

## Modeling Patient-Specific Muscular Dystrophy Phenotypes and Therapeutic Responses in Reprogrammed Myotubes Engineered on Micromolded Gelatin Hydrogels

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In vitro models of patient-derived muscle allow for more efficient development of genetic medicines for the muscular dystrophies, which often present mutation-specific pathologies. One popular strategy to generate patient-specific myotubes involves reprogramming dermal fibroblasts to a muscle lineage through MyoD induction. However. creating physiologically relevant. reproducible tissues exhibiting multinucleated, aligned myotubes with organized striations is dependent on the introduction of physicochemical cues that mimic the native muscle microenvironment. Here, we engineered patient-specific control and dystrophic muscle tissues in vitro by culturing and differentiating MyoD-directly reprogrammed fibroblasts isolated from one healthy control subject, three patients with Duchenne muscular dystrophy (DMD), and two Limb Girdle 2A/R1 (LGMD2A/R1) patients on micromolded gelatin hydrogels. Engineered DMD and LGMD2A/R1 tissues demonstrated varying levels of defects in a-actinin expression and organization relative to control, depending on the mutation. In genetically relevant DMD tissues amenable to mRNA reframing by targeting exon 44 or 45 exclusion, exposure to exon skipping antisense oligonucleotides modestly increased myotube coverage and alignment and rescued dystrophin protein expression. These findings highlight the value of engineered culture substrates in guiding the organization of reprogrammed patient fibroblasts into aligned muscle tissues, thereby extending their value as tools for exploration and dissection of the cellular and molecular basis of genetic muscle defects, rescue, and repair.

Keywords: DMD, LGMD, exon skipping, hydrogels, calpain 3, dystrophin

### INTRODUCTION

Muscular dystrophies are a heterogenous group of genetic disorders characterized by progressive muscle weakness. Duchenne (DMD-OMIM310200) and Limb Girdle 2A/R1 (LGMD2A/R1-OMIM 253600) muscular dystrophies are caused by mutations in the DMD and CAPN3 genes, respectively. DMD generally presents early in childhood and results in loss of ambulation in early teenage years and fatal cardiac or respiratory insufficiencies in their twenties (Flanigan, 2014). LMGD2A/R1 has a more variable presentation, with onset of muscle weakness ranging between 0 and 40 years of age and different rates of progression (Kramerova et al., 2007). DMD-encoded dystrophin and CAPN3-encoded calpain proteins have both been implicated in contributing to the structural integrity and maintenance of the sarcomere and muscle health (Blau et al., 1983; Muntoni, 2001; Kramerova et al., 2007; van der Wal et al., 2018; Pakula et al., 2019; Verhaart et al., 2019; Caputo et al., 2020; Ortiz-Cordero et al., 2021). Therefore, culture platforms that enable sarcomere maturation may help in elucidating the molecular basis of dystrophin and calpain 3 contributions to the organization and maturation of striated skeletal muscle. Whereas molecular characterization of these dystrophies has led to the development of mutation specific genetic medicines, few human mutationally defined pre-clinical cell models suitable for testing of drugs with target mutation subsets have been developed.

A major challenge in developing culture models for muscular dystrophies and other rare muscle diseases is cell source. Primary myoblasts require access to fresh muscle tissue, have limited capacity to divide, and often require purification (Blau et al., 1983; Pakula et al., 2019). Because most diagnoses are now made through genetic testing, biopsies of muscular dystrophy patients are rarely performed, and fresh muscle biopsy tissue is largely unavailable (Muntoni, 2001; Verhaart et al., 2019). Alternatively, dermal fibroblasts derived from patient skin punches can be reprogrammed to induced pluripotent stem cells (iPSCs) and subsequently differentiated to myoblasts (van der Wal et al., 2018). Although iPSC technology has led to useful models for DMD and other muscle disorders (Caputo et al., 2020; Ortiz-Cordero et al., 2021), iPSCs can be difficult and costly to derive and expand (Speciale et al., 2020). A simpler approach is to reprogram dermal fibroblasts directly to myoblasts by expression of MyoD, a master regulator of muscle cell development. We and others have stably expressed an inducible MyoD construct in dermal fibroblasts partially immortalized through expression of human telomerase reverse transcriptase (hTERT), termed iDRMs (induced directly reprogrammed myotubes), which can be expanded as fibroblasts and then reprogrammed to myoblasts and multi-nucleated myotubelike cells upon MyoD induction (Chaouch et al., 2009; Kendall et al., 2012; Kim et al., 2016; Wein et al., 2017; Barthélémy et al., 2019). We previously used iDRM from

patients with DMD on standard culture dishes to evaluate exon skipping strategies aimed at dystrophin rescue by reframing the RNA through exclusion of an additional exon (Wein et al., 2014; Barthélémy et al., 2018; Barthélémy et al., 2019; Gibbs et al., 2019). Although we were able to detect low levels of rescued dystrophin protein for certain DMD patient lines (Barthélémy et al., 2019), iDRMs were randomly organized and rarely survived longer than 1 week due to cell death and delamination, which may not be sufficient to detect dystrophin rescue in all patient lines.

