BMJ Open Atrial fibrillation detection using single lead portable electrocardiographic monitoring: a systematic review and meta-analysis

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ABSTRACT

Objectives Recent technology advances have allowed for heart rhythm monitoring using single-lead ECG monitoring devices, which can be used for early diagnosis of atrial fibrillation (AF). We sought to investigate the AF detection rate using portable ECG devices compared with Holter monitoring.

Setting, participants and outcome measures We searched the Medline. Embase and Scopus databases (conducted on 8 May 2017) using search terms related to AF screening and included studies with adults aged >18 years using portable ECG devices or Holter monitoring for AF detection. We excluded studies using implantable loop recorders and pacemakers. Using a random-effects model we calculated the overall AF detection rate. Metaregression analysis was performed to explore potential sources for heterogeneity. Quality of reporting was assessed using the tool developed by Downs and Black. **Results** Portable ECG monitoring was used in 18 studies (n=117 436) and Holter monitoring was used in 36 studies (n=8498). The AF detection rate using portable ECG monitoring was 1.7% (95% Cl 1.4 to 2.1), with significant heterogeneity between studies (p<0.001). There was a moderate linear relationship between total monitoring time and AF detection rate (r=0.65, p=0.003), and metaregression identified total monitoring time (p=0.005) and body mass index (p=0.01) as potential contributors to heterogeneity. The detection rate (4.8%, 95% Cl 3.6% to 6.0%) in eight studies (n=10199), which performed multiple ECG recordings was comparable to that with 24 hours Holter (4.6%, 95% Cl 3.5% to 5.7%). Intermittent recordings for 19 min total produced similar AF detection to 24 hours Holter monitoring.

Conclusion Portable ECG devices may offer an efficient screening option for AF compared with 24 hours Holter monitoring.

PROSPERO registration number CRD42017061021.

Atrial fibrillation (AF) is a leading cause of stroke and heart failure worldwide, and is associated with increased all-cause mortality¹² as well as substantial financial cost.³⁴ The prevalence of AF increases with age, exceeding >15% for those aged 85 years and older.⁵ The epidemics of obesity, diabetes mellitus and

Strengths and limitations of this study

- First systematic review comparing single-lead ECG monitoring with 24 hours Holter monitoring for atrial fibrillation (AF) detection.
- Comprehensive literature search and specific inclusion criteria allowing for large patient numbers.
- Heterogeneity among individual studies with regard to patient population, AF definitions and monitoring time.
- Poor reporting of CHA₂DS₂-VASC scores among individual studies.
- Patient compliance unable to be accounted for in this meta-analysis.

metabolic syndrome have also been associated with the increasing prevalence of AF.^{6–8} Up to 20% of patients with stroke have underlying AF, and detection allows the initiation of anticoagulation, which is associated with a significant reduction in stroke recurrence.⁹

Early diagnosis of AF may have several benefits, including individualised lifestyle intervention¹⁰ and anticoagulation, and may be associated with a reduction in complications and healthcare costs. The importance of early diagnosis has been recognised in recent guidelines from the European Society of Cardiology, which recommended opportunistic screening using pulse palpation and 12-lead ECG.¹¹ However, screening for AF is challenging for several reasons; many patients are asymptomatic or may have atypical symptoms. There are a variety of monitoring techniques available, all of which vary in diagnostic accuracy and sensitivity, and there is no accepted reference standard. Subclinical AF is associated with an increased risk of stroke, cardiovascular disease and all-cause mortality,¹² although there is controversy surrounding the significance of brief paroxysms of AF and the potential benefit of

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anticoagulant therapy. Implantable devices are expensive, and not cost-effective for mass screening, and the use of external devices for long periods of monitoring require electrodes, which may be poorly tolerated by patients.

Recent advances in technology have allowed for the development of single-lead portable ECG monitoring devices. Multiple devices are available, all using multiple points of finger contact to create a single-lead ECG trace. The in-built memory of these devices allows for single or multiple time-point screening. Interpretation from a cardiologist or by automated algorithms has achieved high sensitivity and specificity for AF detection.^{13–15} Although they have not been incorporated into the latest AF guide-lines, the accuracy, ease of use and potential cost-effectiveness of these devices may lead to them having an important role in AF screening. This paper describes a systematic review of the published literature to investigate the overall AF detection rate using portable ECG devices compared with traditional Holter monitoring.

METHODS

Search strategy

We conducted our systematic review and meta-analysis using the Preferred Reporting Items for Systematic Reviews and Meta-Analyses guideline (PRISMA).¹⁶ We searched the Medline, Scopus and Embase databases using key terms including 'atrial fibrillation/AF and screening/monitoring and electrocardiographic/Holter monitoring', which were mapped to subject headings. We also searched the reference lists to identify other potential articles. The search was limited to adult human subjects aged >18 years and limited to the English language (see search strategy for Medline database in online supplementary material 1). The study was prospectively registered on the PROSPERO database on 22 April 2017 (CRD42017061021), and the search was conducted on 8 May 2017.

Study selection

Titles and abstracts of studies identified from the search were reviewed by two independent reviewers (SR and DDS). Studies which had a primary aim of AF detection in adult participants were included. We included all cohorts including community screening, those with risk factors and recent stroke. The screening methods included portable single-lead ECG devices or continuous (Holter) monitoring (up to 1week). We included studies which used single-lead ECG devices for single episode screening or multiple intermittent screening periods. We included conference abstracts if demographic and outcome data were available. We excluded studies if participants were aged <18 years or if other forms of monitoring were used (pacemaker, implantable loop recorders, event recorders, monitoring patches and inpatient telemetry). We also excluded studies where AF detection was not the primary aim.

The primary outcome of interest was the detection rate of new AF using either single-lead intermittent or continuous monitoring. Our secondary objective was to determine the optimal time of intermittent monitoring, which produced equivalent AF detection to continuous monitoring.

Data collection

Full-text manuscripts of studies fitting the inclusion criteria were obtained. Quality of reporting and risk of bias was assessed using the tool developed by Downs and Black.¹⁷ A standardised data-extraction form was used by the reviewers, which included information about the patient demographics, comorbidities, screening strategy, patients with known AF and overall new AF detection rate. Where data were not reported, we attempted to contact the primary authors of the study. Any disagreements between the two reviewers were resolved by consensus or by consulting a third reviewer (THM).

Statistical analysis

The cumulative AF detection rate for continuous and intermittent monitoring and the 95% CI was calculated using a random-effects model. The results were displayed as a forest plot and heterogeneity among the studies was assessed using the I^2 statistic. A subgroup analysis was performed by comparing the cumulative detection rate of single-lead ECG studies, which performed multiple timepoint recordings with 24 hours Holter monitoring studies. Linear regression analysis was used to determine the association between the total monitoring time and AF detection using single-lead ECG devices. This formula was used to determine the monitoring time using singlelead ECG devices to approximate the overall AF detection rate using 24 hours continuous monitoring. Univariate meta-regression analysis was performed to assess the influence of various clinical and screening factors with AF detection. Publication bias was assessed using a funnel plot and the Egger test. Statistical analysis was performed using Stata V.13 (StataCorp, College Station, Texas, USA) with two-tailed p values <0.05 used to denote statistical significance.

