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A novel electrochemical aptasensor for fumonisin B₁ determination using DNA and exonuclease-I as signal amplification strategy

Min Wei*, Fei Zhao, Shuo Feng and Huali Jin

Abstract

In this work, using DNA and exonuclease-I (Exo-I) as signal amplification strategy, a novel and facile electrochemical aptasensor was constructed for fumonisin B₁ (FB₁) detection. The G-rich complementary DNA (cDNA) was immobilized onto the electrode surface. Then, aptamer of FB₁ was hybridized with cDNA to form double-stranded DNA. In the absence of FB₁, double-stranded DNA and G-rich cDNA on the electrode surface promoted effectively methylene blue (MB) enrichment and amplified the initial electrochemical response. In the presence of FB₁, the combination of aptamer and FB₁ led to the release of aptamer from the electrode surface and the expose of 3' end of single-stranded cDNA. When Exo-I was added onto the electrode surface, the single-stranded cDNA was degraded in the 3'-5' direction. The decrease of double-stranded DNA and G-rich cDNA resulted in the less access of MB to the electrode surface, which decreased the electrochemical signal. The experimental conditions including incubation time of FB₁, the amount of Exo-I and incubation time of Exo-I were optimized. Under the optimal conditions, the linear relationship between the change of peak current and the logarithmic concentration of FB₁ was observed in the range of 1.0×10^{-3} – 1000 ng mL⁻¹ with a low limit of detection of 0.15 pg mL⁻¹. The experimental results showed that the prepared aptasensor had acceptable specificity, reproducibility, repeatability and stability. Therefore, this proposed aptasensor has a potential application in the food safety detection.

Keywords: Electrochemical aptasensor, Fumonisin B₁, Exonuclease-I, G-rich DNA, Methylene blue

Introduction

As the metabolic product of Fusarium moniliforme Sheld, fumonisin B₁ (FB₁) is a kind of the most toxic and prevalent fumonisins [1]. FB₁ can contaminate various food and feedstuff such as corn, wheat, rice, peanut, beer, and animal feed. A large number of studies have reported that FB₁ can cause serious diseases such as horse white matter softening, nephrotoxicity, hepatotoxicity and liver cancer [2, 3]. Therefore, it is necessary to monitor FB₁ for food safety and human health.

Among the various methods for FB₁ detection [4-7], the electrochemical aptasensor has attracted widespread attention due to their low cost, simple operation, high selectivity and affinity, chemical stability, and easy storage [8, 9]. Recently, with the advantages including effective amplification strategy, easy design, simple operation and rapid reaction, the nuclease-based electrochemical aptasensor has become research focus [10, 11]. Among the different nucleases, exonuclease I (Exo-I) has attracted increasing attention, owing to its structuresensitive digestion for the single-stranded DNA in the direction of 3' to 5', low cost, good specificity and buffer compatibility [12-14]. As a kind of electrochemical signal probe, methylene blue (MB) can highly interact with G-rich single-stranded DNA and double-stranded DNA,

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and is therefore suitable for the application in electrochemical aptasensor [15, 16].

Herein, based on MB, Exo-I, aptamer of FB $_1$ (Apt) and G-rich cDNA, a novel signal-off sensor was firstly designed for the electrochemical detection of FB $_1$. The existing double-stranded DNA on the electrode surface, came from the hybridization of Apt and G-rich cDNA, enriched abundant MB and amplified the initial electrochemical response. In the presence of FB $_1$, the formation of Apt-FB $_1$ made aptamer release from the electrode surface. Then, the effect of Exo-I on G-rich cDNA of the electrode surface resulted in the less access of MB, which further decreased the electrochemical signal and amplified ΔI . The change of MB electrochemical signal can be applied for FB $_1$ detection.

In virtue of the favorable combination of MB with double-stranded DNA and G-rich cDNA, and the advantages of Exo-I including easy design, simple operation, high amplification efficiency and excellent selectivity, the proposed signal amplification strategies can save the tedious preparation process and is beneficial to the experimental stability.

