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Radiomics and Deep Learning from Research to Clinical Workflow: Neuro-Oncologic Imaging

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Imaging plays a key role in the management of brain tumors, including the diagnosis, prognosis, and treatment response assessment. Radiomics and deep learning approaches, along with various advanced physiologic imaging parameters, hold great potential for aiding radiological assessments in neuro-oncology. The ongoing development of new technology needs to be validated in clinical trials and incorporated into the clinical workflow. However, none of the potential neuro-oncological applications for radiomics and deep learning has yet been realized in clinical practice. In this review, we summarize the current applications of radiomics and deep learning in neuro-oncology and discuss challenges in relation to evidence-based medicine and reporting guidelines, as well as potential applications in clinical workflows and routine clinical practice. Keywords: Radiomics; Deep learning; Neuro-oncology; Clinical workflow

INTRODUCTION

Radiomics involves the extraction of high-dimensional quantitative data reflecting imaging phenotypes. The methods currently adopted in oncologic imaging studies rely strongly on machine learning (1, 2). Deep learning, a form of machine learning involving a special type of artificial neural network (3), is gaining much attention for its use in image-based pattern recognition in oncologic imaging. The goals of radiomics and deep learning studies in oncology are as follows: 1) classification of tumors, 2) providing links to genomics, 3) prediction of outcomes,

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This is an Open Access article distributed under the terms of the Creative Commons Attribution Non-Commercial License (https://creativecommons.org/licenses/by-nc/4.0) which permits unrestricted non-commercial use, distribution, and reproduction in any medium, provided the original work is properly cited. and 4) response monitoring. Potential applications for deep learning and radiomics have been discussed and published in leading peer-reviewed neuro-oncologic journals, but none of these potential applications has yet been realized in clinical practice. This may be because of the rare occurrence of many brain tumors and the low availability of the source material, with magnetic resonance imaging (MRI) being used as the main diagnostic tool. More importantly, the implementation of deep learning and radiomics is technically challenging and complicated to integrate into the clinical workflow, and there is not enough consideration of evidence-based medicine in deep learning and radiomics research. Because "if it was never used, it did not exist" (4), this article reviews the potential clinical applications of radiomics and deep learning, and discusses the special considerations in neuro-oncology, with the hope of yielding more actionable change to clinical workflows.

Trends of Radiomics and Deep Learning Research in Neuro-Oncology

Deep learning involves a special type of artificial neural network that resembles the human cognitive system and is a form of machine learning. Deep learning methods, especially convolutional neural networks (CNNs), excel at pattern recognition and finding complex patterns



in imaging data, and are generally more effective than previous algorithms (3). Deep learning algorithms use a data-driven approach and do not require prior definition by human experts.

Radiomics approaches involve the extraction of hundreds of quantitative features from images to assess the entire three-dimensional (3D) tumor phenotype. The resulting features may then be used as quantitative imaging biomarkers. Briefly, morphologic features (volume/shape), histogram features (first-order), texture features (secondorder), and transform-based features are the most commonly used radiomics features (1, 5). Typically, machine-learning techniques are subsequently applied to the extracted radiomics features in a feature selection step to reduce the dimensions of the data.

Figure 1 demonstrates imaging-based radiomics and

deep learning tasks in neuro-oncology. Extensive research articles using deep learning and radiomics in neurooncology have been published. The clinical situations include the differential diagnosis of neoplasms, prognosis determination at initial imaging, distinguishing tumor recurrence from post-treatment contrast enhancement due to pseudoprogression or early tumor progression in glioblastoma (6) on post-therapeutic imaging after first-line treatment regimens, and predicting the treatment response to anti-angiogenic (7, 8) and immunotherapies (9) at the time of recurrence. Representative applications of deep learning and radiomics in neuro-oncology are summarized in Table 1. Later in this review, we will demonstrate the utility of radiogenomics as a supplement to preexisting diagnostic techniques.



