

Article

Enhancement of Long-Range Surface Plasmon Excitation, Dynamic Range and Figure of Merit Using a Dielectric Resonant Cavity

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Abstract: In this paper, we report a theoretical framework on the effect of multiple resonances inside the dielectric cavity of insulator-insulator-metal-insulator (IIMI)-based surface plasmon sensors. It has been very well established that the structure can support both long-range surface plasmon polaritons (LRSPP) and short-range surface plasmon polaritons (SRSPP). We found that the dielectric resonant cavity under certain conditions can be employed as a resonator to enhance the LRSPP properties. These conditions are: (1) the refractive index of the resonant cavity was greater than the refractive index of the sample layer and (2) when light propagated in the resonant cavity and was evanescent in the sample layer. We showed through the analytical calculation using Fresnel equations and rigorous coupled wave theory that the proposed structure with the mentioned conditions can extend the dynamic range of LRSPP excitation and enhance at least five times more plasmon intensity on the surface of the metal compared to the surface plasmon excited by the conventional Kretschmann configuration. It can enhance the dip sensitivity and the dynamic range in refractive index sensing without losing the sharpness of the LRSPP dip. We also showed that the interferometric modes in the cavity can be insensitive to the surface plasmon modes. This allowed a self-referenced surface plasmon resonance structure, in which the interferometric mode measured changes in the sensor structure and the enhanced LRSPP measured changes in the sample channel.

Keywords: long-range surface plasmon polariton; short-range surface plasmon polariton; dielectric resonant cavity; multiple reflections; plasmonic; surface plasmon resonance sensor; instrumentation

1. Introduction

Surface Plasmon Resonance (SPR) has been a powerful scientific tool for biological protein kinetic studies [1–4]. The SPR sensing platforms are usually implemented based on the optical configuration proposed by Kretschmann-Raether in 1968 [5,6]. That same year, Otto also proposed an optical configuration that allowed the SPR to be excited on a bulk gold surface [7]. The Otto configuration has not been exploited much in biosensing applications since the structure requires a very narrow spacing gap (less than a wavelength spacing height) between the coupling prism and the bulk plasmonic metal.

It has been very well established that double plasmonic metal interfaces such as: (1) insulator-metal-insulator (IMI) structures [8] or (2) metal-insulator-metal (MIM) structures [9–11] can support two plasmonic modes, so-called, long-range surface plasmon polaritons (LRSPP) and short-range surface plasmon polaritons (SRSPP) [12]. These LRSPP and SRSPP modes have been experimentally verified by several groups including Lee et al. [13] and Slavík et al. [14]. The LRSPP mode has several preferable features over the SRSPP mode including (1) it can be excited at a lower incident k -vector (lower angle and lower incident wavelength) and (2) it has a higher figure of merit (FoM). The FoM

is a quantity used to measure the detection performance, relative to a ratio of the sensitivity to the full-width half maximum (FWHM) of the reflectance dip position in SPR biosensing platform. This is due to the change of the SPR signal upon local refractive index changes. Thus the narrow reflection dip and enhancement of the sensitivity improves the *FoM* of SPR sensors [15]. The enhanced *FoM* has proven itself very useful in biosensing platforms and applications. Khan et al. [16] reported the implementation of an interdigitated capacitor (IDC)-based glucose biosensor with high detection sensitivity of 10^{-7} refractive index units (RIU) and wide dynamic range for fast response and recovery in which the limit of detection reached nanomolar concentration. Zhen et al. [17] has reported an ultra-sensitive plasmonic biosensor having the detection sensitivity down to 10^{-18} molar concentration of ssDNA sensing by nanostructures hybridized gold thin film. Yu et al. [11] have recently proposed the side-coupled Fabry-Perot cavity as a resonator for ultrahigh wavelength selection. Wu et al. [18] have reported the theoretical performance of MIM plasmonic structures with a ring resonator.

The LRSPP and SRSPP modes occur due to a hybridization between the two bound SPR modes on two metal surfaces. This lower excitation angle, of course, reduces the requirement of using high numerical aperture (NA) objective lens to excite the LRSPP [19]. The LRSPP does, however, still have two main issues. Firstly, it does have a very limited dynamic range since it can only be excited when refractive indices sandwiching the plasmonic metal layer are similar. Secondly, although the LRSPP reflectance dip is much narrower than the conventional Kretschmann SPR, the dip sensitivity in refractive index sensing is much less. The longer propagation length of LRSPP can offer a larger detection area of the binding sample region allowing the LRSPP to be more sensitive than the conventional SRSPP [12].

The insulator-insulator-metal-insulator (IIMI) structure for LRSPP excitation was first introduced by Abelès and Lopez-Rios in 1974 [20]. The major differences for the IIMI structure [13,14,20] reported by others and this paper are that we are interested in the IIMI as shown in Figure 1 under certain conditions which were: (1) the refractive index of the dielectric resonant cavity (n_0) was larger than the refractive index of the sensing sample region (n_3); (2) the k -vectors where the light propagated in the dielectric cavity were evanescent in the sample region.

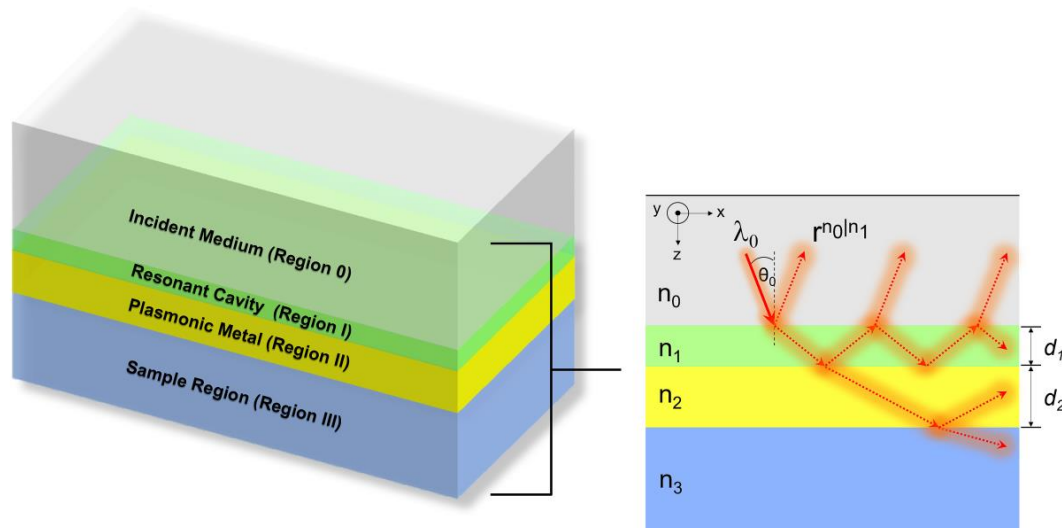


Figure 1. The proposed IIMI structure. The incident medium (Region 0) was a semi-infinite glass substrate with refractive index n_0 serving as an incident medium. The resonant cavity (Region I) was made of a dielectric layer with refractive index n_1 and thickness d_1 . The plasmonic medium (Region II) was a noble metal layer with refractive index n_2 and thickness d_2 . The sample medium (Region III) was also the dielectric layer with refractive index n_3 which was the sample channel of the proposed SPR sensor.

The thickness of the dielectric cavity considered here ranged from 0.5 to 4 μm , which is much thicker than the LRSPP structures reported in the literature. Thus the proposed structure served as a resonator allowing multiple reflections inside the cavity and interferometric modes. By matching the k -vectors of the resonant cavity and the LRSPP, these conditions can enhance the properties of the LRSPP excitation, dynamic range and FoM in SPR sensing applications. To the best of the authors' knowledge, these features of the LRSPP excited through the dielectric resonant cavity have never been reported before.

2. Structure and Simulation Methods

2.1. Simulation Methods

The multi-layer type structure shown in Figure 1 was analysed using a transfer matrix approach for Fresnel equations [21]. The following variables were used throughout the paper: r_p and t_p are the reflection coefficient and transmission coefficient for p-polarization and s-polarization, respectively. Rigorous coupled wave theory [22] has been implemented to determine the mode profiles in the structure and stored optical power per unit length in the resonant cavity. E_x , E_y and E_z are the electric fields along the x -, y - and z -axes, respectively. H_x , H_y and H_z are the magnetic fields along the x -, y - and z -axes, respectively. The axes were defined as indicated in Figure 1.

2.2. Terms and Definitions

There are several definitions for figure of merit (FoM) [23]. The commonly used FoM that is defined to evaluate the dip position measurement in SPR systems [15], which is also used in this paper and defined as:

$$FoM = \frac{S}{FWHM} \quad (1)$$

where FoM is the figure of merit for dip position measurement.

S is the sensitivity term. In the SPR biosensing platforms, the sensitivity is herein defined in term of $dk_{x,resonance}/dn_{sample}$ for bulk sensitivity where the $k_{x,resonance}$ is the k -vector position of the resonant mode along the x -axis and the n_{sample} is the refractive index of the bulk sample medium.

FWHM is the full-width half maximum of the reflectance dip. The width of the dip is measured at 0.5 intensity level of the reflectance curve. Dynamic range (D) is defined as the range of refractive indices that the plasmonic reflectance dip intensity is below 0.25. The illumination k -vector in this paper is presented as a normalized k -vector, $\frac{k_x}{k_{free-space}} = n_0 \sin \theta_0$ or numerical aperture (NA).

