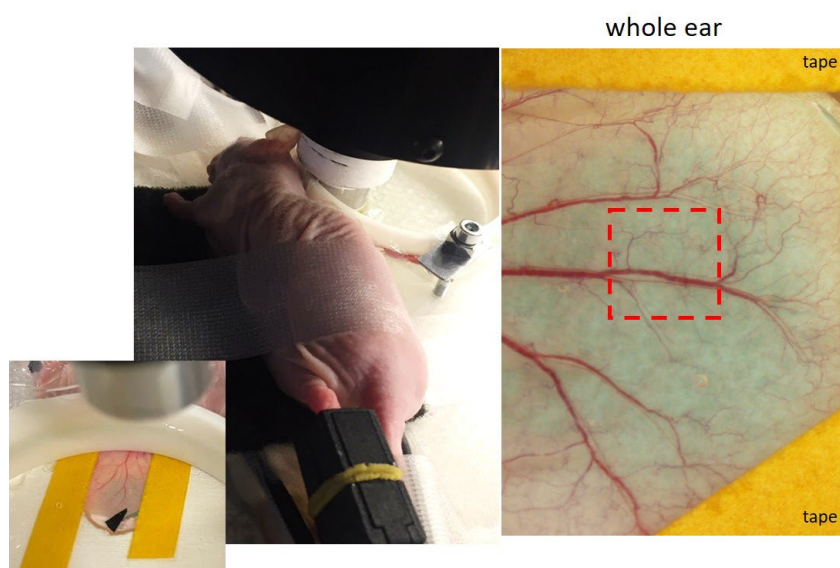


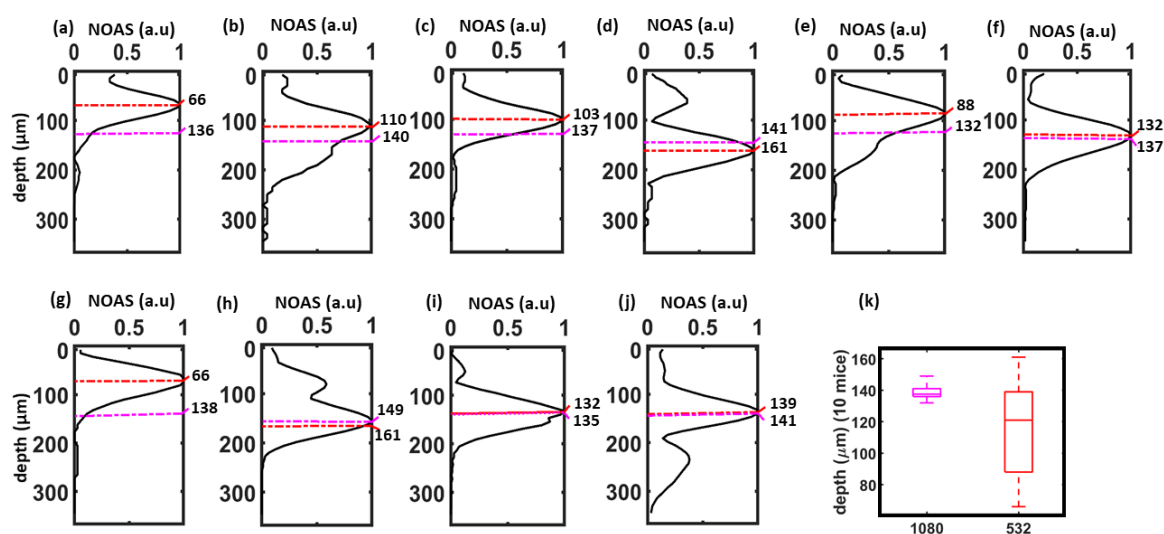
Non-invasive measurements of blood glucose levels by time-gating mid-infrared optoacoustic signals

