### **RESEARCH ARTICLE**

### WILEY

## Microstructural alterations in medial forebrain bundle are associated with interindividual pain sensitivity

Thomas Weiss<sup>1</sup> | Zora Kikinis<sup>2</sup>

Maria Geisler<sup>1</sup> | Elizabeth Rizzoni<sup>2</sup> | Nikolaos Makris<sup>2,3,4</sup> | Ofer Pasternak<sup>2,3</sup> | Yogesh Rathi<sup>2,3</sup> | Sylvain Bouix<sup>2,3</sup> | Marco Herbsleb<sup>5</sup> | Karl-Jürgen Bär<sup>6</sup>

<sup>1</sup>Department of Clinical Psychology, Friedrich-Schiller-University Jena, Jena, Germany

<sup>2</sup>Psychiatry Neuroimaging Laboratory, Department of Psychiatry, Brigham and Women's Hospital, and Harvard Medical School, Boston, Massachusetts

<sup>3</sup>Departments of Radiology and Psychiatry, Harvard Medical School, Boston, Massachusetts

<sup>4</sup>Departments of Radiology and Psychiatry, Massachusetts General Hospital, Charlestown, Massachusetts

<sup>5</sup>Department of Sports Medicine and Health Promotion, Friedrich-Schiller-University Jena, Jena, Germany

<sup>6</sup>Department of Psychosomatic Medicine. University Hospital Jena, Jena, Germany

#### Correspondence

Maria Geisler, Department of Clinical Psychology, Friedrich-Schiller-University, Am Steiger 3/1, D-07743 Jena, Germany. Email: maria.geisler@uni-jena.de

**Funding information** 

German Academic Scholarship Foundation

#### Abstract

The perception of pain to noxious stimuli, also known as pain sensitivity, varies among individuals. The comprised brain structures and their white matter pathways are complex and elusive. Here, we aimed to investigate whether variation of microstructure of the medial forebrain bundle (MFB), a tract connecting the basal forebrain with the brain stem, is associated with interindividual pain sensitivity. We assessed interindividual pain sensitivity as a rating of pain intensity to heat stimuli (45, 47, and 48.9°C) in 38 healthy men (age: 27.05 ± 5.7 years). We also reconstructed the MFB using multitensor tractography from diffusion magnetic resonance imaging (dMRI) and calculated free-water corrected dMRI measures of fractional anisotropy (FAt), radial diffusivity (RD<sub>t</sub>), and axial diffusivity (AD<sub>t</sub>). Lower ratings of interindividual pain intensity correlated with higher  $FA_t$  and lower  $RD_t$  of the MFB. As changes in  $FA_t$ and RD<sub>t</sub> may reflect abnormalities in myelination, the results might be interpreted as that a lower pain rating is associated with higher degree of myelination of the MFB and could represent an inhibitory pathway of pain. Our results suggest that alteration of microstructure in the MFB contributes to the interindividual variation of pain perception.

#### **KEYWORDS**

diffusion magnetic resonance imaging (dMRI), endogenous pain modulation, fractional anisotropy (FA)

#### INTRODUCTION 1 |

The neuromatrix of pain (lannetti & Mouraux, 2010) is a complex network comprised of ascending and descending pathways. The ascending pathways transmit nociceptive information from the periphery to the brain. This transmission can be modulated by descending pathways leading to an altered perception and experience of pain (Ossipov, Dussor, & Porreca, 2010; Tracey & Mantyh, 2007). The \_\_\_\_\_ descending system consists of several areas in the limbic forebrain, including the medial, orbitofrontal, and dorsolateral prefrontal cortex (mPFC, OFC, DLPFC), the anterior cingulate cortex (ACC), nuclei in the amygdala, and the hypothalamus (Ossipov et al., 2010). These limbic forebrain structures project to the periaqueductal gray (PAG). PAG is the best known control region of the descending system and is located in the midbrain (Linnman, Moulton, Barmettler, Becerra, & Borsook, 2012). The PAG projects to the rostral ventromedial medulla,

-----

This is an open access article under the terms of the Creative Commons Attribution License, which permits use, distribution and reproduction in any medium, provided the original work is properly cited.

© 2020 The Authors. Human Brain Mapping published by Wiley Periodicals LLC.

which further projects to dorsal horn neurons. The neurons of the descending pathway can inhibit or facilitate pain, such that the person experiences less or more discomfort (Heinricher, Tavares, Leith, & Lumb, 2009).