3. Results and Discussion

3.1. LRSPP and SRSPP

Before looking at the IIMI plasmonic structure, let us consider the case where we only had pure plasmonic modes in a three homogenous-layer structure, when either d_1 was treated as 0 nm or n_0 equalled n_1 . The structure was a thin plasmonic gold layer with thickness d_2 sandwiched by two semi-infinite dielectric media with refractive indices of n_0 and n_3 . Gold has been chosen in this study since it is suitable for biological sensor fabrication because gold is chemically stable, inductive and non-toxic to biological samples [3,24]. The refractive index of gold is $0.18344 + 3.4332i$ at 633 nm free-space wavelength (λ) extracted from Johnson and Christy [25]. Note that we have compared and discussed the performance of silver with refractive index of $0.056206 + 4.2776i$ [25] as reported and shown in Figure S1 and Table S1 in the Supplementary Information (SI). The silver results tell the same story as the gold results. The results are therefore omitted from the main manuscript. Figure 2a–c shows $\ln(|r_p|^2)$ for different values n_0 ranging from 1.29 (Teflon™ AF2400 [26]), 1.33 and 1.3616 (potassium fluoride: KF [27]), respectively, when n_3 was fixed at 1.33. It is important to point out that the $n_0 \sin \theta_0$ range in the calculation was 1.33 to 1.52. This made the $\sin \theta_0$ greater than 1 indicating

that the SPR modes shown here were excited by an evanescent wave and the structure required a higher coupling index medium or a grating to satisfy the k -vector condition. Of course, if another higher refractive coupling layer had been added to the structure, this would form an IIMI structure. The interferometric modes in the IIMI can unavoidably interact with the plasmonic modes explained in the later section. These Fresnel calculations have enabled us to identify the mode coupling strength and the k -vector positions for the pure SRSPP and pure LRSPP modes without any influence from the coupling layer. It has been very well established that the LRSPP exists under certain conditions, which are (1) the refractive indices, which sandwich the plasmonic metal, have to be similar [12] and (2) the plasmonic metal thickness is usually thinner than the metal used in Kretschmann configuration. Figure 2b showed that when the n_0 and n_3 refractive indices were perfectly matched, the coupling strength for the both LRSPP (symmetric mode) and SRSPP (asymmetric mode) were similar. On the other hand, when they were mismatched, the LRSPP had a stronger coupling compared to the SRSPP when n_0 was lower than n_3 as shown in Figure 2a in a comparison with Figure 2c. The separation in k -vector space between the two SPP modes was wider when the plasmonic gold was thin. On the other hand, when the gold was thicker than 75 nm the two SPP modes combined to a single mode. The LRSPP k -vector appeared at a larger k -vector value with the larger n_0 refractive index. The thickness of the gold d_2 and the refractive index sandwiching the plasmonic gold will be employed as a key parameter to vary the k -vector positions of the two plasmonic modes in the next section.

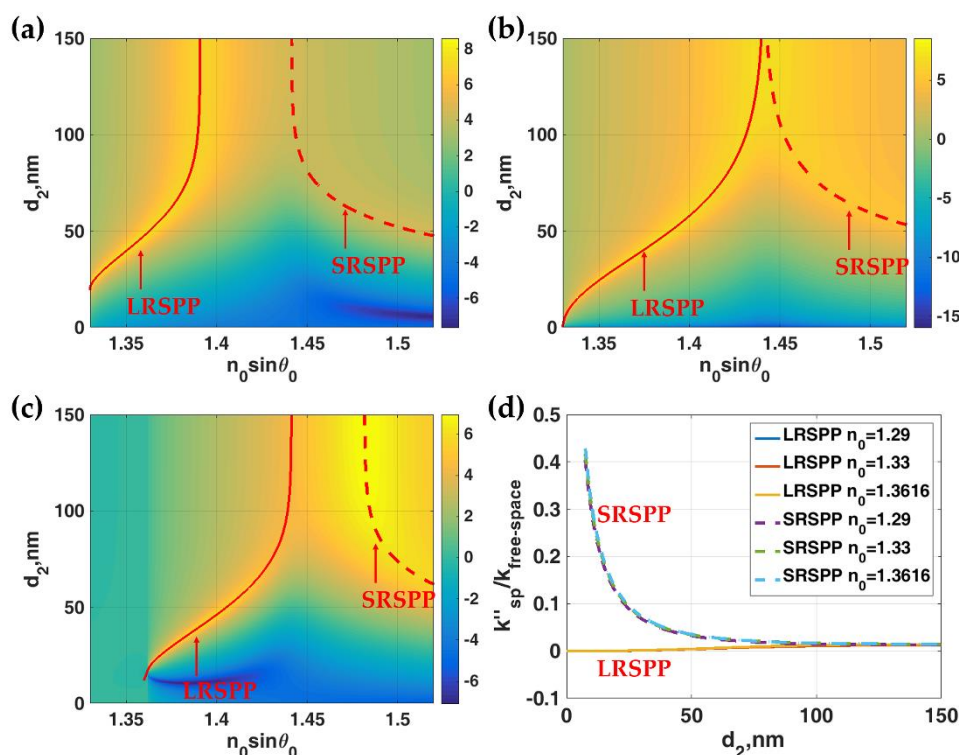


Figure 2. Comparison of coupling strength, $\ln |r_p|^2$, of LRSPP and SRSPP in the case where $n_0 = n_1$ and $d_1 = 0$ nm considered as pure plasmonic modes for (a) $n_0 = n_1 = 1.29$; (b) $n_0 = n_1 = 1.33$ and $n_0 = n_1 = 1.3616$. Other parameters are $\lambda = 633$ nm, $n_2 = 0.18344 + 3.4332i$ and $n_3 = 1.33$; (d) Normalized attenuation coefficients $k''_{sp}/k''_{free-space}$ for the cases in (a–c). The solid red curves in (a–c) were the solutions to Equation (2) for LRSPP mode and the dashed red curves are the solutions for SRSPP mode.

Stegeman and Burke [28] have reported a dispersion relation for the two plasmonic modes for asymmetric metal waveguide [29], which is given by:

$$\tanh(k_{z2}d_2)(\epsilon_0\epsilon_3k_{z2}^2 - \epsilon_2^2k_{z0}k_{z3}) - \epsilon_2k_{z2}(\epsilon_0k_{z3} + \epsilon_3k_{z0}) = 0 \quad (2)$$

where k_{z0} , k_{z2} , and k_{z3} are the k -vectors along the z -axis in the region 0, II and III. ϵ_0 , ϵ_2 and ϵ_3 are the permittivity of the region 0, II and III. These permittivity values can be determined by $\epsilon_0 = n_0^2$, $\epsilon_2 = n_2^2$ and $\epsilon_3 = n_3^2$.

Equation (2) allows us to solve for complex surface plasmon k -vector: $k_x = k_{sp} = k'_{sp} + ik''_{sp}$, where k_{sp} is the complex surface plasmon k -vector, where k'_{sp} is the real part of the complex surface plasmon k -vector and k''_{sp} is the attenuation coefficient. k_x is the k -vector along the x -axis, which is given by $\frac{2\pi n_0}{\lambda} \sin \theta_0$. θ_0 is the incident angle in the incident medium as shown in Figure 1. The normalized k'_{sp} solutions to the Equation (2) were shown in Figure 2a–c as solid red curves for the LRSPP and dashed red curves for the SRSPP. The normalized k'_{sp} solutions to the Equation (2) for the cases described in Figure 2a–c is shown in Figure 2d. The attenuation loss for the LRSPP was much lower than the SRSPP. It was dependent mostly on the thickness of the metal, not the coupling refractive index.

3.2. IIMI Structure for LRSPP Excitation through Evanescent Wave Coupling $n_1 \leq n_3$

The coupling refractive index of 1.3616 was not sufficient to excite the surface plasmon modes. It was, therefore, essential to provide a higher refractive index coupling media such as the glass substrate with the refractive index of 1.52. This glass substrate did not only provide the sufficient k -vector to excite the surface plasmons, but it also provided the interferometric modes and the second dielectric layer can also serve as a resonant cavity. These interference fringes were formed by the direct reflection from the first interface between the region 0 and the region I, $r_p^{n_0|n_1}$, and the multiple reflected beams as depicted in Figure 1. For the $n_1 \leq n_3$ case, here n_1 of 1.34 was calculated as an example. In this case, all interferometric mode k -vectors appeared below the k -vectors of the two SP modes as shown in Figure 3.

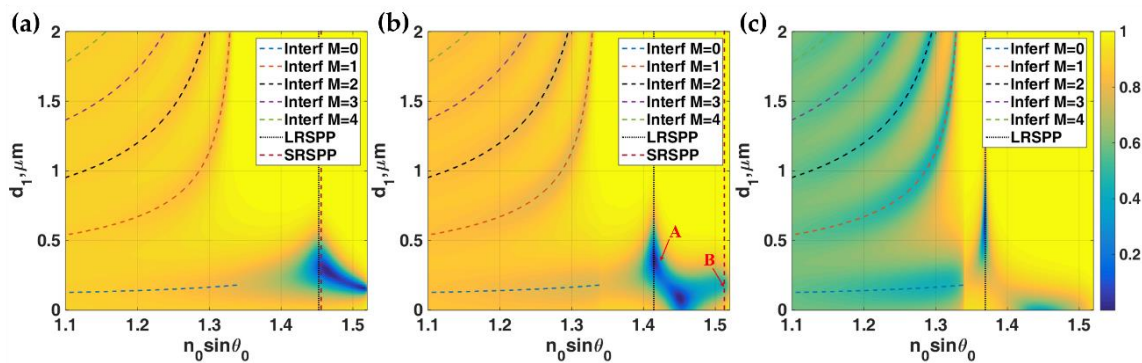


Figure 3. Responses showed $|r_p|^2$ for $\lambda = 633$ nm $n_0 = 1.52$, $n_1 = 1.34$ with thickness d_1 and $n_2 = 0.18344 + 3.4332i$ with thickness d_2 , $n_3 = 1.34$ (a) $d_2 = 150$ nm (b) $d_2 = 60$ nm and (c) $d_2 = 30$ nm. The colored curves shown in these figures were the interferometric mode positions calculated using Equation (3) and the two plasmonic modes calculated using Equation (2). ‘A’ and ‘B’ were labeled as plasmonic modes calculated using Equation (2). ‘C’, ‘D’ and ‘E’ are labelled as interferometric modes.

