

Review Article

Update on the Development of Toehold Switch-Based Approach for Molecular Diagnostic Tests of COVID-19

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A high volume of diagnostic tests is needed during the coronavirus disease 2019 (COVID-19) pandemic to obtain representative results. These results can help to design and implement effective policies to prevent the spread of severe acute respiratory syndrome coronavirus 2 (SARS-CoV-2). Diagnosis using current gold standard methods, i.e., real-time quantitative PCR (RT-qPCR), is challenging, especially in areas with limited trained personnel and health-related infrastructure. The toehold switch-based diagnostic system is a promising alternative method for detecting SARS-CoV-2 that has advantages such as inexpensive cost per testing, rapid, and highly sensitive and specific analysis. Moreover, the system can be applied to paper-based platforms, simplifying the distribution and utilization in low-resource settings. This review provides insight into the development of toehold switch-based diagnostic devices as the most recent methods for detecting SARS-CoV-2.

1. Introduction

Since its first identification in late 2019 in Wuhan, the People's Republic of China, the severe acute respiratory syndrome coronavirus 2 (SARS-CoV-2) has caused a global pandemic of coronavirus disease 2019 (COVID-19) [1, 2]. In April 2022, the Center for Systems Science and Engineering (CSSE) at Johns Hopkins University (JHU) announced in their COVID-19 dashboard that the pandemic has led to more than 490 million confirmed cases with more than 6 million deaths worldwide [3]. Besides increasing the burden on public healthcare systems, COVID-19 negatively impacts the global economic and social conditions [4]. Preventive methods such as social distancing, lockdowns, and travel restriction policies were considered effective in limiting the spread of SARS-CoV-2. Unfortunately, the consequences of these methods have weakened the global economy [5, 6].

In late 2020, the COVID-19 vaccination program was started [7–9], and by April 2022, there were more than 11 billion doses of vaccine administered, with more than 64%

of the world population having received at least one dose of the vaccine [10]. Although the number of vaccinated people kept increasing, preventive efforts to control the spread of COVID-19 via diagnostic tests are still critical. Efficient diagnostic tests are crucial to prevent the spread of SARS-CoV-2 infection by identifying positive individuals to be quarantined and preventing unnecessary quarantine of negative individuals [11, 12].

The most commonly used diagnostic tests for SARS-CoV-2 detection are nucleic acid amplification tests (NAATs), including reverse transcriptase real-time quantitative PCR (RT-qPCR). The workflow of RT-qPCR comprises the specimen sampling from patients, RNA extraction, conversion of purified RNAs to DNAs using reverse transcriptase (RT), and amplification of the obtained virus-originated DNA fragments. These fragments can detect unique viral RNA sequences in nucleocapsid (N), envelope (E), spike (S), or RNA-dependent RNA polymerase (RdRp) genes using the fluorescence signals [13, 14]. The mentioned method is currently considered the “gold standard” in COVID-19 diagnostics due to its high sensitivity and

