

Article

# Electrical Characteristics and pH Response of a Parylene-H Sensing Membrane in a Si-Nanonet Ion-Sensitive Field-Effect Transistor

Bo Jin <sup>1,†</sup>, Ga-Yeon Lee <sup>2,†</sup>, ChanOh Park <sup>3,†</sup>, Donghoon Kim <sup>1</sup>, Wonyeong Choi <sup>1</sup>, Jae-Woo Yoo <sup>4</sup>, Jae-Chul Pyun <sup>2,\*</sup>  and Jeong-Soo Lee <sup>1,\*</sup>

<sup>1</sup> Department of Electrical Engineering, Pohang University of Science and Technology, Pohang 37673, Korea; shengzhi86@postech.ac.kr (B.J.); kdong620@postech.ac.kr (D.K.); pathfinder@postech.ac.kr (W.C.)

<sup>2</sup> Department of Materials Science and Engineering, Yonsei University, Seoul 03722, Korea; gayeon@yonsei.ac.kr

<sup>3</sup> Division of IT Convergence Engineering, Pohang University of Science and Technology, Pohang 37673, Korea; chduckling@postech.ac.kr

<sup>4</sup> IM Healthcare Co. Ltd., Yongin 26354, Korea; jwyo@im-healthcare.com

\* Correspondence: jcpyun@yonsei.ac.kr (J.-C.P.); ljs6951@postech.ac.kr (J.-S.L.); Tel.: +82-22-123-5851 (J.-C.P.); +82-54-279-2380 (J.-S.L.)

† These authors contributed equally to this work.

Received: 28 October 2018; Accepted: 10 November 2018; Published: 12 November 2018



**Abstract:** We report the electrical characteristics and pH responses of a Si-nanonet ion-sensitive field-effect transistor with ultra-thin parylene-H as a gate sensing membrane. The fabricated device shows excellent DC characteristics: a low subthreshold swing of 85 mV/dec, a high current on/off ratio of  $\sim 10^7$  and a low gate leakage current of  $\sim 10^{-10}$  A. The low interface trap density of  $1.04 \times 10^{12} \text{ cm}^{-2}$  and high field-effect mobility of  $510 \text{ cm}^2\text{V}^{-1}\text{s}^{-1}$  were obtained. The pH responses of the devices were evaluated in various pH buffer solutions. A high pH sensitivity of  $48.1 \pm 0.5 \text{ mV/pH}$  with a device-to-device variation of  $\sim 6.1\%$  was achieved. From the low-frequency noise characterization, the signal-to-noise ratio was extracted as high as  $\sim 3400 \text{ A/A}$  with the lowest noise equivalent pH value of  $\sim 0.002 \text{ pH}$ . These excellent intrinsic electrical and pH sensing performances suggest that parylene-H can be promising as a sensing membrane in an ISFET-based biosensor platform.

**Keywords:** parylene-H; ion-sensitive field-effect transistor (ISFET); pH response

## 1. Introduction

The ion-sensitive field-effect transistor (ISFET) sensor is a potential candidate for future bioassay applications due to its low cost, fast response, high sensitivity and small sensing size. Recently, studies have been conducted on channel materials such as carbon nanotubes and graphene-based materials [1,2]; channel structures such as silicon nanowire (Si NW) arrays, Si-nanonet structure and suspended Si NW [3–5]. Other approaches to improve the sensing responses have been made by introducing alternative sensing materials instead of  $\text{SiO}_2$  as the gate insulator in ISFET. Several issues related to sensing membranes such as insufficient isolation between the electrolyte and ISFET channel and dangling bonds in the sensing membrane can degrade the sensing responses, reliability and lifetime [6,7].

Parylene (polymer of *p*-xylene), which is extensively used as a biocompatible encapsulant for implantable microdevices [8], can be utilized as an ISFET gate insulator due to its high electrical resistivity. More recently, a new parylene modified with a formyl group (parylene-H) was proposed

as a sensing membrane in microplate-based immunoassay and surface plasmon resonance (SPR) biosensor applications [9,10]. It has been demonstrated that the formyl group of parylene-H can covalently bond to the primary amine group of target molecules without any additional surface modification steps [10].

In this paper, we fabricated Si-nanonet ISFETs with parylene-H gate insulator (p-H ISFETs) and investigated their DC and reliability characteristics. We also evaluated the pH sensitivity of the p-H ISFETs in various buffer solutions and conducted low frequency noise analysis for potential development in bioassay applications.

