

Physically Active Adults with Low Back Pain do not Demonstrate Altered Deadlift Mechanics: A Novel Application of Myotonometry to Estimate Inter-Muscular Load Sharing

Jared M. McGowen¹[®], Stephanie R. Albin², Carrie W. Hoppes³, Jeffrey S. Forsse¹, John Abt⁴, Shane L. Koppenhaver⁵

¹ Health, Human Performance, and Recreation, Baylor University, ² School of Physical Therapy, Regis University, ³ Army-Baylor University Doctoral Program in Physical Therapy, Baylor University, ⁴ Children's Health Andrews Institute for Orthopaedics and Sports Medicine, ⁵ Doctoral Program in Physical Therapy, Baylor University

Keywords: Muscle stiffness, neuromuscular function, rehabilitation, clinical decision making https://doi.org/10.26603/001c.90707

International Journal of Sports Physical Therapy

Vol. 19, Issue 1, 2024

Background

Rehabilitation clinicians that work with physically active populations are challenged with how to safely return patients back to performing deadlift movements following low back injury. Application of reliable and valid tests and measures to quantify impairments related to low back pain (LBP) enhances clinical decision making and may affect outcomes. Myotonometry is a non-invasive method to assess muscle stiffness which has demonstrated significant associations with physical performance and musculoskeletal injury.

Hypothesis/Purpose

The purpose of this study was to compare the stiffness of trunk (lumbar multifidus [LM] and longissimus thoracis [LT]) and lower extremity (vastus lateralis [VL] and biceps femoris [BF]) muscles between individuals with and without LBP during the lying, standing, and deadlifting body positions.

Study Design

Cross-sectional cohort comparison

Methods

Muscle stiffness measures were collected in the VL, BF, LM, and LT muscles with participants in lying (supine and prone), standing, and the trap bar deadlift position. Separate analyses of covariance were conducted to compare absolute and relative muscle stiffness between the groups for each muscle and condition.

Results

Sixty-eight participants (41 female, 21.3 years, 34 LBP) volunteered for the study. Within the deadlift condition there was a significantly greater increase in the percent-muscle stiffness change in the VL (p = .029, 21.9%) and BF (p = .024, 11.2%) muscles in the control group than in the LBP group. There were no differences in percent-muscle stiffness changes for the standing condition nor were there any absolute muscle stiffness differences between the two groups for the three conditions.

Conclusion

No differences in muscle stiffness were identified in the lying, standing, or deadlifting conditions between participants with and without LBP. Differences in percent stiffness

changes were noted between groups for the deadlift position, however the differences were modest and within measurement error. Future studies should investigate the utility of myotonometry as a method to identify LBP-related impairments that contribute to chronic and/or recurrent low back injury.

Level of Evidence

Level 3

INTRODUCTION

Low back pain (LBP) is one of the most commonly reported musculoskeletal conditions amongst adults in the United States.¹ Although populations that consistently engage in physically demanding activities such as athletes, tactical professionals (law enforcement, first responders, military), and manual laborers may sometimes possess higher levels of fitness, they too have demonstrated high rates of low back injuries.²⁻⁷ The responsibility of musculoskeletal providers to effectively manage LBP and make appropriate return to activity decisions is arguably more challenging in physically active than in sedentary populations due to the physically demanding requirements of their sport or occupation.⁸⁻¹⁰ Deadlift variations are common movement patterns that are present within strength and conditioning programs and within physically demanding occupations.^{7,} ¹¹ Deadlift training is intended to strengthen the musculature of the lumbopelvic region and lower extremities to help individuals prepare for and improve upon the specific physical demands of their sport, occupation, and active lifestyle.¹²⁻¹⁴ However, little evidence exists to inform rehabilitation clinicians about when neuromuscular impairments resulting from low back injury may preclude an individual from safely returning to deadlift training or when using deadlift variations as a rehabilitation exercise is indicated.^{15,16} The high incidence of low back injuries amongst individuals who are expected to return to perform deadlift or deadlift-like movements (e.g. hip-hinge) places an urgent requirement on researchers and clinicians to further identify neuromuscular impairments that may be prohibitive of a safe return to deadlift training following low back injury.15-17

Stiffness is a mechanical property of muscle that has been suggested as an important measure of muscle health and function.¹⁸⁻²⁰ Myotonometry is a non-invasive, objective method of quantifying muscle stiffness through portable, handheld devices called myotonometers.²¹ During isometric contractions, muscle stiffness has demonstrated a stronger, positive linear relationship with force production ($R^2 = 0.977$) than the linear relationship demonstrated between electromyography (EMG) and force (R^2 = 0.936).²² The relationship between muscle stiffness and force indicates that stiffness may be a superior metric than EMG to determine the relative force that an individual muscle is contributing to a multi-muscle task.^{23,24} Furthermore, the ability of myotonometry to quantify muscle stiffness under relaxed and contracted states makes it a more versatile method for identifying neuromuscular impairments than EMG which can only measure neural drive from an actively contracting muscle.²⁵ The ability to reliably

identify impairments under passive conditions is not a trivial matter as numerous studies have demonstrated that abnormal passive muscle stiffness levels are present in individuals with a variety of neuromusculoskeletal disorders, including LBP.^{18,26,27} The MyotonPRO Digital Palpation Device (Myoton AS, Tallinn, Estonia) is a myotonometer that can quantify active and passive muscle stiffness in a quick and reliable manner that is necessary for obtaining tests and measures in clinical settings.^{28,29} Utilization of the MyotonPRO in individuals with LBP may help clinicians identify and monitor neuromuscular impairments to improve plan of care decisions that improve outcomes and help to reduce LBP re-injury rates.