These interferometric mode positions can be calculated using the asymmetric Fabry Perot cavity resonant mode number [30], which is given by:

$$2k_{z1} + \text{Phase}(r_p^{n_1|n_2|n_3}) + \text{Phase}(r_p^{n_1|n_0}) = 2M\pi \quad (3)$$

where $\text{Phase}(r_p^{n_1|n_0})$ and $\text{Phase}(r_p^{n_1|n_2|n_3})$ are the phase of reflection coefficients for p-polarization for the light travelling the region I to the region 0 and the region I to the region II and the region III, respectively. M is the resonant mode number, $M = 0, 1, 2, 3, \dots$.

The 0th order did not have a cut-off k -vector unlike the other higher order modes [31] and it can excite the LRSPP mode. The interferometric mode positions matched very well with the Fresnel

simulations. The interferometric dips were not very deep indicating that the gold layer cannot provide sufficient loss for the interferometric modes. Figure 3a–c shows $|r_p|^2$ responses of the IIMI structure with different gold thicknesses. The two plasmonic modes were excited through attenuated total reflection (ATR) evanescent wave, where the light was evanescent in the region I after $n_0 \sin \theta_0$ of 1.34. The two plasmonic mode k -vectors changed when the gold thickness changed as predicted from Figure 3. The dielectric cavity height d_1 played a crucial role in the plasmonic mode coupling. It cannot be too high because of the short penetration of the evanescent wave. Figure 4 showed the phase transition through the gold layer of the two plasmonic modes labelled ‘A’ and ‘B’ in Figure 3b. The LRSPP had an anti-phase pattern at the two interfaces of the gold layer as shown in Figure 4a whereas the SRSPP had an in-phase phase pattern at the gold interfaces.

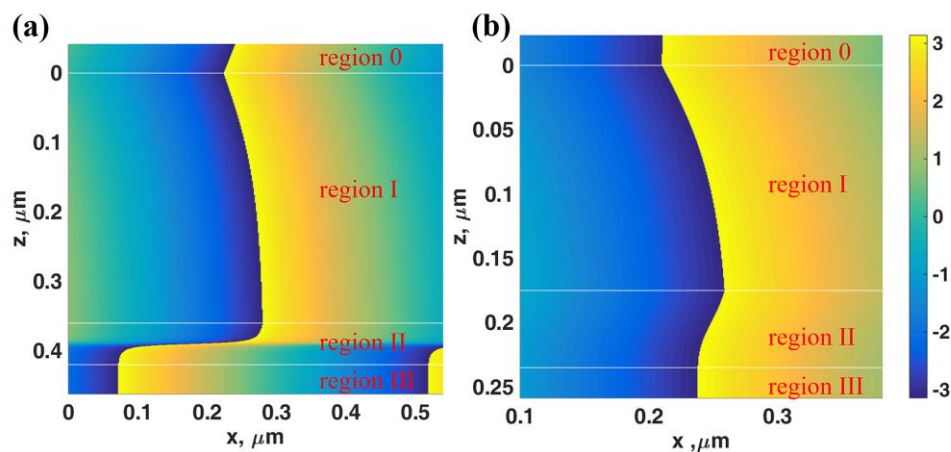


Figure 4. Phase profiles of E_x in rad for (a) LRSPP mode labelled ‘A’ in Figure 3b: $n_0 \sin \theta_0 = 1.4156$, $n_1 = 1.34$ with $d_1 = 360$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 60$ nm and $n_3 = 1.34$ and (b) SRSPP mode labelled ‘B’ in Figure 3b: $n_0 \sin \theta_0 = 1.513$, $n_1 = 1.34$ with $d_1 = 175$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 60$ nm and $n_3 = 1.34$.

3.3. LRSPP Excited by the Dielectric Resonator $n_1 > n_3$

In this section, let us look at the case where $n_1 > n_3$. There was a range of k -vectors that the light was a propagating wave in the region I and evanescent in the region III. The range was the k -vectors with $n_0 \sin \theta_0$ between n_3 and n_1 . Figure 5a,b showed $|r_p|^2$ for the IIMI structure with $n_0 = 1.52$, $n_1 = 1.39$ (lithium fluoride: LiF [27]) with thickness d_1 and $n_2 = 0.18344 + 3.4332i$ with thickness d_2 and the last dielectric medium $n_3 = 1.34$ for different gold layer thicknesses $d_2 = 30$ nm and $d_2 = 20$ nm, respectively. These figures were the cases when before the LRSPP k -vector matched to the range of interferometric mode k -vectors and when they matched.

Consequently, the interferometric modes dissipated the light power more efficiently through the plasmon coupling and appeared as very deep and narrow reflectance dips at 0 intensity level as shown in Figure 5b. It is interesting to note that the LRSPP excited by the 0th order interferometric mode is, of course, excited by a propagating wave mode inside the region I. Therefore the LRSPP can be excited at any cavity thickness d_1 as if the thickness allows the interferometric mode. This makes the device conveniently practical to fabricate. Not only the 0th order ($M = 0$) interferometric mode can excite the LRSPP, but also the other higher order interferometric modes if they were within the LRSPP k -vector range as shown in Figure 5b. In addition to the 633 nm wavelength, the other wavelengths of SPR excitation in the near-infrared region, i.e., 785 nm and 1024 nm were also presented and discussed in the SI.

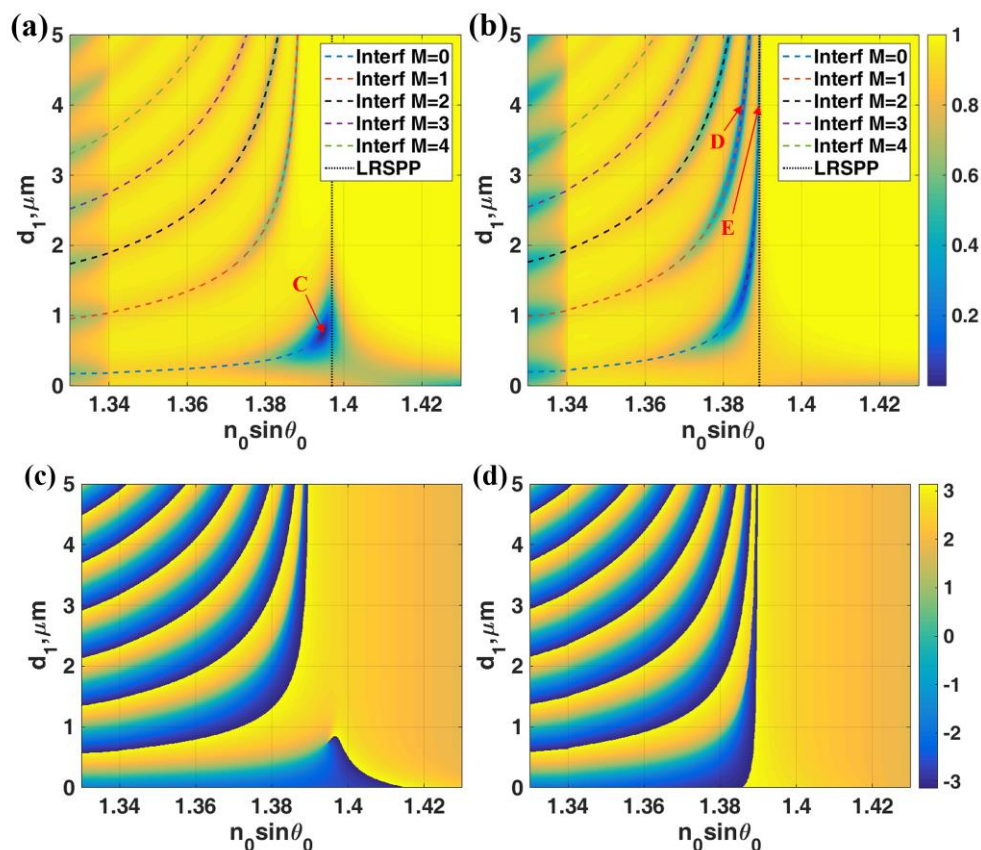


Figure 5. Simulation results for $\lambda = 633$ nm, $n_0 = 1.52$, $n_1 = 1.39$ with thickness d_1 and $n_2 = 0.18344 + 3.4332i$ with thickness d_2 and $n_3 = 1.34$. (a) $|r_p|^2$ when $d_2 = 30$ nm and (b) $|r_p|^2$ when $d_2 = 20$ nm (c) $\text{Phase}(r_p)$ in rad when $d_2 = 30$ nm and (d) $\text{Phase}(r_p)$ in rad when $d_2 = 20$ nm. The colored curves shown in (a,b) are the interferometric mode positions calculated using Equation (3) and the LRSPP mode

Figure 6a shows the $|H_y|^2$ field distributions of the LRSPP excited by the evanescent wave coupling labelled 'C' in Figure 5a. There was no standing wave inside the resonant cavity only the re-radiated leaky LRSPP wave leaked their power back through the cavity. Figure 6b,c shows the $|H_y|^2$ field distributions of the LRSPP excited by the 1st order ($M = 1$) and the 0th order ($M = 0$) interferometric modes labelled 'D' and 'E' in Figure 5b. There was the 1st order TM_1 guided mode pattern inside the resonant cavity in Figure 6b and the fundamental 0th order mode TM_0 guided mode pattern in Figure 6c. The sharpness LRSPP dips excited by the resonant cavity depended on the cavity thickness d_1 . Figure 5c,d shows the phase profiles of Figure 5a,b. The gradient of phase transitions for the interferometric modes depended strongly on the thickness of the resonant cavity. For the cavity thickness less than $1 \mu\text{m}$, the phase gradients of all the interferometric modes were shallower than the LRSPP as shown in Figure 5a and became much sharper when the thickness increased. This feature allowed us to excite the LRSPP with the different sharpness of the reflectance dip, in other words, it allowed us to vary the FWHM of the LRSPP mode. We will illustrate that not only the FWHM can be adjusted by the cavity thickness, but it also gives different dip refractometric sensitivity. These will be fully quantified in the next section.