Experimental

Materials and chemicals

The used oligonucleotides were provided by Sangon Biological Engineering Technology & Services Co. Ltd. (Shanghai, China), and their sequences were as follows: cDNA: 5'-SH-GAG GGG TGG GCG GGA GGG AGA TTG CAC GGA CTA TCT AAT TGA ATA AGC-3'. Apt: 5'-ATA CCA GCT TAT TCA ATT AAT CGC ATT ACC

TTA TAC CAG CTT ATT CAA TTA CGT CTG CAC ATA CCA GCT TAT TCA AGT AGA TAG TAA GTG CAA TCT-3′. FB₁ and Exo-I were purchased from Acros and TaKaRa, respectively. 0.05 M of pH 7.4 Tris-HCl buffer (containing 0.05 M Tris, 0.2 M NaCl and 0.001 M EDTA) was used.

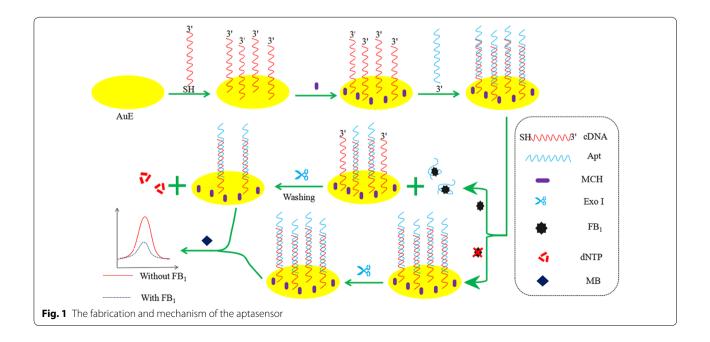
Apparatus

The CHI 660E Electrochemical Workstation was used for the electrochemical experiments (Shanghai Chenhua Instrument Corporation, China). The gold electrode (AuE) was used as working electrode. Differential pulse voltammetry (DPV) and electrochemical impedance spectroscopy (EIS) were used for the electrochemical measure.

Fabrication and mechanism of the aptasensor

The fabrication and mechanism of the aptasensor were shown in Fig. 1. 5 μL of 1 μM SH-cDNA was dropped on the AuE surface for immobilization at 37 °C. Then, the AuE was washed by Tris–HCl buffer to remove the unbound cDNA. After that, 5 μL of 6-mercapto-1-hexanol (MCH) was dropped to block the untreated sites. Next, 5 μL of 1 μM Apt was hybridized with cDNA for 2 h at 37 °C to obtain the aptasensor Apt/cDNA/AuE.

When FB₁ was absent, cDNA and Apt could not be degraded by Exo-I because that the 3' end of both cDNA and Apt were protected by the formation of double-stranded DNA. MB could intercalate into G-rich cDNA and double-stranded DNA, and produce a strong current signal. When FB₁ was present, the complex of Apt and



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 ${\rm FB}_1$ was formed and released from the surface of the electrode, leading to the expose of 3' end of single-stranded cDNA on the electrode surface. When Exo-I was added onto the electrode surface, the single-stranded cDNA was degraded in the 3'-5' direction. The decrease of double-stranded DNA and G-rich cDNA resulted in the less access of MB to the electrode surface and the decrease of the electrochemical signal. The change of MB electrochemical signal can be applied for ${\rm FB}_1$ detection.

Results and discussion

Electrochemical characterization of the prepared aptasensor

Figure 2 showed the EIS characterization for the aptasensor fabrication. The charge transfer resistance (R_{ct}) increased from 251.3 Ω of the bare AuE (a) to 1219 Ω of the cDNA/AuE (b), indicating that the cDNA was immobilized to the electrode surface. For the Apt/cDNA/AuE (c), the R_{ct} was increased to 1381 Ω , indicating that Apt hybridized successfully with cDNA on the electrode surface. After the Apt/cDNA/AuE was incubated by 1 μg mL $^{-1}$ FB $_1$ and Exo-I, respectively, the R_{ct} (d) was decreased to 836 Ω . This was because that Apt was specifically combined with FB $_1$ and released from the electrode, and cDNA was digested by Exo-I due to the expose of its 3' end, resulting in the less negative charge on the electrode surface.