Increased stiffness of lumbar spine muscles has been demonstrated in those with LBP, but this has only been demonstrated with the participants lying in prone.^{20,27,30} No study has investigated muscle stiffness in LBP populations in body positions relevant to sport and occupational function such as in the standing and deadlifting positions. Investigating muscle stiffness of both the lumbar spine and the lower extremities during these positions will help researchers and clinicians better understand how muscle stiffness behaves during loaded body positions and how this may be altered in those with LBP. Therefore, the primary purpose of this study was to compare the stiffness of trunk (lumbar multifidus [LM] and longissimus thoracis [LT]) and lower extremity (vastus lateralis [VL] and biceps femoris [BF]) muscles between individuals with and without LBP during the lying, standing, and deadlifting body positions. The secondary purpose was to compare percent-muscle stiffness changes that occur as participants transition from a relaxed condition to the standing (trunk musculature only) and deadlift positions (trunk and lower extremity musculature). Participants with LBP were hypothesized to demonstrate increased trunk muscle stiffness in the relaxed and standing conditions, but for the deadlift conditions individuals with LBP were hypothesized to exhibit decreased trunk and hamstring muscle stiffness with increased vastus lateralis muscle stiffness secondary due to pain-induced compensatory deadlift mechanics.

METHODS

PARTICIPANTS

Sixty-eight physically active adults were recruited for the study through word of mouth and flyers distributed across the university campus. Healthy volunteers were included if they had no complaint of lower extremity or spine pain that limited their participation in physical activity over the prior six months and were able to achieve the body position required to perform a trap bar deadlift (Figure 1). Healthy vol-



Figure 1. Trap bar deadlift position.

unteers were excluded if they were pregnant or had a body mass index (BMI) categorized as obese (30 kg/m²). Individuals with BMI that qualified as obese were excluded because subcutaneous adipose exceeding 20 mm in thickness may interfere with the MyotonPRO's ability to accurately measure muscle stiffness.³¹ Volunteers with LBP were included if they were currently experiencing pain between the 12th rib and the gluteal fold, had moderate LBP-related disability (defined as a score of \geq 20 on the Oswestry Disability Index [ODI]), and were able to achieve the trap bar deadlift position. Volunteers with LBP were excluded if they were pregnant, had a BMI that qualified as obese, or any current medical conditions of a serious nature (fracture, cancer, systemic disease, lower quarter neurological deficits). Participants were first screened for study eligibility (ODI score and BMI) via email and again the day of study participation. Prior to data collection, all participants signed an informed consent form approved by the university's Institutional Review Board (Project ID: 1921195-3) and the study was performed in accordance with the ethical standards of the Declaration of Helsinki.

PROCEDURES

Prior to collection of muscle stiffness measures, participants had their height and weight recorded with a stadiometer (Seca 777, Hamburg, Germany), then completed self-report questionnaires for demographic, activity level, exercise frequency, LBP-related disability, pain, and anxiety. Physical activity level was assessed with a single question, "Over the last year, how would you assess your activity level?" with possible responses being "inactive", "somewhat active", "active", and "very active." This question has demonstrated adequate reliability and validity to assess activity level when compared to more comprehensive questionnaires.³² Furthermore, activity level assessed with this single question has been shown to have a positive relationship with lumbar muscle stiffness.^{32,33} Weekly participation in aerobic and resistance exercise was assessed with a training frequency question that asked participants, "Over the last year, how frequently (on average) did you participate in at least 30 minutes of aerobic or resistance training?" with possible answers being "less than 1 day per week", "1-3 days per week", and "greater than 3 days per week." The numeric pain rating scale (NPRS) is an 11-point (0-10) scale that is a reliable and responsive measure in people with LBP.³⁴ Participants with LBP rated their pain in each body position that stiffness measures were collected. The ODI is a reliable and valid 0-100 scale measuring LBPrelated disability where higher scores relate to higher disability.³⁵ Anxiety was assessed with the Beck Anxiety Inventory (BAI) which is a 21-item questionnaire that scores somatic symptoms of anxiety on a 0-63 point scale (higher scores represent more anxiety).³⁶ The BAI has demonstrated adequate reliability and validity when compared to other anxiety questionnaires and anxiety assessed with this measure has been shown to demonstrate a negative relationship with muscle stiffness.^{36,37} Upon completion of questionnaires, participants with LBP received a subjective and neuromusculoskeletal exam to determine their appropriateness for the study.

