

Intercalary Reconstruction of the “Ultra-Critical Sized Bone Defect” by 3D-Printed Porous Prosthesis After Resection of Tibial Malignant Tumor

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Purpose: This study aimed to evaluate the early stability, limb function, and mechanical complications of 3D-printed porous prosthetic reconstruction for “ultra-critical sized bone defects” following intercalary tibial tumor resections.

Methods: This study defined an “ultra-critical sized bone defect” in the tibia when the length of segmental defect in the tibia was >15.0 cm or >60% of the full tibia and the length of the residual fragment in proximal or distal tibia was between 0.5 cm and 4.0 cm. Thus, five patients with “ultra-critical sized bone defects” following an intercalary tibial malignant tumor resection treated with 3D-printed porous prosthesis between June 2014 and June 2018 were retrospectively reviewed. Patient information, implants design and fabrication, surgical procedures, and early clinical outcome data were collected and evaluated.

Results: Among the five patients, three were male and two were female, with an average age of 30.2 years. Pathological diagnoses were two osteosarcomas, one Ewing sarcoma, one pseudo-myogenic hemangioendothelioma, and one undifferentiated pleomorphic sarcoma. The average length of the bone defects following tumor resection was 22.8cm, and the average length of ultra-short residual bone was 2.65cm (range=0.6cm–3.8cm). The mean follow-up time was 27.6 months (range=14.0–62.0 months). Early biological fixation was achieved in all five patients. The average time of clinical osseointegration at the bone–porous interface was 3.2 months. All patients were reported to be pain free and have no limitations in their walking distance. No prosthetic mechanical complications were observed.

Conclusion: Reconstruction of the “ultra-critical sized bone defect” after an intercalary tibial tumor resection using 3D-printed porous prosthesis achieved satisfactory overall early biological fixation and limb function. Excellent primary stability and the following rigid biological fixation were key factors for success. The outcomes of this study were supposed to support further clinical application and evaluation of 3D-printed porous prosthetic reconstruction for “ultra-critical sized bone defects” in the tibia.

Keywords: 3D-printed porous, prosthetic reconstruction, intercalary tibial resection, critical sized bone defect

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Introduction

Critical-sized bone defects vary with the anatomical location of the defect as well as the state of the surrounding soft tissues.¹ Tumor-associated defects arising in long bones are frequently associated with considerable segmental bone loss and extensive infiltration of the surrounding soft tissues, fulfilling the criteria of a “critical-sized

bone defect". The tibia is the second most common site for primary bone malignancies following the distal femur, and may also arise as a site of metastatic disease.² For epiphyseal sarcomas in the tibia, it is possible to consider an intercalary resection when more than 1.0 cm of epiphyseal tissue is retained beyond the tumor.³ There are three intercalary tibial tumor resection types: epi-diaphyseal resections with one osteotomy in the epiphyseal bone and one in the diaphyseal bone; meta-diaphyseal resections with one osteotomy in the metaphyseal bone and one in the diaphyseal bone; or diaphyseal resection with both osteotomies in diaphyseal bone.⁴ However, reconstructions after intercalary tibial tumor resection are quite a challenge, and biological reconstructions seem to remain the main option.

Biological reconstructions of intercalary defects include vascularized fibula grafts, allografts, and reinsertions of extra-corporally irradiated autografts.⁵ However, the obvious drawbacks of each method and high complication rates limit their clinical application when there are massive segmental bone defects. For example, the smaller cross-sectional areas associated with fibula grafts leaves the graft weaker than the originally resected long bone and requires longer periods of non-weight-bearing; allografts have a high rate of immune rejection and non-union; extra-corporeally devitalized autografts are contraindicated in marked osteolytic lesions and histological analysis of the whole specimen is not possible.⁶ The recent introduction of the induced-membrane technique, developed by Masquelet et al, has demonstrated promising preliminary results when applied in the reconstruction of bone-tumor defects.⁷ However, the risk of graft resorption and a two-stage surgery with a minimum of 6 months duration of treatment has limited its application. For distraction osteogenesis, the length of preserved epiphysis should be ≥ 1.0 cm after tumor resection, and the complications significantly outweigh the benefits when bone defects are >15.0 cm.⁸

