

REVIEW

Considerations for pre-clinical models and clinical trials of pluripotent stem cell-derived cardiomyocytes

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Abstract

Pluripotent stem cells (PSCs) represent an appealing source from which to develop cell replacement therapies. Different initiatives have been launched to promote their development toward clinical applications. This article will review the main questions that should be considered before translating PSC-derived cardiomyocytes into clinical investigations, including the development of good manufacturing practice-level PSC lines, the development of efficient protocols to generate pure populations of cardiac myocytes, and the development of techniques to improve the retention and survival rate of transplanted cells.

Different disorders, notably through myocardial ischemia, can cause the critical loss of cardiomyocytes. This loss initiates a cascade of detrimental events, including the development of cardiac fibrosis, formation of non-contractile scar tissue and promotion of adverse ventricular remodeling - all mechanisms that can lead to heart failure and eventually death. Replacement of dead or dysfunctional cardiac myocytes through cell-based therapies has thus become an emerging and exciting strategy for the treatment of heart failure.

The restoration of damaged heart muscle tissue can be achieved through different strategies, including cell transplantation approaches [1]. Even if recent evidence suggests the existence of cardiomyocyte renewal in the post-natal mammalian heart [2,3], the heart is one of the least regenerative organs in the body. Hence, a large number of cardiac myocytes are needed for replacement therapy.

However, human donor hearts and cardiomyocytes are in extremely limited supply, motivating a demand for alternative cardiomyocyte sources. The remarkable proliferative and differentiation capacity of stem cells represents an appealing strategy to provide an unlimited supply of specific cell types, including viable functioning cardiac cells.

Different types of autologous cells (including skeletal myoblasts, hematopoietic stem cells and mesenchymal stem cells) have been tested so far in pre-clinical and clinical trials but with inconsistent results [4-6]. In this review, we specifically focus on the use of pluripotent stem cells (PSCs) as a source for cell transplantation. PSCs have the ability to differentiate into cell types of all three germ layers, including cardiac and vascular cells [7-9]. Human embryonic stem cells (ESCs) were first isolated in 1998 and are derived from the inner cell mass of blastocyst stage embryos. They have the unique ability to self-renew indefinitely while maintaining the potential to differentiate into all cell types in the human body [10]. The use of human ESCs is, however, limited by different issues, including ethical concerns. The revolutionary discovery of induced pluripotent stem cells (iPSCs), whereby somatic cells (such as dermal fibroblasts or white blood cells) can be reprogrammed into an embryonic-like pluripotent state by the forced expression of a defined set of transcription factors [11], has provided another source of pluripotent stem cells [12]. Like ESCs, iPSCs are multipotent and clonogenic but can also offer autologous personalized therapy. The seminal understanding of pluripotency holds great promise for regenerative medicine and the use of ESCs or iPSCs as a source for cardiac repair has thus become an emerging and exciting field.

However, studies involving the transplantation of PSC-derived cardiomyocytes into the heart have begun only recently. There are currently a very limited number of clinical studies using ESCs or iPSCs that have been approved [13]. In 2009, the Food and Drug Administration

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approved the first clinical trial using ESCs in patients with spinal cord injury, but the trial was discontinued due to funding challenges. PSCs are currently being tested to treat patients with two different forms of macular generation (Stargardt's macular dystrophy and age-related macular degeneration) using PSC-derived retinal pigment epithelial cells [14]. A pilot clinical study using iPSC-derived retinal pigment epithelium cells in patients with exudative age-related macular degeneration has been launched in Japan during summer 2013. It is noteworthy that no clinical trials using PSC-derived cardiomyocytes for the treatment of heart failure have been approved so far, but different research programs have been launched with the objective of treating patients within the next 5 years. This article reviews the main questions that should be considered before translating PSC-derived cardiomyocytes into clinical investigations (Figure 1).