One way to assess the activity of the descending system is to measure pain sensitivity. Pain sensitivity describes the reaction to various standardized noxious stimuli (Ravn, Frederiksen, Skovsen, Christrup, & Werner, 2012) and has been shown to vary between subjects (Nielsen et al., 2008). There are several factors (e.g., ethnic (Campbell, Edwards, & Fillingim, 2005), physical (Abrishami, Chan, Chung, & Wong, 2011) psychological (Baum, Huber, Schneider, & Lautenbacher. 2011; Oosterman, Dijkerman, Kessels. & Scherder, 2010), genetic (Afari et al., 2011), and social (Vigil et al., 2013) that influence pain sensitivity. However, the exact neuronal mechanisms (e.g., white matter tracts of the descending system) that underlie the variability of pain sensitivity are only fragmentarily understood. A major fiber tract connecting lateral and medial OFC, DLPFC, ACC, amygdala, and hypothalamus with the ventral tegmental area (VTA) and brain stem (and vice versa) is the medial forebrain bundle (MFB) (Coenen et al., 2018: Coenen, Panksepp, Hurwitz, Urbach, & Madler, 2012). The MFB has been studied so far in affective disorders and addiction as this tract also mediates reward and motivation (Bracht, Linden, & Keedwell, 2015; Rivas-Grajales et al., 2018; Russo & Nestler, 2013: Wise, 2005). However, the neural substrates of the descending pain system are the same as those of the MFB. suggesting that this fiber tract is a part of that system. Variability between subjects and within the axons of the MFB can potentially have an effect on the perception of pain. For instance, a higher degree of myelination or larger diameter of the MFB could exert higher modulation of endogenous pain. Consequently, the person would experience less pain.

The methodology of diffusion magnetic resonance imaging (dMRI) allows reconstruction of white matter tracts and evaluation of microstructural features of fiber tracts in vivo (Basser & Pierpaoli, 1996). The most common diffusion indices in dMRI are fractional anisotropy (FA), axial diffusivity (AD), and radial diffusivity (RD). A high value of FA (closer to 1) represents diffusion anisotropy (water molecules move faster in a certain direction) and, among other effects, may reflect fiber density and/or degree of myelination (Kingsley, 2006). To gain additional information about microstructural changes, AD and RD are used. In a series of animal experiments, it has been shown that FA decreases and RD increases in demyelinating axons (Song et al., 2003; Song et al., 2005), while FA and AD decreases with axonal degeneration (Song et al., 2003). Further, the specificity of these measures to tissue changes can be improved by eliminating free-water (FW) contribution of the signal (Metzler-Baddeley, O'Sullivan, Bells, Pasternak, & Jones, 2012; Pasternak, Sochen, Gur, Intrator, & Assaf, 2009).

The MFB has not been successfully delineated from dMRI until recently. While associations, projection and commissural fiber tracts could be reconstructed using the approach of single tensor tractography (Catani & Thiebaut de Schotten, 2008), white matter tracts connecting subcortical and cerebellar regions are much more difficult to reconstruct because of the presence of crossing and fanning fibers in this area. The problem can be solved by applying probabilistic or multitensor tractography (Malcolm, Shenton, & Rathi, 2010), approaches that were applied to reconstruct the MFB (Rivas-Grajales et al., 2018; Zhang et al., 2020).

The relationship between brain white matter and pain sensitivity has been explored previously, but the findings are inconsistent. Several dMRI studies examined differences in FA in brains of patients with chronic pain and healthy controls, and report correlation of FA in specific white matter tracts with specific pain conditions (for review see (Martucci, Ng, & Mackey, 2014). Recently, Zhang et al. (2020) reconstructed nine brainstem fiber trajectories of pathways (including the medial forebrain tract [MFT]) that are potentially involved in pain modulation and reported no significant association between FA in the MFT and the assessed pain levels "pain right now," and "worst pain in last month." In contrast, the dMRI study examining the structural relationship of the white matter of the descending pain system and placebo hypoalgesia reported that pain sensitivity was associated with lower FA of white matter tracts connecting the PAG with the rostral ACC (rACC) and DLPFC in healthy subjects (Stein, Sprenger, Scholz, Wiech, & Bingel, 2012). The findings are promising and encourage investigation of the relationship between MFB and pain sensitivity. However, the later study only focused on FA as single outcome variable. Furthermore, the study has been restricted to explore the fiber connections of PAG with rACC and DLPFC, only.

In the present study, we aimed to investigate whether the microstructure of the MFB was associated with interindividual pain sensitivity as measured by pain intensity ratings to standardized physical stimuli. We explored the microstructure of the MFB in 38 healthy men using dMRI of the brain and applied the FW imaging method (Pasternak et al., 2009) to eliminate partial volume effects of FW CSF on dMRI measures. We expected that pain sensitivity of the individual will be inversely associated with FAt in the MFB. Furthermore, to investigate whether myelination and/or increased number of tracts/ larger diameter of the MFB might contribute to pain sensitivity, we examined the association of RDt and ADt, in addition to FAt. We hypothesized that interindividual pain intensity rating will correlate negatively with FA<sub>t</sub> and positively with RD<sub>t</sub> if myelination of MFB plays a role, while interindividual pain intensity rating will correlate negatively with FA<sub>t</sub> and negatively with AD<sub>t</sub> if the number or size of axons in the MFB play a role. Additionally, we aimed to explore whether changes in FW in MFB were involved with pain.

#### 2 | MATERIALS AND METHODS

#### 2.1 | Participants

Participants were recruited by advertisements posted at the University of Jena, Germany. We only included male subjects in the study to prevent menstruation related influences to pain processing (Riley, Robinson, Wise, & Price, 1999). Inclusion criteria were as follows: age 18–40 years; BMI 18.5–30 kg/m<sup>2</sup>; no pain disorder, no psychiatric or neurological disease; MRI suitable. The final sample size included 38 healthy men (age:  $27.05 \pm 5.7$  years). Subjects were paid for

#### 2.2 | Study design

After the subjects had been informed about the study's procedure, a high-resolution anatomical scan of the whole brain was assessed. Then the pain paradigm was conducted followed by the acquisition of diffusion weighted images (DWI; see Figure 1).

