



Clinical Study

Metabolic Volumetric Parameters in ^{11}C -Choline PET/MR Are Superior PET Imaging Biomarkers for Primary High-Risk Prostate Cancer

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Purpose. Positron emission tomography/magnetic resonance imaging (PET/MRI) can facilitate the use of noninvasive imaging biomarkers in clinical prostate cancer staging. Although multiparametric MRI is a widely used technique, the clinical value of simultaneous PET imaging remains unclear. This study aimed at investigating this issue. **Methods.** Between January 2015 and December 2016, 31 high-risk prostate cancer patients underwent ^{11}C -choline PET/MRI for staging purposes. Clinical characteristics and imaging parameters, including the standardized uptake value (SUV) and metabolic volumetric parameters from PET imaging; apparent diffusion coefficient (ADC) values from diffusion-weighted imaging; and volume transfer rate constant (K_{trans}), reflux rate constant (K_{ep}), and initial area under curve (iAUC) in 60 seconds from dynamic contrast-enhanced (DCE) MRI were analyzed. **Results.** ^{11}C -Choline PET imaging parameters were significantly correlated with prostate-specific antigen (PSA) levels, and metabolic volumetric parameters, including metabolic tumor volume (MTV) and uptake volume product (UVP), showed significant correlations with other MRI parameters. In our cohort analysis, the PET/MRI parameters UVP/minimal ADC value (ADC_{min}) and kurtosis of K_{ep} (K_{ep_{kur}})/ADC_{min} were significant predictors for progression-free survival (PFS) (HR = 1.01, 95% CI: 1.00–1.02, *p* = 0.031 and HR = 1.09, 95% CI: 1.02–1.16, *p* = 0.009, respectively) in multivariate Cox regression analysis. High UVP/ADC_{min} and K_{ep_{kur}}/ADC_{min} values were significantly associated with shorter PFS. **Conclusions.** Metabolic volumetric parameters such as MTV and UVP can be routinely used as PET imaging biomarkers to add prognostic value and show better correlations in combination with MR imaging parameters in high-risk prostate cancer patients undergoing ^{11}C -choline PET/MRI.

1. Introduction

Prostate cancer (PCa) is the leading cause of cancer-related death among men in Taiwan, with its incidence increasing rapidly from 26.22 per 100,000 males in 2002 to 47.86 per 100,000 males in 2012 [1]. The conventional imaging

modalities used to assess PCa include computed tomography (CT), magnetic resonance imaging (MRI), transrectal ultrasound (TRUS), and bone scintigraphy. However, simultaneous positron emission tomography (PET)/MRI has great potential to enhance clinical practice in these cases by combining functional, molecular, and anatomic information [2].

Although ^{11}C -choline has been approved for patients with suspected PCa recurrence by the U.S. FDA, the combination of ^{11}C -choline and MRI may also be effective for staging, especially in patients with a high Gleason score, advanced clinical stage, and elevated prostate-specific antigen (PSA) levels [3, 4].

Biomarkers derived from medical images offer several advantages, including ready availability, noninvasiveness, and serial patient monitoring [5]. The apparent diffusion coefficient (ADC) in diffusion-weighted MRI and the standardized uptake value (SUV) in PET have been used together as an imaging biomarker in several previous studies [6–8]. However, studies on the use of ^{11}C -choline PET metabolic volumetric parameters in combination with the SUV and ADCs and dynamic contrast-enhanced (DCE) parameters from multiparametric prostate MRI, which may theoretically maximize the value of simultaneous PET/MRI assessments, in cases of high-risk PCa are still lacking. Herein, we sought to identify clinically significant integrated ^{11}C -choline PET/MRI parameters for high-risk primary PCa by assessing the correlations of these parameters with clinical characteristics and progression-free survival (PFS).

2. Materials and Methods

2.1. Study Patients. This was a retrospective analysis of a prospective study. The study was approved by the hospital's institutional review board (approval numbers: 102-3271A and 201701793B0; ClinicalTrials.gov identifier: NCT02852122), and informed consent was obtained from all patients. Between January 2015 and December 2016, 54 consecutive patients with a clinical indication for PCa staging were scheduled to undergo an ^{11}C -choline PET/MRI examination, and a total of 31 patients were eventually assessed in this retrospective analysis. The study scheme is shown in Figure 1. All 31 patients had pathologically proven high-risk prostate cancer according to the D'Amico Risk Classification [9].

We recorded primary treatments (i.e., radical prostatectomy, hormone therapy, and radiation therapy plus hormone therapy) for prostate cancer in all 31 patients, and their follow-up status after treatments. The follow-up period was until June 2018. Disease progression after primary treatments was considered if the patients showed local or nodal relapse, new metastasis, or biochemical failure (a PSA value ≥ 0.2 ng/ml with a secondary confirmatory PSA value > 0.2 ng/ml after radical prostatectomy; PSA value > 2 ng/ml above nadir after radiation therapy without or with hormone therapy; or a continuous increase in PSA values after hormone therapy) [10–12]. The follow-up durations from diagnosis to disease progression or death/last visit of all patients were recorded.

