

## ORIGINAL ARTICLE

# Unifying the Notions of Modularity and Core–Periphery Structure in Functional Brain Networks during Youth

Shi Gu<sup>1,2,3</sup>, Cedric Huchuan Xia<sup>2</sup>, Rastko Ciric<sup>2</sup>, Tyler M. Moore<sup>2</sup>, Ruben C. Gur<sup>2</sup>, Raquel E. Gur<sup>2</sup>, Theodore D. Satterthwaite<sup>2,†</sup> and Danielle S. Bassett<sup>2,3,4,5,6,7,†</sup>

<sup>1</sup>School of Computer Science and Engineering, University of Electronic Science and Technology of China, Chengdu, 611731, China, <sup>2</sup>Department of Psychiatry, Perelman School of Medicine, University of Pennsylvania, Philadelphia, PA 19104, USA, <sup>3</sup>Department of Bioengineering, School of Engineering & Applied Science, University of Pennsylvania, Philadelphia, PA 19104, USA, <sup>4</sup>Department of Physics and Astronomy, College of Arts and Sciences, University of Pennsylvania, Philadelphia, PA 19104, USA, <sup>5</sup>Department of Electrical and Systems Engineering, School of Engineering & Applied Science, University of Pennsylvania, Philadelphia, PA 19104, USA, <sup>6</sup>Department of Neurology, Perelman School of Medicine, University of Pennsylvania, Philadelphia, PA 19104, USA and <sup>7</sup>Santa Fe Institute, 1399 Hyde Park Rd, Santa Fe, NM 87501 USA

Address correspondence to Danielle S. Bassett, 210 S. 33rd Street, 240 Skirkanich Hall, Philadelphia, PA 19104-6321, USA. Email: dsb@seas.upenn.edu.

<http://orcid.org/0000-0002-6183-4493>

<sup>†</sup>Theodore D. Satterthwaite and Danielle S. Bassett contributed equally to this work.

## Abstract

At rest, human brain functional networks display striking modular architecture in which coherent clusters of brain regions are activated. The modular account of brain function is pervasive, reliable, and reproducible. Yet, a complementary perspective posits a core–periphery or rich-club account of brain function, where hubs are densely interconnected with one another, allowing for integrative processing. Unifying these two perspectives has remained difficult due to the fact that the methodological tools to identify modules are entirely distinct from the methodological tools to identify core–periphery structure. Here, we leverage a recently-developed model-based approach—the weighted stochastic block model—that simultaneously uncovers modular and core–periphery structure, and we apply it to functional magnetic resonance imaging data acquired at rest in 872 youth of the Philadelphia Neurodevelopmental Cohort. We demonstrate that functional brain networks display rich mesoscale organization beyond that sought by modularity maximization techniques. Moreover, we show that this mesoscale organization changes appreciably over the course of neurodevelopment, and that individual differences in this organization predict individual differences in cognition more accurately than module organization alone. Broadly, our study provides a unified assessment of modular and core–periphery structure in functional brain networks, offering novel insights into their development and implications for behavior.

**Key words:** development, functional brain networks, rich-club, modularity, executive function, adolescence

## Introduction

Human cognition and behavior are grounded in the brain's complex neuroanatomical architecture and reflected in its functional dynamics. Recent efforts in network neuroscience (Bassett and Sporns 2017), an interdisciplinary fusion of network science and neuroimaging, have begun to uncover network-level explanations for this architecture (Bullmore and Sporns 2009, 2012) and mechanisms for these dynamics (Hutchison et al. 2013; Chaudhuri et al. 2015). Here, network nodes are defined as brain regions, and network edges are defined as summary statistics, reflecting either interregional tractography in a structural brain graph or statistical relationships among regional activity time series in a functional brain graph (Fornito et al. 2013). The formal representation of the brain as a graph facilitates the application of graph theoretical tools to link the graph's topology and dynamic properties to higher-order cognition (Bassett et al. 2011, 2015; Chai et al. 2016), including changes in cognitive capabilities that accompany development (Gu et al. 2015; Chai et al. 2017).

In the context of human neuroimaging, one particularly important set of tools—community detection—offers methods to decompose a network into modules or communities (Sporns and Betzel 2016). A common example applied to both structural (Sporns et al. 2005; Hagmann et al. 2007) and functional (Van Den Heuvel and Pol 2010) brain graphs is modularity maximization (Newman 2006), which identifies groups of nodes such that nodes within a group are more densely connected to other nodes in their group than anticipated in an appropriate random network null model. While useful, modularity maximization and similar approaches such as Infomap (Rosvall and Bergstrom 2008) make the important assumption that the brain's mesoscale architecture is best characterized by modules that are maximally independent from one another. Such an assumption is not without support from philosophical work in neuroscience and psychology over the last few decades. For example, the Fodorian view is that modules are characterized by informational encapsulation, with little need to refer to other psychological systems in order to operate (Fodor 1983).

Nevertheless, despite its historical roots, recent empirical evidence and emerging theoretical understanding have begun to call into question the notion that the brain network architecture supporting complex cognition is best characterized by largely independent modules. At a neuroanatomical level, the pattern of white matter connections displays structural connectivity among modules (Hagmann et al. 2008), and the strength of that intermodule connectivity differs according to the modules involved (Betzel et al. 2018, 2019). The heterogeneous pattern of strong and weak intermodule connectivity at the large-scale level of white matter structure is thought to facilitate and constrain integration of neural activity across diverse cognitive systems, enabling their collective function (Baum et al. 2017). Consistent with these observations of underlying structure, at the physiological level, the pattern of functional connections also displays nontrivial integration between modules, with some module pairs being more or less integrated than others (Meunier et al. 2009). For example, executive modules such as the frontoparietal system tend to be more integrated with other brain systems (Power et al. 2013). The strength of between-module connectivity changes over development (Gu et al. 2015), differs in individuals in accordance with cognitive capabilities (Satterthwaite, Wolf, et al. 2015), and is altered in psychi-

atric diseases in both adults (Sharma et al. 2017) and youth (Satterthwaite, Vandekar, et al. 2015), underscoring its relevance to brain function.

An important open question is whether there is a simple organizing principle that explains the heterogeneous patterns of intermodule connectivity observed in both anatomy and function. For example, are modules connected in a small-world organization, where modules tend to form clusters enabling local integration between modules, with a few modules extending topologically long-distance connections to other modules enabling global integration? Or perhaps, a few modules serve as hubs in the intermodule network, while most modules are sparingly connected. While the literature has not settled on conclusive answers to these questions, one coarse-grained topological principle that has been shown to account for some of this heterogeneity is rich-club organization (Colizza et al. 2006), a specific sort of core-periphery structure (Borgatti and Everett 2000; Rombach et al. 2014; Zhang et al. 2015) whereby a set of highly connected and strongly interconnected hubs in the brain is complemented by a more sparsely connected network periphery (van den Heuvel and Sporns 2013). The core-periphery structure of underlying anatomy has important implications for the dynamics that can occur upon them (Betzel et al. 2016), to some degree explaining the core-periphery organization that is also observed in functional networks estimated from functional magnetic resonance imaging (fMRI) data collected during task performance (Ekman et al. 2012; Bassett, Wymbs, et al. 2013) and during the resting state (Gu et al. 2017).

The observation that both modular structure and core-periphery structure characterize brain graphs raises several challenging questions. How are modules related to cores or to peripheries? Is there a simple organizational principle explaining these 2 characteristics of network architecture? How is that principle altered across development or manifested in different individuals? Answering these questions is particularly challenging because the methodological tools to identify modules are entirely distinct from the methodological tools to identify core-periphery structure. Here, we employ a recently developed model-based approach—the weighted stochastic block model (WSBM) (Aicher et al. 2014)—that simultaneously uncovers modular structure, core-periphery structure, and other organizational features that can occur in networks with richly and heterogeneously connected modules (Betzel et al. 2018, 2019). We apply the WSBM to functional networks extracted from resting-state data acquired in a large sample of youth imaged as part of the Philadelphia Neurodevelopmental Cohort (PNC) (Satterthwaite et al. 2014). We hypothesized that functional brain networks would display rich mesoscale organization beyond that sought by modularity maximization techniques, that richer mesoscale organization would change over the course of normative neurodevelopment, and that individual differences in this organization would be more predictive of individual differences in cognition than individual differences in module organization alone (Gordon et al. 2016).

## Materials and Methods

### Participants

Resting-state fMRI data were obtained from  $n = 1601$  youth who participated in a large community-based study of brain development, now known as the PNC (Satterthwaite et al. 2014). The present sample includes  $n = 872$  participants between

the ages of 8 and 22 years (mean = 15.65, standard deviation [SD] = 3.3; 377 males, 495 females). A total of 729 of the initial 1601 participants were excluded for the following reasons. First, as in-scanner motion is the most important confound for studies of development, we used exclusion criteria that have been applied in many prior papers (Satterthwaite et al. 2012; Satterthwaite, Wolf, et al. 2013; Satterthwaite et al. 2014). The motion threshold for exclusion is either mean relative displacement > 0.2 mm or more than 20 frames with motion exceeding 0.25 mm. These criteria resulted in the exclusion of 478 subjects due to motion during the resting-state scan. Additionally, we excluded 80 subjects due to a poor quality  $T_1$  image, as judged by 3 expert manual raters who evaluated each image (for full details, see Rosen et al. 2018). Finally, as in prior studies of the PNC (Satterthwaite et al. 2014), we excluded 340 participants due to other factors that could impact brain function, including medical problems that could impact the central nervous system, potentially psychoactive medications, or a history of psychiatric inpatient hospitalization. Naturally, some subjects met more than 1 exclusion criterion, and therefore, the total number of excluded subjects was 729.

### Neurocognitive Battery

Cognition was measured outside the scanner using the Penn Computerized Neurocognitive Battery (CNB) (Gur et al. 2010, 2012). Briefly, the 1-h CNB was administered to all participants and consisted of 14 tests that evaluated a broad range of cognitive functions. Twelve of the tests measure both accuracy and speed, while 2 of the tests (motor and sensorimotor) measure only speed. Here, we used the factor score for executive efficiency from a best-fitting 4-factor solution comprising tests from the executive function domain, attention, abstraction, and working memory (Moore et al. 2015). The tests contributing to the executive efficiency score include the Penn Continuous Performance Test, the Letter N-Back task, and the Penn Verbal Reasoning Test (Moore et al. 2015, 2016, 2019). In the present study, we use this factor score for executive efficiency as our primary measure, hereafter referred to simply as “executive function.”

### Imaging Data Acquisition and Preprocessing

MRI data were acquired on a 3-Tesla Siemens Tim Trio whole-body scanner and 32-channel head coil at the Hospital of the University of Pennsylvania. A  $T_1$ -weighted image was acquired for each subject. All subjects underwent functional imaging (time repetition = 3000 ms, time echo = 32 ms, flip angle =  $90^\circ$ , field of view =  $192 \times 192$  mm, matrix =  $64 \times 64$ , slices = 46, slice thickness = 3 mm, slice gap = 0 mm, effective voxel resolution =  $3.0 \times 3.0 \times 3.0$  mm) during a 6-min resting-state sequence, during which a cross-hair for fixation was displayed.

Raw resting-state fMRI blood oxygen level-dependent (BOLD) data were processed using a preprocessing pipeline that has been shown to markedly reduce the impact of in-scanner motion with greater efficacy than other commonly used pipelines (Satterthwaite, Elliott, et al. 2013; Ciric et al. 2017). This pipeline included 1) distortion correction with FSL’s FUGUE utility, 2) template registration with MCFLIRT, 3) despiking with AFNI’s 3DDESPIKE utility, 4) demeaning to remove linear or quadratic trends, 5) boundary-based registration to the individual high-resolution structural image, 6) 36-parameter

global confound regression, and 7) first-order Butterworth filtering to retain signal in the 0.01 Hz to 0.08 Hz range. For all analyses of fMRI data, we excluded subjects with incomplete data or excessive motion, as previously noted.

