# Specific Preoperative Dynamic Contrast-Enhanced MRI Semi-quantitative Markers Can Correlate With Vascularity in Specific Areas of Glioblastoma Tissue and Predict Recurrence

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## Abstract

Background: Glioblastoma is one of the most aggressive tumours despite all advanced therapies. We aimed to investigate the correlation between qualitative markers of dynamic contrast-enhanced magnetic resonance imaging and vascularity in different tumour regions and elucidate their potential in predicting recurrence.

Methods: Radiological markers of vascularity as wash-in rate, washout rate, and capillary time to peak in different single tumour regions were extracted for all glioblastoma patients before being surgically resected using preoperative dynamic contrast-enhanced MRI (DCE-MRI). Tissue samples were obtained from different intratumoral regions and peritumoral oedema and evaluated for the vascular endothelial growth factor (VEGF).

Results: Two hundred sixty individuals were included in the final analysis, with 180 dead ones and 80 survivors. Radio- and chemo-therapy were received by all surviving patients and 77.8% (n= 140) of the dead ones. The mean time to peak, in seconds, was longest at the peritumoral oedema region (71.7 $\pm$ 23.5), followed by the tumour's necrotic centre (50.0 $\pm$ 28.5) and its periphery (2.9 $\pm$ 1.8). The expression of VEGF at the peritumoral edema region was inversely correlated to the washout rate at the periphery (r= -0.66; P-value= 0.014) and positively correlated to peritumoral TTP (r= 0.94; P-value< 0.001).

Conclusion: Using DCE-MRI, VEGF expression may be used as a non-invasive marker to estimate tumour grade for clinical diagnosis and treatment. Moreover, the risk of glioblastoma recurrence could be determined by evaluating the washout rate at the tumour's periphery. Further large-scale studies are needed to validate the results and to have concrete evidence.

**Categories:** Neurology, Neurosurgery, Oncology **Keywords:** brain tumours, dce, mri, glioblastoma, glioma

## Introduction

Glioblastoma (GBM) is considered to be the most aggressive primary brain tumour with a horrible prognosis. Recurrence after treatment is a significant problem. The survival rate for one year is about 39.7% [1]. Ideal outcomes are still challenging to be achieved despite recent treatment combinations. The ultimate capacity to regrow after resection is due to the availability of self-regenerating stem cell populations. The biology of GBM is complex and involves many signalling pathways.

One of the most striking features of GBM is hypoxia. GBM is a highly vascularized tumour with characteristically aberrant vessels [2]. Pseudopalisading, areas of necrosis and abnormal capillary growth are typical microscopic features of GBM [3]. Tumour hypoxia is a critical biological feature that affects the response of GBM to different therapies [4]. Since Folkman tried to expose the biological aspect of tumour angiogenesis, several advances have been made [5]. Hypoxia plays an essential role in gene regulation, stem cell recapitulation, and tumour vascularization [6]. Conventional MRI techniques provide details about the anatomy and gross morphology of cerebral lesions, but they fail to unveil the physiological changes at the microcapillary level. Recent MRI techniques can capture certain parameters based on physiological tumour features [7]. Conventional anatomical MRI is sometimes fallacious in the preoperative prediction of tumour pathological grade and vascularity, impacting treatment strategy [8]. Dynamic contrast-enhanced MRI (DCE-MRI) can quantitatively and qualitatively evaluate the hemodynamic changes as blood flow and vascularity at the tissue level [9]. The measured parameters are considered markers for tissue hypoxia.

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Azab M A, Ghozy S, Hassanein S, et al. (June 08, 2021) Specific Preoperative Dynamic Contrast-Enhanced MRI Semi-quantitative Markers Can Correlate With Vascularity in Specific Areas of Glioblastoma Tissue and Predict Recurrence. Cureus 13(6): e15528. DOI 10.7759/cureus.15528 The maestro regulator of hypoxia-induced changes is the HIF gene [10]. Several tissue markers of hypoxia are identified as vascular endothelial growth factor (VEGF), glucose transporter-1 (GLUT-1), and carbonic anhydrase [11,12]. There is a degree of correlation between tumour vascularity, pathological grade, and hypoxia. We did not find any association between the most prominent vascular marker VEGF expression and GBM recurrence, although some studies reported a correlation [13,14]. That may be because the sampling of the tumour's different regions was random and not fully representative. We hypothesize that the measured radiological markers may correlate with pathological markers in different areas of GBM. They may also have a role in predicting recurrence.

