

## Article

# Aggregation and Oligomerization Characterization of $\beta$ -Lactoglobulin Protein Using a Solid-State Nanopore Sensor

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**Abstract:** Protein aggregation is linked to many chronic and devastating neurodegenerative human diseases and is strongly associated with aging. This work demonstrates that protein aggregation and oligomerization can be evaluated by a solid-state nanopore method at the single molecule level. A silicon nitride nanopore sensor was used to characterize both the amyloidogenic and native-state oligomerization of a model protein  $\beta$ -lactoglobulin variant A ( $\beta$ LGa). The findings from the nanopore measurements are validated against atomic force microscopy (AFM) and dynamic light scattering (DLS) data, comparing  $\beta$ LGa aggregation from the same samples at various stages. By calibrating with linear and circular dsDNA, this study estimates the amyloid fibrils' length and diameter, the quantity of the  $\beta$ LGa aggregates, and their distribution. The nanopore results align with the DLS and AFM data and offer additional insight at the level of individual protein molecular assemblies. As a further demonstration of the nanopore technique,  $\beta$ LGa self-association and aggregation at pH 4.6 as a function of temperature were measured at high (2 M KCl) and low (0.1 M KCl) ionic strength. This research highlights the advantages and limitations of using solid-state nanopore methods for analyzing protein aggregation.

**Keywords:** protein aggregation; solid-state nanopore;  $\beta$ -lactoglobulin; protein oligomerization; protein volume



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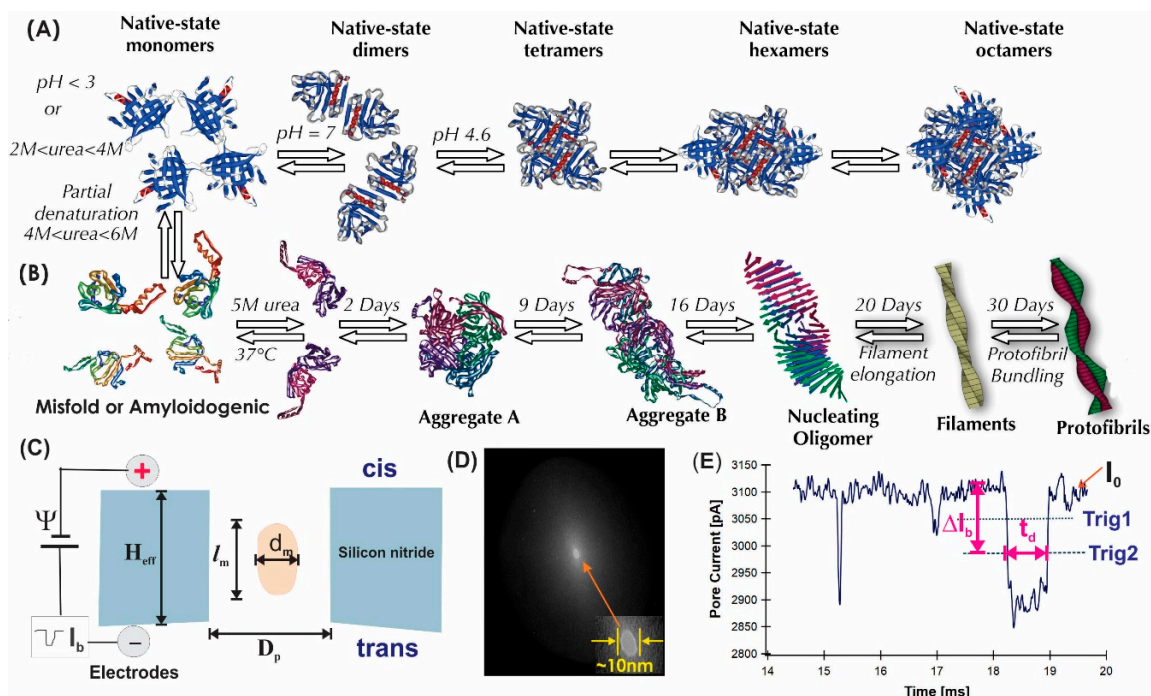
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## 1. Introduction

Protein aggregation is linked to many chronic and devastating neurodegenerative human diseases [1,2] and is strongly associated with aging [3]. There are over 20 diseases associated with pathological protein aggregation including Alzheimer's, Parkinson's, and type II diabetes [4–7]. Protein aggregation is also a major concern for protein-based biopharmaceuticals because it can potentially affect drug activity and trigger allergic responses in patients [8]. It is challenging to characterize aggregated proteins due to their heterostructure forms [9] such as dimer, tetramer, hexamer, octamer, filaments, etc. Protein aggregation can be evaluated with ensemble methods such as analytical ultracentrifugation, field flow fractionation [8,10], size-exclusion chromatography, gel electrophoresis, and dynamic light scattering [11,12]. These ensemble techniques provide average protein aggregation states but no information on each protein molecule. As such, they rely on the deconvolution of signals to resolve the aggregate size. Protein aggregation has also been measured by single molecule methods such as atomic force microscopy (AFM) [11]. However, AFM measurements require a protein sample to be on a solid surface, and this requirement could influence the protein aggregation state.

This study employs a silicon nitride nanopore-based sensor for characterizing protein aggregation under varied solution conditions. Solid-state nanopore based devices [13–16], previously used for analyzing single molecules of DNA [17–27], RNA [28–34], proteins [35–56], protein–DNA complexes [57–69], as well as protein oligomerization [69] and interaction with other analytes [70,71]. For this study, a chief advantage of the solid-state nanopore method is that the measurement of protein aggregation can be performed under solution conditions very close to the native environment, while varying temperature, pH, and salt concentration at the single molecule level. This approach aims to provide a method for more the accurate and detailed understanding of protein aggregation.

In this study, a cow's milk protein,  $\beta$ -lactoglobulin variant A ( $\beta$ LGa MW = 18.3 kDa/monomer), serves as our model protein. There are many possible species of  $\beta$ LGa amyloid particles present physiologically. The species that are relevant to this work are shown in Figure 1A,B. The  $\beta$ LGa protein aggregation species can be classified into two categories: one is the native-state oligomers (top panel), the other is the amyloidogenic aggregates (bottom panel). When  $\beta$ LGa is at a native state (no denaturing agent present in solution), it can present as monomers, dimers, tetramers, hexamers, and octamers (Figure 1A). When  $\beta$ LGa is incubated in 5 M urea (partially denatured condition) at 37 °C, depending on the incubation time (Figure 1B), it can be in the form of a native-state monomer, partially denatured monomer, completely unfolded monomer, forming dimers through disulfide bonding, and further forming tetramers (Aggregate A), octamers (aggregate B), amyloid filaments (a species of amyloid with diameter of 3–6 nm and length <100 nm), and amyloid fibrils ~10 nm in diameter and >100 nm in length. Interest in  $\beta$ LGa aggregation and its amyloid growth has been driven by basic science, by the importance of  $\beta$ LGa to the dairy and food processing industries, and by finding the mechanism of protein aggregation related to diseases. Detecting these  $\beta$ LGa aggregation and oligomerization species under different solution conditions will allow us to evaluate the advantages and limitations of the solid-state nanopore method.



**Figure 1.** (A)  $\beta$ -lactoglobulin native-state oligomerization. (B) Amyloidogenic aggregation of 1 mg/mL (55  $\mu$ M)  $\beta$ LGa incubated in 5 M Urea, 10 mM phosphate buffer at pH 7.0 and 37 °C. (C) An illustrated nanopore experimental setup for characterization of proteins in globular shape. (D) A TEM image of a ~10 nm diameter silicon nitride nanopore used in this work for Day-1 and Day-10 samples. (E) An example event recorded from a Day-10 sample of  $\beta$ LGa in 2 M KCl and 5 M Urea.