Fig. 1. Imaging-based radiomics and deep learning tasks in neuro-oncology. Deep learning can be applied to automated tumor segmentation to track tumor volumetry and pattern recognition to conduct various end-to-end classification tasks. Radiomics approaches using engineered features and machine learning-based feature selection have also been applied to radiogenomics classification tasks, differential diagnoses, and diagnosis of early tumor progression. Imaging phenotypes identified using deep learning and radiomics could ultimately be combined with clinical characteristics to assess prognosis and treatment response of individual patients.

Table 1. Representative Applications of Radiomics and DL in Neuro-Oncology

Торіс	Methods	References	Data (Train:Test)	Outcomes	Test Performance	External Validation	Imaging Modalities
Differential	Radiomics	Artzi et al.	439 (351:88)	Glioblastoma,	Accuracy = 85%	No	Conventional
diagnosis		(10)		metastasis	AUC = 0.98		MRI
	Radiomics	Kang et al. (11)	154 (112:42)	PCNSL, glioblastoma	AUC = 0.94 (external validation)	Yes	Conventional MRI, DWI
	Radiomics	Kniep et al. (12)	189	Metastasis cell type	AUC = 0.64 for non-small cell lung cancer AUC 0.82 for melanoma	No	Conventional MRI
Prognostication	Radiomics	Kickingereder et al. (14)	119 (179:40)	Glioblastoma survival	C-index = 0.696 (radiomics + clinical) C-index = 0.637 (radiomics only)	No	Conventional MRI
	Radiomics	Kickingereder et al. (16)	181 (120:61)	Glioblastoma survival	IBS = 0.103 (molecular + clinical + radiomics) IBS = 0.127 (radiomics only)	No	Conventional MRI
	Radiomics	Bae et al. (15)	217 (split-sample)	Glioblastoma survival	Integrated AUC = 0.652	No	Conventional MRI
	DL	Lao et al. (19)	102 (75:37)	Glioblastoma survival	C-index = 0.739 (clinical + radiomics) C-index = 0.710 (radiomics only)	No	Conventional MRI
	DL	Nie et al. (20)	69	WHO grade II and III	Accuracy = 89.9% (low- and high-risk)	No	Conventional MRI, fMRI, DTI
Pseudoprogression vs. progression	Radiomics	Kim et al. (6)	118 (61:57)	Glioblastoma pseudoprogression	AUC = 0.96 (internal validation), 0.85 (external validation)	Yes	Conventional MRI, DWI, DSC
	DL	Hu et al. (21)	31	Glioblastoma pseudoprogression	AUC = 0.95	No	Conventional MRI, DWI, DSC
	DL	Qian et al. (24)	35	Glioblastoma pseudoprogression	AUC = 0.867	No	DTI
	DL	Jang et al. (25)	78 (59:19)	Glioblastoma pseudoprogression	AUC = 0.83	Yes	Conventional MRI
Treatment response assessment	Radiomics	Kickingereder et al. (7)	172 (112:60)	Glioblastoma Anti-angiogenic treatment	Stratification between low- and high-risk HR = 1.85 (PFS) HR = 2.60 (OS)	No	Conventional MRI
	Radiomics	Grossmann et al. (8)	293 (126:167)	Glioblastoma Anti-angiogenic treatment	Stratification between low- and high-risk HR = 4.5 (PFS) HR = 2.5 (OS)	Yes	Conventional MRI
	Radiomics	Bhatia et al. (9)	88	Metastasis (melanoma) Immune checkpoint inhibitor	HR = 0.68 (0S)	No	Conventional MRI

AUC = area under receiver operating characteristic curve, Conventional MRI = to T1-weighted, T2-weighted, fluid-attenuated inversion recovery, or contrast-enhanced T1-weighted imaging, DL = deep learning, DSC = dynamic susceptibility contrast, DTI = diffusion-tensor imaging, DWI = diffusion-weighted imaging, fMRI = functional MRI, HR = hazard ratio, IBS = integrated Brier score, OS = overall survival, PCNSL = primary central nervous system lymphoma, PFS = progression-free survival, WHO = World Health Organization

