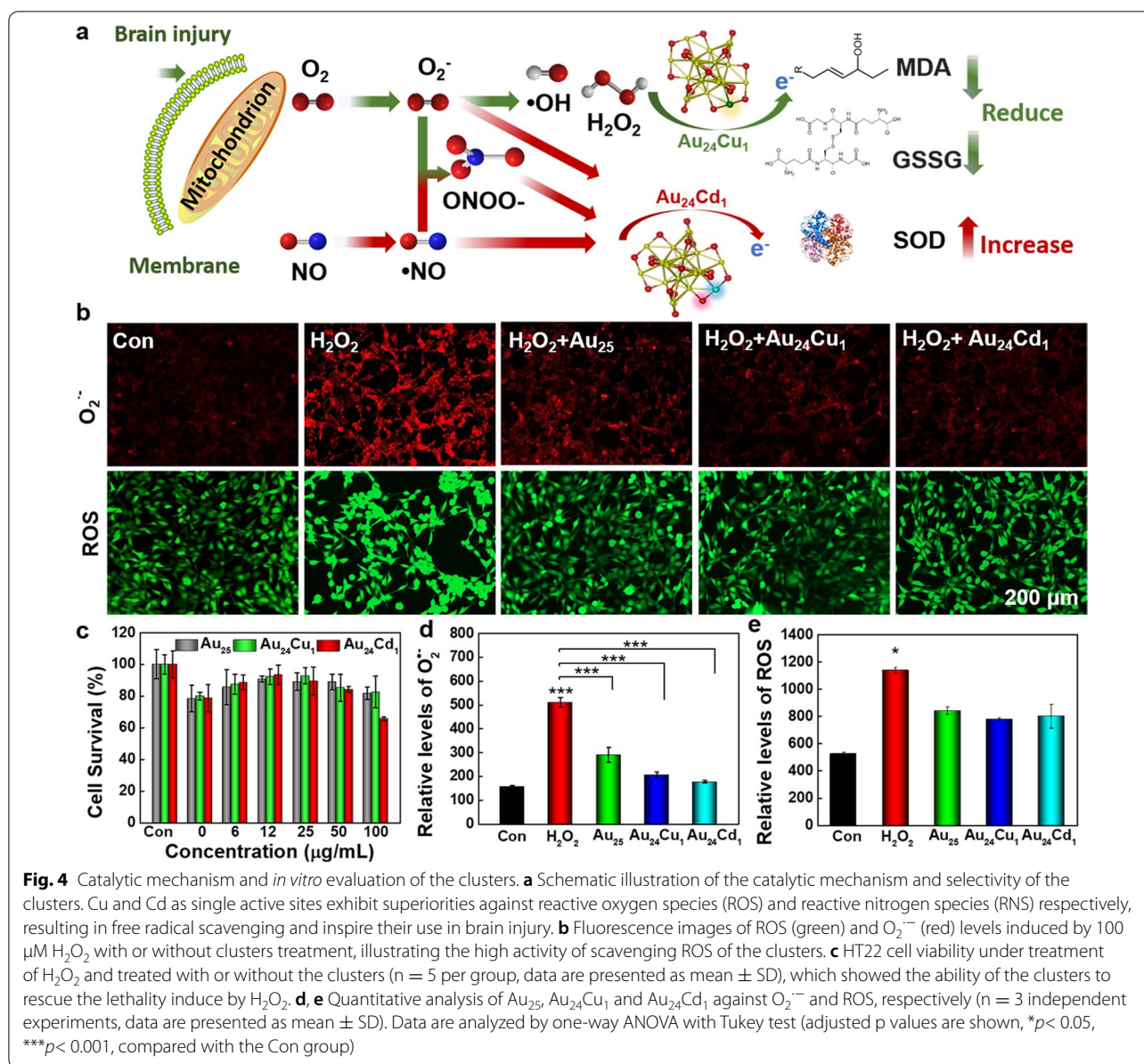


Fig. 3 Catalytic activities of the Au_{25} clusters. **a** CVs of GC electrode modified with as-prepared Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters in O_2 -saturated 0.01 M PBS (pH 7.4). Scanning rate: 0.050 V s^{-1} . **b** LSV of GC electrode modified with as-prepared Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters in O_2 -saturated 0.01 M PBS (pH 7.4). Scanning rate: 0.005 V s^{-1} . **c** Compared the ORR activities of Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters at the potential of -0.8 V . **d** CVs of GC electrode modified with as-prepared Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters in the presence of 9.8 mM H_2O_2 in N_2 -saturated 0.01 M PBS (pH 7.4). Scanning rate: 0.050 V s^{-1} . **e** LSV of GC electrode modified with as-prepared Au_{25} , $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters in the presence of 9.8 mM H_2O_2 in N_2 -saturated 0.01 M PBS (pH 7.4). Scanning rate: 0.010 V s^{-1} . Rotation rate: 1600 rpm. **f** Compared the H_2O_2 scavenging activities of clusters at the potential of -0.8 V



mL to different neural cell lines (HT22, BV2 and MA-c) determined by 3-[4,5-dimethylthiazol-2-yl]-2,5 diphenyltetrazolium bromide (MTT) assays (Additional file 1: Fig. S3), presenting favorable metabolic properties [26].