2.2. ^{11}C -Choline PET/MRI Protocol. After fasting for at least 6 h, patients received a single intravenous bolus of 10–20 mCi (370–740 MBq) ^{11}C -choline; the mean dose was 16.5 ± 3.6 mCi. Approximately 5 min after ^{11}C -choline injection

and bladder evacuation, whole-body PET/MRI scanning was performed using an integrated PET/MRI system (Biograph mMR; Siemens Healthcare, Erlangen, Germany). PET scans were performed from the mid-thigh to the head in five bed positions (acquisition time, 3 min per position) with the patient in a supine arms-down position. Simultaneous MRI was performed with a transverse T2-weighted half-Fourier single-shot TSE (turbo spin-echo) sequence (1,000 ms repetition time (TR)/84 ms echo time (TE), 6 mm slice thickness, 320×256 matrix, and 380×309 mm² field of view (FOV)) and a coronal T1-weighted TSE sequence (500 ms TR/9.5 ms TE, 5 mm slice thickness, 1.5 mm intersection gap, 384×276 matrix, and 450×310 mm² FOV), while acquiring PET data in each bed position.

The simultaneous whole-body PET/MRI acquisition was followed by pelvic PET/MRI scans (Figure 2) involving a pelvic PET scan in one bed position (emission period, 15 min). The MRI pulse sequences included a sagittal T2-weighted TSE sequence (4,000 ms TR/91 ms TE, 4 mm slice thickness, 320×224 matrix, and 200×200 mm² FOV), coronal T2-weighted TSE sequence (4,000 ms TR/80 ms TE, 4 mm slice thickness, 0.4 mm intersection gap, 256×179 matrix, and 180×177 mm² FOV), and transverse T2-weighted TSE sequence (3,600 ms TR/80 ms TE, 4 mm slice thickness, 0.4 mm intersection gap, 256×179 matrix, and 180×177 mm² FOV), and acquisitions were performed in the pelvic region. Axial diffusion-weighted imaging (DWI) was performed using a single-shot spin-echo echo-planar imaging technique under free-breathing conditions (5,000 ms TR/65 ms TE, b values of 50 and 1000 s/mm², 4 mm slice thickness, 106×106 matrix, 260×205 mm² FOV, and NEX 6). Axial DCE-MRI was performed using a 3D T1-weighted spoiled gradient-echo sequence (3.91 ms TR/1.6 ms TE, 4 mm slice thickness, 128×128 matrix, 256×200 mm² FOV, and 13°FA). A total of 72 volumes were acquired with a temporal resolution of 4.16 seconds and acquisition time of 5 minutes. After four acquisitions of dynamic baseline scanning, a standard dose (0.1 mmol/kg body weight) of gadopentetate dimeglumine (Gd-DTPA; magnevist; Bayer-Schering, Burgess Hill, UK) was administered by a power injector through a cannula placed in the antecubital vein at a rate of 3 mL/s and immediately followed by a saline flush.

Attenuation correction of the PET data was performed using a four-tissue (air, lung, fat, and soft tissue) segmented attenuation map acquired with a two-point Dixon MRI sequence. Images were reconstructed using a high-definition PET (HD-PET) iterative algorithm (three iterations; 21 subsets) with a 5.4 mm post-reconstruction Gaussian filter and an image matrix of 344×344 .

2.3. PET Imaging Parameter Analysis. The PMOD 3.3 software package (PMOD Technologies Ltd., Zurich, Switzerland) was used for tumor segmentation. A volume of interest was manually drawn around the PCa lesion using an SUV cutoff of 2.5 in accordance with previous studies [13, 14]. PET imaging features were calculated in an SUV analysis. The maximum SUV (SUV_{max}), mean SUV