#### 2.2.1 | Paradigm to assess pain intensity

A pseudorandom sequence of twelve 20-s thermal stimuli with different intensities (38, 45, 47, and  $48.9^{\circ}$ C; three trials each) was applied using a 27 mm diameter fMRI-compatible Peltier thermode (PATHWAY Model, Contact Heat-Evoked Potential Stimulator; Ramat Yishai, Israel). Each trial started with a visual cue "+." After presenting the cue for 1 s, the thermal stimulus was administered for 20 s (approximately 1.5-s ramp up, 17-s plateau, approximately 1.5-s ramp down) at the left thigh. After a short delay (10-16 s; Rest 1), participants had 8 s to rate the level of pain of each stimulus on the presented visual analogue scale (VAS) ranging from 0 = no pain to 100 = unbearable pain. A variable intertrial interval (3-6 s; Rest 2) followed before the start of the next thermal stimulation (see Figure 1).

#### 2.3 | MRI data acquisition and preprocessing

Anatomical and diffusion MRI sequences were performed with a 3 T MRI scanner (Siemens Magnetom Prisma fit, Erlangen, Germany) using a 64-channel standard head coil. DWI were acquired using an echo planar image sequence with the following parameters: TR = 6,800 ms; TE = 57 ms; diffusion encoding directions = 81, b = 1,200 s/mm<sup>2</sup>; 72 slices, resolution =  $1.7 \times 1.7 \times 1.7$  mm. Additionally, a high-resolution



FIGURE 1 Study design. DWI, diffusion weighted images

T1-weighted anatomical scan (3D-MP-RAGE sequence, TE = 3.03 ms, TR = 2,300 ms, 192 slices, resolution =  $1 \times 1 \times 1$  mm) was used. An inhouse script was used to postprocess the MRI data of each participant in this study. The quality of the images was visually checked, and all images passed this test. Motion and eddy current correction of diffusion images was performed using an affine registration algorithm in FSL (http://www.fmrib.ox.ac.uk/fsl). Then structural and diffusion images were manually masked using 3DSlicer software, Version 5.2 (Surgical Planning Laboratory, Brigham and Women's Hospital, Boston, MA; http://www.slicer.org). The mask defines the area of the brain. For each DWI, we performed multitensor whole-brain tractography with Free Water estimation (with the following parameter settings: minFA: 0.08, seedFALimit: 0.1. Om (expected variance in orientation from one step to next): 0.001, QI (expected variation in eigenvalues from one step to next): 50, Rs (expected noise level in data): 0.02, stepLength: 0.3, recordLength: 0.9, Qw (expected variance in FW fraction from one step to next): 0.0015, minGA (minimum generalized anisotropy): 0.08, seedsPerVoxel: 1) using the multifiber tracking method (Malcolm et al., 2010) (https://github.com/pnlbwh/ukftractography). The multifiber tracking method has very high reliability and reproducibility of tracing the same fiber connections across scans, across a wide age range, and across a variety of different acquisition protocols (Zhang et al., 2019). In addition, this method was able to reliably trace fibers through crossing fiber regions (Fillard et al., 2011) and is therefore suitable for the reconstruction of whole brain white matter, including tracts connecting subcortical and cortical structures. The output of the multifiber tracking was streamlines, with FAt, ADt, RDt, and the FW fraction at every point along the streamlines. The structural masks were then applied to generate a label map for white and gray matter parcellation using FreeSurfer software. Version 6.0 (Desikan et al., 2006: Fischl et al., 2002). This resulted in cortical and subcortical parcellations as described by Desikan et al. (2006) and Salat et al. (2009). After visual quality control, the FreeSurfer label maps were registered to the diffusion images using the advanced normalization tools (Avants, Epstein, Grossman, & Gee, 2008).

#### 2.4 | Extraction of the MFB

We delineated the MFB from DWI using the White Matter Query Language (WMQL). WMQL is a semi-automated fiber delineation method that allows extraction of fiber tracts from whole-brain tractography based on FreeSurfer labels (Wassermann et al., 2016). The MFB connects the PFC and the VTA. The VTA is split between two FreeSurfer labels, namely the brainstem and the ventral diencephalon (ventral DC). Including both labels (brainstem and ventral DC) as the seed region for WMQL of MFB would have been overinclusive. Therefore, we manually split the ventral DC in an anterior and a posterior part at the mammillary bodies, such that the bodies were not included in the posterior part. The posterior part of the ventral diencephalon and brain stem was the new VTA ROI, which also contains PAG, and we have visualized streamlines of the MFB in close relationship with the anatomical location of PAG in Figure 2. Similar