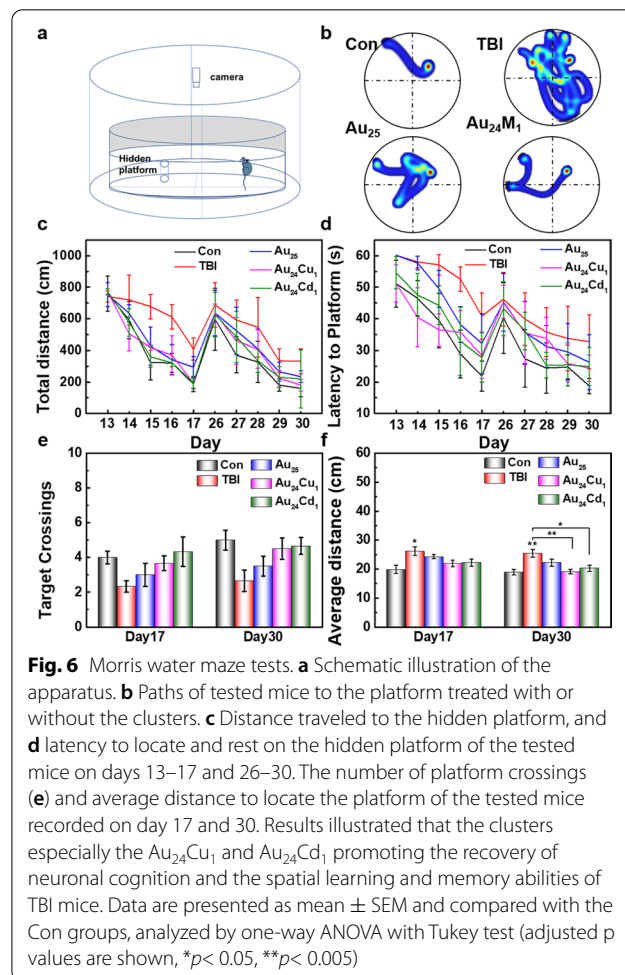
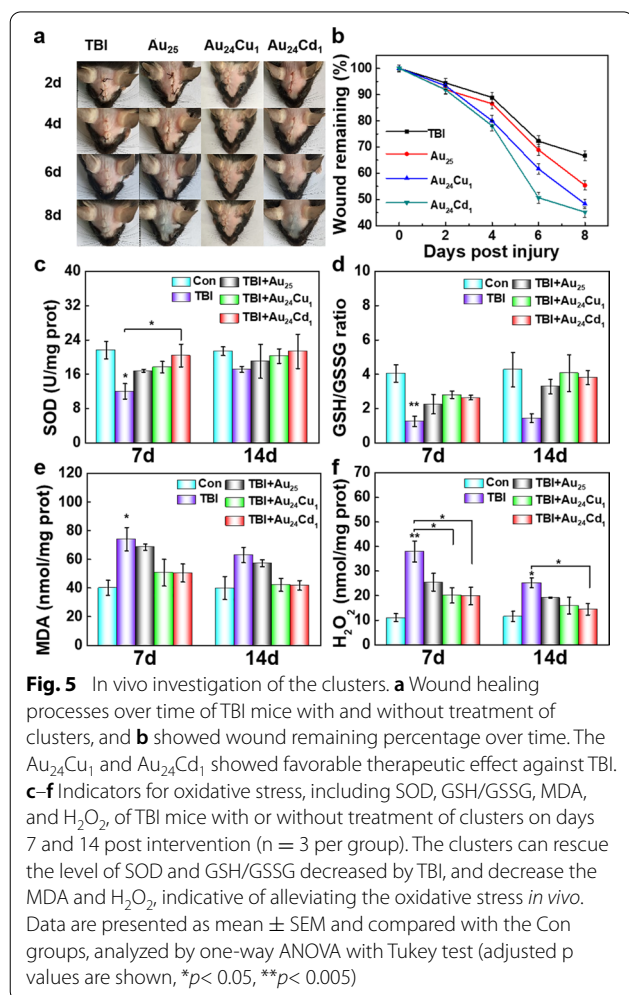
To investigate the biological activity of clusters, imaging of H_2O_2 -treated neuron cells with or without Au_{25} , $\text{Au}_{24}\text{Cd}_1$ and $\text{Au}_{24}\text{Cu}_1$ clusters was obtained (Fig. 4b). The H_2O_2 stimulation can significantly elevates signals, indicating the presence of excessive amount of ROS and $O_2^{\cdot-}$ [53]. All clusters can decrease the ROS and $O_2^{\cdot-}$ signals, while $\text{Au}_{24}\text{Cd}_1$ shows the best clearance efficiency. Meanwhile, $\text{Au}_{24}\text{Cu}_1$ displays better clearance capability against ROS than Au_{25} and $\text{Au}_{24}\text{Cd}_1$,

