ORIGINAL RESEARCH

Synergistic Combination of an Intelligent Nanozyme and Radiotherapy for Treating Renal Cancer

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Background: Preserving nephrons while avoiding tumor recurrence during the treatment of renal cell carcinoma remains as a challenge in clinic. To achieve desired therapeutic outcome, we developed specific nanozymes based on the tumor microenvironment and evaluated its efficacy in combination with radiotherapy.

Methods: Herein, a hybrid nanozyme $CeO_2@Au$ -PEG nanocomposite nanoparticle (NPs) was developed for the treatment of renal tumor. It was composed of gold nanozyme decorated CeO_2 nanorods and exhibited both glucose-oxidase like by gold nanozyme and peroxidase-like catalytic activities. Due to the high metabolic rate of tumor cells, they take up a huge amount of glucose to survive and proliferate. Therefore, we generated $CeO_2@Au$ -PEG NPs, which exhausted glucose in the tumor tissue and generated hydrogen peroxide, depleting the source of energy and causing tumor cell death. Then the generated hydrogen peroxide was degraded by the peroxidase-mimicking properties of $CeO_2@Au$ -PEG NPs, elevating oxidative stress and thus enhancing tumor cell death. Moreover, due to the high mass nuclei of gold and cerium, they could further sensitize the tumors to radiotherapy and thus thoroughly eliminate tumors.

Results: With enough biocompatibility, $CeO_2@Au$ -PEG NPs showed superior ability to deplete glucose as well as enhance oxidative stress by producing reactive oxygen species in RENCA cells under ionizing irradiation. Moreover, $CeO_2@Au$ -PEG NPs greatly improved radiotherapy mediated tumor ablation in tumor bearing mice.

Conclusion: Systematic experiments demonstrated the synergistic therapeutic effects of the combination of $CeO_2@Au-PEG$ NPs and radiotherapy in renal tumor model, which may serve as a promising strategy for treating renal cancer patients in the clinic. **Keywords:** nanozyme, radiotherapy, glucose consumption, reactive oxygen species, renal cell carcinoma

Introduction

According to the cancer statistics estimated in 2023, the incidence rate of tumors in the urinary system ranked among the top ten cancers.¹ Among all the estimated cases of urinary cancer, cancers occurring in the kidney and renal pelvis account for one-third of new diagnoses with renal cell carcinoma accounting for 90% of the cases with kidney cancer.² Surgery including partial nephrectomy as well as radical nephrectomy is widely performed during the treatment of renal cell carcinoma patients.^{3,4} Targeted therapies utilizing chemotherapeutic drugs and immunotherapy are being utilized as strategies for systemic therapy.⁵ However, it is necessary to preserve as much nephron as possible during the treatment of renal cell carcinome of cancer cells might lead to tumor recurrence.^{6,7} Therefore, to improve the patient's quality of life as well as inhibit tumor recurrence, researchers are exploring nanocomposites, which can specifically respond to the tumor microenvironment (TME) or can be tailored according to the tumor characteristics.^{8–10} The introduction of nanocomposite promotes tumor ablation without impairing kidney function, suggesting its promising potential for treating renal cell carcinoma patients.

Compared to normal tissues, tumor tissues with high metabolism tend to consume more glucose. Due to this, glucose oxidase (GOx) which catalyzes the conversion of glucose and oxygen to gluconolactone and hydrogen peroxide has gained increasing attention in the nanomedicine field.^{11–14} The energy depletion caused by these enzymes, and the release of hydrogen peroxide (H_2O_2) cause tumor cell death. In a recent study, tri-metal nanospheres decorated with glucose oxidase termed AuPtAg-GOx were engineered for synergistic tumor therapy via starvation therapy and photothermal therapy to

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augment immunotherapy efficacy. Under laser irradiation, the glucose depletion efficiency of AuPtAg-GOx was augmented, which enhanced the therapeutic outcome.¹⁵ Zhang et al reported a MnSiO₃@Met@GOx nanocomposite that could be triggered in mild-acidic pH and GSH overexpressing TME. H_2O_2 derived from glucose in the presence of the nanocomposite was converted to toxic hydroxyl radicals (OH) by decomposed Mn²⁺, leading to cell death and tumor ablation.¹⁶ To effectively inhibit glioma tumor recurrence after surgery, Li et al developed a sprayed gel containing GOx@MnCaP nanoparticles (NPs), which improved the therapeutic outcome. GOx decomposes glucose to produce H_2O_2 , which is then converted to cytotoxic reactive oxygen species (ROS) by Mn²⁺ to induce tumor cell apoptosis and suppress proliferation.¹⁷