For fabricating consideration, the structure with such thin gold film around 20 nm to 30 nm, the gold films are likely to have some defects such as gold islands [32]. There are several research groups working on ultra-thin gold film fabrication. Kossoy [33] have achieved an artifact-free 5.4 nm gold film. Another issue that we need to consider is that for all the simulations presented in this paper, the gold layers were treated as a uniform bulk gold layer. There is no standard threshold and criteria for the thinnest thickness gold film that can be still treated as bulk gold. There are several research articles

reporting an abnormal optical transmission through a thin gold film when the thickness is below 15 nm [34,35]. Laref et al. [36] have reported that the complex permittivity of gold does depend on the thickness of the gold film when the gold film is ultrathin <7 nm. The gold layer needs to be treated as an anisotropic material. The complex permittivity can no longer be approximated by Drude's model. This ultrathin layer is not in the range of our study. Olmon [37] have reported with experimental validation that the gold film thicker than 20 nm can be treated as a bulk-like material which is suitable for the range of gold thicknesses used in this proposed study.

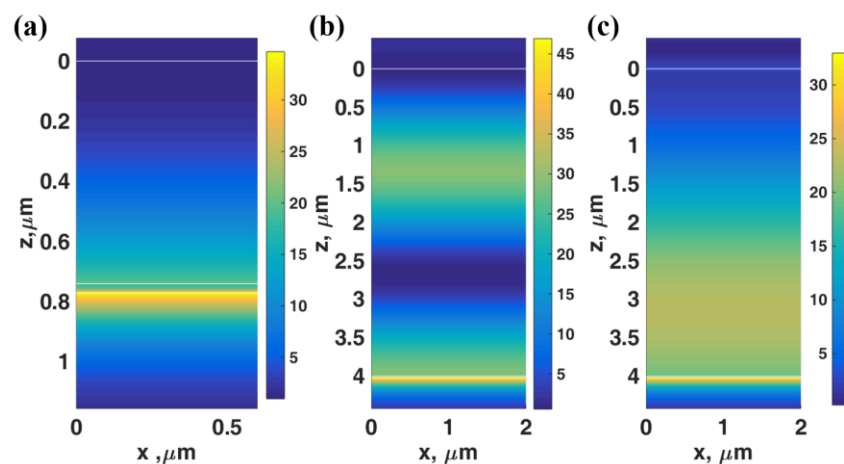


Figure 6. Field distributions of $|H_y|^2$ for (a) the LRSP excited by the evanescent wave coupling labelled 'C' in Figure 5, (b) the LRSP excited by the 1st order ($M = 1$) labelled 'D' in Figure 5b and (c) the LRSP excited by the 0th order ($M = 0$) labelled 'E' in Figure 5b.

3.4. Key Properties of LRSP Excited in IIMI Structure

In this section, the sensitivity (S), full-width half maximum (FWHM), dynamic range (D) and figure of merit (FoM) for different LRSP modes were quantified against the conventional SPR in Kretschmann configuration. Here the refractive indices were varied from 1.34 to 1.45 in order to quantify the sensitivity of the SPR sensor. This refractive index range covered a typical range for biological samples refractive indices [38,39]. Having explained above that the LRSP can be excited through the evanescent wave coupling and the resonator interferometric modes.

For the Kretschmann SPR configuration, the plasmonic dips appeared at higher k -vector compared to the other cases presented in this section. The S for the Kretschmann SPR was 1.07573 for d_1 of 48 nm. The maximum NA of 1.52 can only accommodate the refractive index of 1.39833 before the dip falls off the NA. One way to get around this, of course, to use a higher refractive index coupling such as NA of 1.65 [40] with coupling oil with a refractive index of 1.78 and with specially made of a sapphire coverslip [41]. This is not convenient for general biological measurements since the cover glass is very expensive and the immersion is also quite toxic and volatile. The FoM for the Kretschmann SPR is 22.93443.

For LRSP excited by evanescent wave coupling, the n_1 of 1.34 was chosen as the cavity refractive index to ensure that all the sample refractive indices were below the cavity refractive index. The IIMI structures with different gold thicknesses d_2 and fixed sample refractive index of 1.34 were then calculated by varying the cavity thickness d_1 to determine the lowest reflectance intensity position for the LRSP for each gold thickness. The operating points where the lowest intensity dips occurred for the gold thickness between 20 nm to 75 nm were shown in Figure 7. It can be seen from the Figure 2c that the cut-off of the plasmonic mode is around 20 nm of gold thickness for LRSP excitation. The dip movement responses are shown in Figure 8b–d for the gold thicknesses of 20 nm, 40 nm and 60 nm, respectively. It can be seen from Figure 8a for the 20 nm thick that the plasmonic dip became very sharp with 21 times narrower FWHM boosting up to the FoM by 12 times, but it does lose half of the dip

refractometric sensitivity compared to the Kretschmann case. The dynamic range for the 20 nm case was around 1.36595, which was very limited and also shorter than the Kretschmann case. This was due to the LRSPP coupling becoming inefficient when the refractive indices sandwiching the gold had a larger mismatch. An increase in the gold thickness can extend the dynamic range, but the dip refractometric sensitivity, the FWHM and consequently the FoM became worse. To cover the whole range of the sample refractive indices, the gold thickness of at least 60 nm was required and the FoM became 12.90102, which was almost two times worse than the Kretschmann setup.

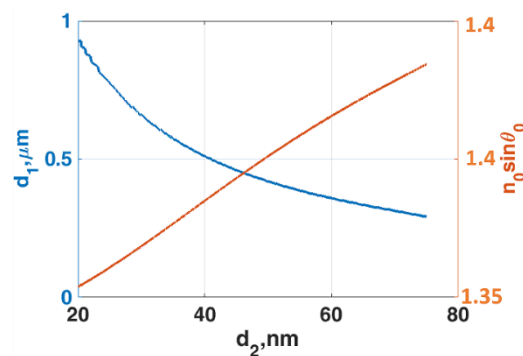


Figure 7. The optimal operating parameters for LRSPP excitation by evanescent wave coupling when $n_0 = 1.52$, $n_1 = 1.34$, $n_2 = 0.18344 + 3.4332i$ and $n_3 = 1.34$ for different thicknesses of gold d_2 ranging from 20 to 75 nm. The blue curve shows the cavity thickness d_1 where the lowest intensity dip occurs. The red curve showed the $n_0 \sin \theta_0$ positions where the LRSPP excited.

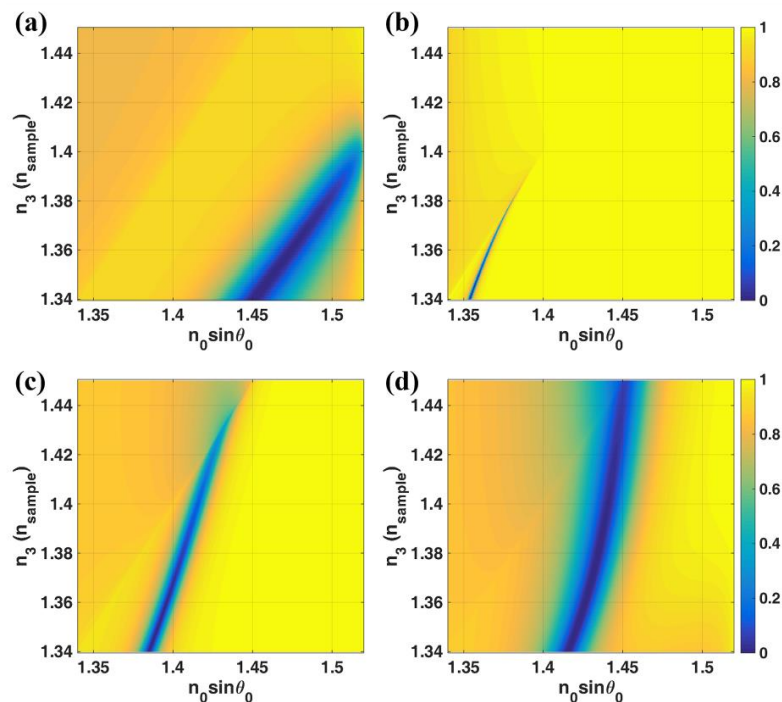


Figure 8. $|r_p|^2$ responses when the sample refractive index n_3 changed from 1.34 to 1.45. (a) $n_0 = n_1 = 1.52$, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 48$ nm and varying n_3 ; (b) $n_0 = 1.52$, $n_1 = 1.34$ with $d_1 = 930$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm and varying n_3 ; (c) $n_0 = 1.52$, $n_1 = 1.34$ with $d_1 = 510$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 40$ nm and varying n_3 ; and (d) $n_0 = 1.52$, $n_1 = 1.34$ with $d_1 = 3600$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 60$ nm and varying n_3 .

For the LRSPP excited through interferometric modes provided the resonant cavity, two refractive indices of the dielectric cavity were chosen in this study. The n_1 refractive indices were 1.3616 (KF) and 1.3900 (LiF). The $|r_p|^2$ contours for different structure parameters are shown in Figure 9. To demonstrate different sensitivity responses at different cavity thicknesses d_1 and refractive indices n_1 , the $|r_p|^2$ contours for n_3 of 1.34, 1.35 and 1.36 shown in left, middle and right columns, respectively. Figure 9a,b shows the LRSPP structures with n_1 of 1.3616 for d_2 of 20 nm and 30 nm, respectively. Figure 9c,d shows the LRSPP structures with n_1 of 1.3900 for d_2 of 20 nm and 30 nm, respectively. The performance parameters for these four structures at 500 nm d_1 thickness step were summarized in Table 1. It can be seen from the Table 1 that the LRSPP excited through the interferometric modes can be employed to extend the dynamic range of the LRSPP covering the whole sample refractive indices without losing too much of the dip refractometric sensitivity, the FWHM and the FoM such as (1) n_1 of 1.3616 with d_1 of 1000 nm and d_2 of 20 nm and (2) n_1 of 1.3900 with d_1 of 1000 nm and d_2 of 20 nm. It can be seen that these two example cases had a longer dynamic range than the 20 nm case of the LRSPP excited by the evanescent wave.

