Research Article

Can Transcutaneous CO₂ Tension Be Used to Calculate Ventilatory Dead Space? A Pilot Study

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Dead space fraction (V_d/V_t) measurement performed using volumetric capnography requires arterial blood gas (ABG) sampling to estimate the partial pressure of carbon dioxide (P_aCO_2). In recent years, transcutaneous capnography ($P_{tc}CO_2$) has emerged as a noninvasive method of estimating P_aCO_2 . We hypothesized that $P_{tc}CO_2$ can be used as a substitute for P_aCO_2 in the calculation of V_d/V_t . In this prospective pilot comparison study, 30 consecutive postcardiac surgery mechanically ventilated patients had V_d/V_t calculated separately using volumetric capnography by substituting $P_{tc}CO_2$ for P_aCO_2 . The mean V_d/V_t calculated using P_aCO_2 and $P_{tc}CO_2$ was 0.48 ± 0.09 and 0.53 ± 0.08, respectively, with a strong positive correlation between the two methods of calculation (Pearson's correlation = 0.87, p < 0.05). Bland-Altman analysis showed a mean difference of -0.05 (95% CI: -0.01 to -0.09) between the two methods. $P_{tc}CO_2$ measurements can provide a noninvasive means to measure V_d/V_t , thus accessing important physiologic information and prognostic assessment in patients receiving mechanical ventilation.

1. Introduction

The ventilatory dead space fraction (V_d/V_t) is defined as the portion of tidal volume that does not participate in gas exchange because it does not reach perfused lung units. Clinically, V_d/V_t may be measured using volumetric capnography and the Enghoff modification of the Bohr equation, which states

$$\frac{V_{\rm d}}{V_{\rm t}} = \frac{\left(P_{\rm a} \rm CO_2 - P_e \rm CO_2\right)}{\left(P_{\rm a} \rm CO_2\right)},\tag{1}$$

where P_aCO_2 is the partial pressure of carbon dioxide in the arterial blood and P_eCO_2 is the partial pressure of carbon dioxide in exhaled air [1]. V_d/V_t may increase in a variety of pathological situations, especially conditions with obstruction of the pulmonary vasculature [2]. Measuring V_d/V_t requires arterial blood gas (ABG) sampling to measure P_aCO_2 [3]. Transcutaneous capnography ($P_{tc}CO_2$) has emerged as a noninvasive method of estimating P_aCO_2 [4]. The objective of our study was to evaluate the relationship between $P_{tc}CO_2$ and P_aCO_2 in calculating V_d/V_t . We hypothesized that $P_{tc}CO_2$ can be used as a substitute for P_aCO_2 in the calculation of V_d/V_t .

2. Methods

This was a prospective pilot comparison study conducted at a single 383-bed urban, community-teaching hospital. We recruited thirty consecutive adult patients admitted to the Surgical Intensive Care Unit (SICU) after cardiac surgery from May 1, 2014, until December 1, 2014. We excluded patients who were extubated within 4 hours of arrival to the SICU. The Bridgeport Hospital Institutional Review Board (IRB) approved this study.

Volumetric capnography was performed within 12 hours of patient arrival to the SICU. A CAPNOSTAT® CO₂ sensor was attached between the subject's endotracheal tube and the Y-piece of the ventilator circuit to obtain breath-by-breath volumetric capnography using NICO₂ volumetric capnography (Philips-Respironics®, Wallingford, CT). We measured PtcCO2using the Tosca 500 (Radiometer®, Copenhagen, Denmark), according to the manufacturer's instructions. A fully automated calibration of the transcutaneous CO₂ sensor (Tosca sensor 92) containing a Stow-Severinghaus type electrode was performed using CAL-Gas (Radiometer), which contained 12% O₂, 7% CO₂, and 81% N₂ prior to each monitoring period and every time the membrane of the transcutaneous sensor was changed (every 14 days). First, the sensor probe and the subject's earlobe were cleaned with alcohol and dried prior to each measurement. Then, the sensor was placed on the earlobe after placing a drop of contact solution provided by the manufacturer and secured by means of an adhesive clip. No PtcCO2 values were collected until the ear lobe reached an appropriate temperature of 42°C and stable signals for both $P_{tc}CO_2$ and P_eCO_2 were achieved after at least 15 minutes. The PtcCO2 was recorded at the same time an arterial blood sample was collected from an existing radial arterial line, placed on ice, and sent immediately for standard blood gas analysis. P_aCO₂ was measured using the arterial blood gas sample analyzed with Cobas b221 blood gas analyzer (Roche®). Turnaround time for the result was under 10 minutes for all samples. We calculated $V_{\rm d}/V_{\rm t}$ using both simultaneously measured values for P_aCO₂ and P_{tc}CO₂ using NICO₂ volumetric capnography according to the manufacturer's instructions. In this study, we used single measurements of P_eCO_2 , P_aCO_2 , and $P_{tc}CO_2$ to calculate V_d/V_t , with all values obtained simultaneously. The $V_{\rm d}/V_{\rm t}$ calculated using $P_{\rm a} CO_2$ was considered the reference standard [5].

2.1. Statistical Analysis. Statistical analysis was performed using SPSS version 9.0. Results from descriptive statistics are presented as mean \pm standard deviation (SD). Linear regression and Bland-Altman analyses were performed to compare the values of V_d/V_t using $P_{tc}CO_2$ and P_aCO_2 measurements.

