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Nanotherapies for sepsis by regulating inflammatory signals and reactive oxygen and nitrogen species: New insight for treating COVID-19



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ABSTRACT

SARS-CoV-2 has caused up to 127 million cases of COVID-19. Approximately 5% of COVID-19 patients develop severe illness, and approximately 40% of those with severe illness eventually die, corresponding to more than 2.78 million people. The pathological characteristics of COVID-19 resemble typical sepsis, and severe COVID-19 has been identified as viral sepsis. Progress in sepsis research is important for improving the clinical care of these patients. Recent advances in understanding the pathogenesis of sepsis have led to the view that an uncontrolled inflammatory response and oxidative stress are core factors. However, in the traditional treatment of sepsis, it is difficult to achieve a balance between the inflammation, pathogens (viruses, bacteria, and fungi), and patient tolerance, resulting in high mortality of patients with sepsis. In recent years, nanomaterials mediating reactive oxygen and nitrogen species (RONS) and the inflammatory response have shown previously unattainable therapeutic effects on sepsis. Despite these advantages, RONS and inflammatory response-based nanomaterials have yet to be extensively adopted as sepsis therapy. To the best of our knowledge, no review has yet discussed the pathogenesis of sepsis and the application of nanomaterials. To help bridge this gap, we discuss the pathogenesis of sepsis related to inflammation and the overproduction RONS, which activate pathogen-associated molecular pattern (PAMP)-pattern recognition receptor (PRR) and damage-associated molecular pattern (DAMP)-PRR signaling pathways. We also summarize the application of nanomaterials in the treatment of sepsis. As highlighted here, this strategy could synergistically improve the therapeutic efficacy against both RONS and inflammation in sepsis and may prolong survival. Current challenges and future developments for sepsis treatment are also summarized.

1. Introduction

Coronavirus disease 2019 (COVID-19) broke out in late 2019 and has quickly spread across the world. In just 1 year, COVID-19 has infected more than 127 million people worldwide and caused 2.78 million deaths. Most patients with severe COVID-19 eventually develop typical septic shock, including an inflammatory cytokine storm response, cold extremities, weak peripheral pulses, oxidative stress injury, and microcirculation dysfunction [1]. Some patients exhibit obvious multiple organ dysfunction, such as heart damage, liver impairment, and kidney malfunction in addition to severe lung injury. According to the 2016 Sepsis-3 International Consensus, many critically ill COVID-19 patients satisfy the diagnostic criteria for sepsis [2]. In the latest guidelines for the treatment of COVID-19, the "surviving sepsis campaign" has been adopted as the guideline for the treatment of severely ill patients [3]. Therefore, advances in sepsis research are important for improving the clinical care of COVID-19 patients.

Sepsis is a systemic inflammatory response syndrome (SIRS) induced by an imbalance in homeostasis after exposure to a variety of injuries, including infection, trauma, and surgery, causing extremely high morbidity and mortality. Sepsis is characterized by uncontrolled inflammation and overproduction of reactive oxygen and nitrogen

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species (RONS), which the host immune system is unable to eliminate [4–6]. Subsequently, this uncontrolled inflammation and excessive RONS can damage cells and tissues, causing immune system dysfunction and eventually leading to multiple organ failure syndrome (MODS) [7–10]. Currently, organ dysfunction caused by sepsis remains the main cause of death among hospitalized patients in intensive care units (ICUs) [8,11–13]. Undoubtedly, mortality from sepsis remains high, affecting more than 48.9 million people worldwide each year and is regarded as the one of the main causes of death in critically ill patients worldwide [12,14,15]. Therefore, it is necessary to investigate effective therapies to increase the survival rate of patients with sepsis.

Current therapies for treating sepsis are dominated by antiinflammatory drugs, such as melatonin [[16]], and traditional antioxidants, such as vitamin C [17] and N-acetylcysteine [18]. However, many studies have reported that currently available anti-inflammatory drugs and antioxidants for the treatment of sepsis are invalid and even decrease survival rates [19,20]. These drugs have many shortcomings, including low efficacy and side effects, which make it difficult to effectively reduce the inflammatory response and overproduction of RONS in sepsis [17]. Therefore, it is urgent to investigate valid strategies that focus on combating inflammation and RONS. In recent decades, the application of nanomaterials in biomedicine has been among the most fascinating areas of research, and considerable progress has been made. Nanomaterials exhibit biocompatibility, high targeting, and low toxicity, and hold immense potential for development in biomedicine [21]. For example, melanin nanoparticles that can serve as RONS scavengers to protect the ischemic brain from RONS-induced damage in a rat model of ischemic stroke have been developed [22]. Similarly, the application of nanomaterials in the treatment of sepsis has received much attention with great prospects.

The size of nanomaterials is between that of biomolecules and cells. In theory, careful design of nanomaterials can achieve regulation of cell state and function. Therefore, the use of nanomaterials for sepsis treatment has received tremendous interest in the past two decades. Advances in nanotechnology have also made it possible to engineer complex nanostructures with unique physical properties and surface chemistry, with many potential merits compared to traditional therapeutic agents. In this review, we aim to provide a detailed account of sepsis pathology and nanotherapies for regulating inflammation and RONS in sepsis. We start with an introduction to sepsis pathology to elucidate the underlying mechanisms involved in sepsis progression, which mainly include the vicious circle of inflammation and RONS mediated by the pathogen-associated molecular pattern (PAMP)/damage-associated molecular pattern (DAMP)-pattern recognition receptor (PRR) signaling pathways, damage and dysfunction of vascular endothelial cells and immune cells caused by inflammation and RONS, and the mechanism of vascular leakage and multiple organ damage. We then highlight the progress in nanotherapies for regulating inflammation and RONS in sepsis (Table 1), which can be divided into four categories: nanomaterials blocking the PRR signaling pathways mediated by PAMPs/DAMPs, nanomaterials eliminating RONS, nanomaterials eliminating inflammation, and multifunctional nanomedicine (Fig. 1, Table 1). Finally, we discuss strategies for further improving inflammation and RONS in sepsis and the impact of treating sepsis with nanotherapies. Throughout our discussion, we provide perspectives regarding the challenges and future directions of sepsis treatment.

2. RONS production and pathogenesis of sepsis

The pathogenesis of sepsis has not been well investigated, but uncontrollable inflammation and excessive RONS are thought to be two key factors that promote the progression of sepsis [51]. Therefore, an in-depth understanding of the mechanisms involved in immune response-induced inflammation and inflammation-induced RONS production is crucial for exploring sepsis pathogenesis and effective means of therapy [52]. In sepsis patients, the activated innate immune system is mediated by PRRs expressed on immune cells (e.g., macrophages and neutrophils) and non-immune cells (e.g., vascular endothelial cells) [8, 53]. PRRs include Toll-like receptors (TLRs), nucleotide-binding oligomerization domain (NOD)-like receptors (NLRs), retinoic acid-inducible gene-like receptors (RLRs), and C-type lectin receptors (CLRs) [51,54]. In sepsis, inflammation is mainly mediated by the TLR and NLR signaling pathways [55] (Fig. 2).

The TLR-mediated signaling pathway can be overactivated by PAMPs or DAMPs and lead to the overproduction of pro-inflammatory cytokines, such as interleukin-1 β (IL-1 β), tumor necrosis factor (TNF- α), and IL-6, causing mitochondrial dysfunction, such as an impaired respiratory chain, decreased ATP production, mitochondrial matrix swelling, and collapse of the membrane potential [56-59]. Eventually, a large amount of O_2^- is produced by electron leakage at the ubiquinone sites of mitochondrial respiratory chains complex I and complex III [55, 60-62]. Excessive O_2^{-} can be catalyzed by superoxide dismutase (SOD) to H_2O_2 , and the unstable oxygen bond of H_2O_2 can react with Fe^{2+} or another metal ion to form the powerful oxidant OH. [63,64]. Under inflammation, inducible nitric oxide synthase (iNOS) can be over-activated by pro-inflammatory cytokines [65] and cause excessive NO generation. Importantly, excessive O₂ can react with NO to generate highly reactive ONOO⁻. Excess RONS can cause cell apoptosis, necrosis, and lysis, which release high quantities of DAMPs [66]. These DAMPs are further recognized by TLRs and prompt inflammatory cytokine and RONS production, forming a vicious circle [51]. NLRs are another important type of receptor that induces excessive inflammation and RONS during sepsis. Under septic conditions, NLRP can form a multiprotein complex or inflammasome, which assembles with the adaptor protein apoptosis-associated speck-like containing a CARD domain (ASC) and caspase-1 [67-69]. After the NLRP inflammasome is activated, it can promote caspase-1-induced cleavage and maturation of pro-IL-1 β and pro-IL-18 to form IL-1 β and IL-18, which induce mitochondrial damage, such as TLR signals, and accelerated generation of highly reactive RONS [70]. Importantly, excessive RONS then induce the assembly and activation of NLRP3 inflammasomes.