suggesting higher selectivity for ROS. The related quantification further confirmed the remarkable biological catalytic activity and laying the groundwork for *in vivo* utilization (Fig. 4d, e). In addition, H_2O_2 induces decreases in cell viability ($\sim 78\%$) due to oxidative stress and inflammation [54], while Au_{25} , $\text{Au}_{24}\text{Cd}_1$ and $\text{Au}_{24}\text{Cu}_1$ clusters can rescue cell viability back to 90%, indicative of great potential to protect nerves and lower the lethality from H_2O_2 -induced cytotoxicity (Fig. 4c). All the *in vitro* results manifest good catalytic activities of $\text{Au}_{24}\text{Cd}_1$ and $\text{Au}_{24}\text{Cu}_1$ clusters on ROS scavenging, revealing their potential as biocatalysts and suggesting further investigation *in vivo*.

The primary injuries triggers a cascade of biochemical reactions, leading to the long-lasting secondary injuries. The secondary brain injuries generate harmful molecules and cytokines, leading to acute or chronic neuronal damage, memory impairment and inflammation. Traditional intravenous administration have shown great potential in brain diseases, but toxicity remains a major concern for clinical translation [15, 28]. Therefore, the above *in vitro* preliminary results inspired us to treat TBI non-invasively and it is reasonable to develop a noninvasive routine to treat TBI at the early stage. The clusters were dropped in the injured area of TBI mice. The wound size was significantly reduced to healthy levels after clusters treatment, whereas the untreated mice only showed a partial recovery (Fig. 5a, b). We further evaluated the oxidative stress-related indicators, including SOD, GSH/GSSG, MDA, and H_2O_2 in TBI mice [28, 55]. Brain injuries generate excessive ROS in tissues, consume lots of SOD and GSH, and produce harmful lipid peroxidation (Fig. 5c–f). SOD and GSH/GSSG are sharply decreased

on day 7 post-injury and slightly increased on day 14 post-injury, and MDA and H_2O_2 are relatively serious on day 7 post-injury and a little alleviated on day 14 post-injury for TBI groups, indicating severe oxidative stress after brain injuries. However, clusters can effectively decrease the MDA and H_2O_2 levels, suggesting the ROS elimination of clusters, and can significantly recovered the SOD and GSH/GSSG levels, maintaining the balance of ROS levels.

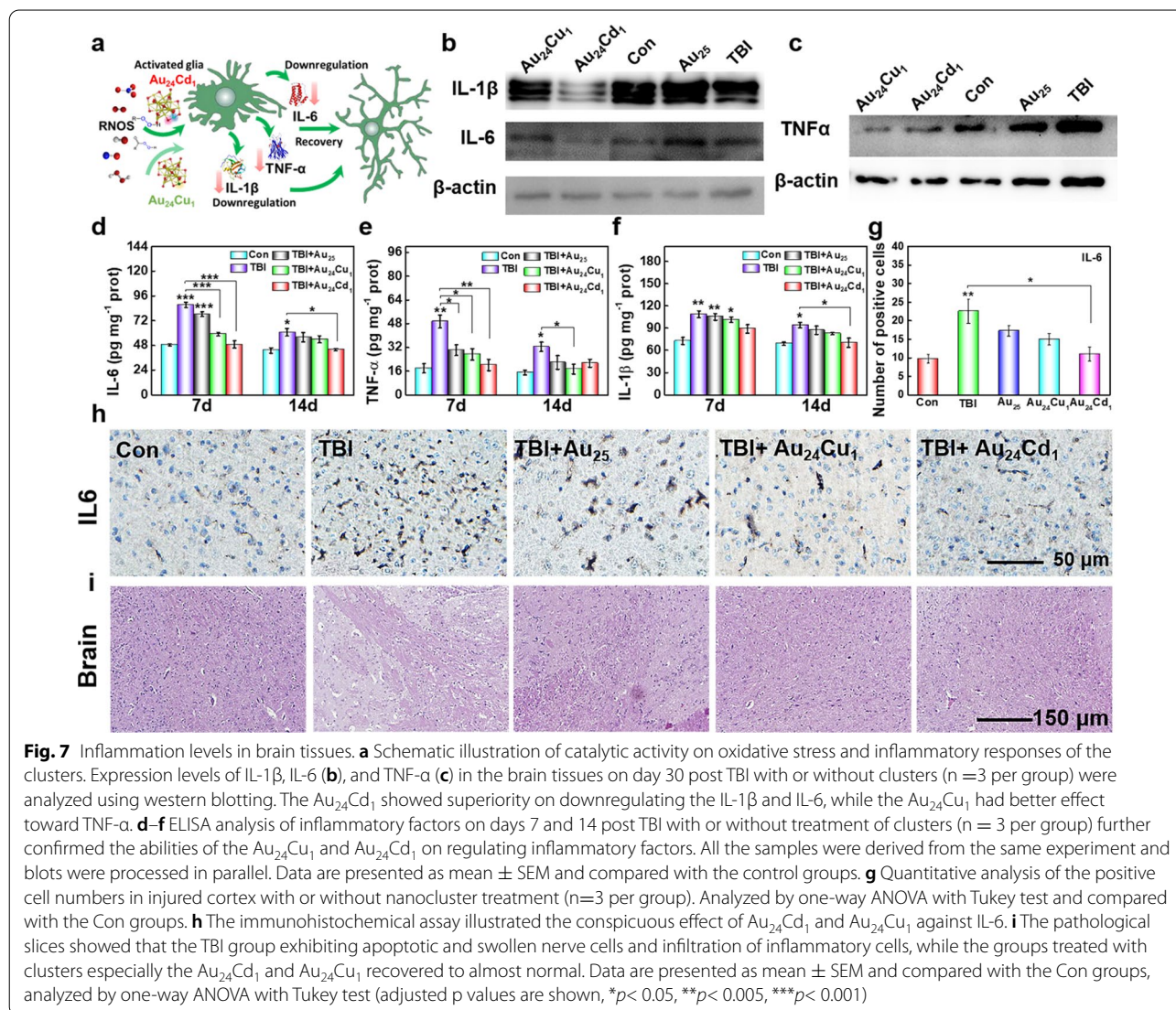
Moreover, the behavior tests were conducted to evaluate the spatial learning and memory abilities by Morris water maze (Fig. 6). All mice were trained to learn to search for the platform during the acquisition phase on days 13–17 and 26–30 including the total distance travelled and the latency to the hidden platform. Compared with TBI groups, both travel distance and latency to platform gradually decrease with training after clusters treatment (Fig. 6c, d), indicating that clusters can effectively improve the motor function following brain injury. $Au_{24}Cu_1$ or $Au_{24}Cd_1$ clusters show better results than Au_{25} , indicating the efficiency enhancement by Cu and