The aim of this study was to demonstrate that a solid-state nanopore device can be used to characterize the species (Figure 1A,B) involved in  $\beta$ LGa protein native-state oligomerization and amyloid formation at the single molecule level under near-native conditions. Linear and circular dsDNA as reference molecules of known dimensions were also measured in the same nanopores used to estimate the  $\beta$ LGa aggregation states.

To validate the nanopore approach, we used a combination of atomic force microscopy (AFM) and dynamic light scattering (DLS) techniques in parallel to measure the  $\beta$ LGa protein samples. The strategy here was to allow for the overlapping capability of AFM and DLS to connect all the ranges of the particle sizes. AFM is less-suited for small, partially denatured proteins, but resolves medium-to-large aggregates and fibrils quite well. Conversely, DLS provides good information about small-to-medium-sized aggregates, but those signals become lost once large particles such as protofibrils are present in the sample.

## 2. Materials and Methods

### 2.1. The Principle of Detecting Protein Aggregation by Nanopore Technology

The principle of nanopore characterization of protein aggregation is illustrated in Figure 1C. The main component of a solid-state nanopore sensing system is a single nanometer pore fabricated in silicon nitride membrane that separates two salt solution-filled chambers, the only connection of which was via the electrolyte solution inside the nanopore. A TEM image of a  $\sim 10$  nm diameter silicon nitride nanopore is shown in Figure 1D. Briefly, when a voltage  $\Psi$  is applied through a pair of AgCl electrodes across the membrane with a nanopore submerged in a salt solution, a stable open pore current,  $I_0 = \Psi / R_{\text{pore}}$ , can be established by the flowing of ions and measured ( $R_{\text{pore}}$  is the pore resistance). When charged protein molecules are present in the *cis* chamber, the electric field of right polarity near the nanopore can capture the protein molecules and drive them through the pore to the *trans* side, one at a time, if the right size of nanopore is selected. A protein molecule translocating through a nanopore partially blocks the flow of ions that would increase the pore resistance (decrease the pore current) and produce a current blockage pulse or event, as shown in Figure 1E.

Previous studies with particles of various shape and size that translocate through various sizes of pores [72–75] have shown that the instantaneous current blockage amplitude  $\Delta I_b(t)$  is approximately proportional to the instantaneous excluded volume  $\Lambda(t)$  of the passing DNA or protein molecule, as well as the applied voltage  $\Psi$ , as described in Equation (1) [18,76]

$$\Delta I_b \simeq I_0 \frac{\gamma \Lambda_{\text{Pr}}}{V_{\text{po}}} = \left( \frac{\gamma \sigma \Lambda_{\text{Pr}}}{H_{\text{eff}}^2} \right) \Psi \quad (1)$$

Here, by Ohm's law,  $I_0 = \Psi / R_{\text{pore}} = (\sigma A_{\text{po}} / H_{\text{eff}}) \Psi$ ,  $\sigma$  is the solution conductivity (see Appendix A for all  $\sigma$  used in this work),  $\gamma$  is a shape factor of a protein molecule [45,46],  $V_{\text{po}} = A_{\text{po}} \times H_{\text{eff}}$  is the nanopore effective volume of pore area  $A_{\text{po}}$  (determined by TEM image) and an effective thickness,  $H_{\text{eff}}$ . The  $H_{\text{eff}}$  can be determined by the slope ( $\sigma A_{\text{po}} / H_{\text{eff}}$ ) of  $I_0$  vs.  $\Psi$  curve (see Appendix B Table A1 for all  $H_{\text{eff}}$  determined in this work) and is usually larger than its physical thickness because of the access resistance of a nanopore. By using a standard molecule that has a known diameter, dsDNA for example, we can calibrate the effective thickness,  $H_{\text{eff}}$  (or  $V_{\text{po}}$ ), of the nanopore under the experimental solution conditions. By measuring the relative current drop,  $\Delta I_b / I_0$ , the product of the volume and shape factor,  $\gamma \Lambda_{\text{Pr}}$ , of a translocating protein can be estimated. For example, a tetrameric aggregate will have approximately 4 times larger relative current drop than a monomer,  $\beta$ LGa,  $\Delta I_b / I_0$  (tetramer)  $\approx 4 \Delta I_b / I_0$  (monomer).

In this study, we focus on measuring the relative current drop amplitudes,  $\Delta I_b / I_0$ , to probe the  $\beta$ LGa protein native-state oligomerization and amyloid assembly. We first present nanopore characterization of  $\beta$ LGa protein aggregation at different stages under amyloid formation conditions (in 5 M urea at 37 °C, Figure 1B). DLS was used to measure and verify the number of aggregates and AFM was used to measure and calibrate the dimensions of the  $\beta$ LGa aggregates from the same stages. Furthermore, we demonstrate

the characterization of  $\beta$ LGa protein native-state oligomerization (Figure 1, top panel) as a function of solution temperature at biological salt concentration (0.1 M KCl) and high salt concentrations (2 M KCl).

## 2.2. Materials and Sample Preparation

### 2.2.1. Nanopore Experiment

The fabrication and characterization of silicon nitride nanopores have been described in detail in our previous work [20,76,77]. The thickness of the silicon nitride nanopores fabricated was estimated to be 10 to 30 nm, depending on the ion species used [77–79]. The diameters of the nanopores used in this work were from 8 to 16 nm, selected based on the size of the protein aggregates to be measured. The parameters of the 3 nanopores used in this report are listed in the Supporting Information (S-I-Table S1). A pair of Ag/AgCl electrodes is embedded in each PDMS (polydimethylsiloxane) chamber [20].

Current blockage event traces were recorded with an Axopatch 200B (Molecular Devices, San Jose, CA, USA) integrated system in event-driven mode with its low-pass Bessel filter set at 10 kHz. The recorded events were sorted, and the current drop amplitudes ( $\Delta I_b$ ) and dwell times ( $t_d$ ) were extracted using a home-made MATLAB program. The events analyzed here were those that had the current dropping below both Trig 1 and Trig 2, then came back above Trig 1 (Figure 1E) with  $t_d > 35 \mu\text{s}$ . Trig 1 was set just below the baseline noise level and Trig 2 was set at approximately half the average peak height where  $t_d$  was measured. For those events with  $t_d < 35 \mu\text{s}$ , no meaningful parameters can be extracted due to the 10 kHz filter. A total of 200 data points before and after each event were also recorded to determine the open pore current for the event. When using a low-pass Bessel filter set to 10 kHz, pulse widths shorter than 100  $\mu\text{s}$  maintain accurate time durations ( $t_d$ , fwhm), but the pulse heights are attenuated. Pulse height attenuation for short  $t_d$  ( $< 100 \mu\text{s}$ ) was corrected, as described in our previous publication [23]. The applied voltage was set at  $\Psi = 120 \text{ mV}$  for all nanopore measurements, unless otherwise mentioned.

### 2.2.2. Data Analysis

As illustrated in Figure 1E, the current blockage amplitude,  $\Delta I_b$ , was calculated by averaging the current during the dwell time,  $t_d$ , corresponding to the data points below the Trig 2. Each event is represented by one point in plots of  $\Delta I_b$  vs.  $t_d$  in this paper. The peak values of  $\Delta I_b$  and  $t_d$  were obtained from fitting their histograms to Gaussians (or multi exponentials for  $t_d$ ). Their errors were half the width of the fits.

### 2.2.3. AFM and DLS Measurements

The sample preparation, as well as AFM and DLS measurements have been described in detail in Giurleo et al. [11]. Below, we summarize them briefly.

**AFM.** The  $\beta$ LGa samples were imaged on mica surfaces by a MultiMode Scanning Probe Microscope (Digital Instruments, New York, NY, USA) with a TESP tip in tapping mode. To obtain better adhesion of protein aggregates to the mica surface, chemical surface modification with (3-aminopropyl) triethoxysilane was implemented, as described in Giurleo et al. [11].