Intercalary reconstruction using prosthesis allows for early prosthetic stability, rapid rehabilitation and weight-bearing, when compared with biological reconstructions.⁹ However, the fixation of the stem if there is only a very short bone stock left after intercalary resection is quite difficult. The high stress concentration at the bone–stem interface heralds the high loosening probability in the future. So, it is commonly accepted for conventional prosthetic stems insertion that the adjacent joint needs to be sacrificed when the residual bone is ultra-short, potentially leading to increased instability but permanent reduction in the limb function.¹⁰ Ahlmann et al¹¹ have suggested that

the shortest length of bone required for fixation of the implant stem is 5.0 cm. And fixation in a short segment <4.0 cm was reported as hazardous owing to the possibility of early loosening and peri-prosthetic fracture.¹² Thus, in addition to producing a critical-sized bone defect after intercalary tumor resection of long bones, an ultra-short residual bone also poses many challenges for the reconstruction. Hence, we proposed that the concept that an "ultra-critical sized bone defect" may be more precise, reflecting the clinical intervention of some tumor defects after intercalary resection. An "ultra-critical sized bone defect" in tibia should basically follow the two clinical criteria: the length of segmental defect in tibia >15.0 cm or $>60\%$ of full tibia;¹³ and the length of residual fragment in proximal or distal tibia was between 0.5–4.0 cm.

3D-printed porous prosthesis is regarded as a new and exciting generation of uncemented implants which are demonstrating marked clinical success.^{14,15} For the reconstruction large-bone defects, 3D-printed porous titanium scaffolds supply adequate mechanical support and facilitate bone formation, which results in high mechanical integrity.¹⁶ Clinically, implants with 3D-printed porous prosthesis had shown feasible primary stability for massive segmental bone tumoral defects.¹⁷ And the first application of 3D printed porous prosthesis for massive proximal tibia defect was successful.¹⁸ Thus, we were highly interested in the efficacy of prosthesis with 3D-printed porous for intercalary tibia tumoral defects. In this study, we evaluated the early clinical outcome of patients with "ultra-critical sized bone defect" in tibia receiving 3D-printed porous prosthetic reconstruction.

Methods

Patients

This retrospective study was conducted with the approval of the ethics committee of West China Hospital, Sichuan University. Informed consent was obtained from all individual participants included in the study.

Between June 2014 and June 2018, five patients with "ultra-critical sized bone defects" after intercalary tibial tumor resection received 3D-printed porous prosthetic reconstruction (Figure 1), including one previously reported case.¹⁸ Biopsy was performed for each patient before undergoing definitive surgery. The surgical stage was determined according to the Enneking bone and soft tissue sarcoma staging system,¹⁹ and the AJCC staging system.²⁰ Among the five patients, three were male and two were female, with