To overcome some limitations of conventional in vitro techniques, several approaches to engineer DMD muscle tissue have been developed (Santoso and McCain, 2020). Fibronectin has been microcontact-printed as line patterns onto elastomeric polydimethylsiloxane (PDMS) substrates that were then laser-engraved into cantilevers to measure force generation. Primary control and DMD myoblasts seeded on these surfaces fused into aligned myotubes, with DMD myotubes exhibiting less actin and nuclear alignment and therefore lower contractile stress (Nesmith et al., 2016). However, PDMS is far stiffer than native muscle tissues, which is thought to contribute to delamination of cell linederived myotubes after approximately 1 week in culture (Bettadapur et al., 2016a). Three-dimensional (3-D) muscle tissues have also been engineered by mixing myoblasts in matrix-derived hydrogels and allowing the tissue to compact and align across two anchor points, providing a closer match to the compliance of native tissue and a more relevant microenvironment. 3-D tissues engineered with DMD iPSC-derived myoblasts have demonstrated nuclear, cytoskeletal, and contractile abnormalities (Maffioletti et al., 2018; Ebrahimi et al., 2021). However, 3-D tissues models require high numbers of cells and generally entail complex fabrication procedures, limiting their overall throughput.

Micromolded gelatin hydrogels have been developed by us and others as substrates for lengthening the culture lifetime and improving the alignment and maturation of myotubes differentiated from C2C12 (Bettadapur et al., 2016a; Denes et al., 2019a), primary chick (Santoso et al., 2021a; Gupta et al., 2021), and human control and DMD iPSCderived myoblasts (Al Tanoury et al., 2021). These gelatin substrates are relatively inexpensive and easy to fabricate while also matching the compliance of native muscle tissue. Here, we cultured iDRM control and DMD patientderived myotubes on micromolded gelatin hydrogels to promote their alignment and stability. We demonstrate that iDRM on the hydrogels align and form myofiber-like structures with different degrees of maturity, evaluated with a-actinin immunostaining and confocal microscopy. Moreover, we treated tissues with Antisense oligonucleotid-directed exon skipping molecules and evaluated dystrophin gene and protein expression. We also engineered tissues from two newly derived LGMD2A/R1 iDRM, demonstrating the application of these approaches to other rare muscle diseases. Together, these findings

highlight the value of combining patient-derived reprogrammed cell models with engineered substrates to evaluate and screen personalized therapies for rare muscle diseases.

### MATERIAL AND METHODS

## iDRM Derivation and Dermal Fibroblast Donor Characteristics

MyoD-reprogrammed skin punch fibroblasts (iDRM) were derived from three DMD subjects (Wang et al., 2018; Gibbs et al., 2019). As reported, iDRM derived from DMD subject 1003, who lost ambulation at 13.5 years, has an out-offrame deletion of DMD exons 46-51 and is predicted not to express the dystrophin protein (Wang et al., 2018). DMD subject 1023 has an in-frame deletion of DMD exons 3 to 23 with sub-typical, albeit significant, sarcolemmal dystrophin protein expression (Gibbs et al., 2019) and remains ambulatory at age 20. Subject 1015 lost ambulation at age 15 and harbors a deletion of DMD exon 45, low levels of selfcorrected exon 44 "skipped" mRNA in derived iDRM (Wang et al., 2018), and an increased frequency of clusters of dystrophin-positive revertant fibers. Muscle biopsies were only available from subjects 1015 and 1023 and a healthy 20-year-old female volunteer who served as a positive control for normal dystrophin expression and localization.

MyoD-reprogrammed skin fibroblasts (iDRM) from two LGMD2A/R1 were established for this study. Subject 1077 is a 52-year-old male who lost ambulation at 44 years old with compound heterozygous mutations: c.550delA (p.T184Rfs\*36) and c.1342C > G (p448R > G) in CAPN3. Both mutations are predicted to be pathogenic (https:// databases.lovd.nl/shared/genes/CAPN3). Subject 1081 is a 37-year-old female presenting a homozygous deletion of CAPN3 exons 17 to 24 [  $c.(1914 + 1_{1915-1})_{(*544_?)}$ del]. Deletion of these exons leads to a short truncated non-functional CAPN3 protein (BhattBHATT1 et al., 2019). All these variants leading to LGMD2A/R1 have been previously described in other patients (BhattBHATT1 et al., 2019; Krahn et al., 2006; Nallamilli et al., 2018).