### Network Construction

Here, we model the resting-state functional connectivity of each subject as a network (Bassett et al. 2018). We begin by noting that a simple networked system can be represented by the graph  $\mathcal{G} = (\mathcal{V}, \mathcal{E})$ , where  $\mathcal{V}$  and  $\mathcal{E}$  are the vertex and edge sets, respectively. Let  $a_{ij}$  be the weight associated with the edge  $(i, j) \in \mathcal{E}$ , and define the weighted adjacency matrix of  $\mathcal{G}$  as  $A = a_{ij}$ , where  $a_{ij} = 0$  whenever  $(i, j) \notin \mathcal{E}$ . In this study, each network node represents 1 of 333 cortical areas specified by the Gordon atlas (Fig. 1A). Each network edge was defined as the Pearson correlation coefficient between the regional mean BOLD time series of region  $i$  and region  $j$ , followed by the application of a Fisher’s  $r$ -to- $z$  transformation (Fig. 1B).

### Weighted Stochastic Block Model

Fundamentally, the stochastic block model is a generative model for random graphs that seeks to partition nodes into sets such that nodes with similar patterns of binary connectivity to the rest of the brain are grouped together with one another. Here, we applied a recent extension of this method to weighted graphs, commonly referred to as the WSBM (Aicher et al. 2014). Formally, we follow the notation in Aicher et al. (2014), which describes the generative model for weighted pairwise interactions among  $n$  vertices, with an exponential family distribution  $\mathcal{F}$  and a block structure  $\mathcal{R}$ . For a subject  $s$  with an adjacency matrix  $A^s$ , the probability of observing that graph given the model is

$$\Pr(A^s | z^s, \theta^s, \mathcal{M}_{\mathcal{F}, \mathcal{R}}^s) = \prod_{i \leq j} f^s \left( A_{ij}^s | \theta^s_{\mathcal{R}(z_i, z_j)} \right), \quad (1)$$

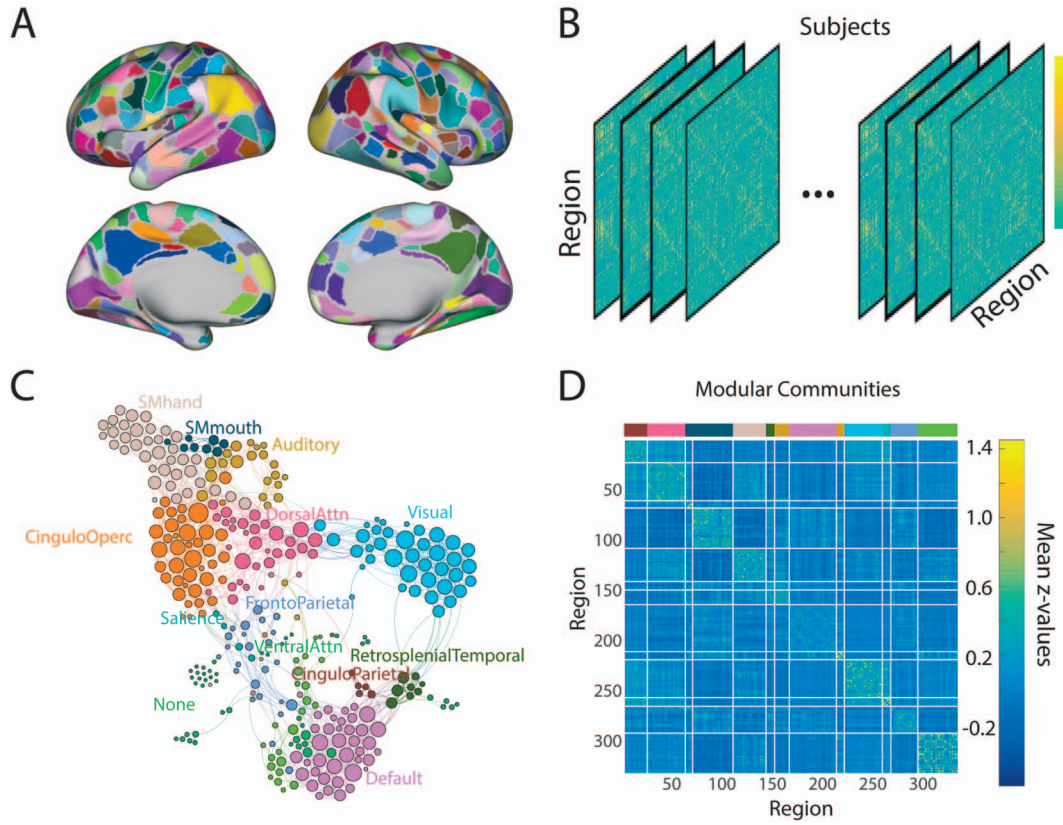
where  $z^s$  is the community label and  $\theta^s$  is the matrix of edge bundle parameters  $\theta$ . For an estimated model  $\mathcal{M}_{\mathcal{F}, \mathcal{R}}$ , the log-evidence score

$$\mathcal{L}_{\mathcal{M}_{\mathcal{F}, \mathcal{R}}} = \log \Pr(A | \mathcal{M}_{\mathcal{F}, \mathcal{R}}) \quad (2)$$

is used to quantify the goodness of fit and to inform model selection.

Next, we define summary statistics that can be used to describe the organization of the estimated block structure, and we also consider how to extend the model to reflect the shared structure in a group of subjects. We begin by supposing that we have  $N$  subjects with adjacency matrix  $A^1, \dots, A^N$  and the optimized density  $f^s$  with  $\Pr(A^s) = f^s(A^s)$ . Because the WSBM groups nodes together into sets (or blocks), we have the opportunity to quantify the interblock connectivity strength as well as the intrablock connectivity strength. For the block average adjacency matrix  $\Omega^s = \omega_{mn}^s$  with corresponding block set  $C_m$ , the block average strength between block  $m$  and  $n$  of subject  $s$  is defined as

$$\omega_{mn}^s = \begin{cases} \frac{\sum_{i \in C_m, j \in C_n, i \neq j} A_{ij}^s}{|C_m| \cdot |C_n| - |C_m|} & \text{if } m = n, \\ \frac{\sum_{i \in C_m, j \in C_n} A_{ij}^s}{|C_m| \cdot |C_n|} & \text{if } m \neq n, \end{cases} \quad (3)$$



**Figure 1.** A conceptual schematic. (A) We first subdivide the brain into 333 cortical areas from the Gordon atlas (Gordon et al. 2016) and extract the regional mean BOLD time series. (B) Next, we estimate the functional connectivity between all pairs of regions by calculating the Pearson correlation coefficient between regional time series and applying a Fisher  $r$ -to- $z$  transformation. For each subject, this approach produces a graph or network that we represent in an  $|\mathcal{V}| \times |\mathcal{V}|$  weighted adjacency matrix. (C) Traditionally, this sort of network has been subdivided into functional modules based on various community detection methods. Here, we show 1 example partition of network nodes (brain areas) into 13 modules (Power et al. 2007) forming auditory, cingulo-opercular (CinguloOperc), cingulo-parietal (CinguloParietal), default mode (Default), dorsal attention (DorsalAttn), salience, frontoparietal, retrosplenial temporal, somatomotor hand (SMhand), somatomotor mouth (SMmouth), ventral attention (VentralAttn), and visual systems. For clarity of visualization, nodes are color coded according to their module assignment, and we show the strongest 3% of edges in the group-averaged functional brain network. (D) When we plot the group-averaged functional connectivity matrix with nodes ordered by the 13 a priori defined modules, we observe a nonzero mean and heterogeneous pattern of intermodule connectivity.

and the block allegiance matrix  $F^s$  representing the expected strength between 2 regions for each subject is defined as

$$F_{ij}^s = \mathbb{E}^s \left( A_{ij}^t | \theta^s_{\mathcal{R}(z_i, z_j)} \right) = \omega_{z_i, z_j}^s, \quad (4)$$

where  $\mathbb{E}^s$  is the expectation of the estimated model of the  $s$ -th subject and  $z_i, z_j$  are the block labels of region  $i$  and region  $j$ .

The mean block average strength  $\bar{\Omega} = \{\bar{\omega}_{mn}\}$  is then defined as the mean of  $\Omega^s$  across subjects:

$$\bar{\omega}_{mn} = \frac{1}{N} \sum_{s=1}^N \omega_{mn}^s, \quad (5)$$

and the average block allegiance matrix is defined as the mean of  $F_{ij}^s$  across subjects:

$$F_{ij} = \frac{1}{N} \sum_{s=1}^N F_{ij}^s, \quad (6)$$

where  $N$  is the number of subjects.

### Identification of Group-Level Hierarchical Mesoscale and Macroscale Structures

In order to obtain an estimated hierarchical block structure at the group level, we designed a 4-step procedure composed of repeated application of the WSBM. At the first scale of the hierarchy (Step 1), we applied the WSBM-based clustering to single-subject functional connectivity matrices, and we varied the number of blocks  $k_s$  from  $k_{\min}$  to  $k_{\max}$  in increments of 1 to obtain individual-level estimates of block structure. To move to the next level of the hierarchy (Step 2), we computed the average block allegiance matrix  $F$  for each  $k_s$  using Equation (6). We examined the effect of  $k_s$  on  $F_{ij}$  to determine the value of  $k_s$  above which  $F_{ij}$  remained relatively stable. For the remaining steps in this hierarchical procedure, we fixed  $F$  at this stable architecture. Next (Step 3), we applied the WSBM to the fixed  $F$  and tuned the number of blocks  $k$  to attain the highest log-evidence. This procedure produced an optimal group-level mesoscale structure. From this structure, we next computed the associated mesoscale connectivity matrix, where each node represented a block from the WSBM and where each edge was weighted by the mean connectivity strength between pairs of blocks. Finally (Step 4), we applied the WSBM to this mesoscale connectivity matrix to



obtain a macroscale structure that represented the relationships among blocks. Through this 4-step procedure, we acquired the individual block structures as well as representative group-level mesoscale and macroscale structures, which we study throughout the article. For a flow diagram of the 4 steps, please see Supplementary Figure 1.

### Quantitative Examination of Core–Periphery Structure: Estimating the Regional Core Score

We used the core scores defined in Rombach et al. (2014) to perform our core–periphery analysis. The core score for node  $i$  is defined as

$$CS(i) = Z \sum_{\gamma} C_i(\gamma) \times R_{\gamma}, \quad (7)$$

where  $Z$  is the normalization factor so that  $\max_i[CS(i)] = 1$ , and  $\gamma = (\alpha, \beta)$  is the scale parameter for the local core value

$$C_i(\gamma) = C_i(\alpha, \beta) = \frac{1}{1 + \exp(-(\beta - |\mathcal{V}|) \times \tan(\pi\alpha/2))}, \quad (8)$$

where  $|\mathcal{V}|$  is the number of nodes, and  $R_{\gamma} = \sum_{ij} A_{ij} C_i C_j$  is the core quality.

### Identification of Interblock Relations in the Mesoscale Structure

After examining the existence of core–periphery relationships in the resting functional brain networks, we further investigated how different blocks interact with each other on the mesoscale. Consider a given pair of blocks  $m, n$  with associated within-block mean strengths  $\omega_{mm}$  and  $\omega_{nn}$  and with associated between-block mean strength  $\omega_{mn}$ . We say that this pair forms a “core–periphery pair” when  $|\omega_{mm}| \leq |\omega_{mn}| \leq |\omega_{nn}|$  (or  $|\omega_{nn}| \leq |\omega_{mn}| \leq |\omega_{mm}|$ ), a “bipartite pair” when  $|\omega_{mn}| \geq \max\{|\omega_{mm}|, |\omega_{nn}|\}$ , or an “independent pair” when  $|\omega_{mn}| \leq \min\{|\omega_{mm}|, |\omega_{nn}|\}$ .