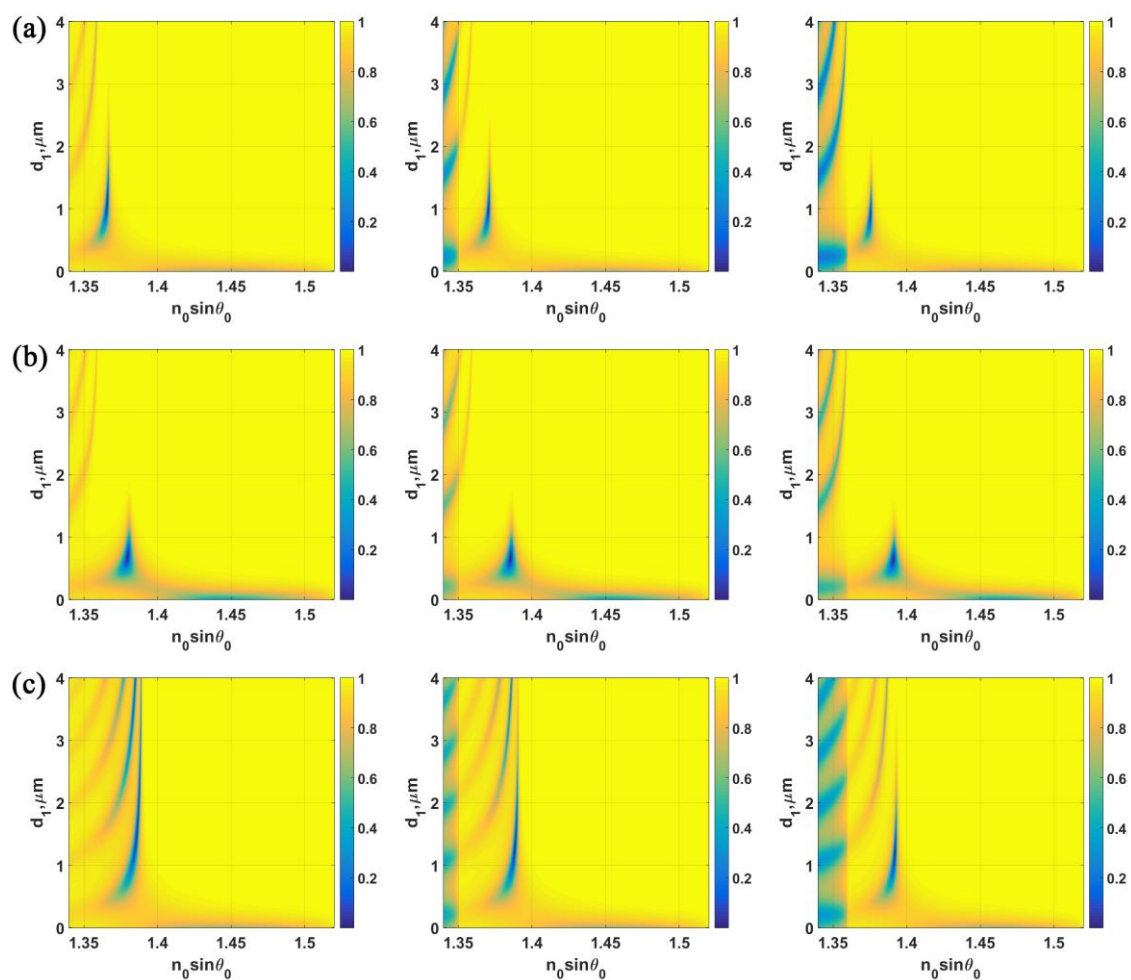


Figure 9. Cont.

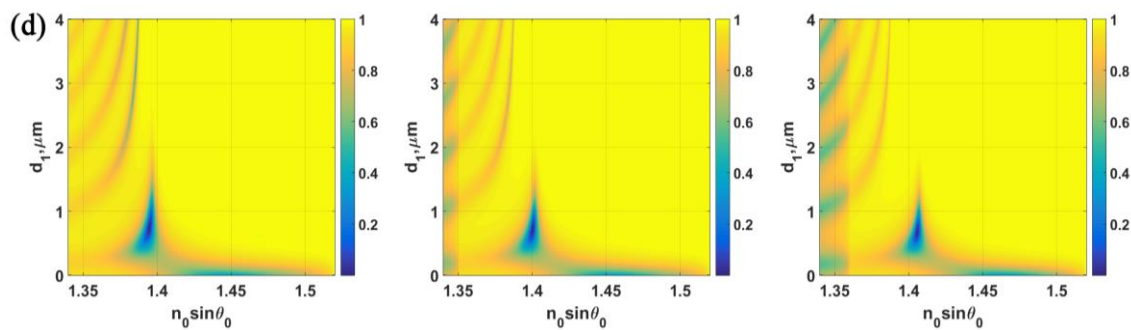


Figure 9. $|r_p|^2$ responses for the following structure parameters. (a) $n_0 = 1.52$, $n_1 = 1.3616$, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm; (b) $n_0 = 1.52$, $n_1 = 1.3616$, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 30$ nm; (c) $n_0 = 1.52$, $n_1 = 1.39$, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm; (d) $n_0 = 1.52$, $n_1 = 1.39$, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 30$ nm. Each column represents responses due to different sample refractive indices, $n_3 = 1.34$, 1.35 and 1.36 shown in left, middle and right columns, respectively.

Table 1. The performance evaluation parameters for SPR excited by Kretschmann configuration, LRSPP excited through evanescent wave coupling and LRSPP excited by interferometric mode.

Structure Parameters n_1 , d_1 , d_2 (in nm)	Dynamic Range (D)	$n_0 \sin \theta_0$ at Lower D Limit	$n_0 \sin \theta_0$ at Upper D Limit	Sensitivity (S)	FWHM at $ r_p ^2 = 0$	$n_0 \sin \theta_0$ Where the FWHM Calculated	FoM	Shown in Figure
Kretschmann Configuration								
1.5200, 0, 48	1.3400–1.3983	1.4510	1.5137	1.0757	0.0469	1.3400	22.9344	8a
LRSPP excited by evanescent wave coupling								
1.3400, 930, 20	1.3400–1.3660	1.3538	1.3697	0.6127	0.0022	1.3400	273.6243	8b
1.3400, 660, 30	1.3400–1.3885	1.3685	1.3960	0.5680	0.0056	1.3400	101.8497	-
1.3400, 510, 40	1.3400–1.4191	1.3849	1.4247	0.5030	0.0108	1.3400	46.4032	8c
1.3400, 420, 50	1.3400–1.4485	1.4010	1.4485	0.4380	0.0176	1.3400	24.9548	-
1.3400, 360, 60	1.3400–1.4500	1.4155	1.4516	0.3276	0.0254	1.3400	12.9010	8d
1.3400, 310, 70	1.3400–1.4500	1.4284	1.4573	0.2621	0.0371	1.3400	7.0632	-
LRSPP excited by interferometric mode								
1.3616, 500, 20	1.3955–1.4157	1.3971	1.4151	0.8927	0.0165	1.4092	54.1772	9a
1.3616, 1000, 20	1.3400–1.3778	1.3655	1.3858	0.5374	0.0024	1.3709	223.4523	9a
1.3616, 1500, 20	1.3400–1.3404	1.3665	1.3667	0.4198	0.0011	1.3665	373.7145	9a
1.3616, 500, 30	1.3400–1.4439	1.3783	1.4439	0.6315	0.0072	1.4207	87.5131	9b
1.3900, 500, 20	1.4218–1.4477	1.4249	1.4474	0.8673	0.0122	1.4412	71.0818	9c
1.3900, 1000, 20	1.3400–1.4029	1.3829	1.4133	0.4836	0.0026	1.3984	182.3115	9c
1.3900, 1500, 20	1.3400–1.3652	1.3860	1.3947	0.3456	0.0026	1.3872	132.2752	9c
1.3900, 2000, 20	1.3400–1.3512	1.3873	1.3901	0.2490	0.0018	1.3873	138.0813	9c
1.3900, 2500, 20	1.3400–1.3454	1.3881	1.3891	0.1840	0.0012	1.3881	154.6768	9c
1.3900, 3000, 20	1.3400–1.3425	1.3885	1.3889	0.1391	0.0008	1.3885	170.0563	9c
1.3900, 3500, 20	1.3400–1.3408	1.3888	1.3889	0.1073	0.0006	1.3888	185.0506	9c
1.3900, 4000, 20	1.3400–1.3397	1.3890	1.3890	0.0840	0.0004	1.3890	199.8070	9c
1.3900, 500, 30	1.3400–1.4500	1.3921	1.4570	0.5903	0.0077	1.4479	76.5967	9d
1.3900, 1000, 30	1.3400–1.3477	1.3960	1.4001	0.5388	0.0042	1.3960	127.6527	9d
1.3900, 500, 40	1.3400–1.4500	1.4093	1.4726	0.5754	0.0137	1.4170	42.0868	-
1.3900, 500, 48	1.3400–1.4067	1.4214	1.4655	0.6605	0.0138	1.4214	48.0453	-

The dynamic range can be extended further covering the whole range of the sample refractive indices by increasing the thickness of the gold to just 30 nm with n_1 of 1.3900 and d_1 of 500 nm whereas the gold thickness needed to be increased to 60 nm for the LRSPP excited by evanescent wave coupling case. The FoM for this 30 nm case is six times higher than the 60 nm gold for LRSPP excited by evanescent wave and three times higher than the Kretschmann case.