Recently, enzyme mimicking nanocomposites termed nanozymes are extensively being investigated.^{18–20} Compared with natural enzyme, these nanozymes possess advantages such as physiological stability, suitability for mass production and high catalytic efficiency.^{21,22} Numerous nanozymes have been applied for treating cancers, owing to their catalase, superoxide dismutase, peroxidase (POD) or oxidase mimicking properties.^{23–25} Specifically, with high accumulation of H_2O_2 in the TME, nanozymes with peroxidase-mimicking property are capable of turning these H_2O_2 molecules into cytotoxic ROS, killing tumor cells. According to Dong et al, CaF₂ nanozyme was synthesized to enable Ca²⁺ release and ROS generation from ultrasonic (US) amplified POD-catalytic activity, which promoted Ca²⁺ overload and mitochondrial dysfunction. This strategy, based on CaF₂ nanozyme, showed enhanced ability to kill both breast tumor and liver tumor upon US exposure.²⁶ A titanium nitride-based nanoparticle termed TLGp was reported by Liu et al for photo-enhancing POD catalytic activity. GOx in TLGp produced abundant H_2O_2 , which was then converted to ROS to achieve tumor therapy while minimizing side effects.²⁷ In addition, Nan et al reported iron phthalocyanine-based Fe (II) Pc-A for cascade reaction, including POD, CAT and OXD activities, where H_2O_2 was decomposed to ROS to enhance oxidative stress in cancer cells and to realize multi-modal cancer therapy.²⁸

Ionizing irradiation is widely used for suppressing tumor growth and elimination of tumors. To completely ablate tumor tissues while protecting normal tissues and augment radiotherapy (RT) efficacy, numerous noble elements have been utilized to design nanoplatforms.^{20,29,30} Here, we constructed a novel nanozyme (CeO₂@Au-PEG) by decorating gold nanozyme on CeO₂ nanorods and then modified this nanocomposite with PEG. Under X-ray irradiation, energy deposited on both gold and cerium was enhanced, which further enhanced anti-tumor therapeutic efficacy of RT. Notably, although there is excessive amount of H_2O_2 in the TME compared with normal tissues, the ROS generated with the assistance of POD-mimicking nanozymes may not thoroughly eliminate tumor cells, leaving the possibility for tumor recurrence. Considering that abundant H_2O_2 is produced via the process of glucose oxidization, this nanozyme was designed to possess dual-catalytic properties including glucose-depletion as well as POD-mimicking activity (Scheme 1). In other words, it could produce sufficient H_2O_2 from intracellular glucose, which deprived cancer cells of the nutrients. Next, the generated H_2O_2 was decomposed into toxic ROS, inducing tumor cell death. Both in vitro and in vivo experiments demonstrated that the nanocomposites possessed desired biocompatibility, and that CeO₂@Au-PEG not only converted intracellular glucose into ROS by dual-catalytic properties, but also enhanced the cellular damage caused by ionizing radiation during RT to achieve highly efficient therapeutic outcome against renal cell carcinoma.

Results and Discussion

Preparation and Characterization of CeO₂@Au-PEG

The preparation of CeO₂@Au-PEG consisted of three steps, including the synthesis of porous CeO₂ nanorods with precursor of Ce(NO₃)₃·6H₂O and NaOH, loading of gold nanozyme on CeO₂ nanorods to obtain CeO₂@Au nanorods and decoration of polyethylene glycol (PEG) on nanorods to obtain CeO₂@Au-PEG nanocomposite (Figure 1a). As shown in Figure 1b, CeO₂ displayed the morphology of nanorods with a length of approximately 90 nm. CeO₂@Au was found to be composed of gold nanozyme coated around CeO₂ (Figure 1c). TEM images of Au-PEG were shown in Figure S1. Besides, the zeta potential of CeO₂, CeO₂@Au and CeO₂@Au-PEG were measured to be -11.5 mV, -21.0 mV and -23.0 mV, respectively. The change in zeta potential from -21.0 mV to -23.0 mV suggested the improved colloidal stability after PEGylation. After CeO₂@Au-PEG and Au-PEG were dissolved in phosphate buffered solution (PBS) for 24 h (Figure S2), the solution still remains uniform and clarified, demonstrating satisfied stability of CeO₂@Au-PEG and Au-PEG.