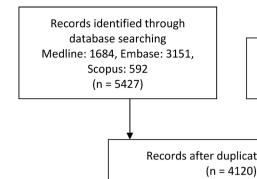
Patient and public involvement

Patients were not involved in this review.

RESULTS

Study characteristics

The PRISMA flow chart of our included studies is shown in figure 1 and the search strategy in online supplementary table 1. Our initial search strategy identified 5427 studies, with another 26 identified through other sources. After removing duplicate records, 4122 studies were left. After screening those using the inclusion/exclusion criteria, we identified 111 full-text studies for detailed review, which excluded 59 studies, leaving 52 full-text studies for inclusion in the meta-analysis (see online supplementary



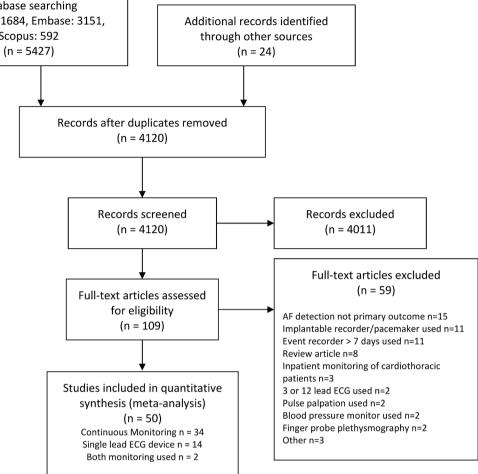


Figure 1 Overview of inclusion and exclusion of studies based on the Preferred Reporting Items for Systematic Reviews and Meta-Analyses flow chart.

table 2 for excluded studies). Of the 52 studies included, 34 used continuous (Holter) monitoring (n=8154),¹⁸⁻⁵¹ 16 studies (n=117092) used single-lead portable ECG monitoring^{14 15 52-65} and 2 studies (n=344) used both continuous and intermittent single-lead monitoring for AF detection in a head-to-head comparison.^{66 67}

The baseline characteristics of the individual studies is presented in table 1. There was a considerable range in age (54-76 years), and gender (male 29%-77%) between studies. As many studies chose healthy volunteers and other studies focused on patients poststroke or those with AF risk factors, there was significant variation in comorbidities such as diabetes, hypertension and obesity. Stroke risk determined by the CHADS or CHA₂DS₂-VASC score was reported in only 14/52 studies (27%). Of the 52 studies, 36 (69%) were conducted in Europe, 8 (15%) in Asia, 5 (10%) in North America and 3 (6%) in Australia. Nine studies (17%) were retrospective, the remainder all being prospective cohort or randomised controlled trials.

Of the 18 studies using single-lead ECG devices, 10 studies (56%) used a single 10-60s recording for AF detection while 8 studies (44%) used multiple readings over a 1-week to 52-week period. There were five portable

ECG devices used (table 1). Sixteen studies (89%) used healthy participants with risk factors.^{14 15 52-61 63-65 67} Two studies assessed patients following stroke or transient ischaemic attack (TIA).^{62 66}

Of the 36 studies using continuous (Holter) monitoring, 27 studies (75%) used 24 hours continuous monitoring, $^{18-23}$ $^{25-28}$ $^{33-36}$ 38 39 $^{41-45}$ $^{47-50}$ 66 67 4 studies (11%) used 1-week monitoring, $^{30-32}$ 51 2 studies (6%) used 48 hours monitoring, 37 46 2 studies (6%) used 72 hours monitoring^{24 29} and 1 study (3%) used 96 hours monitoring.40

Overall AF detection

The combined AF detection rate using single-lead ECG monitoring (n=117436 from 18 studies) was 1.7% (95%) CI 1.4% to 2.1%). The cumulative AF detection rate using continuous (Holter) monitoring (n=8498 from 36 studies) was 5.5% (95% CI 4.4% to 6.6%). There was significant heterogeneity between studies ($I^2=94\%$) for single-lead ECG monitoring, 87% for Holter monitoring). The overall new AF detection rate is presented in figure 2.

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Omron HeartScan HCG-801

Community heart rhythm screening programme through medical centres

Irregular RR intervals, absence of P waves and variable atrial cycle length (when visible)