# **Materials And Methods**

All methods were carried out following relevant guidelines and regulations. The ethical board approved all experimental protocols used in this study. Informed consent was obtained from all subjects or a parent/legal guardian if under 18 years of age. In the case of dead patients, the legal guardian consented.

## Patient enrollment

This is a prospective single-centre study. Patients with a history of newly diagnosed GBM with a maximum diameter from 3 to 5 cm as a single lesion identified by MRI were enrolled (Figure 1). The lesions were surgically resected at the time of the presentation. The survival status of the patients was tracked from the follow-up records of patients at the out-patient clinic and oncology referrals. The out-patient and emergency hospital records helped us to identify cases who died and those with recurrence.



## FIGURE 1: DCE workstation at the enrollment center

#### **Diagnosis of recurrence**

In most cases, recurrence was considered when there was either an unequivocal increase in fluid-attenuated inversion recovery (FLAIR)/T2 signal abnormality or newly detected areas of contrast enhancement on follow-up MRI requiring further surgery, radiation, or chemotherapy.

## **Preoperative imaging**

Patients who fulfilled all the inclusion criteria underwent preoperative conventional gadolinium-enhanced MRI brain and DCE-MRI. We identified three regions of interest for further analysis to extract qualitative vascular markers. We divided the tumour into a necrotic centre, a peripheral thickness of the tumour, and a peritumoral oedema region (Figure 2). All images were uploaded to the intraoperative navigation system for patients who were defined for surgery.

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FIGURE 2: Different GBM regions that were sampled intraoperatively. Created with BioRender.com

#### **DCE-MRI** data extraction

At first, standard preoperative non-contrasted MRI was obtained, and then, the lesion of interest was identified. Utilizing a fast 3-dimensional gradient echo, the dynamic perfusion MRI was obtained on the 1.5T Philips machine. About 0.1 mmol/kg of gadolinium particles (Omniscan) were injected over 4 seconds through an 18-gauge catheter into a prominent vein using a power injector.

Semi-quantitative parameters are more manageable and more straightforward than quantitative parameters using the T1-weighted sequence after gadolinium injection. We defined specific parameters to extract in a region of interest about 5 mm in diameter. T0 was considered as the basal contrast at a duration of 0 seconds. Time to peak (TTP) was defined as the beginning of contrast injection to the highest enhancement peak. Wash-in is the time of contrast rush in the capillary from zero to peak level, while the washout rate of the contrast is the time elapsed from the peak to the return to zero level (Figure 3).



FIGURE 3: Semi-quantitative parameters of DCE-MRI. Created with BioRender.com

#### Surgery

Surgery was done at a maximum of two days post-imaging. Contrasted MRI was loaded into the navigation system to target the predefined areas we specified for sampling. Sampling was done before completely resecting the lesion to avoid the volume shift from debulking and the resulting brain relaxation. The first sample was sent for frozen section pathology. According to the WHO classification 2016 [15,16] and VEGF staining, region-specific samples were sent for histopathological examination.

#### Immunohistochemistry

All slides were examined under a 200X magnification microscope and scored by a neuropathologist blinded to the tumour, the imaging, and the patient's data. All samples retrieved were labelled according to the region from where they were obtained. All were stained with VEGF and scored from zero to four based on the proportion of cells stained.

#### Statistical methods and data analysis

All the data were analyzed using R software version 4.0.2 and two-sided, considering P-value  $\leq 0.05$  was considered statistically significant for all tests. Categorical variables were represented as frequencies and percentages with Chi-square test (or Fisher's exact test, as appropriate) for testing the difference, according to their living/death status. Following the normal distribution test, continuous variables were expressed as means, and standard deviations (SDs) with independent t-test (or Mann-Whitney Test, as appropriate) were used for testing the difference, according to their living/death status.

Pearson's correlation coefficient (r) was used to determine the relationship between different variables and their recurrence correlation. Moreover, univariable and multivariable Cox proportional hazard regression models were used to identify all possible prognostic factors affecting GBM recurrence. The adjustment in the multivariate model was made for other co-founders; TTP (all sites), washout rate (other than periphery), VEGF (all sites), radiotherapy status, and chemo-therapy status of the included patients. Regression results were expressed as hazard ratios (HRs) and 95% confidence interval (95% CI) for both regression models. Kaplan-Meier analysis in the form of survival curves was used to present the recurrence probabilities of significant predictors, and a log-rank test was used to compare their recurrence rates.