Initial Diagnosis: Differential Diagnosis Using Radiomics

Radiomics

Radiomics has been applied to cases of differential diagnoses that were challenging even for radiologists. Furthermore, studies have assessed the added value of radiomics over the performance of radiologists. The differential diagnosis between a single brain metastasis and glioblastoma for a solitary contrast-enhancing (CE) mass is challenging. However, radiomics based on conventional post-contrast T1-weighted imaging showed an accuracy of 85% and an area under the receiver operating characteristic curve (AUC) of 0.96 (10). Primary central nervous system lymphoma (PCNSL) may exhibit internal necrosis and heterogeneous contrast enhancement that mimics glioblastoma. The potential of radiomics from the apparent diffusion coefficient (ADC) has been shown to differentiate PCNSL from glioblastoma (11), showing high performance on both internal (AUC 0.984) and external (AUC 0.944) validation sets. Radiomics was shown to be feasible for classifying the subtype of brain metastases (12), with its performance ranging from an AUC of 0.64 for non-small-cell lung cancer to 0.82 for melanoma. As diagnostic decisionmaking for patients with unknown primary lesion sites requires extensive steps, early differential diagnoses may be helpful to narrow down the diagnostic processes. However, few studies have been conducted regarding using deep learning for differential diagnoses, which may be due to the low availability of MRI source data from patients.

Survival Prediction

Radiomics

The prognostication of glioblastoma is of particular interest, as the prognosis for patients with glioblastoma remains poor, with a median survival of 15 months (13). The poor prognosis may arise from intratumoral heterogeneity, with resistance to treatment occurring both spatially and temporally. Radiomics allows for the noninvasive quantitative characterization of tumors, and studies have shown the added value of radiomics to the well-established prognostic markers of age, the extent of surgery, Karnofsky performance score, and methylation status of the *O6methylguanine-DNA methyltransferase (MGMT) gene*. Using standard-of-care imaging, radiomic analysis improved survival prediction when combined with clinical data (C-index improving from 0.637 to 0.696) (14) or genetic data (15, 16). One study emphasizes the automatization and reproducibility of a radiomics model (17).

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Deep Learning

To overcome the problem of small datasets, transfer learning, and fine-tuning has been adopted (18) for survival prediction in glioma patients. A deep feature-based radiomics model using transfer learning to extract a large number of deep features from hidden lavers of the CNN was applied to glioblastoma (19) and showed a C-index of 0.710 using radiomics features alone and 0.739 using radiomics and clinical predictors. Using multimodal imaging, including conventional MRI, functional MRI, and diffusion-tensor imaging (DTI), a deep learning architecture involving a 3D CNN extracted defining features from high-grade gliomas (20). This CNN showed an accuracy of 89.9% for predicting overall survival (OS) in 69 patients with high-grade gliomas, although it was without independent validation. The above findings suggest the feasibility of deep learning methods coupled with traditional radiomics features and machine learning classifiers for predicting survival. Nonetheless, studies are limited to showing the technical feasibility of deep learning applied for glioma survival prediction with small datasets, with or without an independent validation set. The proof of real-world performance on a large dataset is ultimately needed.

Follow-Up: Pseudoprogression vs. Tumor Progression

Radiomics

The differentiation of true progressive disease from pseudoprogression is challenging on conventional MRI. Before the advent of radiomics, machine learning classifiers (21) and clustering (22) methods have been adopted to solve this question using multiparametric imaging parameters, not with radiomics but with the quantitative value obtained from diffusion-weighted and perfusionweighted imaging. Using high-dimensional radiomics features, multiparametric MRI can include physiologic information that helps improve the differentiation of pseudoprogression from tumor progression. MR perfusion radiomics using relative cerebral blood volume (CBV) and the capillary permeability measure K_{trans} showed the diagnostic ability for pseudoprogression in a multiinstitution setting (23). A multiparametric radiomics model including the ADC and CBV showed better performance on external validation (AUC, 0.90) than a single ADC or CBV

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parameter (AUC, 0.57–0.79), or a radiomics model based on T1-weighted images (T1WIs), or T2-weighted images (T2WIs; AUC, 0.76) (6).