## 2. Experimental Section

### 2.1. Device Fabrication

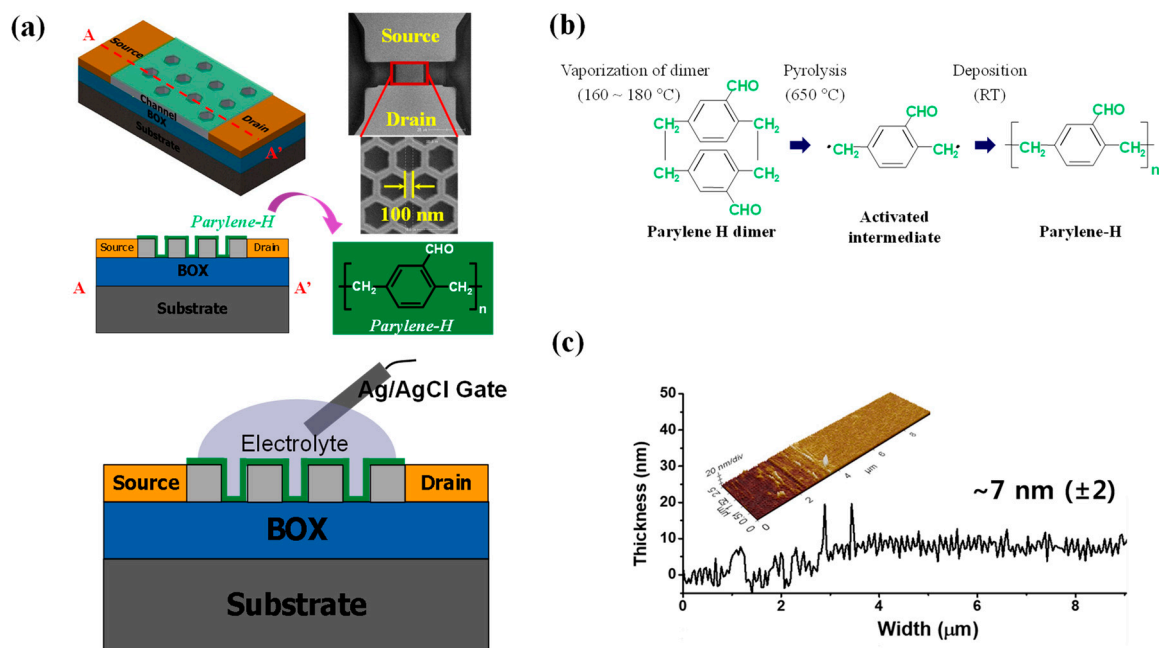
The p-H ISFETs were fabricated on an 8-inch silicon on an insulator substrate comprising a 100-nm top Si layer (<100> oriented, boron-doped,  $10 \Omega\cdot\text{cm}$ ) and a 400-nm buried oxide layer. The active region was formed by photolithography and inductively-coupled plasma reactive etching (ICP-RIE). To form the source and drain regions, arsenic ions with a dose of  $5 \times 10^{15} \text{ cm}^{-2}$  were implanted by an ion implantation process with masking the ISFET active channel region by photoresist, and post-annealing at  $1000 \text{ }^\circ\text{C}$  for 20 s was performed to activate the dopants. Then, the nanonet structure was defined on the ISFET channel region by electron-beam lithography and ICP-RIE. A metal layer of  $\sim 200 \text{ nm}$  was deposited and patterned by a lift-off process on the source and drain regions to provide low contact resistance. A  $1.5\text{-}\mu\text{m}$  SU-8 layer was coated to provide a passivation layer while opening the FET channel and the source and drain contact pad regions.

The parylene-H layer was thermally deposited by the following polymerization steps: (1) evaporation of parylene dimers at  $160 \text{ }^\circ\text{C}$ , (2) production of a highly reactive *p*-xylene radical by pyrolysis at  $650 \text{ }^\circ\text{C}$  and (3) deposition of the wafer at room temperature [11,12]. To control the thickness of the parylene-H layer, the quartz crystal microbalance response was measured from the beginning of the evaporation step. Finally, after the deposition of the parylene-H layer so as to form the gate insulator, the contact pad regions were opened.