The detection of FB₁ on Apt/cDNA/AuE sensor

Figure 3 showed the DPV results of MB on the Exo-I/Apt/cDNA/AuE (a), FB₁/Apt/cDNA/AuE (b) and Exo-I/FB₁/Apt/cDNA/AuE (c) in Tris-HCl buffer. In the absence of FB₁, the Exo-I/Apt/cDNA/AuE showed an

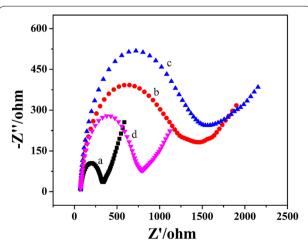


Fig. 2 EIS of 10 mM [Fe(CN) $_6$]^{3–4–} containing 0.1 M KCl on the AuE (a), the cDNA/AuE (b), and the Apt/cDNA/AuE before (c) and after (d) addition of FB $_1$ and Exo-I

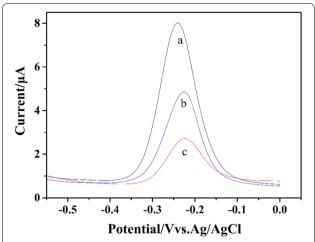


Fig. 3 The DPV results of MB on the Exo-I/Apt/cDNA/AuE (a), FB1/Apt/cDNA/AuE (b) and Exo-I/FB₁/Apt/cDNA/AuE (c) in Tris-HCl buffer

initial peak current of 7.29 μA (a). With the addition of 1 $\mu g \cdot m L^{-1}$ FB₁, the peak current of FB₁/Apt/cDNA/AuE (b) decreased to 4.02 μA . This is because that in the presence of FB₁, the formation of Apt-FB₁ composite made Apt release from double-stranded DNA on the electrode surface, resulting in that the amounts of MB intercalated into the double-stranded DNA were decreased. After the addition of Exo-I, the DPV value of Exo-I/FB₁/Apt/cDNA/AuE (c) further decreased to 2.41 μA , indicating that Exo-I could digest the single-stranded cDNA on the electrode surface and achieve the signal amplification.

Optimization of the aptasensor

Figure 4 showed the effect of FB₁ incubation time (A), Exo-I amount (B) and Exo-I incubation time (C) on the electrochemical signal. As shown in Fig. 4a, it can be seen that ΔI increased with the increasing of FB₁ incubation time and reached the maximum of $5.3~\mu A$ at 10~min. Therefore, 10 min was selected as the optimal FB₁ incubation time. As can be seen from Fig. 4b, ΔI increased with increasing of Exo-I amount and reached the maximum at 5 U, then decreased when the amount was further increased. This may due to that the limit of active surface area on the fabricated electrode led to the inefficiency of redundant Exo-I. So, 5 U of Exo-I was used for the subsequent experiments. As shown in Fig. 4c, the ΔI increased quickly with increasing the incubation time in the first 30 min, then changed slightly when the incubation time was more than 30 min. Therefore, 30 min was used as the optimal Exo-I incubation time.

Analytical performance of the designed aptasensor

Figure 5 showed the calibration plot of the fabricated aptasensor for FB_1 detection. With the concentration

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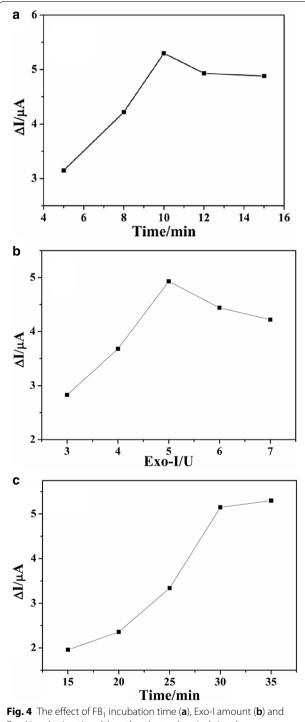
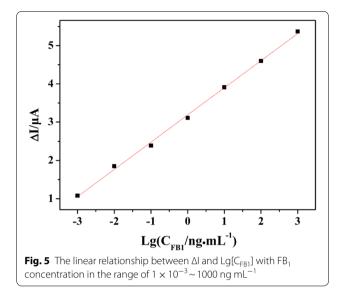