Excessive inflammation and RONS cause damage to proteins, lipids, and nucleic acids, which can cause massive immune cell and endothelial cell injury and apoptosis, ultimately leading to an immunosuppressive state in the body [55,71]. Excessive inflammation and RONS also impair the activity of non-immune cells, such as endothelial cells [72]. The endothelium is a selective permeable barrier between the vascular wall and blood flow and one of the first protective barriers against external invasion [73]. In sepsis, excessive inflammation and RONS will increase endothelial cell permeability, leading to the leakage of fluids and proteins through the vascular wall, decreased tissue perfusion, hypovolemia, tissue edema, and eventually multiple organ failure [51,74]. Therefore, it is crucial to control inflammation and remove excessive RONS, breaking the cycle between inflammation and RONS. Preventing immune disorders caused by the damaged immune cells and protecting the function of non-immune cells (i.e., endothelial cells) is also necessary for the treatment of sepsis (Fig. 3). Notably, damaged tissues have greatly increased vascular permeability, which also greatly increase the selective enrichment of nanomaterials in damaged tissues and organs during sepsis. As a result, nanotherapy is very promising for the treatment of sepsis. Rationally designing nanomaterials can not only block PAMPs/DAMPs, but also eliminate ROS and decrease pro-inflammatory factors in damaged organs to achieve high efficiency treatment of sepsis.

3. The correlation between COVID-19 and sepsis

Sepsis is dominantly caused by an imbalance of host to infection, which is mainly induced by bacteria, viral, fungus [75]. The characteristics of viral sepsis and bacterial sepsis are extremely resemblance at the pathophysiological level. One of the manifestations of COVID-19 is fulminant disease characterized by sepsis [76]. For example, COVID-19 can cause uncontrolled inflammatory response characterized by

Table 1

Category	Nanomaterials	Classification of nanomaterials	Cargo	Biological target	Efficacy	Advantages of nanomaterials	Defects of nanomaterials	Refs
Nanomaterials Blocking PRR Signaling Pathways	SAuNCs	Au	/	LPS	Decreased inflammatory cytokines levels and prolonged survival time in sepsis mice	Effectively inhibited the activation of TLR4 signaling pathway	Potential toxicity, including specific toxicity such as gastrointestinal perforation and bleeding, to the GI route [23].	[24]
	MΦ-NPs	PLGA	/	LPS	Presented a low level of inflammatory cytokines and death rate in LPS- induced sepsis mice	Inherited the biological characteristics of macrophage cell membrane	The manufacturing process of biomimetic nanoparticle is complicated and expensive.	[25]
	Fe3O4 nanoparticles coated with macrophage membrane	Fe ₃ O ₄	/	LPS	Decreased ROS and inflammatory cytokines levels; increased SOD activity and survival time in sepsis mice	High selectivity and affinity to PAMPs and PRRs; increased stability	Magnetic iron oxide nanoparticles are toxic to many organs [26]	[27]
	MSN-PEI	Silica	/	cfDNA	Scavenging cfDNA; decreasing inflammatory cytokines levels; improving tissue and survival rate in sepsis mice	Exhibited high accumulation in inflamed tissue with negligible toxicity	Nanoparticles with higher charge density have toxicity to liver and kidney.	[28]
	TD-NT	High polymer materials	/	PAMPs/ DAMPs	Decreased inflammatory cytokines levels and improved tissue damage in sepsis mice	Captured DAMPs and PAMPs simultaneously	/	[29]
Nanomaterials for RONS Elimination	CeNPs	Ceria	/	Antioxidant enzyme	Decreased RONS and inflammatory cytokines levels; improved survival rate and protected liver from sepsis-induced injury	/	Large doses of ceria oxide nanoparticles may induce liver injury and oxidative stress.	[30]
			/		Improved diaphragmatic inflammation and function	/		[31]
			/		Inhibited inflammatory cytokines secretion; alleviated hepatic damage; increased survival rate	/		[32]
	CZ-NPs	Cerium and Zirconia	/	Antioxidant enzyme	Exhibited a decreased RONS levels and an improvement of tissues damage in sepsis mice	Exhibiting a stronger antioxidant activity	Large doses of ceria oxide nanoparticles may induce liver injury and oxidative stress	[33]
	6-AHA-CeNPs	6-AHA-modified cerium oxide	/	Antioxidant enzyme	Exerted antioxidant and anti-inflammatory capacity; increased survival rates; improved lung and liver tissues damage	Increasing stability and bioavailability of ceria nanozyme; decreasing toxicity	Large doses of ceria oxide nanoparticles may induce liver injury and oxidative stress.	[34]
	Co/PMCS	Co and porphyrin	/	Antioxidant enzyme	Presented a low level of RONS and an improvement of DNA damage, lipid peroxidation and inflammatory cytokines release	Exhibiting a stronger antioxidant activity	<u>/</u>	[6]
	2D-TMD	WS ₂ /MoSe ₂ /WSe ₂	/	/	Exerting antioxidant and anti-inflammatory effects; alleviating multiple tissues damage; increased survival rate	Scavenging various RONS	/	[35]
	Nanoparticles loaded with melatonin	PEG-b-PPS	Melatonin	/	Ameliorated inflammatory and oxidative injury	Increasing bioavailability and targeting of melatonin	/	[36]
			APS	/		/	/	[37]

(continued on next page)

Table 1 (continued)

Category	Nanomaterials	Classification of nanomaterials	Cargo	Biological target	Efficacy	Advantages of nanomaterials	Defects of nanomaterials	Refs
Inflammation Regulation	APS nanoparticles	Chitosan/ tripolyphosphate			Inhibited inflammatory cytokines secretion; improved the structure and function of cardiac tissue			
	Nanoparticles loaded with curcumin	Solid lipid	Curcumin	/	Exerted anti- inflammatory activity; increased survival rate	Protecting curcumin from chemical degradation; controlling sustained release; increasing bioavailability	Unpredictable gelation tendency and inherent low incorporation rates [38]	[39]
	Macrophage- derived NVs	Leukosomes	/	94 nm	Alleviated inflammation; prolonged survival time	Retaining the characteristics of	/	[40]
	MSC-derived NVs	MSCs	/	/	Exerting anti- inflammatory effects	Retaining the characteristics of source cells; selective in vivo distribution	/	[41]
	AuNPs	Au	/	/	Induced M2 macrophage polarization and exerted anti- inflammatory effects	/	/	[42]
	SPIONs	Fe ₂ O ₃	/	/	Alleviated inflammation and tissue damage in septic mice	Low toxicity and excellent biocompatibility	Oxidative stress and disturbance in iron homeostasis [43].	[44]
	Polymer nanoparticles	PLGA _{HI} -PEMA, PLGA _{HI} -PVA, PLGA _{LO} -PEMA, PLGA _{LO} -PVA, PLA- PEMA, PLA-PVA	/	/	Exerted strong anti- inflammatory effects	/	/	[45]
	TFMG	sFn	1	Endothelial cells	Alleviated vascular inflammatory response including decreased the vascular permeability, CAM expression, as well as inhibited the migration of circulating leukocyte to vascular endothelium.; increased survival rate; improved tissues damage	Avoiding the risk of bleeding; increasing efficacy	/	[46]
Multifunctional Nanomedicine	DOX-hyd-BSA NPs	BSA nanoparticles	DOX	Neutrophils	Alleviated inflammatory injury by inducing neutrophils apoptosis and inhibiting inflammatory cytokines secretion; increasing survival rate	Increasing targeting and cell uptake	/	[47]
	SQAd/VitE NPs	SQ nanoparticles	Ad/VitE	1	Exerted strong anti- inflammatory effects; improved survival rate, increased systolic blood pressure and decreased MSS in sepsis mice	Prolonging circulation time; reducing toxicity; increasing targeting and selectively; achieving anti- inflammatory and antioxidation combined therapy	/	[48]
	Nanoparticles loaded with CLP and TPCA-1	Biotin-PEG-b-PAE (-g-PEG-b-DSPE)-b- PEG-Biotin	CLP/ TPCA-1	/	Suppressed the peritoneal infection; protected vascular integrity; inhibited inflammatory response in septic mice	Increasing targeting and selectively; achieving the anti- inflammatory and antibiotic combined therapy; increasing the bioavailability of the cargo	/	[49]
	Nanoparticles loaded with SFX and TAC	PLGA	SFX/TAC	/	Decreased the secretion of proinflammatory cytokines; inhibited bacterial proliferation; improved survival rates of sepsis mice	Possessing excellent bioavailability, low systemic toxicity, and hemolysis ratio	/	[50]