After identifying the core–periphery pairs in the functional connectivity matrix, it is necessary to ask whether the findings are statistically significant. Here, we conduct a nonparametric permutation test to assess statistical significance. For a subject  $s$  with a block average adjacency matrix  $\Omega^s$ , we define  $H^s = \eta_{mn}^s$  as its characteristic matrix of core–periphery structure, where

$$\eta_{mn}^s = \begin{cases} -1 & \text{if } \omega_{mm} < \omega_{mn} \leq \omega_{nn} \\ 1 & \text{if } \omega_{nn} \leq \omega_{mn} < \omega_{mm} \\ 0 & \text{otherwise} \end{cases}. \quad (9)$$

The average core–periphery role  $H$  is then defined as the mean of  $H^s$  across subjects:

$$H = \frac{1}{N} \sum_{s=1}^N H^s. \quad (10)$$

To determine whether the core–periphery pairs are located uniformly at random, we consider a null model in which core–periphery pairs are chosen uniformly at random for each subject. Under the null hypothesis instantiated by this model, the probability  $\eta_{mn}^0$  that a pair  $mn$  is a core–periphery pair is estimated as  $(\sum_{s=1}^N |\eta_{mn}^s|) / N$  and its SD is  $\sigma_{mn}^0 = \sqrt{\eta_{mn}^0(1 - \eta_{mn}^0) / N}$ ,

where  $N$  is the number of subjects. The score of a pair  $mn$  being a core–periphery pair is then defined as

$$z_{mn} = \frac{|\eta_{mn}| - \eta_{mn}^0}{\sigma_{mn}^0}, \quad (11)$$

which represents the regularized difference between the frequency of pair  $mn$  and the expected probability of a random pair to appear as a core–periphery interaction. The associated  $p$  values are denoted as  $p_{mn}$  and calculated following the standard normal distribution. By applying a false discovery rate (FDR) correction for multiple comparisons, we can binarize the average core–periphery role  $H$  to  $\tilde{H} = \{\tilde{\eta}_{mn}\}$ , where  $\tilde{\eta}_{mn} = 1$  for  $p_{mn}^{\text{corrected}} < p_{\text{FDR}}$ , representing the existence of a significant core–periphery pair.

### Identification of Core–Periphery Junctions

After identifying core–periphery interactions, we next explored the possibility of complex conjunctions among multiple blocks. Specifically, by integrating core–periphery pairs with common blocks, we recognized a pattern that we call a “core–periphery junction.” Mathematically, a core–periphery junction is defined as a connected component of the core–periphery relationship graph (see Eqs. 9–10). Intuitively, a junction represents a sector of the system in which specific blocks act as linkers between a core block and a periphery block. By examining this integrated structure, we can probe relations between more integrative structures (cores) and more segregated structures (peripheries).

### Modularity Maximization

The modular structure is obtained by modularity maximization with a Newman–Girvan null model, where the modularity function is defined as

$$Q = \sum_{ij} \left[ \left( A_{ij}^+ - \gamma^+ \frac{p_i^+ p_j^+}{2\mu^+} \right) + \left( A_{ij}^- - \gamma^- \frac{p_i^- p_j^-}{2\mu^-} \right) \right] \delta(c_i, c_j), \quad (12)$$

where  $A^+$  is the positive part of the weighted adjacency matrix  $A$ ,  $A^-$  is the negative part of  $A$ ,  $p_i^+ = \sum_j A_{ij}^+$ ,  $p_i^- = \sum_j A_{ij}^-$ ,  $\mu^+ = \sum_{ij} A_{ij}^+$ ,  $\mu^- = \sum_{ij} A_{ij}^-$ ,  $c_i$  is the community assignment for node  $i$ , and  $\gamma^+$  and  $\gamma^-$  are resolution parameters that tune the relative size of modules detected. We optimized this modularity quality function using a Louvain-like locally greedy algorithm (Jutla et al. n.d.; Blondel et al. 2008). We performed a parameter sweep across values of  $\gamma$  (Bassett, Porter, et al. 2013) to identify a  $\gamma$  value that produced the same number of modules as the number of blocks in the WSBM. At that  $\gamma$  value, we then identified a consensus partition across multiple runs of the algorithm.

### Assessing the Variability or Consistency of Intra-block Edge Weights

We assessed the performance of the WSBM and modularity maximization algorithms by calculating the variance in the edge weights located within blocks or modules. Intuitively, this metric served to probe the fit of the model to the data, with low edge weight variability indicating greater internal homogeneity of blocks or modules. Biologically, we speculate that such homogeneity could be driven by the recently reported redundancy

of genetic encoding of functional connectivity, and age-related changes in that homogeneity could reflect developmental programming (Bertolero et al. 2019). Specifically, for subject  $s$  with  $k_s$  blocks or modules in its adjacency matrix, we denote the SD of edge weights within block  $m$ 's upper triangle as  $\sigma_m^s$ . Then, we calculate the SD  $\bar{\sigma}^s$  as the squared mean of  $\sigma_m^s$ 's, that is,

$$\bar{\sigma}^s = \sqrt{\frac{\sum_{m=1}^{k_s} (\sigma_m^s)^2}{k_s}}. \quad (13)$$

### Statistical Testing

Throughout the majority of the Results section, we reported standard parametric statistical tests and associated  $P$  values. In the context of Figures 4 and 5, we employed nonparametric permutation testing due to the nonnormal distribution of the data. First, the  $P$  value reported in Figure 4 was computed via a permutation test in which each of the 100 000 random instantiations was created by randomly shuffling the block labels and recalculating the within-block mean of core scores. These estimates then formed the null distribution of block-averaged core scores shown in the bottom row in Figure 4. Second, the  $P$  value reported in Figure 5B was computed via a 2-sample  $t$ -test between the distribution of the number of core-periphery pairs in the partition by WSBM and that in the partition obtained in a nonparametric permutation-based null model. For each subject, we randomly shuffled the block association achieved by WSBM for each node with the block size retained. Next, we applied the rule implemented in Figure 5A and Equation 9 to identify the number of core-periphery pairs for each subject. These estimates formed the null distribution that we used in the 2-sample  $t$ -test.

In the context of Figure 6, the correlations were computed between the block connectivity strength and age, after partialing out the effects of mean framewise displacement and sex. The standard  $P$  values associated with partial correlations were reported here. In the context of Figure 7, the  $P$  values were associated with the Pearson's correlation between block connectivity strength and age-regressed executive score. We note that no significant correlations were observed between the age-regressed executive function scores and covariates of no interest, including in-scanner motion and sex.

## Results

In this study, we seek to unify the detection and quantitative characterization of modular and core-periphery structure under a single framework and to understand how such mesoscale organization is associated with neurodevelopment and cognitive ability. To achieve this goal, we study functional brain networks estimated from resting-state fMRI data acquired in 872 youth between the ages of 8 and 22 years. An increasingly common approach to studying these sorts of data is to consider modules that are defined a priori from other data using community detection techniques (Fig. 1C) or to apply a community detection technique directly to the data to extract modules. Currently, both approaches depend on techniques that frequently remain agnostic to any structure of connectivity observed outside those modules, for example, in the off-diagonal blocks of the connectivity matrix (Fig. 1D). To provide a broader perspective on potential interactions between modules, we use the WSBM to coarse-grain the data, identifying mesoscale structure that is characteristic of each individual and that is characteristic of

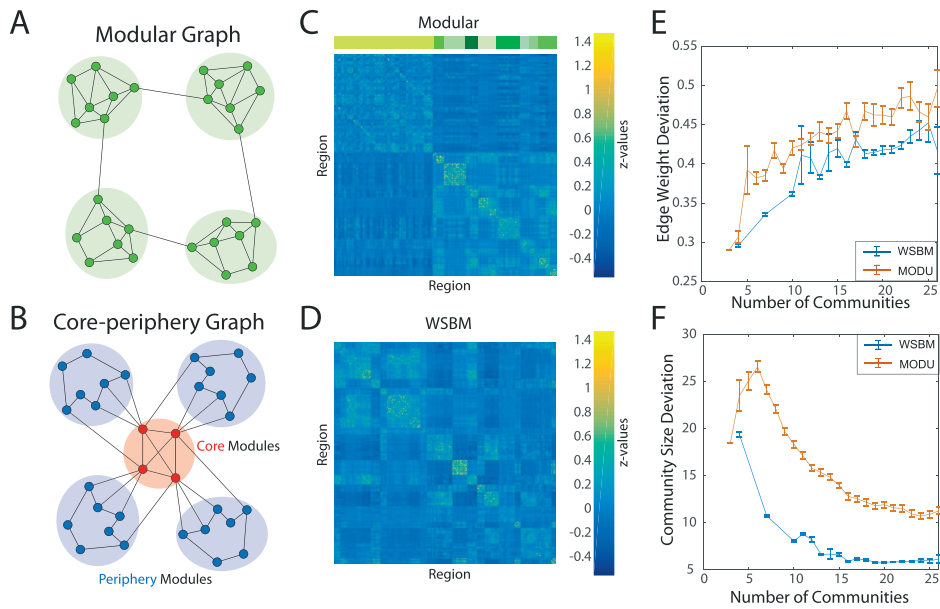
the group, at both finer and coarser topological scales. After characterizing this mesoscale structure, we map the association between structure and age and reveal associations with individual differences in cognitive function. We demonstrate that a unified assessment of modular and core-periphery structures, made possible through use of the WSBM, provides novel insights into functional network organization, its development in youth, and its implications for behavior.

### Comparison Between WSBM and Modularity Maximization

Fundamentally, the WSBM follows the rule to group nodes by similar patterns of connectivity different from that employed by other common approaches for community detection such as modularity maximization and Infomap. Moreover, the focus on pattern similarity allows the WSBM to simultaneously detect modules, cores, and other mesoscale structures. Specifically, if a few nodes are all densely connected to one another and sparsely connected to the rest of the brain, they will be identified as a block using the WSBM and also tend to be identified as a module using community detection techniques such as modularity maximization (Fig. 2A). If a few nodes are strongly connected to one another and more weakly connected to (but not disconnected from) the rest of the brain, they will be identified as a block using the WSBM and also tend to be identified as a core using core-periphery detection techniques (Fig. 2B). A third type of mesoscale structure that is not explicitly detected by either modularity maximization or core-periphery techniques, but is explicitly detected by the WSBM, is bipartite structure, where one set of very sparsely intracommunity nodes is strongly and preferentially connected to another set of sparsely intracommunity nodes.

The fact that the WSBM groups nodes with similar connection patterns provides it with the flexibility to identify such diverse mesoscale structures simultaneously. To gain an intuition for the WSBM's sensitivity, we considered a group-averaged functional brain network constructed by taking the mean over all subject-specific connectivity matrices. To this group network, we applied both the WSBM and modularity maximization methods. We separately tuned the free parameter of both models to ensure that the subsequent solutions separated brain regions into 21 groups (a number that we will justify further below), referred to as "blocks" in the case of the WSBM and as "modules" in the case of modularity maximization. We observed that the modularity maximization approach produced a nonuniform distribution of module sizes, tending to group nearly half of the nodes into a single module (Fig. 2C). In contrast, the WSBM produced a more uniform distribution of block sizes, tending to group nodes into similarly sized blocks (Fig. 2D).

To determine the generalizability of this observation across subjects and across parameter choices, we considered the functional connectivity matrices derived for each subject separately. We then applied both modularity maximization and the WSBM to each matrix and varied the free parameter in both algorithms to sweep across scales of the network's community architecture. We assessed performance with 2 metrics. First, we calculated the variance in the edge weights located within blocks or modules (Eq. 13); this metric served to probe the fit of the model to the data, with low edge weight variability indicating greater internal homogeneity of blocks or modules. Second, we calculated the variance in the sizes of blocks or modules; this metric served to probe the capacity of the method to assess the presence of



**Figure 2.** Comparison between the WSBM and modularity maximization. (A) Modularity maximization is designed for community detection in a modular graph where the within-community connectivity is much stronger than the between-community connectivity. (B) Accurate and reliable detection of core-periphery structure requires a distinct methodological approach. Notably, characterizations of networks that display both modular and core-periphery structures require yet another distinct method, an example being the WSBM. (C) Group-averaged functional connectivity matrix with nodes ordered according to an example partition obtained from the modularity maximization approach, with the resolution parameter  $\gamma$  tuned to obtain 21 modules. (D) Group-averaged functional connectivity matrix with nodes ordered according to an example partition obtained from the WSBM, with  $k$  tuned to obtain 21 blocks. (E) Compared with the modularity maximization approach, the WSBM recognized communities with a lower SD in the edge weights located within blocks or modules (Eq. 13). (F) Compared with the modularity maximization approach, the WSBM also recognized communities with a lower SD in community size. In panels E and F, the thick line indicates the mean calculated over the 872 subjects, and the error bars indicate the standard error of the mean.

community structure evenly across the network, with low community size variability indicating the capacity to detect blocks or modules of similar sizes. We observed that the WSBM achieved a lower SD in both metrics (Fig. 2E,F). The more evenly distributed nature of the WSBM blocks suggests that the method detects the presence of structure in functional brain networks that exists more homogeneously than has perhaps been previously appreciated.