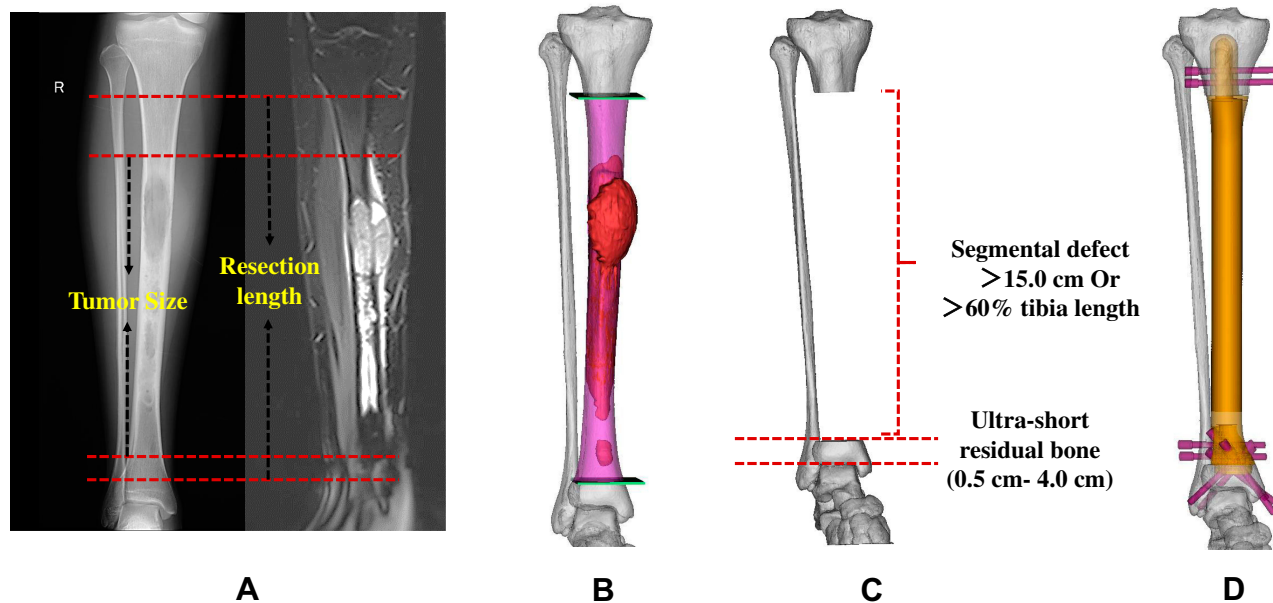


Figure 1 An “ultra-critical sized bone defect” after intercalary tibia tumor resection. (A) A critical sized bone defect with ultra-short residual fragment may be produced after intercalary tibial tumor resection; (B) Reconstructed tumoral 3D model of the affected tibia with resection boundary; (C) An “ultra-critical sized bone defect” was the length of segmental defect over 15.0 cm with one side of the residual tibial between 0.5 cm and 4.0 cm in length; (D) Reconstructed 3D model indicated the initial reconstruction plan for the “ultra-critical sized bone defect” after intercalary tibia tumoral resection.

an average age of 30.2 years. Pathological diagnoses were osteosarcoma in two cases, Ewing sarcoma, pseudo-myogenic hemangioendothelioma, and undifferentiated pleomorphic sarcoma in one case each (Table 1). Four patients who were Enneking and AJCC stage IIB at the time of diagnosis received the standard pre-operative chemotherapy regimen in use at the time of treatment. Clinical characteristics of patients, including age, gender, tumor size, defects length, and the length of residual proximal or distal tibia, were collected.

Implants Properties

All prostheses were designed by our clinical team and fabricated by Chunli Co, Ltd., Tongzhou, Beijing, China. The porosity of printed titanium alloy was 60–70% with a size of 600 μm .²¹ 3D computed tomography (CT) scan data 2 weeks before the planned surgery was obtained and imported into the Mimics V17.0 software (Materialise Corp., Belgium) to evaluate the parameters of the defects. Then, all design of the prosthesis was comprehensively considered based on the specific defect of each patient to achieve the best stability (Figure 2). Specifically, for residual tibia <1.0 cm (case 3), two strategies were adopted to increase the primary stability: (a) Cross screws fixation was designed according to the 3D space anatomical distribution; (b) Due to the extremely limited space for stem

insertion, a strain was produced by a 2.0–3.0 mm exceeded length of implants over the defect (Figure 3A). When the length of proximal tibia was between 1.0 cm and 4.0 cm, a conformal design complementary to the residual proximal tibia with cross screws fixation was adopted (case 1 and case 4). For distal tibia, when bone stock was between 1.0 cm and 2.0 cm in length, an at least 0.5 cm insertion porous portion was fabricated to increase the interface of bone–porous (Figure 3B). This special design supplied the capability of against rotation force and bend force that can apparently increase the stability of implantation. When residual distal bone was between 2.0 cm and 4.0 cm in length, the designed plan was determined according to the proximal ultra-short component design (case 1 and 3). Generally, short stem with cross screws fixation was maximumly adopted at this condition (Figure 3C). Based on the comparative long term survival of porous prosthesis,²² for residual bone between 4.0 cm and 10.0 cm in length, a short curve 3D-printed porous stem with transvers screws fixation was adopted (Figure 3D) (case 2). For residual bone over 10.0 cm in length, we chose a short uncemented casting stem with hydroxyapatite (HA) coating according to our previous study (case 4 and case 5).²³ All 3D-printed porous component can be combined with the modular endoprosthesis system used at our hospital (Chunli Co, Ltd., Tongzhou, Beijing, China.). The

Table 1 Basic Information and Follow-Up Metrics of the Included Five Patients

Cases	Age (Years)	Gender	Pathological Diagnosis	Enneking Stage	AJCC Stage	Tumor Size (cm)	Defect Length (cm)	Residual Bone Length (Proximal/ Distal, cm)	Total Tibia Length (cm)/Ratio of Defect on Total Tibia Length*	Follow-Up (Months)	Time of Osseointegration (Months)	MSTS Score	OKS	AOFAS
1	55	Male	Pseudomyogenic hemangioidothelioma	IB	IB	21.1	27.1	3.1/3.5	33.7 (80.4%)	25	3	28	44	94
2	13	Male	Osteosarcoma	IIB	IIB	19.6	23.3	10.1/0.6	34.0 (68.5%)	21	4	24	45	81
3	19	Female	Ewing sarcoma	IIB	IIB	21.7	28.7	5.8/1.4	35.9 (79.9%)	14	3	26	46	84
4	16	Male	Osteosarcoma	IIB	IIB	12.1	16.4	3.8/13.3	33.5 (49.0%)	62	3	28	44	95
5	48	Female	Undifferentiated Pleomorphic Sarcoma	IIB	IIB	14.7	18.7	3.5/11.4	33.6 (55.7%)	16	3	28	45	95