### 2.2. Apparatus

The entire parylene-H coating procedure was reproducibly conducted using a microprocessor-controlled parylene coater. The morphology of the as-fabricated ISFET channel was observed by scanning electron microscopy (SEM), and the thickness of parylene-H was confirmed by atomic force microscopy (AFM). The electrical characteristics of the fabricated ISFETs were measured for current-voltage (I-V) with a Keithley 4200-SCS analyzer and capacitance-voltage (C-V) with an Agilent 4284A Precision LCR Meter at room temperature. Low frequency noise characteristics were measured with a noise analyzer Cadence BTA9812A/B and a vector signal analyzer Agilent 89441A. The gate bias was applied to the liquid gate through the external Ag/AgCl reference electrode. All the electrical characterizations of the devices were performed in  $0.01 \times$  PBS solution at room temperature.

Si-nanonet ISFETs with a 100-nm branch width were fabricated, as shown in Figure 1a. The illustration of the parylene-H deposition process is shown in Figure 1b. A 7 nm-thick parylene-H layer was deposited on the nanonet channel. The thickness was measured using AFM, as shown in Figure 1c.



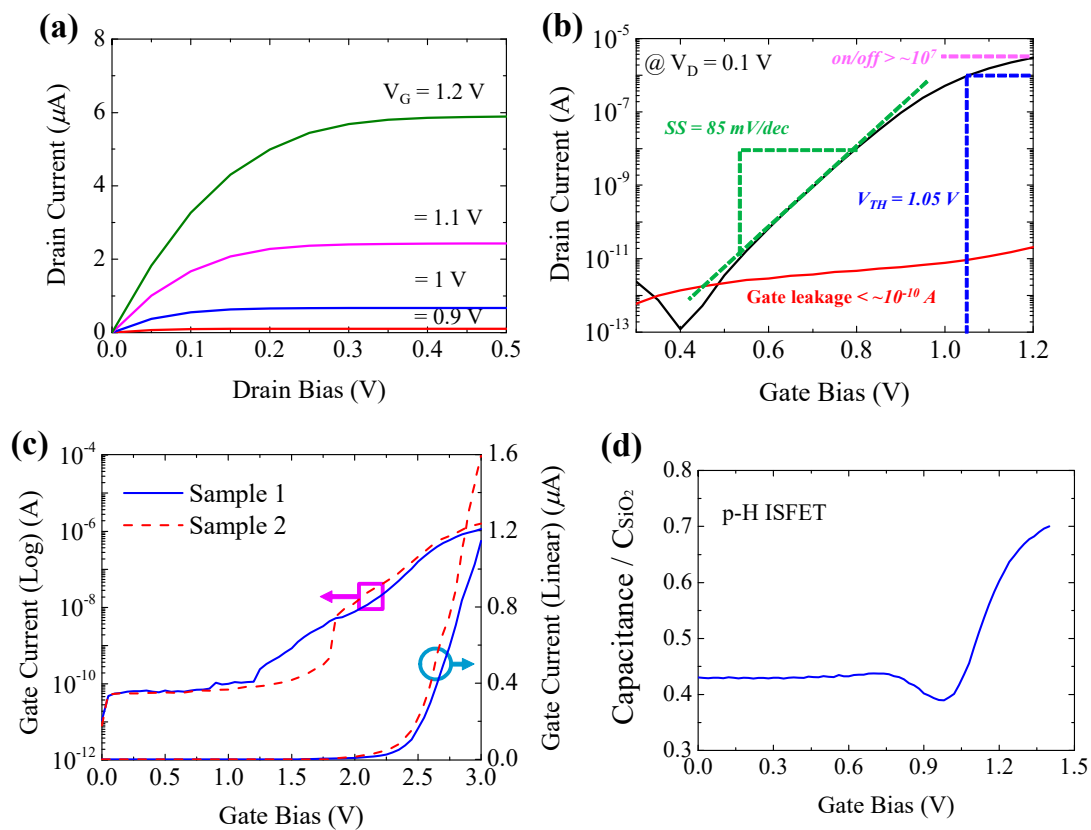
**Figure 1.** (a) Schematics and top-view SEM images of the fabricated Si-nanonet ISFET with parylene-H as the gate insulator. (b) Illustration of the parylene-H deposition process. (c) AFM images of the parylene-H nanolayer with a 7-nm thickness.