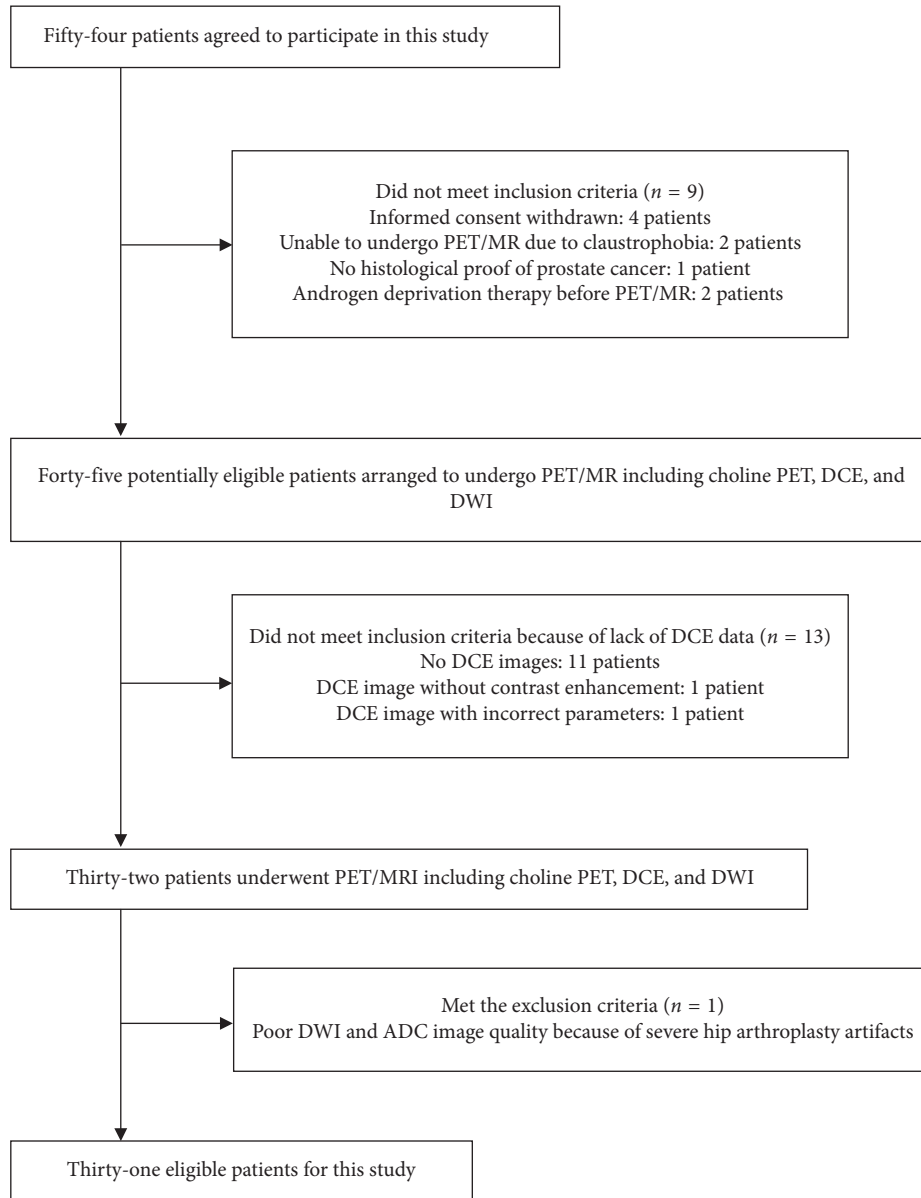


FIGURE 1: Flow diagram of the 31 patients eligible for this study.

(SUV_{mean}), metabolic tumor volume (MTV), and uptake volume product (UVP) were derived according to the following equations: $SUV = (\text{tissue radioactivity}/\text{tissue weight (g)})/(\text{total radioactivity (Bq)}/\text{body weight (g)})$ and $UVP = SUV_{mean} \times MTV$. Computations for imaging features were performed using the CGITA (Chang Gung Image Texture Analysis) toolbox implemented using MATLAB 2012a (MathWorks, Inc., Natick, MA, USA) [15].

2.4. MR Imaging Parameter Analysis. Postprocessing for DWI and DCE-MRI was performed using the software integral to the MRI unit (Siemens Syngo Via and Tissue 4D; software version, VA20B). The ADC was calculated from the diffusion-weighted images. The Toft model [16] was used for pharmacokinetic analysis to derive the following parameters from the DCE-MRI data: the volume transfer

rate constant (K_{trans}), reflux rate constant (K_{ep}), and initial area under curve (iAUC) in 60 seconds. The ADC- and the DCE-MRI-derived parameter maps were reconstructed on a pixel-by-pixel basis. On axial DCE images, an urologist with over 20 years of experience manually drew the largest region of interest (ROI) within each primary tumor on each image (Figure 3). ROIs on axial ADC images were obtained using a similar approach with the aid of diffusion-weighted images. The histogram data of the derived parameters from the ROIs—including maximal value and kurtosis of K_{trans} ($K_{trans,max}$ and $K_{trans,kur}$), K_{ep} ($K_{ep,max}$ and $K_{ep,kur}$), and iAUC ($iAUC_{max}$ and $iAUC_{kur}$)—and the minimal value, mean value, and kurtosis of ADC (ADC_{min} , ADC_{mean} , and ADC_{kur}) were exported for statistical analysis using a homemade software written in MATLAB (R2015b; MathWorks, Inc., Natick, MA, USA).