In the format provided by the
authors and unedited

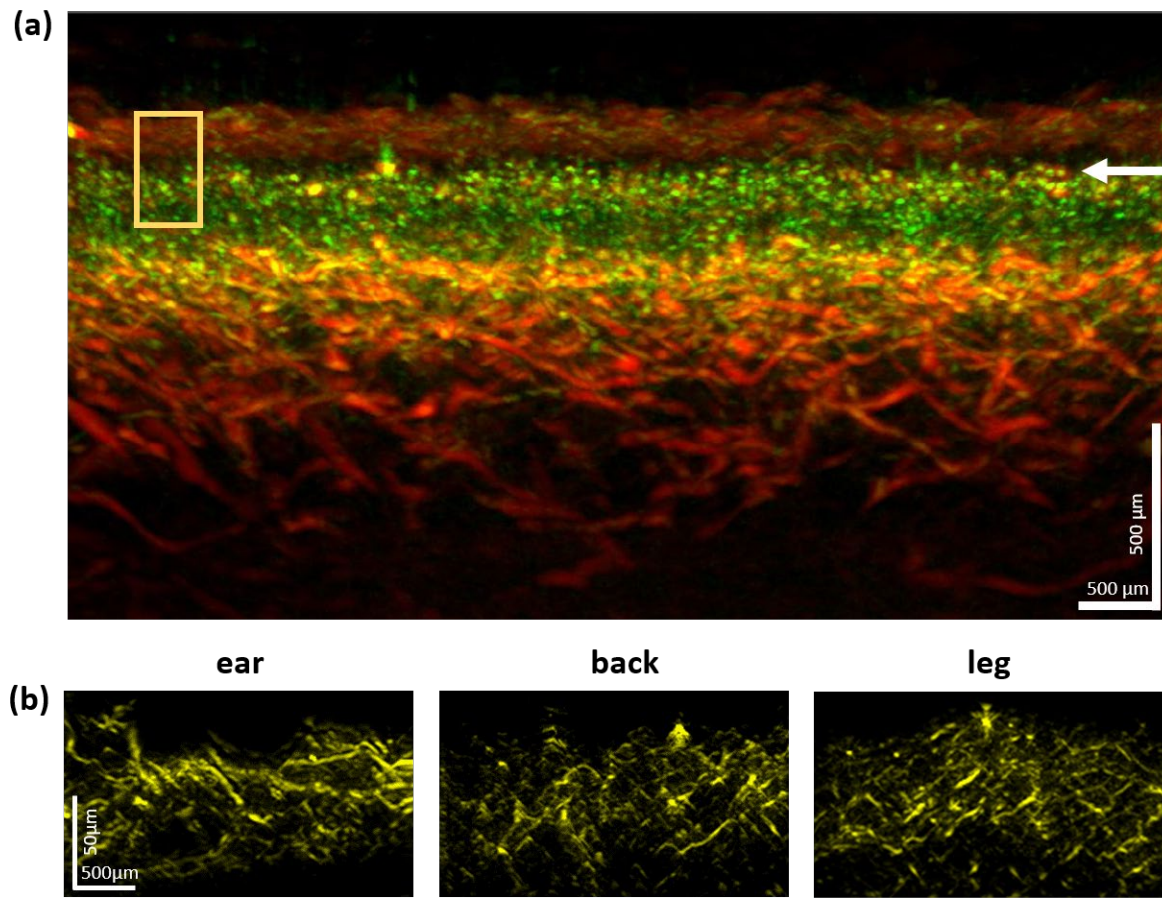
Supplementary Figures



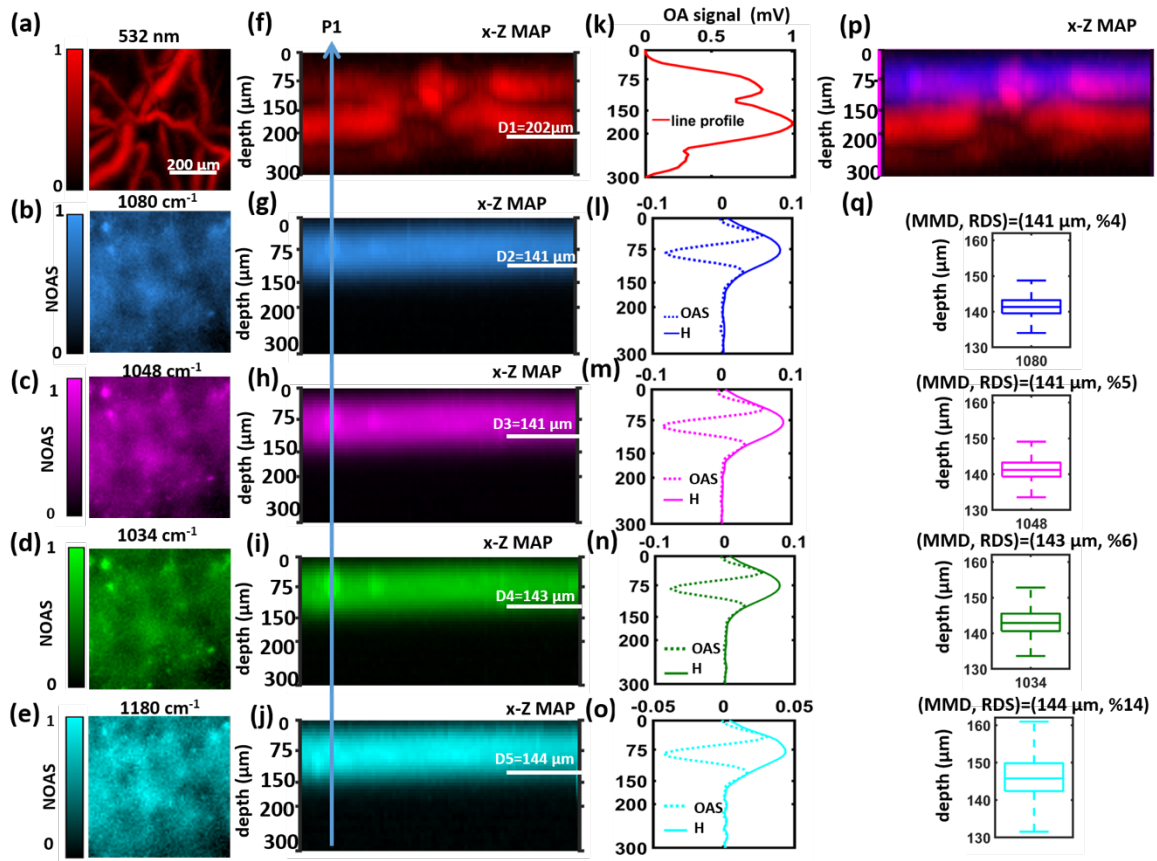
Supplementary Figure 1: Photograph of a mouse ear showing the scanning area. Photographs (from ten independent experiments) showing positioning of an anesthetized mice and mouse ear vasculature. A scanning area of 70x70 points, indicated by red-dashed line, was measured in all 10 mice.