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Zenicor

Sweden

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Hendrikx *et* a/⁵⁸

Patients referred to respiratory clinics with suspicion of obstructive sleep

apnoea

10758 Belgium

Claes *et al*⁶¹

Irregular supraventricular extra systoles in series for 30 s

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Table 1	Continued	ned																	
Study	۲	Country	Type of patients used	Device used	Duration of 1 recording (s)	Frequency of ' recording/ day	Total monitoring (days)	Mean/ median age Me (vears) (%	BMI Male (kg/ (%) m ²)	HTN (%)	N DM (%)	0%) (%)	Previous diagnosis of AF (%)	* HF (%)	Previous stroke (%)	Mean/ median s CHADS/ CHA_DS VASC	Definition of AF	New AF (n)	New AF rate (%)
Samol et a ⁶²	132	Germany	Large proportion poststroke/TIA. Also recruited from diabetes, HTN and dyslipidemia clinics	Omron HeartScan HCG-801	e R	F	0	64 58	ЧZ	67	27	R	0	e	49	NR	Cardiologist Interpretation×2	4	51
Battipaglia et al ⁶³	855	Ъ	Community shopping centre screening	MyDiagnostik	15	-	0	NR	ЯN	NR	RN	В	RN	ЧN	R	RN	NR	7	0.8
Chan and Choy ⁵⁹	13 122	Hong Kong	Nationwide community Alive Cor screening programme	 Alive Cor 	R	÷	0	64.7 29	23.7	38.2	2 14.8	3 2.2	0	0.7	2.8	RN	Software algorithm definition with minimum of 30 s	101	0.8
Chan et a ⁶⁵	10735	Hong Kong	Nationwide community Alive Con screening programme	/ Alive Cor	0 B	÷	0	NR	Ш	NR	R	В	1:2	Н	RN	RN	Cardiologist interpretation (≥30s)	74	0.7
Halcox et al ⁶⁴	501	ЛК	Community based with individuals aged >65 years with CHA2DS2-VASC score≥2	Alive Cor	8	2× per week	365	72.6 48	R	54	26	4	0	1.0	7.0	3.0	30s duration of an irregular rhythm without P waves	19	3.8
Gladstone et al ¹⁸	277	Canada	Patients admitted with cryptogenic stroke	Holter	Continuous	Continuous	-	73.2 56	R	67	19.3	3 14.7	0	4	12.6	R	30s or longer duration of irregular rhythm	თ	3.2
Barthélémy et ar ⁱ⁹	60	France	Consecutive patients admitted with stroke/ TIA	Holter	Continuous	Continuous	-	64.4 55	ЧZ	50	17	R	0	Ц	27	RN	Fibrillatory waves associated with irregular ventricular response ratio at least 30s duration	œ	13.3
Jabaudon et a/ ²⁰	149	Switzerland	I Consecutive patients admitted with stroke/ TIA	Holter	Continuous	Continuous	-	66.9 68	R	58	16.7	16.8	4.7	НN	16.8	RN	Щ	~	4.7
Koudstaal et a/ ²¹	100	Holland	Retrospective study of 100 patients admitted with stroke/TIA	Holter	Continuous	Continuous	-	60.9 74	R	N	RR	41	NR	RN	NR	NR	ЯN	Ð	5
Hornig <i>et al</i> ²²	268	Germany	Consecutive patients admitted with stroke/ TIA	Holter	Continuous	Continuous		59.1 61	R	43.7	.7 34	Н	RN	14.9	45	RN	RN	10	3.3
Rizos <i>et al²³</i>	496	Germany	Patients admitted with stroke/TIA	Holter	Continuous	Continuous	-	69 62	NR	78.8	.8 24.6	NR	NR	RN	22.2	ი	Cardiologist interpretation (≥30s)	44	2.8
Schuchert et a ^{p4}	82	Germany	Consecutive patients admitted with stroke/ TIA	Hoiter	Continuous	Continuous	n	59.7 57	Ë	36.5 2	к Z	17.1	٣	Ë	щ	н	Small irregular baseline undutations of variable anplitudes and morphology at a rate >350/min with an irregular ventituclar response for at least 1 min	۵	۵
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Table 1	Continued	ned																	
Study	۲	Country	Type of patients used	Device used	Duration of 1 recording (s)	Frequency of recording/ day	Total monitoring (days)	Mean/ median age N (years)	BMI Male (kg/ (%) m ²)		HTN DM (%) (%)	(%) (Previous diagnosis of AF (%)	HF (%)	Previous stroke (%)	Mean/ median CHADS/ CHA ₂ DS ₂ - VASC	Definition of AF	New AF (n)	New AF rate (%)
Schaer <i>et al²⁵</i>	241	Switzerland	Consecutive patients admitted with stroke/ TIA	Holter	Continuous	Continuous	-	68.7 5	59 NR	76	3 25	41	7	NR	4.6	NR	NR	0	0
Schaer et al ²⁶	425	Switzerland	Retrospective review of patients poststroke/ TIA with Holter monitoring	Holter	Continuous	Continuous	-	67.4 6	RN NR	щ	R	R	۳	R	5.	щ	Self-terminating sequence of >30s of irregular RR intervals and the presence of fibrillatory P waves	თ	5.
Shafqat <i>et al²⁷</i>	465	Pakistan	Retrospective review of consecutive patients admitted with stroke/TIA	Holter	Continuous	Continuous	-	66.8	56 NR	RN	R R	R	RN	RN	RN	R	R	5	2.4
Lazzaro et a/ ⁸⁸ 133	133	NSA	Consecutive patients admitted with stroke/ TIA	Hoiter	Continuous	Continuous	-	63.1	50 NR	20	29.3	3 - 18.88	0	Ë	- - - - 3	۳	Supraventricular tachyarrhythmia characterised by uncoordinated atrial activation with fibrillatory waves varying in amplitude, shape and timing, replacing consistent P aduration >30 s	ω	ω
Grond et al ²⁹	1135	Germany	Patients admitted in seven German centres with stroke/TIA	Holter	Continuous	Continuous	n	5	55 27.4	4	20.4	4 7.3	0	α ω	17.4	٣	≥1 period of >30 s duration of an absolute arrhythmia without defectable P waves and without a pattern wore consistent with an alternate diagnosis	49	4.3
Stahrenberg et al ³⁰	224	Germany	Consecutive patients admitted with stroke/ TIA	Holter	Continuous	Continuous	2	68	58 27.6		72.9 22.3	3 14.8	0	5.2	16.2	щ	2x Cardiologist interpretation of software algorithm detection of events	58	12.5
Ritter <i>et al</i> ³¹	60	Germany	Patients admitted with cryptogenic stroke	Holter	Continuous	Continuous	2	61.8 5	57 NR	20	11.7	7 13.3	RN	0	RN	4	Cardiologist interpretation (>30 s)		1.7
Higgins <i>et al³²</i>	2 50	Scotland	Patients admitted with Holter stroke/TIA	Holter	Continuous	Continuous	4	67.1 4	48 NR	56	80	16	0	ЯN	EN N	RN	Cardiologist interpretation (>30 s)	4	Ø
Hendrikx <i>et</i> a/ ⁶⁷	95	Sweden	Patients investigated for palpitations and presyncope	Holter	Continuous	Continuous	F	54.1 4	42 NR		28.4 1.1	8.4	0	0	6.3	-	30s irregular rhythm without P waves	0	2.1
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	CHA ₂ DS ₂ - Definition New VASC of AF AF	CHA,DS, Definition New VASC of AF AF (n) NR 30s irregular 3 rhythm without P waves	CHADBS, Definition New VASC of AF AF (n) NR an integular 3 rhythm without 3 P. vaves P. vaves RR intervals and the presence of fibrillatory P waves waves	CHADBS, Definition New VASC of AF AF (n) NR an integular 3 rhythm without 3 P. vaves A.8 -30s rhythm 9 with irregular and the presence of fibrillatory P waves NR NR 2 NR NR 2	CHADBO MSC of AF Definition AF (n) New AF (n) NR 30s irregular inythm without 3 4.8 >30 s trythm P waves 9 A.8 >30 s trythm waves 9 NR of florillatory P waves 9 NR NR 2 NR Irregular waves 2 NR Irregular waves 1 NR Irregular waves 1 NR vertificular waves 1	CHAZADS. Definition New VASC of AF AF (n) NR 30s irregular AF (n) 14.8 30s irregular 3 14.8 >30s irregular 3 14.8 >30s irregular 3 14.8 >30s irregular 3 14.8 >30s irregular 3 15.9 >3 >3 16.1 NR 1 17.1 NR 2 18.1 NR 2 19.2 NR 2 10.1 NR 2 11.1 11 11 11.1 vertricular 3 11.1 vertricular 11 11.1 vertricular 3 11.1 NR 11 11.1 vertricular 3 11.1 vertricular 3 11.1 vertricular 3 11.1 NR 11 11.1 NR 3 11.1 3	CHAZADS. Definition New AF(n) NR 30s irregular rhythm without 30s 1.8 30s irregular rhythm without 3 1.8 >30 s rhythm 9 Pwaves -30 s rhythm 9 NR >30 s rhythm 9 NR Nith irregular the presence of fibrillatory P 2 NR NR 11 NR Irregular waves 11 NR Irregular waves 5 3 firregular without visible P 5 NR NR NR 1 venticular waves 15	CHAZADS, of AF Definition AF (n) New AF (n) NR 30s stregular rhythm without 3 4.8 >30 s rhythm with irregular RR intervals and the presence of fibrillatory P 9 NR NR 2 NR NR 2 NR NR 2 NR NR 2 NR NR 11 NR rregular the presence of p waves 11 NR Irregular the verticular solution withs 5 NR NR NR 15 NR NR NR 15	CHALDAD ASCC, of AF MASC ASCC, of AFDefinition AF(n)NewNR30s irregular rhythm without P waves NR30s rhythm with irregular with irregular with irregular of finilatory P waves9NR>30s rhythm p waves the presentand the presentand with irregular the presence of p absence of p waves9NRNRNR2NRNR11NRIrregular the presence of p waves11NRIrregular thythm absence of p waves5NRNRNR15NRNRNR15NRNRNRNRNRNRNR15NRNRNRNRNRNRNR15NRNRNR17	CHAPPS MSC MSC MSC MSC MSC MSC MSCDefinition ActionNew MSC Action14.830s irregular hythm without Pwaves MR30s irregular hythm without34.8>-30 s thythm hwaves difinilatory P3	CHAPPAS MSCDefinition of AF (n)New AF (n)NIN30 s irregular rhythm without p waves30 s irregular thythm without8 w4.8>30 s irregular thythm regular the presence of fibrillatory b waves or with the presence of p waves or with the pular9NINNRNR2NINNR2NINNR2NINIrregular waves or with the pular the pular11NINNR15NINNR15NINNR15NINNR15NINNR17NINNR17NINNR15NINNR17NINNR17NINNR17NINNR17NINNR17NINNR17NINNR17NINNR17NINNR17NINNR17NINNR17NINSmall irregular mater of 300-350/3 at a min associated within regular mothology at a wettroularNINSmall irregular mulations of variables26NINSmall irregular mulations of variables26NINSmall irregular mulations of variables26NINSmall irregular mulations of variables26NINSmall irregular mulations26NINSmall irregular mulations26 <th>CHARLONG MSCC, GAF MSCC, GAFDefinition AGF(I)NewUNS30s irregular inythm without30 strythm with irregular30 strythm with irregular4.8>30 s irregular inythm without30 strythm invatus30 strythm stregular30 strythm stregular0.1NRNRNR20.1NRNR110.1Irregular waves110.1NRNR150.1NRNR150.1NRNR17<td< th=""></td<></th>	CHARLONG MSCC, GAF MSCC, GAFDefinition AGF(I)NewUNS30s irregular inythm without30 strythm with irregular30 strythm with irregular4.8>30 s irregular inythm without30 strythm invatus30 strythm stregular30 strythm stregular0.1NRNRNR20.1NRNR110.1Irregular waves110.1NRNR150.1NRNR150.1NRNR17 <td< th=""></td<>
HF stroke (%) (%)		1.7 7.7 NR	21.7	7.7 21.7 RN	7.7 21.7 NR 6.3	7.7 21.7 6.3 6.3	7.7 21.7 6.3 8.3 NR	7.7 21.7 6.3 8.3 NR NR	7.7 21.7 6.3 6.3 NR NR NR	7.7 21.7 6.3 8.3 NR NR NR NR NR	7.7 21.7 6.3 6.3 8.3 8.3 NR NR NR NR NR	7.7 21.7 6.3 6.3 8.1 NIR NIR NIR NIR
Previous IHD diagnosis (%) of AF (%)	15.4 0		0 1.0	0 AN AN	9.1 0 AN 14.1 0 AN 14.1 0	9.1 0 14.1 0 0 MR 0 0 0	9.1 0 NR NR 14.1 0 20 0 15.7 7.4	9.1 0 NR NR 14.1 0 20 0 25 0 31 NR 35 7.4	9.1 0 NR NR 14.1 0 20 0 231 NR 11.3 NR	9.1 0 H4.1 0 R1 15.7 7.4 11.3 R1 11.3	9.1 0 NR NR 11.3 15.7 7.4 0 11.3 NR 11.3 NR 20 0 11.3 NR 20 1 21 1.5 22 1.5	9.1 0 14.1 0 13.1 15.7 2.4 0 11.3 NR NR NR NR NR 20.4 0 20 20 20 20 20 20 20 20 20 20 20 20 20
BMI (kg/ HTN DM m ²) (%) (%)	NR 51.9 23.1		NR 80.7 26.4	80.7 NR	80.7 58.2	80.7 58.2 65	80.7 58.2 35.3	80.7 58.2 35.3 65 61 61	80.7 88.7 58.2 35.3 65 61 71.3	80.7 81.7 85 85 85 85 85 85 85 85 85 85 85 85 85	80.7 80.7 58.2 65 61 71.3 71.3 70.1	80.7 80.7 58.2 65 65 61 81 71.3 70.1 70.1
Mean/ Mean/ median age Male (k (years) (%) m	59.5 77 N		73.2 62 N	62 NR	62 48 NR	62 57 48 NR	62 53 AR NR 53	62 57 48 69	62 84 87 62 63 63 53 69 53 53 53 53 53 53 53 53 53 53 53 53 53	62 NR 53 69 43 57 NR	62 NR 84 57 59 69 60 NR 62	69 53 69 53 69 69 69 69 69 69 69 69 69 69 69 69 69
/ of Total / monitoring (days)	1		-				N	~ ~	0			
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Type of patients used	Consecutive patients admitted with stroke/	H I										
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Table 1	Continued	ned																	
Study	ح	Country	Type of patients used	Device used	Duration of recording (s)	Frequency of Total recording/ monit day (days	Total monitoring (days)	Mean/ median age M (years)	BMI Male (kg/ (%) m ²)	и 9() НТN (%)	N DM (%)	(%)	Previous diagnosis of AF (%)	HF (%)	Previous (stroke ((%)	Mean/ median CHADS/ CHA ₂ DS ₂ - VASC	Definition of AF	New AF (n)	New AF rate (%)
Yodogawa et al ⁴⁴	68	Japan	Consecutive patients admitted with ischaemic stroke	Holter	Continuous	Continuous	-	Q 0.0	54 NR	66.2	.2 14.7	7 NR	RN	щ	۲ ۳	RN	Irregular and uncoordinated atrial electrical activity on surface ECG lasting >30 s	17	25
Atmuri <i>et al</i> ⁴⁵	140	Australia	Retrospective audit of patients admitted with ischaemic stroke/TIA	Holter	Continuous	Continuous	-	NN	NR NR	8 65	20	37.1	18.6	NR	RN	NR	NR	5	8.6
Salvatori et al ⁴⁶	274	Italy	Cohort study of patients aged ≥65 years with HTN in multiple GP clinics	Hotter	Continuous	Continuous	N	70 5.	54 NR	100	0 15	Ø	2	4	2.2	Ч	Cardiologist interpretation	4	1.5
Beaulieu- Boire <i>et al</i> ⁴⁷	284	Canada	Consecutive patients admitted with stroke/ TIA	Holter	Continuous	Continuous	-	70.6 5	52 NR	8 68.7	.7 26.7	7 27.4	NR	2:2	22.3	R	Cardiologist interpretation	18	6.3
Dogan <i>et al</i> ⁴⁸	400	Turkey	Retrospective review of patients admitted poststroke	Hotter	Continuous	Continuous		RN	NN NN	RN	AN S	ЯN	R	RN	RN	R	RN	40	10
Douen <i>et al</i> ⁴⁹	126	Canada	Retrospective review of patients admitted poststroke	Holter	Continuous	Continuous	-	NN	NR NR	AN NR	S NR	R	7	NR	RN	NR	NR	6	7.1
Suissa <i>et al</i> ⁵⁰	354	France	Consecutive patients admitted with ischaemic stroke	Hotter	Continuous	Continuous	-	62.4 5	57 NR	s1.1	.1 18.6	6 NR	0	ЯN	RN	R	Cardiologist interpretation	N	0.6
Wohlfahrt et al ⁵¹	224	Germany	Patients admitted with Holter ischaemic stroke	Holter	Continuous	Continuous	7	68.5 5	59 NR	t 73.2	.2 22.3	3 15.2	RN	5.4	24.1 1	NR	>30 s irregular rhythm	29	12.9
AF, atrial fibril	illation; BMI	I, body mass i	AF, atrial fibrillation; BMI, body mass index; DM, diabetes mellitus; GP, general practitioner;	us; GP, general p		eart failure; HT	N, hypertensic	HF, heart failure; HTN, hypertension; IHD, ischaemic heart disease.	lic heart c	disease.									