**DLS.** Fluctuations of scattered light intensity were measured using a homodyne technique. Round borosilicate glass cuvettes (Kimble Glass, Düsseldorf, Germany) were used for all DLS measurements. For the DLS study (details in S-II), 250  $\mu\text{L}$  of incubated sample was placed in a clean dry cuvette. Twenty correlation functions were measured sequentially for 30 s apiece for the incubated sample. The cuvette chamber was held at a constant temperature of 37  $^{\circ}\text{C}$ .

### 2.2.4. Chemicals

$\beta$ LGa, urea, KCl, and dibasic and monobasic sodium phosphate were purchased from sigma-Aldrich.  $\beta$ LGa at a concentration of 1 mg/mL ( $\sim 55 \mu\text{M}$ ) was incubated in 5 M urea,



10 mM phosphate buffer at pH 7.0 and 37 °C. The Day-1, Day-10, and Day-29 samples were measured on day 1, days 10–11, and days 29–31 of incubation, respectively. The reference DNA molecules, 2.7 kbp linear dsDNA, and 5.4 kbp circular dsDNA were purchased from New England Biolabs.

### 3. Results and Discussion

#### 3.1. LGa Aggregation and Amyloid Formation

##### 3.1.1. Nanopore Measurements of $\beta$ LGa Incubated on Day 1 and Day 10

In a solution of 2 M KCl with 5 M urea and 10 mM phosphate buffer at pH 7.0 and 20 °C, at applied voltage  $\Psi = 120$  mV, the  $\sim 10$  nm nanopore shown in Figure 1D had an open pore current  $I_0 = 3.1$  nA. The incubated  $\beta$ LGa protein of Day-10 and freshly prepared Day-1 samples were diluted 550 times to a final concentration of  $\sim 100$  nM. The Day-10 sample was added to the cis chamber and the current blockage events were observed in a few minutes. After about ten thousand events were recorded, the cis chamber solution was flushed out several times until no events were observed, and the freshly made Day-1 sample was added to the cis chamber and measured.

The traces from the Day-10 sample (Figure 2A) show more current drop events with a larger current drop ( $\Delta I_b$ ) and longer durations ( $t_d$ ) compared to those from the Day-1 sample (Figure 2B). Both the Day-10 and Day-1 samples show variations in the current drop amplitudes,  $\Delta I_b$ , and time durations,  $t_d$ , suggesting that several species of  $\beta$ LGa protein existed in the solution. For the Day-10 sample, the event distribution plot of  $\Delta I_b$  versus  $t_d$  in Figure 2C shows two main clusters of events, labeled as cluster-1 and cluster-3. The histogram of  $\Delta I_b$  on the right axis (Figure 2C) shows a broad peak for the cluster-3 events, indicating a wide range of  $\beta$ LGa aggregate sizes. For the Day-1 sample, the event distribution plot shows three clusters of events (Figure 2D). We selected each cluster of events and fit their  $\Delta I_b$  (Figure 2E) and  $t_d$  (Figure 2F,G) histograms with Gaussians. The fitting peak values and their fitting errors are listed in Table 1.

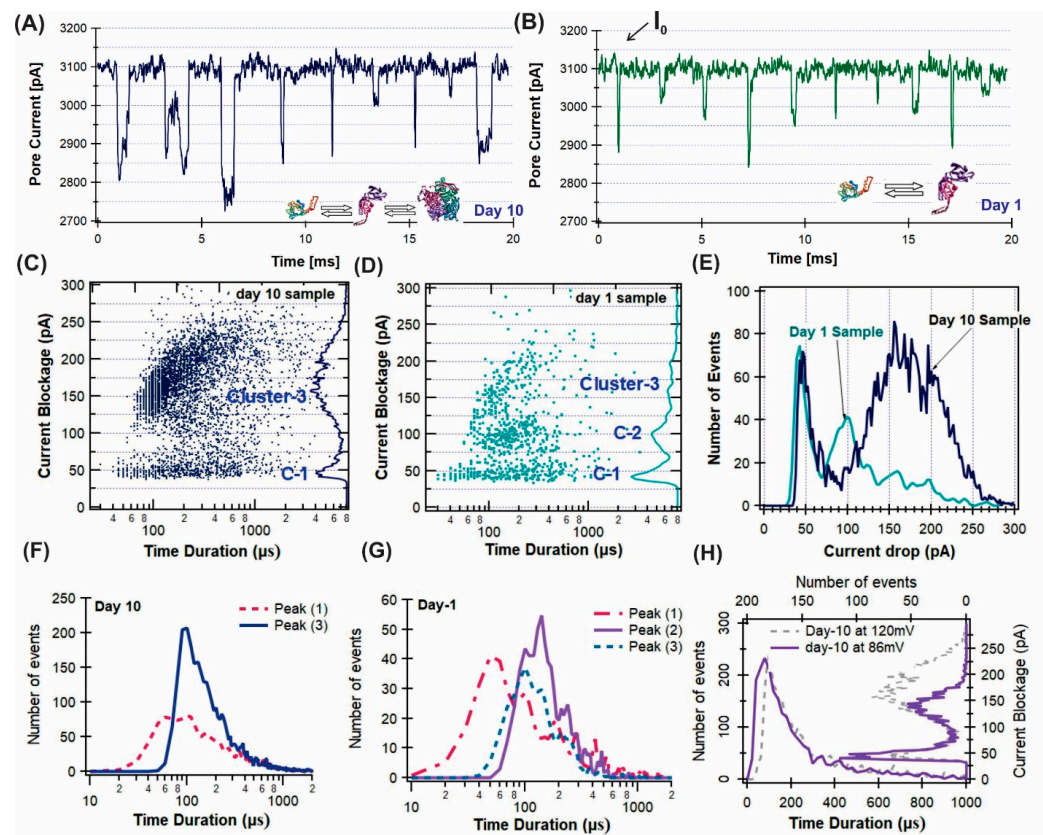
Through examining the number of events vs.  $\Delta I_b$  distribution for the Day-1 and Day-10 samples (Figure 2E), the ratio of cluster-3/cluster-1 was found to be approximately 12 times larger for the Day-10 than the Day-1 sample, indicating the  $\beta$ LGa species in cluster-3 had grown significantly during the 10-Day incubation. Further analysis shows that the ratio of the current blockage amplitude peak values of cluster-3 to cluster-1 were  $\Delta I_{b,3}/\Delta I_{b,1} \sim 3.6$  for both the Day-10 and Day-1 samples. Therefore, we conclude that the cluster-3 events represented the  $\beta$ LGa protein aggregates that had grown in the incubated sample.

Assuming the shape factors,  $\gamma$ , in Equation (1) were the same, the excluded volume of cluster-3 events was about four times larger than the cluster-1 events, or  $\Lambda_{Pr}^3/\Lambda_{Pr}^1 \sim 4$ , so the aggregation number was most likely to be  $n = 4$  (Aggregate A in Figure 1). The cluster-2 events in the Day-1 sample,  $\Delta I_b^2/\Delta I_b^1 \sim 2$ , were most likely representing the dimers formed through the disulfide bonding of the partially unfolded  $\beta$ LGa protein in 5 M urea.

As a control measurement, the current blockage events were also recorded at a lower voltage,  $\Psi = 86$  mV (Figure 2H). The peak values of the  $\Delta I_b$  histogram for the cluster-3 events show that  $\Delta I_b = 137 \pm 17$  pA at  $\Psi = 86$  mV, which is smaller compared to  $\Delta I_b = 171 \pm 31$  pA at 120 mV (Figure 2H, right panel), which was consistent with Equation (1). No big difference was observed for the  $t_d$  recorded at the two voltages (Figure 2H, bottom panel). The small changes in  $\Delta I_b$  for the cluster-1 events as well as the time,  $t_d$ , for the two voltages were consistent with the results reported in our earlier studies [39]; that cluster-1 was most likely representing events from the partially unfolded  $\beta$ LGa monomer translocation through a nanopore, together with the events of collision and noise spikes.