Fig. 4 The effect of FB₁ incubation time (**a**), Exo-I amount (**b**) and Exo-I incubation time (**c**) on the electrochemical signal

range of $1 \times 10^{-3} \sim 1000$ ng·mL⁻¹, a linear relationship between ΔI and Lg [C_{FB1}] was observed, and the linear regression equation was $\Delta I = 0.71036$ Lg[C_{FB1}] + 3.18714 ($R^2 = 0.998$). The limit of detection (LOD) was calculated to be 0.15 pg·mL⁻¹ at a signal-to-ratio of 3. Compared to



the previous reports, the designed aptasensor obtained a wider linear range and lower LOD, and the result was shown in Table 1.

Specificity, reproducibility, repeatability and stability

The specificity of the aptasensor to ochratoxin A (OTA), zearalenone (ZEA) and aflatoxin B_1 (AFB₁) was studied, and the results were shown in Fig. 6. Only when the prepared aptasensor was incubated in FB₁, the peak current decreased significantly, indicating that the designed aptasensor had good specificity and could meet the experimental requirements.

Under the optimized conditions, the reproducibility and the repeatability of the fabricated aptasensor was respectively evaluated with inter-assay and intra-assay. Under the same experimental conditions, five fabricated aptasensors were tested by monitoring the peak current of MB with 1 μg mL $^{-1}$ FB $_1$ on the FB $_1$ /Apt/cDNA/AuE, and a relative standard deviation (RSD) of 5.72% was calculated, implying that the fabricated sensor had satisfactory reproducibility. The one aptasensor was investigated by monitoring the peak current of MB in the presence of 1 μg mL $^{-1}$ FB $_1$ for five replicate determinations under the same conditions, and RSD of 5.38% was calculated, implying that the fabricated aptasensor had acceptable repeatability.

For the study on stability of the fabricated aptasensor, the peak current of MB on the three Exo-I/Apt/cDNA/AuE was detected, and the average peak current is 7.21 μA . Then the fabricated aptasensors were stored at 4 °C. After a 35-day storage period, the average peak current of MB on the Exo-I/Apt/cDNA/AuE was 6.14 μA , and the aptasensor retained 85.2% of its initial current response, indicating the acceptable stability.

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Table 1 Comparison with other reported methods for FB₁ detection	Table 1	Comparison	with other re	ported methods	for FB₁ detection
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Method	Amplification strategy	Linearity, (ng mL ⁻¹)	LOD, (ng mL ⁻¹)	Refs.
Chemiluminescence and enzyme-linked immunosorbent	ECL-ELISA based on anti-FB ₁ IgG and HRP	0.14-0.9	0.09	[17]
Chemiluminescence	Charge-coupled device	2.5-500	2.5	[18]
Fluorescence	Anti apt/Apt-NH ₂ /TiO ₂ -PSi	0.001-10	0.21×10^{-3}	[5]
Fluorescence resonance energy transfer	AuNPs-MB-UCNPs	0.01-100	0.01	[19]
Electrochemiluminescence	MIP/Ru@SiO ₂ /CS/AuNPs/GCE	$1 \times 10^{-3} \sim 100$	0.35×10^{-3}	[6]
Electrochemical immunosensor	AP-anti-antibody/anti-FB ₁ /FB ₁ -BSA-SWNTs/CS/GCE	0.01-1000	2×10^{-3}	[20]
Electrochemical immunosensor	Ab-AuNPs-PPy/ErGO-SPE	200-4500	4.2	[21]
Electrochemical magneto immunosensor	FB1-HRP/Ab-FB ₁ /MB&protein G/CSPE	0.73-11.2	0.33	[22]
Electrochemical aptasensor	Apt-AuNPs-SPCE	$1 \times 10^{-2} \sim 50$	3.4×10^{-3}	[7]
Electrochemical aptasensor	GS-TH/S2/S1/Au/GCE	$1 \times 10^{-3} \sim 1000$	1×10^{-3}	[23]
Electrochemical aptasensor	Exo-I/Apt/cDNA/AuE	$1 \times 10^{-3} \sim 1000$	0.15×10^{-3}	This wo