Cd single-atom substitution. Figure 6e, f show that platform crossings and average distance obviously decrease in TBI group and can almost return back to normal levels with clusters treatment after injury. These facts imply that clusters can effectively improve the learning ability and spatial memory of mice with TBI-induced brain injury.

Since brain injuries can lead to chronic inflammation, we were examined their therapeutic effects on the neuroinflammation. Figure 7a demonstrates the schematic illustration for the TBI-associated inflammatory responses and relevant modulation with the clusters [1, 8]. IL-1 β , IL-6 and TNF- α are all upregulated after injury, revealing strong local inflammation. Au₂₅ only shows minor downregulation toward the three inflammatory factors, while Au₂₄Cd₁ and Au₂₄Cu₁ exhibit exceptional efficiency to reduce their levels, manifesting that substitution of Cu and Cd atom has great influence on the

catalytic activity (Fig. 7b, c). Au₂₄Cu₁ performs better than Au₂₄Cd₁ in downregulating overexpressed TNF- α , whereas Au₂₄Cd₁ behaves better in mediating IL-1 β , IL-6, implying catalytic selectivity to different inflammatory cytokines. ELISA kits further verified the immunoblot results that Au₂₄Cd₁ and Au₂₄Cu₁ are superior to Au₂₅ on inhibiting inflammatory factors in brain tissues including IL-1 β , IL-6, and TNF- α (Fig. 7d, f). Additionally, the immuno histochemical assay illustrated the conspicuous anti-inflammation effect of Au₂₄Cd₁ and Au₂₄Cu₁ against IL-6 (Fig. 7h), consistent with quantitative results in Fig. 7g. Furthermore, significant differences on the pathological slices can be seen that the TBI group exhibited swelling of nerve cells and obvious infiltration of inflammatory cells; while the groups treated with clusters especially the Au₂₄Cd₁ and Au₂₄Cu₁ recovered to almost normal (Fig. 7i). These results demonstrated that