Fig. 1. The scope and focus of this article. The pathogens caused by infection will enter the blood and excessively accumulate in the lesion foci, causing massive inflammation and releasing RONS through activation of the innate immune system. This will lead to blood vessel leakage and further organ dysfunction, and even death. Therefore, blocking activation of the immune system and eliminating the inflammation and RONS is extremely important in treating sepsis. Nanomaterials provide a breakthrough for the treatment of sepsis and can be divided into the following categories: blockade of PRR signaling pathways, nanomaterials for RONS elimination, nanomaterials for eliminating inflammation, and multifunctional nanomedicine.

prominent pro-inflammatory cytokine release in patients with severe COVID-19 [77,78]. Ivan Cekerevac et al. evaluated the concentrations of RONS, as well as the activity of enzymes of the antioxidative defense system in COVID-19 patients, and confirmed that the levels of O₂⁻, NO, and catalase activity are differently change in the different severity of COVID-19 infection [79]. Mireille Laforge et al. postulate neutrophils generated ROS that exacerbates the host immunopathological response, resulting in more severe disease and concluded that ROS generation are positive correlation with COVID-19 disease severity [80]. In short, Sepsis caused by COVID-19 can induce the overproduction of RONS and cytokines storm. These characteristics are accordant with bacterial sepsis. It is very difficult to distinguish between viral sepsis and bacterial sepsis. Recent studies have found that the distinct of viral and bacterial sepsis can only be distinguished by a complex method of whole blood

genomics [81]. The therapy of sepsis is mainly combining the supportive therapy with the interventions aimed at the root causes of pathogens. For example, the therapeutic of bacterial sepsis is the combine of antibiotic with supportive therapy, and the viral one is the unite of antiviral and supportive therapy [82]. Simple antibiotic treatment or antiviral treatment is often ineffective for sepsis. Supportive treatment is the key to restore the patient's immune system to treat sepsis. Supportive treatment is mainly aimed at the pathophysiological characteristics of the treatment, such as cytokine storm and oxidative stress damage. Therefore, the latest advances of nanotherapies for sepsis by regulating inflammatory signals and RONS are crucial referential value for the therapy of sepsis in COVID-19 patients.

4. Nanomaterials blocking PRR signaling pathways

As discussed above, PAMPs and DAMPs can induce the vicious cycle between the inflammatory response and RONS through the recognition of PRRs on immune cells or non-immune cell membranes [51,83]. The binding of PAMPs/DAMPs to PRRs is the trigger that activates the vicious cycle [84]. Thus, it is an effective approach to target signaling pathways with specific nanomaterials for the treatment of sepsis (Fig. 4).

PAMPs are mainly derived from Gram-negative bacteria, Grampositive bacteria, fungi, and viruses. Lipopolysaccharide (LPS) is the cell wall component of Gram-negative bacteria. It associates with serum LPS binding protein and binds to membrane receptor CD14 and accessory molecule MD2 to induce TLR4 signaling, producing proinflammatory factors and RONS. Therefore, reducing the binding capacity of LPS and TLR4-MD2 is an effective way to block the PAMP-PRR signaling pathway. The major toxic component of LPS is lipid A, and the affinity between lipid A and TLR4-MD2 receptor complexes is closely related to the molecular conformation (aggregation degree) of lipid A; the denser the aggregation degree of lipid A, the lower the affinity of LPS and TLR4-MD2. Recently, Liao et al. developed a sheet-like nanomaterial based on gold nanoclusters (SAuNCs) coated with a layer of short-chain alkanes (Fig. 4A) [24]. The short-chain alkanes on the surface of the SAuNC can bind to LPS and cause the aggregation density of lipid A to increase. As a result, SAuNC can effectively inhibit activation



Fig. 2. Pathological mechanism of sepsis. Under septic conditions, the invasion of immunogens (PAMPs and DAMPs) can overactivate the innate immune system through TLR- and NLR-mediated signaling pathways, causing massive inflammatory cytokine release. These inflammatory cytokines damage the mitochondrial respiratory chain, triggering RONS overproduction. Importantly, because RONS can induce cell apoptosis and reactivate PRR signaling pathways by inducing DAMP formation, it creates a vicious cycle between inflammation and RONS. Thus, inflammation and RONS are the two core factors in the pathological mechanism of sepsis.



Fig. 3. In sepsis, PAMPs/DAMPs cause the overproduction of RONS, which damage immune cells (macrophages and neutrophils) and non-immune cells (endothelial cells). In addition, RONS cause increased permeability of the endothelium, leading to PAMP/DAMP leakage across the vascular wall to other non-infected tissue, damaging normal cells and tissues and causing apoptosis.



Fig. 4. The nanomaterials including the Sheet-like Au nanomaterial (A), Biomimetic nanocomposites (B), Mesoporous silica nanoparticles with PEI(C), and Size-exclusive resin(D) blocking the binding of PAMPs/DAMPs and PRRs, thereby inhibiting the production of inflammation and RONS.

of the TLR4 pathway and reduce the generation of pro-inflammatory cytokines and RONS. In the LPS-induced septic mouse model, SAuNC significantly inhibits NF- κ B-dependent pro-inflammatory cytokines and chemokines. Decreased cytokines can inhibit RONS production, prolong

the survival of mice with sepsis.

The capture of PAMPs with specific nanoparticles is also an important method of blocking the PAMP-PRR signaling pathway [85,86]. As mentioned above, PAMPs usually include substances derived from a variety of different pathogens. Therefore, only blocking the LPS/PRR pathway cannot effectively treat sepsis caused by COVID-19. It has been extremely challenging to design nanomaterials that can directly capture a wide range of PAMPs. This bottleneck can effectively be solved using biomimetic nanocomposites, which are mainly prepared by coating specific nanomaterials with immune cell membranes. Immune cell membranes (e.g., macrophage cells) usually contain abundant TLRs, which can efficiently bind different kinds of PAMPs [87-89]. Furthermore, binding of PAMPs and the biomimetic nanocomposites cannot initiate activation of the PRR signaling pathway due to lack of downstream effectors, such as MyD88. A well-designed nanoparticle core can stabilize the immune cell membrane and prolong its activity in the physiological environment. For example, Thamphiwatana et al. developed a biomimetic nanoparticle consisting of a biodegradable poly acid) (PLGA) nanoparticle (lactic-co-glycolic core and macrophage-derived cell membrane (denoted MΦ-NPs) [25]. The hydrophilic surface glycans of the PLGA core can stabilize the macrophage cell membrane and improve the stability of MQ-NPs in serum. In addition, M Φ -NPs inherit the biological characteristics of the macrophage cell membrane and can effectively combine with PAMPs. Following the treatment of septic mice, MΦ-NPs decrease the concentrations of pro-inflammatory cytokines in the blood and spleen, inhibit RONS production, and improve survival in mice with sepsis. Recently, magnetic separation technology has been applied to biomimetic nanocomposites to further improve the efficiency of capturing PAMPs [90, 91]. For example, Shen et al. designed biomimetic nanocomposites composed of macrophage membrane and polyethyleneimine (PEI)-modified Fe₃O₄ nanoparticles (Fe₃O₄@MM NPs) [27]. The positively charged Fe₃O₄ cores can stabilize the macrophage membrane, increase the affinity for PAMPs, and achieve magnetic separation of PAMPs. Fe₃O₄@MM NPs effectively avoid activation of the PRR signaling pathway and reduce the secretion of TNF- α and IL-6 and other cytokines, ultimately improving the survival rate of sepsis mice.

