VP Very Important Paper

Size-Dependent Cellular Uptake of RGD Peptides

Isabell Kemker,^[a] Rebecca C. Feiner,^[b] Kristian M. Müller,^[b] and Norbert Sewald^{*[a]}

Monomeric RGD peptides show unspecific fluid-phase uptake in cells, whereas multimeric RGD peptides are thought to be internalized by integrin-mediated endocytosis. However, a potential correlation between uptake mechanism and molecular mass has been neglected so far. A dual derivatization of peptide c(RGDw(7Br)K) was performed to investigate this. A fluorescent probe was installed by chemoselective Suzuki–Miyaura cross-coupling of the 7-bromotryptophan and a poly(ethylene glycol) (PEG) linker was attached to the lysine residue. Flow cytometry and live cell imaging confirmed unspecific uptake of the small, non-PEGylated peptide, whereas the PEG₅₀₀₀ peptide conjugate unveiled a selective internalization by M21 cells overexpressing $\alpha_v\beta_3$ and no uptake in α_v -deficient M21L cells.

Integrins play a crucial role in cell adhesion and signaling. In particular, RGD-binding integrins emerged as targets for selective tumor therapy as they regulate processes like apoptosis, metastasis, or angiogenesis, and are overexpressed on malignant cells, while being downregulated on most healthy cells.^[1,2] Since their first discovery in the late 1980s^[3] a variety of ligands targeting integrins like $\alpha_v\beta_3$ were developed. However, prominent small-molecule ligands as cilengitide,^[4] c(RGDf(NMe)V), failed in clinical trials also due to its ambiguous role in angiogenesis.^[5] Nevertheless, ¹⁸F-galacto-RGD and derivatives are currently under clinical investigation and show promising results as a positron emission tomography tracer.^[6] Especially because much is known about the relationship between structure and activity for RGD ligands, they represent a versatile and easily accessible toolkit for drug targeting. In this context, the internalization pathway into the target cell is an important issue.

As shown previously, monomeric RGD peptides undergo a fluid-phase rather than a clathrin-dependent uptake.^[7] Interestingly, a tetrameric regioselective addressable functionalized

[a] I. Kemker, Prof. Dr. N. Sewald Organische und Bioorganische Chemie Fakultät für Chemie, Universität Bielefeld Universitätsstrasse 25, 33615 Bielefeld (Germany) E-mail: norbert.sewald@uni-bielefeld.de

[b] R. C. Feiner, Prof. Dr. K. M. Müller Zelluläre und Molekulare Biotechnologie Technische Fakultät, Universität Bielefeld Universitätsstrasse 25, 33615 Bielefeld (Germany) template peptide (RAFT-RGD-Cy5) does not only provide higher affinity toward $\alpha_v \beta_3$ but was shown to undergo clathrinmediated internalization.^[8] Thus, multivalent RGD peptides are considered superior for in vivo studies. However, in a contradictory report Ga-labeled trimeric and monomeric ligands were compared. It was found that improved in vitro properties of multimers were not consistent with better in vivo performance.^[9] These case studies demonstrate the complex interaction patterns and show that predictions of translation from in vitro to in vivo are not straightforward.

In the last decades, a variety of RGD-drug conjugates has been synthesized for targeted drug delivery.^[10] However, the pathway of uptake was only studied sparingly and reports are conflicting. For example, studies by us revealed colocalization of an RGD-cryptophycin-52 conjugate with lysosomes in WM-115 cells^[11] (overexpressing $\alpha_{v}\beta_{3}$) and in contrast, an RGD-cryptophycin-55 conjugate was internalized both by M21 (overexpressing $\alpha_{v}\beta_{3}$) and M21L (α_{v} knockout) cells.^[12] Likewise, cytotoxic RGD- α -amanitin conjugates did not provide specific uptake.^[13] It was further demonstrated that a monomeric RGDdoxorubicin conjugate afforded good binding affinities toward $\alpha_{v}\beta_{3}$ in a cell adhesion assay, but was not internalized.^[14] Additionally, RGD conjugates tend to accumulate on the cell surface as described for c(diketopiperazine-RGD)-sCy5 conjugates.^[15] However, in vivo experiments confirmed that numerous multivalent RGD conjugates are associated with improved uptake at tumor sites.^[16,17] These findings indicate that integrin-mediated endocytosis is favored for peptides with multifold RGD sites.