Note: *The percentage of defect length on total tibia length.

designing and fabricating of these custom prostheses takes about 7–10 days.

Surgical Procedure

Resection margin was determined according to preoperative magnetic resonance imaging (MRI) and CT scans which were obtained to evaluate the extent of soft tissue extension of tumor and bone destruction. Segmental resection was under the principle to achieve a safe margin for osteogenic sarcoma. Generally, the osteotomy level was determined at least 2.0 cm beyond the boundary, and a custom cutting guide was made corresponding to the resection principle. During the osteotomy, bone markers were customized according to the guide plate: the guide plate for proximal tibial osteotomy was riveted with the tibial tubercle; For distal tibia osteotomy, the guide plate was riveted with the median point of the leading edge of tibia and ankle acupoint. After all osteotomies were completed, intra-operative X-ray was used for verification. Tibial tuberosity was maximumly preserved during osteotomy in all patients (Figure 4). The mean width of the distal tibiofibular syndesmosis anteriorly between the tip of the anterior tibial tubercle and the nearest point of the fibula was 2.0 mm.²⁴ So, we preserved at least 1.0–1.5 mm width of distal tibiofibular syndesmosis to guarantee the stability of the ankle joint.

Reconstruction procedure was performed from the side with the longer residual bone to the shorter one. The residual tibia of proximal or distal parts was reamed to fit the 3D-printed porous component with our customized reaming instruments. Implanting the porous part of the prosthesis exactly at the original position was relatively demanding. Stems were press-fit inserted into the reamed tibia medulla cavity. After confirming both locations of the proximal and distal parts of the prosthesis, screws were inserted to enhance primary stability according to the pre-operative designing. Intraoperative X-ray was adopted to confirm the placed position of these components. For soft tissue coverage, as the volume of prosthesis was smaller than the host bone, so directly suturing the residual gastrocnemius and tibialis anterior muscle were performed in the majority of cases. And the medial head of the gastrocnemius muscle flap was used to cover the upper part of the prosthesis when necessary. If soft tissue defects were quite large, free skin grafting was considered.

Post-Operative Management

The rehabilitation protocol was customized to the patient depending on the rigidity of biological fixation. Generally,