#### **Results**

### Patients' clinical data

Two hundred sixty individuals were included in the final analysis, with 180 dead ones and 80 survivors. Radio- and chemo-therapy were received by all surviving patients, and 77.8% (n= 140) of the dead ones. In total, recurrence was confirmed in 69.2% (n= 180) of the patients; seven patients have passed away (Table 1).

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		Dead				Total			
Parameter	n= 180		)	n= 80	n= 80		N= 260		
		Mean	Standard Deviation	Mean	Standard Deviation	Mean	Standard Deviation		
TTP center (seconds)		52.5	31.1	44.3	24.6	50.0	28.5		
TTP periphery (seconds)		3.2	2.0	2.3	0.8	2.9	1.8		
TTP peritumoral (seconds)		79.7	14.6	53.7	31.9	71.7	23.5		
Washout rate center (seconds)		54.1	26.5	50.7	35.7	53.1	28.1		
Washout rate periphery (seconds)		24.3	21.4	39.9	34.3	29.1	25.6		
Wash out rate peritumoral (seconds)		73.4	23.3	63.3	28.0	70.3	24.1		
VEGF center (%)	12.2	4.6	10.9	5.9	11.8	4.8			
VEGF periphery (%)		6.4	2.6	5.9	3.6	6.3	2.8		
VEGF peritumoral (%)		17.2	3.5	11.7	7.8	15.5	5.5		
Duration till the first recurrence (months)		8.4	9.0	9.8	11.8	8.8	9.5		
Parameter		n	%	n	%	n	%		
Pagurranga	No	40	22.2	40	50.0	80	30.8		
necurrence	Yes	140	77.8	40	50.0	180	69.2		
Received Radiotherapy and	No	40	22.2	0	0.0	40	15.4		
chemotherapy	Yes	140	77.8	80	100.0	220	84.6		

#### TABLE 1: Summary of all parameters stratified by survival outcome.

TTP: time to peak, VEGF: vascular endothelial growth factor

#### Radiological markers of vascularity and immunohistochemistry

The mean TTP, in seconds, was longest at the peritumoral oedema region ( $71.7\pm23.5$ ), followed by the tumour's necrotic centre ( $50.0\pm28.5$ ) and its periphery ( $2.9\pm1.8$ ). The same pattern was observed in the measured washout rates (seconds), where they were high at the peritumoral oedema region ( $70.3\pm24.1$ ) and the tumour's centre ( $53.1\pm28.1$ ) compared to its periphery ( $29.1\pm25.6$ ) (Table 1).

In the same context, the immunohistochemical analysis indicated that VEGF is expressed not only in GBM tissue but also in the peritumoral oedema region. Furthermore, the mean percentage of VEGF positive cells was significantly higher in the peritumoral oedema region  $(15.5\pm5.5)$  and tumour's centre  $(11.8\pm4.8)$ , compared with that noted in the surrounding peripheries  $(6.3\pm2.8)$ . For all tested parameters, there were no statistically significant differences based on the survival status (Table 1).

#### Correlation of different biomarkers with recurrence

The expression of VEGF at the peritumoral edema region was inversely correlated to the washout rate at the periphery (r=-0.66; P-value= 0.014) and positively correlated to peritumoral TTP (r=0.94; P-value< 0.001). Additionally, VEGF expression at the tumor's center was positively correlated to central TTP (r=0.89; P-value< 0.001) and the central wash out rate was inversely correlated to TTP at tumor's periphery (r=-0.56; P-value= 0.045) (Table 2).