Skin punches and muscle biopsies were obtained with informed consent from patients of the Center for Duchenne Muscular Dystrophy (CDMD) at UCLA under University of California Los Angeles Institutional Review Board (IRB)-approved protocols #11-001087 and #18-001547. Open or needle skeletal muscle biopsies were performed and processed as previously described (Barthelemy et al., 2020; Lee et al., 2020). Muscle samples were sectioned at 10 µm thickness and stained with hematoxylin and eosin for global histology assessment or dystrophin/laminin using standard immunohistochemistry (Barthelemy et al., 2020), where dystrophin NCL-2 (Leica, Buffalo Grove, IL, United States) at a dilution of 1:50 and laminin L9393 (Sigma, St. Louis, MO, United States) at a dilution of 1:25 were used. Digital histological images were

acquired using standard light and fluorescence using an Axioplan 2 microscope (Carl Zeiss Inc., United States). Pictures were then processed with AxioVision software (Zeiss) and/or ImageJ software.

## Inducible Directly Reprogrammable Myotube (iDRM) Lines

iDRMs were generated from dermal fibroblasts cultured from skin punches of 3 mm diameter obtained from each participant. After the establishment of a fibroblast culture, cells were immortalized using a lentivirus encoding hTERT and subsequently infected with a lentivirus encoding a tamoxifeninducible MyoD to allow commitment to skeletal muscle lineage, as we have previously reported for derivation of DMD 1023 and DMD 1015 iDRM (Barthélémy et al., 2019; Gibbs et al., 2019) (**Figure 1A**).

iDRMs were cultured as previously described, modified by plating on coverslips with micromolded gelatin hydrogels (described below) at the time of fibroblast plating, before MyoD induction (Figure 1B) (Barthelemy et al., 2018). Briefly, cells were kept in fibroblast growth media [DMEM (+ phenol red, high glucose) (Thermo Fisher Scientific, Grand Island, NY, United States) + 15% fetal bovine serum (Omega Scientific, Tarzana, CA, United States) + 1% nonessential amino acids (Thermo Fisher Scientific, Grand Island, NY, United States) + 1% penicillin/streptomycin Scientific, Island. (Thermo Fisher Grand NY. United States)]. To induce differentiation to myotubes, cells were first incubated in fibroblast growth media containing 5 µM of 4-OH tamoxifen (Sigma, St. Louis, MO, United States; dissolved in ethanol) for 48 h. On day 3, cells were washed in PBS (Thermo Fisher Scientific), and fusion media containing 1 µM 4-OH-tamoxifen was added [1:1 Ham's F-10: DMEM (phenol red free, high glucose), 2% horse serum (Thermo Fisher Scientific, Grand Island, NY, United States), and 2% insulin-transferrin-selenium (Thermo Fisher Scientific, Grand Island, NY, United States)]. During the first week of differentiation, SB431542 (a TGF- $\beta$  inhibitor) was added at a final concentration of 5 µM. All lines were kept for up to 2 weeks in fusion conditions before analysis, and the medium was changed every other day (Figure 1B).

### **Gelatin Hydrogel**

The fabrication of micromolded gelatin hydrogels cross-linked with transglutaminase was performed as previously described (Santoso et al., 2021a; Gupta et al., 2021) and illustrated in **Figure 1A**. Briefly, 260-mm<sup>2</sup> hexagons were cut from 150-mm polystyrene dishes and masked with tape. Inside each hexagonal coverslip, circles were laser-cut into the tape with a 30W Epilog Mini 24 Laser Engraver. Regions of the tape were removed such that only the outer border of substrates was covered. Coverslips were then treated with plasma (Harrick Plasma, Ithaca, NY, United States) for 10 min in ambient conditions to increase adherence of polystyrene.

PDMS stamps with 10- $\mu$ m-wide grooves separated by 10  $\mu$ m and 2  $\mu$ m in height were manufactured using photolithography



and soft lithography (Suh et al., 2017). Then, 20% porcine gelatin solution (Sigma, St. Louis, MO, United States) and 8% transglutaminase (Ajinomoto, Ontario, CA, United States) solutions in ultrapure water were mixed 1:1 with a centrifugal mixer (Thinky United States, Laguna Hills, CA, United States). The mixed solution (200  $\mu$ l) was added to each coverslip, and stamps were slowly applied. Hydrogels were incubated at room temperature overnight to solidify. The next day, hydrogels were rehydrated. Stamps and remaining tape were carefully removed (**Figure 1A**). Substrates were washed and stored in PBS at 4°C until cell seeding.

### **AO Transfection**

On day 7 (week 1) or 14 (week 2) of differentiation, iDRM cells (1015 or 1003) were transfected with 25 or 250 nM 2-O-methyl AO targeting exon 44 (using H44A-TGTTCAGCTTCT GTTAGCCACTGA and 45 (using H45A -CCAATGCCATCC TGGAGTTCCTGTAA) (Wilton et al., 2007), respectively, using oligofectamine (Thermo Fisher Scientific) transfection reagent according to our previously published protocol (Barthélémy et al., 2019).