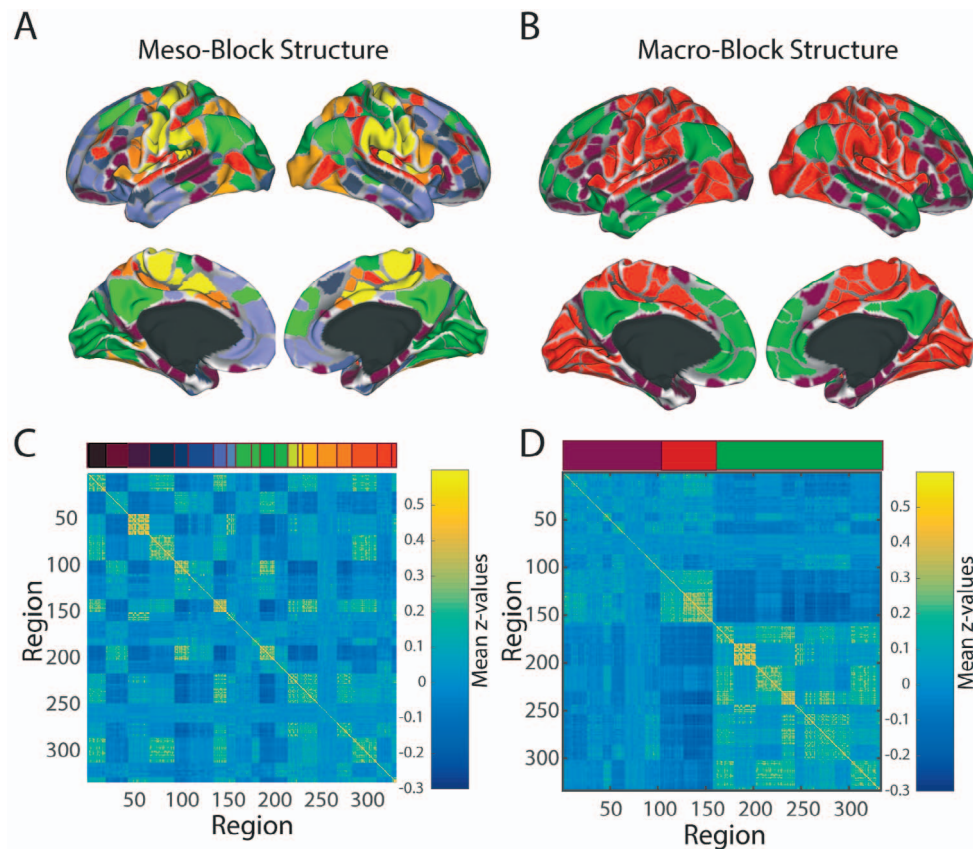
### Hierarchical Mesoscale Structure of Resting-State fMRI in Youth

After noting broad dissimilarities between the partitions obtained from modularity maximization and the WSBM, we next sought to better understand the full mesoscale organization of subject-level resting-state connectivity matrices in the youth of the PNC. Moreover, we wished to extract features of that mesoscale organization that were specific to individuals as well as features that were conserved across the group. We therefore developed a multistep clustering procedure, where we obtained an estimate for the block structure characteristic of single individuals, an estimate for the block structure characteristic of fine-scale organization in the group (Fig. 3A,C), and an estimate for the block structure characteristic of coarse-scale organization in the group (Fig. 3B,D).

In first considering the block structure characteristic of single individuals, we note that the WSBM has one important free parameter:  $k$ , or the number of blocks. To determine the impact of this parameter on the block solution and to offer statistical support for a specific choice of  $k$ , we varied  $k$  in

4, 7, 10, 13, 16, 19, 22, 25, 28 and estimated the model's goodness of fit with the log-evidence for each subject (see Eq. 2 in Methods and Supplementary Figure 1). We observed that the goodness of fit first increased as  $k$  increased from 4 to 16 and then appeared to plateau for  $15 < k < 28$ . As a second measure of reliability and robustness, we calculated the average block allegiance matrix (see Eq. 4 in Methods) over all subjects for each  $k$  in the above range. We found that matrices were highly similar to one another for  $k > 10$ , as measured by a Pearson correlation coefficient between the vectors representing the upper triangles of the matrices (see Supplementary Figure 1). Given these tests, we chose to set  $k = 16$  for each subject, which is in fact a value that is similar to that chosen for the number of functional modules or cognitive systems in previous literature (Power et al. 2007; Ye0 et al. 2011).

We next turned to the question of understanding consistent block structure characteristic of all youth in the sample. We applied the WSBM to the average block allegiance matrix and again varied the number of blocks from 3 to 30 (see Supplementary Figure 1). We observed maximal log-evidence for 21 blocks (see Eq. 2 in Methods and Fig. 3A). That a larger number of blocks are required to accurately fit the group-level data in comparison with the individual-level data is expected: With the added statistical power of 872 subjects, we are able to accurately observe structure at a finer scale within the matrix. Next, we calculated the block-level average adjacency matrix as the average strength of connectivity within each of the  $21 \times 21$  blocks across subjects (see Eq. 5 in Methods). By visual inspection of this matrix, we note the existence of a nonzero edge weights in off-diagonal blocks, and we also note that this nontrivial interblock



**Figure 3.** Hierarchical representation of mesoscale structure in resting-state fMRI in youth. We apply the WSBM to each functional network extracted from a single individual. (A) Next, we calculated the average block allegiance matrix (see Eq. 4 in Methods) over all subjects and applied the WSBM to this matrix to obtain the fine-scale block structure characteristic of the group. This fine-scale block structure segregates the functional network into 21 blocks. (B) Next, we calculated the block-level average adjacency matrix as the average strength of connectivity within each block across subjects (see Eq. 5 in Methods). Upon this average matrix, we again applied the WSBM to obtain the coarse-scale block structure characteristic of the group. This coarse-scale block structure segregates the functional network into 3 components: a set of regions reminiscent of the frontotemporal system, a set of regions reminiscent of the default mode system, and a set of regions reminiscent of the sensory system. Panels C and D show the reordered matrices corresponding to panels A and B, where the regions below the same color strip are located within the same block.

connectivity displays a heterogeneous pattern indicative of a complex mesoscale architecture, which is not well described by the simpler notion of modularity (Fig. 3C).

We note that group-level blocks differ appreciably in size (Fig. 3C) and in their spatial extent across the brain (Fig. 3A). It is therefore compelling to ask whether there exists a meaningful coarse-grained summary of these 21 blocks that accurately describes the spatial organization of the brain in broader strokes. In order to evaluate whether such a hierarchical structure exists, we applied the WSBM to the block-level average adjacency matrix (of size  $21 \times 21$ ; see Eq. 5 in Methods) and observed maximal log-evidence for 3 blocks (see Supplementary Figure 1). This coarse-grained solution segregates the functional brain network into 3 groups composed of regions that are reminiscent of systems defined in prior reports, including a frontotemporal system, a default mode system, and a sensory-motor system (Gordon et al. 2016).

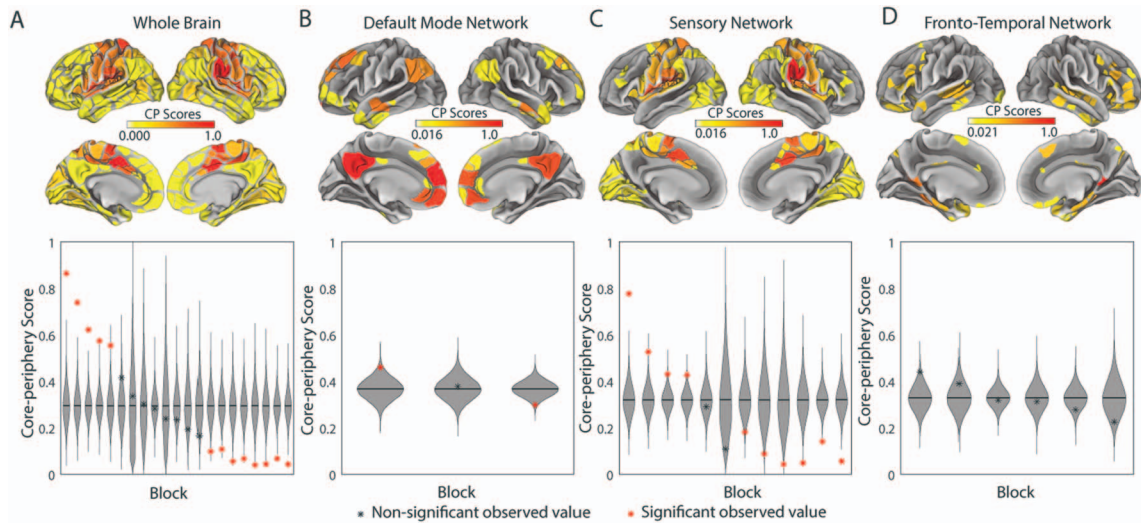
### Cores, Peripheries, and Other Building Blocks of Mesoscale Structure

Next, we used the WSBM to investigate how modular structure and core-periphery structure might coexist in brain networks.

Specifically, we examined each block and asked whether some blocks were more core-like while others were more periphery-like. To assess the degree to which a given block played the role of a network core, we calculated the core score of each node in the network that assesses the node's relevant associations to dense versus sparse blocks (see Methods), and then we averaged these values over nodes in a block to obtain a core score for the block (Rombach et al. 2014). Our null hypothesis was that core scores would be uniformly distributed across regions and therefore also uniformly distributed across blocks. We first observed that core scores were heterogeneously distributed across regions of the cortex, with the highest values present in the motor strip (Fig. 4A, top). Across blocks, the average core score was also heterogeneously distributed, with 6 blocks displaying greater core scores than expected (FDR correction with  $q < 0.1$ ,  $P < 0.05$  for a nonparametric permutation test in which region labels were permuted uniformly at random) and 9 blocks displaying weaker core scores than expected (Fig. 4A, bottom).

We next evaluated the coarse-grained group-level structure constituting the 3 large blocks shown in Figure 3B. For each block, we computed the core scores of each region assigned to that block, and we examined the distribution of core scores within a block. In the block reminiscent of the default mode





**Figure 4.** Anatomical distribution and statistical testing of core scores. We compute core scores for each region both in the network representing the whole brain and in the subnetworks representing the 3 macroscale blocks identified in the group-level WSBM analysis. (A, top) In the whole brain, the motor strip generally and the temporo-parietal junction specifically exhibited higher core scores than expected in the nonparametric null model. (A, bottom) Across blocks, the average core score is heterogeneously distributed, with 6 blocks showing greater core scores than expected and 9 blocks showing lower core scores than expected. (B, top) In the subgraph constituting the coarse-scale block that is reminiscent of the default mode network, we observed the strongest core scores in known default mode hubs including the posterior cingulate and ventromedial prefrontal cortex and the weakest core scores along the lateral surfaces. (B, bottom) Across meso-blocks within the default mode macro-block, the average core score is also heterogeneously distributed, with 1 block showing a greater core score than expected and 1 block showing a lower core score than expected. (C, top) In the subgraph constituting the coarse-scale block composed predominantly of sensory regions, we observed that the temporo-parietal junction displayed the greatest core score. (C, bottom) Across meso-blocks within the sensory macro-block, the average core score is also heterogeneously distributed, with 4 blocks showing greater core scores than expected and 5 blocks showing lower core scores than expected. (D, top) In the subgraph constituting the macro-block composed predominantly of frontal and temporal regions, we observed no clear anatomical localization of high core scores. (D, bottom) Across meso-blocks within the frontotemporal macro-block, the average core score was not significantly different than that expected in the nonparametric null model. In the bottom panels of each figure, violin plots are ordered according to the mean core score of each block. Red asterisks indicate  $P < 0.05$ , FDR corrected at  $q < 0.1$ .