Stiffness measurements were collected on the VL, BF, LM (L5 spinal segment), and LT (L1 spinal segment) muscles during the lying (prone/supine) and contracted (standing and trap bar deadlift positions) conditions. These muscles were selected due to their demonstrated importance to deadlift performance as well as spinal health and function in individuals with LBP.27,30,38,39 Measurement locations were determined using documented electromyography (EMG) that were with sites consistent recommendations stated on the device manufacture's website (myoton.com).⁴⁰ Measurements were acquired with the participant's shoes off, recorded from the more symptomatic side in individuals with LBP, and randomized to the left or right side in asymptomatic individuals. Measures were only collected on the more symptomatic side in participants with LBP to reduce the number of deadlift repetitions that participants had to perform. Furthermore, higher muscle stiffness measures have been found on the more symptomatic side in people with LBP.²⁰ Participants with LBP were asked to withhold from receiving any therapeutic interventions for their back pain and from taking any back pain specific medications (pain relievers, anti-inflammatories, muscle relaxers) 12 hours prior to study participation. All participants were asked to maintain their usual level of physical activity 24 hours prior to study participation.

MYOTONPRO MEASUREMENTS

Stiffness measures were obtained using a single measure with the single tap mode of the MyotonPRO to reduce the time required to obtain the measurements in the deadlift position. A previous study found good to excellent testretest reliability (intraclass correlation coefficients = 0.81 to



Figure 2. Obtaining stiffness measure of the lumbar multifidus muscle with the MyotonPRO.

0.97) using this method in the same muscles and body positions.²⁹ Muscle stiffness measures were acquired by the examiner positioning the probe of the MyotonPRO perpendicularly on the belly of the targeted muscles at the recommended locations.⁴⁰ The examiner lowered the device into measurement range which was identified by illumination of a green light on the device (Figure 2).⁴¹ A quick (15 ms) and light (0.4 N) device-initiated mechanical impulse force was transmitted through the probe, causing the targeted tissue to respond with a damped oscillation that was registered by the device accelerometer.⁴¹ The tissue's stiffness measurement (Nm) was computed and displayed on the device screen.²³

STANDARDIZATION OF MEASURES

Measures were first obtained in the lying (supine and prone) position then measured in the standing and trap bar deadlift positions. Lying measures were obtained in supine for the VL muscle and in prone for the BF, LM, and LT muscles. Prior to collecting stiffness measures, trunk angles were collected with an inclinometer at the T12 spinal segment in both the standing and deadlift positions to assess for spinal angle differences between groups. Lying and standing measures were collected in the same order (VL, BF, LM, LT) whereas the deadlift measurements were randomized to account for a possible order effect. Standing measures were obtained with the participants standing with a cone positioned between their feet to standardize stance width. Plastic cones were used to simulate the width and height of trap bar handles to prevent participants from lifting or resting on the trap bar while in the deadlift position (Figure 3). Participants were positioned between two

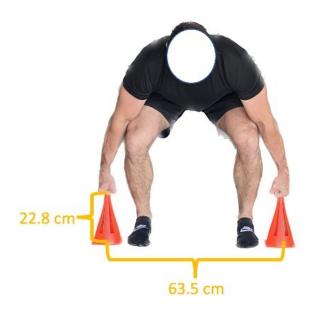


Figure 3. Trap bar deadlift set-up position. Cone dimensions represent height and width of trap bar handles.

cones that were 63.5 cm apart (width of the trap bar handles). Participants self-selected a stance width that was most comfortable for them to achieve the trap bar deadlift position. The stance width was recorded and maintained for all subsequent deadlift repetitions. Participants were required to squat to a depth that allowed them to contact the top of the cones with closed fists. The height of the cones (22.8 cm) was selected because it is the approximate height of the top of a trap bar handle when loaded with bumper plates. Furthermore, it was reasoned that abnormalities in muscle stiffness were most likely to occur when LBP participants were in the starting position of the deadlift where the highest spine loads have been shown to occur.42 Participants were required to squat and hold the trap bar deadlift position for approximately 2-5 seconds during four separate repetitions while the examiner obtained muscle stiffness measures on each muscle.

STATISTICAL ANALYSIS

Data analyses were performed using SPSS, version 28.0 software (IBM Corp, Armonk, New York) and included data from all 68 participants for the VL, BF, LM, and LT for the relaxed and deadlift positions and the LM and LT for the standing position. Sixty-eight participants ensured at least 80% power to detect an effect size of 0.7 (28 Nm) between groups when using a 2-tailed alpha of .05. Baseline characteristics were summarized by treatment group and compared with independent t-tests for parametric data and Mann-Whitney-U and Chi-squared tests for categorical and dichotomous data, respectively. Variables that were significantly different per group were used in linear regression analyses with each muscle stiffness outcome to assess for use as a covariate. Variables that were statistically different between groups and linearly related to the dependent variable were used as covariates. Additionally, variables such

Table 1.	Characteristics	of participar	its per group
----------	-----------------	---------------	---------------