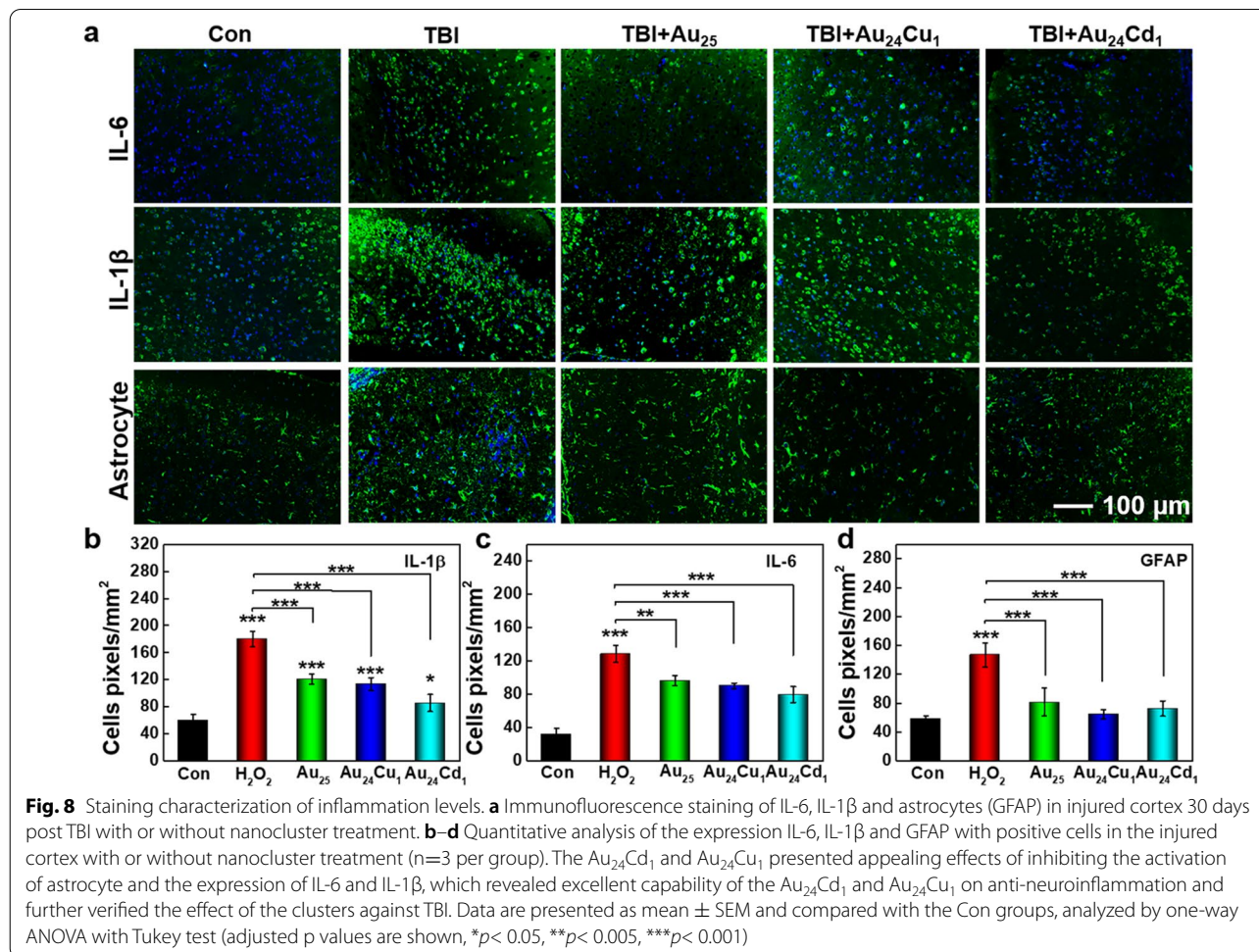


the clusters especially $\text{Au}_{24}\text{Cd}_1$ and $\text{Au}_{24}\text{Cu}_1$ can accelerate the wound healing of traumatically injured brain by inhibiting the inflammatory factors.

Brain injuries can also mediate the recruitment of microglia and astrocytes in the injured areas, which are the key cellular mediators of TBI after brain injury [1]. As shown in Fig. 8a, lots of astrocytes are produced and activated along with inflammatory cytokines, indicating strong local inflammation. The $\text{Au}_{24}\text{Cd}_1$ and $\text{Au}_{24}\text{Cu}_1$ clusters can inhibit the activation of astrocytes and remarkably reduce the overexpression of IL-1 β and IL-6. The relative quantification further exhibited the significant effect of $\text{Au}_{24}\text{Cd}_1$ and $\text{Au}_{24}\text{Cu}_1$ clusters (Fig. 8b–d). Immune response associated IL-1 β and IL-6 can be alleviated by $\text{Au}_{24}\text{Cd}_1$, while $\text{Au}_{24}\text{Cu}_1$ shows better effect on reducing TNF- α , indicating their catalytic selectivity and potential selectivity towards the treatment of neuroinflammation. Also, it is noted that the performance of mice in $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ groups is superior to that in Au_{25} groups, indicating that $\text{Au}_{24}\text{Cu}_1$ and $\text{Au}_{24}\text{Cd}_1$ clusters possess a better anti-inflammation property by

efficiently eliminating excessive free radicals and inhibiting neuroglia activation. Additionally, hematology analysis and tissue toxicology analysis showed no toxicity in the long term, suggesting the good biological safety of clusters (Additional file 1: Figs. S4–S6).