##### 3.1.2. $\beta$ LGa Incubated on Day 29

A larger nanopore ( $\sim 16$  nm diameter, Figure 3e) was used for this experiment. A circular relaxed 4.4 kbp dsDNA, as a reference molecule, was measured first. The cis chamber solution was washed (not completely; some DNA molecules were still present) then the  $\beta$ LGa Day-29 sample was added.

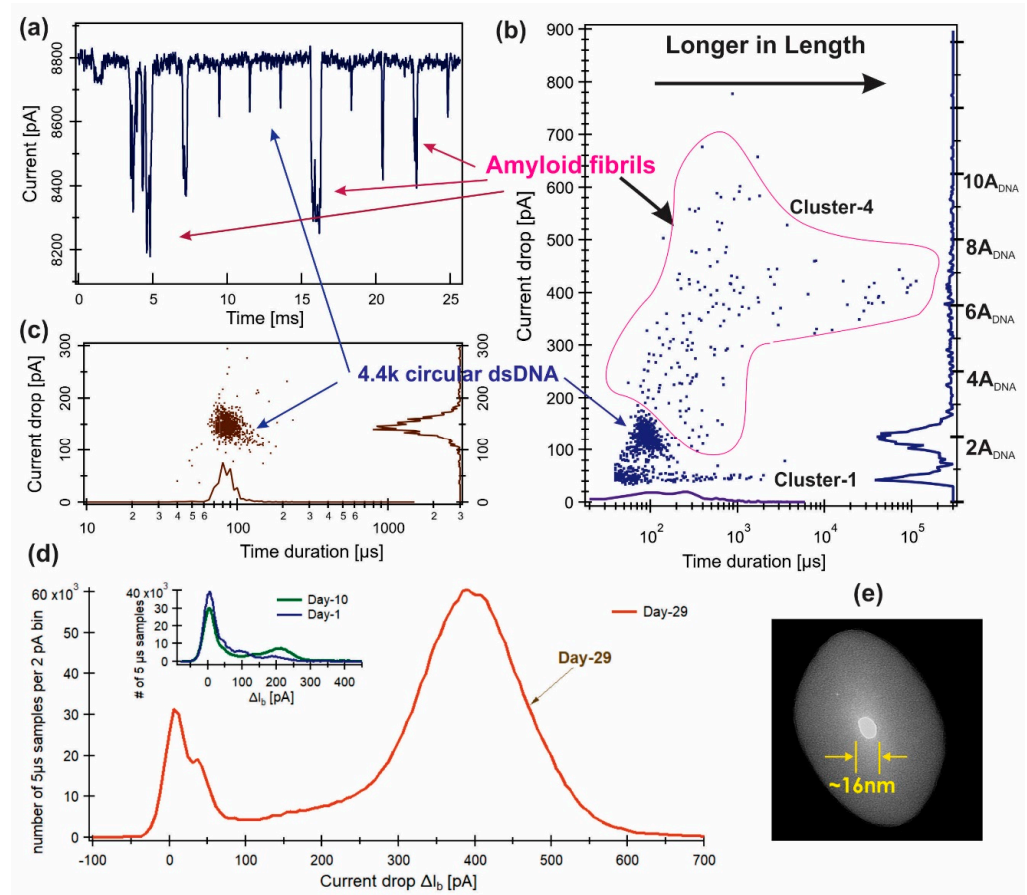


**Figure 2.** Ionic current traces recorded for Day-10 (A) and Day-1 (B) samples measured in a  $\sim 10$  nm pore (TEM image is shown in 1D) in 2 M KCl, 10 mM Phosphate, 5 M Urea, at pH 7. The inserts are possible forms of  $\beta$ LGa species. The open pore current was  $I_0 \sim 3.1$  nA at 120 mV. Event distributions displayed as current blockage amplitude,  $\Delta I_b$ , versus time duration,  $t_d$ , for the samples from Day 10 (C) and Day 1 (D). (E) Histograms of  $\Delta I_b$  for the Day-10 and Day-1 samples. Time duration histograms of  $t_d$  for the two clusters of events for the Day-10 sample (F) and three clusters of events for the Day-1 sample (G). (H) Comparison of  $\Delta I_b$  and  $t_d$  histograms at  $\Psi = 120$  mV and 86 mV.

**Table 1.** Summary of parameters measured and estimated for the Day-1, Day-10, and Day-29 samples.

	Method	Parameters	Cluster-1	Cluster-2	Cluster-3	Cluster-4
Day1	nanopore	$\Delta I_b$ (pA)	$44 \pm 6$ pA	$98 \pm 14$ pA	$158 \pm 29$ pA	
		$t_d$ ( $\mu$ s)	$66 \pm 28$ $\mu$ s	$127 \pm 35$ $\mu$ s	$105 \pm 33$ $\mu$ s	
Day10	nanopore	$\Delta I_b$ (pA)	$44 \pm 6$ pA		$171 \pm 31$ pA	
		$t_d$ ( $\mu$ s)	$130 \pm 65$ $\mu$ s		$142 \pm 41$ $\mu$ s	
	AFM	Diameter (nm)			$1.5 \pm 0.2$ nm	$4.0 \pm 0.2$ nm
		Length (nm)			$11.4 \pm 5.0$ nm	$80 \pm 10$ nm
		Area ( $\text{nm}^2$ )			$1.77$ $\text{nm}^2$	$12.6$ $\text{nm}^2$
Day29	nanopore	$\Delta I_b$ (pA)	42 pA			$400 \pm 100$ pA
		$t_d$ ( $\mu$ s)	$\sim 50$ $\mu$ s			$200$ $\mu$ s $\sim 2$ ms
		Area ( $\text{nm}^2$ )				$10.7$ $\text{nm}^2$
		Volume $\gamma \Lambda_{Pr}$	$37.0$ $\text{nm}^3$			$*352$ $\text{nm}^3$
	AFM	Diameter (nm)			1.5 nm	$4 \pm 0.2$ nm
		Length (nm)			$15 \pm 5$ nm	$80 \pm 10$ nm
		area			$1.77$ $\text{nm}^2$	$12.6$ $\text{nm}^2$
		volume			$26.5$ $\text{nm}^3$	$1004.8$ $\text{nm}^3$
dsDNA	nanopore	$\Delta I_b$ (pA)	$145 \pm 10$ pA			$122 \pm 11$ pA
		$I_0$ (nA)	9.51 nA			8.8 nA
		$t_d$ ( $\mu$ s)	$84 \pm 4$ $\mu$ s			
		Diameter (nm)				1.5 nm
		area				$1.8$ $\text{nm}^2$

\*352  $\text{nm}^3$  of volume  $\gamma \Lambda_{Pr}$  is the volume of the portion of a long  $\beta$ LGa filament inside the pore.



**Figure 3.** Nanopore measurements for the “mature” amyloid fibrils (Day 29 of incubation) at conditions 1.6 M KCl, 20% Glycerol, 10 mM Tris-EDTA buffer at pH.7. (a) Typical events, (b) event distribution, (c) dsDNA control, (d) instantaneous time distribution of blockade current,  $\Delta I_b$ , over all events selected (including 200 samples or 1 ms before and after each event). The same plot for the Day-1 and Day-10 samples from Figure 2 are shown in the insert. (e) The ~16 nm diameter pore nanopore used for the experiment. All measurements were performed at  $\Psi = 120$  mV.