Next, X-ray diffraction (XRD) analysis was conducted to further confirm the structure of CeO_2 and $CeO_2@Au$. Several peaks corresponding to (1 1 1), (2 0 0), (2 2 0), (3 1 1), (2 2 2), (4 0 0) and (3 3 1) facets in XRD pattern of CeO_2 were identified

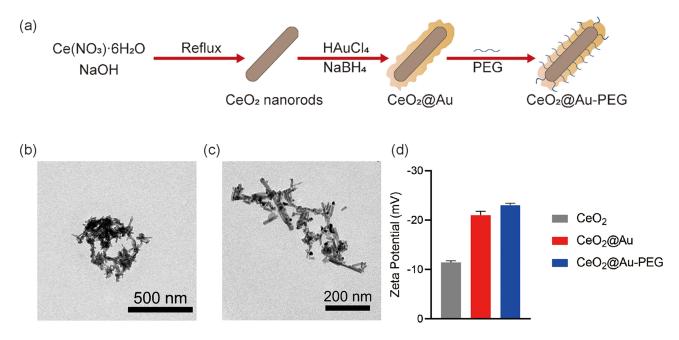


Figure I (a) Schematic illustration of the preparation of $CeO_2@Au$ -PEG nanocomposite NPs, TEM images showing the morphology of (b) CeO_2 and (c) $CeO_2@Au$, (d) Zeta potential of $CeO_2@Au$ and $CeO_2@Au$ -PEG NPs.

as shown in Figure 2a. Diffraction peaks representing gold nanozyme including (1 1 1), (2 0 0), (2 2 0) and (3 1 1) crystal plane were observed in the XRD pattern of CeO₂@Au (Figure 2b). X-ray photoelectron spectroscopy (XPS) wide scan spectra of CeO₂ and CeO₂@Au are displayed in <u>Figures S3</u> and 2c. It can be seen that cerium and oxygen were present in the obtained CeO₂. And XPS spectra of CeO₂@Au showed typical peaks including Ce 3d, O 1s and Au 4f, confirming the existence of cerium, oxygen and gold. Further investigation of high-resolution spectra of cerium from CeO₂ and CeO₂@Au are shown in <u>Figures S4</u> and 2d, which possessed similar binding energy peaks. Typically, the Ce 3d spectra of CeO₂@Au showed five

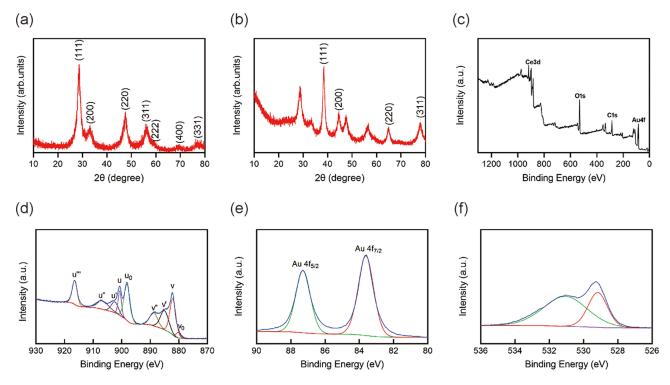


Figure 2 (a and b) XRD patterns of CeO2 and CeO2@Au NPs. (c) XPS analysis of CeO2@Au NPs. (d-f) High-resolution XPS spectra of Ce 3d, Au 4f and O 1s.

peaks labeled u and five peaks labeled which can be attributed to $3d_{5/2}$ and $3d_{3/2}$ respectively. Moreover, the binding energy peaks of gold in the high-resolution spectra at 87.6 eV and 83.8 eV were attributed to $4f_{5/2}$ and $4f_{7/2}$ respectively. The binding energy peaks at 531.3 eV and 529.6 eV were designated to surface oxygen and lattice oxygen (Figure 2e). The above results thus demonstrated the successful fabrication of CeO₂@Au-PEG.