### 3. Results and Discussion

#### 3.1. DC and Reliability Characteristics of p-H ISFETs

To investigate the DC characteristics of parylene-H as a gate insulator, the output characteristic curve ( $I_D$ - $V_D$ ) and transfer curve ( $I_D$ - $V_G$ ) of the p-H ISFET with a 7 nm-thick parylene-H were measured, as shown in Figure 2. The drain bias ( $V_D$ ) was swept from 0–0.5 V by applying the liquid gate bias ( $V_G$ ) from 0.9–1.2 V in steps of 0.1 V. The drain current ( $I_D$ ) showed a linearly increasing behavior as explained by  $I_D \propto (V_G - V_{TH}) \cdot V_D$  at low  $V_D$ , while the saturation condition was obtained at higher  $V_D$  as explained by  $I_D \propto (V_G - V_{TH})^2$ , indicating typical n-type FET behaviors. In Figure 2b,  $V_G$  was swept from 0.3–1.2 V at constant  $V_D = 0.1$  V. Excellent electrical characteristics were obtained with a high  $I_D$  on/off ratio of  $>10^7$ , a low subthreshold swing (SS) of  $\sim 85$  mV/dec, a low threshold voltage ( $V_{TH}$ ) of 1.05 V at a constant current level of  $10^{-6}$  A and a low gate leakage current of  $<10^{-10}$  A in the whole swept range. These DC characteristics suggest that parylene-H shows outstanding electrical properties in electron device applications, replacing conventional silicon dioxide material.

To further evaluate the reliability of parylene-H as a gate insulator, the breakdown behavior was investigated by applying gate bias stress from 0–3 V. As shown in Figure 2c, the gate current ( $I_G$ ) increased with the applied gate bias. Within the range of  $V_G = 1.5$ –2.5 V, the  $I_G$  showed a soft breakdown where an abnormal increase of the leakage current at relatively lower gate bias was observed; over  $V_G = 2.5$  V, the  $I_G$  increased greatly, leading to a hard breakdown [13]. By C-V characterization, both of the capacitances of p-H ISFET and  $\text{SiO}_2$  gate insulator ISFET (Ox ISFET) with the same channel area were measured, and Figure 2d shows the normalized C-V characteristics of the p-H ISFET. The capacitance of p-H ISFET was extracted to be  $3.92 \times 10^{-7}$  F/cm<sup>2</sup>, and therefore, the dielectric constant of parylene-H was estimated to be  $\sim 3.1$ , comparable to the 2.6–3.2 range of the parylene series as reported in the literature [14]. Therefore, the equivalent oxide thickness (EOT) of a 7 nm-thick parylene-H in p-H ISFET was calculated as low as  $\sim 8.8$  nm.



**Figure 2.** Electrical characteristics of the fabricated parylene-H (p-H) ISFET in  $0.01 \times$  PBS buffer solution. (a) Typical  $I_D$ - $V_D$  output characteristics in the linear scale. (b) Typical  $I_D$ - $V_G$  transfer characteristics and  $I_G$ - $V_G$  gate leakage current characteristics at  $V_D = 0.1$  V in log scale indicating a typical n-type behavior. (c)  $I_G$ - $V_G$  characteristics in log and linear scale. (d) Normalized C-V characteristics of the p-H ISFET.

The interface trap density ( $N_{it}$ ) at the Si/parylene-H interface was extracted by the following equation [15]:

$$N_{it} = \left[ \left( \frac{SS}{\ln 10} \right) \left( \frac{q}{kT} \right) - 1 \right] \cdot \frac{C_i}{q}, \quad (1)$$

where  $q$  is the electron charge,  $k$  is the Boltzmann constant,  $T$  is the absolute temperature and  $C_i$  is the capacitance of the gate insulator per unit area. The  $N_{it}$  of p-H ISFET was estimated to be as low as  $\sim 1.04 \times 10^{12} \text{ cm}^{-2}$ . The field-effect mobility ( $\mu_{FE}$ ) in the linear region was also extracted based on the following equation [15]:

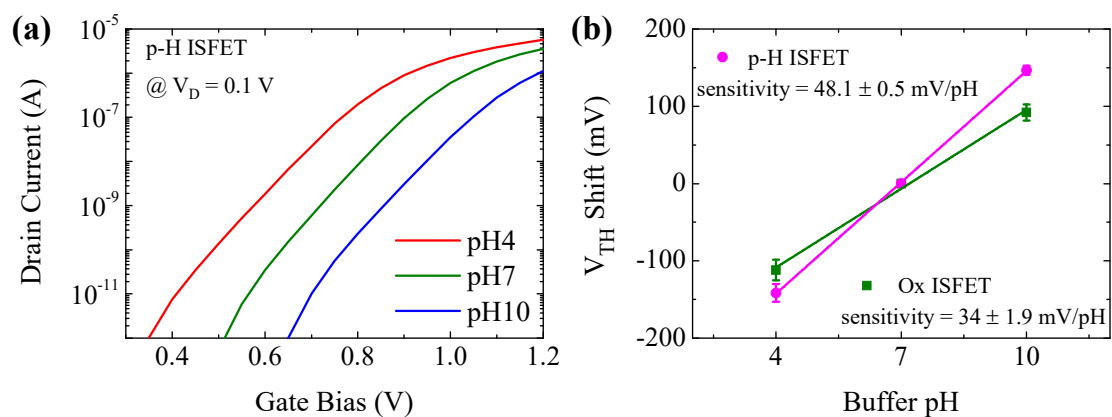
$$\mu_{FE} = \frac{L \cdot g_{m,\max}}{W \cdot C_i \cdot V_D}, \quad (2)$$

where  $L$  is the channel length,  $W$  is the channel width and  $g_{m,\max}$  is the maximum transconductance. The extracted  $\mu_{FE}$  of our p-H ISFETs reached as high as  $\sim 510 \text{ cm}^2 \text{ V}^{-1} \text{ s}^{-1}$ .

### 3.2. Sensitivity of p-H ISFETs

To evaluate the pH sensor response of the p-H ISFETs for potential bioassay applications, the output characteristics were measured at pH = 4, 7 and 10 buffer solutions by sweeping  $V_G$  from 0.3–1.2 V at constant  $V_D = 0.1$  V. Figure 3a shows the  $I_D$ - $V_G$  curve shifts as a function of pH value in the buffer solution. Figure 3b shows the change of  $V_{TH}$  of the p-H ISFETs measured in different pH solutions. The calculated pH sensitivity ( $S_{pH}$ ) was as high as  $48.1 \pm 0.5 \text{ mV/pH}$ , which is  $\sim 40\%$  higher than that of ISFETs with  $\text{SiO}_2$  gate insulator (Ox ISFET). The device-to-device variation was as low as  $\sim 6.1\%$ . The pH sensitivity of ISFETs with a bare  $\text{SiO}_2$  membrane was reported to be  $34 \text{ mV/pH}$  and

can increase up to 45 mV/pH with surface modification by functional molecules [16]. The parylene-H layer deposition process can simply control the formyl group concentration without additional surface modification. Our p-H ISFETs without any surface modification was comparable or even superior to other Si NW-based sensor platforms (see Table 1) reported in the literature [3,16–18]. The high sensitivity of p-H ISFETs is attributed to the formation of a high density formyl group (H-C=O) at the surface of the parylene-H/electrolyte, which can release or capture H<sup>+</sup> [9,19]. Formyl groups can have polarity due to the difference in electro negativity, and protons can attach to carbon by electrostatic interaction. The p-H ISFETs have higher pH sensitivity than Ox ISFETs due to the higher density of hydrogen ions at the gate insulator/electrolyte interface, which contribute to inducing carrier generation in the ISFET channel.



**Figure 3.** pH-dependent field-effect characteristics. (a)  $I_D$ - $V_G$  transfer characteristics at  $V_D = 0.1$  V in pH 4, 7, 10 buffer solutions for a p-H ISFET. (b)  $V_{TH}$  shift indicating a linear pH response: the sensitivity of  $48.1 \pm 0.5$  mV/pH and device-to-device variation of  $\sim 6.1\%$  for p-H ISFETs; the sensitivity of  $34 \pm 1.9$  mV/pH for Ox ISFETs.

**Table 1.** Comparison of the characteristics of Si nanostructure-based ISFETs.

Gate Insulator and Sensing Membrane	Device Channel	SS (mV/dec)	On/Off Ratio	Surface Treatment	pH Sensitivity (mV/pH)	Ref.
parylene-H	Si Nanonet	$\sim 85$	$>10^7$	w/o <sup>1</sup>	$48.1 \pm 0.5$	This work
SiO <sub>2</sub>	Si Nanonet	$\sim 63$	$>10^7$	w/o	35	[5]
SiO <sub>2</sub>	Si NW	/	/	w/o	$34 \pm 2$	[16]
SiO <sub>2</sub>	Si NW	/	/	w <sup>2</sup>	$45 \pm 0.3$	[16]
SiO <sub>2</sub>	Si NW	$\sim 600$	$>10^5$	w	$48 \pm 1$	[17]
SiO <sub>2</sub>	Si NW	$\sim 150$	$>10^5$	w	$43 \pm 3$	[3]
Ta <sub>2</sub> O <sub>5</sub>	Si NW	$\sim 300$	$>10^3$	w	$51.8 \pm 0.1$	[18]

<sup>1</sup> w/o—without; <sup>2</sup> w—with.