For the Day-29 sample, events of very large  $\Delta I_b$  ( $>200$  pA) and long  $t_d$  (~ms) were observed (Figure 3a) and the distribution of the events is shown in Figure 3b. For the circular dsDNA, the event distribution plot (Figure 3c) shows that the most probable peak values were at  $\Delta I_b = 145 \pm 10$  pA and  $t_d = 84 \pm 4$  μs. The  $\Delta I_b$  histogram for the Day-29 sample (Figure 3b) had a major peak at  $\Delta I_b \sim 122 \pm 11$  pA. This was most likely a peak of mixed 4.4 kbp circular dsDNA together with some events from the βLGa Day-29 sample that could not be resolved. The Day-29 cluster-1 events (Figure 3b) had a current blockage peak value of  $\Delta I_{b,1} \approx 42$  pA and  $t_{d,1} \approx 50$  μs, which was similar to the cluster-1 events observed for the Day-10 and Day-1 samples. The Day-29 cluster-4 for the large current drop events (Figure 3b) had a very broad distribution of  $\Delta I_b$ , centered at  $\Delta I_{b,4} \approx 400 \pm 100$  pA. The Day-29  $t_{d,4}$  histogram at the bottom axis shows multiple time scales spanning from 200 μs–2 ms (see Figure S1 in S-I for details). The plot of the Day-29 instantaneous time distribution of the blockade current,  $\Delta I_b$ , over all the selected events (Figure 3d) shows more clearly a large current drop peak at  $\Delta I_{b,4} \approx 400 \pm 100$  pA. The same plots for the Day-10 and Day-1 data from Figure 2 are in the insert to show the major peak values.

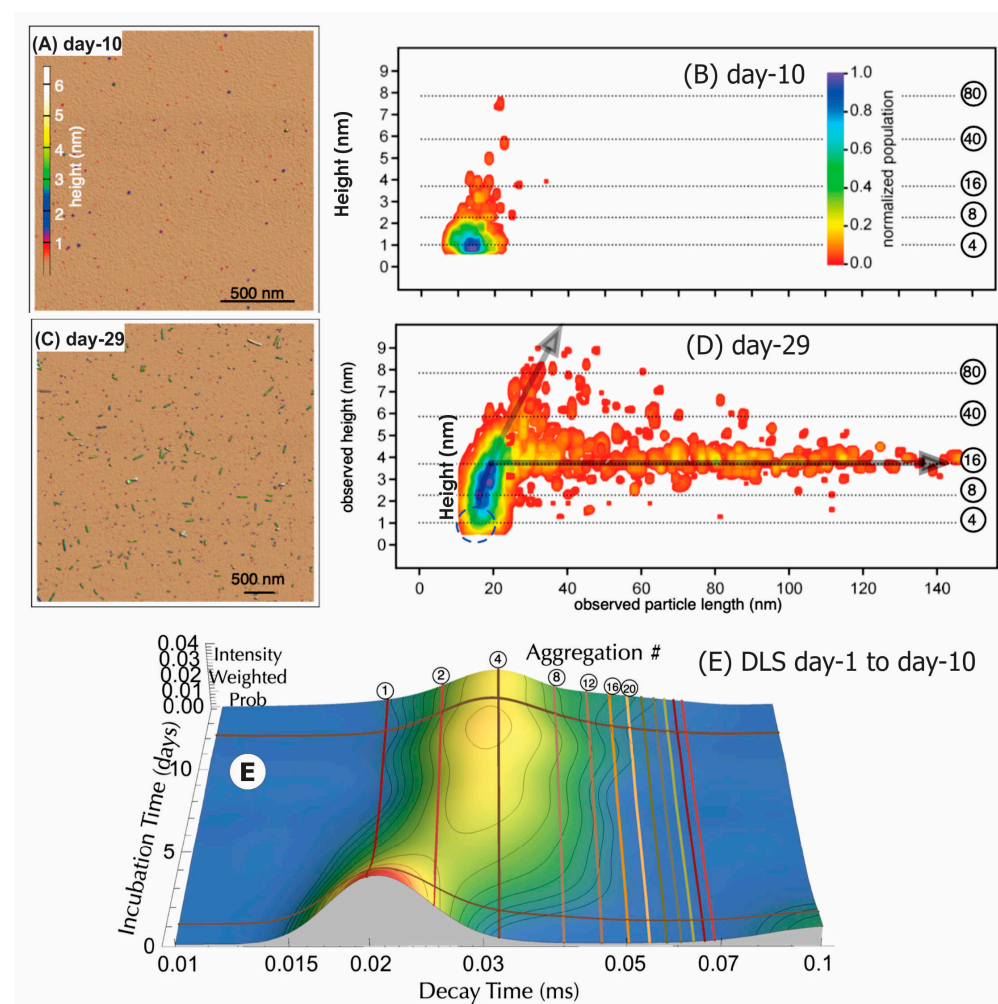
The open pore current ( $I_0$ ) for a given nanopore was consistent across all the DNA and βLGa measurements, suggesting that the nanopore area ( $A_{po}$ ) remained constant. Using the known cross section area of a dsDNA,  $A_{dann} = (1.8 \text{ nm}^2)$  [80], the arft hethe nanopore estimated was  $A_{po} = 2dann / \left( \frac{\Delta I_b}{I_0} \right) = 236.2 \text{ nm}^2$  (Table A1), with a diameter of 17.8 nm. Using the open pore current,  $I_0 = 8.80$  nA, the estimated effective thickness of the pore was  $H_{eff} = \frac{\Psi \sigma A_{po}}{I_0} = 32.8 \text{ nm}$ ,



therefore the effective volume of the pore was  $V_{\text{po}}(2\text{MKCl}) = A_{\text{po}}H_{\text{eff}} = 7750 \text{ nm}^3$ . Interpreting that the cluster-4 events of the Day-29 sample arose from the  $\beta\text{LGa}$  filaments, and using the DNA calibrated nanopore geometry of  $\gamma\Lambda_{\text{Pr}} \simeq \left(\frac{\Delta l_b}{l_0}\right) V_{\text{po}}$  with  $\gamma = 1$  for long filaments of length  $> H_{\text{eff}}$ , the estimated most probable excluded volume of the  $\beta\text{LGa}$  fibril in the pore with  $H_{\text{eff}} = 32.8 \text{ nm}$  was  $\Lambda_{\text{Pr}}(\text{cluster 4}) = 352.0 \text{ nm}^3$ , which gives an area of  $10.7 \text{ nm}^2$  (Table 1). For the cluster-1 events,  $\gamma\Lambda_{\text{Pr}}(\text{cluster 1}) = 37.0 \text{ nm}^3$ .

### 3.1.3. AFM and DLS Measurements

*AFM measurement of  $\beta\text{LGa}$  Day-10 sample.* The AFM images of the Day-10  $\beta\text{LGa}$  sample on functionalized mica (Figure 4A) and their histograms (Figure 4B) show that the most probable values were length,  $l_3 = 11.4 \pm 5 \text{ nm}$ , and diameter,  $d_3 = 1.5 \pm 0.2 \text{ nm}$ . The calculated cross-section area,  $A^3_{\text{AFM}}$ , (Day-10) =  $1.77 \text{ nm}^2$  and the estimated volume was  $V^3_{\text{AFM}}(\text{Day-10}) \approx l_3 \times A^3_{\text{AFM}} \approx 20 \text{ nm}^3$ . An aggregated species with a larger diameter (height  $d = 4.0 \pm 0.2 \text{ nm}$ ) and longer in length,  $l = 20\text{--}40 \text{ nm}$  long, was also detected.



**Figure 4.** AFM images and histograms of Day-10 and Day-29 samples. For the Day-10 sample (A,B), the most probable values were  $l_1 = 11.4 \pm 5 \text{ nm}$  long,  $d_1 = 1.5 \pm 0.2 \text{ nm}$  in diameter were measured. For the Day-29 sample (C,D), the most probable values were  $l_1 = 15 \pm 5 \text{ nm}$  long,  $d_1 = 1.5 \text{ nm}$  in diameter. Second broad peak of fibrils:  $l_4 = 80 \pm 10 \text{ nm}$  long,  $d_4 = 4 \pm 0.2 \text{ nm}$  in diameter. (E) Dynamic light scattering data taken as a function of incubation time from Day 1 to Day 10 under aggregation-prone amyloidogenic conditions. Aggregation number equivalents to the diffusion times are marked by labeled mesh lines.