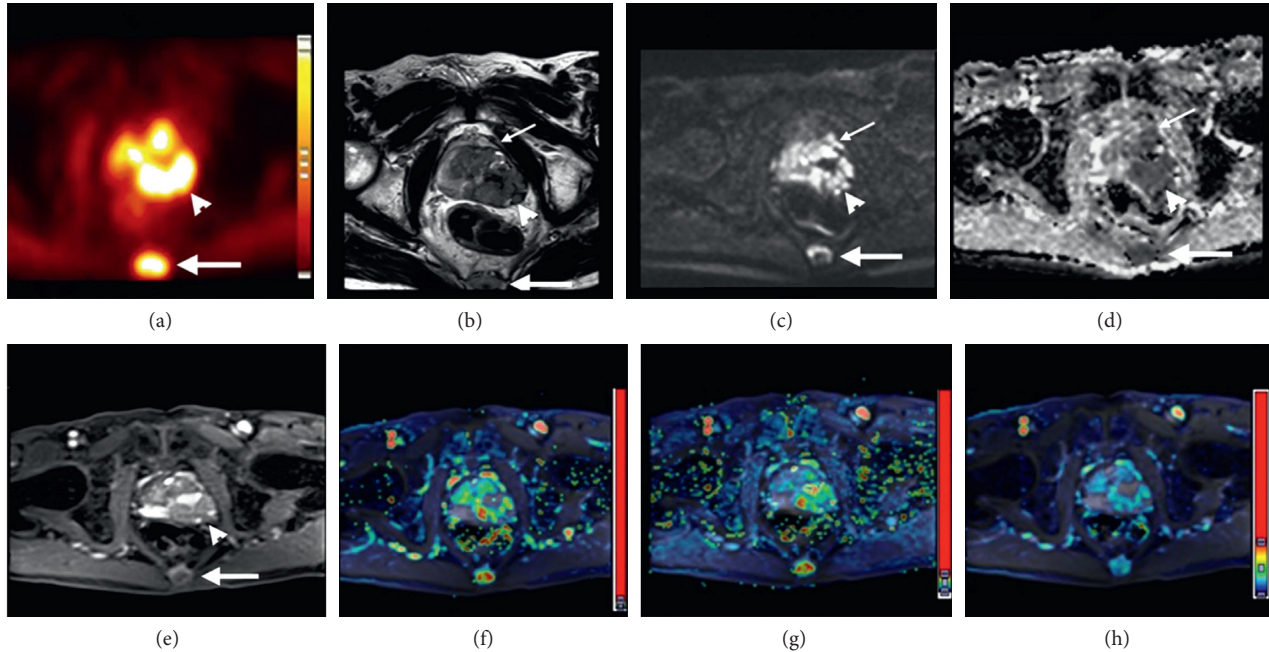


FIGURE 2: Simultaneous ^{11}C -choline PET/MRI images of the prostate region of a 74-year-old man with prostate cancer. (a) PET, (b) T2WI, (c) DWI, $b=1000$, (d) ADC, (e) DCE, (f) Ktrans, (g) Kep, and (h) iAUC maps derived from DCE showing tumor invasion of the left levator ani muscle (small arrows) and left gross extracapsular extension (arrowheads) by the primary tumor and bone metastasis at the sacrum (large arrows). Liver metastasis is also depicted on PET/MRI (not shown), and the clinical stage is T4N0M1c. Histological examination of the patient's biopsy specimens revealed a Gleason score of 8 and a prostate-specific antigen level of 591.9 ng/ml before PET/MRI.

2.5. Statistical Analysis. Descriptive statistics were calculated to summarize the data, using the median (range) for continuous variables and count (percentage of total) for categorical variables. Intergroup comparisons of continuous variables were based on the Mann–Whitney U-test. Correlations among study variables were investigated using the Spearman's correlation method. PFS was defined as the interval between diagnosis and disease progression. Univariate and stepwise multivariate Cox regression analyses based on the forward Wald method, with thresholds of 0.05 and 0.1, respectively, for entering and removing variables, were performed to identify predictors significantly associated with PFS. Two-sided p values less than 0.05 were considered statistically significant.

3. Results

3.1. Patient Clinical Characteristics. The clinical characteristics and PET/MR imaging parameters are listed in Table 1. More than half of the patients were aged ≥ 70 years. PSA values of 20–50 ng/ml and Gleason scores of 7 were the most common. Clinical T4 tumors were present in more than half of the patients. The majority of patients had clinical stage IV disease, and hypertension was the most common comorbidity.

3.2. Correlations among PET/MR Parameters, PSA Levels, and Gleason Scores. Table 2 shows the correlations between PET and MRI parameters. Among the PET imaging parameters, MTV and UVP more frequently showed

significant correlations with DCE and ADC parameters. MTV was significantly correlated with $\text{Ktrans}_{\text{max}}$, Kep_{max} , Kep_{kur} , iAUC_{max} , and iAUC_{kur} ($\sigma = 0.39\text{--}0.51$, all $p < 0.05$), whereas UVP was significantly correlated with $\text{Ktrans}_{\text{max}}$, iAUC_{max} , and iAUC_{kur} ($\sigma = 0.37\text{--}0.51$, all $p < 0.05$). SUV_{max} showed moderate and significant correlation with iAUC_{max} . Other SUV and DCE parameters showed no significant correlations. Both MTV and UVP were negatively correlated with ADC_{min} and positively correlated with ADC_{kur} . Other SUV and ADC parameters showed no significant correlations. There were no significant correlations between DCE and ADC parameters, except between $\text{Ktrans}_{\text{max}}$ and ADC_{kur} ($\sigma = 0.37$, $p < 0.05$).

PSA levels were positively correlated with PET imaging parameters, including SUV_{max} , SUV_{mean} , UVP, and MTV, and negatively correlated with ADC_{min} and ADC_{mean} of MRI. Gleason scores showed positive and significant correlations with both Kep_{kur} and iAUC_{kur} .