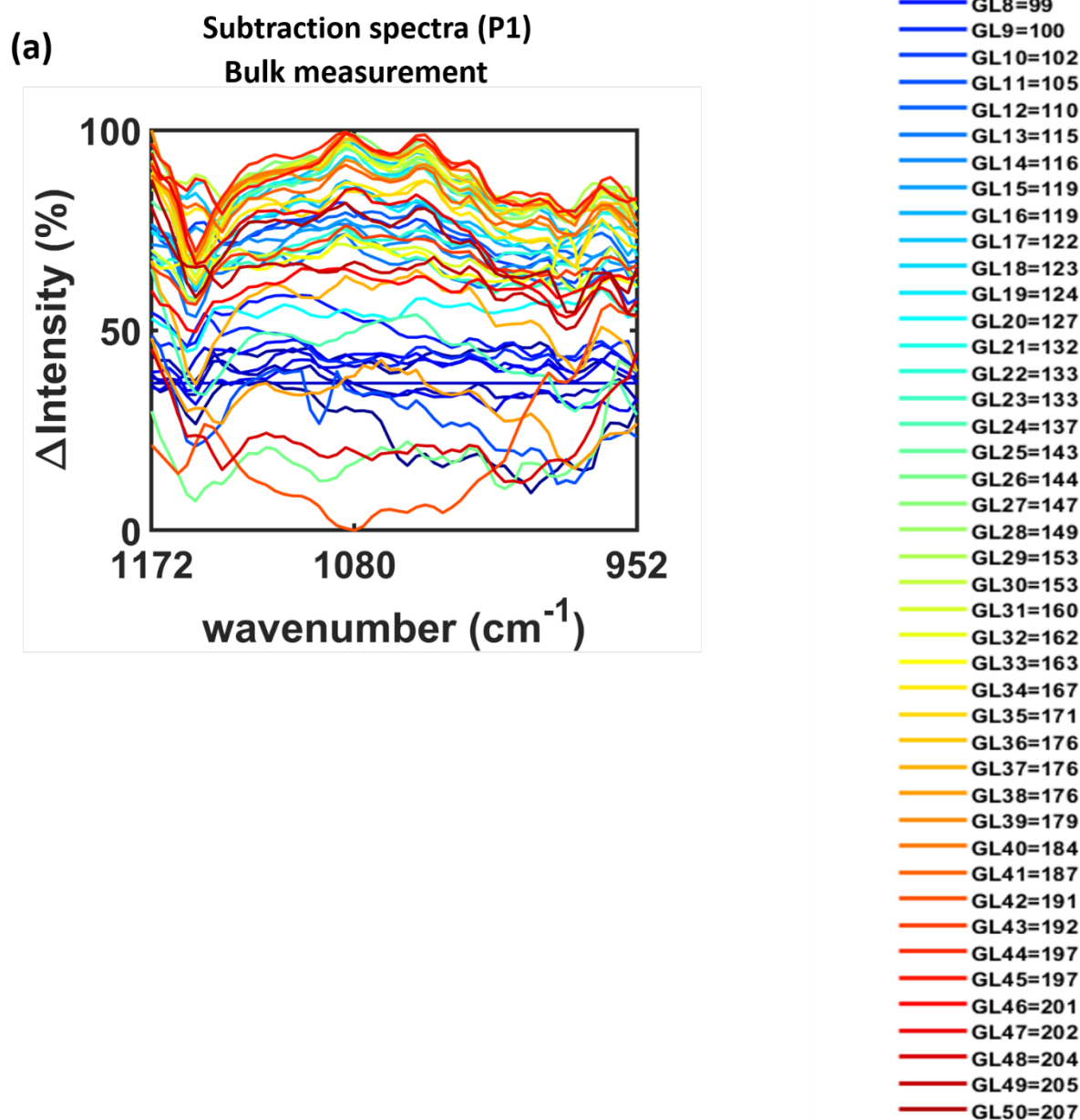
Supplementary Figure 2: Comparative DIROS/VIS-OA depth analysis at 1080 cm⁻¹ and 532 nm for ten mice experiments. (a-j) Depth contrast profiles at P1 (blood vessel location) for 532 nm excitation. The penetration depth ($1/e^2$ of the Hilbert transform) at P1 for 1080 cm⁻¹ and the depth for the maximum intensity obtained for blood vessels at 532 nm, are indicated by magenta and red dashed lines, respectively. (k) Comparison of the depth distribution of blood vessels (obtained at 532 nm) and the distribution of penetration depths reached by DIROS (at 1080 cm⁻¹), summary of 10 mice. NOAS = normalized optoacoustic signal; box plots indicate the upper and lower quartiles (box limits), median (center line) and minimum and maximum values (whiskers).