Study	Sample size (n)	New AF detection rate (%)	ES (95% CI)	% Weigh
Single Lead ECG monitoring	.,	. ,		
	855	.8	• 0.82 (0.33, 1.68)	7.55
Chan et al. (2016)	1013	.5	0.49 (0.16, 1.15)	8.47
Chan et al. (2016)	13122	.8	0.77 (0.63, 0.93)	9.54
Chan et. al. (2017)	10735	.7	0.69 (0.54, 0.86)	9.52
Claes et. al. (2012)	10758	1.6	1.55 (1.33, 1.80)	9.31
Doliwa et. al. (2009)	606	1	◆ 0.99 (0.36, 2.14)	6.53
Engdahl et. al. (2013)	848	4.7	4.72 (3.39, 6.37)	3.74
lalcox et. al. (2017)	501	3.8	3.79 (2.30, 5.86)	3.04
lendrikx et. al. (2013)	928	3.8	★ 3.77 (2.64, 5.21)	4.46
	95	9.5	9.47 (4.42, 17.22)	0.34
	201	6.5	6.47 (3.49, 10.81)	0.97
	3269	1.1	• 1.13 (0.80, 1.56)	8.80
owres et. al. (2014)	1000	1.5	1.50 (0.84, 2.46)	6.72
	65747	1.1	• 0.92 (0.85, 0.99)	9.67
	204	9.8	9.80 (6.09, 14.73)	0.69
Samol et. al. (2012)	132	5.3	5.30 (2.16, 10.62)	0.78
Sobocinski et. al. (2012)	249	6	6.02 (3.41, 9.74)	1.24
Svennberg et. al. (2015)	7173	3	● 3.04 (2.65, 3.46)	8.64 100.0
Subtotal (I^2 = 93.63%, p = 0.00)			0 1.74 (1.39, 2.09)	100.0
Holter Monitoring	100	0.5		0.05
Alhadramy et. al. (2010)	426 140	2.5 8.6	2.58 (1.30, 4.57)	3.95 2.48
Atmuri et. al. (2012)			8.57 (4.51, 14.49)	
	60	13.3	13.33 (5.94, 24.59)	1.23
	284	6.3	6.34 (3.80, 9.83)	3.35
	51 400	29.4 10		0.69 3.30
logan et. al. (2011) louen et. al. (2008)	126	7.1	10.00 (7.24, 13.37) 7.14 (3.32, 13.13)	2.54
	80	21	21.25 (12.89, 31.83)	1.16
	277	3.2	3.25 (1.50, 6.08)	3.71
	1135	4.3	4.32 (3.21, 5.67)	4.06
Gumbinger et. al. (2011)	192	1	1.04 (0.13, 3.71)	3.98
	26	42.3	42.31 (23.35, 63.08)	0.33
	95	2.1	2.11 (0.26, 7.40)	3.33
Higgins et. al. (2013)	50	8	8.00 (2.22, 19.23)	1.48
fornig et. al. (1996)	268	3.3	3.73 (1.80, 6.75)	3.63
abaudon et al. (2004)	149	4.7	4.70 (1.91, 9.44)	3.07
(oudstaak et. al. (1986)	100	5	5.00 (1.64, 11.28)	2.65
azzaro et. al. (2012)	133	6	6.02 (2.63, 11.51)	2.76
Manina et. al. (2014)	114	25.4	25.44 (17.75, 34.45)	1.36
litter et. al. (2013)	60	1.7	1.67 (0.04, 8.94)	3.15
Rizos et. al. (2012)	496	2.8	2.82 (1.55, 4.69)	3.97
	274	1.5	1.46 (0.40, 3.70)	3.98
chaer et. al. (2004)	425	2.1	4 2.12 (0.97, 3.98)	4.00
chuchert et. al. (1999)	82	6	6.10 (2.01, 13.66)	2.25
hafqat et. al. (2004)	465	2.4	1.08 (0.35, 2.49)	4.13
hibazaki et. al. (2012)	536	2.2	4 2.24 (1.16, 3.88)	4.04
obocinski et. al. (2012)	249	2	2.01 (0.66, 4.62)	3.86
tahrenberg et. al. (2010)	224	12.5	12.50 (8.47, 17.56)	2.62
uissa et. al. (2012)	354	.6	0.56 (0.07, 2.03)	4.16
agawa et. al. (2007)	308	8.4	8.44 (5.59, 12.12)	3.22
hakkar et. al. (2014)	52	5.8	5.77 (1.21, 15.95)	1.82
andebroucke et. al. (2004)	136	5.1	5.15 (2.09, 10.32)	2.91
achter et. al. (2017)	198	5	4.55 (2.10, 8.45)	3.32
Vohlhahrt et. al. (2013)	224	12.9	12.95 (8.84, 18.06)	2.59
adogawa et. al. (2013)	68	25	25.00 (15.29, 36.98)	0.94
Schaer et. al. (2009)	241	0	(Excluded)	
ubtotal (I^2 = 87.45%, p = 0.00)			 5.49 (4.36, 6.63)	100.0