### **RNA Isolation and PCR**

On the day of analysis, duplicate or triplicate coverslips from each condition were removed from the well, and the remnant cells growing on the side of the coverslips were scraped directly and combined in TRIzol (Thermo Fisher Scientific). Total RNA was isolated using the Purelink RNA mini kit (Thermo Fisher Scientific). Exon skipping analysis was performed accordingly to our previously published protocol, and skipping efficiency is indicated by the ratio of skipped mRNA transcript over the total mRNA transcripts (skipped plus unskipped) (Barthélémy et al., 2019). For both cell lines, a nested PCR was performed to amplify the targeted DMD region: between exons 43 and 52 using the previously described primers for cell line CDMD1003 (Ex42-o, 5'-GTCCGTGAAGAAACGATGATG-3' + Ex53-0, 5'-CTCCGG TTCTGAAGGTGTTC-3' and Ex43-i, 5'- TCTCTCCCAGCT TGATTTCC-3' and Ex52-i, 5'- TCTAGCCTCTTGATTGCT GG-3') or between exons 42 and 46 (Ex42-o, 5'-CAATGC TCCTGACCTCTGTGC-3' + Ex46-o, 5'-GCTCTTTTCCAG GTTCAAGTGG-3' and Ex43-i, 5'-GTCTACAACAAAGCT CAGGTCG-3' + Ex46-i, 5'-GCAATGTTATCTGCTTCCTCC AACC-3') for cell line CDMD1015.

# Immunofluorescence Staining and Microscopy

iDRMs were seeded at 350,000 cells onto micromolded gelatin hydrogel coverslips in 12-well plates and MyoD was induced with tamoxifen as described above. During all procedures, cells were kept at room temperature unless specified otherwise. After myotube formation, cells were fixed with acetone for dystrophin staining or ice-cold methanol for a-actinin staining. Primary antibodies were incubated overnight at 4°C: dystrophin NCL-2 (Leica, Buffalo Grove, IL, United States) at a dilution of 1:20 and a-actinin (Sigma, St. Louis, MO, United States) at a dilution of 1:200. Secondary antibodies were used at a dilution of 1:500: goat anti-mouse IgG (SA5-10173) and goat anti-rabbit (35553) from Thermo Fisher Scientific for 1 h. Coverslips were mounted in ProLong Gold Antifade with DAPI (Thermo Fisher Scientific). Confocal fluorescence microscopy was performed using a Confocal Module Nikon C2 with 20× air or 60× oil objectives. Z-stacks were acquired (step size: 1 µm), and average intensity projections were used for data analysis on ImageJ (NIH).

To quantify myogenic index, CellProfiler was first used to mask a-actinin signal. Then, the proportion of total nuclei in masked areas that contained at least three nuclei was taken as the myogenic index; we chose to count areas with at least three nuclei as a stringent filter of multi-nucleated myotubes. The myotube coverage was defined as the area percentage of positive  $\alpha$ -actinin signal after autothresholding using ImageJ. As a proxy for myotube width, we used an automated CellProfiler calculation to define a minor axis length based on the ellipse encompassing a mask of  $\alpha$ -actinin that defined a single myotube. To quantify the degree of myotube alignment based on a-actinin staining, the ImageJ plugin OrientationJ was used with a Gaussian filter window of  $\sigma = 10$  pixels to calculate the coherency and orientation angles at each pixel. Then, a global orientation order parameter was calculated from the orientation angles of at least three images per sample, as previously described (McCain et al., 2013; Petersen et al., 2020).

### **Statistics**

Student's t-test was performed between week 1 and week 2 groups for each patient iDRM lines or between them, or between AO and non-treated patient iDRM lines. Comparisons with *p*-values less than 0.05 were considered statistically significant.

### RESULTS

### Engineering Aligned DMD and LGMD2A/R1 iDRMs on Micromolded Gelatin Hydrogels

To engineer mutation-specific DMD muscle tissues *in vitro*, we isolated dermal fibroblasts from DMD 1015, DMD 1023, DMD 1003, and one control subject (1001). All fibroblasts were engineered to iDRM by expressing a tamoxifen-inducible MyoD and hTERT (**Figure 1A**), as described previously (Barthelemy et al., 2018; Wang et al., 2018). iDRMs were seeded on gelatin hydrogels micromolded with 10-µm-wide

alternating grooves affixed to coverslips (**Figure 1A**). iDRMs were then triggered to become myoblasts with induction of MyoD 1–2 days after seeding and maintained in differentiation media for 1 to 2 weeks to induce fusion into myotubes (**Figure 1B**).

To characterize the morphological events characteristic of muscle development, we co-visualized nuclei and sarcomeric  $\alpha$ -actinin in engineered iDRM tissues after 1 and 2 weeks in culture. We chose sarcomeric  $\alpha$ -actinin because it is expressed relatively late in myogenesis, especially compared to other markers, such as desmin, myogenin, or myosin heavy chain (White et al., 2014; Bettadapur et al., 2016b; Nguyen et al., 2016; Denes et al., 2019b; Santoso et al., 2021b). Sarcomeric αactinin is also present in the z-lines in sarcomeres and thus clearly demarcates mature myofibrils. All cell lines formed multi-nucleated, aligned myotubes at both time points (Figure 2), although to different degrees. To compare this, we quantified myotube coverage (a-actinin positive proportion), myogenic index (proportion of nuclei in aactinin positive myotubes with more than three nuclei), myotube width (minor axis length), and myotube alignment (Figures 3A-D and Supplementary Figure S1). We report both myotube coverage and myogenic index to collectively indicate myotube fusion, myotube adhesion, and tissue cellularity. Healthy 1001 iDRM formed myotubes with stable sarcomeric  $\alpha$ -actinin coverage and myogenic index throughout the 2-week culture period. Organized striations were detectable at week 1 and remained constant through week 2. Myotube width peaked in the first week and declined slightly by week 2, likely due to detachment of some of the most mature myotubes. The distribution of myotube width, shown as histograms in Supplementary Figure S1, also illustrates this trend. Myotube alignment for healthy iDRM was also high and indicated successful tissue patterning by the micromolded gelatin hydrogels.