Evaluation of the in vitro Catalytic Activity of the Nanocomposite

Endowed with dual-catalytic properties, CeO₂@Au-PEG was internalized by cells, generating sufficient H₂O₂ from glucose, the primary source of cellular energy. Next, H₂O₂ was then converted to ROS by POD-mimicking properties of CeO₂@Au-PEG (Figure 3a). Ionizing irradiation caused significant damage in cells when treated in combination with CeO₂@Au-PEG. To evaluate these two reaction processes, both POD-mimicking catalytical activity and glucose consuming of CeO₂@Au-PEG were measured. The oxidation of glucose by gold nanozyme of CeO₂@Au-PEG can produce H₂O₂ and gluconic acid, resulting in a decrease in the pH value. As shown in Figure 3b, a reduction of pH values was seen as a consequence of gluconic acid generation, indicating the oxidation of glucose + Au-PEG (Figure 3c). The POD-mimicking activity was also measured using 3, 3', 5, 5' - tetramethylbenzidine (TMB), which turned blue in the presence of \cdot OH. As shown in Figure 3d, typical absorption peaks at wavelength of 450 nm increased as the concentration of CeO₂@Au-PEG increased, which was due to the generation of \cdot OH by the catalytic activity of CeO₂@Au-PEG. The solution became more blue as concentration of CeO₂@Au-PEG increased. This confirmed that CeO₂@Au-PEG contributed to production of \cdot OH derived from H₂O₂, which was in turn generated upon the oxidation of glucose.

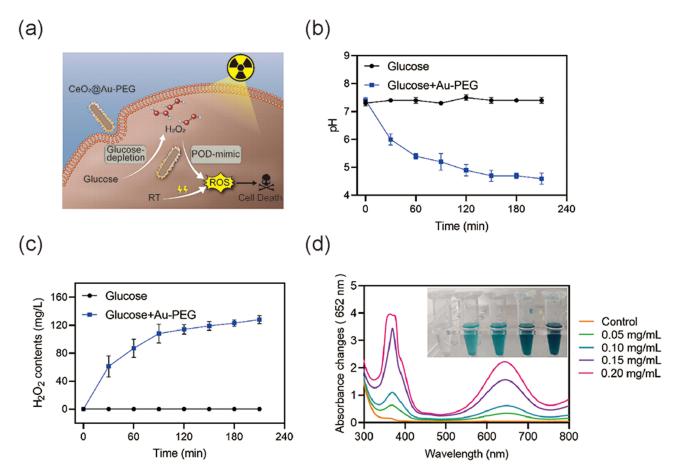


Figure 3 (a) Schematic illustration of ROS generation by CeO₂@Au-PEG in cells. (b and c) Evaluation of oxidation of glucose by measuring pH values and H_2O_2 concentration. (d) Evaluation of peroxidase-like activities of various CeO₂@Au-PEG concentrations.

Evaluation of the Catalytic Performance of CeO₂@Au-PEG in Cancer Cells

Inspired by the above results, we further evaluated the antitumor effects of $CeO_2@Au-PEG$ in vitro. Before the application of $CeO_2@Au-PEG$ to cancer cells, it was necessary to confirm its biocompatibility. Cytotoxicity of $CeO_2@Au-PEG$ was tested at various concentrations on tubular epithelial cells (TECs) and murine renal adenocarcinoma RENCA cells. As shown in Figure 4a, no obvious decrease of cell viability was observed in both cell lines. And over 80% cells survived at a concentration of 200 µg/mL. After PEGylation, Cy 5 labeled-CeO₂@Au-PEG exhibited rapid cellular uptake 1 h after co-incubation