	Asymptomatic Controls	LBP	<u>p-value</u>	
Participants	34	34		
% Female	44%	76%	0.01*	
Age	20.7 (5.1)	21.9 (4.5)	0.97	
Body Mass Index	23.4 kg/m ² (2.7)	22.5 kg/m ² (2.6)	0.98	
Physical Activity Level			0.05	
Inactive	O (O%)	3 (9%)		
Somewhat active	7 (21%)	4 (12%)		
Active	4 (12%)	14 (41%)		
Very active	23 (67%)	13 (38%)		
Aerobic Frequency			0.02*	
< 1 x per week	2 (6%)	8 (24%)		
1-3 x per week	17 (50%)	18 (52%)		
> 3 x per week	15 (44%)	8 (24%)		
Resistance Frequency			0.05	
< 1 x per week	7 (21%)	10 (29%)		
1-3 x per week	10 (29%)	16 (47%)		
> 3 x per week	17 (50%)	8 (24%)		
ODI	N/A	14.0 (3.9)	N/A	
NPRS	N/A	4 (2)	N/A	
BAI	4.5 (5.4)	11.4 (8.4)	< 0.001*	

ODI, Oswestry Disability Index for low back pain disability (scored 0-50 with higher scores indicating greater disability). NPRS, numeric pain rating scale (scored 0-10 with higher scores indicating greater pain). BAI, Beck's Anxiety Inventory (scored 0-63 with higher scores indicating greater anxiety). LBP, low back pain. Values reported as mean (SD) except where noted. *Statistically significant difference at p < 0.05.

as physical activity that have demonstrated a linear relationship with muscle stiffness²⁰ were assessed for use as a covariate with linear regression analyses. Separate analyses of covariance were conducted to compare absolute and relative (percent-muscle stiffness change from the relaxed to the standing and deadlifting positions) muscle stiffness measures between the groups for each muscle and condition. Percent-muscle stiffness change was calculated for each muscle of interest for the standing and deadlift conditions with the appropriate formula ([standing or deadlift stiffness – lying stiffness]/lying stiffness x 100). Finally, ttests were used to compare trunk angles and stance widths between groups.

RESULTS

Table 1 displays demographic, physical activity, pain, and low back disability data for each group. Sex and physical activity were identified as significant covariates. Comparisons of adjusted means and 95% confidence intervals (CI) are displayed for each muscle across the three conditions in Table 2. The only difference between the two groups was in the VL muscle with the LBP group demonstrating a higher adjusted mean stiffness of 22 Nm (95% CI, 0.21 to 43.8) in the relaxed position. Table 3 and Figure 4 displays percent-muscle stiffness changes that occurred as participants transitioned from the relaxed to the standing and deadlift positions. There were no significant differences in percentmuscle stiffness change between the lying and standing positions between the two groups. Within the trap bar deadlift position there was a significantly greater increase in the percent-muscle stiffness change that occurred in the VL (p= .029, 21.9%) and BF (p = .024, 11.2%) muscles in the control group than in the LBP group. No between group differences were identified for standing and deadlifting trunk angles or for deadlifting stance widths (p-value range = .205 to .573). Mean LBP intensity was 4/10 (SD = 2) for each body position and 11 (32%) of the participants with LBP reported at least a 1-point increase in pain when they were in the deadlift position.

DISCUSSION

Little is known about how thigh and trunk muscle stiffness behave in individuals with LBP under loaded conditions. The results of this study demonstrate that in young, physically active adults with moderately disabling LBP, stiffness of the VL, BF, LM, and LT muscles are not statistically different than healthy controls during standing and deadlifting positions. Although significant percent-muscle stiffness increases were found in the control group for the VL and BF muscles for the deadlift position, these increases were modest and within measurement error.²⁹ These findings contribute to the growing body of literature regarding how muscle stiffness relates to LBP and how myotonometry may be used to monitor for neuromuscular deficits that have been difficult to reliably quantify with other clinical methods.⁴³ Furthermore, these findings have important

	Mean Stiffness (SD)		Adjusted Mean Differences ^a (95% Confidence Interval)	
	Control (n = 34)	LBP (n = 34)		<i>p</i> -value
VL				
Relaxed	303.9 (32.5)	314.8 (57.8)	22.0 (0.21 to 43.8)	0.05*
Standing	427.3 (115.0)	375.2 (102.9)	19.0 (-66.6 to 28.7)	0.43
Deadlift	640.1 (175.0)	553.5 (186.5)	26.1 (-49.6 to 101.8)	0.49
BF				
Relaxed	263.0 (50.4)	251.9 (51.6)	6.3 (-14.8 to 27.4)	0.56
Standing	291.0 (86.6)	272.5 (68.2)	7.4 (-25.3 to 40.1)	0.65
Deadlift	285.7 (106.6)	230.6 (55.2)	28.0 (-8.3 to 64.3)	0.13
LM				
Relaxed	234.1 (71.5)	237.3 (66.4)	11.1 (-23.4 to 45.6)	0.52
Standing	291.7 (153.7)	301.3 (156.5)	32.6 (-43.8 to 109.0)	0.40
Deadlift	675.2 (279.1)	612.7 (244.6)	0.7 (-121.7 to 123.0)	0.99
LT				
Relaxed	316.5 (50.5)	312.6 (55.7)	2.4 (-24.7 to 29.4)	0.86
Standing	366.1 (105.4)	364.0 (124.0)	7.4 (-50.6 to 65.4)	0.80
Deadlift	645.0 (173.1)	614.2 (216.6)	2.3 (-94.4 to 99.0)	0.96

Table 2. Muscle stiffness comparisons per condition, all values are reported in Newton-meters.