Deep Learning

Deep learning applications have adopted multiparametric MRI, with both conventional and physiologic MRIs being frequently used. One study used longitudinal DTI, dictionary learning, and feature pooling to characterize two conditions (24), and showed an AUC of 0.867 for 35 patients without an independent validation set. More recently, a CNN with long short-term memory (25) was applied to differentiate tumor progression from pseudoprogression based on post-contrast T1-weighted MRI data from two institutions, with 59 patients in the training set and 19 patients in the external validation set, yielding an AUC of 0.83. The above deep learning applications were designed as proof-of-concept studies with small numbers of patients and a cross-sectional design.

Before Second-Line Treatment: Predicting Treatment Response Using Radiomics

The anti-angiogenic agent bevacizumab is the single most widely used second-line therapeutic option for recurrent glioblastoma. However, no validated imaging biomarker is available to identify patients for whom this agent is likely beneficial. Two articles demonstrated the application of radiomics approaches to anti-angiogenic treatment. Using 4842 radiomics features of T1WI, T2WI, and contrastenhanced T1WI and analyzed with a supervised principalcomponent analysis, Kickingereder et al. (7) stratified patients into those with a low- or high-risk of recurrent glioblastoma (hazard ratio [HR] = 1.85 for progression-free survival [PFS] and HR = 2.60 for OS), and the low-risk group (172 patients, training:validation = 2:1). Using 65 radiomics features extracted from T1WI, T2WI, and contrast-enhanced T1WI of the multicenter BRAIN trial data, another study (8) showed successful stratification of recurrent glioblastoma patients according to OS (HR = 2.5) and PFS (HR = 4.5).

A recent study (9) showed the potential of the radiomics approach with contrast-enhanced T1WI brain metastasis treated with immune checkpoint inhibitors. In a total of 196 melanoma brain metastases from 88 patients, multiple radiomics features were found to be associated with OS, and the Laplacian of the Gaussian features best explained the OS (HR = 0.68), which was also confirmed in a validation dataset consisting of 17 patients.

Evidence-Based Medicine: Challenges for Radiomics and Deep Learning in the Clinical Workflow

The critical assessment of deep learning and radiomics studies should be based on the widely recognized principles of evidence-based medicine. Although these requirements are not always paid much attention in technical papers, they have paramount importance in clinical studies and applications. Prediction models developed from radiomics and deep learning aim to support clinical decision-making by the use of large amounts of complex data, and the validation and transparent reporting of results is important.

Validation in Deep Learning and Radiomics

For external validation, it is recommended to use adequately sized datasets that are collected either from newly recruited patients or from institutions other than those that provided the training data from which the deep learning and radiomics was developed (26).

A prospective diagnostic cohort design is a way to adequately represent the manifestation spectrum of target patients in real-world clinical settings, with a before-after study design being applied (27). In this design, patients undergo evaluation both without (before) and with (after) a diagnostic or predictive deep learning/radiomics tool, and the clinical decisions, instead of patient outcomes, are compared between the two diagnostic evaluation sessions (28, 29).

One study evaluated radiomics studies (30) published up until 2018 using the search terms "radiomics" and "radiogenomics" in the PubMed, MEDLINE, and EMBASE databases. Among 77 studies with impact factors above 7.0, only 18.2% (14 studies) performed external validation. Only three studies performed prospective validation, but even this was a post-hoc analysis of the prospective registry or database. None of the studies used a diagnostic cohort design or performed a cost-effectiveness analysis.