Figure 2 Forest plot showing the overall atrial fibrillation (AF) detection rate between single-lead ECG devices and Holter monitoring.

Comparison of multiple intermittent monitoring with 24 hours Holter

There was significant variation in the monitoring time using both single-lead and Holter monitoring, which contributed to the difference in the cumulative detection rate seen in figure 2. Figure 3 compares the detection rate of multiple intermittent single-lead recordings with 24 hours continuous monitoring, which is used routinely in clinical practice. There were eight studies (n=10199, mean weighted age 68.8±8.4 years from six studies, 47% male from eight studies) that performed multiple intermittent single-lead ECG recordings and 27 studies (n=6284, mean weighted age 67.8±5.1 years from 23 studies, 58% male from 23 studies) that used 24 hours Holter monitoring. From the data available, the multiple intermittent ECG group had a lower AF risk to the 24 hours Holter group (hypertension 55% (n=8 studies) vs 65% (n=20 studies); diabetes mellitus 15% (n=8 studies) vs 22% (n=20 studies); heart failure 3.3% (n=8 studies) vs 3.9% (n=11 studies); ischaemic heart disease 11% (n=6 studies) vs 19% (n=15 studies) and previous stroke/TIA

9% (n=7 studies) vs 16% (n=15 studies)), respectively. The combined AF detection rate was 4.8% (95% CI 3.6% to 6.0%) using multiple intermittent ECG recordings. The cumulative AF detection rate using 24 hours Holter monitoring was 4.6% (95% CI 3.5% to 5.7%).