**FIGURE 2** Medial forebrain bundle. Three-dimensional reconstructions of the medial forebrain bundle (MFB). MFB fiber tracts are in green. In the background, structural MRI in sagittal or axial view are given in shades of gray. (a) Sagittal view of the MFB. (b) Axial view of the MFB. (c-e) Sagittal view of a subset of fibers of the MFB in close relationship with the anatomical location of periaqueductal gray (PAG) (circled in red). (f-g) Axial view of a subset of fibers of the MFB in close relationship with the anatomical location of PAG (circled in red). (h-j) Representation of PAG in a high-resolution data set as transverse segmented sections through the brainstem. For each subfigure, a sagittal view of the brainstem is shown on the left with a yellow line representing the plane of the section that corresponds to the axial view on the right panel. PAG is segmented as shown in the paper by Makris et al. (2019) using the Calabrese et al. (2015) high-resolution brainstem dataset. ACC, anterior cingulate cortex; NAc, nucleus accumbens, OFC, orbitofrontal cortex,

to the study by Rivas-Grajales et al. (2018), we seeded for MFB between the VTA (the posterior part of the ventral diencephalon and brain stem) and the following structures: nucleus accumbens (NAc), OFC (lateral and medial), ACC hippocampus, and amygdala (see Figure 2). We were able to track the projections in all 38 participants (number of streamlines:  $M = 51.4 \pm 17.1$ , range: 32–129). To demonstrate specificity of the MFB in reducing pain, we have chosen the thalamooccipital tract as a control tract and tested the dMRI indices of this tract for associations to pain sensitivity. There were no statistically significant correlations between any of the dMRI indices of the thalamooccipital tract and pain intensity rating (see Table S1).

#### 2.5 | Statistical data analysis

All statistical analyses were performed using R version 3.4.1 (R Core Team, 2017). Significance levels were set to  $p \le .05$ . We defined the individual pain intensity rating as a mean of all nine-pain ratings to applied heat pain stimuli (45, 47, and 48.9°C). We first tested whether there is a relationship between dMRI indices of the MFB and age by calculating Pearson correlations between age and FA<sub>t</sub>, RD<sub>t</sub>, AD<sub>t</sub>, and FW respectively. The correlations revealed no statistically significant relationships (FA<sub>t</sub>: r = -.06, p = .741; RD<sub>t</sub>: r = -.02, p = .902; AD<sub>t</sub>: r = -.18, p = .287; FW: r = .13, p = .439). Therefore, age was not included as covariate in subsequent correlations.

To test our hypothesis, we calculated Pearson correlations between brain measures of MFB (FA<sub>t</sub>, RD<sub>t</sub>, AD<sub>t</sub>, FW) and mean pain intensity rating, as data were normally distributed. Because multiple correlations were performed, we corrected the *p*-values of FA<sub>t</sub>, RD<sub>t</sub>, AD<sub>t</sub>, and FW using the false discovery rate (FDR) procedure (Benjamini & Hochberg, 1995).

#### 3 | RESULTS

#### 3.1 | Descriptive data

On average, participants rated the pain intensity (0 = no pain, 100 = unbearable pain) of the applied noxious stimuli with  $51.4 \pm 17.1$  (range: 15.6–87.2), indicating a large between-subject variability in pain perception.

# 3.2 | Correlation analyses of pain intensity and brain measures of MFB

Rating of pain intensity correlated negatively with  $FA_t$  (Figure 3a) and positively with  $RD_t$  (Figure 3b). Correlation analysis of pain intensity rating and  $AD_t$ , as well as pain intensity rating and FW was not significant (see Table 1).



**FIGURE 3** Association analysis. Correlation between pain sensitivity and free-water corrected fractional anisotropy (FA<sub>t</sub>) (Panel a) and free-water corrected radial diffusivity (RD<sub>t</sub>) (Panel b) of medial forebrain bundle (MFB) in study subjects. RD<sub>t</sub> is given in  $10^{-3}$  cm<sup>2</sup>/s. A lower rating of pain intensity is associated with higher FA<sub>t</sub> and lower RD<sub>t</sub>. This could be interpreted as that people with a higher degree of myelination of the MFB tract experience less pain

	Pain intensity rating		
	r	р	p-FDR corrected
MFB			
$FA_{t}$	372	.021	.043
$RD_{t}$	.383	.018	.043
$AD_{t}$	.001	.994	.994
FW	120	.473	.630

**TABLE 1** Results of correlation analyzes

Note: Pearson correlations coefficient (r) of brain measures, rating of pain intensity, and the corresponding p-values (p) are listed. The p-values of FA<sub>t</sub>, RD<sub>t</sub>, AD<sub>t</sub>, and FW were corrected using the FDR procedure. Bold values denote statistical significance at the p < 0.05 level. Abbreviations: AD<sub>t</sub>, free-water corrected axial diffusivity; FA<sub>t</sub>, free-water corrected fractional anisotropy; FDR, false discovery rate; FW, free-water;

MFB, medial forebrain bundle; RDt, free-water corrected radial diffusivity.

## 4 | DISCUSSION AND CONCLUSIONS

We conducted the present dMRI study to gain knowledge about the neuronal substrates of interindividual variability of pain sensitivity. We analyzed the association between microstructural dMRI measures of the MFB and rating of pain intensity to applied heat stimuli in 38 healthy men. Our results indicate a higher FA<sub>t</sub> and lower RD<sub>t</sub>, which might be explained by a better (stronger) myelination status in MFB, are associated with more efficient pain control after heat stimuli. Analyses of FW and AD<sub>t</sub> in MFB revealed no association with pain.