We wondered whether the route of internalization solely correlates with multivalency or whether it might be affected by merely increasing the size of a monomeric RGD peptide. As this has not yet been investigated to the best of our knowledge, we synthesized monomeric RGD peptides differing in size and investigated a potential correlation with the mode of uptake.

c(RGDw(Br)V)-derived peptides containing a halogenated D-Trp residue w(Br) were chosen as an intermediate for latestage dual modification. Halotryptophans can selectively be synthesized by biocatalytic halogenation effecting regioselective bromination of the indole ring. They represent versatile handles for chemoselective installation of aryl moieties by cross-coupling reactions, which can eventually be used to generate fluorescent probes.^[18-20] In particular, a large aromatic system as in the pyrene derivative (1) permits an excitation (λ_{ex} : 365 nm) suitable for biological applications (Figure S1 in the Supporting Information). Structure–activity relationship studies on c(RGDfV) disclosed that any amino acid can be incorporated instead of valine without significantly compromising bioactivity.^[21,22]

Supporting information and the ORCID identification numbers for the authors of this article can be found under https://doi.org/10.1002/ cbic.201900512.

^{© 2019} The Authors. Published by Wiley-VCH Verlag GmbH & Co. KGaA. This is an open access article under the terms of the Creative Commons Attribution Non-Commercial NoDerivs License, which permits use and distribution in any medium, provided the original work is properly cited, the use is non-commercial and no modifications or adaptations are made.



This allows for the use of lysine in this position, enabling a dual, chemoselective late-stage modification using bromotryptophan for cross-coupling and lysine for nucleophilic substitution. PEGylation has become a popular method to increase blood circulation times, enhance stability toward enzymatic degradation and bioavailability.^[24,25] For our experiments, a 5 kDa PEG linker was attached to increase the size relative to peptide **1**. The crude peptide was treated with 4 M HCI/dioxane to selectively cleave the Boc protecting group. The peptide was purified by RP-HPLC before addition of the NHS-activated PEG moiety and the PEGylated intermediate was purified prior to Pbf cleavage, as separation of unreacted PEG and PEGylated peptide could only be achieved at this stage. Precipitation by diethyl ether after removal of protecting groups gave peptide **2** (Scheme 1).



Scheme 1. Dual late-stage functionalization of RGD peptides by cross-coupling and PEGylation. Cross-coupling was performed similarly as described previously.^[23] The *t*Bu protecting group is cleaved under the applied reaction conditions, which does not cause any side reactions during PEGylation. sSPhos = sodium 2'-dicyclohexylphosphino-2,6-dimethoxy-1,1'-biphenyl-3-sulfonate hydrate; DIPEA = *N*,*N*-diisopropylethylamine; TFA = trifluoroacetic acid; TIS = triisopropylsilane; NHS = *N*-hydroxysuccinimide.

Affinities toward isolated integrins $\alpha_{\nu}\beta_3$ and $\alpha_5\beta_1$ were determined in a competitive ELISA (Table 1). Peptide 1 shows somewhat decreased affinity toward $\alpha_{\nu}\beta_3$ relative to the reference cilengitide (3), but an improved selectivity over $\alpha_5\beta_1$. Interestingly, peptide 2 exhibits similar affinities toward $\alpha_{\nu}\beta_3$ in comparison with reference peptide 3. As demonstrated previously, substitution of valine by lysine does not have a major impact

Table 1. Affinities determined by an ELISA using purified, isolated integrins.							
No.	Sequence	IC ₅₀ [nм] а.в. а.в.		Ratio			
		0.003	0.5P1				
1	c(RGDw(pyren-1-yl)V)	5.11 ± 0.90	2079 ± 237	1:41			
2	c(RGDw(pyren-1-yl)K(PEG ₅₀₀₀))	0.88 ± 0.03	73.6 ± 10.7	1:84			
3	c(RGDf(NMe)K)	0.54 ± 0.02	15.4 ± 4.0	1:29			

on the affinity.^[22] Previous studies have demonstrated increased as well as decreased affinity for peptides modified at lysine with different spacers,^[26,27] chelators,^[28] or peptides with short PEG linkers.^[29,30] Loss in affinity can mostly be ascribed to the steric bulk of conjugates that hinder interactions with the binding pocket. However, larger molecules may have a greater ability to interact unspecifically with the protein surface at more sites and thus, decrease dissociation leading eventually to apparent affinity.^[31]

Cellular internalization was studied in vitro. M21 cells overexpress $\alpha_{v}\beta_{3}$, whereas the variant M21L lacks α_{v} and thus does not express α_{v} integrins.^[12] As described previously, uptake of monomeric RGD peptides is fluid-phase dependent,^[7,8] whereas for multimeric peptides internalization is clathrin-dependent.^[8] We investigated by flow cytometry (FC) as a quantitative method and live cell imaging as a qualitative method to which extent molecular size can influence cellular uptake.