DMD 1015 iDRM performed relatively similar to the healthy 1001 iDRM, in terms of sarcomeric a-actinin coverage (Figure 3A), myogenic index (Figure 3B), and myotube width (Figure 3C and Supplementary Figure S1), with a potential modest delay in the time to peak myotube width relative to healthy control. Similar to the healthy control, striations in DMD 1015 myotubes were also detectable (Figure 2). We attempted to quantify  $\alpha$ -actinin striations, but the heterogeneity of the cells precluded a systematic and meaningful analysis. DMD 1023 and DMD 1003 iDRM also differentiated into multi-nucleated myotubes with near-typical myogenic index and myotube width. These results are similar to previous studies that have shown relatively unimpaired fusion in human iPSC-derived myoblasts from DMD (Caputo et al., 2020) or LGMDR9 (Ortiz-Cordero et al., 2021) patients. However, striations in DMD 1023 and DMD 1003 myotubes were qualitatively impaired relative to healthy 1001 myotubes. Likewise, myotube coverage was lower in DMD 1023 and DMD 1003 compared to healthy 1001. Myotube alignment was also high for the healthy and DMD myotubes (Figure 3D), indicating that all cell lines were instructed by the micromolded features. Myotube alignment trended lower for DMD 1003 compared to



DMD 1015 and DMD 1023, possibly due to the greater severity of the mutation in this line. The healthy 1001 myotubes also had relatively low alignment, likely because myotubes tended to bridge across the micromolded features in the control line compared to the DMD lines.

To determine whether our approach was suitable for other genetic muscle diseases, we similarly isolated fibroblasts from two LGMD2A/R1 subjects, engineered them to iDRM, and differentiated them to myotubes on micromolded gelatin hydrogels (**Figure 1A**). LGMD2A/R1 line 1077 exhibits compound heterozygous mutations c.550delA (p.T184Rfs\*36) and c.1342C > G (p448R > G) in *CAPN3*. LGMD2A/R1 line 1081 exhibits homozygous deletion of *CAPN3* exons 17 to 24 [c.(1914 + 1\_1915-1)\_(\*544\_?)del]. Whereas LGMD2A/R1 1077 showed lower α-actinin coverage

(Figure 3A) and normal or lower myogenic index (Figure 3B) compared to the healthy control, LGMD2A/R1 1081 had similar sarcomere α-actinin coverage and a much higher myogenic index. For certain time points, LGMD2A/R1 1077 had lower myotube width, whereas LGMD2A/R1 1081 had higher myotube width, compared to control (Figure 3C and Supplementary Figure S1). However, neither LGMD2A/R1 1077 or LGMD2A/R1 1081 developed well-organized, discrete striations (Figure 2). Both LGMD2A/R1 1077 and LGMD2A/R1 1081 exhibited high degrees of myotube alignment (Figure 3D). Thus, our engineered tissues revealed distinct differences in disease- and mutation-specific muscle morphology, which is an advantage of using patient-derived cells. Importantly, the variability within each cell line is relatively modest.



## Morphology of Muscle Fibers in Healthy and DMD Patients

As a baseline comparison for our culture models, we evaluated morphological differences in muscle biopsy tissue sections from a healthy subject and the two DMD subjects for which we had access to muscle tissue sections, DMD 1015 and DMD 1023. Both patients were biopsied before loss of ambulation and had substantial preservation of skeletal myofibers. DMD 1015 exhibits an out-of-frame deletion of DMD exon 45 predicted to lead to total loss of dystrophin expression. DMD 1023 exhibits an in-frame deletion of DMD exons 3 to 23 predicted to express a partially functional dystrophin protein lacking the actin binding site. As expected, muscle fibers in the healthy subject robustly expressed sarcomeric a-actinin throughout their cross-sectional area, were encircled by dystrophin, and were relatively consistent in size (Figure 4). Both DMD biopsies demonstrated weaker sarcomeric a-actinin staining, variations in muscle fiber size, and fibro-fatty infiltrates, concordant with a DMD phenotype (Figure 5). Sarcomeric  $\alpha$ -actinin expression (Figure 5) and fiber size were lowest in DMD 1023 tissues despite significant expression of internally truncated sarcolemmal dystrophin protein in every myofiber (Figures 4 and 5). Whereas most 1015 fibers do not express dystrophin, we observe some patches of dystrophin expressing revertant fibers and higher aactinin expression relative to 1023, in keeping with findings

regarding  $\alpha$ -actinin coverage in the iDRM culture models (**Figures 2** and **3**). However, it is important to consider that the degeneration process *in vivo* is vastly more complex and on a much longer timescale than what can be observed *in vitro*. Thus, comparing patient muscle biopsies to *in vitro* engineered muscle tissues should be done with much caution and conservativeness (Forbes et al., 2020).