The LRSPP excited by the interferometric mode can have a higher FoM than the LRSPP excited by evanescent wave coupling, however, it does have a very narrow dynamic range as shown in Table 1 for n_1 of 1.3616 with d_1 of 1500 nm and d_2 of the 20 nm cases. It is interesting to note that for the same gold thickness as Kretschmann configuration of 48 nm the LRSPP excited by the resonant cavity n_1 of 1.3900 and d_1 of 500 nm has a longer dynamic range and three times narrower plasmonic dip but the dip refractometric sensitivity is less than the Kretschmann case. The plasmonic dips for the LRSPP cases appear at a lower k -vectors than the Kretschmann SPR.

3.5. Field Enhancement

One key feature of surface plasmon resonance is the field enhancement on the surface of the metal. This unique feature is very useful for several applications including fluorescent excitation [42] and non-linear optics [43]. The field enhancement here was calculated as $|t_p|^2$ or the amount of transmitted light intensity on the metal layer. In this section, several layered structures were simulated and compared. The sample channel was again placed in the last dielectric layer with refractive indices ranging from 1.34 to 1.45, which cover a typical range for biological samples refractive indices [38,39]. Figure 10 shows $|t_p|^2$ for the different layered structure. A typical configuration for evanescent wave excitation in total internal reflection microscopy [44,45] was an interface between glass substrate and sample. The field enhancement $|t_p|^2$ for glass/sample interface calculated as shown in Figure 10a had the maximum value of 5.22. Figure 10b showed the conventional SPR excited using Kretschmann configuration. The maximum $|t_p|^2$ was 14.89, which was 2.8 times higher than the glass/sample interface. There were also a number of inconvenient issues for microscopy imaging. Firstly, $|t_p|^2$ values for each sample refractive index were not constant, forming a non-uniform field and secondly the SPR cannot cover the sample required refractive index range. Several recently developed microscopy techniques have included spatial light modulator devices such as an amplitude spatial light modulator [46], a phase spatial light modulator [47–49] or a digital micromirror device (DMD) [50]. Thirdly, they were excited at different k -vector positions making illumination control and difficulty in modulation. The same issues were also applied to the LRSPP excited by the evanescent wave as shown in Figure 10c,d. The 20 nm gold has been chosen since it can provide a decent amount of plasmons and a high-quality film can be fabricated. The maximum $|t_p|^2$ in Figure 10c was 6.45 times higher than the Kretschmann case shown in Figure 10a. The differences between the cases shown in Figure 10c,d was that the coupling index n_0 where the Figure 10c case was 1.52 and the Figure 10d was 1.7. The n_0 of 1.7 case had 1.48 times higher $|t_p|^2$ than the n_0 of 1.52 case. This is because of the higher index contrast between n_0 and n_1 providing the higher evanescent wave enhancement. Note that the highest NA available in the market at the moment is the NA 1.7 APON100 × HOTIRF [51].

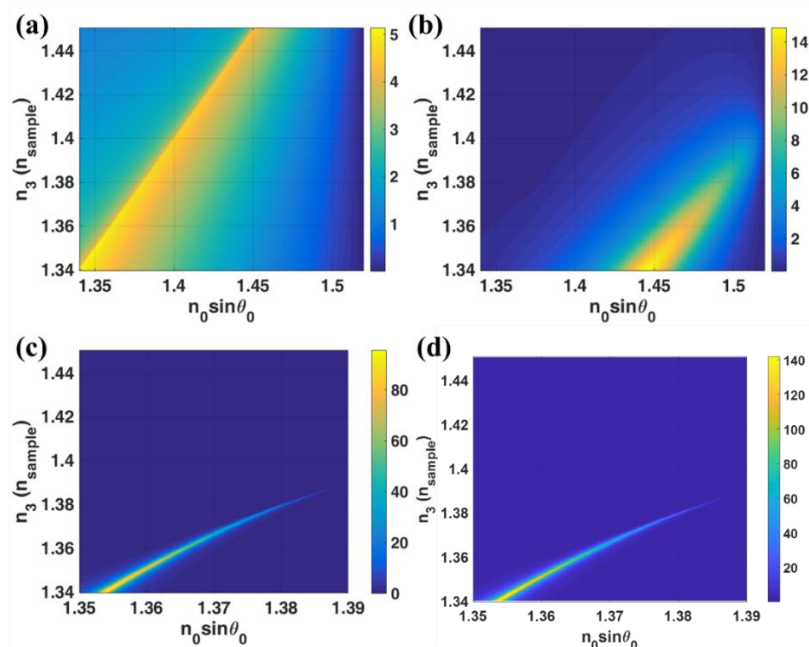


Figure 10. $|t_p|^2$ responses when the sample refractive index n_3 changed from 1.34 to 1.45. (a) $n_0 = n_1 = n_2 = 1.52$, and varying n_3 ; (b) $n_0 = n_1 = 1.52$, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 48$ nm and varying n_3 ; (c) $n_0 = 1.52$, $n_1 = 1.34$ with $d_1 = 930$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm and varying n_3 and (d) $n_0 = 1.70$, $n_1 = 1.34$ with $d_1 = 930$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm and varying n_3 .

Having explained in the earlier section, the properties of the LRSPP excited by the interferometer modes can be engineered through the resonant cavity parameters d_1 and n_1 . The sample refractive index dynamic range of the field enhancement can be controlled by the cavity refractive index n_1 as shown in Figure 11a,b. Both of the structures in Figure 11a,b had the same cavity thickness d_1 of 1000 nm, the difference between the two structures was that the n_1 refractive indices for Figure 11a,b was 1.39 and 1.45 (silicon dioxide: SiO₂ [52]), respectively. The field enhancement in n_1 of 1.39 case was much greater than the n_1 of 1.45 case, however, the dynamic range was much shorter. Having explained in Table 1 that the structure with the thicker cavity thickness had lower sensitivity to the refractive index change, this was also applicable to the structure design for field enhancement application. Figure 11c showed the $|t_p|^2$ responses for the cavity with n_1 of 1.45 and d_1 of 5000 nm. It can be seen that the k -vector position for each interferometric orders that excited the LRSPP became more linear than the thinner cavity case and independent of the sample refractive index. The magnitude of the field enhancement of 46.04 in the LRSPP excited through the interferometric mode was independent of the cavity thickness since the LRSPP was excited by the propagating wave in the cavity. Figure 11d showed the effect of the coupling refractive index n_0 of 1.7. The higher coupling refractive case can enhance the field enhancement to 91.41 which was at least 5 times more than the conventional Kretschmann case.

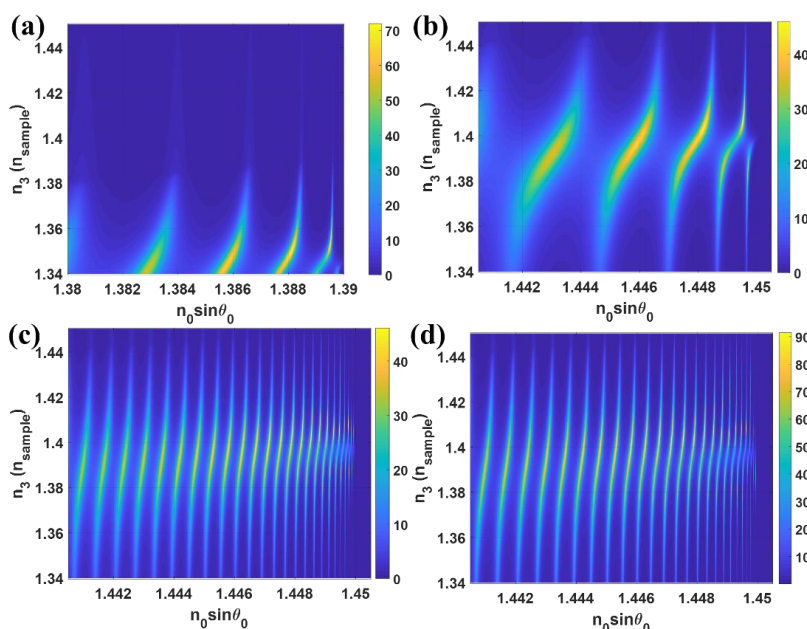


Figure 11. t_p responses when the sample refractive index n_3 changed from 1.34 to 1.45. (a) $n_0 = 1.52$, $n_1 = 1.39$ with $d_1 = 1000$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm and varying n_3 ; (b) $n_0 = 1.52$, $n_1 = 1.45$ with $d_1 = 1000$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm and varying n_3 ; (c) $n_0 = 1.52$, $n_1 = 1.45$ with $d_1 = 5000$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm and varying n_3 and (d) $n_0 = 1.7$, $n_1 = 1.45$ with $d_1 = 5000$ nm, $n_2 = 0.18344 + 3.4332i$ with $d_2 = 20$ nm and varying n_3 .

3.6. Self-Referenced SPR System

We have demonstrated in the previous section that the interferometric modes can be designed so that it does not excite the LRSPP, therefore they will not be sensitive to the sample region. On the other hand, they can also excite the LRSPP and these LRSPPs can be more sensitive than the LRSPP excited by the evanescent wave coupling as shown in Table 1. This feature enables us to design a self-referenced SPR sensor having two reflectance dips, which the dip position movement due to the variations in the sensor can be distinguished from the signal change due to the sample refractive index change. The variations in the sensor are, for example, temperature fluctuation in the sensor, evaporation of oil immersion liquid. Figure 12a showed our proposed structure, which the structure

was readily integratable on an oil immersion microscope. The incident wavelength of $1.064\ \mu\text{m}$ was used in this section allowing the LRSPP to be excited at a lower incident k -vector to ensure that 1.4 NA can accommodate all the two modes. The proposed structure consisted of the following layers: glass substrate ($n_0 = 1.52$), $3\ \mu\text{m}$ thick of LiF with 1.39 refractive index (n_1), $4\ \text{nm}$ thick of Cr layer with $3.5408 + 3.5777i$ [25] refractive index (n_2) (this also served as adhesion layer between gold and glass), $55\ \text{nm}$ of gold layer with refractive index of $0.25846 + 6.9654i$ [25] (n_3) and the sample channel with refractive index n_4 was placed on the top of the sensor. Figure 12b showed $|r_p|^2$ response when the cavity thickness d_1 was varied from $0\ \mu\text{m}$ to $5\ \mu\text{m}$. It can be seen from the figure that at d_1 of $3\ \mu\text{m}$ the LRSPP occurred at the incident k -vector lower than the 1st order interferometric mode. The two modes were well separated enough so that the interferometric mode was independent of the LRSPP as explained in the earlier section.