3.3. PET/MR Imaging Parameters Stratified by Clinical Characteristics. The relevant intergroup comparisons of imaging parameters are shown in supplementary Tables S1–S3. All PET parameters but none of the MRI parameters were associated with $\text{PSA} \geq 20$ ng/ml (all $p < 0.05$). Three MRI parameters (Kep_{kur} , iAUC_{kur} , and ADC_{mean}) were associated with Gleason scores of 8–10 (all $p < 0.05$). Multiple PET/MRI parameters were associated with the disease stage T3–4, including MTV and UVP from PET, $\text{Ktrans}_{\text{max}}$ and Kep_{max} from DCE-MRI and ADC_{min} and ADC_{kur} from ADC assessments in MRI (all $p < 0.05$). In contrast, none of the

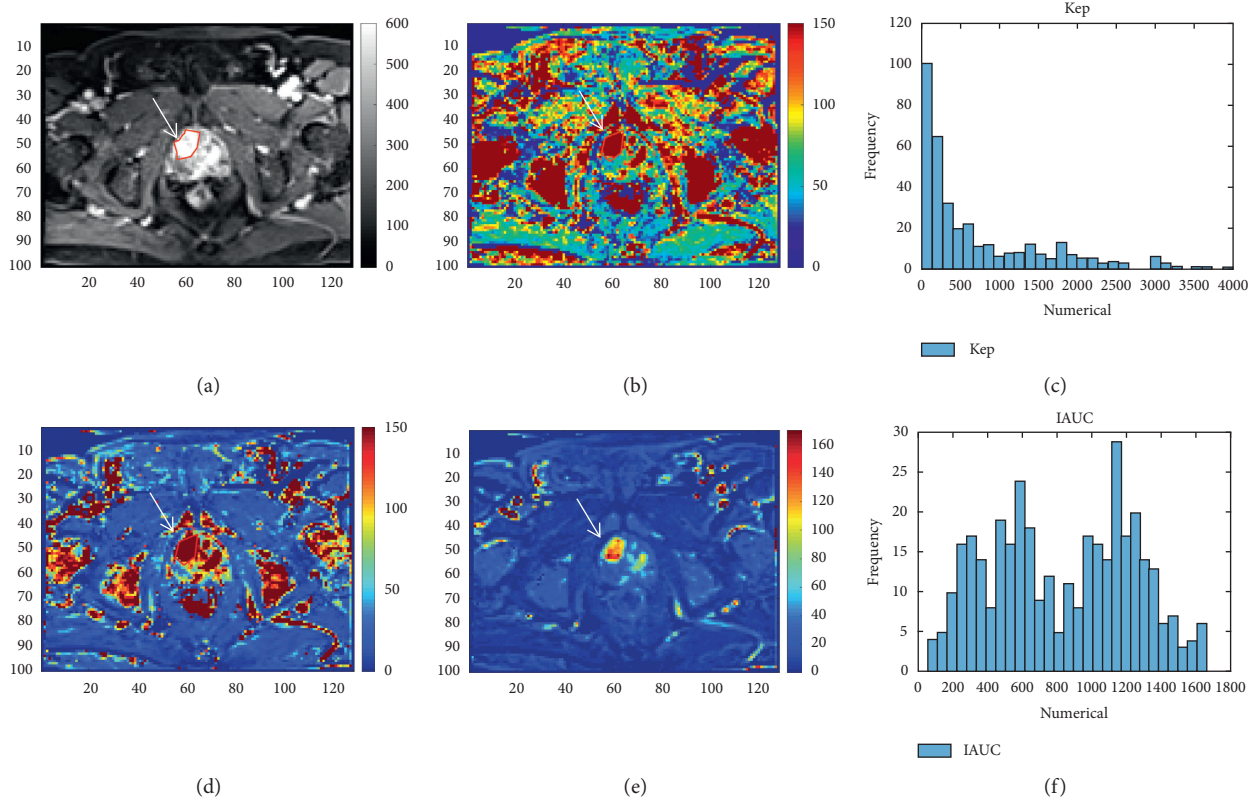


FIGURE 3: A DCE image and its derived parameter maps at the prostate region of a 76-year-old man who underwent simultaneous ¹¹C-choline PET/MRI and had a prostate-specific antigen level of 76.6 ng/ml. A region of interest (ROI) was drawn in the cancer localized at the right lobe of the prostate gland (arrows) to obtain ROI histograms on DCE parameter maps. The $K_{trans,max}$, $K_{trans,kur}$, Kep_{max} , Kep_{kur} , $iAUC_{max}$, and $iAUC_{kur}$ values for prostate cancers in this patient were 3993.0/min, 3.34, 4000.0/min, 4.46, 1716.0, and 1.66, respectively. (a) DCE. (b) K_{trans} . (c) Kep histogram. (d) Kep . (e) $iAUC$. (f) $iAUC$ histogram.