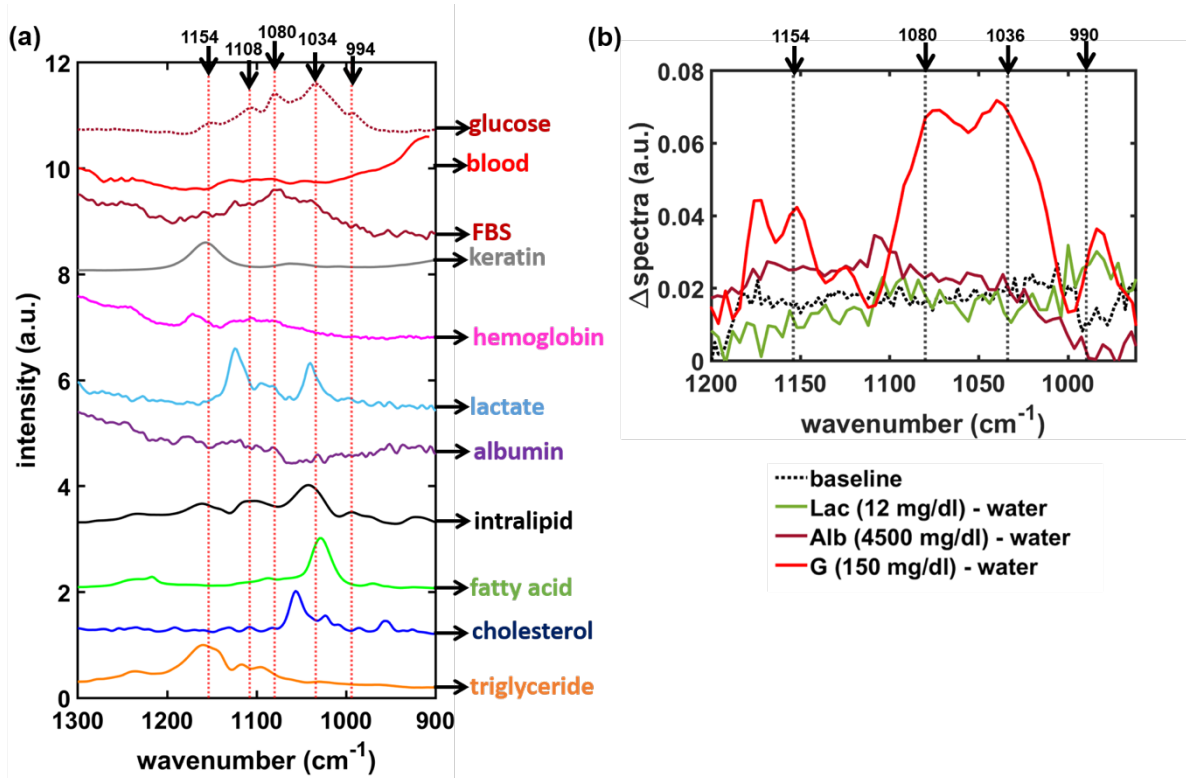
Supplementary Figure 3: Cross-sectional raster-scan optoacoustic mesoscopy images from human and mice skin. (a) Cross-sectional raster-scan optoacoustic mesoscopy (RSOM) image of human skin. The arrow points to the epidermal-dermal junction, which is a superficial layer rich in micro-vasculature. Green color marks the capillary loops in this layer. The yellow box indicates the depth scanned by DIROS, according as showcased in **Fig. 1**. Reproduced from Aguirre J., et al., *Nature Biomedical Engineering* (2017).³² (b) Cross-sectional RSOM images of the mouse ear, back and leg. Representative example from 3 independent measurements (n=3). Similar microvasculature distribution is found at different mice skin locations.



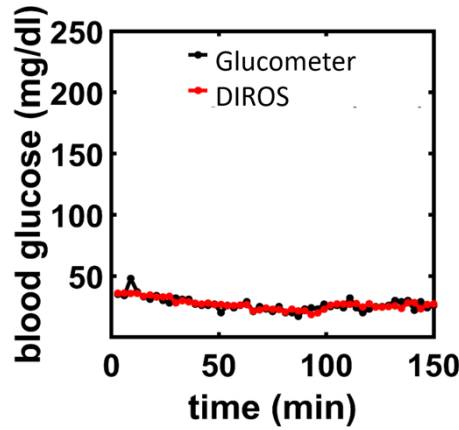
Supplementary Figure 4: Imaging depths achieved by DIROS in mouse skin *in vivo*. Representative xy-projected mouse ear images obtained from 3 independent experiments at (a) 532 nm, (b) 1080 cm⁻¹, (c) 1048 cm⁻¹, (d) 1034 cm⁻¹, and (e) 1180 cm⁻¹, (f-j) Maximum projections of corresponding xy images (a-e). (k) Line profile of blood vessels at P1 (blue line on panel f). (l-o) Depth profiles of mid-infrared (IR) optoacoustic (OA) transients with Hilbert transform at P1 (blue line on panels g-j). (p) Merged visible (f) and mid-IR (g) optoacoustic images. (q) Mean maximum depths achieved by DIROS at 1080 cm⁻¹, 1048 cm⁻¹, 1034 cm⁻¹, and 1180 cm⁻¹ for 4900 measurement points on mouse skin; box plots of optoacoustic contrast for each channels in the micrographs (g-j) indicating the upper and lower quartiles (box limits), median (center line) and minimum and maximum values (whiskers). 3 biologically independent samples were used for the experiments (n = 3). All the data are presented as mean values +/- SEM. H – Hilbert transform, MMD – mean maximum depth, NOAS – normalized optoacoustic signals, OAS – Optoacoustic signal, SEM–standard error of mean.