Association between monitoring time and AF detection

Using single-lead ECG devices, we found a moderate linear relationship between the total monitoring time and AF detection rate (β =0.13, R²=0.42). Using this formula, we noted that approximately 19 min of total intermittent monitoring produced similar AF detection to 24 hours continuous monitoring (figure 4). The study by Halcox *et al* was an outlier, with a much lower AF detection rate than other studies (3.8% from 52min of total monitoring) and this reduced the linear correlation between total monitoring time and AF detection rate.⁶⁴ Exclusion of these data led to a stronger linear relationship (β =0.26, R²=0.80) and a much lower total intermittent monitoring time required (12min) to produce a similar AF detection rate to 24 hours Holter monitoring.

1

Study	Sample size (n)	New AF detectior rate (%)										ES (95% CI)	% Weight
Sludy	(1)	Tale (70)										E3 (95 % CI)	weight
Multiple ECG Recordings		. –										/	
Engdahl et. al. (2013)	848	4.7										4.72 (3.39, 6.37)	17.05
Halcox et. al. (2017)	501	3.8										3.79 (2.30, 5.86)	15.63
Hendrikx et. al. (2013)	928	3.8	· • ·									3.77 (2.64, 5.21)	18.21
Hendrikx et. al. (2014)	95	9.5			-							9.47 (4.42, 17.22)	3.48
Hendrikx et. al. (2017)	201	6.5		_								6.47 (3.49, 10.81)	7.98
Ramkumar et. al. (2017)	204	9.8										9.80 (6.09, 14.73)	6.21
Sobocinski et. al. (2012)	249	6		•								6.02 (3.41, 9.74)	9.47
Svennberg et. al. (2015)	7173	3	•									3.04 (2.65, 3.46)	21.97
Subtotal (I^2 = 73.78%, p =	= 0.00)		\diamond									4.78 (3.58, 5.97)	100.00
Holter													
Alhadramy et. al. (2010)	426	2.5	-									2.58 (1.30, 4.57)	5.31
Atmuri et. al. (2012)	140	8.6										8.57 (4.51, 14.49)	2.96
Barthelemy et. al. (2003)	60	13.3		-		-						13.33 (5.94, 24.59)	1.34
Beaulieu-Boire et. al. (2013	3)284	6.3		-								6.34 (3.80, 9.83)	4.29
Dogan et. al. (2011)	400	10	_	•—								10.00 (7.24, 13.37)	4.20
Douen et. al. (2008)	126	7.1										7.14 (3.32, 13.13)	3.05
Fonseca et. al. (2013)	80	21					_					21.25 (12.89, 31.83)	1.26
Gladstone et. al. (2014)	277	3.2										3.25 (1.50, 6.08)	4.89
Gumbinger et. al. (2011)	192	1	•									1.04 (0.13, 3.71)	5.35
Gunalp et. al. (2006)	26	42.3			-							42.31 (23.35, 63.08)	0.34
Hendrikx et. al. (2014)	95	2.1										2.11 (0.26, 7.40)	4.24
Hornig et. al. (1996)	268	3.3										3.73 (1.80, 6.75)	4.74
Jabaudon et al. (2004)	149	4.7	-	•								4.70 (1.91, 9.44)	3.84
Koudstaak et. al. (1986)	100	5		_								5.00 (1.64, 11.28)	3.20
Lazzaro et. al. (2012)	133	6		_								6.02 (2.63, 11.51)	3.36
Rizos et. al. (2012)	496	2.8										2.82 (1.55, 4.69)	5.34
Schaer et. al. (2004)	425	2.1										2.12 (0.97, 3.98)	5.40
Shafqat et. al. (2004)	465	2.4	•									1.08 (0.35, 2.49)	5.63
Shibazaki et. al. (2012)	536	2.2	-									2.24 (1.16, 3.88)	5.47
Sobocinski et. al. (2012)	249	2										2.01 (0.66, 4.62)	5.14
Suissa et. al. (2012)	354	.6	•									0.56 (0.07, 2.03)	5.70
Tagawa et. al. (2007)	308	8.4		_								8.44 (5.59, 12.12)	4.07
Thakkar et. al. (2014)	52	5.8										5.77 (1.21, 15.95)	2.07
Vandebroucke et. al. (2004) 136	5.1	-	-								5.15 (2.09, 10.32)	3.60
Wachter et. al. (2017)	198	5										4.55 (2.10, 8.45)	4.23
Yadogawa et. al. (2013)	68	25		_		•						25.00 (15.29, 36.98)	1.01
Schaer et. al. (2009)	241	0										(Excluded)	
Subtotal (I^2 = 84.75%, p =	= 0.00)		\diamond									4.59 (3.45, 5.72)	100.00
					I								
			4 8	12 16	6 20 2 AF Dete	24 28 ction ra	32 36	40 4	44 48	52 56	60 64		
					AF Dele	CIUITA	10 70						

Figure 3 Forest plot comparing the atrial fibrillation (AF) detection rate between 24 hours Holter monitoring and performing multiple intermittent single-lead ECG recordings.

Meta-regression

Sources of heterogeneity in the 18 studies using singlelead ECG monitoring were investigated using meta-regression (table 2). Monitoring time per participant (β =0.11, 95% CI 0.04 to 0.18, p=0.005) and body mass index (β =1.1, 95% CI 0.58 to 1.5, p=0.01) were associated with AF detection.

Sensitivity analysis

A number of outlier studies were observed in the meta-analysis that could influence the cumulative AF detection rate.^{37–40 44} Removal of these outlier studies resulted in a reduction in the overall AF detection rate in all Holter studies (table 3) and for 24 hours Holter studies (table 4). When these outlier studies were removed, the

overall AF detection rate for 24 hours Holter was 3.86% (95% CI 2.88% to 4.83%), much lower than the detection rate by multiple intermittent ECG recordings using portable single lead devices (4.78%, 95% CI 3.58% to 5.97%). A cumulative meta-analysis (figure 5) did not show any significant variation in the AF detection rate over time using either Holter or single-lead ECG monitoring.

Publication bias

Publication bias was explored using a funnel plot of all included studies (see online supplementary figure 1). There was significant publication bias in both single-lead ECG device and Holter monitoring studies (Egger test, p=0.003 and p<0.001 respectively).

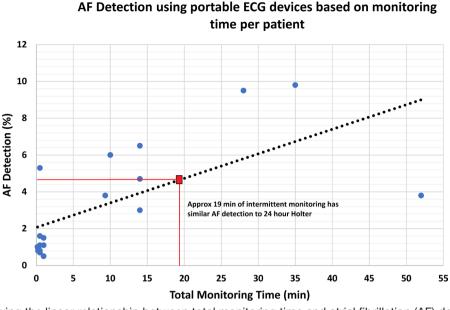


Figure 4 Graph showing the linear relationship between total monitoring time and atrial fibrillation (AF) detection rate in single-lead ECG devices.

Quality of studies

A summary of the quality analysis (see online supplementary table 3) showed that overall quality of reporting was moderate. All studies described the primary objective of the trial and included a summary of the main findings. Detailed comorbidities of the study participants were only adequately reported in 28/52 (54%), and limitations were discussed in 35/52 (67%) of studies. Most had a very selective patient population, 31/52 (60%) were poststroke/TIA cohorts.