VL, vastus lateralis; BF, biceps femoris; LM, lumbar multifidus; LT, longissimus thoracis. ^aMean stiffness differences and confidence interval values are adjusted for sex and activity level. ^aStatistically significant difference at p < or = 0.05.

	Percent Mean Stiffness Change (SD)		Adjusted Mean Differences ^a (95% Confidence Interval)	
	Control (n = 34)	LBP (n = 34)		<i>p</i> -value
Standing				
LM	21.5 (42.1)	22.3 (38.2)	12.0 (-14.1 to 25.9)	0.56
LT	15.2 (26.5)	14.9 (26.3)	2.7 (-11.1 to 15.5)	0.74
Deadlift				
VL	107.9 (43.3)	73.6 (44.6)	21.9 (2.3 to 41.4)	0.03*
BF	6.7 (24.6)	-8.0 (13.8)	11.2 (1.5 to 21.0)	0.02*
LM	184.9 (78.0)	155.7 (74.2)	12.0 (-23.8 to 47.8)	0.50
LT	101.9 (41.8)	95.2 (59.7)	2.7 (-22.2 to 27.7)	0.83

Table 3. Percent muscle stiffness changes between relaxed and deadlift conditions, all values are reported in Newton-meters

LBP, low back pain; VL, vastus lateralis; BF, biceps femoris; LM, lumbar multifidus; LT, longissimus thoracis; ^aMean stiffness and confidence interval values are adjusted for sex and activity level. *Statistically significant difference at p < 0.05.

implications for rehabilitation providers managing physically active individuals who have LBP and will be returning to deadlift training and/or performing similar deadlift-like movements upon completion of rehabilitation.

The lack of statistically significant differences in muscle stiffness between the two groups across all conditions was not an expected finding. Earlier studies have shown increased erector spinae stiffness in those with LBP and demonstrated that muscle stiffness was positively related to pain scores and negatively related to function.^{27,30} In contrast, this study found no between group differences for LM or LT stiffness in the relaxed condition despite the participants with LBP exhibiting higher levels of LBP-related

disability than in previous studies (<u>Table 1</u>). However, it is worth highlighting that in younger individuals with LBP, Ilahi et al.³⁰ found that only females demonstrated an increase in relaxed erector spinae stiffness compared to ageand activity-matched controls. Moreover, Wu et al.²⁷ found statistically significant increases in a mixed-sex group of elderly with LBP, but the mean muscle stiffness differences (42.1 Nm) between the healthy and LBP groups did not exceed minimal detectable differences reported in their study (47.2-50.2 Nm). The inconsistency in findings clearly highlights that further research is necessary to better understand the relationship between lumbar musculature stiffness and LBP.

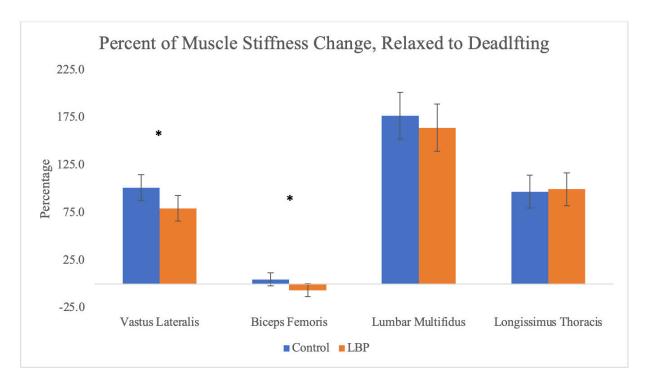


Figure 4. Graph depicting percent-muscle stiffness change per muscle for the trap bar deadlift in healthy controls and participants with low back pain (LBP).

*Statistically significant difference at p < or equal to 0.05.

The hypotheses that participants with LBP would demonstrate differences in the standing and deadlift postures was also mostly unsupported by the results. Movement and motor control impairments are known to occur secondary to pain.44,45 Thus, it was expected that LBP symptoms would be exacerbated under these relatively loaded conditions, leading to compensatory motor control strategies that would manifest as altered stiffness in the muscles of interest. The absence of muscle stiffness differences in these positions suggests there may have been an insufficient level of pain intensity and/or LBP-related disability to result in muscle dysfunction. It is also possible that the MyotonPRO measures were not sensitive enough to detect mild differences that may have been present between the two groups. Specific to the deadlift position, pain data analysis demonstrated that only 32% (n = 11) of the LBP group reported an increase in pain while they were in the deadlift posture. Furthermore, only two participants reported a 2-point increase in pain that is necessary for clinical significance.³⁴ Though speculative, it may be that a compensatory deadlift posture (e.g. adopting a more upright trap bar deadlift set-up) may only be found in individuals who experience a clinically meaningful increase in LBP symptoms that are specific to the deadlift set-up position. Another explanation could be that individuals with mild to moderate levels of spinal pain and disability only demonstrate compensatory trap bar deadlift mechanics with deadlift attempts of higher intensities. Future studies should seek to answer these questions as they could help to further clarify when individuals with LBP may be safe to return to deadlift training and at what capacity.