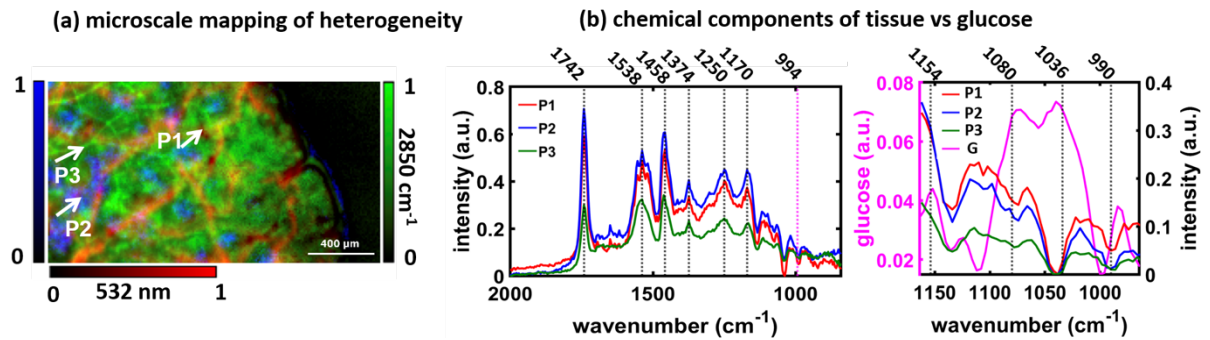
Supplementary Figure 5. Differential spectra analysis at time points post glucose administration. Difference spectra (a) generated as a subtraction of a baseline spectrum (obtained prior to glucose administration) from 50 spectra obtained at different time-points post glucose administration, and hence at different glucose values –color-coded in the legend in (b).



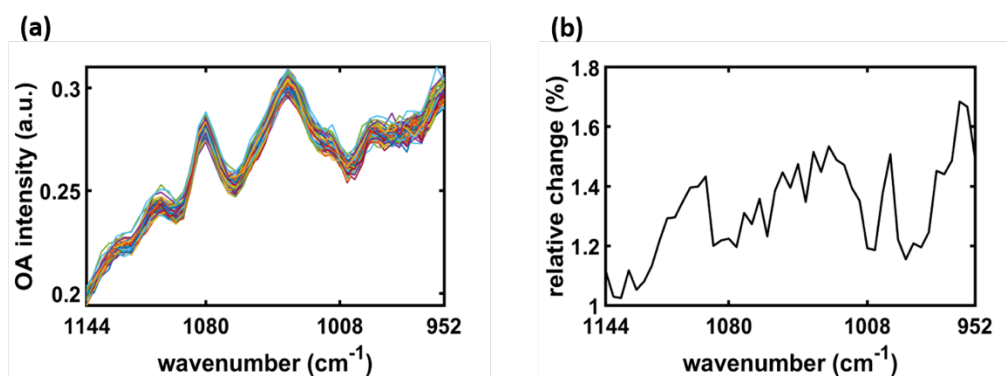
Supplementary Figure 6: Comparison of spectral features of glucose and relevant components in tissue and blood by FTIR and DiROS spectroscopy. (a) The five major absorption peaks of glucose are marked with vertical red dotted lines in the mid-infrared range (1300 to 900 cm^{-1}) for comparison with relevant blood and in tissue components at concentrations above the physiological range. A potential source of interference for glucose sensing is the two distinct peaks of lactate (1040 and 1125 cm^{-1}) that partially overlapping with those from glucose (1036 cm^{-1} and 1108-1154 cm^{-1}). **(b)** DIROS spectra of lactate, albumin, and glucose at physiological concentration after subtraction of water spectrum. The dashed-vertical lines indicated main absorption bands of glucose.