### 3.3. Noise Analysis of p-H ISFETs

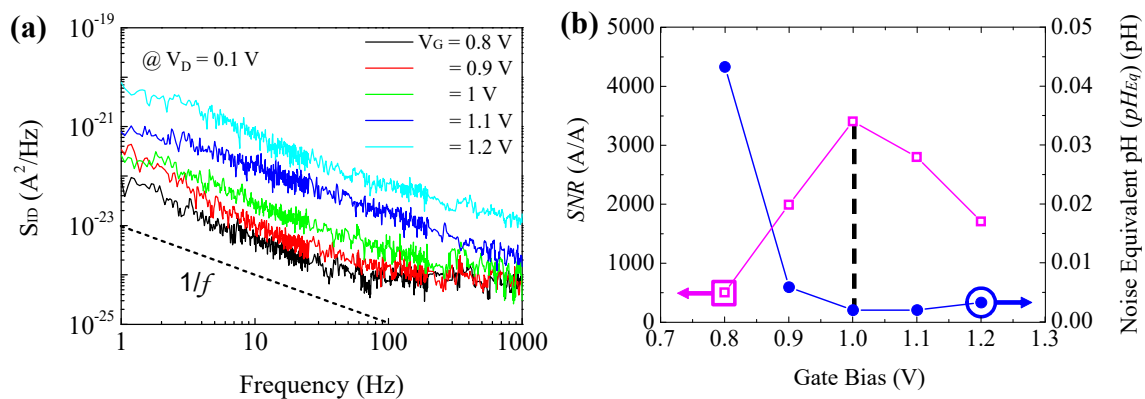
Noise is another important characteristic because it can fundamentally limit the sensitivity and resolution of the p-H ISFETs. The low frequency noise measurements of our p-H ISFETs were performed in pH = 7 buffer solution under various gate bias conditions. Figure 4a shows the drain current noise spectra  $S_{ID}$  vs. frequency at  $V_G = 0.8$ – $1.2$  V in steps of 0.1 V with constant  $V_D = 0.1$  V. The  $S_{ID}$  shows a typical  $1/f^\alpha$  behavior with the exponential slope  $\alpha \sim 1$  in a 3-dec frequency bandwidth of  $f_1 \sim f_2 = 1$ – $1000$  Hz. The signal to noise ratio (SNR) of our p-H ISFET was extracted based on the following equation [20]:

$$SNR = \Delta I / \sqrt{\int_{f_1}^{f_2} S_{ID}(f) df}, \quad (3)$$

where  $\Delta I$  is the drain current change in the range of pH = 4–10. The noise equivalent pH ( $pH_{Eq}$ ) of our p-H ISFETs as determined by  $SNR$  and sensitivity was evaluated using the following equation [21] with  $SNR = 1$ ,

$$pH_{Eq} = \sqrt{\int_{f_2}^{f_1} S_{ID}(f) df} / (g_m S_{pH}), \quad (4)$$

where  $g_m$  is the transconductance. The extracted  $SNR$  and  $pH_{Eq}$  are shown as a function of gate bias in Figure 4b. The highest  $SNR$  of ~3400 A/A and the lowest  $pH_{Eq}$  of ~0.002 pH were obtained at  $V_G = 1$  V for our p-H ISFETs, clearly indicating that the p-H ISFETs should be operated at near threshold voltage.



**Figure 4.** (a) Low frequency drain current noise characteristics of the p-H ISFET at various gate biases at  $V_D = 0.1$  V. (b)  $SNR$  and noise equivalent pH vs. gate bias.

#### 4. Conclusions

In conclusion, we proposed a p-H ISFET with a parylene-H sensing nanolayer. The excellent electrical properties of our p-H ISFETs such as subthreshold swing, threshold voltage, drain current on/off ratio and gate leakage current have been characterized. The low Si/parylene-H interface trap density and high field-effect mobility demonstrated the excellent electrical performance of our devices. In addition, it was demonstrated that the highly sensitive pH-dependent behaviors of p-H ISFETs exhibited pH sensitivity as high as  $48.1 \pm 0.5$  mV/pH, which is ~40% higher than that of the conventional  $SiO_2$  gate insulator-based ISFETs. Furthermore, in accordance with the low frequency noise analysis, the  $SNR$  and noise equivalent pH of p-H ISFETs were investigated for potential development in ISFET-based biosensor applications. Future work will address p-H ISFETs for use in various biomarker sensing.