For flow cytometry studies, cells (2×10⁶) were incubated with peptides (30 μ M) for 0, 10, or 30 min, washed with buffer and analyzed. Interestingly, the 0 min samples already show strong fluorescence for both cell lines that increases slightly with longer incubation times (Figure 1A). As M21L cells do not present integrin $\alpha_{v}\beta_{3}$, uptake of peptide **1** proceeds in an integrin-independent fashion.^[7] The large shift between the negative control (no peptide) and the 0 min sample is caused by ionic interactions of positively charged Arg side chains with negatively charged phospholipids of the membrane resulting in an accumulation of RGD peptides on the cell surface.^[15,32] Therefore, the localization of peptides was further studied by live cell imaging. Cells were grown overnight on glass-slip chambers and first counterstained with LysoTracker Red DND-99 before incubation with peptide (5 $\mu \textrm{m})$ for 10 min. Careful but thorough washing steps were performed prior to analysis by confocal microscopy. Care was taken not to detach the semi-adherent M21L cells which lack α_{ν} integrins responsible for adherence. As shown in Figure 1B, peptide 1 is hardly internalized and shows strong interaction with the cell membrane. Moreover, the peptide present inside the cell is not colocalized with lysosomes indicating integrin-independent uptake like reported previously.^[10, 23]

In contrast, flow cytometry reveals significant fluorescence for peptide **2** in M21 cells but not for α_v deficient M21L cells (Figure 2A). Contrary to peptide **1**, the negative control (no peptide) largely overlaps with the 0 min samples. Fluorescence imaging confirmed the presence of peptide inside the cells by *z*-stacking (Figure S2). Furthermore, peptide **2** colocalizes largely with lysosomes (Figure 2B). As peptide **2** is barely found inside M21L cells, integrin-mediated endocytosis can be concluded. Other internalization studies with a 10 kDa PEGylated peptide were unsuccessful: no peptide fluorescence was detected during live cell imaging or flow cytometry (Figure S3). We assume that this conjugate is either highly prone to bind to residual serum proteins still present from cultivation or the larger PEG shields integrin binding.^[33]

An additional negative control experiment was performed to support integrin-mediated endocytosis for peptide 2. Integrin $\alpha_v\beta_3$ was incubated with a monoclonal anti- $\alpha_v\beta_3$ antibody for

ChemBioChem	2020,	21,	496 – 499	
-------------	-------	-----	-----------	--

www.chembiochem.org



CHEMBIOCHEM Communications



Figure 1. Uptake studies with peptide **1**. A) Flow cytometry analysis after incubation of cells with peptide **1** (30 μм) for 0 min (blue), 10 min (orange), and 30 min (green). No peptide was added in the negative control (red). B) M21 and M21L cells were stained with LysoTracker Red DND-99 and incubated for 10 min with peptide **1** (5 μм) prior to fluorescence microscopy. In combination both experiments clearly show an unspecific, fluid-phase uptake of peptide **1**.



Figure 2. Internalization studies with peptide **2**. A) For flow cytometry peptide **2** ($30 \mu \mu$) was incubated with cells for 0 min (blue), 10 min (orange), and 30 min (green). No peptide was added in the negative control (red). Analysis revealed an uptake of peptide **2** only by M21 cells. B) Live cell imaging of peptide **2** confirmed specific uptake only for M21 cells. For a better signal-to-noise ratio higher concentrations of peptide **2** ($10 \mu \mu$) were applied. The gain was adjusted in channel 1 to ensure the absence of peptide **2** in M21L cells. White spots in merged channels represent colocalization with lysosome.

15 min on ice to block but not internalize $\alpha_{v}\beta_{3}$ integrins. Subsequent incubation with peptides 1 and 2 gave significant fluorescence for peptide 1, yet not for 2 (Figure S4). Furthermore, incubation of peptide 1 at 37 and 4°C, respectively, resulted in significantly decreased uptake at 4°C (Figure S5), which again supports specific uptake.

These results strongly support that in vitro integrin-mediated endocytosis for monomeric RGD peptides can be triggered by attaching a PEG linker. We hypothesize that steric and physicochemical effects contribute to this switch in uptake pathway. Similar to findings that particle size influences whether endocytosis is clathrin- or caveolae-mediated,^[34] the increased



CHEMBIOCHEM Communications

size of peptide **2** could favor integrin-mediated over a fluidphase uptake. However, the hydrodynamic radius of a 5 kDa PEG (2.3 nm) is only slightly increased in comparison with a 10 kDa dextran (1.9 nm), which is commonly applied as a fluidphase marker.^[35] Therefore, the PEG linker might also minimize ionic interactions with the membrane preventing an accumulation on the cell membrane or enhances conformational changes of the integrin and thus, promote internalization. It also can be envisaged that upon binding of PEGylated peptide its local concentration increases initiating self-assembly and thus, creating a multivalent ligand.^[36] Despite the uncertainties as to why PEGylation induces integrin-mediated internalization, these results question whether multivalency is the ultimate prerequisite for integrin-mediated endocytosis.