This is the first study to use muscle stiffness to determine inter-muscular load sharing percentages while performing a variation of the deadlift. Figure 4 and Table 3 demonstrate the relative change in muscle stiffness as participants transitioned from the lying (relaxed) position to the deadlift position. The substantial increases in stiffness for the VL, LM, and LT muscles suggests that these muscles are important force producing muscles during performance of the trap bar deadlift. These results are supported by previously recorded deadlift muscle activation patterns measured with EMG,³⁸ and demonstrates the versatility of myotonometry as a method to estimate individual muscle contributions (through the surrogate of muscle stiffness) to a compound movement such as the deadlift.

Finally, this is the first study to compare performance of a deadlift variation between healthy and LBP cohorts using muscle stiffness as an outcome. The results are largely consistent with a similar study that used force production and EMG to compare isometric deadlift performance between individuals with and without LBP.¹⁶ Stock et al.¹⁶ demonstrated that individuals with acute, non-specific LBP had the same force output and muscle excitability patterns as healthy controls. Collectively, these findings suggest that within young, active individuals with mild to moderate pain levels and LBP-related disability, deadlift variation training may be able to be performed without any added concern for re-injury secondary to lumbar spine or lower extremity neuromuscular impairments. Additionally, this study adds to the growing body of literature evaluating if and how myotonometry may be a useful clinical method to assist clinicians with detecting neuromuscular deficits.

LIMITATIONS

The present study had several important limitations. First, the generalizability of this study is limited to young, active individuals with mild to moderate levels of LBP-related disability. Similarly, the deadlift variation used in this study was specific to the trap bar and the starting ("initial pull") position of the lift and therefore does not apply to other deadlift variations, positions, or to dynamic movements. Additionally, the deadlift inter-muscular stiffness percentages identified in this study occurred under minimal load (body weight) and may not accurately represent individual muscle contributions as isometric deadlifts are performed at higher intensities. Finally, the MyotonPRO measurements are limited by subcutaneous fat thickness that exceeds 2 cm and can only target superficial tissues that can me palpated.³¹ Despite attempts to combat these limitations by requiring participants to have BMIs less than $30 \text{kg}/\text{m}^2$ and using recommended muscle stiffness measurement locations it is possible that fat, non-target muscle, and fascia located over the target muscles may have interfered with some muscle stiffness measures.

CONCLUSION

The results of this study indicate that no significant differences in muscle stiffness exist between participants with LBP and healthy controls in the lying, standing, or deadlifting conditions. Although differences in percent-muscle stiffness changes were noted between groups for the deadlift position, the differences were within measurement error. Future studies should seek to expand on these findings by using myotonometry to further investigate the relationships between muscle stiffness and deadlift performance in LBP populations of varying degrees of pain and/or disability.

CONFLICTS OF INTEREST

The authors report no conflicts of interest.

Submitted: June 22, 2023 CST, Accepted: November 06, 2023 CST © The Author(s)

This is an open-access article distributed under the terms of the Creative Commons Attribution 4.0 International License (CCBY-NC-4.0). View this license's legal deed at https://creativecommons.org/licenses/by-nc/4.0 and legal code at https://creativecommons.org/licenses/by-nc/4.0/legalcode for more information.

REFERENCES

1. Manchikanti L, Singh V, Falco FJE, Benyamin RM, Hirsch JA. Epidemiology of low back pain in adults. *Neuromodulation*. 2014;17(Suppl 2):3-10. <u>doi:10.111</u> <u>1/ner.12018</u>

2. Knox J, Orchowski J, Scher DL, Owens BD, Burks R, Belmont PJ. The incidence of low back pain in active duty United States military service members. *Spine*. 2011;36(18):1492-1500. <u>doi:10.1097/brs.0b013e3181f</u> <u>40ddd</u>

3. Antwi-Afari MF, Li H, Edwards DJ, et al. Identification of potential biomechanical risk factors for low back disorders during repetitive rebar lifting. *Construct Innovat.* 2018;18(2). <u>doi:10.1108/ci-05-201</u> <u>7-0048</u>

4. Strömbäck E, Aasa U, Gilenstam K, Berglund L. Prevalence and consequences of injuries in powerlifting: a cross-sectional study. *Orthop J Sports Med.* 2018;6(5):2325967118771016. <u>doi:10.1177/2325</u> <u>967118771016</u>

5. Hootman JM, Dick R, Agel J. Epidemiology of collegiate injuries for 15 sports: summary and recommendations for injury prevention initiatives. *J Athl Train*. 2007;42(2):311-319.