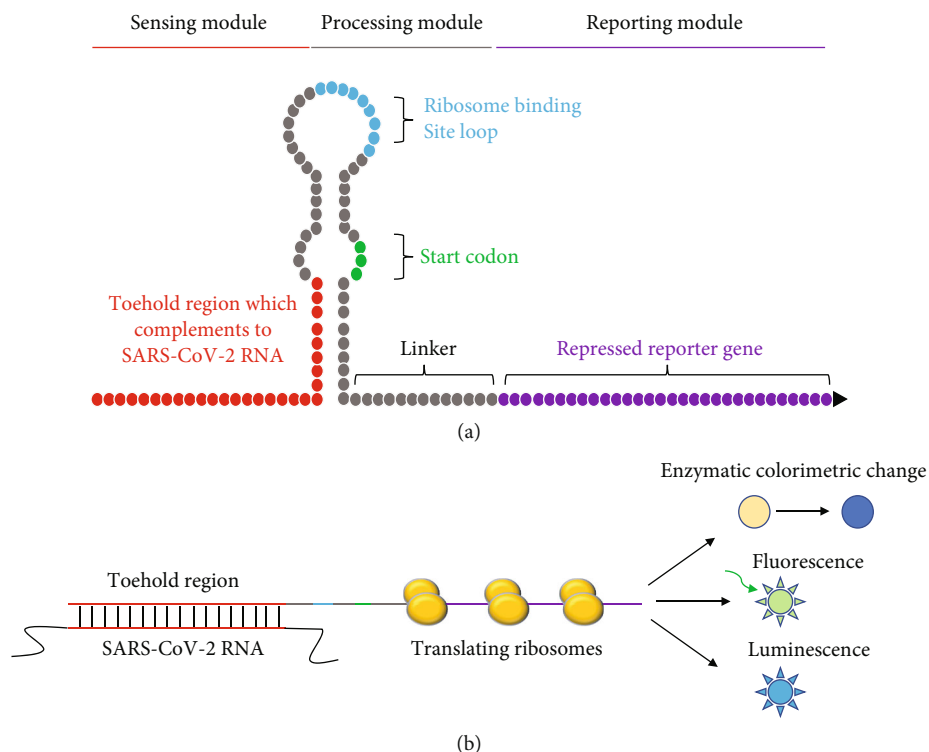


FIGURE 1: Toehold switch-based diagnostics for SARS-CoV-2. (a) General scheme of toehold switch riboregulator. In the absence of trigger RNA (SARS-CoV-2 RNA), RBS and start codon are hidden in the hairpin loop structure and inaccessible to the ribosome. (b) In the presence of SARS-CoV-2 RNA, the RBS and start codon are “released” to translate reporter genes, resulting in expression that acts as a signal detectable by naked eyes or specific instruments.

specificity and its straightforward quantitative analysis [15, 16]. However, SARS-CoV-2 diagnostic using RT-qPCR requires substantial hours and relatively expensive instruments, chemicals, and consumables to generate results [17]. Furthermore, the process involved, such as sample collection from patients, DNA purification and amplification, and result interpretation, requires skilled technicians, which increases the costs of the diagnostics [11, 18]. Consequently, various alternative techniques to detect SARS-CoV-2 RNA in patient’s samples are being developed to obtain a more cost-efficient and rapid method.

2. Synthetic Biology-Based Diagnostics

Synthetic biology combines molecular biology and engineering approach to create new biological functions [19]. Synthetic biology has enabled the construction of biological systems rationally and systematically [20]. Furthermore, as the synthetic biology field matured, most components and parts to build novel biological systems, including diagnostic systems, are standardized and cataloged [21, 22]. Those facts, coupled with the availability of various biological data and the advancement of *in silico* biological analysis, have allowed for more straightforward, rapid, and inexpensive development of diagnostic systems. [23, 24].

Among the emerging synthetic biology-inspired diagnostic platforms for COVID-19 are toehold switch- and clustered regularly interspaced short palindromic repeats/CRISPR-associated- (CRISPR/Cas-) based systems. Both

systems detect the genetic materials from pathogens and report the detection via visual signal.

The toehold-based system uses an RNA switch containing sequences complementary to the target SARS-CoV-2 RNA (Figure 1(a)) [18, 25]. The binding of target SARS-CoV-2 RNA will activate the reporter gene’s expression, resulting in a visually observed product. Meanwhile, the CRISPR/Cas-based systems involve CRISPR RNA (crRNA) that is specifically designed to bind the target pathogen DNA or RNA and activate the nonspecific cleavage activity of Cas nuclease (i.e., Cas12 and Cas13) to cleave quenched fluorescent DNA or RNA reporter [26–28]. The cleaved DNA or RNA reporter will emit a fluorescence signal which can be detected visually. Both systems can be applied to a paper-based and wearable platform that simplifies diagnosis, reduces analysis costs, and facilitates storage and deployment in areas lacking advanced infrastructures and medical experts [29].

Both systems have been developed to detect the presence of SARS-CoV-2 in patients’ samples, and comprehensive reviews on the CRISPR/Cas-based system for COVID-19 diagnosis were reported [30–32]. This review focuses on discussing the application of toehold switches for COVID-19 diagnosis.