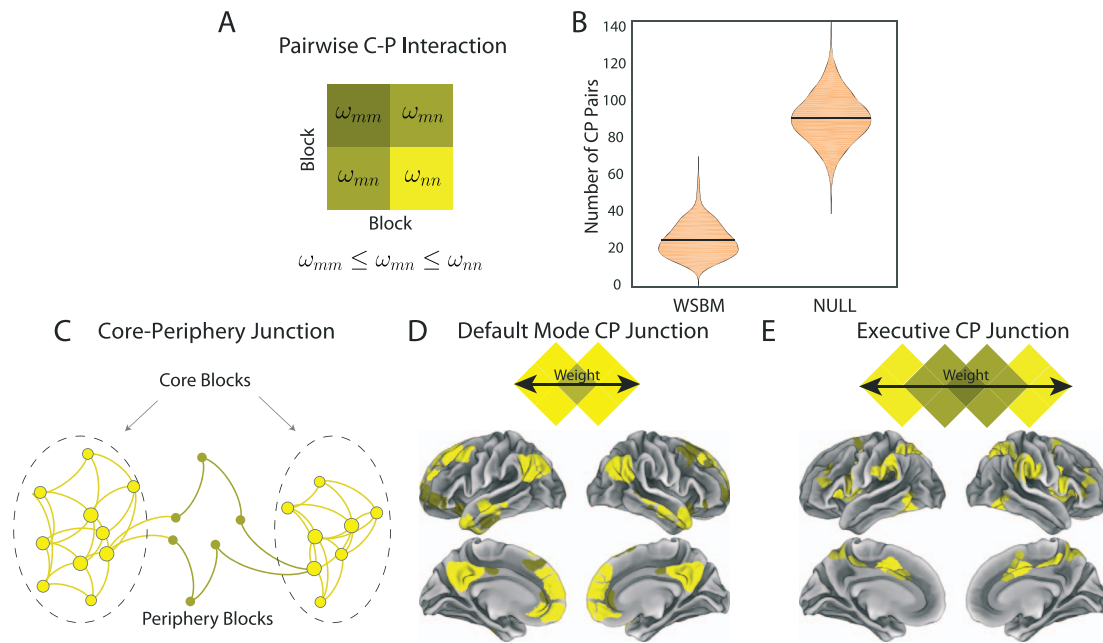
network, we observed that the posterior cingulate and medial orbitofrontal areas displayed higher core scores than expected and that the supramarginal, middle frontal, and inferior frontal areas displayed lower core scores than expected (FDR  $q < 0.1$ ,  $P < 0.05$ ; Fig. 4B, top). Across blocks, the average core score was also heterogeneously distributed, with 1 block displaying a greater core score than expected (FDR  $q < 0.1$ ,  $P < 0.05$ ) and 1 block displaying a weaker core score than expected (Fig. 4B, bottom). In the block consisting predominantly of sensory regions, we observed a pattern of core scores that is consistent with that observed in the whole brain, with the highest values in the right temporo-parietal junction (FDR  $q < 0.1$ ,  $P < 0.05$ ; Fig. 4C, top). Across blocks, the average core score was also heterogeneously distributed, with 4 blocks displaying greater core scores than expected (FDR  $q < 0.1$ ,  $P < 0.05$ ) and 5 blocks displaying weaker core scores than expected (Fig. 4C, bottom). In the block consisting predominantly of frontotemporal regions, a few spatially distributed areas displayed higher core scores than expected, but no blocks were significantly different from the null model (FDR  $q < 0.1$ ,  $P < 0.05$ ; Fig. 4D, top). Collectively, these results indicate that the WSBM identifies blocks that play variable roles within a global core–periphery structure and therefore motivates a more thorough examination of the nature of those roles.

### Interactions Between Blocks in the Mesoscale Structure

We sought to better understand how blocks interact with one another and whether we could distinguish important principles guiding interblock connectivity. We began by considering a pair of blocks, which is the smallest unit in which interblock connectivity can be studied. From the relative strength between the 2

blocks in a pair, we could determine whether the 2 blocks were relatively independent or tended to interact in either a core–periphery or bipartite manner. In applying this heuristic (Fig. 5A; see Methods for details) to the data, we found a preponderance of independent pairs, some core–periphery pairs, and only a few bipartite pairs. To assess statistical significance, we considered a nonparametric permutation-based null model in which nodes are randomly assigned to blocks. We observed that the true data displayed a greater number of independent pairs and a smaller number of core–periphery pairs than expected in the null model (Fig. 5B), indicating that core–periphery architecture, while present, complements a broad segregation consistent with the modularity commonly studied in resting fMRI.

In the exposition that follows, we did not consider the independent pairs, as it is impossible (by definition) to infer principles of interblock connectivity from total independence. We also neglected bipartite pairs due to their infrequent existence, hampering statistical power in hypothesis testing (0.8 per subject on average). Focusing on core–periphery pairs, we first wished to determine whether their anatomical location was consistent across subjects. To address this question, we defined a characteristic measure  $\eta_{mn}^s$  (see Eq. 9), which we will refer to as the core–periphery role, to represent the core–periphery relation between blocks  $m$  and  $n$  of subject  $s$ . The value of this measure is +1 if block  $m$  acts as the core in the pair, –1 if block  $n$  acts as the periphery in the pair, and 0 if the pair does not display a core–periphery relationship. The average core–periphery role is defined as the mean of  $\eta_{mn}^s$  over subjects, and intuitively, it represents the empirical probability of a pair appearing as a core–periphery pair (see Eq. 10). Here, we confine ourselves to considering the pairs that are core–periphery pairs in at least



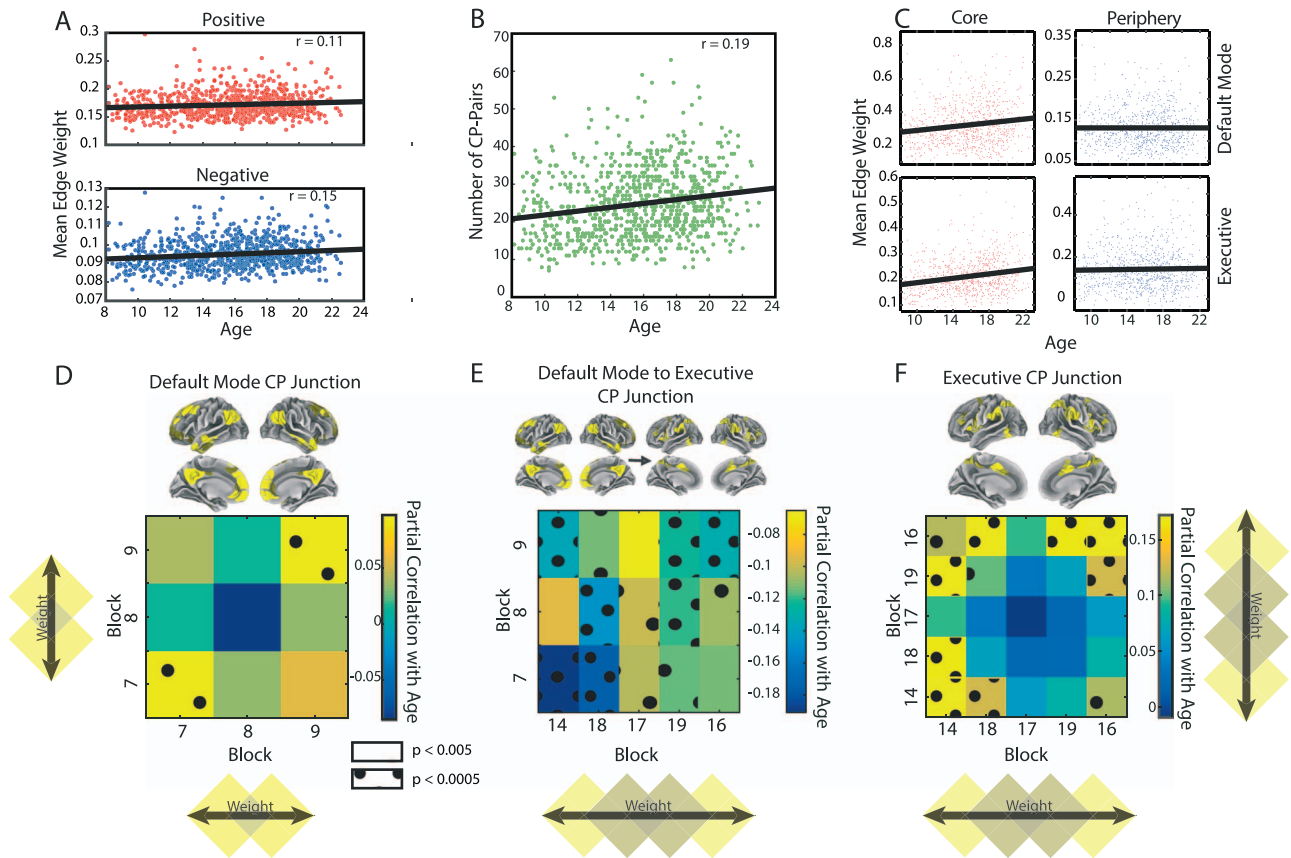
**Figure 5.** Existence of core–periphery junctions. (A) For each pair of blocks, we classified an interaction as a core–periphery interaction if the average interblock strength was intermediate between the average intrablock strength. (B) We compared the number of core–periphery pairs that we detected in the true data with the number of core–periphery pairs that we detected in a nonparametric permutation-based null model in which nodes are randomly assigned to blocks. We observed that the true data displayed a greater number of independent pairs and a smaller number of core–periphery pairs than expected in the null model (2-sample t-test  $t = -127$ ,  $P < 0.0001$ ). (C–E) We detected 2 core–periphery junctions where (C) different core blocks were connected through common periphery blocks. (D) The default mode core–periphery junction consisted of 3 meso-blocks: 2 core blocks sharing the same periphery block. (E) The executive core–periphery junction consisted of 5 meso-blocks: 2 hierarchical core–periphery chains sharing the same periphery block. Abbreviations: C, core; P, periphery.

half of the participant sample: That is, the block pair  $mn$  displays an  $\eta_{mn}^s$  of +1 (or of  $-1$ ) in at least 50% of the subjects. We find that core–periphery pairs do not appear at random locations in each subject but instead display a consistent anatomical distribution across subjects ( $z > 40$  for Eq. 11; see Methods for a description of the null model).

In addition to observing that the anatomical distribution of core–periphery block pairs was relatively conserved across subjects, we also observed that some core–periphery pairs interacted with one another in what we term “core–periphery junctions.” We observed the existence of 2 core–periphery junctions: one composed of regions in the default mode system and one composed of regions in the executive system. The default mode core–periphery junction consisted of 3 blocks: The periphery block—composed of regions in the rostral anterior cingulate and frontal pole—linked 2 core blocks, one of which was located in the superior and medial frontal area and the other was located in the precuneus and inferior parietal area (Fig. 5D). The executive core–periphery junction consisted of 5 blocks: Core blocks were connected through a periphery block in a 2-tier hierarchical core–periphery structure (Fig. 5E). More specifically, the periphery block in the superior frontal area connected 2 core blocks: One core block was located in the supramarginal and posterior cingulate area, and the other core block was distributed across superior parietal, pars opercularis, and fusiform areas. Two blocks in the superior frontal, precuneus, and rostral middle frontal areas acted as the provincial cores. The presence of these 2 core–periphery junctions suggests an important principle by which hubs that are located in the 2 extreme cores might communicate with one another via shared peripheries.