In summary, dual late-stage functionalized RGD peptides were synthesized to elucidate the influence of size for integrinmediated endocytosis. Bromotryptophan as a non-canonical amino acid and lysine served as platforms to chemoselectively introduce a fluorescent probe and PEG linker. Interestingly, PEGylation of a monomeric RGD peptide effects integrin-mediated endocytosis and presents a new approach to obtain monomeric conjugates suitable for specific targeting.

Acknowledgements

Financial support by Deutsche Forschungsgemeinschaft (SE609/ 16-1) is gratefully acknowledged. We thank Prof. Dr. Horst Kessler and his group for support concerning the ELISA-type affinity assay and Dr. Veronica Dodero for helpful discussions. We appreciate technical support in confocal microscopy by Dr. Thorsten Seidel and by Prof. Dr. Thomas Hellweg and his group on absorption and fluorescence measurements.

Conflict of Interest

The authors declare no conflict of interest.

Keywords: halogenated tryptophan · internalization poly(ethylene glycol) · RGD peptides · selective uptake

- M. Nieberler, U. Reuning, F. Reichart, J. Notni, H.-J. Wester, M. Schwaiger, M. Weinmüller, A. Räder, K. Steiger, H. Kessler, *Cancers* 2017, 9, 116.
- [2] Z. Liu, F. Wang, X. Chen, Drug Dev. Res. 2008, 69, 329-339.
- [3] M. D. Pierschbacher, E. Ruoslahti, *Nature* **1984**, *309*, 30–33.
- [4] M. A. Dechantsreiter, E. Planker, B. Mathä, E. Lohof, G. Hölzemann, A. Jonczyk, S. L. Goodman, H. Kessler, J. Med. Chem. 1999, 42, 3033–3040.
- [5] A. R. Reynolds, I. R. Hart, A. R. Watson, J. C. Welti, R. G. Silva, S. D. Robinson, G. Da Violante, M. Gourlaouen, M. Salih, M. C. Jones, D. T. Jones, G. Saunders, V. Kostourou, F. Perron-Sierra, J. C. Norman, G. C. Tucker, K. M. Hodivala-Dilke, *Nat. Med.* **2009**, *15*, 392–400.
- [6] H. Chen, G. Niu, H. Wu, X. Chen, Theranostics 2016, 6, 78-92.
- [7] S. Castel, R. Pagan, F. Mitjans, J. Piulats, S. Goodman, A. Jonczyk, F. Huber, S. Vilaró, M. Reina, *Lab. Investig. J. Tech. Methods Pathol.* 2001, *81*, 1615–1626.
- [8] L. Sancey, E. Garanger, S. Foillard, S. Schoehn, A. Hurbin, C. Albiges-Rizo, D. Boturyn, C. Souchier, A. Grichine, P. Dumy, J.-L. Coll, *Mol. Ther.* 2009, *17*, 837–843.