3. Toehold Switch-Based SARS-CoV-2 Diagnostic Systems

Toehold switches are riboregulators that control gene expression via base pairing with target RNA sequences.

TABLE 1: Characteristics of currently developed toehold switch-based diagnostics for COVID-19.

Methods (references)	Amplification step	Viral RNA sources	Detection time	Observation results	Limit of detection	Estimated price per reaction
PHAsed NASBA-translation optical method (PHANTOM) [40]	Yes, isothermal NASBA (nucleic acid sequence-based amplification)	Nasopharyngeal swab samples	60-100 minutes	Naked eye, camera, and microplate reader	100 copies of viral RNA per sample	N/A
[41]	Yes, isothermal NASBA (nucleic acid sequence-based amplification)	Nasopharyngeal swab samples	60-120 minutes	Naked eye, camera, and microplate reader	1800 copies of viral RNA per sample	<1.00 USD
[42]	Yes, reverse transcription loop-mediated amplification (RT-LAMP)	Saliva	70 minutes	Naked eye, camera, and microplate reader	120 copies of viral RNA per sample	N/A
[43]	No	Saliva	Up to 7-12 minutes	Naked eye in the darkroom, camera	10 nM RNA per sample	<0.50 USD

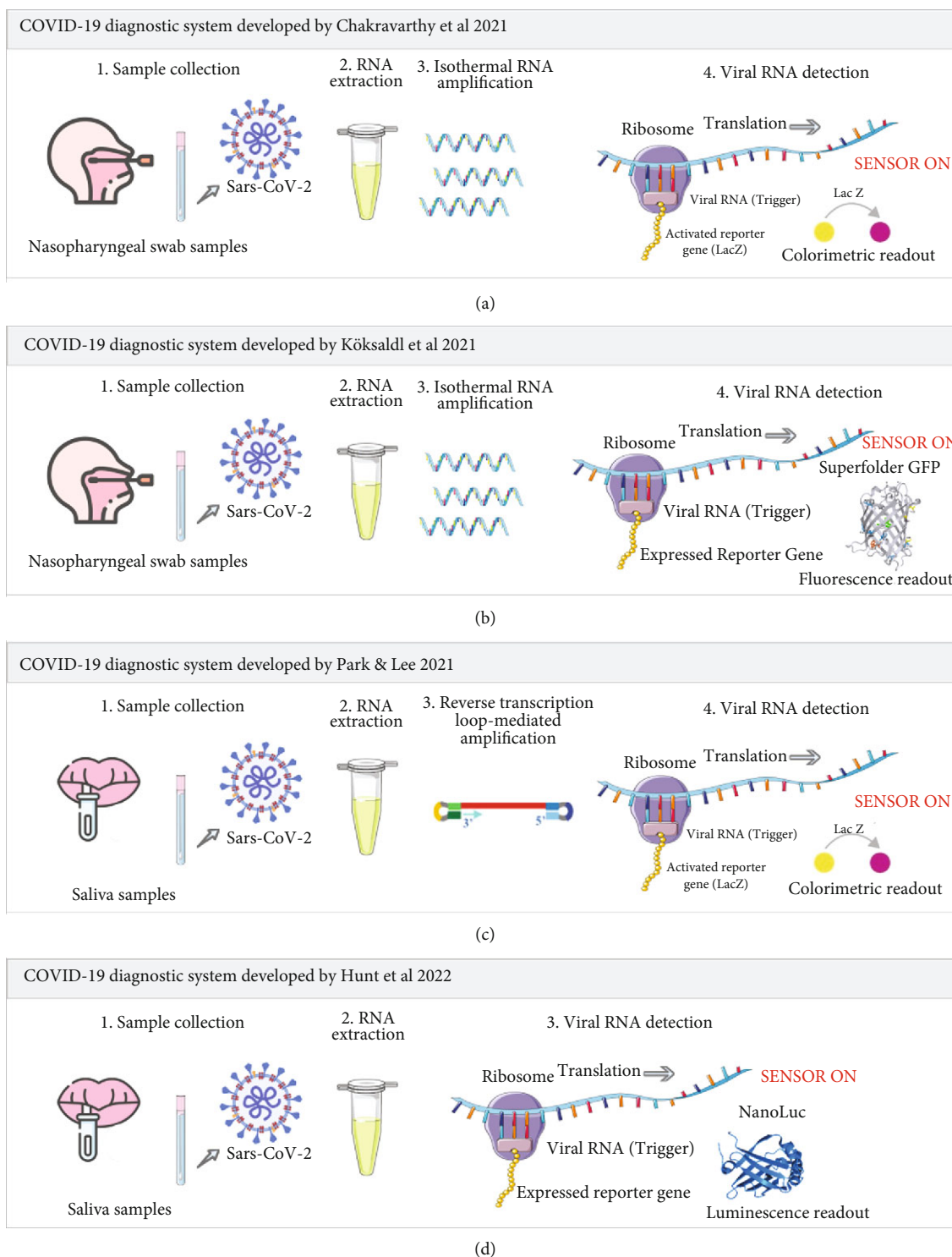


FIGURE 2: General scheme of the currently developed toehold switch-based diagnostics for COVID-19: (a) a system developed by Chakravarthy et al. [40] which utilized NASBA (nucleic acid sequence-based amplification) for amplifying trigger RNA from patient's nasopharyngeal swab sample and toehold switch-based biosensor with *lacZ* as a reporter gene, (b) a system developed by Köksaldı et al. [41] which utilized NASBA for amplifying trigger RNA from patient's nasopharyngeal swab sample and toehold switch-based biosensor with superfolder GFP as a reporter gene, (c) a system developed by Park et al. [42] which utilized reverse transcription loop-mediated amplification (RT-LAMP) for amplifying trigger RNA from patient's saliva sample and toehold switch-based biosensor with *lacZ* as a reporter gene, and (d) a trigger RNA amplification-free system developed by Hunt et al. [43] which detected SARS-CoV-2 RNA from patient's saliva sample using toehold switch-based biosensor with NanoLuc as a reporter gene.