DAMPs are endogenous molecules that can initiate and enhance the non-infectious inflammatory response [92,93]. For example, many DAMPs (e.g., cell-free DNA [cfDNA]) are released into the circulatory system after cell breakdown and necrosis in sepsis. DAMPs over-activate the TLR9-MyD88-NF-KB signaling pathway and induce the overproduction of inflammatory cytokines and RONS [92,94,95]. Therefore, blocking the DAMP-PRR signaling pathway is also an important aspect of inhibiting the host's overactive immune system. In theory, PEI has a positive charge and can effectively capture cfDNA. However, PEI also has strong cytotoxicity that cannot be ignored. The efficiency of PEI in blocking TLR9 activation and its toxicity both positively correlate with the charge density on PEI. To solve this dilemma, Dawulieti et al. prepared biodegradable mesoporous silica nanoparticles functionalized with PEI (MSN-PEI) [28]. The PEI of MSN-PEI can effectively prevent activation of the TLR9-MyD88-NF-kB signaling pathway by capturing cfDNA. Here, large-pore MSN served as the PEI carrier to reduce toxicity and maintain the capture efficiency of PEI. Accordingly, MSN-PEI administration effectively inhibited the secretion of TNF- α , IL-6, and MCP-1 in serum and the peritoneal fluid in cecal ligation and puncture (CLP)-induced septic mice. In addition, MSN-PEI alleviated multiple organ damage and markedly reversed the increase alanine aminotransferase (ALT), aspartate aminotransferase (AST), blood urea nitrogen, creatinine, creatine kinase, and total bilirubin levels in serum.

In sepsis patients, immune system dysfunction is largely the result of the synergistic effects of PAMPs and DAMPs [51]. Therefore, simultaneously blocking the DAMP- and PAMP-PRR pathways is more effective than blocking a single pathway [96]. In terms of molecular structure, most DAMPs and PAMPs contain hydrophobic groups and negatively charged groups. As for immune regulatory factors in the body, pro-inflammatory factors generally have a negative charge and anti-inflammatory factors a positive charge. On this basis, Shi et al. designed a linear-dendritic telodendrimer nanotrap (TD-NT) with multiple charges and hydrophobic moieties to capture PAMPs, DAMPs, and pro-inflammatory factors [29]. The TD-NTs can bind PAMPs, DAMPs, and inflammatory cytokines to reduce excessive inflammation during sepsis through interactions between multivalent electrostatic and hydrophobic domains. In addition, the molecular weight of cytokines and PAMPs/DAMPs is usually less than 30 kDa, smaller than most serum proteins (>50 kDa). The authors loaded the TD-NTs into 50-kDa hydrogel resins, which prefer capturing cytokines and PAMPs/DAMPs in serum.

5. Nanomaterials for RONS elimination

Under physiological conditions, redox homeostasis is preserved in the body by redox buffering systems. The system's delicate balance is preserved by antioxidant enzymes containing SOD, catalase, and glutathione peroxidase (GPx) [55]. In sepsis, excessive RONS far exceed the scavenging ability of antioxidant enzymes in vivo and can cause oxidative stress in the body, which in turn produces more RONS [57,97, 98]. Therefore, it is necessary to rely on the administration of exogenous antioxidants to maintain the body's redox balance. However, traditional antioxidants present many shortcomings, such as severe side effects, rapid clearance, and low stability and bioavailability, which limits their clinical application. Recent studies have found that nanomaterials have great potential in the treatment of sepsis by directly removing RONS or by delivering traditional antioxidants, which not only overcome the shortcomings of traditional antioxidants, but also improve clinical efficacy [99] (Fig. 5).

5.1. Nanozymes and single-atom catalysts

Natural antioxidant enzymes in the body exert excellent ROS scavenging activity [100]. However, their practical application is not satisfactory for two reasons. First, natural enzymes are unstable under physiological conditions and easily degraded by proteolytic enzymes [101]. Second, these natural antioxidant enzymes usually only eliminate one type of ROS and sepsis is caused by multiple RONS. Thus, only eliminating one kind of RONS cannot achieve the desired therapeutic effect and it is necessary to find antioxidant enzyme mimics that effectively scavenge multiple RONS. Notably, some nanomaterials are inherently antioxidant, which can decrease the levels of multiple RONS in the body by mimicking antioxidant enzymes. Nanomaterials with enzyme-mimetic activity are nanozymes [101–103]. Due to the high catalytic activity, good stability, low manufacturing cost, and ability to mimic multiple antioxidant enzymes [102,104], nanozymes have great advantages in removing excess RONS during sepsis. Currently, cerium oxide (ceria) nanozyme and single-atom catalyst (SAC) nanozyme have been developed and exhibit excellent therapeutic effects in sepsis.

On the nanoscale, ceria has stronger catalase or SOD enzyme-like activity, and the Ce³⁺/Ce⁴⁺ surface ratio is closely related to the antioxidant enzyme-mimetic activity [105,106]. For example, ceria nanozyme has high Ce⁴⁺ state surface atoms that behave as catalase-mimics (Ce⁴⁺ + H₂O₂ + 2OH· \rightarrow O₂ + 2Ce³⁺ + H₂O), whereas the ceria enzyme with high amounts of Ce³⁺ acts as a SOD-mimic (Ce³⁺ + 2H⁺ + O₂² \rightarrow H₂O₂ + Ce⁴⁺) [107,108]. In addition, the ceria nanozyme can eliminate OH· through a redox reaction ($Ce^{3+} + 2OH \rightarrow 2Ce^{4+} + H_2O$) [109]. Therefore, ceria nanozyme can be applied in the treatment of sepsis by eliminating ROS (Fig. 5A). Selvaraj et al. prepared ceria nanozymes to effectively eliminate excessive ROS in sepsis, with a distinct reduction in NO generation and iNOS expression observed in septic mice after treatment with ceria nanozymes [30]. The ceria nanozymes also decreased the expression of cyclooxygenase-2 (COX2) and the levels of pro-inflammatory cytokines (TNF- α , IL-6, and IL-1 β) in macrophages from septic mice. Notably, COX-2 could induce the synthesis of prostaglandin E2 (PGE2), which stimulated pain and inflammation. The ceria nanozyme significantly improved survival and protected the liver from sepsis-induced injury. Similarly, other studies have also shown that ceria nanozymes can reduce functional sepsis-induced injury to the liver and



Fig. 5. Some of nanomaterials can eliminate excessive RONS in vivo through mimicking multiple antioxidant enzyme, including Ceria nanozymes(A) and Singleatom catalysts(B). Except that, TMDs nanosheets can effectively scavenge various RONS to treat sepsis(C), as well as nanomaterial can serve as carriers delivering antioxidant to inflammation site(D).

diaphragm through their antioxidant and anti-inflammatory activities [31,32].