### Age-Related Differences in Block Structure during Neurodevelopment

Next, we asked whether features of core–periphery structure are associated with age. We recognize that changes in topology can occur upon changes in overall network strength and that it is important to distinguish between the two. Thus, we first examined the association between overall network strength and age (Fig. 6A). We observed that the average magnitude of the positive edge weights increased significantly with age ( $r = 0.11$ ,  $P = 0.0017$ ) and that the average magnitude of the negative edge weights decreased significantly with age ( $r = -0.15$ ,  $P = 1.63 \times 10^{-5}$ ), after partialing out the effects of sex and motion. These observations are consistent with previous reports of growing system segregation with development (Fair et al. 2007; Gu et al. 2015). To determine whether this segregation resulted from the emergence of more core–periphery interactions, we calculated the Pearson correlation coefficient between the number of core–periphery pairs and age, after partialing out the effects of sex and motion. We observed a significant positive relationship ( $r = 0.19$ ,  $P = 2.25 \times 10^{-8}$ ; Fig. 6B), which remains significant after partialing out the average magnitude of the positive and negative edge weights ( $r = 0.16$ ,  $P = 1.28 \times 10^{-6}$ ). Next, focusing solely on the 2 core–periphery junctions described in the previous section, we found that the interaction strength among core blocks increased significantly with age ( $r = 0.15$ ,  $P = 4.93 \times 10^{-6}$ ;  $r = 0.21$ ,  $P = 1.89 \times 10^{-10}$ ), while the interaction strength among periphery blocks was unchanged with age ( $P > 0.05$ ; Fig. 6C), again after partialing out the effects of sex and motion. These results suggest that neurodevelopment can be described as an enhancement of



**Figure 6.** Development of core–periphery junctions in youth. (A) The average strength of functional connectivity increases with age. The average magnitude of positive edge weights increases significantly with age ( $r = 0.11$ ,  $P = 0.0017$ ), and the average magnitude of negative edge weights increases significantly with age ( $r = 0.15$ ,  $P = 1.63 \times 10^{-5}$ ). These observations are consistent with previous reports of growing system segregation with development. (B) To better understand changes in network topology beyond that explained by changes in the strength of connectivity, we calculated the correlation between age and the number of core–periphery block pairs. We observed a significant relation between these 2 variables, both based on their raw values ( $r = 0.19$ ,  $P = 2.25 \times 10^{-8}$ ) and after partialing out the average magnitude of positive edge weights and the average magnitude of negative edge weights ( $r = 0.16$ ,  $P = 1.28 \times 10^{-6}$ ). These results indicate an increase in heterogeneous mesoscale network architecture with age. (C) Focusing on the 2 core–periphery junctions in Figure 5D,E, we next calculated the correlation between age and the average edge strength within the core and periphery blocks. We found that the cores increase in strength over development ( $r = 0.15$ ,  $P = 4.93 \times 10^{-6}$ ;  $r = 0.21$ ,  $P = 1.89 \times 10^{-10}$ ), while the peripheries remain unchanged ( $P > 0.05$ ). To further investigate the source of change in connectivity strength, we considered the (D) default mode, (E) default mode to executive, and (F) executive core–periphery junctions. Default mode and executive core–periphery junctions display similar changes in block strength with developmental trajectories, where the interaction strength among core areas increases with age (D,F). In contrast, the interaction strength between the 2 junctions decreases with age (E). Abbreviation: CP, core–periphery.

core–periphery structure, driven in part by a strengthening of network cores in higher-order cognitive systems.

To better understand age-related effects on the 2 core–periphery junctions that we identified in higher-order association areas, we considered the elemental blocks that composed each junction. In the default mode core–periphery junction composed of 2 core blocks sharing a periphery, we observed that the edge weights within cores increased significantly with age ( $P < 0.005$ ; Fig. 6D). Considering the connectivity between the default mode and executive core–periphery junctions, we observed that interjunction edges tended to decrease in weight with age (Fig. 6E), indicating a growing segregation between the 2 junctions. Here, we report the significant effects at different levels of stringency in statistical testing to present an even-handed account. Specifically, of the 15 interjunction relations, 13 displayed decreasing edge weight with age at a level of  $P < 0.005$  and 7 displayed decreasing edge weight with age at a level of  $P < 0.0005$ . In the executive core–periphery junction, we observed that the edge weights within

cores tended to increase significantly with age ( $P < 0.0005$ ; Fig. 6F). Notably, all of these trends held when we computed the correlation after partialing out the effects of sex and motion. See the Supplementary Information (SI) for details on the partial correlation values and associated estimates of statistical significance. Collectively, these results support the more general conclusion that development is associated with a strengthening of network cores in higher-order cognitive systems and an increasing segregation between such systems.

### Cognitive Correlates of Mesoscale Block Structure

As mentioned previously, the WSBM groups similarly-connected regions together into a block, and each of these blocks can play a different role in the brain's mesoscale network organization, including the role of a core and the role of a periphery. In the previous section, we showed that the interaction strength among core blocks changed appreciably over development. Here, we asked whether individual differences in cognitive perfor-



mance were related to the partition of nodes into blocks identified by the WSBM. If such a relationship existed, it would be important to determine whether the relationship was specific to the WSBM or whether it could also have been found with previously developed approaches. To address this question of specificity, we tested whether individual differences in cognitive performance were also related to the partitions of nodes into modules identified from the modularity maximization algorithm (Newman 2006). Specifically, we tested for significant correlations between interblock (or intermodule) strength and age-regressed executive function score (see Methods). We note that the age-regressed executive function scores used here were not significantly associated with sex ( $r = -0.017$ ,  $P = 0.598$ ) and were also not significantly associated with mean framewise displacement ( $r = 0.0022$ ,  $P = 0.949$ ).

In the WSBM partition, we observed 19 intrablock and interblock strengths distributed throughout the brain that were significantly correlated with individual differences in executive function (Pearson correlation coefficients, FDR corrected for multiple comparisons at  $q < 0.05$ ). In the modularity maximization partition, we found only 3 modules whose intermodule strength was correlated with individual differences in executive function; these modules were composed of regions in the default mode, dorsal attention, and visual systems (see Supplementary Figure 3 for details). Given the more extensive relation between the WSBM blocks and executive function, we probed the WSBM partition further. Specifically, we observed that executive function scores were positively correlated with overall core strength in both of the core–periphery junctions and were not strongly correlated with periphery strength (Fig. 7A,B). We also noted that the block pairs whose interblock strengths were significantly correlated with individual differences in cognition tended to be located at the centers of the 2 core–periphery junctions that we identified in a previous section. The interaction strength between the cores located within junctions was positively correlated with individual differences in executive function (Fig. 7C). In contrast, the interaction strength between the cores located between junctions was negatively correlated with individual differences in executive function. In assessing the sensitivity of our findings, we note that the age-regressed cognitive scores that we used here were uncorrelated with age (by definition), and they were also uncorrelated with sex and motion, and thus we did not include these 3 covariates in our analysis. Broadly, the pattern of results that we uncover suggests that the extent of segregation between the default mode junction and the executive junction explains significant variance in individual differences in cognitive performance.

## Discussion

Here, we adopted the weighted stochastic model (WSBM) to investigate the nature, development, and cognitive significance of mesoscale architecture in functional brain networks. Unlike other common approaches, the WSBM is built on a generative model of graph architecture, which is sensitive to modular structure, core–periphery structure, and other mesoscale motifs (Betzel et al. 2018, 2019). Because each block is composed of nodes with a similar pattern of connectivity to the rest of the network, the method fundamentally crystallizes interblock interactions, facilitating a rich quantitative assessment of mesoscale graph structure. By applying the method to resting-state functional brain networks estimated from 872 youth ages 8–22 years in the PNC, we observed that blocks vary in

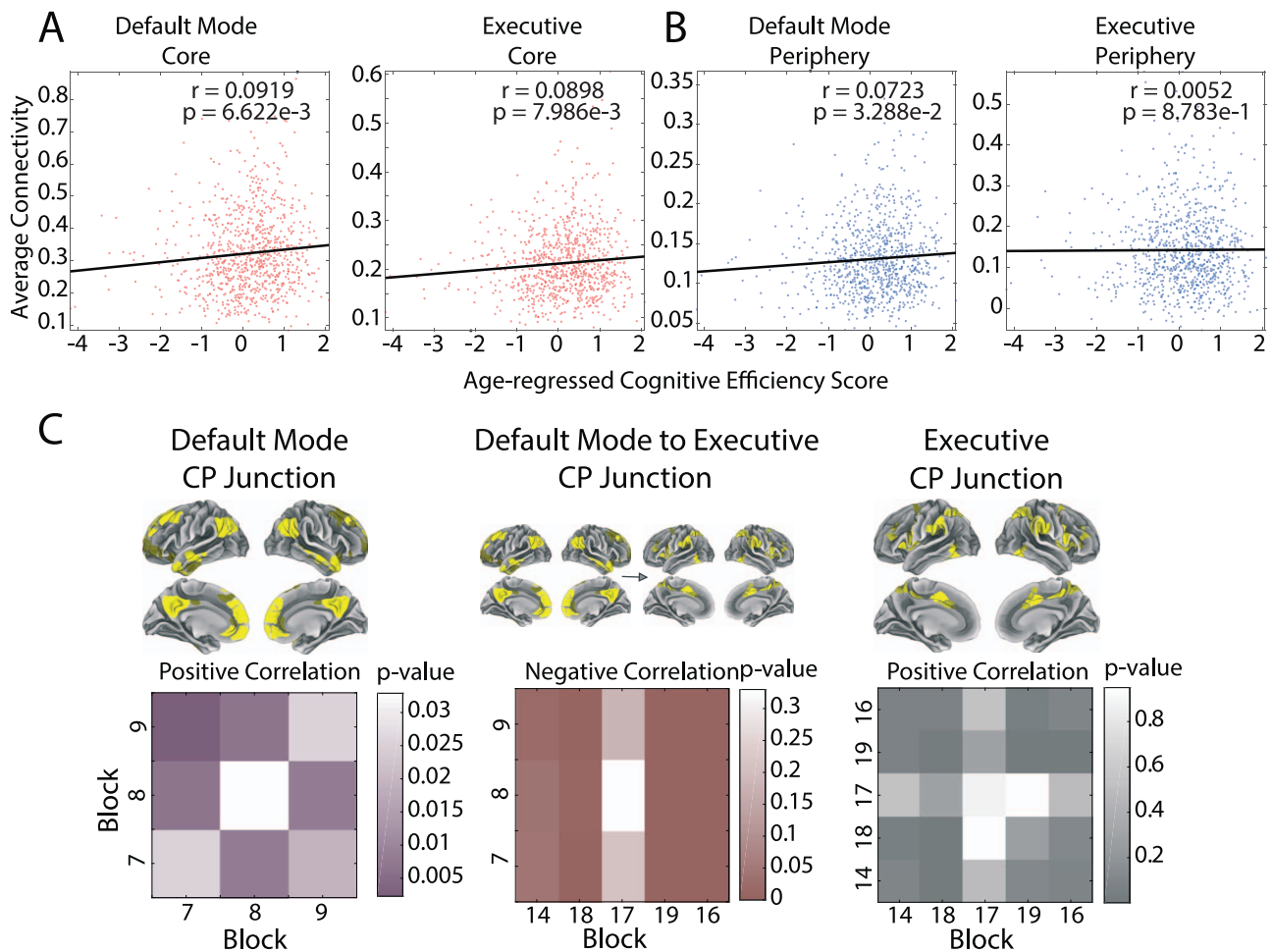
their topological nature, with some blocks being composed predominantly of regions that play a core role within the network, other blocks being composed predominantly of regions that play a peripheral role within the network, and still other blocks being composed of regions of both types. Core and periphery roles were not only played by single regions within blocks, but they were also played by blocks themselves in their interactions with one another. Notably, we uncovered the existence of block junctions in which different cores shared the same periphery and demonstrated that the strength of cores increased with development. Finally, we observed that individual differences in the interaction strength between cores were correlated with individual differences in executive function, particularly among the cores that participated in core–periphery junctions. Collectively, our results offer a rich depiction of mesoscale structure in functional brain networks and highlight the role of core–periphery structure in cognition and development.

## Mesoscale Block Structure in Functional Brain Networks

Traditionally, mesoscale structure in resting-state functional brain networks has been studied from the perspective of modularity (Betzel and Bassett 2016; Sporns and Betzel 2016), where brain regions are more strongly connected to other regions in their module than expected in an appropriately defined null model (Newman 2006). The notion that modules are important for brain function, development, and cognition has a long intellectual history (Fodor 1983), and the recent formalization of that notion with the mathematical tools of network science has led to important insights into the role of modules in development (Gu et al. 2015; Baum et al. 2017) and aging (Meunier et al. 2009). The notion of modularity has also become important in understanding individual differences in cognitive capacity such as probed by general measures of executive function in youth (Baum et al. 2017; Chai et al. 2017) as well as more specific measures of response to training both in healthy adults and in individuals with brain injury (Arneemann et al. 2015; Gallen et al. 2016). However, common tools for community detection that are applied in the neuroimaging field focus on identifying modules with algorithms that seek independent groups of brain regions (Porter et al. 2009; Fortunato 2010; Fortunato and Hric 2016). This assumption of module independence that is implicit or explicit in common algorithms is fundamentally at odds with our intuitions, supported by neuroscience, that some modules may control, compete, or cooperate with other modules and that these interactions might change according to context, differ in youth and the elderly, and vary in health and disease. The assumption that modules are independent also stands at odds with recent empirical evidence underscoring the importance of the patterns of intermodule connectivity for transitions between cognitive states (Cole et al. 2014; Mattar et al. 2015), long-term changes in behavior (Bassett et al. 2015), and alterations in connectivity characteristic of adolescent development (Gu et al. 2015).