**Author Contributions:** Conceptualization, methodology, formal analysis, investigation, writing, original draft preparation and visualization, B.J., G.-Y.L. and C.P.; resources and validation, B.J., G.-Y.L., C.P., D.K. and W.C.; writing, review and editing, B.J., G.-Y.L., C.P., J.-S.L. and J.-C.P.; supervision, J.-S.L. and J.-C.P.; project administration, J.-W.Y.; funding acquisition, J.-S.L., J.-C.P. and J.-W.Y.

**Funding:** This work was supported by Nano Convergence Foundation ([www.nanotech2020.org](http://www.nanotech2020.org)) funded by the Ministry of Science, ICT and Future Planning (Korea) and the Ministry of Trade, Industry and Energy (MOTIE, Korea) (Commercialization of Si nano nanonet FET biosensor for influenza diagnostic), by the Nano Material Technology Development Program through the National Research Foundation of Korea (NRF) funded by the Ministry of Science, ICT and Future Planning (2009-0082580) and by Korea Institute of Planning and Evaluation for

Technology in Food, Agriculture, Forestry and Fisheries(IPET) through Animal Disease Management Technology Development Program, funded by Ministry of Agriculture, Food and Rural Affairs(MAFRA)(grant no.116167-3).

**Conflicts of Interest:** The authors declare no conflict of interest.

## References

1. Justino, C.I.L.; Rocha-Santos, T.A.P.; Duarte, A.C.; Rocha-Santos, T.A.P. Advances in point-of-care technologies with biosensors based on carbon nanotubes. *TrAC Trends Anal. Chem.* **2013**, *45*, 24–36. [[CrossRef](#)]
2. Balasubramanian, K.; Kern, K. 25th Anniversary Article: Label-Free Electrical Biodetection Using Carbon Nanostructures. *Adv. Mater.* **2014**, *26*, 1154–1175. [[CrossRef](#)] [[PubMed](#)]
3. Rani, D.; Pachauri, V.; Mueller, A.; Vu, X.T.; Nguyen, T.C.; Ingebrandt, S. On the Use of Scalable NanoISFET Arrays of Silicon with Highly Reproducible Sensor Performance for Biosensor Applications. *ACS Omega* **2016**, *1*, 84–92. [[CrossRef](#)] [[PubMed](#)]
4. Rim, T.; Kim, K.; Kim, S.; Baek, C.-K.; Meyyappan, M.; Jeong, Y.-H.; Lee, J.-S. Improved Electrical Characteristics of Honeycomb Nanowire ISFETs. *IEEE Electron Device Lett.* **2013**, *34*, 1059–1061. [[CrossRef](#)]
5. Kim, K.; Rim, T.; Park, C.; Kim, D.; Meyyappan, M.; Lee, J.-S. Suspended honeycomb nanowire ISFETs for improved stiction-free performance. *Nanotechnology* **2014**, *25*, 345501. [[CrossRef](#)] [[PubMed](#)]
6. Kao, C.-H.; Chang, C.L.; Su, W.M.; Chen, Y.T.; Lu, C.C.; Lee, Y.S.; Hong, C.H.; Lin, C.-Y.; Chen, H. Magnesium Oxide (MgO) pH-sensitive Sensing Membrane in Electrolyte-Insulator-Semiconductor Structures with CF<sub>4</sub> Plasma Treatment. *Sci. Rep.* **2017**, *7*, 7185. [[CrossRef](#)] [[PubMed](#)]
7. Kao, C.-H.; Chang, C.-W.; Tzu Chen, Y.; Ming Su, W.; Cheng Lu, C.; Lin, C.-Y.; Chen, H. Influence of NH<sub>3</sub> plasma and Ti doping on pH-sensitive CeO<sub>2</sub> electrolyte-insulator-semiconductor biosensors. *Sci. Rep.* **2017**, *7*, 2405. [[CrossRef](#)] [[PubMed](#)]
8. Trantidou, T.; Payne, D.J.; Tsiligiridis, V.; Chang, Y.-C.; Toumazou, C.; Prodromakis, T. The dual role of Parylene C in chemical sensing: Acting as an encapsulant and as a sensing membrane for pH monitoring applications. *Sens. Actuators B* **2013**, *186*, 1–8. [[CrossRef](#)]