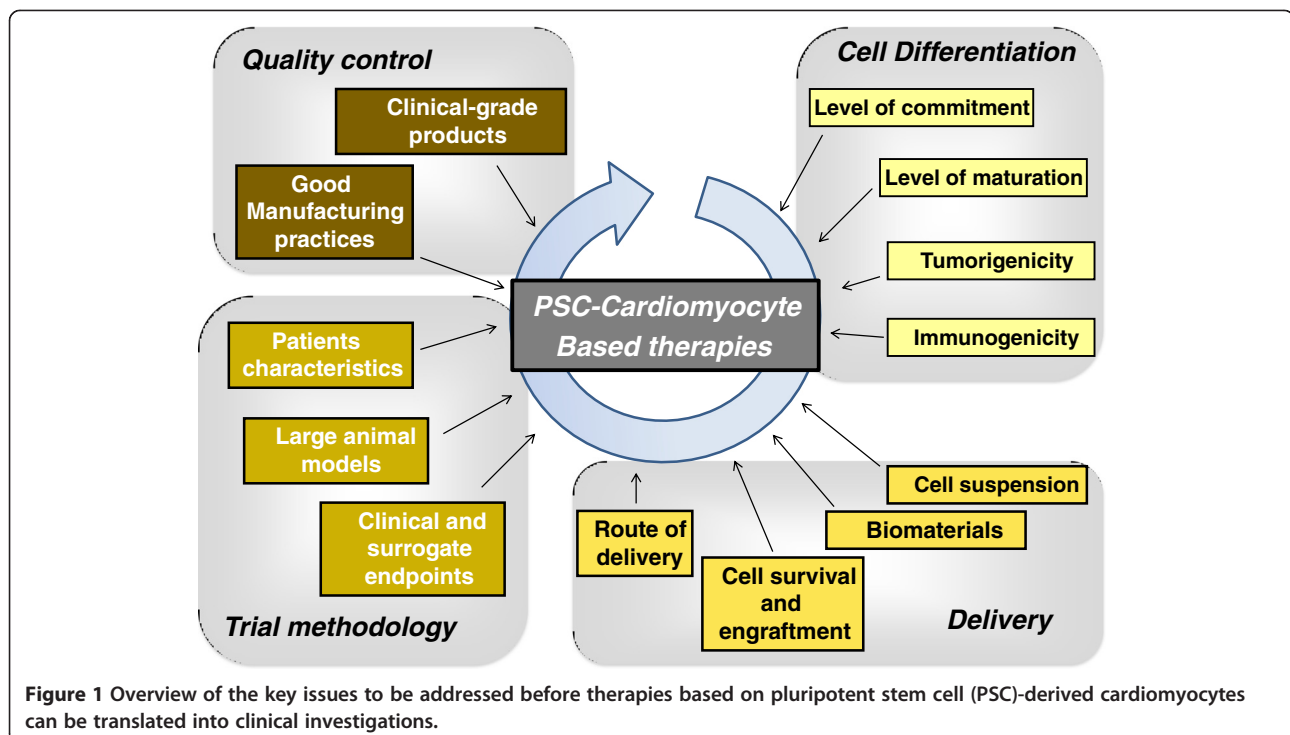
Generating good manufacturing practice and clinical-grade pluripotent stem cell lines

Good manufacturing practice (GMP) criteria have been established by both the European Medicines Agency and the Food and Drug Administration to ensure optimally defined quality and safety in cell transplantation studies. The directive and guidelines are progressively evolving but include requirements for cell therapy products, including PSCs [15]. GMP is a requirement for good clinical practice

and requires the development of standardized operating procedures and quality control methodology for the entire process from cell generation to storage of the cell therapy products [16]. For example, appropriate safety testing will be required for all animal-derived products. The use of feeder-free derivation protocols and the development of specific culture conditions that avoid xeno-components but rather use GMP-quality human derivatives would be preferable. Similarly, the generation of clinical-grade iPSCs with the use of virus-free non-integrative reprogramming techniques is probably desirable in the future. It is beyond the scope of this review to detail all the requirements to achieve a GMP-level cell product, but it is worth mentioning that the generation of clinical-grade PSCs is a critical first step toward future applications [16]. Even though the use of human ESCs and the derivation of iPSCs have become very popular during the past years and have been implemented in many research laboratories, the development of GMP-grade PSCs will require significant effort and resources that might be supported by a much smaller number of laboratories.

Defining the ideal level of differentiation

Different studies have clearly established that ESCs and iPSCs can differentiate into myocytes with some structural and functional properties of cardiomyocytes [9,17]. The differentiation is, however, heterogeneous, raising concerns about the persistence of undifferentiated



pluripotent cells in the cell mixture. The ability of undifferentiated ESCs to form teratomas, an encapsulated tumor that contains tissue components resembling normal derivatives of all three germ layers, when transplanted into normal or diseased hearts has been reported by different groups [18,19]. These concerns might even be stronger for iPSCs, as reprogramming and *in vitro* culture of these cells can induce genetic and epigenetic abnormalities [20,21]. As a consequence, ESCs or iPSCs will require some degree of pre-differentiation to restrict their differentiation repertoire and prevent tumor growth. Significant efforts are thus being made to optimize culture conditions for the generation of cardiac-committed cells from PSCs. Applying knowledge in developmental biology has guided the development of most of these protocols. *In vitro* cardiomyocyte differentiation mimics the process of cardiogenesis *in vivo*. The generation of human PSC-derived cardiomyocytes has primarily been performed through embryoid body formation [22,23] but is highly increased when human PSCs are exposed to activin A and bone morphogenic protein 4 [24]. Different types of cardiomyocytes, including atrial-, ventricular-, and nodal-like cells, are formed, however, which might not be optimal for cell transplantation purposes where highly homogenous populations of each cardiac subtype is desirable. The inhibition of the Wnt signaling pathway in later stages of the differentiation process has recently been associated with a marked increase in the production of ventricular-like cardiomyocytes [25,26].