The present work demonstrated the high catalytic activity of $\text{Au}_{24}\text{Cd}_1$ and $\text{Au}_{24}\text{Cu}_1$ clusters and their availability as TBI therapeutics. Unlike traditional nanozymes, gold clusters overcame the water insolubility and exhibited the well-defined structure at the atomic level with ultrasmall size and good biocompatibility. Catalytic activity and selectivity of clusters can be further increased and availability as TBI therapeutics can also be improved via single atom substitution. Moreover, since noninvasive administration can directly and rapidly release the biocatalysts into the damaged area, it shows promising potential for TBI treatment, eliminating the RNOS and inhibiting subsequent neuroinflammation [15, 26, 56, 57]. Necessarily, exploiting new biocatalysts with high catalytic activities and favorable biocompatibility, and developing new delivery modes for the biocatalysts for the



noninvasive intervention of TBI remain constant challenges in this field [15, 43]. As more biocatalysts with distinguished catalytic activities against oxidative stress are under development [20, 58], there will be more potential therapeutics in the use of noninvasive intervention against TBI.

Conclusions

In summary, we have reported a noninvasive therapeutic to treat brain trauma at the early stage with gold clusters of well-defined structure and high catalytic selectivity. Compared with reported nanozymes, the gold clusters showed higher catalytic activities toward water splitting and reduction of O_2 and H_2O_2 by introducing the Cu or Cd catalytic active site. The biological results reveal that clusters can modulate the oxidative stress and further alleviate neuroinflammation by noninvasive administration. Besides, these results conclude that $Au_{24}Cd_1$ preferentially decreases IL-1 β and IL-6, while $Au_{24}Cu_1$ shows the tendency to decrease TNF- α , indicating their different selectivity for alleviating neuroinflammation. Behaviors and histology illustrated their favorable effects against TBI after noninvasive administration. In conclusion, our work shows the great potential of noninvasive early intervention for the treatment of TBI with enzymatic biocatalysts.

Materials and methods

Materials and reagents

All chemicals and reagents were purchased from commercial sources and used without further purification. Gold chloride ($HAuCl_4 \cdot 3H_2O$) was purchased from Sigma-Aldrich. Copper nitrate ($Cu(NO_3)_2$), Cadmium nitrate ($Cd(NO_3)_2$), 3-Mercaptopropionic acid (MPA), Sodium borohydride ($NaBH_4$), Sodium hydroxide (NaOH), were purchased from Aladdin. Ultrapure water ($18.2 M\Omega \cdot cm$) was used for all the experiments. Kits and fluorescent probes were purchased from commercial sources and used as per the instructions.

Materials preparation, characterization and catalytic activities

The MPA-protected Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ clusters were prepared as per the previous reports [26, 59, 60]. Briefly, $HAuCl_4$ (aqueous, 20 mM, 0.25 mL) and MPA (aqueous, 5 mM, 2 mL) were added to water (2.35 mL) and stirred for 5 min at room temperature. Then, NaOH solution (aqueous, 1 M, 0.3 mL) was added to the reaction mixture, followed by the addition of 0.1 mL of $NaBH_4$ (43 mg of $NaBH_4$ powder in 10 mL of 0.2 M NaOH solution). $Au_{25}MPA_{18}$ was collected after the final reaction mixture stirred at room temperature for 3 h in the dark and aged at 4 °C for 12 h. The

$Au_{24}Cu_1$ and $Au_{24}Cd_1$ were synthesized based on the same method, except the Au atoms in $HAuCl_4$ (20 mM, 0.25 mL) were replaced by various nitrate metal ions (Cu^{2+} , Cd^{2+}) at a 4% molar ratio. Ultrafiltration tubes of 3 and 10 K at 3500 rpm/min were used for ultrafiltration to remove smaller organic ligands and larger-sized clusters, and lyophilization was used to collect the purified product for further test and investigation.

A JEM-2100 F electron microscope (JEOL, Japan) was employed to acquire transmission electron microscopic (TEM) images. A Malvern Zetasizer Nano ZS90 (UK) was employed to measure dynamic light scattering (DLS) to test the hydrodynamic size and determine the zeta potential of clusters.

The XPS spectrum of the metal elements was performed using ESCALAB Xi+ spectrometer, with a monochromatic Al K α X-ray source (Thermo Fisher Scientific). All XPS spectra are processed with XPSPEAK41 software and corrected with the peak of C1s (standard: 428.8 eV). ICP-MS (Agilent, US) was used to determine the content of each metal element in the clusters.

The clusters were deposited onto the surface of glassy carbon (GC) electrodes for electrochemical assay [14, 40]. Briefly, as-prepared MPA-protected Au_{25} , $Au_{24}Cu_1$ and $Au_{24}Cd_1$ clusters (20 μ L, 0.5 mg/mL) were deposited onto the surface of GC electrodes and dried naturally, then Nafion solution (3 μ L) was dropped onto the surface of GC electrodes and dried, the modified electrodes were used for catalytic activity tests.