## Evaluation of Dystrophin Rescue in DMD iDRMs Treated With Exon Skipping AOs

Development of precision medicines requires human mutation specific platforms for assessing mechanisms of action and efficacy. AO DMD exon skipping drugs function to reframe mutant *DMD* mRNA through removal of an "extra" exon, enabling rescue of an internally deleted but partially functional dystrophin protein. "Exon skipping" drugs are mutation-specific, in so far as only some *DMD* mutations adjacent to the targeted region can be reframed. 1015 mutation can be rendered in frame by exclusion of exon 44, whereas 1003 mutation is amenable to reframing by targeting exon 45.

To determine whether AO treatment rescued dystrophin expression in iDRM, DMD 1015 and DMD 1003 iDRMs were exposed to exon skipping drug targeting exon 44 or exon 45, respectively, after 1 or 2 weeks of differentiation on micromolded hydrogels. We performed immunostaining on healthy and DMD



iDRM engineered tissues treated with or without AO to determine whether we could observe rescue of dystrophin (Figure 6A). Myotubes generated from the healthy iDRM demonstrated dystrophin staining at both time points (Figure 6A). In DMD 1015 iDRMs, low levels of dystrophin protein were detected without AO treatment after 2 week of culture on the micromolded platform, consistent with detection of low levels of skipped DMD message in the absence of AO. Exposure to AO increased the rescued exon 44 deleted DMD mRNA and dystrophin proteins expression and after both 1 and 2 weeks of culture, consistent with levels of exon 45 skipped mRNA induced (Figure 6B). In DMD 1003 iDRMs, dystrophin was not detectable in 1003 in the absence of skipping drug. Exposure to exon 45 skipping AO rescued low levels of dystrophin protein when AO was added after 1 week and to a greater extent when AO was added after 2 weeks of differentiation (Figures 6A,B). Thus, both DMD 1015 and DMD 1003

demonstrated brighter dystrophin staining with the addition of skipping AO.

We next measured the effects of dystrophin rescue induced by exon skipping on myotube morphology for DMD 1015 and DMD1003 at week 1 or 2 of differentiation (**Figure 7**). We performed staining for  $\alpha$ -actinin and nuclei (**Figure 7**) and calculated myotube coverage (**Figure 8A**), myogenic index, (**Figure 8B**), myotube width (**Figure 8C** and **Supplementary Figure S2**), and myotube alignment (**Figure 8D**). DMD 1015 iDRMs developed striations at weeks 1 and 2, regardless of exon skipping and dystrophin rescue. There were also no noticeable changes in myogenic index, myotube coverage, myotube width, or myotube alignment in 1015 due to AO treatment, except for slight but non-significant increases in the first three metrics after 2 weeks of AO treatment. The distribution of myotube width from iDRM DMD 1015 and 1003 samples with and without AO treatment is shown as histograms in **Supplementary Figure S2** 



and shows a particular shift toward a higher proportion of wider myotubes after AO treatment at week 2. The effects on dystrophin rescue in DMD 1003 were more noticeable, with exon skipping AO inducing greater myotube coverage, myogenic index, and myotube alignment at both time points. However, these increases did not reach statistical significance. Nonetheless, taken together, these findings highlight a potential role for rescued dystrophin protein in maturation or stability of myotubes and sarcomeres.

### DISCUSSION

Development of genetic medicines aimed at repairing or replacing DMD and LGMDDR1/LGMD2A mutations is an active area of research, and several drugs have been already approved or are in human pre-clinical or clinical trials (Sheikh and Yokota, 2021). However, there is a paucity of DMD and LGMD mutation specific human culture models for assessing mechanisms of action or improving efficacy of therapeutic strategies. Here, we report that culturing one heathy subject, three DMD, and two LGMD-derived iDRM on micromolded gelatin hydrogel coverslips induces tissue alignment, prolongs culture lifetime, and promotes myotube development in culture over 2 weeks. This relatively long culture period enabled us to characterize myotube development and dystrophin rescue in DMD myotubes in response to AO skipping drugs. We also show that our approach is compatible with iDRM from LGMD2A/R1 patients, demonstrating its modularity for modeling other forms of muscular dystrophy.