However, the application of ceria nanozyme is limited by its potential toxicity and low stability in sepsis. Therefore, current studies have tried to improve the antioxidant activity of ceria nanozymes, as well as reduce its potential toxicity. For example, Min Soh et al. synthesized 2nm ceria-zirconia (CZ) nanozymes to serve as enhanced antioxidants for sepsis treatment [33]. The CZ-nanozymes have a higher Ce^{3+}/Ce^{4+} ratio and faster conversion from Ce^{4+} to Ce^{3+} than ceria nanozymes due to the addition of Zr to the ceria nanozyme. Therefore, CZ-nanozymes exhibit stronger antioxidant activity for scavenging ROS than ceria nanozymes. In addition, the small size (2 nm) gives CZ-nanozymes lower toxicity than ceria nanozymes, which have a size of 3-4 nm. Consequently, CZ-nanozymes markedly reduce inflammatory injury in major tissues, including the liver, lungs, cecum, stomach, and small intestine in mice with CLP-induced sepsis. Cerium oxide nanozymes can also increase the ROS-eliminating activity and reduce toxicity to a certain extent by improving their stability under physiological conditions. Jeong et al. fabricated polyethylene glycol (PEG)ylated ceria nanozymes with 6-aminohexanoic acid (6-AHA) as a surface stabilizer [34]. The 6-AHA-PEG stabilizer increases the colloidal stability of ceria nanozymes in the physiological environment and prevents surface adsorption of the biological components, including phosphate ions and serum proteins. Notably, phosphate ions preferentially bond to surface Ce³⁺ or Ce⁴⁺ sites to form CePO₄-like complexes on the ceria nanozymes and prevent redox cycling between Ce³⁺ and Ce⁴⁺. In addition, the PEGylated formulation increases the circulating blood half-life and cellular uptake, avoiding rapid clearance and cytotoxicity. Therefore, PEGylated 6-AHA-ceria nanozymes possess excellent ROS scavenging and anti-inflammatory capacity.

The catalytic active centers of many nanozymes and natural enzymes are generally coordinated metal centers. SACs are catalysts in which the catalytic active center of the metal is embedded in a catalytic carrier with a single atomic scale. For nanozymes, the catalytic activity comes from the metal located on the surface of the nanozymes. Most of the metal atoms are buried under the surface and cannot be reached by the reactants. SACs can ensure that all metal active centers play a catalytic role and usually have higher catalytic activity and less potential cytotoxicity [110,111]. Recently, Cao et al. developed an enzyme-mimicking SAC (Co/PMCS) by atomically dispersing co-porphyrin centers in nitrogen-doped carbon-supported nanomaterials for sepsis treatment (Fig. 5B) [6]. Co/PMCS could scavenge O_2^{-} by simulating SOD, eliminate H₂O₂ by simulating catalase and GPx, and remove OH· via the oxidative-reduction cycle. Furthermore, it could eliminate NO· via coordination of the co-porphyrin center. Co/PMCS significantly decreased the level of RONS and further reduced the secretion of inflammatory cytokines, such as IL-6 and TNF- α . The survival rate and damage to multiple organs in mice with sepsis also improved, which suggests that Co/PMCS can effectively protect cells from oxidative stress and inflammatory damage.

5.2. RONS nanoscavengers

In addition to nanozymes, RONS nanoscavengers also play important roles in antioxidant therapy by directly reacting with excessive RONS [112]. Recently, two-dimensional (2D) transition-metal dichalcogenide (TMD) nanosheets were proposed as novel RONS scavengers that can be applied in the treatment of sepsis [35]. Compared to conventional antioxidants, 2D-TMD nanosheets can effectively remove various RONS with low cytotoxicity, good biocompatibility, structural stability, and durability of action [113,114]. Notably, Yim et al. synthesized three kinds of 2D-TMD nanosheets (WS2, MoSe2, and WSe2) functionalized with poly(ɛ-caprolactone) (PCL)-b-PEG for the treatment of sepsis (Fig. 5C) [35]. The amphiphilic PCL-b-PEG contributes to the exfoliation of 2D-TMD nanosheets in water. These nanosheets undergo oxidation reactions with multiple RONS and exhibit a superior capacity for continuously removing H2O2, O2, OH, and NO. The WS2 TMD nanosheets exhibit stronger ROS scavenging capacity than the molybdenum (Mo)-based TMDs ($WS_2 > WSe_2 > MoSe_2$). Accordingly, these TDMs significantly decrease RONS in inflammatory cells, suppress the secretion of inflammatory cytokines, and have no effects on anti-inflammatory cytokines. In the septic mouse model, these TDMs

significantly improve survival and tissue damage in the lungs, liver, and spleen. Similarly, the WS_2 nanosheet has the best therapeutic effects in sepsis treatment, which may be attributed to their long retention in the body.

5.3. Nanocarriers loaded with antioxidant

Sepsis is a disease closely related to oxidative stress. In theory, treatment of sepsis with antioxidants is a promising strategy. However, the therapeutic potential of many antioxidants (e.g., natural antioxidants, endogenous antioxidants, synthetic organic antioxidants) is restricted by factors such as solubility, stability, and low bioavailability (e.g., poor gastrointestinal absorption). Recently, some novel nanocarriers were developed for the delivery of antioxidants to treat sepsis [115,116], which has higher bioavailability and efficacy in clinical practice. Such nanocarriers provide many benefits over conventional formulations, including superior solubility and stability, extended half-life, improved epithelial permeability and bioavailability, enhanced tissue targeting, and minimal side effects. Recently, Chen et al. developed a ROS-responsive polymeric nanocarrier of melatonin via the self-assembly of diblock copolymers of PEG and poly (propylene sulfide) (PPS) (Fig. 5D) [36]. PPS undergoes an oxidative conversion from hydrophobic to hydrophilic. As a result, the nanoparticles become swollen and disassemble when exposed to H2O2, and then release the encapsulated drugs. The melatonin nanocarriers significantly alleviate sepsis-induced liver injury by decreasing the hepatic lipid peroxidation level, tissue neutrophil accumulation, and inflammatory cytokine levels. The mechanism of melatonin activity was associated with decreased phosphorylation of the NF-kB p65 subunit, which could down-regulate the expression of inflammatory mediators, including IL-6, IL-1β, COX-2, iNOS, and NLRP3. In particular, the therapeutic effects of the melatonin nanocarriers were superior to free melatonin alone. Eventually, the liver function in septic mice improved and was accompanied by a decrease in the plasma levels of ALT and AST after treatment with the melatonin nanocarriers.

6. Inflammation regulation

Inflammation imbalance is the most critical mechanism responsible for the onset and progression of sepsis, which underlies the whole pathological process [94]. The inflammation response in sepsis can be divided into two different but overlapping stages. In the initial stage of sepsis, activated immune cells, such as macrophages and neutrophils, secrete a large amount of pro-inflammatory cytokines, causing excessive inflammation and damage by RONS [117-119]. In the later stages of sepsis, a prolonged or intense low-inflammatory state may lead to immune effector failure, eventually leading to immunosuppression. Therefore, inflammation regulation is necessary for the treatment of sepsis. Steroidal or non-steroidal anti-inflammatory drugs are often used for anti-inflammatory treatment, but these drugs are not effective for the treatment of sepsis. The latest anti-TNF α or anti-IL-1 monoclonal antibodies and other drugs have limited therapeutic effects on sepsis. The main reasons for the poor effect of these drugs in sepsis are non-specific distribution, short drug half-life, and low bioavailability. The development of well-designed nanomedicine creates some new prospects for the treatment of sepsis, as nanomaterials can be specially designed to adjust the expression of pro-inflammatory and anti-inflammatory molecules and can be given priority to enter target tissues from the site of administration, which can solve the disadvantages of off-target organ side effects and systemic toxicity. Different types of nanomaterials have been developed to control inflammation in sepsis, including nanocarrier devices for anti-inflammatory drugs, anti-inflammatory nanomaterials, and nanomaterials that actively target inflammatory cells (Fig. 6).