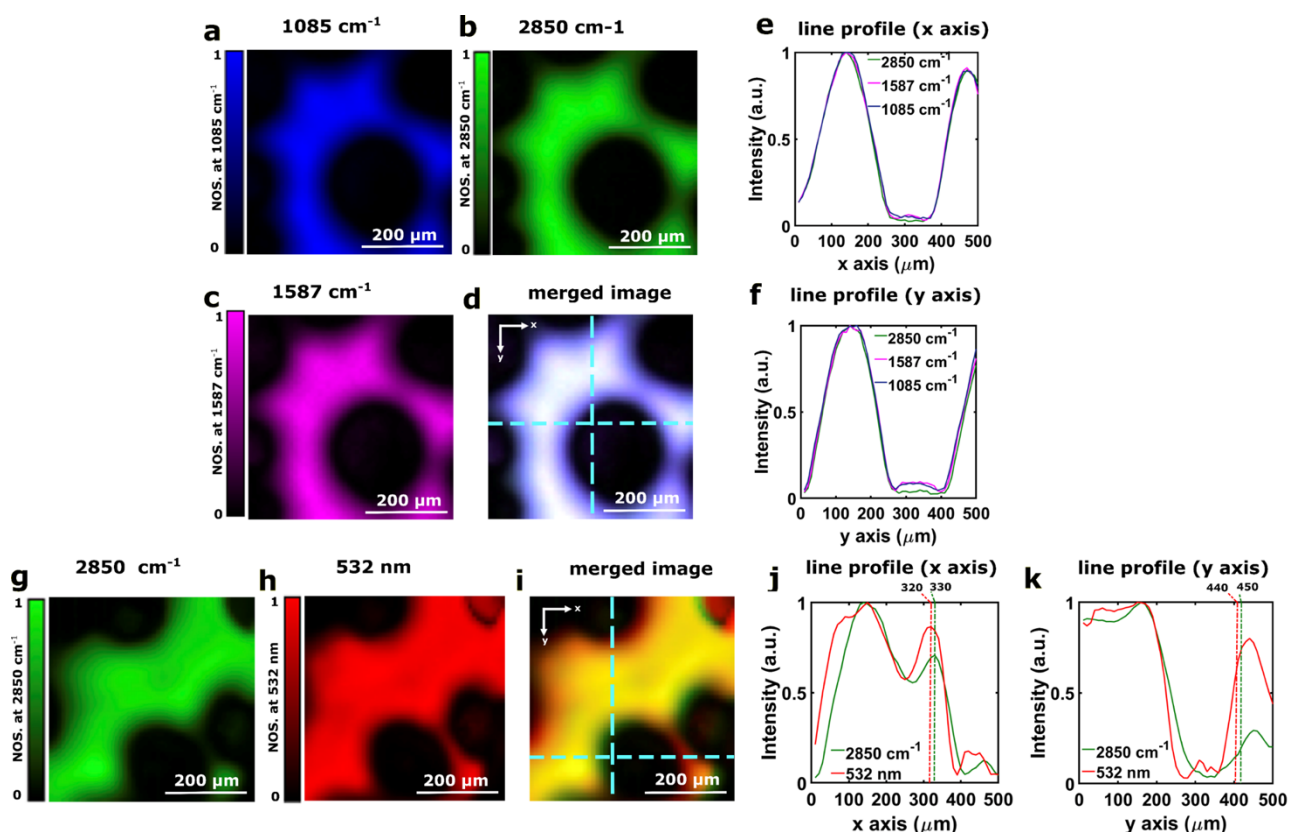
Supplementary Figure 7: Time course of glucometer and DIROS measurements after injection of phosphate buffer saline (PBS) in a mouse. When PBS is injected instead of glucose we observed a virtually constant OA response throughout the time course of the measurement, as compared to the reference blood glucose; further supporting that DiROS retrieve glucose-specific signals.



Supplementary Figure 8: The *in vivo* spectra of mouse skin obtained by DIROS. (a) Merged mid-IR/visible optoacoustic images. Three locations are marked: P1 - blood vessel, P2 - sebaceous gland, P3 - wrinkle. (b) Overlaid *in vivo* skin spectra of P1, P2, and P3 (indicated by arrows in (a)). The panel to the right shows glucose spectrum overlaid with the spectra of P1, P2, and P3 in the 964 - 1164 cm^{-1} range. G - glucose at 150 m/dl.



Supplementary Figure 9: System fluctuations in DIROS. (a) 48 representative spectra collected from repeated measurements of 5 g/dl glucose (in water), (b) Relative change (%) of the 48 spectra shown in (a). OA – optoacoustic. The maximum system fluctuation is about 1.7%, with a mean of 1.4%.



Supplementary Figure 10: Co-registration accuracy test for the combined VIS-OA/MiROM system. Micrograph of carbon tape at (a) 1085 cm⁻¹, (b) 2850 cm⁻¹, (c) 1587 cm⁻¹. (d) Merged image of (a-c). Intensity line profile at the dashed line in (d) along the (e) x-axis, (f) y-axis. Data in a–d are representative of three independent experiments. Micrograph of carbon tape at (g) 2850 cm⁻¹ and (h) 532 nm. (i) Merged image of (g-h). Intensity line profiles at the dashed line in (i) along the (j) x-axis and (k) y-axis. While negligible misalignment between mid-IR micrographs was observed, a maximum deviation of 10 μm between visible and mid-IR micrographs was found. Data in g–i are representative of 3 independent experiments (n=3).