Although all healthy and DMD iDRM demonstrated myogenic potential and a high degree of alignment, DMD 1003 showed the most severe defects in  $\alpha$ -actinin expression, followed by DMD 1023. We were largely unable to distinguish DMD 1015 from healthy control using these measures. The *in vitro* results for DMD 1015 and DMD 1023 mirror the trends of the patient muscle biopsies, for which defects were more substantial for DMD 1023 compared to DMD 1015. Thus, our combination of patient-derived iDRM with micromolded gelatin hydrogels replicated select histological phenotypes of native muscle and further demonstrates that muscle development *in vitro* is regulated by distinct *DMD* mutations.

iDRM DMD 1003 harbors a deletion of exons 46-51 of DMD, which encodes an out-of-frame mRNA, produces no dystrophin protein, and demonstrates defects in a-actinin coverage and the development of striations. These data support a role for dystrophin in the development or stabilization of myotubes and sarcomeres. Such a suggestion is consistent with reports that the dystrophin-glycoprotein complex slows depolymerization of actin filaments in vitro (Rybakova et al., 1996; Rybakova and Ervasti, 1997). Alternatively, low α-actinin coverage and myotube width may be secondary to impaired cell survival or earlier developmental defects dependent on dystrophin. DMD reframing and dystrophin rescue induced within DMD 1003 by exposure to exon 45 skipping AO modestly improved measures of myotube coverage, fusion, and alignment, further supporting a role for dystrophin in these processes and highlighting the value of this model as a screening tool for drug development and optimization of precision medicines.

iDRM DMD 1023 has an in-frame mutation *DMD* 3–23, which creates substantial amounts of dystrophin properly localized at the sarcolemma but lacking the primary actin binding site (Gibbs et al., 2019). We identified defects in myotube maturation and organization, potentially highlighting requirements for dystrophin actin binding in myogenesis and myotube sarcomere maturation, consistent with a previous report (Banks et al., 2007). Additional experiments will be needed to support this hypothesis.

iDRM DMD 1015 has an exon 45 deletion of DMD amenable to reframing by exon 44 AO skipping. We have previously demonstrated that iDRM DMD 1015 constitutively expresses low levels of exon 45 skipped and reframed DMD mRNA, even in the absence of AO, as we have reported for several DMD iDRM with exon 45 deletions (Wang et al., 2018). Likewise, immunostaining frozen muscle biopsy sections from the DMD 1015 fibroblast donor showed some clusters expressing low levels of dystrophin rescue in vivo. The predisposition of exon 45 deletion DMD mutants to selfcorrect by skipping exon 44 to produce low levels of dystrophin has been suggested as the molecular basis of mild disease progression relative to typical DMD frameshifting mutations and highlights that even low levels of dystrophin can have functional consequences. We also detected low levels of exon 45 skipped DMD mRNA in the absence of any treatment and increased exon 44 exclusion and robust induction of dystrophin protein expression in cells exposed to



skipping AO. Unlike the other two DMD patient-derived iDRM, DMD 1015 behaved much closer to wild type, with no defect in aactinin coverage or striation. It is possible that the low levels of rescued dystrophin constitutively expressed in DMD 1015 are sufficient to partially overcome the developmental defects in myotube development or sarcomere stability observed in dystrophin null DMD 1003. Exon 44 skipping AO increased dystrophin expression and induced modest improvements in myogenic index, myotube coverage, and myotube width, further supporting a role for rescued dystrophin in facilitation of myotube maturation in DMD 1015. Moreover, multiple a-actinin isoforms have been linked to dystrophin and DMD. a-Actinin 3 has been identified as a known modifier of DMD, a-actinin 2 has been identified as an extended member of the DGC, and a progressive depletion of a-actinin proteins has been observed in DMD (Minetti et al., 1991; Hance et al., 1999; Hogarth et al., 2017), making this

protein family an underestimated marker of pathophysiological changes in this disease.

Although differentiation on micromolded gelatin hydrogels enabled visualization of rescued dystrophin expression, we did not observe the expected patterning of dystrophin. In native muscle, dystrophin is enriched in costamere protein assemblies, which circumferentially align with the  $\alpha$ -actinin enriched Z disk and couple force-generating sarcomeres with the sarcolemma. Similarly, although we did detect some punctate sarcomere-like structures in myotubes derived from select iDRM lines, the overall maturity of the myofibrils and sarcomeres was limited, especially compared to myotubes derived from primary myoblasts. Similar issues related to myofibril immaturity have routinely been observed in myotubes derived from a variety of reprogrammed (Boularaoui et al., 2018) and iPSC-derived myoblasts (Lainé et al., 2018; Rao et al., 2018) and likely reduce the baseline and drug-induced differences



in the phenotypes of healthy and diseased cells. Overall, the maturity of iDRM-derived myotubes observed in this study was similar or weaker than iPSC-derived myotubes (Caputo et al., 2020; Ortiz-Cordero et al., 2021). Of note, however, iDRMs require less time, cost, and expertise to generate compared to iPSC-derived myoblasts, which may be especially beneficial for generating patient-specific muscle tissues in time-sensitive or resource-limited settings. Extending culture time (Santoso and McCain, 2021), integrating supporting cell types (Juhas et al., 2018; Santosa et al., 2018; Santoso and McCain, 2021), providing electrical (Nedachi et al., 2008; Chen et al., 2021) or mechanical stimulation (Heher et al., 2015; Chang et al., 2016), or engineering 3-D tissues (Madden et al., 2015; Uzel et al., 2016; Costantini et al., 2017; Davis et al., 2019; Ariyasinghe et al., 2020; Ebrahimi et al., 2021) or earlier exposure to AO could also help induce muscle maturation and proper localization of dystrophin and  $\alpha$ -actinin.