A similar trend was found for deep learning studies in an article that evaluated the design characteristics of general artificial intelligence (AI) studies (31) using the search terms "artificial intelligence" OR "machine learning" OR "deep learning" OR "convolutional neural network" for articles published up to 2018 in the PubMed, MEDLINE, and EMBASE databases. This review found that most studies that evaluated the performance of AI algorithms for the diagnostic analysis of medical images were designed as



proof-of-concept technical feasibility studies. Only 31 (6%) of the 516 studies performed external validation, and none of the 31 studies adopted all three design features of a diagnostic cohort design, inclusion of multiple institutions, and prospective data collection for external validation.

A model built with radiomics, and deep learning should not be limited to the patient population used for model construction. A high standard for the validation of radiomics and deep learning must be encouraged to transfer the techniques to routine clinical practice and prevent them from being stranded in the research domain (26).

Reporting Guidelines

Radiomics and deep learning applications in radiology may be sensitive to the characteristics of the study population, predictors, and choice of the reference standard. Comprehensive and transparent reporting is required to ensure that the performance of prediction models is generalizable. For predictive models, the transparent reporting of a multivariable prediction model for individual prognosis or diagnosis (TRIPOD) statement (32) emphasizes the transparent reporting of the study settings, outcome followup intervals, and precise definitions of the study design elements and how outcomes were defined and measured.

In a review of 77 radiomics studies (30), the mean number of TRIPOD items reported was 18.51 ± 3.96 (mean \pm standard deviation; range, 11–26). All articles clearly defined all predictors (item 7a) and described how predictors were handled (item 10a), but no article described the recalibration of the coefficients in the preexisting model in the methods (item 10e) or results (item 17) section. The radiomics studies showed less than 25% adherence to "explicitly describe the development/validation of the model or both in 'title' (2.6%, item 1), 'abstract' (7.8%, item 2), 'or introduction' (16.9%, item 3b)." Furthermore, the radiomics studies did not adhere to "calculate sample size" (6.5%, item 8) and "describe missing data" (11.7%, item 9).

Recently, the importance of adhering to established methodological standards has been identified for machine learning techniques. Although many aspects of the TRIPOD statement apply to radiomics/deep learning-based prediction model studies, TRIPOD focuses on regressionbased prediction model approaches (33). TRIPOD has not been widely adopted by the AI community. A new initiative to develop a version of the TRIPOD statement specific to machine learning will be announced in the near future.

Comparative Accuracy: Potential Applications of Radiomics and Deep Learning in Clinical Workflow in Neuro-Oncology

To be adopted in clinical practice, deep learning and radiomics must address unmet needs or improve existing situations. A conceptual framework for evaluation of the comparative accuracy of new diagnostic tests was developed by Bossuyt et al. (34), and it consists of the following: 1) replacement situation, 2) triage situation, and 3) addon situation. The replacement situation is when a new test differs from existing methods in various ways, including improved accuracy, ease, comfort, and speed, and may replace existing tests. In triage, the new test is used before the existing test or testing pathway, and only patients with a particular result on the triage test continue on the testing pathway. This may be less accurate than existing tests and is not meant to replace them. Add-on test scenarios may also be positioned after the existing pathway, and the use of these tests may be limited to a subgroup of patients. The new test is more accurate but is otherwise less attractive than the existing tests. The matched clinical scenarios in neuro-oncology are tumor segmentation to replace manual segmentation, detection-based triage in brain metastasis, and radiomics to supplement existing information. Figure 2 demonstrates radiomics and deep learning in the clinical workflow and their roles in existing diagnostic pathways.