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Variables	Correlation	TTP center	TTP peritumoral	TTP periphery	washout rate center	wash out rate peritumoral	washout rate periphery	VEGF	VEGF peritumoral	VEGF periphery	Time to recurrence	Survival	Recurrence	Received Radiotherapy and chemo
TTP center	Pearson's r	-												
	P-value	-												
P TTP peritumoral P	Pearson's r	0.30*	-											
	P-value	0.317*	-											
TTP peripheny	Pearson's r	0.25*	0.28*	-										
TT porpriory	P-value	0.403*	0.354*	-										
washout rate center	Pearson's r	0.03*	-0.49	-0.56*	-									
	P-value	0.924*	0.091*	0.045*	-									
wash out rate	Pearson's r	0.02*	-0.32*	-0.29	0.74*	-								
peritumoral	P-value	0.944*	0.282*	0.338*	0.004**	-								
washout rate	Pearson's r	-0.28*	-0.49	-0.11	0.42**	0.45*	-							
periphery	P-value	0.349*	0.087*	0.731*	0.155*	0.121	-							
F	Pearson's r	0.89*	0.47*	0.25	-0.2	-0.09	-0.5*	-						
	P-value	0.001*	0.106	0.411*	0.504**	0.773**	0.081	-						
VEGF peritumoral	Pearson's r	0.54*	0.94*	0.29*	-0.41	-0.29	-0.66*	0.69**	-					
	P-value	0.057	0.001*	0.336*	0.164*	0.34*	0.014*	0.009**	-					
VEGF periphery	Pearson's r	0.28*	0.51*	-0.08	-0.35*	0.06	-0.55*	0.56*	0.6*	-				
	P-value	0.352*	0.075*	0.795*	0.248	0.845*	0.052*	0.044*	0.031*	-				
Duration till the first	Pearson's r	0.23*	-0.33*	0.39*	-0.23	-0.18	-0.33*	0.28*	-0.12*	0.05	-			
recurrence	P-value	0.443*	0.274*	0.191	0.447*	0.567*	0.268*	0.356*	0.691**	0.883*	-			
Survival	Pearson's r	-0.14*	-0.53*	-0.24*	-0.06	-0.2	0.29	-0.13	-0.48*	-0.1*	0.07**	-		
	P-value	0.651*	0.061	0.42*	0.849**	0.51*	0.333**	0.679**	0.095	0.741**	0.83*	-		
Recurrence	Pearson's r	0.21*	0.16	0.47*	-0.42	-0.41*	-0.64	0.23*	0.32*	0.12	0.65*	-0.28*	-	
	P-value	0.487	0.603*	0.104	0.155*	0.162*	0.018*	0.447*	0.294*	0.695*	0.016*	0.358*	-	
Received	Pearson's r	0.4*	-0.22	-0.04*	0.15	-0.08	0.15	0.24*	-0.06	-0.22*	0.34*	0.28*	0.18*	-
chemo	P-value	0.176	0.478*	0.885*	0.623***	0.789**	0.620**	0.424*	0.834*	0.471*	0.249*	0.347*	0.561**	-

#### TABLE 2: Correlation matrix of different outcomes.

TTP: time to peak, VEGF: vascular endothelial growth factor

The risk of recurrence was solely correlated to the washout rate at the tumor's periphery (r= -0.64; P-value= 0.018). In contrast, risk of recurrence was not correlated to central TTP (r= 0.21; P-value= 0.487), peritumoral TTP (r= 0.16; P-value= 0.0498), peripheral TTP (r= 0.47; P-value= 0.049), central washout rate (r= -0.42; P-value= 0.0499), peritumoral washout rate (r= -0.41; P-value= 0.044), central VEGF (r= 0.23; P-value= 0.049), peritumoral VEGF (r= 0.23; P-value= 0.049), or peripheral VEGF (r= 0.12; P-value= 0.046) (Figure 4).



Although the univariate cox regression did not show a significant increase in recurrence risk with higher washout rate at the tumor's periphery (HR= 0.99; 95% CI= 0.95-1.04; P-value= 0.05), the multivariate model showed a highly significant association with recurrence risk (HR= 9.08; 95% CI= 8.44-9.76; P-value= 0.05). To test the effect of different peripheral washout rates, 20 seconds cut-off was used. The Kaplan-Meier analysis showed statistically significant results (Figure 5).



FIGURE 5: Kaplan-Meier curve for the risk of recurrence according to the washout rate at the periphery.

## Discussion

Over the last few years, the DCE-MRI has been introduced as a part of the preoperative assessment and the follow-up of brain tumours, including GBM [17,18]. The DCE signal intensity-time curve reflects the combined microvessel permeability, tissue perfusion, and extravascular-space. Therefore, it could be used for a multiparametric characterization of the microvasculature of tumours [19,20]. The advantages of DCE over dynamic susceptibility contrast (DSC)-MRI include the lower possibility of artefacts and the ability to assess the blood-brain barrier (BBB) integrity [20]. Initially, the main focus of DCE metrics was the volume transfer constant (K-trans), which is identified as a permeability marker with BBB disruption and malignant lesions [20-22]. Fitting the DCE data through the two-compartment models, the plasma/ fractional volume of the intravascular compartment was also assessed as a marker for tumour neoangiogenesis and subsequent grading [23,24]. Also, the plasma/fractional volume of the extravascular-extracellular space was evaluated as a candidate marker of mitotic activity [25]. The DSC-MRI is superior to the DCE-MRI for better temporal resolution, with a more accurate blood volume estimation, making it valuable in GBM grading [17].