The MFB is part of the descending pain system where modulation of pain occurs. We assessed the association of interindividual pain intensity rating after heat stimuli as representing a temporary effect, and the microstructure of the MFB as representing a stable structural status. We predicted lower FAt and higher RDt of the MFB in subjects with a higher ability to modulate pain. In line with our hypothesis, we report that interindividual acute pain intensity rating after heat stimulation correlates negatively with FA<sub>t</sub> and positively with RD<sub>t</sub>. Since higher myelination is expected to increase FAt and decrease RDt, but not AD<sub>t</sub>, our result could suggest that individuals with increased axonal myelination of MFB experience less pain. One explanation for the reduced pain intensity rating in subjects with increased axonal myelination of MFB is that MFB connectivity is associated with effective control of pain sensation after heat stimulation. However, as our results rely on correlation analyses in a cross-sectional study, we cannot identify whether a better effective control of pain causes axonal myelination of MFB (training induced changes, see (Scholz, Klein, Behrens, & Johansen-Berg, 2009; Sevel, Boissoneault, Alappattu, Bishop, & Robinson, 2019)) or whether an increased axonal myelination of MFB results in better effective control of pain (genetic component, see (Chiang et al., 2009; Young, Lariviere, & Belfer, 2012)). We found no association between interindividual pain intensity rating and FW, suggesting no effect of extracellular free water of MFB on pain sensitivity in young, healthy men. Our results are in line with a study by Stein et al. (2012) that reported that interindividual pain sensitivity was associated with lower FA of white matter tracts connecting the PAG with the rACC and DLPFC in healthy subjects (Stein et al., 2012). Our study extends the published study on

two major issues. First, the published study focused on FA as the only outcome variable, whereas we have explored additional measures of the fiber microstructure like RD<sub>t</sub> and AD<sub>t</sub> to explore whether alteration in microstructure of the white matter tract is associated with individual pain sensitivity. Second, the published study has been restricted to the fiber connections of PAG with rACC and DLPFC, whereas our study also includes connections from other structures of the limbic forebrain including the OFC, NAc and amygdala, which are important parts of the descending pain system, but possibly distinct pathways. Indeed, it has been shown that self-regulation and nociceptive input mediate pain perception via different brain systems (Woo, Roy, Buhle, & Wager, 2015). In an fMRI study, Woo et al. (2015) revealed that the neurologic pain signature (a pattern of fMRI activity across thalamus, insula, secondary somatosensory cortex, ACC, PAG, and other brain regions that are sensitive and specific to physical pain (Wager et al., 2013)) mediated the effects of noxious input (different heat stimulation intensities), whereas self-regulation of pain was mediated through functional connections between the NAc and ventromedial prefrontal cortex, subcomponents of the MFB.

Although we did not assess chronic pain intensities, as we only investigated healthy participants, the connections of the brain regions of the mesolimbic pathway have been shown to be important in the development of chronic pain. For instance, a longitudinal study by Baliki et al. (2012) revealed that a greater functional connectivity of the NAc with mPFC predicts pain chronification. Additionally, they have shown that alterations in connections to NAc and mPFC, measured by FA, predetermine the transition from acute to chronic back pain (Mansour et al., 2013). Furthermore, Vachon-Presseau et al. (2016) reported that anatomical characteristics of the dorsal mPFC, amygdala. NAc circuitry predict chronic back pain. In addition, Zhang et al. (2020) reconstructed nine brainstem fiber tracts that are potentially involved in modulation of chronic pain. Three out of these nine tracts also overlap partially with the MFB tract of our study. The three tracts of interest to our study are the MFT (that connects the ventral DC and prefrontal cortex), the dorsal longitudinal fasciculus (DLF that connects the PAG and hypothalamus), and the nigrostriatal tract (NST that connects the VTA and NAc). The authors also assessed the relationship between FA of the brainstem tracts and two pain severity levels-"pain right now," and "worst pain in last month." While no significant association between FA in the MFT and NST tracts and pain severity levels was reported, there was a significant negative correlation between both pain levels and FA in the DLF tract. Given that the DLF tract partially overlaps with the MFB tract, the findings of the Zhang et al., 2020 study and our study indicate correspondence between the descending pain control pathways that determine the strength of both chronic pain (pain severity) and acute pain (pain sensitivity). Studies of acute pain are further important, as individuals that are hypersensitive to acute pain are prone to experience increased musculoskeletal pain (Georgopoulos et al., 2019) and increased postoperative pain (Abrishami et al., 2011). Further, people with a reduced ability to modulate acute pain are at a higher risk to develop chronic pain (Edwards, 2005). Although we did not investigate the structure of MFB in patients with chronic pain, the association of interindividual pain sensitivity (measured by pain intensity rating) and alteration in FA<sub>t</sub> and RD<sub>t</sub> of the MFB highlight that the mesolimbic pathway and the connection between frontal areas of the brain with the brainstem play a major role in pain perception.