*DLS measurement of Day-1 to Day-10 sample.* Dynamic light scattering (DLS) measurements (Figure 4E) show that most of the  $\beta$ LGa was monomeric on Day 1 and began to form pre-amyloidogenic aggregates around Day 10 of incubation. The most likely aggregated size was tetrameric (aggregation number  $n = 4$ ), with larger aggregates beginning to form. These observations were consistent with the results by Giurleo et al. [11]; that the Day-10 sample was likely a mixture of partially denatured monomer and aggregation A (tetramers) and started to form aggregation B (octamers). More details about the DLS measurement are described in S-II.

*AFM measurement of the Day-29 sample.* The Day-29  $\beta$ LGa sample on the mica surface (Figure 4C) and the histograms (Figure 4D) show a main peak of length  $l_3 = 15 \pm 5$  nm and  $d_3 = 1.5$  nm in diameter. The aggregated species for the broad peak had values of  $l_4 = 80 \pm 10$  nm and  $d_4 = 4 \pm 0.2$  nm. For comparison with nanopore measurements, the calculated cross-sectional areas and their volumes are listed in Table 1.

### 3.1.4. Summary of $\beta$ LGa Aggregation Characterization under Partially Denaturing Condition

*The Day-1 and Day-10 sample.* The above results and data analysis suggested (1) the cluster-1 events,  $\Delta I_{b,1} \approx 45$  pA, were partially denatured  $\beta$ LGa monomers; (2) the cluster-2 events measured for the Day-1 sample with  $\Delta I_{b,2}$  (Day1)  $\sim 100$  pA were likely the  $\beta$ LGa dimers; (3) the cluster-3 events (Figure 2C) with  $\Delta I_{b,3} \approx 150$ –200 pA were most likely from tetramers, and possibly some trimers.

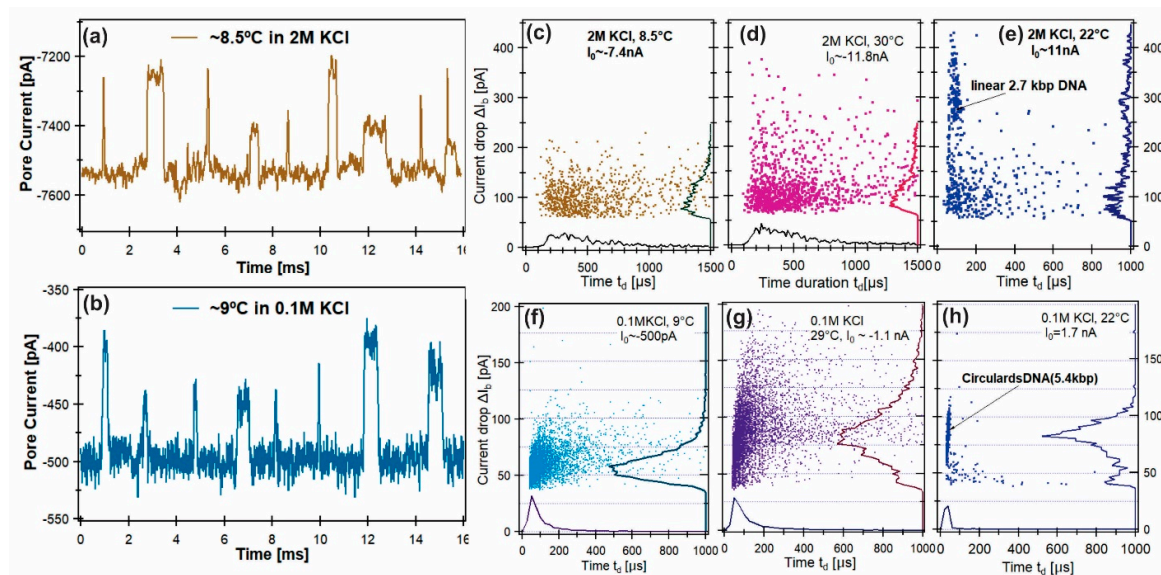
*The Day-29 sample.* The cluster-4 events from the Day-29 sample (Figure 3) with peak values of  $\Delta I_b \approx 400 \pm 100$  pA and  $t_d \sim 200$   $\mu$ s to 2 ms were most likely produced by large  $\beta$ LGa fibrils. Using the most probable length of the fibril measured by AFM,  $l_4 = 80 > H_{eff}(32.8$  nm), the cross-section area of the fibril can be estimated by  $A_{\beta LGa} \approx \left(\frac{\Delta I_b}{I_0}\right) A_{po} = 0.0455 \times 236.2$  nm<sup>2</sup> = 10.7 nm<sup>2</sup> (or diameter = 3.7 nm). This was very close to the AFM-measured diameter  $d_4 = 4.0 \pm 0.2$  nm (area = 12.6 nm<sup>2</sup>, see Table 1). We conclude here that the cluster-4 events represent amyloid protofibrils/filaments, a species of amyloid with a diameter of 3–6 nm and length <100 nm. Note that, here, we used the cross-section area of a dsDNA:  $A_{DNA} = (1.8$  nm<sup>2</sup>) [80]. If we used a diameter for a dsDNA obtained from X-ray diffraction, 2.0 nm [81] and  $A_{DNA} = 3.14$  nm<sup>2</sup>, the estimated diameter of the pore would be unrealistically large, 23.1 nm, not consistent with the TEM image and the observed open pore current value.

### 3.2. Nanopore Characterization of $\beta$ LGa Oligomerization at pH 4.6

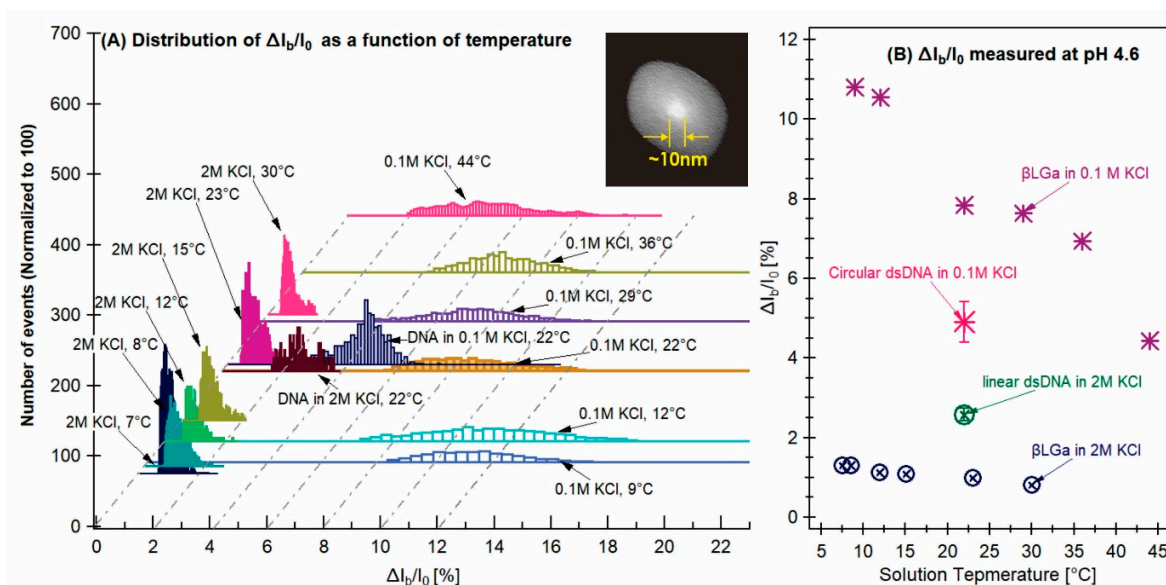
Next, we show that a solid-state nanopore device can be used to characterize the  $\beta$ LGa native-state oligomerization at pH 4.6 and different temperatures (Figure 1A). Early studies have shown that below room temperature, in the pH range of 3.7 to 5.2,  $\beta$ LGa reversibly forms larger oligomers [12,82]. This self-association process is at its maximum around pH 4.6, just below the isoelectric point. The static light scattering data indicated that the large oligomers cooperatively formed octamers, and the radius of gyration, deduced from small-angle X-ray scattering (SAXS), indicated a compact cubic arrangement of eight monomers [12,82]. The BLG protein self-association has also been studied as a function of the solution temperature (1  $^{\circ}$ C–27  $^{\circ}$ C) with no salt present at pH 4.7 by proton magnetic dispersion (MRD) [82], and the results have shown that the BLG are in dimer–octamer equilibrium. Combining static and DLS [12] at pH 4.3, in the temperature range 8  $^{\circ}$ C to 35  $^{\circ}$ C,  $\beta$ LGa aggregation has been measured as a function of the salt concentration. These studies have shown that the  $\beta$ LGa would be in a stable dimer form at 2 M KCl. However, at low salt 0.1–0.5 M conditions, the  $\beta$ LGa would aggregate to tetramers, hexamers, and octamers at the same temperature, with the average aggregation number increasing with a lower temperature.