DISCUSSION

Our study is the only systematic review that we are aware of that has studied the overall AF detection rate of singlelead portable ECG devices. The results of our systematic

Table 2Meta-regdetection (single-le	,	alysis for atrial fibrillat udies)	ion (AF)
Variable	Number of studies	β (95% CI)	P values
Age (years)	15	0.00 (-0.22 to 0.24)	0.95
Monitoring time per participant (min)	18	0.11 (0.04 to 0.18)	0.005
Body mass index (kg/m²)	4	1.1 (0.58 to 1.5)	0.01
CHADS score (%)	11	-0.13 (-2.6 to 2.4)	0.91
Hypertension (%)	14	0.01 (-0.08 to 0.10)	0.75
Previous diagnosis of AF (%)	16	-0.13 (-0.50 to 0.24)	0.46
Ischaemic heart disease (%)	12	-0.10 (-0.42 to 0.21)	0.48
Previous stroke (%)	13	0.06 (-0.09 to 0.19)	0.45
Male gender	16	0.10 (-0.04 to 0.24)	0.16

review suggest a linear relationship between monitoring time per patient and AF detection rate. Single timepoint screening has an approximate 1% AF detection rate, which can be increased to around 5% when multiple recordings are performed. We noted that approximately 19min of intermittent monitoring produced similar detection rates to conventional 24 hours continuous Holter monitoring.

Early diagnosis of AF

AF creates a significant burden on both patients as well as the healthcare system. AF will continue to rise in incidence and the costs to the healthcare system will continue to increase, due to ageing, sedentariness and the prevalence of obesity and the metabolic syndrome.^{3 68} Early diagnosis offers the possibility for early initiation of treatment, which may reduce the occurrence of the complications and may lead to reduced hospital admissions and associated healthcare costs. Early treatment for AF can be achieved in different ways. Patients with subclinical AF have an increased risk of stroke and cardiovascular

Table 3	Outlier studies omitted (all Holter studies) to
assess th	ne change to the overall atrial fibrillation (AF)
detection	n rate

Study omitted	Overall AF detection rate (%)	95% CI (%)
Dangayach et al ³⁷	5.27	4.17 to 6.38
Fonseca <i>et al</i> ³⁹	5.26	4.15 to 6.36
Gunalp et al ³⁸	5.32	4.21 to 6.42
Manina et al ⁴⁰	5.11	4.03 to 6.20
Yadogawa et al 44	5.25	4.14 to 6.35
All studies excluded	4.31	3.36 to 5.26

 Table 4
 Outlier studies omitted (24 hours Holter) to assess

 the change to the overall atrial fibrillation (AF) detection rate

Study omitted	Overall AF detection rate (%)	95% CI (%)
Fonseca et al ³⁹	4.30	3.21 to 5.39
Gunalp <i>et al</i> ³⁸	4.39	3.30 to 5.47
Yadogawa et al ⁴⁴	4.30	3.22 to 5.38
All studies excluded	3.86	2.88 to 4.83

events, like those with established AF.¹²⁶⁹ Anticoagulation may help reduce the incidence of stroke in this cohort.

The close relationship between metabolic syndrome and AF has encouraged research into the benefits of lifestyle intervention. Aggressive lifestyle intervention in patients with AF undergoing catheter ablation has been reported to lead to a reduction in symptom burden, improved quality of life and the need for repeat ablation procedures.¹⁰ It remains to be tested whether initiation of

Study	Year		ES (95% CI)
Single Lead ECG Monitoring)		
Doliwa et. al. (2009)	2009		3.48 (0.29, 6.67)
Sobocinski et. al. (2012)	2012	└─ ◆──	3.37 (0.03, 6.71)
Claes et. al. (2012)	2012		3.28 (0.58, 5.98)
Samol et. al. (2012)	2012		3.24 (0.69, 5.79)
Engdahl et. al. (2013)	2013		3.84 (-1.38, 9.06)
Hendrikx et. al. (2013)	2013		3.72 (-0.90, 8.34)
Lowres et. al. (2014)	2014		4.20 (-6.70, 15.10)
Hendrikx et. al. (2014)	2014		3.29 (-0.54, 7.13)
Svennberg et. al. (2015)	2015		- 3.88 (-4.23, 12.00)
Proietti et. al. (2016)	2016		 4.06 (-3.13, 11.25)
Kaasenbrood et. al. (2016)	2016		4.17 (-2.04, 10.38)
Chan et al. (2016)	2016		3.48 (-0.17, 7.13)
Battipaglia et. al. (2016)	2016		3.31 (0.83, 5.80)
Ramkumar et. al. (2017)	2017		
Hendrikx et. al. (2017)	2017		3.31 (0.36, 6.25) 3.24 (0.48, 5.99)
Chan et al. (2016)	2017		
			3.36 (0.91, 5.81)
Chan et. al. (2017)	2017		3.41 (1.00, 5.82)
Halcox et. al. (2017)	2017		3.40 (1.07, 5.74)
Holter Monitoring			
Koudstaak et. al. (1986)	1986	_ 	2.73 (-0.98, 6.43)
Hornig et. al. (1996)	1996		2.81 (-0.60, 6.22)
Schuchert et. al. (1999)	1999	└─ ◆──	2.88 (-0.05, 5.81)
Barthelemy et. al. (2003)	2003		2.47 (-2.58, 7.52)
Jabaudon et al. (2004)	2004	_ 	2.64 (-1.62, 6.90)
Schaer et. al. (2004)	2004		2.96 (0.16, 5.77)
Shafqat et. al. (2004)	2004		3.07 (0.36, 5.78)
Vandebroucke et. al. (2004)	2004		2.58 (1.14, 4.02)
Gunalp et. al. (2006)	2006		2.69 (1.08, 4.29)
Tagawa et. al. (2007)	2007		2.54 (1.06, 4.02)
Douen et. al. (2008)	2008		2.54 (1.24, 3.85)
Stahrenberg et. al. (2010)	2010		2.95 (0.60, 5.30)
Alhadramy et. al. (2010)	2010		3.10 (1.26, 4.95)
	2010		
Gumbinger et. al. (2011)			3.08 (1.20, 4.96)
Dangayach et. al. (2011)	2011		2.94 (1.23, 4.66)
Dogan et. al. (2011)	2011		2.54 (1.22, 3.86)
Rizos et. al. (2012)	2012		2.90 (-0.32, 6.11)
Lazzaro et. al. (2012)	2012		3.04 (0.48, 5.59)
Sobocinski et. al. (2012)	2012		3.13 (1.33, 4.94)
Shibazaki et. al. (2012)	2012	-+-	2.56 (1.10, 4.03)
Atmuri et. al. (2012)	2012	 →	2.51 (1.14, 3.88)
Suissa et. al. (2012)	2012	←	2.58 (1.29, 3.87)
Grond et. al. (2013)	2013		3.04 (0.57, 5.52)
Ritter et. al. (2013)	2013		3.04 (0.78, 5.29)
Higgins et. al. (2013)	2013		2.98 (0.86, 5.11)
Fonseca et. al. (2013)	2013	→	2.61 (1.06, 4.16)
Yadogawa et. al. (2013)	2013	│ →	2.51 (1.11, 3.90)
Beaulieu-Boire et. al. (2013)	2013	→	2.55 (1.21, 3.89)
Wohlhahrt et. al. (2013)	2013	│ →	2.57 (1.29, 3.84)
Gladstone et. al. (2014)	2014		3.43 (-5.48, 12.33)
Hendrikx et. al. (2014)	2014		3.04 (0.98, 5.09)
Thakkar et. al. (2014)	2014		3.02 (1.05, 4.99)
Manina et. al. (2014)	2014		2.54 (1.03, 4.04)
Salvatori et. al. (2015)	2015		2.54 (1.18, 3.90)
Wachter et. al. (2017)	2017		3.02 (1.11, 4.94)
			0.02 (1.11, 7.07)
	-16 -12	-8 -4 0 4 8	12 16