Different cell sorting strategies based on surface markers, differences in glucose and lactate metabolism or labeling with some fluorescent dyes have also been proposed to generate highly purified populations of PSC-derived cardiomyocytes (up to 99% purity) [27-29]. Some studies have suggested that even a low number of undifferentiated cells might be sufficient to induce teratoma formation [30]. Using these methods, the potential contamination with undifferentiated cells should be kept under the level of concern. Accordingly, several studies found no teratomas in hearts transplanted with cardiomyocytes or cardiac progenitors derived from purified ESCs [17,31], suggesting the risk of tumor formation might be quite low after appropriate cell preparation. However, further analysis of the therapeutic potential of PSCs and their progeny, including the risk of teratoma-forming propensity in animal models with long-term follow-up, is required before cell therapy with human PSCs can advance to clinical trials.

Using the current techniques of differentiation, PSC-derived cardiomyocytes appear to be less mature than adult cardiomyocytes. Maturation of PSC-derived cardiomyocytes is, however, improved in the long term (>80 days of *in vitro* differentiation and culture) [32] or by inducing adult-like metabolism with specific medium

[33]. However, whether more mature cells are preferable for cell transplantation experiments remains unclear. There is an intuitively attractive idea that the adult mammalian heart provides a 'cardiogenic environment' that will drive maturation and orientation of cardiac myocytes from pluripotent stem cells. Transplanted immature cells would have the opportunity to further mature *in vivo* [34]. In addition, the use of less differentiated but mesoderm-committed PSC-derived cells might not only restore myocardial tissue but could also contribute to revascularization. Further investigations are now needed to determine the ideal level of differentiation for cell transplantation using PSC-derived cardiomyocytes.

Avoiding the rejection of transplanted cells

As transplanted PSC-derived cardiomyocytes might not be of patient origin, the possibility of an immune response must be addressed [35]. Transplant rejection is mainly driven by allelic differences in the surface antigens expressed by the donor and recipient. There are three distinct types of transplantation antigens: ABO blood group antigens, minor histocompatibility antigens and major histocompatibility complex (MHC) molecules. Allelic differences in MHC molecules are, by far, the most significant immunological barrier to organ transplantation. Undifferentiated human ESCs are sometimes called 'immunoprivileged' because they express low levels of class I MHC (MHC-I) molecules [36-38]. However, MHC-I expression increases approximately 10-fold with the induction of differentiation [38]. Stem cell graft rejection may be triggered when the recipients' allogeneic T cells recognize the foreign MHC-I surface molecules, whether differentiation occurs before or after transplantation. A number of methods have been proposed to address immunorejection [39]. Among them, derivation of ESCs that have their MHC (also called human leukocyte antigen (HLA) in humans) matched with the patient's could be a potential method for minimizing immunorejection in ESC transplantation [40,41]. In contrast with ESCs, the development of iPSC-derived differentiated cells has been expected to provide personalized sources for cell-based therapy. However, the overall time to generate, expand and characterize patient-specific iPSCs creates an important barrier to the development of such personalized approaches. Moreover, iPSCs were originally believed to be non-immunogenic but recent data have raised concerns about the potential immunogenicity of these cells. A recent study reported that the transplantation of immature iPSCs induced a T-cell-dependent immune response even in a syngeneic mouse, likely due to abnormal gene expression [42]. This immunogenicity could be linked to the over-expression of minor antigens potentially resulting from point mutations in the coding sequences of iPSCs [20] or the epigenetic

regulation of iPSCs [43]. This observation was, however, not confirmed in two subsequent studies [44,45].

One strategy to address this issue and avoid the use of intensive immunosuppressive agents is to create a collection of PSCs with distinct MHCs that will match the majority of the general population. It has, for instance, been reported that the generation of 50 iPSC lines would be sufficient to cover 90% of the Japanese population [46]. The panels of HLA types would, however, be higher in populations with high genetic diversity, thus requiring the generation of a higher number of iPSC lines. These HLA-organized banks of PSCs would certainly help to limit the risk of rejection but might not eradicate the immunogenic risk because of the limited number of HLA-compatible loci and the level of HLA typing resolution [47].