Cyclic Voltammetry (CV, scan rate: HER, 10 $mV s^{-1}$; OER, 100 $mV s^{-1}$) and Linear Sweep Voltammetry (LSV, scan rate: HER, 1 $mV s^{-1}$; OER, 5 $mV s^{-1}$) measurements were taken electrochemical analyzer, CHI760E, Shanghai) to evaluate the performance of the clusters modified electrodes for HER and OER. HER was carried out in 0.5 M H_2SO_4 , and a graphite rod and a saturated calomel electrode were used as the counter electrode and reference electrode, respectively. OER was carried out in 1 M KOH, and a platinum wire and an Ag/AgCl electrode were used as the counter electrode and reference electrode, respectively.

CV (scan rate: 50 $mV s^{-1}$) and LSV (scan rate: 5 $mV s^{-1}$) measurements were taken (electrochemical analyzer, CHI760E, Shanghai) to evaluate the catalytic activities for O_2 and H_2O_2 reduction. A three-electrode cell was adopted for both O_2 and H_2O_2 reduction, a platinum wire and a saturated calomel electrode were used as the counter electrode and reference electrode, respectively. Oxygen reduction reaction (ORR) was carried out in O_2 -saturated in 0.01 M PBS (pH 7.4), and the H_2O_2 reduction was performed in the presence of 9.8 mM H_2O_2 in N_2 -saturated 0.01 M PBS (pH 7.4).

In vitro evaluation of the catalytic activities

Cytotoxicity assay. mouse hippocampal neuronal cell line (HT22) (3×10^3), mouse microglia (BV2) (4×10^3), and mouse astrocytes (MA-c) (4×10^3) were seeded in 96-well plates filled in 100 μ L medium with 0.01 M PBS (Gibco) at the border overnight. The culture medium was replaced by different doses of Au₂₅, Au₂₄Cu₁, or Au₂₄Cd₁ dissolved in the DMEM, and then cells were incubated for another 24 h. Wells were washed with 0.01 M PBS once, and the medium were replaced by fresh culture medium with serum-free DMEM. Cell survival was analyzed using MTT (3-(4,5-dimethyl-2-thiazol)-2,5-diphenyl-2 H tetrazolium bromide, Beyotime) of 5 mg/mL for 2.5 h and detected at optical density (OD) 490 nm.

Cell viability and Immunofluorescence. HT22 was used in all the cellular experiments. Cells were seeded into the 96-well plates and grew in Dulbecco's modified Eagle's medium (DMEM) at 37 °C with 5% CO₂. After being stimulated with 100 μ M H₂O₂ for 6 h, the culture medium was replaced by Au₂₅, Au₂₄Cu₁ and Au₂₄Cd₁ dissolved in the DMEM at different doses, and then cells were incubated for another 24 h. HT22 cells (1×10^5 cells per well) were seeded in 6-well plates for 12 h and stimulated with 100 μ M H₂O₂ for 6 h before being treated with the clusters (12 ng/ μ L). Cell survival was determined at the MTT concentration of 5 mg/mL for 2.5 h and detected at optical density (OD) 490 nm. Fluorescent staining was carried out to evaluate the intracellular oxidative stress levels with different probes such as DHE for O₂⁻ and DCFH-DA for ROS, and cell images were captured by a fluorescence microscope.

In vivo treatment and behavioral experiment

TBI models: C57BL/6 mice at 21–23 g were employed to establish TBI models using an electromagnetically CCI injury device (eCCI-6.3, Custom Design & Fabrication, Inc), with an impactor of 5 m/s velocity, 0.61 mm depth, 150 ms duration, and 20° angle of dura mater on the vertical axis. The mice were divided into control, TBI, TBI+Au₂₅, TBI+Au₂₄Cu₁, and TBI+ Au₂₄Cd₁ group (n = 15) randomly. All mice were anesthetized with 10% chloral hydrate (10 mg/kg) and the scalp was cut before placed on the stereotaxic frame. The craniotomy was carried out by drilling the skull in a circle of 2 mm in diameter. The scalp was sewn together carefully, and the clusters were added to the wound of TBI mice at a concentration of 50 mg/kg. The healing process was recorded photographically and the wound remaining was calculated after treatment.

Oxidative stress level: Brain tissues were taken out on days 7 and 14 post-treatment, then homogenized in 0.9% physiological saline and analyzed for SOD, GSH/GSSG,

MDA, and H₂O₂ using commercially available kits. All testing methods are carried out as per the instructions (Beyotime).

Morris water maze tests: Morris water maze (MWM) was conducted on days 13–17 and 26–30 post-treatment as described in the previously reported literature [12, 61, 62]. Briefly, the water maze was divided into four quadrants, and the platform was set in the center of quadrant I. Before spatial learning, visual discrimination learning was performed to determine whether the vision of mice was normal. In this procedure, each animal performed one trial where the platform was placed above the water to determine whether the vision of mice was normal. Animal with the visual problem would be excluded in the Morris water maze test. Each mouse was put into the pool to be trained and learned to search for the platform under the water in the order of quadrant II, III, IV and I with an inter-trial interval (ITI) of 60 min at almost the same time of each day for five days. The test was carried out without the platform on the fifth day, and each mouse was put into the pool at quadrant II and allowed for 60 s to track them.