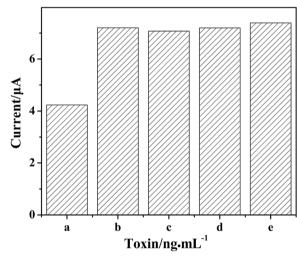


Fig. 6 The peak current of aptasensor incubated in different toxins with the same concentration of 1 ng mL $^{-1}$. a FB₁, b OTA, c ZEA, d AFB₁, e Blank

Analysis of FB₁ in food samples

The accuracy of the fabricated aptasensor was evaluated by studying the recovery of FB $_1$ in beer samples and corn samples, and the results were shown in Table 2. Beer samples were filtrated through a 0.45 μm membrane, and used for subsequent tests by spiking different concentrations of FB $_1$. Non-contaminated corn samples were finely milled to obtain corn powder, and 0.5 g of the corn powder was extracted with methanol—water (60:40, v/v. 5 mL) using an orbital shaker for 30 min. After centrifugation for 15 min, the extract was used for analysis by spiking different concentrations of FB $_1$. By addition of 100 ng mL $^{-1}$, 1 ng mL $^{-1}$ and 1×10^{-2} ng mL $^{-1}$ of FB $_1$, for the beer samples, the average recoveries were 88.5%, 96.1% and 98.6%, respectively. For the corn samples, the

Table 2 Recovery of FB₁ in food samples

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Sample	Added (ng mL ⁻¹)	Average found (ng mL ⁻¹)	Average recovery (%)	RSD (%), n = 3
Beer	100	88.5	88.5	1.75
	1	0.961	96.1	2.25
	1×10^{-2}	0.986×10^{-2}	98.6	5.65
Corn	100	91.4	91.4	4.76
	1	0.873	87.3	7.79
	1×10^{-2}	1.068×10^{-2}	106.8	6.34

average recoveries were 91.4%, 87.3% and 106.8%, respectively. These results indicated that the fabricated aptasensor can be applied in FB₁ detection of the food samples.

Conclusion

In summary, on the basis of DNA and Exo-I as signal amplification strategy, a novel and facile signal-off aptasensor was developed for FB₁ detection. Utilizing the favorable combination of MB with double-stranded DNA and G-rich cDNA, the specific DNA was designed to enrich abundant MB for initial signal amplification. On the other hand, with the advantages of easy design, simple operation, high amplification efficiency and excellent selectivity, Exo-I was used to design a novel signal-off aptasensor for amplifying the ΔI . These two signal amplification strategies can avoid the complicated nanomaterial preparation and instability. As a result, this proposed aptasensor showed the favorable performance with simple preparation, good selectivity, reproducibility, repeatability, stability as well as a wider linear range with lower LOD, providing a promising potential for application in food safety detection.

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Abbreviations

DNA: deoxyribonucleic acid; Exo-I: exonuclease-I; FB₁: fumonisin B₁; cDNA: complementary DNA; MB: methylene blue; Apt: aptamer of FB₁; DPV: differential pulse voltammetry; EIS: electrochemical impedance spectroscopy; MCH: 6-mercapto-1-hexanol; AuE: the gold electrode; R_{ct}: the charge transfer restrance; ΔI : the difference of peak current; LOD: limit of detection; OTA: ochratoxin A; ZEA: zearalenone; AFB₁: aflatoxin B₁; RSD: relative standard deviation.

Acknowledgements

Not applicable.

Authors' contributions

MW, FZ, SF and HJ conceived and designed the experiments; FZ and SF performed the experiments; MW and HJ analyzed the data; MW, FZ, and SF wrote and modified the paper. All authors read and approved the final manuscript.

Funding

This study was supported by the Natural Science Foundation of Henan Province (182300410188) in the design of the study, and collection, analysis, and interpretation of data; supported by the Fundamental Research Funds for the Henan Provincial Colleges and Universities in Henan University of Technology (2016RCJH04) in collection, analysis, and interpretation of data; supported by Key Scientific and Technological Project of Henan Province (192102310255) in writing the manuscript.

Availability of data and materials

All data generated or analyzed during this study are included in this published article. We have presented all data in the form of tables and figures.

Competing interests

The authors declare that they have no competing interests.

Received: 12 July 2019 Accepted: 30 October 2019 Published online: 09 November 2019

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