The main component of toehold switches is the RNA hairpin structure which contains the ribosome binding site (RBS) sequence and start codon (AUG) [33]. The upstream region of the hairpin comprises a single-stranded toehold sequence complemented with the target RNA (trigger RNA). The binding of trigger RNA to the toehold sequence will open the hairpin structure and release the RBS, initiating the downstream reporter gene's translation (Figure 1(b)) [34]. The advantage of using a toehold switch as an RNA biosensing device lies in the unpaired nature of the toehold sequence that can be designed to detect a wide range of trigger RNA, including full-length mRNA. Those features enable the utilization of riboregulators in various applications [35].

Pardee et al. [36] have successfully applied the toehold switch for diagnostic purposes. The portable diagnostic device consisted of a plasmid with the toehold switch and reporter gene encoding sequences, *in vitro* cell-free transcription, and translation systems that were immobilized onto paper or other porous materials [37]. The device successfully detected antibiotic resistance genes, Ebola virus, Zika virus, dengue virus, and various gut bacteria with high specificity and sensitivity [38, 39].

As demonstrated previously, the toehold switch-diagnostic devices were stable for long-term storage at room temperature, enabling the use of the device area with limited medical resources. Furthermore, such diagnostic devices can be designed based on the sequence of the genetic materials of the target pathogen, enabling a short design for the production cycle. Finally, the devices can cost as little as 0.04 USD per sensor using an in-house cell-free expression system than 4.00 USD (reagents only) for PCR-based tests [36, 38].