Ex vivo verification

Western Blotting: The total protein in the brain tissue was extracted and the content of IL-1 β (1:1000), IL-6 (1:1000) and TNF- α (1:1000) was analyzed. SDS-PAGE electrophoresis was performed before transferring to the membrane. Immune responses of the specific antibodies were carried out and the images were captured with autoradiography. All antibodies were purchased from Abcam.

ELISA analysis: Inflammatory cytokines including IL-6, IL-1 β and TNF- α were determined by ELISA kits (Abcam, ab100712, ab197742, ab208348, respectively), and the assays were performed as per the instructions provided by the manufacture.

Tissue staining: Brain tissues were taken out at 30 days post-injury and fixed in 4% paraformaldehyde and embedded in paraffin. Immunofluorescent staining was performed with primary antibodies including anti-GFAP, IL-6, IL-1 β antibodies as per the instructions of (Abcam). Then the slices were incubated with Alexa Fluor 488/594-conjugated goat secondary antibody for 1-1.5 h at room temperature under dark and counterstained with DAPI. Immunohistochemical staining for IL-6 and mice brain tissue was performed according to the instructions (Proteintech).

Toxicological studies: The biosafety of clusters was measured on male C57BL/6J mice at 7-8 weeks (21-23 g). Mice were treated with 200 μ L of clusters at a dose of 50 mg/kg every other day. Hematology and blood biochemical indicators were tested on day 30.

The blood sample was obtained from the retroorbital sinus and stored in a test tube containing K2EDTA for testing. The blood sample used for biochemical analysis was allowed to stand for 30 min, and then centrifuged twice at 3500 rpm for 15 min each time, the supernatant was collected and tested. The main organs of the mice were collected and fixed in 4% paraformaldehyde for 24 h, embedded in paraffin, and mounted on a glass slide (4 μ m coronal section). The slices were stained with hematoxylin and eosin to observe the toxicity of clusters in major organs, including the heart, liver, spleen, lung, kidney and testis.

Statistic methods

Data are presented as mean \pm standard deviation (SD) or standard error of the mean (SEM). For multiple comparisons, one-way analysis of variance (ANOVA) was performed using the SPSS 22 software to assess difference in means among groups and compared with the Con and TBI groups, analyzed by ANOVA.

Abbreviations

TBI: Traumatic brain injury; ROS: Reactive oxygen species; OH \cdot : Hydroxyl radical; O $_2^{\cdot-}$: Superoxide anion radicals; H $_2$ O $_2$: Hydrogen peroxide; RNS: Reactive nitrogen species; NO \cdot : Nitric oxide radicals; ONOO $^-$: Peroxynitrite; RONS: Reactive oxygen and nitrogen species; CAT: catalase; SOD: superoxide dismutase; POD: peroxidase; GPx: glutathione peroxidase; HER: hydrogen evolution reaction; OER: oxygen evolution reaction; DLS: dynamic light scattering; GC: glassy carbon; CV: Cyclic Voltammetry; LSV: Linear Sweep Voltammetry; ORR: Oxygen reduction reaction; ICP-MS: Inductively coupled plasma mass spectrometry; XPS: X-ray photoelectron spectroscopy; ALT: Alanine aminotransferase; ALB: Albumin; AST: Aspartate aminotransferase; TP: Total protein; CREA: Creatinine; TB: Total bilirubin; BUN: Blood urea nitrogen; WBC: White blood cells; RBC: Red blood cell; HCT: Hematocrit; MCV: Mean corpuscular volume; HGB: Hemoglobin; PLT: Platelets; MCH: Mean corpuscular hemoglobin; MCHC: Mean corpuscular hemoglobin concentration.

Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s12951-021-01071-4>.

Additional file 1: Figure S1. The content of metal elements in the clusters were quantified by ICP-MS. **Figure S2.** X-ray photoelectron spectroscopy of clusters. **Figure S3.** Cell survival of (a) HT22, (b) BV2 and (c) MA-c cells in the presence of various concentrations of clusters. **Figure S4.** Hematology of mice treated with or without gold clusters on day 30. **Figure S5.** Blood biochemistry analysis of mice treated with or without gold clusters on day 30. **Figure S6.** Histology of major organs in mice.

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Not applicable.

Authors' contributions

ZX, WH, and XJ originated the concept. ZY and SS wrote the manuscript. SS and LH worked on materials synthesis and characterizations. RQ, HW, and QX worked on biological experiments. All authors read and approved the final manuscript.

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Availability of data and materials

The datasets used and analyzed during the current study are available from the corresponding author on reasonable request.

Declarations

Ethics approval and consent to participate

We have obtained approval of animal ethics and use committee (IRM-DWLL-2019099). All animal procedure was followed the guideline approved by the Institute of Radiation Medicine, Chinese Academy of Medical Sciences and Peking Union Medical College.

Consent for publication

All authors gave their consent for publication.

Competing interests

The authors declare no conflict of interest.

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