Ensuring the survival and the engraftment of transplanted cells

The survival and integration of transplanted cells into the host is a critical challenge. The first evidence that ESC-based therapies can engraft and form myocardium *in vivo* came from small animal models where human ESC-based therapies were directly injected into the normal myocardium [48]. Further experiments were then performed in diseased conditions, especially in ischemic hearts. While in animal models the number of cells and injections may vary, the common concept is to deliver cells in or around the infarcted myocardium. Most of these studies have shown that the grafted PSC-derived cardiomyocytes are mainly found as confluent cell clusters in the infarct border zone [17,18]. Further investigations showed that left ventricular (LV) contractile function was improved (or at least its worsening was prevented) in treated animals compared to non-treated animals. However, extensive data indicate that most cells that were transplanted into the heart do not survive long-term. Cell retention and survival are consistently low when injected into the myocardium, and even lower with intracoronary infusion [17,49,50]. These data are also consistent with the results derived from clinical trials that have transferred different types of autologous cells (including skeletal myoblasts, hematopoietic stem cells and mesenchymal stem cells) into the human myocardium [4-6], which generally came to the conclusion that these cells do not form a significant amount of new myocardium over the long term. Several challenges need to be addressed to improve cell engraftment, retention and survival. As an example, a challenge relates to the orientation of transplanted cells in the heart architecture. The alignment of transplanted cells with the host myocardium would enhance the force generation. In addition, it is generally unclear if cell transplantation is associated with the development of an efficient blood flow to supply the transplanted cells.

Most of the pre-clinical experiments investigating PSC-based therapies were performed in small animal models, which might not be the most appropriate for clinical disease scenarios. The development of electromechanical junctions between transplanted cells and the surrounding host cardiomyocytes is required for synchronous contraction. However, it is likely that human ESC- or iPSC-derived cardiomyocytes have difficulties coupling to rodent host myocardium because human cells cannot keep up with a rodent's high heart rate. Although electromechanical coupling of human ESC-derived cardiomyocytes with host cells has been reported in guinea pigs [51], it has potentially been underestimated. Therefore, the use of large animal models for testing human-derived cardiac stem cell therapies is preferred. Large animal models do, however, have limitations, including the requirement of larger numbers of cells, the development of suitable immunosuppression protocols and higher costs. Different groups have reported the administration of PSC-derived therapies in pigs and monkeys [18,52,53]. ESC-derived cardiovascular progenitors (selected on the SSEA-1 cell surface marker) have been investigated in a Rhesus monkey model of myocardial infarction [18] created by a 90-minute coronary occlusion/reperfusion protocol; the selected cells were injected 2 weeks later in the infarcted area during open-chest surgery. These cells engrafted into the infarcted monkey hearts and differentiated into morphologically mature cardiomyocytes. In a recent study, Xiong and colleagues [53] reported the administration of iPSC-derived vascular cells in a swine model of myocardial infarction. The transplanted cells were engineered to express a fluorescent reporter (green fluorescent protein) and the engraftment rate was estimated to be about 7% after 1 week and about 2% after 4 weeks. Altogether, these studies suggest that improving cell survival over the long term is critical before considering future clinical applications [54].

Defining the optimal delivery route to the myocardium

An alternative approach to direct cell injection is to create a tissue-engineered version of cardiac muscle from human ESCs and iPSCs. In recent publications [55-57], it has been shown that the *ex vivo* combination of ESCs/iPSCs with polymeric scaffolds allows the generation of tissue-engineered muscle constructs. The engineered tissues show coherent contractions 5 to 10 days after casting. They display a dense network of longitudinally oriented, interconnected and cross-striated cardiomyocytes, suggesting that the three-dimensional tissue format improves the maturation of cardiomyocytes [55]. It has been suggested that a geometrically straight structure of the tissue and cyclic strain favor cardiomyocyte maturation [55]. In an early study, human bioengineered

cardiac tissues were transplanted onto the epicardium of a healthy athymic rat heart, showing graft survival and connection to the host myocardium and coronary circulation [56]. In another study [58], a composite construct made of adipose tissue-derived stromal cells and ESC-derived cardiac progenitors was applied surgically in monkeys that underwent myocardial infarction. Two months later, the progenitors had differentiated into cardiomyocytes and there was robust engraftment of the donor tissue associated with increased angiogenesis [58]. These data suggest that *in vivo* engraftment of engineered cardiac tissues created from ESC- or iPSC-derived cardiomyocytes represents an interesting alternative strategy to direct cell injection therapy. In addition to further investigations in pre-clinical models, the use of GMP-level materials would, however, be required for future clinical applications.