There are several limitations of the present study. First, our study focused on pain perception in men. Thus, our conclusion should not be generalized to women. Second, the MFB is a bidirectional structure comprised of ascending and descending fibers. Therefore, a separation of the influence of structural changes within the ascending versus descending system is not possible. However, a new predictive coding theory of pain processing suggests a single pain modulation system with reciprocity connection rather than separate top-down and bottom-up systems (Buchel, Geuter, Sprenger, & Eippert, 2014; Grahl, Onat, & Buchel, 2018; Wiech, 2016). Third, we did not delineate subcomponents of the MFB. However, we visualized the PAG region and a subset of fibers of the MFB in close relationship with PAG in Figure 2. We expect to investigate the segments of the MFB connecting exclusively to the PAG in future studies. Fourth, the data acquired for this study did not include a reverse phase-encoding direction (AP and PA) acquisition as it was not commonly used at that time. Consequently, the present study did not include any EPI geometric distortion correction. However, we were able to consistently trace the MFB in all subjects (at least 32 streamlines per subject). Finally, we only analyzed healthy subjects. Consequently, our drawn assumptions on possible association of structural changes of the MFB and the risk to develop chronic pain should be investigated in further studies.

In summary, the results of the present study provide evidence that the microstructure of the MFB, possibly myelination, is associated with interindividual rating of pain intensity in healthy subjects. This highlights the influence of the mesolimbic pathway to the interindividual variability of pain sensitivity in acute pain and offers new research opportunities towards understanding the course of chronic pain (Jakobs, Fomenko, Lozano, & Kiening, 2019).

#### ACKNOWLEDGMENTS

The authors would like to thank Lisa Brotte and Mareike Sittler for assistance with data acquisition as well as Dr Caroline Dietrich and Prof Wolfgang H. R. Miltner for fruitful discussions of the study. M. G. was funded by German Academic Scholarship Foundation. Open access funding enabled and organized by Projekt DEAL.

#### DATA AVAILABILITY STATEMENT

The data of our study "Microstructural Alterations in Medial Forebrain Bundle are Associated with Pain Sensitivity" will be made available via a request to the authors.

#### ORCID

Maria Geisler b https://orcid.org/0000-0002-0321-2119 Yogesh Rathi https://orcid.org/0000-0002-9946-2314 Karl-Jürgen Bär b https://orcid.org/0000-0003-3861-5679

## <sup>1136</sup> WILEY-

#### REFERENCES

- Abrishami, A., Chan, J., Chung, F., & Wong, J. (2011). Preoperative pain sensitivity and its correlation with postoperative pain and analgesic consumption: A qualitative systematic review. *Anesthesiology*, 114, 445–457.
- Afari, N., Mostoufi, S., Noonan, C., Poeschla, B., Succop, A., Chopko, L., & Strachan, E. (2011). C-reactive protein and pain sensitivity: Findings from female twins. *Annals of Behavioral Medicine*, 42, 277–283.
- Avants, B. B., Epstein, C. L., Grossman, M., & Gee, J. C. (2008). Symmetric diffeomorphic image registration with cross-correlation: Evaluating automated labeling of elderly and neurodegenerative brain. *Medical Image Analysis*, 12, 26–41.
- Baliki, M. N., Petre, B., Torbey, S., Herrmann, K. M., Huang, L., Schnitzer, T. J., ... Apkarian, A. V. (2012). Corticostriatal functional connectivity predicts transition to chronic back pain. *Nature Neuroscience*, 15, 1117–1119.
- Basser, P. J., & Pierpaoli, C. (1996). Microstructural and physiological features of tissues elucidated by quantitative-diffusion-tensor MRI. *Journal of Magnetic Resonance. Series B*, 111, 209–219.
- Baum, C., Huber, C., Schneider, R., & Lautenbacher, S. (2011). Prediction of experimental pain sensitivity by attention to pain-related stimuli in healthy individuals. *Perceptual and Motor Skills*, 112, 926–946.
- Benjamini, Y., & Hochberg, Y. (1995). Controlling the false discovery rate: A practical and powerful approach to multiple testing. *Journal of the Royal Statistical Society. Series B (Methodological)*, 57, 289–300.
- Bracht, T., Linden, D., & Keedwell, P. (2015). A review of white matter microstructure alterations of pathways of the reward circuit in depression. *Journal of Affective Disorders*, 187, 45–53.
- Buchel, C., Geuter, S., Sprenger, C., & Eippert, F. (2014). Placebo analgesia: A predictive coding perspective. *Neuron*, 81, 1223–1239.
- Calabrese, E., Hickey, P., Hulette, C., Zhang, J., Parente, B., Lad, S. P., & Johnson, G. A. (2015). Postmortem diffusion MRI of the human brainstem and thalamus for deep brain stimulator electrode localization. *Human Brain Mapping*, *36*, 3167–3178.
- Campbell, C. M., Edwards, R. R., & Fillingim, R. B. (2005). Ethnic differences in responses to multiple experimental pain stimuli. *Pain*, 113, 20–26.
- Catani, M., & Thiebaut de Schotten, M. (2008). A diffusion tensor imaging tractography atlas for virtual in vivo dissections. *Cortex*, 44, 1105–1132.
- Chiang, M. C., Barysheva, M., Shattuck, D. W., Lee, A. D., Madsen, S. K., Avedissian, C., ... Thompson, P. M. (2009). Genetics of brain fiber architecture and intellectual performance. *The Journal of Neuroscience*, 29, 2212–2224.
- Coenen, V. A., Panksepp, J., Hurwitz, T. A., Urbach, H., & Madler, B. (2012). Human medial forebrain bundle (MFB) and anterior thalamic radiation (ATR): Imaging of two major subcortical pathways and the dynamic balance of opposite affects in understanding depression. *The Journal of Neuropsychiatry and Clinical Neurosciences*, 24, 223–236.
- Coenen, V. A., Schumacher, L. V., Kaller, C., Schlaepfer, T. E., Reinacher, P. C., Egger, K., ... Reisert, M. (2018). The anatomy of the human medial forebrain bundle: Ventral tegmental area connections to reward-associated subcortical and frontal lobe regions. *NeuroImage: Clinical*, 18, 770–783.
- Desikan, R. S., Ségonne, F., Fischl, B., Quinn, B. T., Dickerson, B. C., Blacker, D., ... Killiany, R. J. (2006). An automated labeling system for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest. *NeuroImage*, 31, 968–980.
- Edwards, R. R. (2005). Individual differences in endogenous pain modulation as a risk factor for chronic pain. *Neurology*, *65*, 437–443.
- Fillard, P., Descoteaux, M., Goh, A., Gouttard, S., Jeurissen, B., Malcolm, J., ... Poupon, C. (2011). Quantitative evaluation of 10 tractography algorithms on a realistic diffusion MR phantom. *NeuroImage*, 56, 220–234.
- Fischl, B., Salat, D. H., Busa, E., Albert, M., Dieterich, M., Haselgrove, C., ... Dale, A. M. (2002). Whole brain segmentation: Automated labeling of neuroanatomical structures in the human brain. *Neuron*, 33, 341–355.