The nanopore measurements of the  $\beta$ LGa oligomerization (Figures 5 and 6) were performed as a function of the solution temperature under two salt conditions, 2 M and 0.1 M KCl, both with 100 mM pH 4.6 acetate buffer. A 2.7 kbp linear dsDNA ( $1A_{DNA}$ )

in 2 M KCl and a circular 5.4 kbp dsDNA ( $2A_{DNA}$ ) in 0.1 M KCl solution were used as reference molecules. The  $\beta$ LGa concentration was  $\sim 200$  nM in the cis chamber. The solution temperature was varied from  $5^\circ\text{C}$  to  $45^\circ\text{C}$ . A single  $\sim 10$  nm pore (Figure 6A insert) was used for all the measurements presented in Figures 5 and 6. The open pore current was the same at the end of the experiment under the same solution conditions; therefore, the geometry of the nanopore remained the same for all the data presented in Figures 5 and 6.



**Figure 5.** Examples of current blockage events recorded for  $\beta$ LGa at pH 4.6 and  $\sim 8.5^\circ\text{C}$  in 2 M KCl (a) and  $9^\circ\text{C}$  in 0.1 M KCl (b). Event distribution plots,  $\Delta I_b$  vs.  $t_d$  in 2 M KCl for BLGa at  $\sim 8.5^\circ\text{C}$  (c), at  $\sim 30^\circ\text{C}$  (d), and (e) for linear 2.7 kbp dsDNA at  $\sim 22^\circ\text{C}$ ; in 0.1 M KCl for BLGa at  $\sim 9^\circ\text{C}$  (f), at  $\sim 29^\circ\text{C}$  (g), and for circular 5.4 kbp dsDNA at  $\sim 22^\circ\text{C}$  (h). The histograms of  $\Delta I_b$  are shown on the right axes and  $t_d$  are on the bottom axes. Protein concentration in the cis chamber was  $\sim 200$  nM at pH 4.6. More scattered plots and examples of events can be found in S-I (Figures S3 and S4).



**Figure 6.** (A) The event distributions (normalized to 100) of  $\Delta I_b/I_0$  for the entire set of experiments performed. The TEM image of the  $\sim 10$  nm nanopore used for the set of experiments is shown in the insert. (B) Peak values of  $\Delta I_b/I_0$  as a function of temperature for all the  $\beta$ LGa sample measured at pH 4.6 together with the dsDNA [2 M KCl ( $\otimes$ ) and 0.1 M KCl ( $*$ )] with the same nanopore.

At pH 4.6,  $\beta$ LGa protein is positively charged, thus the *trans* chamber bias was switched to negative, and the open pore currents were negative (Figure 5a,b). For the negatively charged dsDNA molecules, the *trans* chamber was positively biased. The examples of the event distributions for  $\beta$ LGa in 2 M KCl at 30 °C (Figure 5c) and at 8.5 °C (Figure 5d) show that the average blockade current,  $\Delta I_b$  (on the right axis), had similar distributions. The peak values were  $\Delta I_b = 64 \pm 11$  pA at 8.5 °C (Figure 5c) and  $\Delta I_b = 65 \pm 15$  pA at 30 °C (Figure 5d). In 0.1 M KCl, the event distribution for  $\beta$ LGa at 29 °C (Figure 5f) and at 9 °C (Figure 5g) show that the distribution of  $\Delta I_b$  changed significantly. The peak values were  $\Delta I_b = 62 \pm 11$  pA at 9 °C (Figure 5f) and  $82 \pm 15$  pA at 30 °C (Figure 5g). The control experiment performed with the linear dsDNA (Figure 5e) at room temperature ( $\sim 22$  °C) in 2 M KCl shows that the most probable current blockage amplitude was  $\Delta I_b \sim 280$  pA and  $t_d = 87 \pm 17$   $\mu$ s. In 0.1 M KCl, the circular dsDNA in Figure 5h shows a very narrow peak, with values of  $\Delta I_b = 83 \pm 8$  pA ( $\sim 100.6$  pA after amplitude correction [23]) and  $t_d = 31 \pm 8$   $\mu$ s.

The open pore current,  $I_0$ , for both 2 M and 0.1 M KCl solution increased with temperature (Figure S2), consistent with the thermal increase in the solution conductivity. To account for the solution conductivity variation with temperature, we plotted the ratio of the current blockage values to their open pore current,  $\Delta I_b/I_0$ , in Figure 6. For the  $\beta$ LGa protein in 2 M salt solution at pH 4.6, the distributions of  $\Delta I_b/I_0$  did not change significantly as temperature varied from 7 to 30 °C, showing narrow peaks around  $\Delta I_b/I_0 = 0.7\%$ . This was consistent with an earlier report that the  $\beta$ LGa would be in a stable dimer form at 2 M KCl [12]. For  $\beta$ LGa in 0.1 M KCl, the distributions of  $\Delta I_b/I_0$  in Figure 6A show the values of  $\Delta I_b/I_0$  ranged from 2% to 14%, indicating that in 0.1 M KCl, the  $\beta$ LGa protein molecules could be in self-association or in oligomerization forms.

All the peak values of  $\Delta I_b/I_0$  for the entire set of  $\beta$ LGa samples together with the dsDNA performed with the same nanopore are shown in Figure 6B. For the  $\beta$ LGa in 2 M KCl, the most probable value of  $\Delta I_b/I_0$  was between 0.5–0.7% as the solution temperature was decreased from 30 °C to 8 °C ( $\otimes$  in Figure 6B bottom). This measurement indicates that the majority of the  $\beta$ LGa protein molecules are likely in a stable monomer or dimer form in the temperature range tested. In 0.1 M KCl, the ratio of the  $\Delta I_b/I_0$  values increased from 4.5% at 44 °C to 11% at 9 °C, suggesting the aggregation number became larger as the temperature was lowered. This was consistent with the earlier results measured using the MRD and DLS methods [12,82].

Below, we offer an explanation as to why a low salt concentration favors  $\beta$ LGa oligomerization and why the aggregation number became larger as the temperature was lowered.  $\beta$ LGa has positively and negatively charged regions, giving rise to a dipole moment that has been experimentally measured to be  $\sim 700$  Debye [83]. The contribution of the dipole moment to the  $\beta$ LGa– $\beta$ LGa interactions should increase at low salt concentrations and lower temperatures, leading to more oligomerization.