To date, several studies reported a comparable accuracy of DSC-MRI and DCE-MRI in tumour grading [26-29], with a special focus on DCE-derived K-trans. In a multi-centre study of 94 patients, plasma and extravascular-extracellular space volumes had the highest accuracy for glioma grading [29]. An in-vivo study showed a higher wash-in (p= 0.016) and wash-out (p= 0.014) rates in GBM compared to radiation necrosis [30]. Moreover, TTP was significantly lower in GBM compared to radiation necrosis [30]. In another study of 45 patients, the VEGF expression was correlated with peripheral oedema, enhancement percentage, and the tumour's maximum diameter [31]. The same study found that the peripheral oedema index, enhancement percentage, and the maximum diameter of the tumour were significantly higher in the high-grade than the low-grade tumors; therefore, VEGF could be used as a biomarker for glioma invasion [32].

In this study, we obtained DCE-MRI and conventional MRI for all patients with suspected GBM before surgery. We also obtained frameless navigation guided biopsies from different tumour regions as illustrated before, from the centre, tumour edge and peritumoral tissue guided by the increased T2 and FLAIR intensity surrounding the tumour. Localization was a rough estimate of these regions. There are no strict borders between these regions, resulting in a limitation to precisely sample the theoretical partitions of the GBM. Sampling was attempted before debulking surgery to avoid architectural changes resulting from fluid aspiration or volumetric changes. Each sample was analyzed for the degree of vascular hyperplasia, using VEGF staining. A group of researchers used imaging to sample different tumour regions, and found a correlation between histological markers and certain imaging markers. They observed that the semiquantitative markers of DCE-MRI were correlated with the enhanced regions, while diffusion parameters were correlated with the non-enhanced regions [16].

We found that specific semi-quantitative DCE-MRI markers as the washout rate and TTP were high in the peritumoral oedema area, which indicates the profuse vascularity of that area. Moreover, we found that

VEGF expression is high in the peritumoral area and strongly correlates with the washout rate and TTP in the same areas. VEGF expression was higher in the peritumoral area than the centre and tumour edge (Figure 6). At the necrotic centre of the tumour, we observed that VEGF expression was significantly correlated to TTP and microvascular density. We did not observe any correlation of the vascular radiological or histological markers with tumour recurrence except for the washout rate at the tumour's growing edge. The recurrence risk was not correlated with the washout rate at the centre or the peritumoral oedema region.



FIGURE 6: VEGF expression from the area of peritumoral oedema showing high vascular density.

VEGF: vascular endothelial growth factor

The observed results may help us to predict vascularity in different regions of the single GBM lesion. That may guide us to target anti-vascular therapy to the highly vascular regions compared to the low vascular regions. Moreover, preoperative non-invasive determination of the microvascularity may aid in prognosis and follow-up (Figure 6).

# Conclusions

Using DCE-MRI, VEGF expression may be used as a non-invasive marker to evaluate tumour grading for clinical prognosis and therapy. Moreover, the risk of GBM recurrence could be determined by evaluating the washout rate at the tumour's periphery. Further large-scale studies are suggested to validate the results and obtain concrete evidence.

# **Additional Information**

#### Disclosures

Human subjects: Consent was obtained or waived by all participants in this study. Cairo University Ethical Approval Board issued approval N/A. Cairo University Ethical Approval Board indicates approval of research. Animal subjects: All authors have confirmed that this study did not involve animal subjects or tissue. Conflicts of interest: In compliance with the ICMJE uniform disclosure form, all authors declare the following: Payment/services info: All authors have declared that no financial support was received from any organization for the submitted work. Financial relationships: All authors have declared that they have no financial relationships at present or within the previous three years with any organizations that might have an interest in the submitted work. Other relationships: All authors have declared that there are no other relationships or activities that could appear to have influenced the submitted work.