- Georgopoulos, V., Akin-Akinyosoye, K., Zhang, W., McWilliams, D. F., Hendrick, P., & Walsh, D. A. (2019). Quantitative sensory testing and predicting outcomes for musculoskeletal pain, disability, and negative affect: A systematic review and meta-analysis. *Pain*, 160(9), 1920–1932.
- Grahl, A., Onat, S., & Buchel, C. (2018). The periaqueductal gray and Bayesian integration in placebo analgesia. *eLife*, 7.
- Heinricher, M. M., Tavares, I., Leith, J. L., & Lumb, B. M. (2009). Descending control of nociception: Specificity, recruitment and plasticity. *Brain Research Reviews*, 60, 214–225.
- Iannetti, G. D., & Mouraux, A. (2010). From the neuromatrix to the pain matrix (and back). Experimental Brain Research, 205, 1–12.
- Jakobs, M., Fomenko, A., Lozano, A. M., & Kiening, K. L. (2019). Cellular, molecular, and clinical mechanisms of action of deep brain stimulation-a systematic review on established indications and outlook on future developments. *EMBO Molecular Medicine*, 11, e9575.
- Kingsley, P. B. (2006). Introduction to diffusion tensor imaging mathematics: Part II. Anisotropy, diffusion-weighting factors, and gradient encoding schemes. *Concepts in Magnetic Resonance Part A*, 28A, 123–154.
- Linnman, C., Moulton, E. A., Barmettler, G., Becerra, L., & Borsook, D. (2012). Neuroimaging of the periaqueductal gray: State of the field. *NeuroImage*, 60, 505–522.
- Malcolm, J. G., Shenton, M. E., & Rathi, Y. (2010). Filtered multitensor tractography. IEEE Transactions on Medical Imaging, 29, 1664–1675.
- Mansour, A. R., Baliki, M. N., Huang, L., Torbey, S., Herrmann, K. M., Schnitzer, T. J., & Apkarian, A. V. (2013). Brain white matter structural properties predict transition to chronic pain. *Pain*, 154, 2160–2168.
- Martucci, K., Ng, P., & Mackey, S. (2014). Neuroimaging chronic pain: What have we learned and where are we going? *Future Neurology*, 9, 615–626.
- Metzler-Baddeley, C., O'Sullivan, M. J., Bells, S., Pasternak, O., & Jones, D. K. (2012). How and how not to correct for CSFcontamination in diffusion MRI. *NeuroImage*, 59, 1394–1403.
- Nielsen, C. S., Stubhaug, A., Price, D. D., Vassend, O., Czajkowski, N., & Harris, J. R. (2008). Individual differences in pain sensitivity: Genetic and environmental contributions. *Pain*, 136, 21–29.
- Oosterman, J. M., Dijkerman, H. C., Kessels, R. P., & Scherder, E. J. (2010). A unique association between cognitive inhibition and pain sensitivity in healthy participants. *European Journal of Pain*, 14, 1046–1050.
- Ossipov, M. H., Dussor, G. O., & Porreca, F. (2010). Central modulation of pain. The Journal of Clinical Investigation, 120, 3779–3787.
- Pasternak, O., Sochen, N., Gur, Y., Intrator, N., & Assaf, Y. (2009). Free water elimination and mapping from diffusion MRI. *Magnetic Resonance in Medicine*, 62, 717–730.
- R Core Team. (2017). R: A language and environment for statistical computing. Vienna, Austria: R Foundation for Statistical Computing Retrieved from https://www.R-project.org
- Ravn, P., Frederiksen, R., Skovsen, A. P., Christrup, L. L., & Werner, M. U. (2012). Prediction of pain sensitivity in healthy volunteers. *Journal of Pain Research*, 5, 313–326.
- Riley, J. L., III, Robinson, M. E., Wise, E. A., & Price, D. (1999). A metaanalytic review of pain perception across the menstrual cycle. *Pain*, 81, 225–235.
- Rivas-Grajales, A. M., Sawyer, K. S., Karmacharya, S., Papadimitriou, G., Camprodon, J. A., Harris, G. J., ... Makris, N. (2018). Sexually dimorphic structural abnormalities in major connections of the medial forebrain bundle in alcoholism. *NeuroImage: Clinical*, 19, 98–105.
- Russo, S. J., & Nestler, E. J. (2013). The brain reward circuitry in mood disorders. Nature Reviews Neuroscience, 14, 609–625.
- Rushmore, R. J., Wilson-Braun, P., Papadimitriou, G., Ng, I., Rathi, Y., Zhang, F., ... Makris, N. (2020). 3D Exploration of the Brainstem in 50-Micron Resolution MRI. *Frontiers in Neuroanatomy*, 14, http://dx. doi.org/10.3389/fnana.2020.00040.
- Salat, D. H., Greve, D. N., Pacheco, J. L., Quinn, B. T., Helmer, K. G., Buckner, R. L., & Fischl, B. (2009). Regional white matter volume