PET/MRI parameters showed significant differences between patients without and with regional lymph node metastasis. Similarly, many PET/MRI parameters (i.e., MTV, UVP, $iAUC_{kur}$, and ADC_{min}) showed associations with both distant metastasis and stage IV disease (all $p < 0.05$). SUV_{max} was also associated with distant metastasis, and ADC_{mean} with comorbidities (both $p < 0.05$).

3.4. Patients' Disease Progression Predictions by Imaging Parameters. Of the 31 patients, 4 were not treated at our hospital and 27 had undergone radical prostatectomy ($n = 6$), radiation therapy ($n = 2$), hormone therapy ($n = 11$), or radiation plus hormone therapies ($n = 8$). The 31 patients had a mean follow-up duration of 25.5 months (range: 7.7–39.0 months). Ten patients (38.5%) showed disease progression at a mean follow-up duration of 16.5 months after diagnosis. Twenty-eight patients (90.3%) were alive at the last visit, and three patients (9.7%) died of prostate cancer at 7.7, 12.0, and 14.0 months after diagnosis.

Univariate Cox regression analysis of solitary and hybrid imaging biomarkers showed that an increase in Kep_{max} , Kep_{kur} , MTV, UVP, MTV/ADC_{min} , UVP/ADC_{min} , Kep_{max}/ADC_{min} , and Kep_{kur}/ADC_{min} was significantly associated with a shorter PFS. Stepwise multivariate analysis showed that UVP/ADC_{min} (HR = 1.010, 95%

CI: 1.001–1.020, $p = 0.031$) and Kep_{kur}/ADC_{min} (HR = 1.087, 95% CI: 1.021–1.157, $p = 0.009$) were independent predictors of PFS (Table 3).

4. Discussion

Unlike biospecimen-based markers, imaging biomarkers undergo technical, biological, and clinical validation along with assessments of cost-effectiveness before they are routinely used in clinical settings. Although PET/MR offers robust data due to the high soft tissue contrast and the addition of multiparametric MRI improves its ability to evaluate prostate cancer in T-staging, the improvements offered by this approach in the detection of nodal disease or bone involvement appear uncertain [17, 18]. Metabolic volumetric PET parameters such as MTV and UVP are considered better than SUV because they provide more accurate PCa characterization [13]. Increased MTV and UVP values reflect the volume of viable tumor cells and high tissue metabolism. In the current study, we performed a comprehensive analysis of the correlations among imaging biomarkers as well as between imaging biomarkers and clinical parameters. The findings showed that MTV and UVP are significantly correlated with many DCE-MRI parameters, which provide tumor blood microcirculation-related information.

TABLE 1: Clinical characteristics and PET/MR imaging parameters for the patients.

Variables	Descriptive statistics
Age (years)	70 (52–84)
<60.0	2 (6.5%)
60.0–69.9	11 (35.5%)
70.0–79.9	17 (54.8%)
≥80	1 (3.2%)
PSA (ng/ml)	30.56 (4.5–591.9)
<10	2 (6.5%)
10.0–20.0	6 (19.4%)
20.1–50.0	11 (35.5%)
50.1–100.0	3 (9.7%)
>100.0	9 (29.0%)
Gleason score	8 (6–10)
6	5 (16.1%)
7	9 (29.0%)
8	8 (25.8%)
9	6 (19.4%)
10	3 (9.7%)
Primary T	
T2	4 (12.9%)
T3a	5 (16.1%)
T3b	6 (19.4%)
T4	16 (51.6%)
Regional lymph node metastasis	
No	17 (54.8%)
Yes	14 (45.2%)
Distant metastasis	
No	15 (48.4%)
Yes	16 (51.6%)*
Clinical stage	
IIB	2 (6.5%)
III	7 (22.6%)
IV	22 (71.0%)
PET parameters	
SUV _{max}	6.36 (4.30–19.43)
SUV _{mean}	3.63 (2.99–8.03)
MTV	14.42 (1.14–156.70)
UVP	54.97 (4.14–860.33)
MRI DCE parameters	
Ktrans _{max} (1/min)	310.00 (110.00–3993.00)
Ktrans _{kur}	3.38 (1.64–54.62)
KeP _{max} (1/min)	229.00 (66.00–4000.00)
KeP _{kur}	3.16 (1.73–1640.82)
iAUC _{max}	1140.00 (635.00–3398.00)
iAUC _{kur}	2.83 (1.64–11.32)
MRI ADC parameters	
ADC _{min} (μm ² /s)	17.00 (1.00–485.00)
ADC _{mean} (μm ² /s)	1002.78 (674.72–1357.42)
ADC _{kur} (μm ² /s)	3.17 (2.40–5.65)

Descriptive statistics are presented as either median (range) or *n* (%). * Five patients showed both nonregional lymph node and bone metastasis. PSA, prostate-specific antigen.