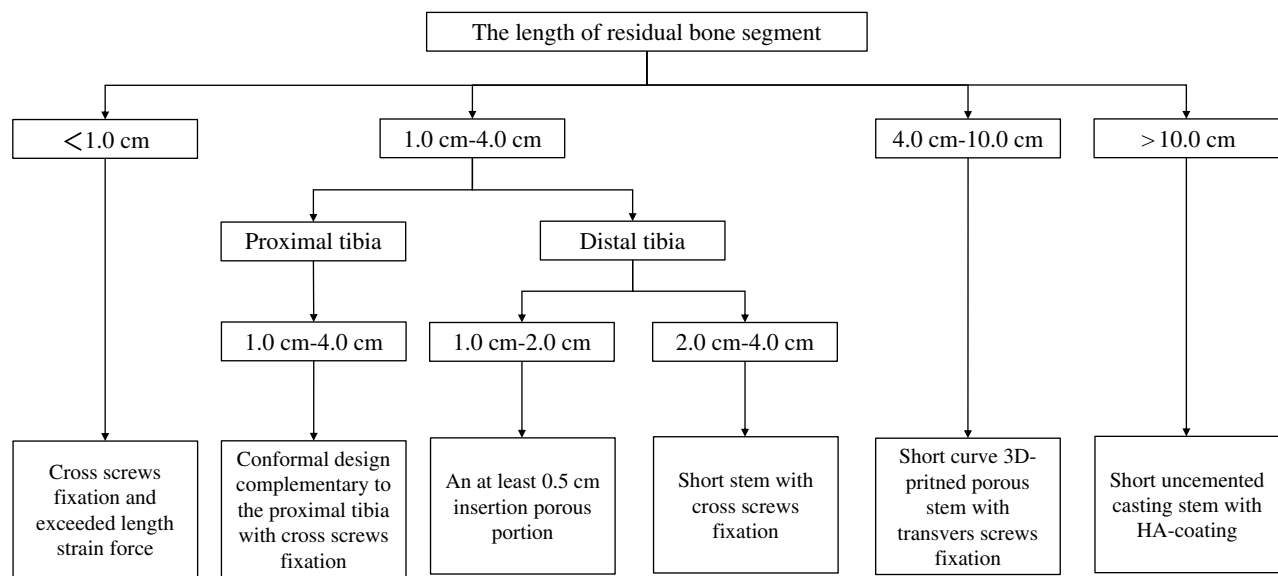


Figure 2 The designing flow diagram of 3D-printed porous prosthesis for “ultra-critical sized bone defect” in the tibia.

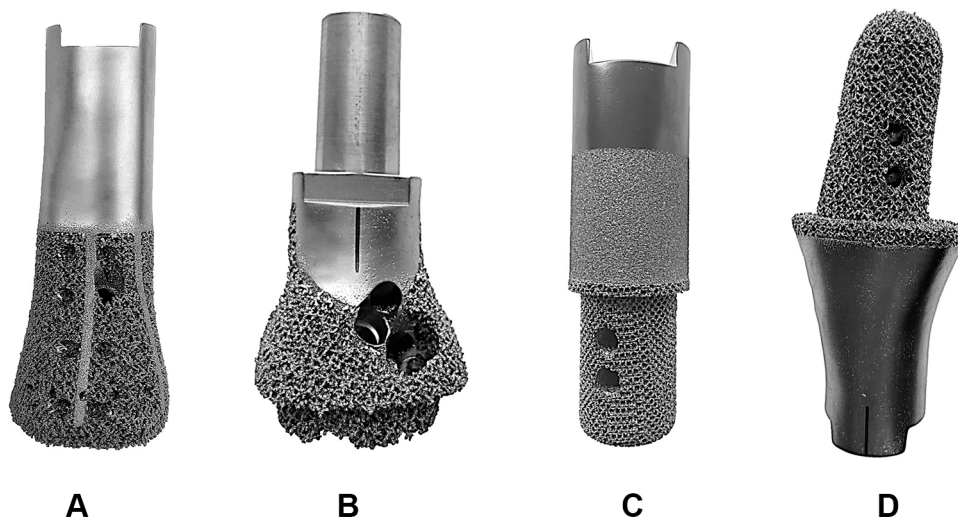


Figure 3 3D-printed porous components for ultra-short residual bone fixation. (A) A distal 3D-printed component designed for ultra-short residual fragment less than 1.0 cm in length; (B) A distal component, at least 0.5 cm insertion part was designed to increase the contact interface of bone–porous. And cross screws fixation was applied according to the three-dimensional anatomical distribution; (C) A distal component, transvers screw fixation was designed to improve the primary stability of implantation; (D) A proximal component, transverse holes for lock nails were designed to enhance the primary stability of prosthesis.

patients were informed about non-weight-bearing standing and walking with crutches for the first 6 weeks after surgery. Active flexion of the knee and dorsal extension of the ankle were encouraged when the patient could walk with partial weight-bearing 6 weeks after surgery. The patient was informed about partial weight bearing at 6 weeks and then full weight bearing from 3 months postoperatively. Patients were followed up every month for the first 3 months, then every 2–6 months to date. Osseointegration was evaluated by Tomosynthesis-

Shimadzu metal artefact reduction technology (T-SMART), which reduced the metal artifacts. Enneking functional evaluation score for limb salvage, the revised Oxford Knee Score (OKS) for knee function and the American Orthopaedic Foot and Ankle Society (AOFAS) for ankle function were assessed at each follow-up visit. Rigid biological fixation was considered when there were at least three solid bony junctions on T-SMART images and should be in accordance with the clinical symptoms during weight-bearing activities.¹³

Results

The average length of bone defects after tumor resection was 22.8 cm, while the average length of “ultra-short” bone was 2.65 cm. The average percentage of defects on full tibia length was 66.7% (Table 1). The mean follow-up was 27.6 months, ranging from 14 months to 62 months. The average time of rigid biological fixation achieving was 3.2 months (Figure 5). For case 2, in which we did not perform transverse screw fixation for proximal stem as good primary stability was required during in-operative evaluation, a hardened area was seen around the stem. This patient was told to be non-weight-bearing for another 4 weeks until biological fixation was achieved. All patients reported to be pain-free and have no limitations in walking distances (Figure 6). The average MSTS score was 26.8/30 at last follow-up visit.