differences in nondemented aging and Alzheimer's disease. *NeuroImage*, 44, 1247–1258.

- Scholz, J., Klein, M. C., Behrens, T. E., & Johansen-Berg, H. (2009). Training induces changes in white-matter architecture. *Nature Neuroscience*, 12, 1370–1371.
- Sevel, L., Boissoneault, J., Alappattu, M., Bishop, M., Robinson, M. (2020). Training endogenous pain modulation: a preliminary investigation of neural adaptation following repeated exposure to clinically-relevant pain. *Brain Imaging and Behavior*, 14(3), 881–896. http://dx.doi.org/10. 1007/s11682-018-0033-8.
- Song, S. K., Sun, S. W., Ju, W. K., Lin, S. J., Cross, A. H., & Neufeld, A. H. (2003). Diffusion tensor imaging detects and differentiates axon and myelin degeneration in mouse optic nerve after retinal ischemia. *NeuroImage*, 20, 1714–1722.
- Song, S. K., Yoshino, J., Le, T. Q., Lin, S. J., Sun, S. W., Cross, A. H., & Armstrong, R. C. (2005). Demyelination increases radial diffusivity in corpus callosum of mouse brain. *NeuroImage*, 26, 132–140.
- Stein, N., Sprenger, C., Scholz, J., Wiech, K., & Bingel, U. (2012). White matter integrity of the descending pain modulatory system is associated with interindividual differences in placebo analgesia. *Pain*, 153, 2210–2217.
- Tracey, I., & Mantyh, P. W. (2007). The cerebral signature for pain perception and its modulation. *Neuron*, 55, 377–391.
- Vachon-Presseau, E., Tetreault, P., Petre, B., Huang, L., Berger, S. E., Torbey, S., ... Apkarian, A. V. (2016). Corticolimbic anatomical characteristics predetermine risk for chronic pain. *Brain*, 139, 1958–1970.
- Vigil, J. M., Rowell, L. N., Chouteau, S., Chavez, A., Jaramillo, E., Neal, M., & Waid, D. (2013). Sex differences in how social networks and relationship quality influence experimental pain sensitivity. *PLoS One*, *8*, e78663.
- Wager, T. D., Atlas, L. Y., Lindquist, M. A., Roy, M., Woo, C.-W., & Kross, E. (2013). An fMRI-based neurologic signature of physical pain. *The New England Journal of Medicine*, 368, 1388–1397.

- Wassermann, D., Makris, N., Rathi, Y., Shenton, M., Kikinis, R., Kubicki, M., & Westin, C.-F. (2016). The white matter query language: A novel approach for describing human white matter anatomy. *Brain Structure and Function*, 221, 4705–4721.
- Wiech, K. (2016). Deconstructing the sensation of pain: The influence of cognitive processes on pain perception. *Science*, 354, 584–587.
- Wise, R. A. (2005). Forebrain substrates of reward and motivation. The Journal of Comparative Neurology, 493, 115–121.
- Woo, C.-W., Roy, M., Buhle, J. T., & Wager, T. D. (2015). Distinct brain systems mediate the effects of nociceptive input and self-regulation on pain. *PLoS Biology*, 13, e1002036.
- Young, E. E., Lariviere, W. R., & Belfer, I. (2012). Genetic basis of pain variability: Recent advances. *Journal of Medical Genetics*, 49(1), 1–9.
- Zhang, F., Wu, Y., Norton, I., Rathi, Y., Golby, A. J., & O'Donnell, L. J. (2019). Test-retest reproducibility of white matter parcellation using diffusion MRI tractography fiber clustering. *Human Brain Mapping*, 40, 3041–3057.
- Zhang, Y., Vakhtin, A. A., Jennings, J. S., Massaband, P., Wintermark, M., Craig, P. L., ... Furst, A. J. (2020). Diffusion tensor tractography of brainstem fibers and its application in pain. *PLoS One*, *15*, e0213952.

#### SUPPORTING INFORMATION

Additional supporting information may be found online in the Supporting Information section at the end of this article.

How to cite this article: Geisler M, Rizzoni E, Makris N, et al. Microstructural alterations in medial forebrain bundle are associated with interindividual pain sensitivity. *Hum Brain Mapp*. 2021;42:1130–1137. <u>https://doi.org/10.1002/hbm.</u> 25281