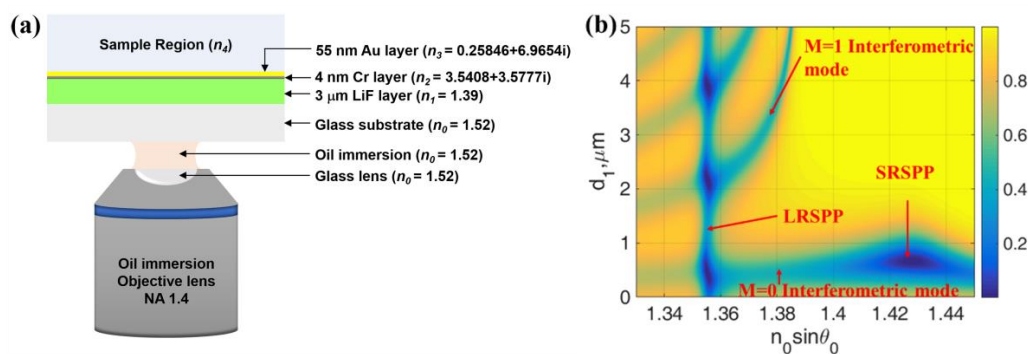


Figure 12. (a) The proposed self-reference SPR sensor (b structure and) $|r_p|^2$ responses when the sample refractive index n_4 was 1.33 calculated for $1.064\ \mu\text{m}$ incident wavelength.

Figure 13a shows the $|r_p|^2$ responses for when the refractive index of the sample changed from 1.33 to 1.34 depicted in blue curve for 1.33 and red curve for 1.34. Note that only the LRSPP dip moved to the higher k -vector when the sample refractive index changed. The 1st order interferometric dip did not move. Figure 13b shows the case where the refractive index in the illumination part changed and the sample refractive index was fixed, we mimicked this scenario by varying the index of the n_1 from 1.39 to 1.4. It can be observed from the figure that the interferometric dip moved whereas the LRSPP did not when the refractive index of the sensor structure changed. This allows us to separate the change due to the illumination structure and the change due to the sample. This unique feature is not available in other structures such as IMIM structure.

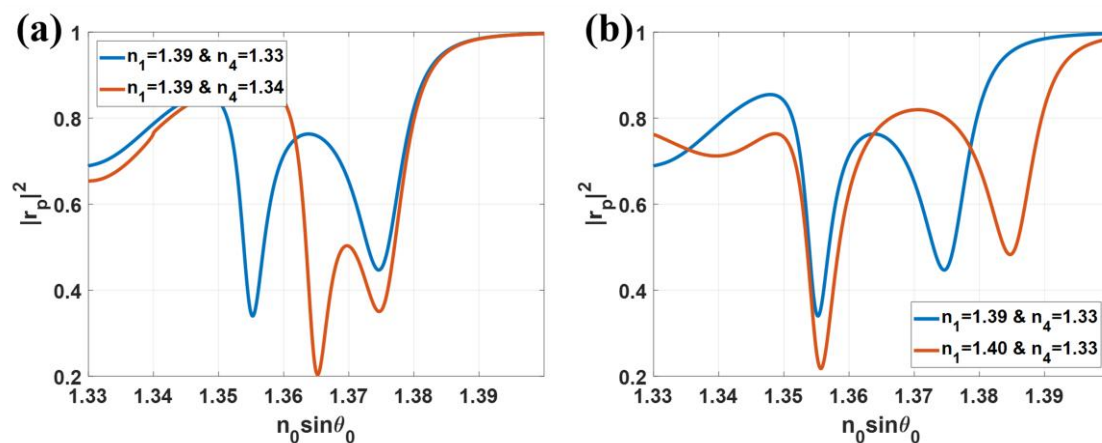


Figure 13. (a) $|r_p|^2$ responses when $n_1 = 1.39$, $n_4 = 1.33$ (blue curve) and 1.34 (red curve) and (b) $|r_p|^2$ responses when $n_1 = 1.39$ (blue curve) and 1.40 (red curve) and $n_4 = 1.33$.

4. Conclusions

In this paper, we have developed a theoretical framework to understand unique characteristics of IIMI structure under the following conditions: (1) the refractive index of the second dielectric layer was large than refractive index of the last dielectric layer and (2) when the light propagated in the second dielectric layer and was evanescent in the last dielectric layer. These conditions allowed multiple reflections in the second dielectric layer and an embedded interferometric detection. The IIMI structure under the conditions can be employed to enhance the LRSP excitation, sensitivity, field enhancement and extend the dynamic range for LRSP excitation. We have proposed structures for: (1) *FoM* enhancement for refractive index sensing application and (2) self-reference structure allowing the signal change due to sensor structure and the signal change due to the sample refractive index change to be distinguished. This feature is only available in the proposed IIMI structure.

Supplementary Materials: The following are available online at <http://www.mdpi.com/1424-8220/18/9/2757/s1>, Figure S1: $|r_p|^2$ responses using silver as the metal layer, Table S1: The performance evaluation for the silver material, Figure S2: $|r_p|^2$ responses for the incident wavelength of 785 nm, Table S2: The performance evaluation for the incident wavelength of 785 nm, Figure S3: $|r_p|^2$ responses for the incident wavelength of 1024 nm, Table S3: The performance evaluation for the incident wavelength of 1024 nm.

Author Contributions: P.S. analyzed the data, discussed and prepared the manuscript, revised manuscript; S.P. conceived, designed the analytical calculation, discussed and revised the manuscript.

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References

- Schasfoort, R.B. *Handbook of Surface Plasmon Resonance*; Royal Society of Chemistry: London, UK, 2017.
- Mayer, K.M.; Lee, S.; Liao, H.; Rostro, B.C.; Fuentes, A.; Scully, P.T.; Nehl, C.L.; Hafner, J.H. A label-free immunoassay based upon localized surface plasmon resonance of gold nanorods. *ACS Nano* **2008**, *2*, 687–692. [[CrossRef](#)] [[PubMed](#)]
- Ferreira de Macedo, E.; Ducatti Formaggio, D.M.; Salles Santos, N.; Batista Tada, D. Gold nanoparticles used as protein scavengers enhance surface plasmon resonance signal. *Sensors* **2017**, *17*, 2765. [[CrossRef](#)] [[PubMed](#)]
- Zeng, S.; Baillargeat, D.; Ho, H.P.; Yong, K.T. Nanomaterials enhanced surface plasmon resonance for biological and chemical sensing applications. *Chem. Soc. Rev.* **2014**, *43*, 3426–3452. [[CrossRef](#)] [[PubMed](#)]
- Kretschmann, E. The determination of the optical constants of metals by excitation of surface plasmons. *Z. Phys.* **1971**, *241*, 313–324. [[CrossRef](#)]
- Kretschmann, E.; Raether, H. Radiative decay of non radiative surface plasmons excited by light. *Z. Naturforsch. A* **1968**, *23*, 2135–2136. [[CrossRef](#)]
- Otto, A. Excitation of nonradiative surface plasma waves in silver by the method of frustrated total reflection. *Z. Phys. A Hadrons Nuclei* **1968**, *216*, 398–410. [[CrossRef](#)]
- Lysenko, O.; Bache, M.; Olivier, N.; Zayats, A.V.; Lavrinenko, A. Nonlinear dynamics of ultrashort long-range surface plasmon polariton pulses in gold strip waveguides. *ACS Photonics* **2016**, *3*, 2324–2329. [[CrossRef](#)]
- Shen, M.; Larkthanakhachon, S.; Pechprasarn, S.; Zhang, Y.; Somekh, M.G. Adjustable microscopic measurement of nanogap waveguide and plasmonic structures. *Appl. Opt.* **2018**, *57*, 3453–3462. [[CrossRef](#)] [[PubMed](#)]
- Zhao, X.; Zhang, Z.; Yan, S. Tunable fano resonance in asymmetric mim waveguide structure. *Sensors* **2017**, *17*, 1494. [[CrossRef](#)] [[PubMed](#)]
- Yu, J.; Ohtera, Y.; Yamada, H. Scattering-parameter model analysis of side-coupled plasmonic fabry–perot waveguide filters. *Appl. Phys. A* **2018**, *124*, 516. [[CrossRef](#)]
- Berini, P. Long-range surface plasmon polaritons. *Adv. Opt. Photonics* **2009**, *1*, 484–588. [[CrossRef](#)]