Replacement: Deep Learning-Based Automatic Tumor Volumetry and Tumor Response Assessment

Deep learning-based segmentation may replace manual segmentation. This would be beneficial as computers do not tire and can provide fast and reproducible segmentation. Deep learning-based segmentation approaches for brain MRI are gaining interest in their self-learning and generalization abilities with large amounts of data (35-37). Most neurooncologic imaging studies are based on MRI, which is particularly challenging with respect to the generalizability and robustness of radiomics analysis, as MRI has nonstandardized pixel values and typically shows large variations in signal intensities. The robust segmentation required for the determination of tissue volumes imposes a great challenge for quantitative imaging analysis (5). Even expert readers show high inter-reader variability in segmentation, which can affect quantitative analysis (38, 39) and the extraction of high-dimensional radiomics features (1, 2, 40, 41).



Fig. 2. Radiomics and deep learning in clinical workflow and their roles in existing diagnostic pathways. Replacement: deep learningbased tumor volumetry has potential to replace human-derived manual tumor volumetry for defining image-based progression and non-progression. Triage: deep learning-based metastasis detection has potential to triage patients and identify those whose imaging needs to be read first and may increase radiologists' specificity and reduce tiredness. Add-on: radiogenomics applications have potential to stratify further high-risk and low-risk groups and may help guide patient management. Adapted from Bossuyt et al. *BMJ* 2006;332:1089-1092 (34).

Deep learning-based segmentation of brain tumors has been a long-standing topic of interest in the field of neurooncology and has mainly been driven through the Brain Tumor Segmentation (BraTS) challenge (42). Specifically, the annual BraTS challenge provides an important forum for evaluating state-of-the-art methods for the volumetric segmentation of brain tumors using multiparametric MRI scans. However, despite recent developments, clinical translation of the volumetric assessment of brain tumors (e.g., for assessing treatment response) is lacking. Currently, the Response Assessment in Neuro-Oncology (RANO) criteria, which primarily rely on manual two-dimensional (2D) measurements of CE target lesions on MRI, are the standard method for assessing the treatment response of brain tumors. Underlying the use of RANO is the assumption that tumors grow spherically and that the 2D measurement of a lesion's largest diameter on MRI is a surrogate marker of tumor volume. However, this assumption is not always accurate in clinical practice, as brain tumors frequently display very complicated shapes and anisotropic growth, influenced in part by the surrounding anatomic boundaries, host tissue-tumor interface, and/or treatment-related effects (e.g., areas of necrosis and surgical cavities). Consequently, there has been a long-standing interest in using volumetric assessment of tumor burden (43-45), with studies indicating that volumetric measurements may be more reliable and accurate than 2D measurements (46, 47). Nevertheless, although volumetric assessment may

arguably be one of the most quintessential parameters for the accurate assessment of tumor burden and response (48), it lacks practicality in a clinical setting. Whereas 2D measurements of tumor diameter can be performed quickly and without dedicated software, volumetric measurements require sophisticated and time-consuming post-processing of MRI data with dedicated software (7, 16, 49).

Recently, the importance and meaningful clinical use of deep learning-based BraTS were demonstrated in terms of the automated and quantitative assessment of treatment response (49). Specifically, it was shown that automated deep learning-based volumetric assessment was highly accurate, with DICE coefficients of more than 0.90 for the segmentation of CE tumor and non-enhancing T2/fluid-attenuated inversion recovery (FLAIR) signal abnormalities on independent multicenter testing (49). Using deep learning-based tumor volumes for guantitative volumetric tumor response assessment, it was shown that 1) the reliability (i.e., agreement in the quantitative volumetrically defined time to progression [comparison of the radiologist's ground truth with the automated assessment with deep learning]) was significantly higher (by a margin of 36%) than the RANO assessment, and 2) that the automated volumetrically defined time to progression was a better surrogate endpoint compared with RANO for the OS of the patients (49). These findings provide evidence that the automated and reliable assessment of tumor response in neuro-oncology with



a high-throughput of cases is feasible, and clinically important for providing high-quality imaging endpoints.