Figure 4 Precise osteotomy during resection procedure. In-operative image of case 1 showed the tibial tuberosity was preserved under precise osteotomy with a safe resection margin.

The mean OKS and AOFAS score were 44.8/48 and 89.8/100, respectively (Table 1). No prosthetic mechanical complications such as aseptic loosening, peri-prosthesis fracture, or implants breakage were observed. Also, there were no tumor recurrence, deep infection, or wound healing problems during the follow-up.

Discussion

With the development of neoadjuvant systemic therapy, the improved life expectancy of patients with malignant tumors of bone has led to an increased emphasis on limb salvage as well as the function preservation. Also, image technology improvement optimized the precise osteotomy procedure to achieve a clear resection margin. However, surgeons choose reconstruction type for an “ultra-critical sized bone defect” on individual patient and oncologic factors as well as on their own surgical experiences. Metallic prosthesis replacement allowed rapid rehabilitation and early weight-bearing activities after surgery. However, when >60% of the tibia was resected, the overall implant survival was much poorer, possibly due to the long arm of force that increased the instability after implantation.²⁵ Biological reconstruction for a massive segmental defect over 15.0 cm or over 60% of tibia required a large amount of bone mass. A two-stage surgery of induced-membrane technical with at least 6-month duration and the bone absorption risk limited its application at this situation.⁷ Parameters critical for the success of distraction osteogenesis include a lesion ≤ 15.0 cm in length with at least 0.5 cm of subchondral bone and sufficient metaphyseal cortex retained after excision of tumors.²⁶ The above two biological reconstructions sacrificing time to fix massive bone defect largely increased the difficulty of post-operative management. In addition, post-operative chemotherapy lowers the success rate of biological reconstructions as the adverse effect on bone healing and is associated with high rates of fracture and infection.²⁷ At this condition, prosthetic reconstruction with rigid biological fixation from 3D-printed porous implant may be one of the solutions. Thus, we set the length of intercalary tibial defects over 15.0 cm or 60% of tibia as the first essential condition of an “ultra-critical sized bone defect”.

For regular limb sparing prosthesis replacement, the use of HA-coating grooved collars may lead to osteointegration of the implant collar and may reduce the rate of aseptic loosening.²⁸ The early implant using cement fixation technique requires an at least 5.0 cm medullary cavity for fixation.¹¹ When the length of the short-segment intramedullary stem is <4.0 cm, there may be a higher rate of aseptic

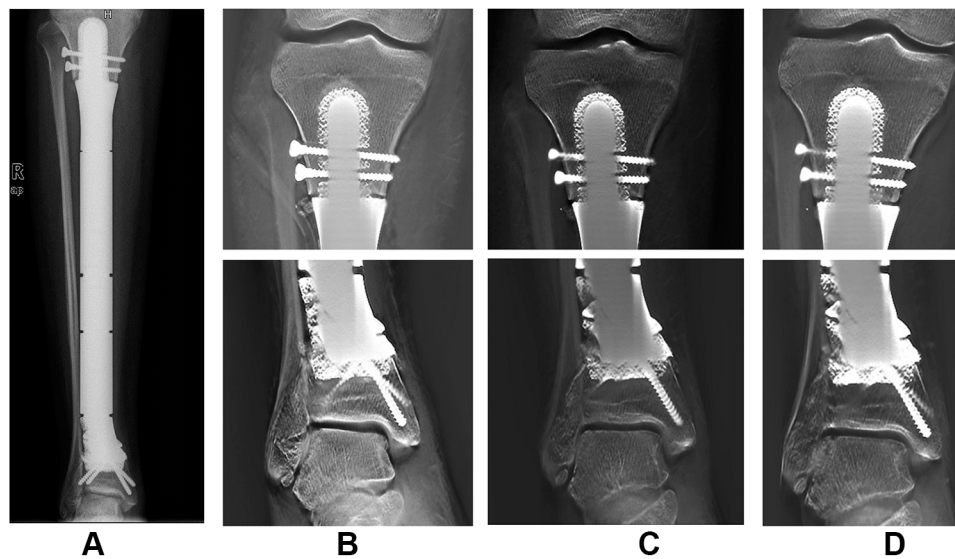


Figure 5 Rigid biological fixation achieved after 3D-printed porous prosthetic reconstruction for a tibial “ultra-critical sized bone defect”. (A) X-ray of full affected tibia at 3-months after surgery of case 3; (B) T-smart images at 1 month after surgery of case 3, indicated excellent press-fit of the stem; (C and D) T-smart images at 2 months and 3 months after surgery, respectively. The hardened area around the proximal component largely decreased when compared with the images at 1 month after surgery, indicating good bone ingrowth processed during this period. The distal component also achieved excellent biological fixation.