The development of toehold switch-based COVID-19 diagnostic devices has been reported since 2021 (Table 1). Chakravarthy et al. [40] developed PHAsed NASBA-translation optical method (PHANTOM), a toehold switch-based biosensor coupled with isothermal NASBA (nucleic acid sequence-based amplification) to detect the SARS-CoV-2 genome (Figure 2(a)). In the PHANTOM system, RNA from SARS-CoV-2 in a patient's sample was extracted and then amplified isothermally using NASBA. A specifically designed toehold-based biosensor then detected the 36-nt amplification product (trigger RNA) in an *in vitro* transcription-translation (IVTT) assay. As a reporter gene, *lacZ* produces β -galactosidase to catalyze the colorimetric reaction of substrates such as ortho-nitrophenyl- β -galactoside (ONPG) or chlorophenol red- β -D-galactopyranoside (CPRG). The PHANTOM system can efficiently detect the presence of viral RNA in patient samples, which correlated well with the Ct value from the RT-qPCR test.

A similar system was developed by Köksaldı et al. [41] which coupled NASBA with a toehold switch-based biosensor to detect trigger sequences from the S gene and ORF1ab of SARS-CoV-2 that cost less than 1.00 USD per reaction. In contrast with PHANTOM, this diagnostic system uses a superfolder green fluorescent protein (sfGFP) as a reporter gene (Figure 2(b)). The system successfully detected the SARS-CoV-2 RNA from the nasopharyngeal swab sample in a relatively short period, i.e., 60 minutes via highly sensi-

tive detectors of a microplate reader, or 2 hours through eye visibility with minimal requirement of 1800 viral RNA copies.

Park et al. [42] reported the development of a toehold switch-based COVID-19 diagnostic system with a relatively faster turnaround time than other similar systems. The diagnostic system coupled toehold switch-based biosensor with reverse transcription loop-mediated amplification (RT-LAMP) using *lacZ* as a reporter gene (Figure 2(c)). The diagnostic system detected SARS-CoV-2 RNA in the patients' saliva samples. The sensitivity of this system relies on its RT-LAMP strategy, which can amplify 120 copies of target SARS-CoV-2 RNA in 20 minutes. The short amplification time shortens the overall target RNA detection to only 70 minutes.

Finally, Hunt et al. [43] reported the toehold switch-based COVID-19 diagnostic device that did not require an amplification step. The system comprises lyophilized cell-free protein synthesis (CFPS) and toehold switch riboregulator that can detect capsid protein gene region in the SARS-CoV-2 genome with NanoLuc as a reporter gene (Figure 2(d)). The system detected the presence of SARS-CoV-2 RNA in saliva samples in just 7 minutes with an estimated cost of 0.50 USD. Similar to the system developed by Park et al., the components of this diagnostic device, i.e., toehold switch module and IVTT, were successfully immobilized in paper matrices which simplified the distribution and utilization of the COVID-19 diagnostic system in developed and developing areas.

4. Conclusion and Future Perspectives

The ongoing COVID-19 pandemic has emphasized the importance of diagnostic testing in outbreak control [44, 45]. Efforts to end the COVID-19 pandemic require the accurate utilization of diagnostic testing in high volumes and the rapid use of the results to help implement the appropriate therapy and policy, preventing further disease spread [46]. Conducting such high throughput diagnostic tests is challenging, especially in areas with limited health personnel and infrastructures. The World Health Organization has developed the ASSURED (affordable, sensitive, specific, user-friendly, rapid and robust, equipment-free, and deliverable to end-users) criteria as a benchmark for diagnostics tests in resource-limited settings [47].

As described in this review, the currently developed toehold switch-based COVID-19 diagnostic has met the ASSURED criteria with low-cost, rapid, and highly sensitive and specific analysis advantages. Toehold switch-based COVID-19 diagnostics also provide more logistical benefits and ease of use than currently used diagnosis methods such as RT-qPCR. Furthermore, the short design to the production cycle of the diagnostics offers a valuable edge to cope with the emergence of new variants of SARS-CoV-2 [48].

To date, there are no commercial toehold switch-based diagnostics for COVID-19. To produce a commercial diagnostic test kit, it must pass clinical testing and trials, including benchmarking against existing diagnostic tools to ensure the quality of the analysis results [27]. Additionally, the

specificity and sensitivity of the toehold switch-based diagnostics for COVID-19 need to be evaluated in an in-field situation, where environmental conditions such as high temperatures, humidity, or dust might reduce the performance of the diagnostics [49].