 $\begin{array}{cccc} LGMD2A/R1 & 1077 & express & mutations \\ [c.550delA \ (p.T184Rfs^*36) \ and \ c.1342C \ > \ G \ (p448R \ > \ G] \end{array}$ 

within the catalytic PC1 and the calcium-binding and phospholipid-binding C2 domains, respectively, and these iDRMs show defects in formation of myotube maturation and structure. Patient cells derived from patient LGMD2A/R1 1081, present with a homozygous deletion of the entire c-terminal region of the protein, were able to form myotubes and showed no quantitative defects in  $\alpha$ -actinin coverage or axis length but did not develop proper maturation of the clearly defined  $\alpha$ -actinin marked sarcomeres upon visual inspection. It is unclear why LGMD 1077 iDRM demonstrates significant defects in myotube maturation, whereas 1081 has an exceptionally high MI and is otherwise near normal.

One advantage of differentiating myotubes in culture is that it allows assessment of sequential myoblast activation, fusion, and the development of mature myofibers with organized sarcomeres, responsible for striated muscle patterning and required for force generation. Thus, iDRM differentiated on micromolded hydrogels may aid in dissecting requirements for each of these developmental



events (White et al., 2014). However, factors other than DMD or LGMD mutation that might influence iDRM performance include the presence/absence of DMD or LGMD2A/R1 disease modifier genes or artifacts of culture selection. Therefore, comparisons between individually derived iDRM to determine relative myogenic activity of particular mutations should be made with caution. Rather, creation of isogenic iDRM expressing defined DMD or LGMD mutations and full-length dystrophin or a panel of distinct patient iDRM with similar mutations may be necessary to confirm preliminary observations made regarding effects of DMD or LGMD mutation based on comparison between two lines. Alternatively, experiments where iDRM DMD 1003 and 1015 activity is measured before and after exposure to a potential therapeutic or disease modifying entity, such as exon skipping AO, do not suffer from this criticism and thus are likely to prove valuable for precision drug optimization and screening.

In summary, our results establish that patient-derived iDRM differentiate into aligned myotubes on micromolded gelatin hydrogels and enable evaluation of myotube formation as a function of patient-specific mutations. This is a promising approach for screening and testing personalized therapies for muscular dystrophies and other genetic muscle diseases *in vitro*. Together, our findings highlight the benefit of human cell models combined with engineered scaffolds that more closely mimic the

*in vivo* microenvironment and encourage the development of new strategies to promote further maturation for proper characterization of morphological differences and evaluation of the efficacy of new therapies.

### DATA AVAILABILITY STATEMENT

The raw data supporting the conclusion of this article will be made available by the authors, without undue reservation.

### **ETHICS STATEMENT**

The studies involving human participants were reviewed and approved by the UCLA OHRPP (IRB). Written informed consent to participate in this study was provided by the participants' legal guardian/next of kin.

### **AUTHOR CONTRIBUTIONS**

FB, JS, LR, RJ, and IL performed all experiments. SN collected human specimens. FB, JS, MMi, and MMc drafted the manuscript with contributions from all co-authors. FB, MMi, and MMc conceived the project and designed the experiments.

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### SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fcell.2022.830415/ full#supplementary-material

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Supplementary Figure S1 | Dystrophic myotubes showed a delayed myotubes enlargement at week 1 that fades away at week 2.  $\alpha$ -Actinin staining were performed to analyze the maturation of myotubes from a healthy donor (1001) or patients presenting with LGMD2A/R1 (1077 - c.550delA, c.1342C > G and 1081 - delta 17–24) or DMD (1015 - delta 45; 1023 - delta 3–23; and 1003 - delta 46–51). For each cell line, cells were differentiated for 1 or 2 weeks and all the myotubes showing more than three nuclei from two independent experiments run in duplicates were analyzed and compiled on these graphs representing the width ranges (in  $\mu m$ ) observed in our cell culture models.

Supplementary Figure S2 | AO treatment promotes enlargement of myotubes from DMD patients' cell lines. DMD 1015 (delta 45) or DMD 1003 (delta 46–51) cells were cultured for 1 or 2 weeks before the addition of antisense oligonucleotides and  $\alpha$ -actinin staining were performed to analyze the maturation of myotubes. All the myotubes showing more than three nuclei from three independent experiments run in duplicates were analyzed and compiled on these graphs representing the width ranges (in µm) observed in our cell culture models.

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**Conflict of Interest:** MLM is an inventor on US Patent No. US9857356B2 by Harvard University, which includes the design and use of micrmolded gelatin hydrogels.

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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