# **References**

- Sherrod BA, Gamboa NT, Wilkerson C, et al.: Effect of patient age on glioblastoma perioperative treatment costs: a value driven outcome database analysis. J Neurooncol. 2019, 143:465-73. 10.1007/s11060-019-03178-z
- Vajkoczy P, Menger MD: Vascular microenvironment in gliomas. J Neurooncol. 2000, 50:99-108. 10.1023/a:1006474832189
- Kleihues P, Louis DN, Scheithauer BW, Rorke LB, Reifenberger G, Burger PC, Cavenee WK: The WHO classification of tumors of the nervous system. J Neuropathol Exp Neurol. 2002, 61:215-25; discussion 226-9. 10.1093/jnen/61.3.215
- 4. Yetkin FZ, Mendelsohn D: Hypoxia imaging in brain tumors . Neuroimaging Clin N Am. 2002, 12:537-552. 10.1016/s1052-5149(02)00029-1
- Folkman J: Tumor angiogenesis: therapeutic implications. N Engl J Med. 1971, 285:1182-6. 10.1056/NEJM197111182852108
- Hockel M, Schlenger K, Aral B, Mitze M, Schaffer U, Vaupel P: Association between tumor hypoxia and malignant progression in advanced cancer of the uterine cervix. Cancer Res. 1996, 56:4509-4515.
- 7. Aronen HJ, Perkiö J: Dynamic susceptibility contrast MRI of gliomas. Neuroimaging Clin N Am. 2002,