Data Availability

The data related to this article are available from the corresponding author upon request.

Conflicts of Interest

The authors declare that they have no conflicts of interest.

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References

- [1] D. Chakhalian, R. B. Shultz, C. E. Miles, and J. Kohn, "Opportunities for biomaterials to address the challenges of COVID-19," *Journal of Biomedical Materials Research Part A*, vol. 108, no. 10, pp. 1974–1990, 2020.
- [2] A. Kumar, R. Singh, J. Kaur et al., "Wuhan to world: the COVID-19 pandemic," *Frontiers in Cellular and Infection Microbiology*, vol. 11, p. 242, 2021.
- [3] E. Dong, H. Du, and L. Gardner, "An interactive web-based dashboard to track COVID-19 in real time," *The Lancet Infectious Diseases*, vol. 20, no. 5, pp. 533–534, 2020.
- [4] S. A. Sarkodie and P. A. Owusu, "Global assessment of environment, health and economic impact of the novel coronavirus (COVID-19)," *Environment, Development and Sustainability*, vol. 23, no. 4, pp. 5005–5015, 2021.
- [5] W. McKibbin and R. Fernando, "The global macroeconomic impacts of COVID-19: seven scenarios," *Asian Economic Papers*, vol. 20, no. 2, pp. 1–30, 2021.
- [6] M. Mofijur, I. M. R. Fattah, M. A. Alam et al., "Impact of COVID-19 on the social, economic, environmental and energy domains: lessons learnt from a global pandemic," *Sustainable production and consumption*, vol. 26, pp. 343–359, 2021.
- [7] R. Al-Amer, D. Maneze, B. Everett et al., "COVID-19 vaccination intention in the first year of the pandemic: a systematic review," *Journal of clinical nursing*, vol. 31, no. 1–2, pp. 62–86, 2022.
- [8] S. Bagcchi, "The world's largest COVID-19 vaccination campaign," *The Lancet Infectious Diseases*, vol. 21, no. 3, p. 323, 2021.
- [9] E. M. Painter, E. N. Ussery, A. Patel et al., "Demographic characteristics of persons vaccinated during the first month of the COVID-19 vaccination program - United States, December 14, 2020-January 14, 2021," *Morbidity and Mortality Weekly Report (MMWR)*, vol. 70, no. 5, pp. 174–177, 2021.
- [10] H. Ritchie, E. Mathieu, L. Rodés-Guirao et al., "Coronavirus pandemic (COVID-19)," *Our World in Data*, 2020, <https://ourworldindata.org/coronavirus#citation>.
- [11] L. J. Carter, L. V. Garner, J. W. Smoot et al., "Assay techniques and test development for COVID-19 diagnosis," *ACS Central Science*, vol. 6, no. 5, pp. 591–605, 2020.
- [12] M. Iyer, K. Jayaramayya, M. D. Subramaniam et al., "COVID-19: an update on diagnostic and therapeutic approaches," *BMB Reports*, vol. 53, no. 4, pp. 191–205, 2020.
- [13] T. Kilic, R. Weissleder, and H. Lee, "Molecular and immunological diagnostic tests of COVID-19: current status and challenges," *iScience*, vol. 23, no. 8, article 101406, 2020.