13. Lee, K.-S.; Lee, T.S.; Kim, I.; Kim, W.M. Parametric study on the bimetallic waveguide coupled surface plasmon resonance sensors in comparison with other configurations. *J. Phys. D Appl. Phys.* **2013**, *46*, 125302. [[CrossRef](#)]
14. Slavík, R.; Homola, J. Ultrahigh resolution long range surface plasmon-based sensor. *Sens. Actuators B Chem.* **2007**, *123*, 10–12. [[CrossRef](#)]
15. Meng, Q.-Q.; Zhao, X.; Lin, C.-Y.; Chen, S.-J.; Ding, Y.-C.; Chen, Z.-Y. Figure of merit enhancement of a surface plasmon resonance sensor using a low-refractive-index porous silica film. *Sensors* **2017**, *17*, 1846. [[CrossRef](#)] [[PubMed](#)]
16. Khan, M.R.; Khalilian, A.; Kang, S.W. Fast, highly-sensitive, and wide-dynamic-range interdigitated capacitor glucose biosensor using solvatochromic dye-containing sensing membrane. *Sensors* **2016**, *16*, 265. [[CrossRef](#)] [[PubMed](#)]
17. Zeng, S.; Sreekanth, K.V.; Shang, J.; Yu, T.; Chen, C.K.; Yin, F.; Baillargeat, D.; Coquet, P.; Ho, H.P.; Kabashin, A.V.; et al. Graphene-gold metasurface architectures for ultrasensitive plasmonic biosensing. *Adv. Mater.* **2015**, *27*, 6163–6169. [[CrossRef](#)] [[PubMed](#)]
18. Wu, C.-T.; Huang, C.-C.; Lee, Y.-C. Plasmonic wavelength demultiplexer with a ring resonator using high-order resonant modes. *Appl. Opt.* **2017**, *56*, 4039–4044. [[CrossRef](#)] [[PubMed](#)]
19. Lan, T.-H.; Chung, Y.-K.; Tien, C.-H. Broad detecting range of objective-based surface plasmon resonance sensor via multilayer structure. *Jpn. J. Appl. Phys.* **2011**, *50*, 09MG04. [[CrossRef](#)]
20. Abeles, F.; Lopez-Rios, T. Decoupled optical excitation of surface plasmons at the two surfaces of a thin film. *Opt. Commun.* **1974**, *11*, 89–92. [[CrossRef](#)]
21. Botten, L.; White, T.; de Sterke, C.M.; McPhedran, R.; Asatryan, A.; Langtry, T. Photonic crystal devices modelled as grating stacks: Matrix generalizations of thin film optics. *Opt. Express* **2004**, *12*, 1592–1604. [[CrossRef](#)] [[PubMed](#)]
22. Moharam, M.G.; Gaylord, T.K. Rigorous coupled-wave analysis of planar-grating diffraction. *J. Opt. Soc. Am.* **1981**, *71*, 811–818. [[CrossRef](#)]
23. Berini, P. Figures of merit for surface plasmon waveguides. *Opt. Express* **2006**, *14*, 13030–13042. [[CrossRef](#)] [[PubMed](#)]
24. Saha, K.; Agasti, S.S.; Kim, C.; Li, X.; Rotello, V.M. Gold nanoparticles in chemical and biological sensing. *Chem. Rev.* **2012**, *112*, 2739–2779. [[CrossRef](#)] [[PubMed](#)]
25. Johnson, P.B.; Christy, R.W. Optical constants of the noble metals. *Phys. Rev. B* **1972**, *6*, 4370–4379. [[CrossRef](#)]
26. Yang, M.K.; French, R.H.; Tokarsky, E.W. Optical properties of teflon[®] AF amorphous fluoropolymers. *J. Micro/Nanolithogr. MEMS MOEMS* **2008**, *7*, 033010. [[CrossRef](#)]
27. Li, H. Refractive index of alkali halides and its wavelength and temperature derivatives. *J. Phys. Chem. Ref. Data* **1976**, *5*, 329–528. [[CrossRef](#)]
28. Stegeman, G.; Burke, J.; Hall, D. Surface-polaritonlike waves guided by thin, lossy metal films. *Opt. Lett.* **1983**, *8*, 383–385. [[CrossRef](#)] [[PubMed](#)]
29. Trapp, J. *Design and Fabrication of a Long-Range Surface Plasmon Polariton Wave Guide for Near-Infrared Light*; LMU München: Munich, Germany, 2011.
30. Pechprasarn, S.; Learkthanakhachon, S.; Zheng, G.; Shen, H.; Lei, D.Y.; Somekh, M.G. Grating-coupled otto configuration for hybridized surface phonon polariton excitation for local refractive index sensitivity enhancement. *Opt. Express* **2016**, *24*, 19517–19530. [[CrossRef](#)] [[PubMed](#)]
31. Saleh, B.E.; Teich, M.C.; Saleh, B.E. *Fundamentals of Photonics*; Wiley: New York, NY, USA, 1991; Volume 22.
32. Yakubovsky, D.I.; Arsenin, A.V.; Stebunov, Y.V.; Fedyanin, D.Y.; Volkov, V.S. Optical constants and structural properties of thin gold films. *Opt. Express* **2017**, *25*, 25574–25587. [[CrossRef](#)] [[PubMed](#)]
33. Kossoy, A.; Merk, V.; Simakov, D.; Leosson, K.; Kéna-Cohen, S.; Maier, S.A. Optical and structural properties of ultra-thin gold films. *Adv. Opt. Mater.* **2015**, *3*, 71–77. [[CrossRef](#)]
34. Azeredo, B.P.; Yeratapally, S.R.; Kacher, J.; Ferreira, P.M.; Sangid, M.D. An experimental and computational study of size-dependent contact-angle of dewetted metal nanodroplets below its melting temperature. *Appl. Phys. Lett.* **2016**, *109*, 213101. [[CrossRef](#)]
35. Tu, J.; Homes, C.; Strongin, M. Optical properties of ultrathin films: Evidence for a dielectric anomaly at the insulator-to-metal transition. *Phys. Rev. Lett.* **2003**, *90*, 017402. [[CrossRef](#)] [[PubMed](#)]

36. Laref, S.; Cao, J.; Asaduzzaman, A.; Runge, K.; Deymier, P.; Ziolkowski, R.W.; Miyawaki, M.; Muralidharan, K. Size-dependent permittivity and intrinsic optical anisotropy of nanometric gold thin films: A density functional theory study. *Opt. Express* **2013**, *21*, 11827–11838. [[CrossRef](#)] [[PubMed](#)]
37. Olmon, R.L.; Slovick, B.; Johnson, T.W.; Shelton, D.; Oh, S.-H.; Boreman, G.D.; Raschke, M.B. Optical dielectric function of gold. *Phys. Rev. B* **2012**, *86*, 235147. [[CrossRef](#)]
38. Zhou, Y.; Chan, K.K.; Lai, T.; Tang, S. Characterizing refractive index and thickness of biological tissues using combined multiphoton microscopy and optical coherence tomography. *Biomed. Opt. Express* **2013**, *4*, 38–50. [[CrossRef](#)] [[PubMed](#)]
39. Jin, Y.; Chen, J.; Xu, L.; Wang, P. Refractive index measurement for biomaterial samples by total internal reflection. *Phys. Med. Biol.* **2006**, *51*, N371. [[CrossRef](#)] [[PubMed](#)]
40. Wazawa, T.; Ueda, M. Total internal reflection fluorescence microscopy in single molecule nanobioscience. In *Microscopy Techniques*; Springer: Berlin/Heidelberg, Germany, 2005; pp. 77–106.
41. Jamil, M.M.A.; Denyer, M.C.; Youseffi, M.; Britland, S.T.; Liu, S.; See, C.; Somekh, M.; Zhang, J. Imaging of the cell surface interface using objective coupled widefield surface plasmon microscopy. *J. Struct. Biol.* **2008**, *164*, 75–80. [[CrossRef](#)] [[PubMed](#)]
42. Bauch, M.; Toma, K.; Toma, M.; Zhang, Q.; Dostalek, J. Plasmon-enhanced fluorescence biosensors: A review. *Plasmonics* **2014**, *9*, 781–799. [[CrossRef](#)] [[PubMed](#)]
43. Huck, A.; Witthaut, D.; Kumar, S.; Sørensen, A.S.; Andersen, U.L. Large optical nonlinearity of surface plasmon modes on thin gold films. *Plasmonics* **2013**, *8*, 1597–1605. [[CrossRef](#)]
44. Byrne, G.D.; Vllasaliu, D.; Falcone, F.H.; Somekh, M.G.; Stolnik, S. Live imaging of cellular internalization of single colloidal particle by combined label-free and fluorescence total internal reflection microscopy. *Mol. Pharm.* **2015**, *12*, 3862–3870. [[CrossRef](#)] [[PubMed](#)]
45. Byrne, G.; Pitter, M.; Zhang, J.; Falcone, F.; Stolnik, S.; Somekh, M. Total internal reflection microscopy for live imaging of cellular uptake of sub-micron non-fluorescent particles. *J. Microsc.* **2008**, *231*, 168–179. [[CrossRef](#)] [[PubMed](#)]
46. Zhang, B.; Pechprasarn, S.; Zhang, J.; Somekh, M.G. Confocal surface plasmon microscopy with pupil function engineering. *Opt. Express* **2012**, *20*, 7388–7397. [[CrossRef](#)] [[PubMed](#)]
47. Pechprasarn, S.; Zhang, B.; Albutt, D.; Zhang, J.; Somekh, M. Ultrastable embedded surface plasmon confocal interferometry. *Light Sci. Appl.* **2014**, *3*, e187. [[CrossRef](#)]
48. Zhang, B.; Pechprasarn, S.; Somekh, M.G. Quantitative plasmonic measurements using embedded phase stepping confocal interferometry. *Opt. Express* **2013**, *21*, 11523–11535. [[CrossRef](#)] [[PubMed](#)]
49. Zhang, B.; Pechprasarn, S.; Somekh, M.G. Surface plasmon microscopic sensing with beam profile modulation. *Opt. Express* **2012**, *20*, 28039–28048. [[CrossRef](#)] [[PubMed](#)]
50. Dan, D.; Lei, M.; Yao, B.; Wang, W.; Winterhalder, M.; Zumbusch, A.; Qi, Y.; Xia, L.; Yan, S.; Yang, Y. Dmd-based led-illumination super-resolution and optical sectioning microscopy. *Sci. Rep.* **2013**, *3*, 1116. [[CrossRef](#)] [[PubMed](#)]
51. Li, D.; Shao, L.; Chen, B.-C.; Zhang, X.; Zhang, M.; Moses, B.; Milkie, D.E.; Beach, J.R.; Hammer, J.A.; Pasham, M. Extended-resolution structured illumination imaging of endocytic and cytoskeletal dynamics. *Science* **2015**, *349*, aab3500. [[CrossRef](#)] [[PubMed](#)]
52. Malitson, I.H. Interspecimen comparison of the refractive index of fused silica. *J. Opt. Soc. Am.* **1965**, *55*, 1205–1209. [[CrossRef](#)]