An approach that embraces the potential heterogeneous patterns of interconnectivity between modules is the WSBM, which explicitly quantifies mesoscale network architecture, thereby offering insights into how control, competition, and/or cooperation between modules can be instantiated. Rather than treating modules as independent, the WSBM explicitly seeks to capture the mesoscale topology connecting modules with one another





**Figure 7.** Individual differences in interblock strength are correlated with individual differences in executive function. For each subject, we calculated the average strength both within and between blocks or modules. We then estimated the correlation coefficient between that value and age-regressed executive function scores across subjects. Focusing on the block structure, we next computed the correlation between the executive function scores and the connectivity strength within the core and periphery blocks recognized in the 2 junctions. (A) Overall, we find that the core strength is positively correlated with the executive function scores. (B) We do not find a strong correlation between periphery strength and executive function scores. (C) By considering the 2 core–periphery junctions and their interaction in greater detail, we observed that the strength of core–periphery junctions was associated with individual differences in executive function. Specifically, we found that interaction strengths particularly among cores were significantly correlated with executive function scores, where the within-junction correlation was positive and the between-junction correlation was negative. The *P* values were exploratory and not corrected for multiple comparisons. Abbreviation: CP, core–periphery.

and can be used to understand small-world organization of modules, as well as the presence of hub modules, connector modules, and provincial modules. Prior studies applying the WSBM to brain networks have compared block structure and module structure (Pavlovic et al. 2014; Rajapakse et al. 2017) and have sought to better understand the diversity of mesoscale architecture consistent across species and aligned with genetic underpinnings (Betzel et al. 2018, 2019). Here, we complement these prior studies by offering a systematic block-based analysis to better understand how blocks interact with one another in the wider brain network and how those interactions might change with development or track cognitive efficiency.

### Core–Periphery Junctions

Using the WSBM, we found compelling evidence for blocks that were best described as 1) core blocks (being strongly connected to most blocks and weakly connected to a few blocks), 2) periphery blocks (being weakly connected to most blocks but strongly

connected to a few blocks), or 3) blocks that—like modules—were neither core-like nor periphery-like. In addition to these more commonly studied mesoscale features (modules, cores, and peripheries), we uncovered the existence of block junctions in which different cores shared the same periphery. While the exact functional role of these block junctions is unknown, it is possible that they offer a means by which cores can transiently communicate with one another. It would be interesting in the future to test this possibility using recently developed tools for measuring transient synchrony (Palmigiano et al. 2017) in the context of tasks that activate these regions and whose demands vary on a time scale that is longer than the time scale of the imaging measurement (Gerraty et al. 2018). Specifically, we note that peripheries are composed of regions that—over long periods of time—display weak static functional connectivity. However, these regions can display transient control processes or coupling dynamics over shorter time scales. Our results are consistent with the possibility that peripheries could engage in these transient dynamics as a means of facilitating

communication between cores and the network hubs that they often contain. Notably, the 2 core–periphery junctions that we uncovered—containing regions of the default mode and executive systems—were reminiscent of the task-positive and task-negative systems commonly observed in resting-state fMRI and associated with executive function (Kelly et al. 2008; Hampson et al. 2010). Notably, the periphery blocks in the center of both junctions contained portions of the medial frontal gyrus, suggesting an important mediating role for this region in mesoscale network function of resting-state brain dynamics, consistent with the region’s known role in top-down control of cognitive processes (Salmi et al. 2009).

### Role of Core–Periphery Structure in Development and Cognition

Two blocks that form a core–periphery structure are collectively referred to as a core–periphery pair. We demonstrate that core–periphery pairs increase significantly in number over the developmental period of 8–22 years of age. Notably, we find that this increase cannot be explained by changes in the overall strength of connectivity across the brain. Rather, it is specifically driven by an increase in the strength of core blocks, a phenomenon that also serves to increase the heterogeneity of block topology and the potential for localization of functional systems. Importantly, this finding is consistent with prior observations of increasing functional segregation of cognitive systems with age (Fair et al. 2009; Gu et al. 2015). Our data put a finer point on the notion of functional segregation, providing insight into a specific topological change—the increase in cores—that supports the more general observation. Based on prior theories regarding the role of core–periphery organization in brain network function (Fedorenko and Thompson-Schill 2014), we speculate that the increasing core–periphery organization in youth facilitates an emerging balance between temporally invariant processes critical for task performance and temporally transient processes critical for adaptation and control (Bassett, Wymbs, et al. 2013). To more explicitly test this hypothesis, we examined the relationship between summary metrics of this organization and individual differences in executive function. Notably, we observed a negative correlation between executive function and the strength of block interactions in the 2 core–periphery junctions, suggesting that the more the 2 junctions were anticorrelated, the greater an individual’s efficiency might be in executing complex tasks. Such enhanced anticorrelation is consistent with greater segregation between the 2 junctions, a finding that is conceptually consistent with prior work providing evidence that age-related improvement of executive function is mediated by increasing segregation of modules (Baum et al. 2017).

### Methodological Considerations

There are several methodological considerations pertinent to this work. First, the broad community cohort that we study here is sampled cross-sectionally, and thus we cannot address any questions related to developmental trajectories. It would be interesting in the future to consider longitudinal samples and samples enriched for deficits in executive functioning. Second, participant motion is a well-known confound that impacts the BOLD signal. In the context of studies of development, this confound is particularly important to address, as in-scanner motion tends to decrease with age. Here, we address this issue with an extensively validated preprocessing pipeline that mitigates

the influence of motion artifact (Ciric et al. 2017, 2018), as well as postprocessing inclusion of motion as a potential confound in all statistical analyses. Third and finally, the WSBM that we use here is applied to the static functional connectivity matrix and is therefore unable to assess any dynamic reconfiguration of network architecture over time. It would be interesting in the future to consider new methods for applying the WSBM to time-evolving graphs (Matias and Miele 2017).

### Conclusion

Our study offers a new perspective that complements 2 competing perspectives in the field: one that describes functional brain networks as composed of segregated modules and one that describes functional brain networks as composed of hubs and a rich club. We unify the 2 perspectives by employing a WSBM, which is a model-based approach with an explicitly network-based prior that can detect groups of brain regions with similar connectivity profiles to the rest of the brain. In addition to providing a unified perspective on functional brain organization, the approach that we take offers a blueprint for other future studies in other populations tackling important questions in development, cognition, and disease.

### Funding

National Institute of Mental Health (grants R21MH106799, R01MH107703, R01MH113550, and RF1MH116920 to D.S.B. and T.D.S.); the John D. and Catherine T. MacArthur Foundation; the Alfred P. Sloan Foundation; the ISI Foundation; the Paul Allen Foundation; the Army Research Laboratory (grant W911NF-10-2-0022 to D.S.B.); the Army Research Office (grants Bassett-W911NF-14-1-0679, Grafton-W911NF-16-1-0474, and DCIST-W911NF-17-2-0181 to D.S.B.); the Office of Naval Research; the National Institute of Mental Health (grants 2-R01-DC-009209-11, R01-MH112847, R01-MH107235, and R21-MH-106799 to D.S.B.); the National Institute of Child Health and Human Development (grant 1R01-HD086888-01 to D.S.B.); National Institute of Neurological Disorders and Stroke (grant R01-NS099348 to D.S.B.); the National Science Foundation (grants BCS-1441502, BCS-1430087, NSF PHY-1554488, and BCS-1631550 to D.S.B.); National Natural Science Foundation of China (grant NSFC-61876032 to S.G.); the Penn-CHOP Lifespan Brain Institute.

### Notes

The content is solely the responsibility of the authors and does not necessarily represent the official views of any of the funding agencies. *Conflict of Interest:* None declared.

### References

- Aicher C, Jacobs AZ, Clauset A. 2014. Learning latent block structure in weighted networks. *J Complex Networks*. 3:221–248.
- Arnamann KL, Chen AJ, Novakovic-Agopian T, Gratton C, Nomura EM, D’Esposito M. 2015. Functional brain network modularity predicts response to cognitive training after brain injury. *Neurology*. 84:1568–1574.
- Bassett DS, Porter MA, Wymbs NF, Grafton ST, Carlson JM, Mucha PJ. 2013a. Robust detection of dynamic community structure in networks. *Chaos An Interdiscip J Nonlinear Sci*. 23: 13142.
- Bassett DS, Sporns O. 2017. Network neuroscience. *Nat Neurosci*. 20:353–364.