6. Aasa U, Svartholm I, Andersson F, Berglund L. Injuries among weightlifters and powerlifters: a systematic review. *Br J Sports Med*. 2017;51(4):211-219. <u>doi:10.1136/bjsports-2016-0960</u> <u>37</u>

7. Kong PW, Kan TYW, Mohamed Jamil RAGB, et al. Functional versus conventional strength and conditioning programs for back injury prevention in emergency responders. *Front Bioeng Biotechnol*. 2022;10. doi:10.3389/fbioe.2022.918315

8. Rhon DI, Teyhen DS, Kiesel K, et al. Recovery, rehabilitation, and return to full duty in a military population after a recent injury: differences between lower-extremity and spine injuries. *Arthrosc Sports Med Rehabil.* 2022;4(1):e17-e27. doi:10.1016/j.asmr.20 21.09.028

9. Ardern CL, Glasgow P, Schneiders A, et al. 2016 Consensus statement on return to sport from the First World Congress in Sports Physical Therapy, Bern. *Br J Sports Med.* 2016;50(14):853-864. <u>doi:10.11</u> <u>36/bjsports-2016-096278</u> 10. Buckthorpe M, Frizziero A, Roi GS. Update on functional recovery process for the injured athlete: return to sport continuum redefined. *Br J Sports Med*. 2019;53(5):265-267. <u>doi:10.1136/bjsports-2018-09934</u> 1

11. Army USGU. *Field Manual FM* 7-22 *Holistic Health and Fitness October 2020*. <u>https://armypubs.army.mil/epubs/DR_pubs/DR_a/ARN30964-FM_7-22-001-WE</u> B-4.pdf

12. STP 21-1-SMCT; Soldiers mannual of common tasks, warrior skills, level 1. <u>https://armypubs.army.m</u> <u>il/ProductMaps/PubForm/Details.aspx?PUB_ID=10278</u> 43

13. Zatsiorsky VM, Kraemer WJ. *Science and Practice of Strength Training, Second Edition*. Second edition. Human Kinetics, Inc.; 2006.

14. Nigro F, Bartolomei S. A comparison between the squat and the deadlift for lower body strength and power training. *J Hum Kinet*. 2020;73(1):145-152. do i:10.2478/hukin-2019-0139

16. Stock MS, Bodden ME, Bloch JM, Starnes KL, Rodriguez G, Girts RM. Acute, non-specific low back pain does not impair isometric deadlift force or electromyographic excitation: a cross-sectional study. *Sports*. 2022;10(11):168. <u>doi:10.3390/sports101</u> <u>10168</u>

17. Molloy JM, Pendergrass TL, Lee IE, Hauret KG, Chervak MC, Rhon DI. Musculoskeletal injuries and United States Army readiness. Part II: management challenges and risk mitigation initiatives. *Mil Med*. 2020;185(9-10):e1472-e1480. <u>doi:10.1093/milmed/us</u> <u>aa028</u>

18. Gervasi M, Barbieri E, Capparucci I, et al. Treatment of achilles tendinopathy in recreational runners with peritendinous hyaluronic acid injections: a viscoelastometric, functional, and biochemical pilot study. *J Clin Med.* 2021;10(7):1397. doi:10.3390/jcm10071397

19. Albin SR, Koppenhaver SL, MacDonald CW, et al. The effect of dry needling on gastrocnemius muscle stiffness and strength in participants with latent trigger points. *J Electromyogr Kinesiol*. 2020;55:102479. doi:10.1016/j.jelekin.2020.102479

20. Koppenhaver S, Gaffney E, Oates A, et al. Lumbar muscle stiffness is different in individuals with low back pain than asymptomatic controls and is associated with pain and disability, but not common physical examination findings. *Musculoskel Sci Pract.* 2020;45:102078. doi:10.1016/j.msksp.2019.102078

21. Davidson MJ, Bryant AL, Bower WF, Frawley HC. Myotonometry reliably measures muscle stiffness in the thenar and perineal muscles. *Physiotherapy Canada*. 2017;69(2):104-112. doi:10.3138/ptc.2015-85

22. Bouillard K, Nordez A, Hug F. Estimation of individual muscle force using elastography. *PLoS ONE*. 2011;6(12):e29261. <u>doi:10.1371/journal.pone.00</u> 29261

23. Kelly JP, Koppenhaver SL, Michener LA, Proulx L, Bisagni F, Cleland JA. Characterization of tissue stiffness of the infraspinatus, erector spinae, and gastrocnemius muscle using ultrasound shear wave elastography and superficial mechanical deformation. *J Electromyogr Kinesiol*. 2018;38:73-80. <u>doi:10.1016/j.j</u> <u>elekin.2017.11.001</u>

25. Hug F, Hodges PW, Tucker K. Muscle force cannot be directly inferred from muscle activation: illustrated by the proposed imbalance of force between the vastus medialis and vastus lateralis in people with patellofemoral pain. *J Orthop Sports Phys Ther.* 2015;45(5):360-365. <u>doi:10.2519/jospt.2015.590</u> <u>5</u>