6.1. Nanocarriers with anti-inflammatory drugs

The therapeutic effects of traditional anti-inflammatory drugs are usually unsatisfactory in the practical applications [19,20]. The



Fig. 6. The balance between pro-inflammation cytokines (TNF- α , IL-3, IL-6, IL-12, MIF and INF- γ) and anti-inflammation cytokines (IL-4, IL-10 and TGF- β) are significantly important in sepsis(A). The disordered homeostasis in sepsis can be regulated by nanomaterials through a variety of ways. It can be divided into three categories: (B) nanocarriers(chitosan derivatives, solid lipid nanoparticles, biomimetic nanoparticles) with anti-inflammation drugs can efficiently delivery anti-inflammation drugs (APS and Curcumin) into inflammation site; (C) nanoparticles with anti-inflammation capacity, including Au nanoparticles, SPIO nano-particles, PLA/PLGA nanoparticles and macrophage/MSC nanovesicles; (D) nanomaterials targeting inflammatory cells (neutrophils and endothelial cells) could decrease the production of inflammation cytokines.

structure and physicochemical properties of anti-inflammatory drugs result in poor water solubility, low bioavailability, and difficulty with absorption. Drug delivery by nanoparticles has gradually become a suitable strategy that avoids the pharmacokinetic limitations of traditional drug formulations (Fig. 6B) [120-123]. For example, astragalus polysaccharide (APS), an important natural anti-inflammatory drug, has been demonstrated to exert anti-inflammatory actions by regulating the TLR4-NF-κB signaling pathway. However, APS does not absorb well through the intestinal tract, and only a small amount is absorbed by the paracellular route. Xu et al. prepared APS nanoparticles using chitosan derivative (chitosan/tripolyphosphate) as the drug carrier [37]. The APS nanoparticle had better therapeutic effects than free APS alone, including a significant reduction in inflammatory cytokine levels and protection of the structure and function of cardiac tissue. Similarly, the clinical application of curcumin is limited due to its hydrophobic nature, rapid degradation, and low bioavailability. Wang et al. encapsulated curcumin in solid lipid nanoparticles, which not only protected the curcumin from chemical degradation, but also contributed to sustained drug release [39]. Consequently, curcumin-loaded nanoparticles exert a superior therapeutic effect compared to free curcumin, including inhibition of inflammatory cytokines, increased anti-inflammatory cytokines, and improved survival of septic mice.

Recent studies have also prepared biomimetic nanoparticles to further increase the bioavailability of anti-inflammatory drugs by coating the cell membrane on the surface of nanoparticles or incorporating proteins derived from the plasma membrane into nanoparticles [121,40,41,124]. Biomimetic nanoparticles can effectively avoid being cleared by the reticuloendothelial system and circulate in the body longer than ordinary nanomaterials [40,41,124,125].

6.2. Anti-inflammatory nanoparticles

Some nanomaterials intrinsically exert anti-inflammatory activity, such as gold nanoparticles (AuNPs), superparamagnetic iron oxide nanoparticles (SPIONs), and poly (lactic acid) (PLA)/PLGA nanoparticles (Fig. 6C). Taratummarat et al. demonstrated that AuNPs can promote the polarization of M1 macrophages into M2 macrophages, induce the secretion of anti-inflammatory cytokines, and inhibit the expression of inflammatory cytokines [42]. Macrophages have been broadly classified into two groups: M1 macrophages that secrete pro-inflammatory cytokines, and M2 macrophages that secrete anti-inflammatory cytokines [126,127]. AuNPs improve the survival rate of septic mice by alleviating systemic inflammation [42]. Similarly, Xu et al. showed that SPIONs can enhance secretion of anti-inflammatory cytokine IL-10 by activating autophagy in macrophages, alleviating inflammation in septic mice [44]. Therefore, the application of these metal nanomaterials offers a new avenue for the treatment of sepsis. Recently, Casey et al. developed cargo-less PLA/PLGA nanoparticles to investigate their anti-inflammatory effects on septic mice [45]. The PLA/PLGA nanoparticles were hydrolyzed in the body to produce lactic acid, which could regulate the immune response [128,129]. The polymer nanoparticles not only significantly inhibited the secretion of inflammatory cytokines, but also influenced the maturation status of bone marrow-derived dendritic cells (BMDCs).

Some cells in the body, such as immune cells and stem cells, have anti-inflammatory effects. The biomimetic nanoparticles based on these cells also inherit the physiological properties of merocytes and perform specific functions, such as targeting inflamed tissues, and possess antiinflammatory activity [124,130]. Macrophage-derived nanovesicles (NVs) and mesenchymal stromal cell (MSC)-derived NVs have been developed for the treatment of sepsis. Because they retain the anti-inflammatory phenotypes of macrophages and MSCs, they have been shown to significantly suppress the release of inflammatory cytokines and increase the levels of anti-inflammatory cytokines, ultimately improve sepsis-induced inflammatory damage [40,41].

6.3. Nanomaterials targeting inflammatory cells

The inflammatory response of sepsis is a very complex process that involves the innate immune system, the adaptive immune system, and endothelial system. In the innate immune system, phagocytosis-related cells, such as macrophages and neutrophils, play critical roles in removing pathogens [131]. However, inflammation can disrupt the neutrophil death program (apoptosis) to prolong neutrophils longevity, and the number of neutrophils rapidly increases in sepsis [117]. These neutrophils secrete massive amounts of inflammatory cytokines, which in turn cause neutrophil migration dysfunction. Subsequently, the deleterious accumulation of these dysfunctional neutrophils could cause tissue injury within remote vital organs [131,132]. Therefore, induction of neutrophil apoptosis is also an important aspect in alleviating sepsis-induced inflammatory damage (Fig. 6D). Recently, Zhang et al. synthesized pH-responsive bovine serum albumin (BSA) doxorubicin (DOX) nanoparticles (DOX-hyd-BSA NPs) via a pH-labile hydrazone bond. Neutrophils specifically bind to BSA because of the upregulated Fcy receptors of neutrophils [47]. As a result, DOX-hyd-BSA NPs can effectively target neutrophils and deliver DOX into neutrophils. In addition, the acidic environment in neutrophils triggers the fracture of a pH-labile bond between albumin and DOX, releasing DOX from DOX-hyd-BSA NPs into neutrophils. Notably, DOX is a highly effective chemotherapeutic agent that can bind DNA bases to kill neutrophils [133]. The DOX-hyd-BSA NPs significantly inhibit the release of inflammatory cytokines from neutrophils and increase the survival of septic mice.

Endothelial cells play important roles in maintaining homeostasis in the body by coordinating anti-inflammatory, anti-coagulant, and antiadhesive states [134]. However, excessive inflammation and RONS could damage endothelial cells, leading to their dysfunction and structural damage under septic conditions [74]. Therefore, inhibiting the inflammatory response of endothelial cells is also a crucial aspect of treating sepsis (Fig. 6D). Notably, recombinant activated protein C (APC), a component of the natural anticoagulant system, has been applied in the treatment of sepsis due to its potent anti-inflammatory activity for endothelial cells [135,136], but the severe bleeding tendency with APC due to the decomposition of procoagulant co-factors Va and VIIIa prevent its clinical application. Recently, Lee et al. designed a protein nanocage (TFMG) composed of short ferritin (sFn), y-Carboxvglutamic Acid of Protein C (PC-Gla), PAR-1-activating peptide (TRAP), and a matrix metalloproteinase (MMP)-2 cleavage site, where sFn acts as a skeleton structure, inserting PC-Gla at the C-terminus and TRAP in the N-terminus [46]. The MMP-2 cleavage site was inserted between the sFn and PC-Gla to allow PC-Gla to escape from nanocomposites when they reach the MMP-activating sites. In particular, TRAP could activate PAR-1 to enhance Gla-ERPC-PAR-1-dependent signal transduction and switch from a pro-inflammatory to cytoprotective role in endothelial cells [135,137,138]. Because LPS can induce the activation and release of MMP-2 in endothelial cells, PC-Gla is released from nanocages at the site of inflamed endothelium after administration of TFMG. Subsequently, PC-Gla and TRAP bond to the ERPC and PAR-1 receptors, respectively, and then inhibit the release of inflammatory cytokines from leukocytes. Cell adhesion molecule (CAM) expression on the surface of endothelial cells promotes the adhesion and migration of leukocytes to inflamed endothelium. Notably, the TFMG protein nanocage significantly alleviates the vascular inflammatory response, with decreased vascular permeability and CAM expression, as well as inhibited migration of circulating leukocytes to the vascular endothelium. The survival rates in the TFMG-treated group were reported to be significantly higher than those in TFG (without the MMP-2 cleavage site) and free PC-Gla-TRAP groups.