Ktrans has been used to quantitatively assess microvascular permeability; KeP reflects the rate of contrast agent transfer from the extravascular extracellular space back to the blood [16]; and iAUC represents the general tumor blood flow, overall perfusion, and tumor interstitial space index. These parameters are correlated with angiogenesis

[19, 20]. The correlations among these parameters are not surprising since primary tumors with higher T stages such as ≥T3 have higher MTV, UVP, Ktrans_{max}, and KeP_{max} values (Supplementary Tables S1 and S2). Furthermore, MTV and UVP values are also significantly correlated with ADC_{min}. ADC values reflect the degree of water restriction, and the increased cellularity of PCa increases water restriction and reduces ADC values. Similarly, patients with distant metastasis also have higher MTV and UVP values but lower ADC_{min} values (Supplementary Table S3). Thus, higher MTV and UVP values may reflect the tumor characteristics of high-risk PCa, not only the higher metabolic activity of larger viable tumors but also the higher angiogenesis and water restriction noted on MRI, and may be useful in categorizing PCa patients by indicating a high likelihood of a higher primary T stage and distant metastasis.

Several promising radiotracers—some of them targeting choline and prostate-specific membrane antigen (PSMA)—are currently being investigated for PET imaging of PCa [21]. An increased cellular membrane synthesis represents a biological substrate for PCa imaging. Specifically, choline enters the cell via the choline transporter, being further phosphorylated to phosphatidylcholine by choline kinase. Both of these molecules are upregulated in tumor cells, ultimately resulting in an enhanced choline uptake [22]. ¹¹C-Choline PET imaging parameters, including SUV_{max}, SUV_{mean}, MTV, and UVP, are significantly correlated with the PSA level, but none of them are correlated with the Gleason score. This may be because several benign entities, especially benign prostate hyperplasia, will also show increased ¹¹C-choline uptake [23]. In our data, KeP_{kur} and iAUC_{kur} were correlated with the Gleason score. Kurtosis, as a parameter of first-order histogram analysis, reflects the outliers of a probability distribution in the tail extremity and is considered to be related to tumor heterogeneity [24–26]. Prostate cancers typically have high Ktrans, KeP, and iAUC values on DCE-MRI, and both Ktrans and KeP affect iAUC since the iAUC reflects the overall blood volume of PCa in the initial 60 seconds [27]. The positive correlation of KeP_{kur} and iAUC_{kur} on DCE-MRI with the Gleason score implies that PCa with a more heterogeneous distribution of contrast back to the blood and overall blood volume is more likely to have higher Gleason scores. Thus, ¹¹C-choline PET/MRI, in combination with DCE-MRI parameters, provides additional information regarding tumor heterogeneity and Gleason scores of prostate cancers.

Consistently with a previous study conducted with ¹⁸F-choline [28], we failed to identify a significant inverse association between SUV and ADC values. In contrast, our cases showed a significant inverse correlation between ADC_{min} and UVP/MTV. Decreased ADC values indicate increased water restriction as a result of increased cellularity, and increased MTV and UVP values reflect the volume of viable tumor cells and high tissue metabolism. This correlation may be explained by the fact that histologic tumor volume is significantly associated with both ADC_{min} and metabolic volumetric parameters (as shown in a study conducted with ¹⁸F-choline) [13]. Combinations of PET and MRI parameters have been considered as imaging

TABLE 2: Correlation matrix of imaging biomarkers and clinical parameters.

	SUV _{max}	SUV _{mean}	UVP	MTV	Ktrans _{max}	Ktrans _{kur}	Kep _{max}	Kep _{kur}	iAUC _{max}	iAUC _{kur}	ADC _{min}	ADC _{mean}	ADC _{kur}	PSA	GS
SUV _{max}	1	0.90	0.69	0.59	0.35	0.15	0.18	-0.04	0.40	0.25	-0.04	-0.19	0.10	0.46	-0.31
		<0.01*	<0.01*	<0.01*	0.06	0.41	0.35	0.85	0.03*	0.18	0.82	0.31	0.60	0.01*	0.10
SUV _{mean}		1	0.56	0.42	0.19	0.06	-0.02	-0.19	0.28	0.25	0.09	-0.30	0.14	0.39	-0.33
			<0.01*	0.02*	0.30	0.76	0.92	0.31	0.13	0.17	0.64	0.10	0.47	0.03*	0.07
UVP			1	0.98	0.37	0.31	0.34	0.30	0.51	0.45	-0.41	-0.31	0.37	0.76	0.16
				<0.01*	0.04*	0.09	0.06	0.11	<0.01*	0.01*	0.02*	0.09	0.04*	<0.01*	0.40
MTV				1	0.39	0.25	0.41	0.40	0.51	0.48	-0.47	-0.28	0.40	0.75	0.25
					0.03*	0.17	0.02*	0.03*	<0.01*	0.01*	0.01*	0.12	0.03*	<0.01*	0.18
Ktrans _{max}					1	0.80	0.55	0.47	0.60	0.47	-0.24	0.02	0.37	0.18	0.04
						<0.01*	<0.01*	<0.01*	<0.01*	0.01*	0.20	0.93	0.04*	0.34	0.83
Ktrans _{kur}						1	0.74	0.71	0.34	0.78	0.01	-0.09	0.30	0.10	0.25
							<0.01*	<0.01*	0.07	<0.01*	0.95	0.64	0.10	0.58	0.17
Kep _{max}							1	0.80	0.50	0.47	-0.31	-0.04	0.21	0.15	0.21
								0.00*	0.00*	0.01*	0.09	0.84	0.26	0.41	0.25
Kep _{kur}								1	0.32	0.47	-0.26	-0.11	0.24	0.20	0.41
									0.09	0.01*	0.15	0.57	0.19	0.29	0.02*
iAUC _{max}									1	0.36	-0.25	-0.01	0.26	0.30	0.11
										0.046*	0.17	0.95	0.16	0.10	0.57
iAUC _{kur}										1	-0.08	-0.35	0.30	0.33	0.36
											0.68	0.05	0.10	0.07	0.049*
ADC _{min}											1	0.14	-0.08	-0.36	-0.33
												0.44	0.66	0.046*	0.07
ADC _{mean}												1	-0.20	-0.38	-0.22
													0.28	0.04*	0.23
ADC _{kur}													1	0.23	0.35
PSA														0.22	0.06
														1	0.17
GS															0.35
															1