Figure 5 Cumulative meta-analysis showing minimal variation in atrial fibrillation (AF) detection over time using Holter and single-lead ECG devices.

lifestyle intervention and aggressive risk factor modification following the early diagnosis of AF may be associated with positive LA remodelling and reduction of disease progression. Such a process may lead to additional health benefits, including reduction in cardiovascular risk and improvement in exercise capacity.

AF screening and feasibility

AF is a leading cause of stroke and heart failure in the community. As well as an association with increased all-cause mortality, it is associated with reduced quality of life. The availability of preventive therapies, including anticoagulation, has led to increasing recognition of the importance of AF screening for early diagnosis. However, AF screening shares the limitations of screening with other diagnostic tests. The screening tool must have high sensitivity, and needs to be inexpensive and cost-effective. We also need to minimise and have a method of addressing false positives. Current guidelines recommend opportunistic screening using pulse palpation and 12-lead ECG.¹¹ In a previous systematic review, this was associated with a new AF detection rate of approximately 1%.⁵ Pulse palpation may be non-specific in patients with other irregular rhythms such as ventricular ectopy, and 12-lead ECG is only able to capture a single timepoint for screening. There are multiple other methods for AF detection. Continuous Holter monitoring is probably the most commonly used in clinical practice, especially in stroke cohorts. It has the potential advantage of assessing heart rhythm throughout the day and may be useful in detecting nocturnal subclinical AF. However, the disadvantages include the cost of Holter monitoring (especially for mass screening), the inconvenience of leads and electrodes (which may affect compliance) and typical limitation to 1-2 days of capture (as extended periods are more cumbersome and less cost-effective). Other event recorders are again expensive and limited to symptomatic patients. Extended period monitoring using implantable devices have shown promise in the cryptogenic stroke population (where many have been diagnosed with paroxysmal AF),⁷⁰ but they are invasive and not feasible for mass screening.

Portable single-lead ECG devices permit multiple 30–60 s recordings to be captured, and downloaded to a computer. These devices have several potential advantages over Holter monitoring. They are leadless and require finger contact (and are hence easy to use and acceptable to patients). They have a high degree of sensitivity for identifying AF.^{71–73} Most interface with a web-based cloud system where ECG rhythms can be wirelessly transferred to clinicians, allowing rapid analysis and diagnosis. The development of automated algorithms to detect AF is helpful for mass screening. In two small studies they have demonstrated superior AF detection compared with 24 hours Holter monitoring.^{66 67} Although screening using these portable devices are currently not in the latest AF guidelines, they may offer

a feasible option for mass screening. Screening using these devices has been demonstrated to be cost-effective. $^{74\,75}$

We noted a moderate linear association between monitoring time and AF detection rate. Single timepoint screening for 30–60s achieved an overall detection rate of approximately 1%. This is no better than what has been reported using pulse palpation or 12-lead ECG, hence does not add any incremental benefit in screening programmes.⁵ Multiple intermittent recordings improve AF detection; we found that at least 19 min of total monitoring should be performed to achieve detection rates similar to 24 Holter monitoring.

The linear relationship between monitoring time and AF detection rate (R^2 =0.80) and the reproduction of AF detection rates of 24 hours Holter monitoring with only 12 min of intermittent monitoring was possible in our study only after exclusion of an outlier.⁶⁴ Despite the inclusion of elderly participants with at least one risk factor for AF, the use of a validated single-lead ECG device and a prolonged monitoring period, that study had a lower AF detection rate (3.8%) than the remaining studies, even using a shorter monitoring period.^{53 56 57} Relatively low rates of adherence (only approximately 25% completed 2×30s ECG recordings every week for the full year of monitoring) may be a potential explanation for the lower AF detection rate noted.⁶⁴

Limitations

There are several challenges inherent in this meta-analysis of studies investigating AF detection. The most important is the target screening population. Most studies did not report the CHADS or CHA₉DS₉-VASC score, a history of previous stroke or other comorbidities. Consequently, it was difficult to ascertain if the risk profiles of patients in these studies were equivalent. Most Holter monitoring studies were performed in the stroke population-which is likely a population with higher AF risk than many studies using portable ECG devices, which recruited mainly healthy participants or those with AF risk factors from the community. The significant heterogeneity among both Holter and portable ECG device studies make it difficult to perform direct comparisons between both groups. The type/duration of monitoring and type of device used will also influence the overall AF detection rate and varied significantly between studies. There are several possible confounders which may not have been taken into account. The validity of the linear regression analysis comparing detection time and rate may be limited due to the significant differences in study population, study design and AF definitions. However, despite these limitations, the analysis may provide some important inferences into AF screening. Multiple intermittent ECG recordings achieved a similar AF detection rate to 24 hours Holter monitoring. This may suggest that in a similar cohort of patients with the same comorbidities, single-lead intermittent monitoring may be superior for AF detection.

Compared with 24 hours continuous monitoring, single-lead portable ECG monitoring is more patient dependent. Good patient compliance is essential to obtain multiple readings across different timepoints which improves sensitivity. The analysis performed does not take into account patient compliance as this is difficult to assess and poorly reported across the individual studies. Most single-lead device manufacturers have proprietary automated AF detection algorithms, which were used for diagnosis. Not all of these algorithms have had rigorous testing and comparison to a reference standard. It is also difficult to distinguish AF from other supraventricular tachycardias using single-lead ECG devices as the P wave is often not readily discernible. The use of different automated algorithms makes AF definitions non-standardised and can potentially create issues with both overdiagnosis and underdiagnosis.

There are other limitations in this analysis. The efficacy of intermittent monitoring is critically dependent on AF burden and density. All studies varied in their monitoring period and strategy. The linear regression model used was able to determine a total intermittent monitoring time, which produced similar AF detection rates to 24 hours continuous monitoring. However, it is difficult to translate the total monitoring time into an effective monitoring strategy. For example, we are unable to determine from our analysis if 12×60s recordings over 12 consecutive days is different to 2×60s recordings daily for six consecutive days. The definitions of AF also vary between studies. Many are based on individual physician interpretation and criteria for diagnosis were not explicitly specified. The duration of AF varied from 10 to 30s between studies, although a cut-off of 30s was the most widely adopted practice.

CONCLUSION

Single-lead portable ECG devices may offer an efficient screening option for AF compared with 24 hours Holter monitoring. Total monitoring time is related to AF detection and a total of 19 min may achieve a similar detection rate to 24 hours Holter monitoring.

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