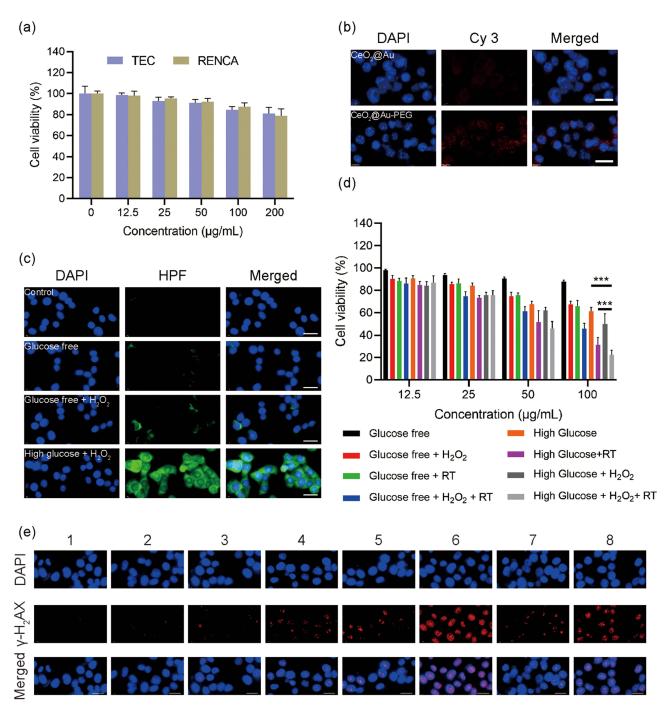


Figure 4 (a) Viability of TEC and RENCA cells pre-treated with CeO₂@Au-PEG. (b) Cellular uptake of Cy 5 labeled CeO₂@Au or CeO₂@Au-PEG by RENCA cells (Scale bar: 50 μ m). (c) Confocal fluorescence images showing 'OH generation in RENCA cells treated with CeO₂@Au-PEG at various concentrations using HPF probe (green) (Scale bar: 50 μ m). (d) Viability of RENCA cells measured by CCK8 assay after various treatments (Scale bar: 50 μ m). (e) DNA damage assessment by γ -H₂AX staining (Scale bar: 20 μ m; group 1: Glucose free, group 2: Glucose free+H₂O₂, group 3: Glucose free+RT, group 4: Glucose free+H₂O₂+RT, group 5: High glucose, group 6: High glucose+RT, group 7: High glucose+H₂O₂, group 8: High glucose+H₂O₂+RT). *** p < 0.001. Statistical analyses were conducted using t-test.

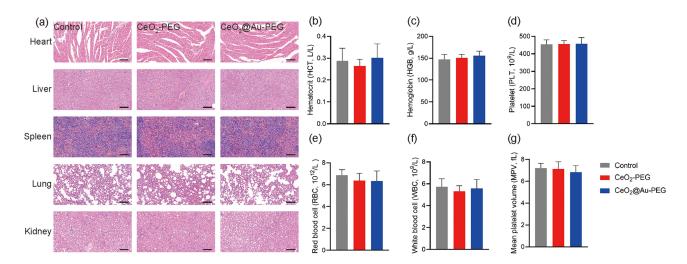


Figure 5 (a) H&E staining of excised organ tissues post injection of saline, CeO₂-PEG or CeO₂@Au-PEG NPs (Scale bar: 50 μm). (b-g) Blood routine analysis of mice under different treatment.