loosening and peri-prosthetic fracture.¹² HA-coating plate and anchorage system are the current two effective options for short residual bone segment less than 4.0 cm (Table 2). HA-coated extracortical plates have been used in joint-sparing surgery with excellent osseointegration at the prosthesis–proximal bone interface and formation of new bone around the HA collar.²⁹ For proximal tibial replacement, using HA-coated extracortical plate fixation when short-segment intramedullary fixation is less than 4.0 cm allows preservation of the knee joint with good function and no early evidence of loosening.³⁰ Guder et al³¹ developed an ultra-short stem anchorage for intercalary tibia reconstruction, but at least 3.0 cm of tibia plateau should remain after

tumor resection. The main complication of the two systems is peri-prosthesis fracture, possibly due to the local high stress and relatively weak biological fixation. However, the individual design and excellent biological fixation of 3D-printed porous implants make the reconstruction of intercalary defects with residual bone less than 1.0 cm available. Thus, with the collected data in literature and our own clinical evidence, we set 0.5–4.0 cm as the second essential requirement for an “ultra-short” residual bone after intercalary tibia tumor resection.

Osteoarticular allograft has better post-operative limb function when compared with metallic prosthesis reconstruction.³² This indicates the benefits of biological

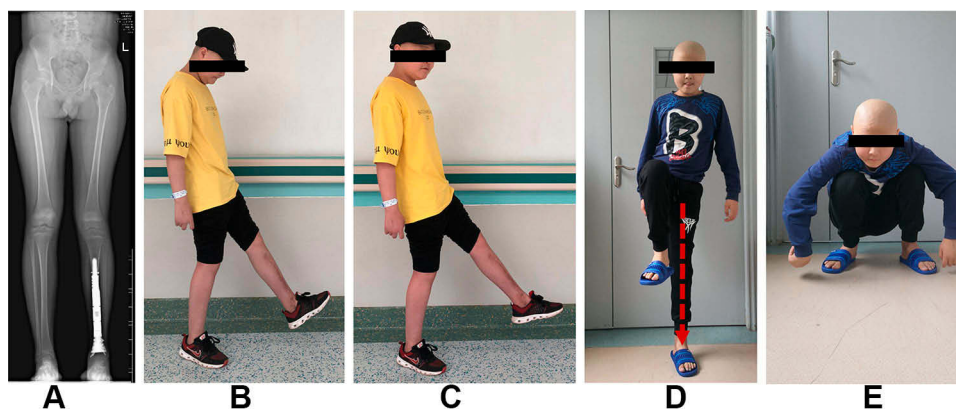


Figure 6 Limb function after 3D-printed porous prosthetic reconstruction. (A) X-ray with full lower limb at 3 months after surgery of case 2; (B and C). Three months after surgery, the ankle flexion and extension of this patient were normal; (D) Six months after surgery, this patient could stand up just with the affected limb without any pain; (E) Six months after surgery, this patient could squat and stand up without any difficulty.

reconstruction for function restore, and the importance of adjacent residual bone preservation. We preserved the distal tibiofibular syndesmosis in case 3 with 0.6 cm distal tibia left after segmental resection. Preserving the distal tibiofibular syndesmosis and other ankle-stabilizing ligaments ensures an early stabilization of implants and a satisfactory function of the affected limb.³³ Tibial tuberosity was preserved in all five patients under the wide resection principle. Avulsion and/or extensor lag may lead to poor function. Titus et al³⁴ reattached the patellar ligament to the tibial tuberosity of the proximal tibial mega-prosthesis with a porous surface, and the repair was protected with a cerclage wire through the patella and the prosthesis. This technique resulted in good quadriceps function and a low incidence of complications. Surgeons also directly repaired the patellar tendon on to the transposed medial head of gastrocnemius if the attachment was sacrificed during the tumor resection procedure.³⁰