*Statistically significant by Spearman's correlation method. PSA, prostate-specific antigen; GS, Gleason score.

TABLE 3: Univariate and multivariate Cox regression for progression-free survival (PFS).

	Univariate analysis				Multivariate analysis			
	HR	95% CI		<i>p</i> value	HR	95% CI		<i>p</i> value
		Lower	Upper			Lower	Upper	
MTV	1.02	1.00	1.03	0.014*	—	—	—	NS
UVP [†]	1.002	1.000013	1.0004	0.049*	—	—	—	NS
Kep _{max} [†]	1.00046	1.000013	1.0009	0.044*	—	—	—	NS
Kep _{kur}	1.02	1.00	1.03	0.019*	—	—	—	NS
1/ADC _{min}	12.52	0.87	180.41	0.063	—	—	—	NS
UVP/ADC _{min}	1.01	1.00	1.02	0.007*	1.01	1.00	1.02	0.031*
MTV/ADC _{min}	1.09	1.03	1.14	0.001*	—	—	—	NS
Kep _{max} /ADC _{min} [†]	1.0035	1.001	1.006	0.002*	—	—	—	NS
Kep _{kur} /ADC _{min}	1.09	1.03	1.15	0.002*	1.09	1.02	1.16	0.009*

[†]Data are expressed as exact numbers; * *p* value <0.05; NS, not significant.

biomarkers with the prognostic value in many studies. In one study, the MTV/ADC_{min} ratio was found to be an independent predictor of PFS in pancreatic cancer [29]. Another study demonstrated that percentage changes in SUV_{max}/ADC_{min} and tumor lesion glycolysis (TLG)/ADC_{min} can predict treatment response to neoadjuvant chemotherapy (NAC) early in the course of breast cancer treatment [30]. Since multiparametric MRI is a routine clinical tool for prostate cancer diagnosis, the possible prognostic predictive value of PET/MR must be considered. In our study, both UVP/ADC_{min} and MTV/ADC_{min} ratio were significant predictors for disease progression in univariate analysis, and UVP/ADC_{min} was a significant predictor for disease progression in multivariate analysis as Kep_{kur}/ADC_{min} (Figure S1).

Our findings need to be interpreted within the context of some limitations. First, most high-risk PCa patients did not undergo prostatectomy, and the number of patients with surgical specimens was small. Although Gleason scores from TRUS biopsies are acceptably accurate in predicting malignancy, 25%–30% of cases may show discrepancies [31]. Second, the treatment was not standardized in all patients. Third, the follow-up durations were relatively short (mean follow-up duration, 25.5 months). These limitations present some uncertainties for the correlation between imaging parameters and biospecimen-based markers and the prognostic significance. However, our study also has several strengths. First, it was the ¹¹C-choline PET/MR study focusing on the high-risk PCa staging setting. Second, comprehensive imaging analysis, including PET, DWI, and DCE-MRI, was performed. Third, our data suggested that metabolic volumetric PET parameters, including MTV and UVP, are superior to SUV, show significant correlations with ADC and DCE values, and have prognostic value when combined with ADC_{min}.

5. Conclusion

The metabolic information provided by ¹¹C-choline PET imaging in integrated PET/MR scans shows significant correlations with the PSA level. Metabolic volumetric parameters such as MTV and UVP can serve as imaging biomarkers and show a prognostic value and may show

better correlations in combination with MR imaging parameters.

Data Availability

The data used to support the findings of this study are included within the article.

Conflicts of Interest

The authors declare that there are no conflicts of interest.

Authors' Contributions

Jing-Ren Tseng and Lan-Yan Yang contributed equally to this work.

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Supplementary Materials

Tables S1, S2, and S3 demonstrate the relationship between imaging parameters and clinical risk features in PET, DCE, and ADC, respectively. Figure S1 shows Kaplan–Meier plots of progression-free survival according to the hybrid imaging parameters (a) UVP/ADC_{min} and (b) Kep_{kur}/ADC_{min}. Comparisons were made with the log-rank test. Youden's index was used to determine the optimal cutoff values based on the area under the receiver operating characteristic curves for the events of interest. (*Supplementary Materials*)

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