Triage: Detecting Metastasis Using Deep Learning

Deep learning can be applied to the radiologists' routine workflow to reduce the effort required for existing tests and improve the overall workflow. Previous studies suggested that in a triage framework, radiologists could control for false-positive classifications through manual inspection, thereby leaving the triaging system to prioritize, review and benefit the workflow, even without accuracy improvements (50, 51). One study demonstrated the utility of CNNbased analysis of computed tomography for triage of acute neurological illnesses in the emergency department (52). After applying CNN-based triage, the urgent cases appeared earlier in the queue in the prioritized list than in the routine list without the application of CNN.

In neuro-oncology, computer-assisted triage may augment the clinician's detection and shorten the reading time. The detection of brain metastases is a tedious and time-consuming task for many radiologists, particularly with the growing use of thin-section multi-sequence 3D imaging. Technical developments have shown the feasibility of using 3D template matching (53, 54) and CNNs (55). One study (54) showed improvement of the radiologist's performance for detecting metastasis less than 100 mm-size from 89.83% to 100%. Imaging onlybased detection and diagnosis of brain metastases without radiologists would be unacceptable under the current regulations. Furthermore, algorithms will generally be overfitted to the training data and the performance will be suboptimal. Instead, an algorithm for automated detection of brain metastases may be initially used, with radiologists then validating the result to ensure that the final diagnoses are correct. Even high-quality weak labels would lead to improved classifier performance, and consequently to superior triage results.

Add-On: Super-Diagnostics for Genetic Mutations Using Deep Learning and Radiomics

Other new tests may be positioned after the existing pathway. The use of these tests may be limited to a subgroup of patients, for example, when the new test is more accurate but otherwise less attractive than the existing test. Add-on tests can increase the sensitivity of the existing pathway, possibly at the expense of specificity. Image-based diagnosis of genetic mutations is of great interest for glioma, and new deep learning or radiomics applications may provide more accurate diagnosis than preexisting methods.

The key genomic landscapes seen in diffuse gliomas (56) are isocitrate dehydrogenase (IDH) mutation, 1p/19a codeletions, MGMT-promoter methylation status, and epidermal growth factor receptor (EGFR) amplification mutation. According to the most recent 2016 World Health Organization classification, the hallmark molecular parameters for better classification of glioma are IDH and 1p/19q co-deletion status (56). MGMT methylation status reflects the ability of tumor cells to repair DNA damage from temozolomide (57). EGFR amplification reflects the molecular pathogenesis of glioblastomas (58). Deep learning and radiomics tend to be focused on a single genomic or molecular classification, with IDH mutation status being the most popular topic, having been investigated with T2/FLAIR imaging (59), contrast-enhanced T1WI (60), diffusion- and perfusion-imaging (61), and in combination with location information (62). Recent radiomics (63-65) and deep learning studies (66-69) have focused more on the characterization of multiple tumoral genetic mutations, rather than single genetic mutations, to provide an integrated view.

Radiomics

Recently, copy number variations and the DNA methylation profile have been adopted in radiogenomics research, with Kickingereder et al. (70) showing that the machine learning analysis of multiparametric MRI including diffusion-, perfusion-, and susceptibility-weighted imaging could potentially predict DNA methylation status and hallmark copy number variations in 152 glioblastomas. Hu et al. (71) demonstrated radiomics-based heterogeneity using 48 image-guided biopsies from glioblastomas and showed significant image correlations with T1WI, T2WI, and contrast-enhanced T1WI for predicting platelet-derived growth factor receptor A (77.1%), EGFR (75%), cyclindependent kinase inhibitor 2A (87.5%), and retinoblastoma transcriptional corepressor 1 (87.5%). The feasibility of predicting the core signaling pathway of glioblastoma was shown by Park et al. (72), who showed that copy number variations, insertion/deletion, and single nucleotide variations from next-generation sequencing could be predicted using multiparametric MRI radiomics. These approaches used multimodal imaging parameters to provide information on various genomic alterations.