7. Multifunctional nanomedicine

The course of sepsis is often the result of a combination of several

factors that influence and interact with one another [10,139]. Therefore, therapies that only intervene with a single factor will compromise therapeutic effects and cannot effectively treat sepsis. Multifunctional nanomedicine can simultaneously deliver multiple therapeutic agents to interfere with multiple pathogenic factors. Thus, multifunctional nanomedicines to treat sepsis have great advantages and prospects for application (Fig. 7).

The vicious circle between inflammation and RONS is a critical factor in the pathogenesis of sepsis [55,140]. Therefore, simultaneous intervention for inflammation and RONS can be an effective combination therapy. Recently, Dormont et al. prepared squalene (SQ)-based multidrug nanoparticles to simultaneously inhibit inflammation and scavenge RONS [48]. The nanoparticles were loaded with endogenous immunomodulator adenosine (Ad) and antioxidant α -tocopherol (vitamin E [VitE]) (SQAd/VitE NPs) (Fig. 7A and B). Ad, an endogenous purine, exerts anti-inflammatory effects by binding to the Ad receptor, but its efficacy is limited by the rapid clearance and severe side effects associated with off-target activation of the Ad receptor. VitE is an antioxidant that can eliminate excessive ROS in the body, but it is water-insoluble and generally binds to low-density lipoproteins (LDLs). The SQAd/VitE NPs not only improve the efficacy of these two drugs by prolonging circulation time, reducing toxicity, and improving targeting, but also exert the advantages of the combined drugs. Meanwhile, the interaction between neutrophils and the vascular endothelium results in an impaired endothelial barrier and increased permeability under excessive inflammation. Thus, SQAd/VitE NPs can selectively aggregate in areas of inflammation and endothelial injury. For the treatment of sepsis, SQAd/VitE NPs exert better therapeutic effects, including RONS scavenging and reducing secretion of pro-inflammatory cytokines (e.g., TNF- $\!\alpha$ and IL-6), in septic mice compared to exposure to free Ad/VitE, SQAd NPs or SQVitE NPs. Furthermore, SQAd/VitE NPs increase the generation of anti -inflammatory cytokine IL-10 and reduce malondialdehyde (MDA) levels, which is an indicator of lipid peroxidation in mice with sepsis. The SQAd/VitE NPs eventually improve the survival rate, increase systolic blood pressure, and decrease the murine sepsis score (MSS) in septic mice. Overall, SQAd/VitE NPs provide an effective treatment by blocking the pathological cross-talk between oxidative stress and inflammation.

Inflammation is the body's natural response to harmful stimuli [141], but excessive inflammation leads to dysfunction of the host's immune system [142,143]. Although anti-inflammatory drugs can reduce inflammation in patients with sepsis, they also lower the host's defenses and induce overactivation of pathogens and constant reproduction [20,139]. Thus, combined anti-inflammatory and antibacterial drugs can further enhance the treatment effect on sepsis. For example, Zhang et al. synthesized a pH/enzyme-responsive amphiphilic block

copolymer consisting of biotinylated PEG-b-poly (β-amino ester)-b-PEG grafted with PEGylated lipid (Biotin-PEG-b-PAE(-g-PEG-b-D-SPE)-b-PEG-Biotin) via Michael-type polymerization (Fig. 7 B-D) [49]. In particular, PAE (tertiary amines and ester bonds) and PEG-DSPE (phosphoester bonds) were pH-sensitive and enzymeresponsive in the amphiphilic block copolymer. The copolymer could self-assemble into micelles and encapsulate an antibiotic (ciprofloxacin [CLP]) and an anti-inflammatory agent (2-[(aminocarbonyl)amino]-5-(4-fluorophenyl)-3-thiophenecarboxamide [TPCA-1]). ICAM-1 antibodies bind to the surface of micelles. Therefore, the polymer nanoparticles (CIP + TPCA-1-NPs-anti-ICAM-1) could selectively accumulate in activated endothelial cells via the activity of the ICAM-1 antibody. Subsequently, the ester bonds of PAE and the phosphoester bonds of PEG-DSPE would break in the infectious microenvironment (low pH and abundant bacterial lipase enzymes). In the septic mouse model, CIP + TPCA-1-NPs-anti-ICAM-1 significantly suppresses peritoneal infection and protects vascular integrity. In addition, CIP + TPCA-1-NPs-anti-ICAM-1 effectively inhibits the inflammatory response of septic mice, reducing the leukocyte count and the levels of pro-inflammatory cytokines. Furthermore, CIP + TPCA-1-NPs-anti-ICAM-1 exhibits better therapeutic effects than free CIP, CIP-NPs -anti-ICAM-1, and CIP-NPs-anti-ICAM-1 by not only inhibiting bacterial proliferation and an inflammatory response, but also significantly increasing the survival rates of septic mice. Similarly, Yang et al. synthesized PLGA nanoparticles encapsulated with the antibiotic sparfloxacin (SFX) and anti-inflammatory immunosuppressant tacrolimus (TAC) [50]. The multidrug nanoparticles exhibited excellent bioavailability, low systemic toxicity, and an improved hemolysis ratio compared to free drugs. The γ 3 peptide (NNQKIVNLKEKVAQLEA) attached to the surface of nanoparticles (SFX-TAC-y3-PLGA nanoparticles) is a 17-mer linear peptide derived from the natural ligand of ICAM-1, which helps the nanoparticles selectively target inflamed endothelial cells. For the treatment of sepsis, SFX-TAC-y3-PLGA nanoparticles selectively accumulate in the infectious and inflamed lung, and then inhibit bacterial proliferation and decrease the secretion of pro-inflammatory cytokines. Accordingly, SFX-TAC-y3-PLGA nanoparticle treatment prevents cytokine storm and improves survival rates in septic mice.

8. The limitation of nanomaterials

The nanotherapies of sepsis are increased for the past few years, and present the exciting therapeutic effect and the great progresses. However, the issues of nanomaterials that involves toxicity and off-target was also brought forward and caught attentions.

Except the therapeutic effect, another crucial problem of nanotherapies of clinical translation is the toxicity. The toxicity of



Fig. 7. Multifunctional nanomedicine integrates multiple functions for treating sepsis, including (A) RONS elimination, (B) antibacterial, (C) anti-inflammatory, and (D)targeting.