26. Kawai T, Takamoto K, Bito I. Previous hamstring muscle strain injury alters passive tissue stiffness and vibration sense. *J Bodyw Mov Ther*. 2021;27(0):573-578. doi:10.1016/j.jbmt.2021.05.002

27. Wu Z, Zhu Y, Xu W, Liang J, Guan Y, Xu X. Analysis of biomechanical properties of the lumbar extensor myofascia in elderly patients with chronic low back pain and that in healthy people. *BioMed Res Int.* 2020;2020:1-10. doi:10.1155/2020/7649157

28. Chuang LL, Wu CY, Lin KC, Lur SY. Quantitative mechanical properties of the relaxed biceps and triceps brachii muscles in patients with subacute stroke: a reliability study of the myoton-3 myometer. *Stroke Res Treat.* 2012;2012:617694. <u>doi:10.1155/201</u>2/617694

29. McGowen JM, Hoppes CW, Forsse JS, Albin SR, Abt J, Koppenhaver SL. Myotonometry is capable of reliably obtaining trunk and thigh muscle stiffness measures in military cadets during standing and squatting postures. *Mil Med.* Published online May 19, 2023:usad179. doi:10.1093/milmed/usad179

30. Ilahi S, T. Masi A, White A, Devos A, Henderson J, Nair K. Quantified biomechanical properties of lower lumbar myofascia in younger adults with chronic idiopathic low back pain and matched healthy controls. *Clin Biomech*. 2020;73:78-85. <u>doi:10.1016/j.c</u> <u>linbiomech.2019.12.026</u>

31. Peipsi A, Kosemets M. MyotonPRO User Manual. Published online 2020:115.

32. Gill DP, Jones GR, Zou G, Speechley M. Using a single question to assess physical activity in older adults: a reliability and validity study. *BMC Med Res Methodol*. 2012;12(1):20. <u>doi:10.1186/1471-2288-12-2</u> <u>0</u>

33. Koppenhaver SL, Scutella D, Sorrell BA, et al. Normative parameters and anthropometric variability of lumbar muscle stiffness using ultrasound shearwave elastography. *Clin Biomech*. 2019;62:113-120. <u>d</u> <u>oi:10.1016/j.clinbiomech.2019.01.010</u>

34. Childs JD, Piva SR, Fritz JM. Responsiveness of the numeric pain rating scale in patients with low back pain. *Spine*. 2005;30(11):1331-1334. <u>doi:10.109</u>7/01.brs.0000164099.92112.29

35. Fritz JM, Irrgang JJ. A comparison of a modified Oswestry Low Back Pain Disability Questionnaire and the Quebec Back Pain Disability Scale. *Phys Ther*. 2001;81(2):776-788. <u>doi:10.1093/ptj/81.2.776</u>

36. JULIAN LJ. Measures of anxiety. *Arthritis Care Res* (*Hoboken*). 2011;63(S11). <u>doi:10.1002/acr.20561</u>

37. Hoffman LR, Koppenhaver SL, MacDonald CW, et al. Normative parameters of gastrocnemius muscle stiffness and associations with patient characteristics and function. *Int J Sports Phys Ther*. 2021;16(1):41-48. doi:10.26603/001c.18803

38. Martín-Fuentes I, Oliva-Lozano JM, Muyor JM.
Electromyographic activity in deadlift exercise and its variants. A systematic review. *PLoS ONE*.
2020;15(2):e0229507. doi:10.1371/journal.pone.02295
07

39. Macdonald DA, Dawson AP, Hodges PW. Behavior of the lumbar multifidus during lower extremity movements in people with recurrent low back pain during symptom remission. *J Orthop Sports Phys Ther.* 2011;41(3):155-164. doi:10.2519/jospt.2011.3410

40. Leis AA, Schenk MP. *Atlas of Nerve Conduction Studies and Electromyography*. Oxford University Press; 2013. <u>doi:10.1093/med/9780199754632.001.00</u> <u>01</u>

41. McGowen JM, Hoppes CW, Forsse JS, Albin SR, Abt J, Koppenhaver SL. The utility of myotonometry in musculoskeletal rehabilitation and human performance programming. *J Athl Train*. Published online July 14, 2022. doi:10.4085/1062-6050-0616.21

42. Cholewicki J, McGill SM, Norman RW. Lumbar spine loads during the lifting of extremely heavy weights. *Med Sci Sports Exerc*. 1991;23(10):1179-1186. doi:10.1249/00005768-199110000-00012

43. Rathbone ATL, Grosman-Rimon L, Kumbhare DA. Interrater agreement of manual palpation for identification of myofascial trigger points: a systematic review and meta-analysis. *Clin J Pain*. 2017;33(8):715-729. <u>doi:10.1097/ajp.0000000000004</u> 59

44. O'Sullivan P. Diagnosis and classification of chronic low back pain disorders: maladaptive movement and motor control impairments as underlying mechanism. *Man Ther*. 2005;10(4):242-255. doi:10.1016/j.math.2005.07.001

45. Hodges PW, Tucker K. Moving differently in pain: A new theory to explain the adaptation to pain. *Pain*. 2011;152(3):S90-S98. doi:10.1016/j.pain.2010.10.020