Deep Learning

With the application of a CNN to 256 brain MRIs from the Cancer Imaging Archives dataset (67), a study showed a prediction accuracy of 94% for IDH status, 92% for *1p/19q* co-deletion status, and 83% for *MGMT*-promoter methylation status. Deep features obtained from DTI and dynamic susceptibility contrast imaging (208 training sets and 53 validation sets) were clustered (73), and different imaging subtypes of glioblastoma were stratified by IDH-1, *MGMT*, and EGFR mutations. Radiogenomic assessment beyond routine imaging diagnosis should stratify low- and high-risk patients and may further guide patient consultations and therapeutic plans.

Infrastructure to Be Integrated into the Clinical Workflow

Ultimately, the driver for clinical adoption may reside in the implementation and availability of AI applications integrated into the picture archiving and communication system (PACS) at the reading station. The integration of concise and standardized AI interpretation results directly into the Digital Imaging and Communications in Medicine standard could enable easier portability among PACSs.

The current AI frameworks are primarily accessible by computer scientists. While this is acceptable for interdisciplinary groups that have both clinical and technical experts, the adoption of such frameworks by primarily clinical sites and for clinical deployment will require substantial effort to improve the transparency of the methods, the accessibility of the frameworks, and enable prospective large-scale on-demand application in clinical routine. A prime example is the open-source Extensible Neuroimaging Archive Toolkit (XNAT; www.xnat.org), which provides the necessary software infrastructure for importing, archiving, processing, and securely distributing neuroimaging studies (74). Specifically, it also enables the integration of custom processing pipelines (e.g., deep learning-based BraTS through the XNAT Container Service Plugin) for large-scale evaluations (e.g., in clinical routine). Successful clinical translation of a deep learningbased processing pipeline and its integration within the XNAT framework was recently shown for automated quantitative (volumetric) tumor response assessment of MRI in neuro-oncology (www.neuroAI-HD.org) (49). Similar future endeavors with open-source deposition of AI-based processing pipelines (e.g., radiomic or deep learning-based prediction models, and deep learning-based BraTS tools)

will be important for independent large-scale validation and clinical adoption of AI-based processing pipelines.

Existing Drawbacks and Perspectives

The most distinct drawbacks of radiomics and deep learning from the feature-based perspective are that the features are data-driven, and there is no direct biological linkage. For example, while there are many existing datadriven features for IDH mutation based on deep learning and radiomics, these features are complex and not intuitive. Contrastingly, MR spectroscopy directly measures the byproduct of IDH mutation, 2-hydroxyglutarate, while the T2/FLAIR mismatch sign gives intuitive information on IDH mutation status. This is one reason why the utilization of 'complex' radiomics is more directed towards providing added value to pre-existing imaging diagnostics, rather than replacing them, especially from the perspective of comparative accuracy.

Another drawback to deep learning is that it is datadependent. Deep learning is 'data-hungry,' and a large amount of good quality data is required to maximize the accuracy of deep learning models. Insufficient data may mean that performance is insufficient to replace or augment pre-existing imaging diagnostics. Changing a modellearning method with meta-learner (75) or increasing the quantity of training data using synthetic data augmentation may improve model performance. From the perspective of comparative accuracy, deep learning will be more directed towards triaging and replacing mundane human tasks.

CONCLUSION

Radiomics and deep learning are active research areas in the field of neuro-oncology, and many studies have shown their potential for future clinical implementation. To be incorporated into existing clinical workflows, studies are recommended to adhere to evidence-based medicine and use data that are validated in the real-world setting. Automated tumor volumetry, the detection of brain metastases, and radiogenomics are highly likely to become end-uses for radiomics and deep learning in clinical practice. Finally, integrated infrastructure for the clinical translation of radiomics and deep learning will ultimately be needed.

Conflicts of Interest

The authors have no potential conflicts of interest to disclose.



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