(Figure 4b). Moreover, the efficacy of RT was enhanced by CeO₂@Au-PEG in vitro. To investigate the amount of OH produced during this process, ROS-staining was conducted using HPF probes. As shown in Figure 4c, no apparent green fluorescence was observed in both the control and glucose free groups while a weak fluorescence was seen in the glucose free + H₂O₂ group, which could be attributed to the POD-mimicking property of CeO₂@Au-PEG. On the contrary, a significantly high level of ROS was detected in the high glucose $+ H_2O_2$ group, which was generated from the cascade catalytical reaction mediated by CeO₂@Au-PEG. Next, to validate the dual-catalytic activities on cells, 8 treatment groups were established, including glucose free, glucose free + H_2O_2 , glucose free + RT, glucose free + H_2O_2 + RT, high glucose, high glucose + H_2O_2 , high glucose + RT and high glucose + H_2O_2 + RT (Figure 4c). It can be seen that in the absence of glucose, CeO₂@Au-PEG showed a weak toxicity on RENCA cells. After the introduction of H_2O_2 , there was a decrease in cell survival due to the PODcatalytic activity of CeO₂@Au-PEG. In addition, cell viability was lower upon exposure to RT. The survival rate of cells in the glucose free + H_2O_2 + RT group decreased to 45.7% due to the therapeutic damage mediated by $\cdot OH$ generation and ionizing irradiation. Cells treated with high glucose only exhibited suppression due to ROS generation from CeO₂@Au-PEG mediated POD-mimicking process. When adding H_2O_2 , a decreasing in cell viability was observed thanks to outstanding POD-like property of CeO₂@Au-PEG. A slightly higher cell death was caused by high glucose + H_2O_2 + RT group than high glucose + RT group, which was due to the fact that the H2O2 level in mimicking tumor microenvironment was relatively low. In addition, with the addition of glucose and H₂O₂, CeO₂@Au-PEG suppressed the tumor cells, which was likely due to the ROS involved in cascade reaction of glucose oxidase and H2O2 depletion. Over 70% of RENCA cells were not viable in the high glucose + $H_2O_2 + RT$ group. Compared with the glucose free + $H_2O_2 + RT$ group, the presence of glucose greatly elevated the cytotoxicity of the nanocomposite. Furthermore, DNA damage post various treatments was assessed by γ -H₂AX staining (Figure 4e). Consistent with the result of CCK 8 assay, the most apparent red fluorescence was observed in the group treated with high glucose + H₂O₂ + RT, suggesting the most severe DNA damage in this group. Further investigation of the expression of caspase 3 in various group confirm the apparent cell apoptosis in CeO_2 @Au-PEG enhanced RT in glucose and H_2O_2 situation (Figures S6). Collectively, the above results indicated that CeO₂@Au-PEG was capable of catalyzing the conversion of intracellular glucose to ROS and decreasing tumor cell survival under RT.

Assessment of in vivo Biocompatibility

To confirm the biosafety of CeO₂-PEG and CeO₂@Au-PEG in vivo, main organs including heart, liver, spleen, lung and kidney of mice injected with saline, CeO₂-PEG or CeO₂@Au-PEG were analyzed by hematoxylin and eosin (H&E) staining (Figure 5a). No apparent lesions were observed in mice administrated with CeO₂-PEG or CeO₂@Au-PEG. Blood routine analysis of parameters including hematocrit (HCT), hemoglobin (HGB), platelet (PLT), red blood cell (RBC), white blood cell (WBC) and mean platelet volume (MPV) in Figure 5c-g demonstrated that blood samples from mice administrated with CeO₂-PEG or

 $CeO_2@Au-PEG$ were close to the values in the control group. These comprehensive results demonstrated that CeO_2-PEG and $CeO_2@Au-PEG$ had good biocompatibility in vivo.

In vivo Efficacy of CeO2@Au-PEG in a Mouse Model of Renal Cancer

To verify the anti-renal tumor efficacy of CeO₂@Au-PEG in combination with radiotherapy, subcutaneous tumors were established in BALB/c mice. First of all, biodistribution of CeO₂@Au-PEG in mice post injection via tail vein was analyzed. As shown in <u>Figure S6</u>, most apparent fluorescence intensity was detected in tumor region at 12 h post injection. Four groups were set up including the control, RT, CeO₂@Au-PEG and CeO₂@Au-PEG + RT groups. Tumor volume and body weight in each group were measured every 3 days and mice were executed on day 16 post treatment. As shown in Figure 6a and b, tumor volume in the group treated with PBS showed significant increase with time. Apparent tumor suppression was observed in the group treated with CeO₂@Au-PEG, thus proving the cascade catalytical reaction mediated by CeO₂@Au-PEG. However, therapeutic efficacy of either RT or CeO₂@Au-PEG alone failed to meet the demand for strong tumor inhibition. By striking contrast, the application of CeO₂@Au-PEG + RT dramatically impeded the tumor growth. Besides, by the end of tumor growth monitoring, tumor volume in the control group and RT