3D printed technology shows promising potential in medical areas.^{35,36} And novel 3D-printed implants with highly porous surface achieved fair biological fixation in orthopedics surgery^{15,37,39} (Table 3). However, a high primary mechanical stability is essential for a successful osseointegration of implants.⁴⁰ The application of transvers or cross screws fixation was rational in our study as rigid stable fixation was associated with a lower failure rate of reconstruction, and was also the precondition of well bone ingrowth and the following rigid biological fixation.¹³ We

proposed that a micromotion of the stem delayed the bone healing in case 2. When the ends of a fractured long bone are reduced, there should be absolutely no movement between the fragments to endorse fracture healing.⁴¹ This happens because movements, even at the micrometer range, can induce a stress or strain that may hinder the formation of new cells in the gap. The same phenomenon is applied at the bone-to-implant interface.⁴² In addition, the induction of micromotion during functional loading may also be responsible for failure of osseointegration. Micromotions above 50–100 μm negatively influence osseointegration and bone remodeling by forming fibrous tissues and inducing bone resorption at the bone-to-implant interface.⁴³ Thus, all cases in our study were restricted to no weight bearing within the first 6 weeks after surgery, during which time the primary bone ingrowth processed.

There were some limitations of this study. First, the number of cases involved in this study was quite small, due to the limited patients with “ultra-critical sized bone defect” after intercalary tibial resection; Second, the duration of follow-up of the five patients was not long, as we aimed here to evaluate the early stability of 3D-printed porous prosthesis for reconstructing the “ultra-critical sized bone defect” in the tibia. So, long-term follow-up is needed; Third, the mechanical analysis of the reconstruction using 3D-printed porous prosthesis for “ultra-critical sized bone defect” should be performed in the future.

Table 2 Custom Implants for Ultra-Short Bone Fixation After Intercalary Tibial Tumoral Resection

References	Technical	Patients	Defect	Ultra-Short (Average)	Follow-Up	MSTS Score	Mechanical Complication
Guder et al 2017 ³¹	Ultra-short anchorage system	4	18.0 cm	3.0–3.5 cm (3.13)	56 months	28/30	Two PF
Spiegelberg et al 2009 ³⁰	HA-coated extracortical plate	8	—	1.3–4.8 cm (2.63)	35 months	24/30	One PF
Our study 2019	3D-printed porous	5	22.8 cm	0.6–3.8 cm (2.65)	27.6 months	26.8/30	None

Abbreviation: PF, Peri-prosthetic fracture.

Table 3 Current Clinical Applications of 3D-Printed Porous Implants in Orthopedics Surgery (Case Series Over 3)

References	Implants	Application	Patients	Follow-Up	Clinical Outcome
Fan et al 2015 ³⁷	3D-printed titanium prosthesis	Limb salvage surgery	3	21 months	No mechanical complications
Sporer et al 2019 ³⁸	3D-printed highly porous tibial baseplate and metal-backed patella	Total Knee Arthroplasty	29	2.0 years	Biological fixation
Guo et al 2019 ³⁹	3D-printed sacral endoprosthesis	Total en-bloc sacrectomy reconstruction	32	22.1 months	Reliable spinopelvic stability
Sultan et al 2020 ¹⁵	3D-printed highly porous titanium-coated baseplate	Total Knee Arthroplasty	496	2.0 years	Biological fixation

Conclusion

Overall, the early clinical outcome in this study was supposed to support the further clinical application of 3D-printed porous prosthesis for “ultra-critical sized bone defect” after intercalary tibial tumor resection. Excellent primary stability and the following rigid biological fixation were the key factors for success if the 3D-printed porous prosthesis was applied under the situation of “ultra-critical sized bone defect”. With the rapid development of adjuvant therapy and image management technics for malignant bone tumors, more patients get favorable tumor control with a relatively long life-expectation. They would like to receive the surgery aiming at functional reconstruction and precise tumor resection. Thus, the concept “ultra-critical-sized bone defect” has practical clinical value in the future. Here, we presented the definition and the two essential conditions of “ultra-critical sized bone defect” in the tibia after intercalary tibial malignant tumor resection. However, due to the differences of anatomy structures, limb function, and mechanical conduction, the length of defects and residual bone for an “ultra-critical sized bone defect” in the femur and humerus varies with tibia. Thus, the future related work to define this concept in these long bones and the mechanical analysis of the 3D-printed porous prosthetic reconstructions are imperative.

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Disclosure

The authors declare that they have no conflict of interest in this work.

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