- [14] M. Takahashi, M. Tehseen, R. Salunke et al., "Quick and easy assembly of a one-step QRT-PCR kit for COVID-19 diagnostics using in-house enzymes," *ACS Omega*, vol. 6, no. 11, pp. 7374–7386, 2021.
- [15] Y.-S. Chung, N.-J. Lee, S. H. Woo et al., "Validation of real-time RT-PCR for detection of SARS-CoV-2 in the early stages of the COVID-19 outbreak in the Republic of Korea," *Scientific Reports*, vol. 11, no. 1, article 14817, 2021.
- [16] C.-J. Lee, W. Shin, S. Mun et al., "Diagnostic evaluation of QRT-PCR-based kit and DPCR-based kit for COVID-19," *Genes & Genomics*, vol. 43, no. 11, pp. 1277–1288, 2021.
- [17] P. Khan, L. M. Aufdembrink, and A. E. Engelhart, "Isothermal SARS-CoV-2 diagnostics: tools for enabling distributed pandemic testing as a means of supporting safe reopenings," *ACS Synthetic Biology*, vol. 9, no. 11, pp. 2861–2880, 2020.
- [18] J. Gao and L. Quan, "Current status of diagnostic testing for SARS-CoV-2 infection and future developments: a review," *Medical science monitor: international medical journal of experimental and clinical research*, vol. 26, pp. e928552-1–e928552-7, 2020.
- [19] K. Bruynseels, "Responsible innovation in synthetic biology in response to COVID-19: the role of data positionality," *Ethics and Information Technology*, vol. 23, no. S1, pp. 117–125, 2021.
- [20] A. Courbet, E. Renard, and F. Molina, "Bringing next-generation diagnostics to the clinic through synthetic biology," *EMBO Molecular Medicine*, vol. 8, no. 9, pp. 987–991, 2016.
- [21] T. Decoene, B. De Paepe, J. Maertens et al., "Standardization in synthetic biology: an engineering discipline coming of age," *Critical Reviews in Biotechnology*, vol. 38, no. 5, pp. 647–656, 2018.
- [22] J. Santos-Moreno and Y. Schaerli, "Using synthetic biology to engineer spatial patterns," *Advanced Biosystems*, vol. 3, no. 4, article 1800280, 2019.
- [23] A. Gheraldi and E. A. Giri-Rachman, "Synthetic biology-based portable *in vitro* diagnostic platforms," *Alexandria journal of medicine*, vol. 54, no. 4, pp. 423–428, 2018.
- [24] T.-Y. Wei and C.-M. Cheng, "Synthetic biology-based point-of-care diagnostics for infectious disease," *Cell Chemical Biology*, vol. 23, no. 9, pp. 1056–1066, 2016.
- [25] T. Hoang Trung Chau, D. Hoang Anh Mai, D. Ngoc Pham, H. Thi Quynh le, and E. Yeol Lee, "Developments of riboswitches and toehold switches for molecular detection—biosensing and molecular diagnostics," *International Journal of Molecular Sciences*, vol. 21, no. 9, p. 3192, 2020.
- [26] J. S. Gootenberg, O. O. Abudayyeh, J. W. Lee et al., "Nucleic acid detection with CRISPR-Cas13a/C2c2," *Science*, vol. 356, no. 6336, pp. 438–442, 2017.
- [27] D. G. Sashital, "Pathogen detection in the CRISPR-Cas era," *Genome Medicine*, vol. 10, no. 1, p. 32, 2018.