12:501-523. 10.1016/s1052-5149(02)00026-6

- Flynn JR, Wang L, Gillespie DL, et al.: Hypoxia-regulated protein expression, patient characteristics, and preoperative imaging as predictors of survival in adults with glioblastoma multiforme. Cancer. 2008, 113:1032-42. 10.1002/cncr.23678
- McDonald DM, Choyke PL: Imaging of angiogenesis: from microscope to clinic . Nat Med. 2003, 9:713-25. 10.1038/nm0603-713
- Kang S, Kwon HN, Kang S, Park S: Interaction between IDH1 WT and calmodulin and its implications for glioblastoma cell growth and migration. Biochem Biophys Res Commun. 2020, 524:224-30. 10.1016/j.bbrc.2020.01.073
- 11. Lal A, Peters H, St Croix B, et al.: Transcriptional response to hypoxia in human tumors . J Natl Cancer Inst. 2001, 93:1337-43. 10.1093/jnci/93.17.1337
- Søndergaard KL, Hilton DA, Penney M, Ollerenshaw M, Demaine AG: Expression of hypoxia-inducible factor 1alpha in tumours of patients with glioblastoma. Neuropathol Appl Neurobiol. 2002, 28:210-7. 10.1046/j.1365-2990.2002.00391.x
- 13. Moeller BJ, Richardson RA, Dewhirst MW: Hypoxia and radiotherapy: opportunities for improved outcomes in cancer treatment. Cancer Metastasis Rev. 2007, 26:241-8. 10.1007/s10555-007-9056-0
- Nordsmark M, Alsner J, Keller J, Nielsen OS, Jensen OM, Horsman MR, Overgaard J: Hypoxia in human soft tissue sarcomas: adverse impact on survival and no association with p53 mutations. Br J Cancer. 2001, 84:1070-5. 10.1054/bjoc.2001.1728
- 15. Komori T: The 2016 WHO classification of tumours of the central nervous system: the major points of revision. Neurol Med Chir (Tokyo). 2017, 57:301-1. 10.2176/nmc.ra.2017-0010
- Barajas RF Jr, Phillips JJ, Parvataneni R, et al.: Regional variation in histopathologic features of tumor specimens from treatment-naive glioblastoma correlates with anatomic and physiologic MR Imaging. Neuro Oncol. 2012, 14:942-54. 10.1093/neuonc/nos128
- Zhang J, Liu H, Tong H, Wang S, Yang Y, Liu G, Zhang W: Clinical applications of contrast-enhanced perfusion MRI techniques in gliomas: recent advances and current challenges. Contrast Media Mol Imaging. 2017, 2017:7064120. 10.1155/2017/7064120
- Jung BC, Arevalo-Perez J, Lyo JK, Holodny AI, Karimi S, Young RJ, Peck KK: Comparison of glioblastomas and brain metastases using dynamic contrast-enhanced perfusion MRI. J Neuroimaging. 2016, 26:240-6. 10.1111/jon.12281
- Patel P, Baradaran H, Delgado D, Askin G, Christos P, John Tsiouris A, Gupta A: MR perfusion-weighted imaging in the evaluation of high-grade gliomas after treatment: a systematic review and meta-analysis. Neuro Oncol. 2017, 19:118-27. 10.1093/neuonc/now148
- Heye AK, Culling RD, Valdés Hernández Mdel C, Thrippleton MJ, Wardlaw JM: Assessment of blood-brain barrier disruption using dynamic contrast-enhanced MRI. A systematic review. Neuroimage Clin. 2014, 6:262-74. 10.1016/j.nicl.2014.09.002
- 21. Li X, Zhu Y, Kang H, Zhang Y, Liang H, Wang S, Zhang W: Glioma grading by microvascular permeability parameters derived from dynamic contrast-enhanced MRI and intratumoral susceptibility signal on susceptibility weighted imaging. Cancer Imaging. 2015, 15:4. 10.1186/s40644-015-0039-z
- 22. Patankar TF, Haroon HA, Mills SJ, et al.: Is volume transfer coefficient (K(trans)) related to histologic grade in human gliomas?. AJNR Am J Neuroradiol. 2005, 26:2455-65.
- Nguyen TB, Cron GO, Bezzina K, et al.: Correlation of tumor immunohistochemistry with dynamic contrastenhanced and DSC-MRI parameters in patients with gliomas. AJNR Am J Neuroradiol. 2016, 37:2217-23. 10.3174/ajnr.A4908
- Alcaide-Leon P, Pareto D, Martinez-Saez E, Auger C, Bharatha A, Rovira A: Pixel-by-pixel comparison of volume transfer constant and estimates of cerebral blood volume from dynamic contrast-enhanced and dynamic susceptibility contrast-enhanced MR imaging in high-grade gliomas. AJNR Am J Neuroradiol. 2015, 36:871-6. 10.3174/ajnr.A4231
- Mills SJ, du Plessis D, Pal P, et al.: Mitotic activity in glioblastoma correlates with estimated extravascular extracellular space derived from dynamic contrast-enhanced MR imaging. AJNR Am J Neuroradiol. 2016, 37:811-7. 10.3174/ajnr.A4623
- 26. Santarosa C, Castellano A, Conte GM, et al.: Dynamic contrast-enhanced and dynamic susceptibility contrast perfusion MR imaging for glioma grading: Preliminary comparison of vessel compartment and permeability parameters using hotspot and histogram analysis. Eur J Radiol. 2016, 85:1147-56. 10.1016/j.ejrad.2016.03.020
- Nguyen TB, Cron GO, Perdrizet K, et al.: Comparison of the diagnostic accuracy of DSC- and dynamic contrast-enhanced MRI in the preoperative grading of astrocytomas. AJNR Am J Neuroradiol. 2015, 36:2017-22. 10.3174/ajnr.A4398
- 28. Falk A, Fahlström M, Rostrup E, et al.: Discrimination between glioma grades II and III in suspected lowgrade gliomas using dynamic contrast-enhanced and dynamic susceptibility contrast perfusion MR imaging: a histogram analysis approach. Neuroradiology. 2014, 56:1031-8. 10.1007/s00234-014-1426-z
- Artzi M, Blumenthal DT, Bokstein F, Nadav G, Liberman G, Aizenstein O, Ben Bashat D: Classification of tumor area using combined DCE and DSC MRI in patients with glioblastoma. J Neurooncol. 2015, 121:349-57. 10.1007/s11060-014-1639-3
- Anzalone N, Castellano A, Cadioli M, et al.: Brain gliomas: multicenter standardized assessment of dynamic contrast-enhanced and dynamic susceptibility contrast MR images. Radiology. 2018, 287:933-43. 10.1148/radiol.2017170362
- 31. Bolcaen J, Descamps B, Acou M, et al.: In vivo DCE-MRI for the discrimination between glioblastoma and radiation necrosis in rats. Mol Imaging Biol. 2017, 19:857-66. 10.1007/s11307-017-1071-0
- 32. Liu Y, Zhou Y, Zhang XS, Shen BZ: Expression of VEGF and MMP-9 and MRI imaging changes in cerebral glioma. Oncol Lett. 2011, 2:1171-5. 10.3892/ol.2011.384