nanomaterials involves many aspects, which is closely related with their composition, size, surface charge and distribution in vivo. The nanomaterials for sepsis therapy dominantly divided to lipid-based nanomaterials, polymer nanomaterials and inorganic nanomaterials. Lipidbased nanomaterials generally have many advantages, like low toxicity, easy preparation, biocompatibility. Currently, lipid-based nanotherapies are the most commonly FDA-approved nanomedicines (such as for the therapy of ovarian cancer, fungal infection, and leukemia) [144,145]. Noteworthily, Sphingomyelin and cholesterol liposomal nanomaterials (Combioxin, SA) for toxin neutralization has been completed phase I clinical trials for the treatment of pneumonia sepsis [145]. Polymer nanomaterials generally have good biocompatible and can be biodegradable in vivo. Nanocarriers based polymers can achieve precise control of drug loading and release kinetics by regulation of their composition, stability, responsiveness, and surface charge. However, polymer nanoparticles easily cause increased aggregation in vivo, and have the risk of potential toxicity. Inorganic nanomaterials for sepsis treatment primary including cerium oxide, Au nanoparticle, iron oxide, 2D-TMD (WS₂, MoS₂), and silica. Particularly, iron oxide and MoS₂ are all composed of elements already in the human body. MoS₂ is already extensively applied to cancer diagnosis and therapy research [146]. Iron oxide has already authorized by FDA for nuclear magnetic contrast agent and the treatment of anemia [145]. These two materials are usually considered to have low toxicity. However, the toxicity of inorganic nanomaterials extremely caught attentions, especially the nanomaterials contained the elements of heavy mental. The distribution, metabolism, and toxicological action of the inorganic nanomaterials require in-depth study. In addition to the composition of nanoparticles, the size of nanoparticles also affects their toxicity. It has been reported that nanoparticles with small size are more likely to cause cytotoxicity. Nanoparticles with diameter less than approximately 10 nm can rapidly eliminated by the kidneys, which might affect the kidneys, and diameter greater than 200 nm may activate the complement system [147]. The surface of nanoparticles also influence toxicity. Cationic nanoparticles maybe caused cytotoxicity by damaged the cytomembrane. Specially, it has been reported the potential toxicity of nanomaterials about cardiorenal- and hepato-toxicity. For example, Abderrahim Nemmar et al. concluded that iron oxide nanoparticles can caused thrombosis, cardiac oxidative and DNA damage through acute intravenous administration [148]. There are also reports that titanium dioxide nanoparticles and others nanoparticles are harmful to kidney [149,150]. Tungsten trioxide nanoparticles and iron oxide nanoparticles can cause liver toxicity in mice [151,152]. There are many nanoparticles that can also damage the liver [153,154]. In general, the toxicity and therapeutic effects of nanomaterials are generally dose-dependent. Therefore, the dosage of nanomaterials needs to be carefully selected, and a balance should be reached between the toxicity of nanomaterials and the therapeutic effect. In addition, some researchers believe that concerns about the toxicity of nanomedicine have been exaggerated. It does not mean it is dangerous just because a material is nanoscale. In fact, nanoparticles were existed since the birth of the earth, for example, the nanoparticles were naturally existing in the organism, volcanic ash and ocean spray [155]. Moreover, human activity also produced excessive nanomaterials, such as dust and fume.

The current nanomaterials targeting for sepsis treatment mainly derived from the passive targeting (ERP) and specific targeting of modified ligands. The concept of ERP derived from tumors where the vasculature system is heterogeneous and abnormal in tumor site. ERP can cause the nanoparticles to accumulate in tumors [156]. Massive studies have reported that up to 10–15% of the injected NP accumulates at the tumor site compared with 0.1% of the free drug. However, Stefan Wilhelm et al. reported that only 0.7% of the nanoparticle injection dose reached the tumor [157]. Very recently, Lauren et al. argued that non-standard calculations was used by Stefan Wilhelm may produce misleading and biased results [158]. After the correction, the enrichment rate of nanoparticles in the tumor site ranged from 2.65 to 7.97%,

much higher than the level of 0.7%. The oxidative stress and inflammatory cytokine storm of sepsis can severely damage the vascular endothelial system. Theoretically, nanoparticles should have better passive targeting in sepsis than in tumor. Nevertheless, future research must rigorously evaluate the metrics to quantify delivery and distribution. Currently, many nanotherapies are efficacious to treat sepsis in animal model, it may be not suitable for humans. There are great differences in the pathology and physiology of sepsis between humans and animals. These nanotherapies may be off-target in the treatment of human sepsis [159]. Lack of understanding of the differences between species may lead to the failure of nanotherapies in the treatment of sepsis in humans.

9. Summary and prospects

As the world continues to experience the effects of COVID-19, we present the latest advances in nanotherapy for sepsis with the aim of contributing to the treatment of this new, severe coronary disease. Here, we summarized recent advances in understanding the pathological mechanism of sepsis and the potential application of nanomedicines for sepsis treatment. Nanotherapies are promising for sepsis treatment, and the nanomaterials mediating RONS and the inflammatory response have achieved previously unattainable therapeutic effects in sepsis.

Despite the rapid advances, further optimization of nanomaterials is urgently needed to treat sepsis in a more comprehensive and effective manner. First, the pathogenesis of sepsis is the result of multiple factors, so single therapeutic agents are currently insufficient. However, the proposed multifunctional therapy is still in its infancy. Developing appropriate nanoparticles to meet the multifunctional requirements for sepsis treatment has become a crucial research focus. Second, ideal nanomaterials should not only have low toxicity and excellent bioavailability and stability, but they should also be able to easily target infectious tissues. The physical and chemical properties of nanomaterials are closely related to the particle size, surface charge, and surface modification [21]. Therefore, it is necessary to continuously optimize the preparation of nanoparticles. Third, inflammation in sepsis is caused primarily by the activation of TLRs and the NLR-mediated signaling pathway. However, recent studies on nanomaterials have focused mainly on blocking activation of the TLR signaling pathway. Yet, blocking the NLR-mediated signaling pathway can also inhibit activation of the innate immune system. Therefore, it is promising to design nanomaterials that block the NLR-mediated signaling pathway or both the TLR and NLR-mediated signaling pathways for the treatment of sepsis. Finally, many bacteria develop multidrug resistance and develop immune escape mechanisms in response to the host immune response and the abuse of antibiotic therapy [160-162]. Particularly in the immunosuppressive stage of late sepsis, there is a very complicated and contradictory relationship between regulating the level of inflammation and killing pathogens. Currently, most nanomaterials are focused on the first stage of sepsis (excessive activation of the inflammatory response) and are rarely involved in the late stage of sepsis. Nanomedicines should have great advantages and prospects through carefully designed multifunctional nanomaterials to balance the complex relationship between the late-stage regulation of inflammation and the elimination of pathogens. The development of new and effective nanomedicines for therapies based on inflammation and RONS will achieve a significant breakthrough in the treatment of sepsis [163,164]. The efficacy of nanomaterials therapy should be assessed in clinical trials.

Declaration of competing interest

The authors declare no conflict of interest, financial or otherwise.

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Abbreviation

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ASC	Apoptosis associated speck-like containing a CARD domain
ALT	Aminotransferase
AST	Aspartate aminotransferase
APS	Astragalus polysaccharide
AuNPs	Gold nanoparticles
APC	Activated protein C
Ad	Adenosine
BSA	Bovine serum albumin
BMDCs	Bone-marrow-derived dendritic cells
CAM	Cell adhesion molecule
CLP	Ciprofloxacin/cecal ligation and puncture
COX2	Cyclooxygenase-2
CLRs	C-type lectin receptors
COVID-19	9 Coronavirus disease 2019
cfDNA	Cell free DNA
DAMPs	Damage-associated molecular patterns
DOX	Doxorubicin
GPx	Glutathione peroxidase
ICU	Intensive care units
iNOS	Inducible nitric oxide synthase
IL-16	Interleukin-1ß
LDLs	Low-density lipoproteins
LPS	Lipopolysaccharide
MSC	Mesenchymal stromal cell
MMP	Matrix metalloproteinase
MDA	Malondialdehyde
MSS	Murine sensis score
MSN	Mesonorous silica nanonarticles
Mo	Molyhdenum
MODS	Multiple organ failure syndrome
NOD	Nucleotide-binding oligomerization domain
NIRe	NOD-like recentors
NVc	Nanovesicles
DAMDe	Pathogen-associated molecular patterns
DC Cla	v Carbovyglutamic Acid of Protein C
	Pattern recognition recentors
	Pattern recognition receptors
DEI	Poly (lactic-co-grycolic acid)
PLI DCF2	Prostaglandin E2
PGEZ	Pitostagianum Ez
PEG	Polyetilytelle glycol
	Poly (legic acid)
PLA	Poly (lactic actu)
PPS	Poly (propyrelie suffice)
RUNS	Reactive oxygen and indogen species
RLKS	Relinoic acid-inducible gene-like receptors
KUS CIDC	Reactive oxygen species
SIKS	Systemic inflammatory response syndrome
SOD	Superoxide dismutase
SAC	Single-atom catalysis
SFII	
SQ	Squalene
SFX	Spariloxacin
SPIONS	Superparamagnetic iron oxide nanoparticles
TAC	I acrollmus
TNF-α	I umor necrosis factor- α
TMDs	Transition-metal dichalcogenides
TD-NT	Telodendrimer nanotrap
TLRs	Toll-like receptors

	VitE	Vitamin/α-tocopherol
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6-AHA 6-aminohexanoic acid

2D Two-dimensional

Author contributions

All authors listed have made a substantial, direct, and intellectual contribution to the work.

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