- [28] J. S. Chen, E. Ma, L. B. Harrington et al., "CRISPR-Cas12a target binding unleashes indiscriminate single-stranded DNase activity," *Science*, vol. 360, no. 6387, pp. 436–439, 2018.
- [29] P. Q. Nguyen, L. R. Soenksen, N. M. Donghia et al., "Wearable materials with embedded synthetic biology sensors for biomolecule detection," *Nature Biotechnology*, vol. 39, no. 11, pp. 1366–1374, 2021.
- [30] U. Ganbaatar and C. Liu, "CRISPR-based COVID-19 testing: toward next-generation point-of-care diagnostics," *Frontiers in Cellular and Infection Microbiology*, vol. 11, 2021.
- [31] H. Rahimi, M. Salehiabar, M. Barsbay et al., "CRISPR systems for COVID-19 diagnosis," *ACS Sensors*, vol. 6, no. 4, pp. 1430–1445, 2021.
- [32] F. Safari, M. Afarid, B. Rastegari, A. Borhani-Haghighi, M. Barekati-Mowahed, and A. Behzad-Behbahani, "CRISPR systems: novel approaches for detection and combating COVID-19," *Virus Research*, vol. 294, article 198282, 2021.
- [33] A. A. Green, P. A. Silver, J. J. Collins, and P. Yin, "Toehold switches: de-novo-designed regulators of gene expression," *Cell*, vol. 159, no. 4, pp. 925–939, 2014.
- [34] J. C. Liang, R. J. Bloom, and C. D. Smolke, "Engineering biological systems with synthetic RNA molecules," *Molecular Cell*, vol. 43, no. 6, pp. 915–926, 2011.
- [35] S. Ausländer and M. Fussenegger, "Toehold gene switches make big footprints," *Nature*, vol. 516, no. 7531, pp. 333–334, 2014.
- [36] K. Pardee, A. A. Green, T. Ferrante et al., "Paper-based synthetic gene networks," *Cell*, vol. 159, no. 4, pp. 940–954, 2014.
- [37] S. Slomovic, K. Pardee, and J. J. Collins, "Synthetic biology devices for in vitro and in vivo diagnostics," *Proceedings of the National Academy of Sciences*, vol. 112, no. 47, pp. 14429–14435, 2015.
- [38] K. Pardee, A. A. Green, M. K. Takahashi et al., "Rapid, low-cost detection of Zika virus using programmable biomolecular components," *Cell*, vol. 165, no. 5, pp. 1255–1266, 2016.
- [39] M. K. Takahashi, X. Tan, A. J. Dy et al., "A low-cost paper-based synthetic biology platform for analyzing gut microbiota and host biomarkers," *Nature Communications*, vol. 9, no. 1, p. 3347, 2018.
- [40] A. Chakravarthy, A. Nandakumar, G. George et al., "Engineered RNA biosensors enable ultrasensitive SARSCoV-2 detection in a simple color and luminescence assay," *Life Science Alliance*, vol. 4, no. 12, article e202101213, 2021.
- [41] İ. Ç. Köksaldi, R. E. Ahan, S. Köse et al., "SARS-CoV-2 detection with de novo-designed synthetic riboregulators," *Analytical Chemistry*, vol. 93, no. 28, pp. 9719–9727, 2021.
- [42] S. Park and J. W. Lee, "Detection of coronaviruses using RNA toehold switch sensors," *International journal of molecular sciences*, vol. 22, no. 4, p. 1772, 2021.
- [43] J. P. Hunt, E. L. Zhao, T. J. Free et al., "Towards detection of SARS-CoV-2 RNA in human saliva: a paper-based cell-free toehold switch biosensor with a visual bioluminescent output," *New Biotechnology*, vol. 66, pp. 53–60, 2022.
- [44] O. Vandenberg, D. Martiny, O. Rochas, A. van Belkum, and Z. Kozlakidis, "Considerations for diagnostic COVID-19 tests," *Nature Reviews. Microbiology*, vol. 19, no. 3, pp. 171–183, 2021.
- [45] R. Wang, Y. Hozumi, C. Yin, and G.-W. Wei, "Mutations on COVID-19 diagnostic targets," *Genomics*, vol. 112, no. 6, pp. 5204–5213, 2020.
- [46] L. M. Bui, H. Thi Thu Phung, T.-T. Ho Thi et al., "Recent findings and applications of biomedical engineering for COVID-19 diagnosis: a critical review," *Bioengineered*, vol. 12, no. 1, pp. 8594–8613, 2021.
- [47] S. Smith, J. G. Korvink, D. Mager, and K. Land, "The potential of paper-based diagnostics to meet the ASSURED criteria," *RSC Advances*, vol. 8, no. 59, pp. 34012–34034, 2018.
- [48] R. Misra, S. Acharya, and N. Sushmitha, "Nanobiosensor-based diagnostic tools in viral infections: special emphasis on Covid-19," *Reviews in medical virology*, vol. 32, no. 2, 2022.
- [49] A. Niemz, T. M. Ferguson, and D. S. Boyle, "Point-of-care nucleic acid testing for infectious diseases," *Trends in biotechnology*, vol. 29, no. 5, pp. 240–250, 2011.