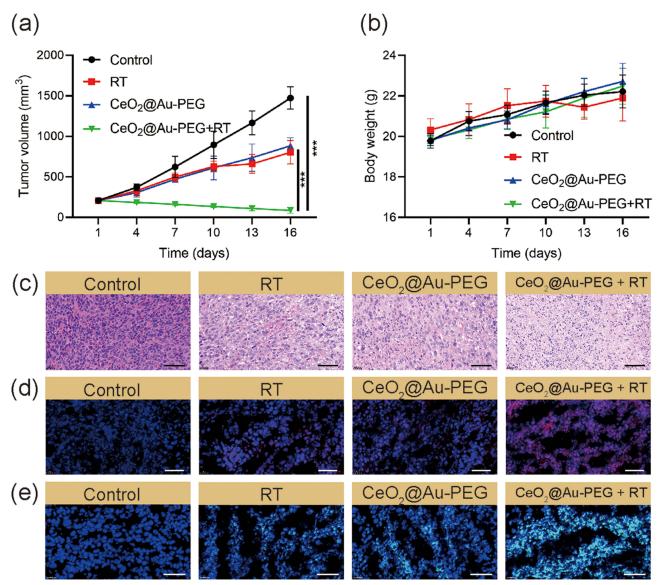


Figure 6 (a) The tumor growth curves and (b) body weight change curves during different treatments (n = 5). (c-e) H&E staining and dihydroethidium (DHE) staining and DCFH-DA staining of tumor tissues after various treatments (Scale bar: 50 μ m). *** p < 0.001. Statistical analyses were conducted using *t*-test.

group was 5 times and 3 times higher than that in the CeO_2 @Au-PEG group, respectively. The image of tumors in four groups in <u>Figure S7</u> further confirmed the results. There was no significant difference in the body weight of mice body among the four groups.

The in vivo effects of different treatments were evaluated by H&E staining and dihydroethidium (DHE) staining of the tumors. As shown in Figure 6c, moderate cell damages were observed in the RT group and CeO₂@Au-PEG group compared with the control group. H&E images demonstrated severe injuries in the CeO₂@Au-PEG + RT group. Consistent with the H&E staining results, the CeO₂@Au-PEG + RT group showed the brightest red fluorescence which was positively correlated to the amount of superoxide anion (O₂••). Meanwhile, green fluorescence representing hydroxyl radicals (•OH) further confirmed the generation of ROS by CeO₂@Au-PEG + RT in vivo.

Conclusion

In conclusion, a novel $CeO_2@Au$ -PEG nanocomposite with dual-catalytic activities was synthesized to enhance the antitumor efficacy of RT in a mouse model of renal cancer. On one hand, $CeO_2@Au$ -PEG could convert glucose in tumor cells into gluconic acid and H_2O_2 , due to its ability to oxidize glucose, cutting off the main source of energy to the cancer cells. On the other hand, the resultant H_2O_2 generated in this process was then decomposed into cytotoxic $\cdot OH$, causing cell damage. Moreover, composed of two noble elements, $CeO_2@Au$ -PEG enhanced the therapeutic efficacy of RT, leading to stronger anti-tumor effects. $CeO_2@Au$ -PEG showed great biocompatibility both in vitro and in vivo. After treating renal tumor bearing mice with $CeO_2@Au$ -PEG, the tumor cells internalized it, leading to a series of chain reactions which generated a large amount of ROS. Meanwhile, $CeO_2@Au$ -PEG amplified the therapeutic effects of RT. The tumor volume shrank remarkably in the group that received the combination of $CeO_2@Au$ -PEG + RT. In summary, our work provides a novel strategy to treat renal tumors via cascade reaction and radiosensitization mediated by $CeO_2@Au$ -PEG nanocomposite.

Acknowledgment

All animal procedures were performed in accordance with the protocol approved by the Ethics Committee of Laboratory Animal of Henan Provincial Chest Hospital ((Document No. 04-04 of 2021, Animal Ethics Committee). All animal experiments were in accordance with the animal ethics guidelines of the Animal Care and Use Committee of the Laboratory Animal Science Department of Henan Provincial Chest Hospital.

Author Contributions

All authors made a significant contribution to the work reported, whether that is in the conception, study design, execution, acquisition of data, analysis and interpretation, or in all these areas; took part in drafting, revising or critically reviewing the article; gave final approval of the version to be published; have agreed on the journal to which the article has been submitted; and agree to be accountable for all aspects of the work.

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Disclosure

The authors declare no conflict of interest.

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