Next, we estimate the excluded volumes,  $\gamma\Lambda_{Pr}$ , from our nanopore measurements. The values of  $\Delta I_b/I_0$ , measured as  $\sim 2.6\%$  for the linear dsDNA in 2 M ( $\otimes$ ) and  $\sim 4.9\%$  ( $\ast 5.9\%$  after correction) for the circular dsDNA in 0.1 M KCl, were consistent with Equation (1). For a dsDNA molecule with a contour length  $L_{DNA} \gg H_{eff}$ , Equation (1) leads to  $\Delta I_b/I_0 \sim A_{DNA}/A_{pore}$ . Using  $A_{dsDNA} = (1.8 \text{ nm}^2)$  [80] and  $A_{CircdsDNA} = 2 \times 1.8 = 3.6 \text{ nm}^2$  for circular dsDNA, the product of the excluded volume and shape factor:  $\gamma\Lambda_{Pr} \simeq \left(\frac{\Delta I_b}{I_0}\right) V_{po}$  of  $\beta$ LGa protein in 0.1 M KCl and in 2 M KCl at pH 4.6 at different temperatures can be estimated (Figure S5). In 0.1 M KCl, the  $\gamma\Lambda_{Pr} = 30.5 \sim 74.3 \text{ nm}^3$ . In 2 M KCl, the  $\gamma\Lambda_{Pr} = 6.6 \sim 10.5 \text{ nm}^3$ . The ratios of  $\gamma\Lambda_{Pr}$  in 0.1 M to 2 M were about 4 to 8 (low temperature) (Figure S5), this was consistent with the expected aggregation numbers.

However, the estimated values of  $\gamma\Lambda_{Pr} = 8.6 \sim 11 \text{ nm}^3$  in 2 M KCl (Figure S5) were only about half the value of  $V_{Pr} = 22.2 \text{ nm}^3$  that was calculated by adding the volumes of the amino acids together for a monomer. Furthermore, if we take the dsDNA diameter as 2.2 nm ( $A_{dsDNA} = 3.8 \text{ nm}^2$ ), the estimated values of  $\gamma\Lambda_{Pr} \sim 25.8$  to  $40.9 \text{ nm}^3$  (Figure S5) are approximately four times larger. This suggests that this study shows a nanopore device can estimate the relative volumes of proteins (aggregation states) for

comparison; however, is not capable of measuring the absolute volume of a protein. The major reason for this was that this value,  $\gamma\Lambda_{Pr}$ , was calculated based on the volume of a nanopore,  $V_{po} = A_{po}H_{eff}$ , and this effective pore volume was difficult to determine accurately under the experimental conditions. The other reasons include the cross-section area of the reference dsDNA molecule in solution was not precisely known and the area of the dsDNA could have become larger at low pH [84], and there was a possibility that the shape of the  $\beta$ LGa protein molecule could change under the electric field strength in a nanopore under the experimental conditions.

In summary, by measuring  $\Delta I_b/I_0$  in the same nanopore together with reference dsDNA molecules, we successfully estimated the native-state oligomerization at pH 4.6 under different solution conditions. Our measurement and analysis showed that in 0.1 MKCl,  $\beta$ LGa molecules were likely in the form of tetramers ( $n = 4$  at high temperature), hexamers ( $n = 6$ ), and octamers ( $n = 8$  at low temperature), and are likely not homogeneous or single species. This set of experiments suggests that a solid-state nanopore device can be used in future studies of the dissociation of protein aggregation.

However, this study showed that the limitation of a nanopore measurement is to measure the absolute volume of a protein molecule,  $\Lambda_{Pr}$ , because it could depend on the nanopore geometry and the geometry of the calibration dsDNA molecules. Further experiments showed that the  $\gamma\Lambda_{Pr}$ , estimated by the nanopore method, also depended on the applied voltages [85]. The advantage of using dsDNA and cir-dsDNA in this study was that the events from the calibration molecule were easily distinguished from the analyte molecules. A better calibration would involve known particles with known geometry nanoparticles of spherical and rod shapes; however, such an approach would necessitate completing the calibration in series with the measurement rather than in parallel.

#### 4. Conclusions

This study has demonstrated that a silicon nitride nanopore device can be used to characterize  $\beta$ -lactoglobulin variant A ( $\beta$ LGa) protein amyloid formation in salt solution under partial denaturation conditions at pH 7.0 and native state self-association oligomerization at pH 4.6. Our results showed that by measuring the relative current blockage amplitudes combined with using a dsDNA molecule as a reference, we can estimate the  $\beta$ LGa protein aggregation state, including the aggregation number and dimensions. This work also indicates that a solid-state nanopore device can also be used for future studies of protein aggregation.

*The advantages and weaknesses of using the nanopore method to evaluate protein aggregation.* Comparing other ensemble methods as well as single molecule techniques at the present time, this study showed that the solid-state nanopore method can characterize protein aggregation close to its native salt solution environment on the single molecule level. This work demonstrated that the nanopore technique is fast; one set of measurements usually takes less than 10 min to record about five thousand events; a small amount of sample is needed ( $\sim 10$   $\mu$ L of 100 nM or  $\sim 10$  pM protein); and it can measure protein aggregation under all biological related parameters such as temperature, pH, electric field strength (voltage), and salt concentration. In addition, nanopore measurement can also estimate the relative aggregation state and its distribution quantitatively. To be able to evaluate protein aggregation under these conditions will be important and valuable and could improve our understanding of protein aggregation mechanisms and allow for the development of new approaches for the prevention and dissociation of amyloid formation and better diagnostics for protein aggregation-related devastating diseases. The limitation of this technique, based on this study, is that the estimated volume of the protein molecules depended on the calibration molecule, the nanopore geometry, and applied voltage. Further investigation is needed to measure the size and shape of the aggregated proteins precisely.



**Supplementary Materials:** The following supporting information can be downloaded at <https://www.mdpi.com/article/10.3390/s24010081/s1>, Figure S1: The time duration ( $t_{d,4}$ ) histogram for the Day-29  $\beta$ LGa sample; Figure S2. Open pore current,  $I_0$ , at different temperatures in 0.1 M KCl and in 2 M KCl; Figure S3. Plots of  $\Delta I_b$  vs.  $t_d$  and example of events for  $\beta$ LGa protein in 0.1 M KCl; Figure S4. Plots of  $\Delta I_b$  vs.  $t_d$  and example of events for  $\beta$ LGa protein in 2 M KCl; Figure S5. The estimated product of the excluded protein volume.

**Author Contributions:** M.C.A. contributed by performing the experiments and data analysis. B.L. contributed to nanopore fabrication and TEM imaging. B.T. contributed by performing nanopore experiments. X.H., J.G. and T.M. contributed to the AFM and DLS experiments and data analysis. D.T. contributed to the experimental design and data analysis. J.L. contributed to the design of the experiments, performing the nanopore experiments, data analysis, and manuscript writing. All authors have read and agreed to the published version of the manuscript.

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## Appendix A

Solution conductivity used for calculations and experiments. For the solution of 2 M KCl with 5 M urea and 10 mM phosphate buffer at pH 7 and room temperature, conductivity  $\sigma \sim 120$  mS/cm. For the solution of 1.6 M KCl 20% Glycerol 10mM phosphate buffer at pH7,  $\sigma \sim 110$  mS/cm. At room temperature, 2 M KCl with 100 mM acetate buffer at pH 4.6,  $\sigma = 150$  mS/cm; 0.1 M KCl with 100 mM acetate buffer at pH 4.6,  $\sigma = 18.4$  mS/cm.

## Appendix B

**Table A1.** Parameters of the 3 nanopores used for this work.

	TEM Diameter	Diameter by $I_0$ or DNA	Area $A_{po}$ by DNA and $I_0$	$H_{eff}$ by $I_0$ or dsDNA	$V_{po} = A_{po} H_{eff}$
Nanopore 1 for Day 1 and Day-10	10 nm	10 nm	78.5 nm <sup>2</sup>	36.5 nm	2870 nm <sup>3</sup>
Nanopore 2 for Day 29	16 nm	17.8 nm	236.2 nm <sup>2</sup>	32.8 nm	7750 nm <sup>3</sup>
Nanopore 3 for pH 4.6	8 nm	9.5 nm (2 M)	69.9 nm <sup>2</sup>	11.4 nm (2 M)	800 nm <sup>3</sup>
		9.7 nm (0.1 M)	73.5 nm <sup>2</sup>	9.36 nm (0.1 M)	688 nm <sup>3</sup>

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