9. Ko, H.; Lee, E.-H.; Lee, G.-Y.; Kim, J.; Jeon, B.-J.; Kim, M.-H.; Pyun, J.-C. One step immobilization of peptides and proteins by using modified parylene with formyl groups. *Biosens. Bioelectron.* **2011**, *30*, 56–60. [[CrossRef](#)] [[PubMed](#)]
10. Ko, H.; Lee, G.-Y.; Jeon, B.-J.; Pyun, J.-C. Fluorescence immunoassay of anti-cyclic citrulinated peptide (CCP) autoantibodies by using parylene-H film. *BioChip J.* **2011**, *5*, 242. [[CrossRef](#)]
11. Jeon, B.-J.; Kim, M.-H.; Pyun, J.-C. Application of a functionalized parylene film as a linker layer of SPR biosensor. *Sens. Actuators B* **2011**, *154*, 89–95. [[CrossRef](#)]
12. Jeon, B.-J.; Kim, M.-H.; Pyun, J.-C. Parylene-A coated microplate for covalent immobilization of proteins and peptides. *J. Immunol. Methods* **2010**, *353*, 44–48. [[CrossRef](#)] [[PubMed](#)]
13. Alam, M.A.; Weir, B.E.; Silverman, P.J. A study of soft and hard breakdown—Part I: Analysis of statistical percolation conductance. *IEEE Trans. Electron Devices* **2002**, *49*, 232–238. [[CrossRef](#)]
14. Kahouli, A. Effect of film thickness on structural, morphology, dielectric and electrical properties of parylene C films. *Br. J. Appl. Phys.* **2012**, *112*, 064103. [[CrossRef](#)]
15. Junyoung, L.; Hojoon, L.; Bo, J.; Hyeongwan, O.; Sangwon, B.; Gilsang, Y.; Yongsu, L.; Rock-Hyun, B.; Jeong-Soo, L. Impact of geometrical parameters on the electrical performance of network-channel polycrystalline silicon thin-film transistors. *Jpn. J. Appl. Phys.* **2018**, *57*, 104001.
16. Nguyen, T.C.; Schwartz, M.; Vu, X.T.; Blinn, J.; Ingebrandt, S. Handheld readout system for field-effect transistor biosensor arrays for label-free detection of biomolecules. *Phys. Status Solidi A* **2015**, *212*, 1313–1319. [[CrossRef](#)]
17. Tran, D.P.; Wolfrum, B.; Stockmann, R.; Pai, J.-H.; Pourhassan-Moghaddam, M.; Offenhäusser, A.; Thierry, B. Complementary Metal Oxide Semiconductor Compatible Silicon Nanowires-on-a-Chip: Fabrication and Preclinical Validation for the Detection of a Cancer Prognostic Protein Marker in Serum. *Anal. Chem.* **2015**, *87*, 1662–1668. [[CrossRef](#)] [[PubMed](#)]
18. Lue, C.-E.; Yu, T.-C.; Yang, C.-M.; Pijanowska, D.G.; Lai, C.-S. Optimization of Urea-EnFET Based on Ta<sub>2</sub>O<sub>5</sub> Layer with Post Annealing. *Sensors* **2011**, *11*, 4562–4571. [[CrossRef](#)] [[PubMed](#)]

19. Trantidou, T.; Tariq, M.; Terracciano, C.M.; Toumazou, C.; Prodromakis, T. Parylene C-Based Flexible Electronics for pH Monitoring Applications. *Sensors* **2014**, *14*, 11629–11639. [[CrossRef](#)] [[PubMed](#)]
20. Haartman, M.V.; Ostling, M. *Low-Frequency Noise in Advanced MOS Devices*; Springer: Berlin/Heidelberg, Germany, 2007; p. 216.
21. Kim, S.; Rim, T.; Kim, K.; Lee, U.; Baek, E.; Lee, H.; Baek, C.-K.; Meyyappan, M.; Deen, M.J.; Lee, J.-S. Silicon nanowire ion sensitive field-effect transistor with integrated Ag/AgCl electrode: pH sensing and noise characteristics. *Analyst* **2011**, *136*, 5012–5016. [[CrossRef](#)] [[PubMed](#)]



© 2018 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<http://creativecommons.org/licenses/by/4.0/>).