- [9] S. Maschauer, J. Einsiedel, D. Reich, H. Hübner, P. Gmeiner, H.-J. Wester, O. Prante, J. Notni, *Pharmaceuticals* **2017**, *10*, 29.
- [10] S. Katsamakas, T. Chatzisideri, S. Thysiadis, V. Sarli, Future Med. Chem. 2017, 9, 579-604.
- [11] M. Nahrwold, C. Weiß, T. Bogner, F. Mertink, J. Conradi, B. Sammet, R. Palmisano, S. Royo Gracia, T. Preuße, N. Sewald, *J. Med. Chem.* 2013, 56, 1853–1864.
- [12] A. Borbély, E. Figueras, A. Martins, S. Esposito, G. Auciello, E. Monteagudo, A. Di Marco, V. Summa, P. Cordella, R. Perego, I. Kemker, M. Frese, P. Gallinari, C. Steinkühler, N. Sewald, *Pharmaceutics* **2019**, *11*, 151.
- [13] L. Bodero, P. López Rivas, B. Korsak, T. Hechler, A. Pahl, C. Müller, D. Arosio, L. Pignataro, C. Gennari, U. Piarulli, *Beilstein J. Org. Chem.* 2018, 14, 407–415.
- [14] D. J. Burkhart, B. T. Kalet, M. P. Coleman, G. C. Post, T. H. Koch, *Mol. Cancer Ther.* 2004, *3*, 1593–1604.
- [15] A. Raposo Moreira Dias, A. Pina, A. Dean, H.-G. Lerchen, M. Caruso, F. Gasparri, I. Fraietta, S. Troiani, D. Arosio, L. Belvisi, L. Pignataro, A. Dal Corso, C. Gennari, *Chem. Eur. J.* **2019**, *25*, 1696–1700.
- [16] Z. Fan, Y. Chang, C. Cui, L. Sun, D. H. Wang, Z. Pan, M. Zhang, Nat. Commun. 2018, 9, 2605.
- [17] J. Zhao, S. Li, Y. Jin, J. Wang, W. Li, W. Wu, Z. Hong, *Molecules* 2019, 24, 817.
- [18] C. Schnepel, H. Minges, M. Frese, N. Sewald, Angew. Chem. Int. Ed. 2016, 55, 14159–14163; Angew. Chem. 2016, 128, 14365–14369.
- [19] H. Gruß, C. Belu, L. M. Bernhard, A. Merschel, N. Sewald, Chem. Eur. J. 2019, 25, 5880-5883.
- [20] A. D. Roy, R. J. M. Goss, G. K. Wagner, M. Winn, Chem. Commun. 2008, 4831.
- [21] G. Müller, M. Gurrath, H. Kessler, J. Comput. Aided Mol. Des. 1994, 8, 709-730.
- [22] R. Haubner, R. Gratias, B. Diefenbach, S. L. Goodman, A. Jonczyk, H. Kessler, J. Am. Chem. Soc. 1996, 118, 7461–7472.
- [23] I. Kemker, C. Schnepel, D. C. C. Schröder, A. Marion, N. Sewald, J. Med. Chem. 2019, 62, 7417-7430.
- [24] K. Knop, R. Hoogenboom, D. Fischer, U. S. Schubert, Angew. Chem. Int. Ed. 2010, 49, 6288-6308; Angew. Chem. 2010, 122, 6430-6452.
- [25] S. Parveen, S. K. Sahoo, Clin. Pharmacokinet. 2006, 45, 965–988.
- [26] D. Pallarola, A. Bochen, H. Boehm, F. Rechenmacher, T. R. Sobahi, J. P. Spatz, H. Kessler, Adv. Funct. Mater. 2014, 24, 943–956.
- [27] A. Bochen, U. K. Marelli, E. Otto, D. Pallarola, C. Mas-Moruno, F. S. Di Leva, H. Boehm, J. P. Spatz, E. Novellino, H. Kessler, L. Marinelli, J. Med. Chem. 2013, 56, 1509–1519.
- [28] J. Šimeček, J. Notni, T.G. Kapp, H. Kessler, H.-J. Wester, Mol. Pharm. 2014, 11, 1687–1695.
- [29] B. Indrevoll, G. M. Kindberg, M. Solbakken, E. Bjurgert, J. H. Johansen, H. Karlsen, M. Mendizabal, A. Cuthbertson, *Bioorg. Med. Chem. Lett.* 2006, 16, 6190–6193.
- [30] T. G. Kapp, F. Rechenmacher, S. Neubauer, O. V. Maltsev, E. A. Cavalcanti-Adam, R. Zarka, U. Reuning, J. Notni, H.-J. Wester, C. Mas-Moruno, J. Spatz, B. Geiger, H. Kessler, *Sci. Rep.* 2017, *7*, 39805.
- [31] K. C. Dee, D. A. Puleo, R. Bizios, An Introduction to Tissue-Biomaterial Interactions, Wiley, Hoboken, 2002, pp. 37–40.
- [32] D. Bernhagen, V. Jungbluth, N. G. Quilis, J. Dostalek, P. B. White, K. Jalink, P. Timmerman, ACS Comb. Sci. 2019, 21, 198–206.
- [33] J. J. F. Verhoef, T. J. Anchordoquy, Drug Delivery Transl. Res. 2013, 3, 499–503.
- [34] J. Rejman, V. Oberle, I. S. Zuhorn, D. Hoekstra, Biochem. J. 2004, 377, 159–169.
- [35] J. K. Armstrong, R. B. Wenby, H. J. Meiselman, T. C. Fisher, *Biophys. J.* 2004, 87, 4259–4270.
- [36] A. Azri, P. Giamarchi, Y. Grohens, R. Olier, M. Privat, J. Colloid Interface Sci. 2012, 379, 14–19.

Manuscript received: August 14, 2019 Accepted manuscript online: September 3, 2019 Version of record online: October 25, 2019