Analyzing the appropriate endpoints post-delivery

Studies evaluating stem cell-based therapies *in vivo* have primarily focused on the changes in LV function and in cardiovascular outcomes. The study methodology, sample size, type of cells and route of administration typically differ between these studies, but most have evaluated the changes in LV ejection fraction as a surrogate of the benefit of stem-cell based therapies. The primary assumption is that the transplanted cells will directly replace the failing tissue and contribute to cardiac contraction, and that the higher the number of cells being engrafted the more the ejection fraction will be increased. There is, however, a large controversy on the mechanisms by which stem cell-based therapies contribute to improving cardiac function [1]. In addition or in place of direct action on contraction, it is plausible that paracrine effects or changes in the myocardial response to injury have an important contribution. In a recent study investigating the functional consequences of human iPSC administration in a swine model of myocardial infarction [53], it was found that iPSC transplantation mobilizes endogenous progenitor cells in the heart, thus reducing LV remodeling. Even if the factors secreted or released from injected cells remain to be fully characterized, the 'paracrine concept' has become very popular among the scientific community.

As a consequence, one of the major objectives will now be to correlate cell engraftment with improvements in local and global cardiac function as well as improvements in morbidity and mortality. Several strategies has been proposed to track the fate of the transplanted cells, including genome editing for molecular imaging [59] and magnetic resonance imaging-based reporter gene technology [60]. Magnetic resonance imaging cell tracking is particularly appealing in cardiology as it would allow a simultaneous assessment of cell engraftment and cardiac function. This can be achieved through genomic engineering of the

transplanted cells or labeling these cells with super-paramagnetic iron oxide particles. These labeled cells might, however, only be compatible with pre-clinical studies. In a recent study conducted in 110 patients with dilated cardiomyopathy, cell homing of administered CD34+ cells was investigated by labeling a fraction of the cells with ^{99m}Tc-hexamethylpropylenamine and performing single-photon emission computed tomography imaging 2 and 18 hours after the intracoronary delivery [61]. The average cell retention rate was 5% at 18 hours after injection but correlated well with functional outcomes at 3 and 12 months, those patients with above-average cell retention demonstrating a significant increase in LV ejection fraction. This study clearly paves the way for the design of a new generation of clinical cell therapy trials [62]. In these studies numerous parameters would be recorded, including cell homing and localization, global cardiac function, hemodynamic parameters and also cardiac volumes and dimensions. The rise of multimodality imaging (including in small animals) provides opportunities to measure global cardiac function parameters (such as LV ejection fraction and LV volumes) and local changes in cardiac fibrosis, scar areas or perfusion markers. Furthermore, this array of parameters could be measured at early and late time points after transplantation to more comprehensively evaluate the full impact of PSC-based therapies.

Finally, it has been suggested that transplanted cells can rapidly diffuse from the heart to other organs (that is, lungs, liver, kidneys, spleen) [63]. Whether this phenomenon exists with PSC-derived cardiomyocytes remains to be determined. However, as for any experimental drug, appropriate biodistribution and toxicology studies will need to be performed in animal models before moving into clinical investigations.

Conclusion

PSCs represent an appealing cell type for developing cell replacement therapies. Different initiatives have been launched to promote their development toward clinical applications. However, ESC/iPSC technologies have several specific issues that remain to be overcome, including the development of GMP-level PSC lines, the development of efficient protocols to generate pure populations of cardiomyocytes, and the development of techniques to improve the retention and survival rate of transplanted cells. Once these are overcome, the first clinical trials will then be on the horizon.

Note: This article is part of a thematic series on *Cardiovascular regeneration* edited by Ronald Li. Other articles in the series can be found online at <http://stemcellres.com/series/cardiovascular>.

Abbreviations

ESC: Embryonic stem cell; GMP: Good manufacturing practice; HLA: Human leukocyte antigen; iPSC: Induced pluripotent stem cell; LV: Left ventricular; MHC: Major histocompatibility complex; PSC: Pluripotent stem cell.

Competing interests

The authors declare that they have no competing interests.

Published: 09 Jan 2014

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10.1186/scrt390

Cite this article as: Hulot et al.: Considerations for pre-clinical models and clinical trials of pluripotent stem cell-derived cardiomyocytes. *Stem Cell Research & Therapy* 2014, **5**:1