- Bassett DS, Wymbs NF, Porter MA, Mucha PJ, Carlson JM, Grafton ST. 2011. Dynamic reconfiguration of human brain networks during learning. *Proc Natl Acad Sci*. 108:7641–7646.
- Bassett DS, Wymbs NF, Rombach MP, Porter MA, Mucha PJ, Grafton ST. 2013b. Task-based core-periphery organization of human brain dynamics. *PLoS Comput Biol*. 9:e1003171.
- Bassett DS, Yang M, Wymbs NF, Grafton ST. 2015. Learning-induced autonomy of sensorimotor systems. *Nat Neurosci*. 18:744–751.
- Bassett DS, Zurn P, Gold JI. 2018. On the nature and use of models in network neuroscience. *Nat Rev Neurosci*. 19:566–578.
- Baum GL, Ciric R, Roalf DR, Betzel RF, Moore TM, Shinohara RT, Kahn AE, Vandekar SN, Rupert PE, Quarmley M et al. 2017. Modular segregation of structural brain networks supports the development of executive function in youth. *Curr Biol*. 27:1561–1572.e8.
- Bertolero MA, Blevins AS, Baum GL, Gur RC, Gur RE, Roalf DR, Satterthwaite TD, Bassett DS. 2019. *The network architecture of the human brain is modularly encoded in the genome*. arXiv preprint arXiv:1905.07606.
- Betzel RF, Bassett DS. 2017. Multi-scale brain networks. *Neuroimage*. 160:73–83.
- Betzel RF, Bertolero MA, Bassett DS. 2018. Non-assortative community structure in resting and task-evoked functional brain networks. *bioRxiv*. 355016.
- Betzel RF, Gu S, Medaglia JD, Pasqualetti F, Bassett DS. 2016. Optimally controlling the human connectome: the role of network topology. *Sci Rep*. 6: 30770.
- Betzel RF, Medaglia JD, Bassett DS. 2018. Diversity of meso-scale architecture in human and non-human connectomes. *Nat Commun*. 9:346.
- Blondel VD, Guillaume J-L, Lambiotte R, Lefebvre E. 2008. Fast unfolding of communities in large networks. *J Stat Mech Theory Exp*. 2008: P10008.
- Borgatti SP, Everett MG. 2000. Models of core/periphery structures. *Soc Networks*. 21: 375–395.
- Bullmore E, Sporns O. 2009. Complex brain networks: graph theoretical analysis of structural and functional systems. *Nat Rev Neurosci*. 10:186–198.
- Bullmore E, Sporns O. 2012. The economy of brain network organization. *Nat Rev Neurosci*. 13:336–349.
- Chai LR, Khambhati AN, Ciric R, Moore TM, Gur RC, Gur RC, Satterthwaite TD, Bassett DS. 2017. Evolution of brain network dynamics in neurodevelopment. *Netw Neurosci*. 1:14–30.
- Chai LR, Mattar MG, Blank IA, Fedorenko E, Bassett DS. 2016. Functional network dynamics of the language system. *Cereb Cortex*. 26:4148–4159.
- Chaudhuri R, Knoblauch K, Gariel M-AA, Kennedy H, Wang X-JJ. 2015. A large-scale circuit mechanism for hierarchical dynamical processing in the primate cortex. *Neuron*. 88:419–431.
- Ciric R, Rosen AFG, Erus G, Cieslak M, Adebimpe A, Cook PA, Bassett DS, Davatzikos C, Wolf DH, Satterthwaite TD. 2018. Mitigating head motion artifact in functional connectivity MRI. *Nat Protoc*. 13:2801–2826.
- Ciric R, Wolf DH, Power JD, Roalf DR, Baum GL, Ruparel K, Shinohara RT, Elliott MA, Eickhoff SB, Davatzikos C et al. 2017. Benchmarking of participant-level confound regression strategies for the control of motion artifact in studies of functional connectivity. *Neuroimage*. 154:174–187.
- Cole MW, Bassett DS, Power JD, Braver TS, Petersen SE. 2014. Intrinsic and task-evoked network architectures of the human brain. *Neuron*. 83:238–251.
- Colizza V, Flammini A, Serrano MA, Vespignani A. 2006. Detecting rich-club ordering in complex networks. *Nat Phys*. 2:110–115.
- Ekman M, Derrfuss J, Tittgemeyer M, Fiebach CJ. 2012. Predicting errors from reconfiguration patterns in human brain networks. *Proc Natl Acad Sci U S A*. 109:16714–16719.
- Fair DA, Cohen AL, Power JD, Dosenbach NUF, Church JA, Miezin FM, Schlaggar BL, Petersen SE. 2009. Functional brain networks develop from a local to distributed organization. *PLoS Comput Biol*. 5:e1000381.
- Fair DA, Dosenbach NUF, Church JA, Cohen AL, Brahmbhatt S, Miezin FM, Barch DM, Raichle ME, Petersen SE, Schlaggar BL. 2007. Development of distinct control networks through segregation and integration. *Proc Natl Acad Sci U S A*. 104:13507–13512.
- Fedorenko E, Thompson-Schill SL. 2014. Reworking the language network. *Trends Cogn Sci*. 18:120–126.
- Fodor JA and Fodor J. 1983. *The modularity of mind: an essay on faculty psychology*. Cambridge (MA): MIT Press.
- Fornito A, Zalesky A, Breakspear M. 2013. Graph analysis of the human connectome: promise, progress, and pitfalls. *Neuroimage*. 80:426–444.
- Fortunato S. 2010. Community detection in graphs. *Phys Rep*. 486:75–174.
- Fortunato S, Hric D. 2016. Community detection in networks: a user guide. *Phys Rep*. 659:1–44.
- Gallen CL, Baniqued PL, Chapman SB, Aslan S, Keebler M, Didehban N, D’Esposito M. 2016. Modular brain network organization predicts response to cognitive training in older adults. *PLoS One*. 11:e0169015.
- Gerraty RT, Davidow JY, Foerde K, Galvan A, Bassett DS, Shohamy D. 2018. Dynamic flexibility in striatal-cortical circuits supports reinforcement learning. *J Neurosci*. 38:2442–2453.
- Gordon EM, Laumann TO, Adeyemo B, Huckins JF, Kelley WM, Petersen SE. 2016. Generation and evaluation of a cortical area parcellation from resting-state correlations. *Cereb Cortex*. 26:288–303.
- Gu S, Satterthwaite TD, Medaglia JD, Yang M, Gur RE, Gur RC, Bassett DS. 2015. Emergence of system roles in normative neurodevelopment. *Proc Natl Acad Sci U S A*. 112: 13681–13686.
- Gu S, Yang M, Medaglia JD, Gur RC, Gur RE, Satterthwaite TD, Bassett DS. 2017. Functional hypergraph uncovers novel covariant structures over neurodevelopment. *Hum Brain Mapp*. 38:3823–3835.
- Gur RC, Richard J, Calkins ME, Chiavacci R, Hansen JA, Bilker WB, Loughhead J, Connolly JJ, Qiu H, Mentch FD et al. 2012. Age group and sex differences in performance on a computerized neurocognitive battery in children age 8–21. *Neuropsychology*. 26:251–265.
- Gur RC, Richard J, Hughett P, Calkins ME, Macy L, Bilker WB, Brensinger C, Gur RE. 2010. A cognitive neuroscience-based computerized battery for efficient measurement of individual differences: standardization and initial construct validation. *J Neurosci Methods*. 187:254–262.
- Hagmann P, Cammoun L, Gigandet X, Meuli R, Honey CJ, Wedeen VJ, Sporns O. 2008. Mapping the structural core of human cerebral cortex. *PLoS Biol*. 6:e159.
- Hagmann P, Kurant M, Gigandet X, Thiran P, Wedeen VJ, Meuli R, Thiran J-P. 2007. Mapping human whole-brain structural networks with diffusion MRI. *PLoS One*. 2:e597.
- Hampson M, Driesen N, Roth JK, Gore JC, Constable RT. 2010. Functional connectivity between task-positive and

- task-negative brain areas and its relation to working memory performance. *Magn Reson Imaging*. 28:1051–1057.
- Hutchison RM, Womelsdorf T, Allen EA, Bandettini PA, Calhoun VD, Corbetta M, Della Penna S, Duyn JH, Glover GH, Gonzalez-Castillo J et al. 2013. Dynamic functional connectivity: promise, issues, and interpretations. *Neuroimage*. 80:360–378.
- Jutla IS, Jeub LGS, Mucha PJ. 2011. A generalized Louvain method for community detection implemented in MATLAB. <http://netwiki.amath.unc.edu/GenLouvain>
- Kelly AM, Uddin LQ, Biswal BB, Castellanos FX, Milham MP. 2008. Competition between functional brain networks mediates behavioral variability. *Neuroimage*. 39:527–537.
- Matias C, Miele V. 2017. Statistical clustering of temporal networks through a dynamic stochastic block model. *J R Stat Soc Ser B Statistical Methodol*. 79:1119–1141.
- Mattar MG, Cole MW, Thompson-Schill SL, Bassett DS. 2015. A functional cartography of cognitive systems. *PLoS Comput Biol*. 11:e1004533.
- Meunier D, Achard S, Morcom A, Bullmore E. 2009. Age-related changes in modular organization of human brain functional networks. *Neuroimage*. 44:715–723.
- Moore TM, Gur RC, Thomas ML, Brown GG, Nock MK, Savitt AP, Keilp JG, Heeringa S, Ursano RJ, Stein MB, et al. 2019. Development, administration, and structural validity of a brief, computerized neurocognitive battery: results from the army study to assess risk and resilience in service members. *Assessment*. 26:125–143.
- Moore TM, Reise SP, Gur RE, Hakonarson H, Gur RC. 2015. Psychometric properties of the Penn Computerized Neurocognitive Battery. *Neuropsychology*. 29:235–246.
- Moore TM, Reise SP, Roalf DR, Satterthwaite TD, Davatzikos C, Bilker WB, Port AM, Jackson CT, Ruparel K, Savitt AP et al. 2016. Development of an itemwise efficiency scoring method: concurrent, convergent, discriminant, and neuroimaging-based predictive validity assessed in a large community sample. *Psychol Assess*. 28:1529–1542.
- Newman ME. 2006. Modularity and community structure in networks. *Proc Natl Acad Sci U S A*. 103:8577–8582.
- Palmigiano A, Geisel T, Wolf F, Battaglia D. 2017. Flexible information routing by transient synchrony. *Nat Neurosci*. 20:1014–1022.
- Pavlovic DM, Vértes PE, Bullmore ET, Schafer WR, Nichols TE, Vértes PE, Bullmore ET, Schafer WR, Nichols TE, Vértes PE et al. 2014. Stochastic blockmodeling of the modules and core of the *Caenorhabditis elegans* connectome. *PLoS One*. 9:e97584.
- Porter MA, Onnela J-P, Mucha PJ. 2009. Communities in networks. *Not Am Math Soc*. 56(1082–1097):1164–1166.
- Power JD, Cohen AL, Nelson SM, Wig GS, Barnes KA, Church JA, Vogel AC, Laumann TO, Miezin FM, Schlaggar BL et al. 2007. Functional network organization of the human brain. *Neuron*. 104:665–678.
- Power JD, Schlaggar BL, Lessov-Schlaggar CN, Petersen SE. 2013. Evidence for hubs in human functional brain networks. *Neuron*. 79:798–813.
- Rajapakse JC, Gupta S, Sui X. 2017. Fitting networks models for functional brain connectivity. In *2017 IEEE 14th International Symposium on Biomedical Imaging (ISBI 2017)*, pp. 515–519. IEEE.
- Rombach MP, Porter MA, Fowler JH, Mucha PJ. 2014. Core-periphery structure in networks. *SIAM J Appl Math*. 74:167–190.
- Rosen AFGG, Roalf DR, Ruparel K, Blake J, Seelaus K, Villa LP, Ciric R, Cook PA, Davatzikos C, Elliott MA et al. 2018. Quantitative assessment of structural image quality. *Neuroimage*. 169:407–418.
- Rosvall M, Bergstrom CT. 2008. Maps of random walks on complex networks reveal community structure. *Proc Natl Acad Sci U S A*. 105:1118–1123.
- Salmi J, Rinne T, Koistinen S, Salonen O, Alho K. 2009. Brain networks of bottom-up triggered and top-down controlled shifting of auditory attention. *Brain Res*. 1286:155–164.
- Satterthwaite TD, Elliott MA, Gerraty RT, Ruparel K, Loughhead J, Calkins ME, Eickhoff SB, Hakonarson H, Gur RC, Gur RE et al. 2013a. An improved framework for confound regression and filtering for control of motion artifact in the preprocessing of resting-state functional connectivity data. *Neuroimage*. 64:240–256.
- Satterthwaite TD, Elliott MA, Ruparel K, Loughhead J, Prabhakaran K, Calkins ME, Hopson R, Jackson C, Keefe J, Riley M et al. 2014. Neuroimaging of the Philadelphia neurodevelopmental cohort. *Neuroimage*. 86:544–553.
- Satterthwaite TD, Vandekar SN, Wolf DH, Bassett DS, Ruparel K, Shehzad Z, Craddock RC, Shinohara RT, Moore TM, Gennatas ED et al. 2015a. Connectome-wide network analysis of youth with Psychosis-Spectrum symptoms. *Mol Psychiatry*. 20:1508–1515.
- Satterthwaite TD, Wolf DH, Loughhead J, Ruparel K, Elliott MA, Hakon H, Gur RWC, Gur RWC. 2012. Impact of in-scanner head motion on multiple measures of functional connectivity: relevance for studies of neurodevelopment in youth. *Neuroimage*. 60:623–632.
- Satterthwaite TD, Wolf DH, Roalf DR, Ruparel K, Erus G, Vandekar S, Gennatas ED, Elliott MA, Smith A, Hakonarson H et al. 2015b. Linked sex differences in cognition and functional connectivity in youth. *Cereb Cortex*. 25:2383–2394.
- Satterthwaite TD, Wolf DH, Ruparel K, Erus G, Elliott MA, Eickhoff SB, Gennatas ED, Jackson C, Prabhakaran K, Smith A et al. 2013b. Heterogeneous impact of motion on fundamental patterns of developmental changes in functional connectivity during youth. *Neuroimage*. 83C:45–57.
- Sharma A, Wolf DH, Ciric R, Kable JW, Moore TM, Vandekar SN, Katchmar N, Daldal A, Ruparel K, Davatzikos C et al. 2017. Common dimensional reward deficits across mood and psychotic disorders: a connectome-wide association study. *Am J Psychiatry*. 174:657–666.
- Sporns O, Betzel RF. 2016. Modular brain networks. *Annu Rev Psychol*. 67:613–640.
- Sporns O, Tononi G, Kötter R. 2005. The human connectome: a structural description of the human brain. *PLoS Comput Biol*. 1:e42.
- van den Heuvel MP, Pol HEH. 2010. Exploring the brain network: a review on resting-state fMRI functional connectivity. *Eur Neuropsychopharmacol*. 20:519–534.
- van den Heuvel MP, Sporns O. 2013. Network hubs in the human brain. *Trends Cogn Sci*. 17:683–696.
- Yeo BTT, Krienen FM, Sepulcre J, Sabuncu MR, Lashkari D, Hollinshead M, Roffman JL, Smoller JW, Zollei L, Polimeni JR et al. 2011. The organization of the human cerebral cortex estimated by intrinsic functional connectivity. *J Neurophysiol*. 106:1125–1165.
- Zhang X, Martin T, Newman MEJ. 2015. Identification of core-periphery structure in networks. *Phys Rev E*. 91: 32803.