3. Results

30 consecutive postcardiac surgery patients were included and 30 separate volumetric capnography measurements were obtained. Statistical description of the study population can be found in Table 1. 24 patients were males, mean age was 68.25 ± 6.36 years, and the mean Acute Physiology and Chronic Health Evaluation (APACHE) II score was $14.5 \pm$ 3.92. The mean V_d/V_t calculated using P_aCO_2 and $P_{tc}CO_2$ was 0.48 ± 0.09 and 0.53 ± 0.08 , respectively, with a strong positive correlation between the two methods of calculation (Pearson's correlation = 0.87, p < 0.05) as shown in Figure 1. Bland-Altman analysis showed a mean difference of -0.05(95% CI: -0.01 to -0.09) between the two methods of V_d/V_t measurements as shown in Figure 2.

4. Discussion

Measuring V_d/V_t at the bedside can be easily performed with volumetric capnography, in which both exhaled tidal volume and P_eCO_2 are measured. The P_eCO_2 is compared to P_aCO_2 determined from the arterial blood, and the Enghoff

TABLE 1: Patient demographic and clinical characteristics (n = 30).

Mean age (years) \pm SD	68.25 ± 6.36
Males	24
Types of cardiac surgery	
Valve replacement	12
CABG	12
Valve + CABG	4
Aneurysm	2
Cardiopulmonary bypass status	
On bypass	26
Off bypass	4
Mean APACHE II score ± SD	14.5 ± 3.92
Patient comorbidities ¹	
Cardiovascular	28
Respiratory	6
Endocrine	8
Neurology	3
Miscellaneous*	4
Vasopressor or inotrope support	14
Mean tidal volume on ventilator ² (mL) \pm SD	660 ± 95.95
Mean P_aCO_2 (mm of Hg) ± SD	35.93 ± 5.19
Mean $P_{tc}CO_2$ (mm of Hg) ± SD	39.73 ± 5.82
Mean shunt fraction $(Q_s/Q_t)^3$	0.19 ± 0.08

¹Patients may have more than one comorbidity.

*Miscellaneous comorbidities included cirrhosis, chronic kidney disease, HIV and malignancy.

²All patients maintained on volume assist control mode of mechanical ventilation.

³Measured only in 27 patients who had a pulmonary artery catheter.

Abbreviations: CABG: coronary artery bypass graft; APACHE: acute physiology and chronic health evaluation.

modification of the Bohr equation is used to calculate V_d/V_t [3]. V_d/V_t has been shown to be useful in identifying cardiac surgery patients with microthrombosis of the pulmonary circulation [6] and ARDS patients who have an increased risk for death [7]. It has also been proposed to help identify patients with pulmonary embolism [8] and to risk-stratify intubated patients for extubation failure [9]. A drawback of this method is that it requires sampling of the arterial blood, which can be painful and may cause complications. Thus, a noninvasive test to estimate V_d/V_t might be helpful.

A transcutaneous measurement of CO_2 is based on the principle that an increase in skin capillary blood flow facilitates diffusion of CO_2 , hence allowing its detection by a sensor located at the skin surface. The sensor is also equipped with a thermostatically controlled heater unit, which allows an increase in temperature of the skin surface. The Stove-Severinghaus type CO_2 sensor is a potentiometric sensor combining a silver/silver chloride reference electrode and a miniature glass pH electrode. $P_{tc}CO_2$ is determined by a change in pH of the electrolyte solution [4, 10].

 $P_{tc}CO_2$ is a noninvasive method of estimating P_aCO_2 used frequently in clinical practice. Its application has been widely noted during mechanical ventilation, anesthesia, bronchoscopy, and sleep studies [4]. Whether substituting $P_{tc}CO_2$ for P_aCO_2 yields accurate measurements of V_d/V_t



FIGURE 1: Scatter plot of V_d/V_t using P_aCO_2 against V_d/V_t using $P_{tc}CO_2$.



FIGURE 2: Modified Bland-Altman plot of $V_d/V_t(P_aCO_2) - V_d/V_t(P_{tc}CO_2)$ against mean of $V_d/V_t(P_aCO_2)$ and $V_d/V_t(P_{tc}CO_2)$.

is unreported in the scientific literature. We performed a prospective pilot comparison to explore whether using $P_{tc}CO_2$ in place of P_aCO_2 in the Enghoff-Bohr calculation would yield accurate estimates of V_d/V_t . Our observations show a strong positive correlation between both methods of estimating V_d/V_t with good agreement between the two techniques.

Our study has some limitations. First, the sample size is small. We consider our findings to be preliminary. They will require confirmation in a larger cohort of patients. Second, we conducted our study exclusively in patients who had undergone cardiac surgery, both emergent and elective. We chose this group because it is relatively homogeneous with regard to complicating respiratory and metabolic disorders, thereby minimizing residual confounders that might bias the results. Whether our findings can be extrapolated to other critically ill populations will require further investigation. For example, it is plausible that transcutaneous CO₂measurements will be less accurate in patients with circulatory failure or shock, as peripheral blood flow may be diminished. Finally, our goal was limited. We sought to test how well V_d/V_t calculations using $P_{tc}CO_2$ measurements compared to V_d/V_t calculations using P_aCO_2 . We did not employ a reference standard measurement of V_d/V_t such as mixed inert gas elimination technique, as such techniques are found only in highly specialized research centers. It is possible that unmeasured confounders that affect volumetric capnography might result in random or systematic biases that make our findings unreliable. Indeed, PtcCO2 could be influenced by advanced age, hypothermia, hypercapnia, and use of vasopressor and inotropic support. A larger observational study would be essential to determine the influence of these potential confounders on V_d/V_t measurement. Nonetheless, we believe that our methods represent a real-world approach to use bedside V_d/V_t measurements and that $P_{tc}CO_2$ may be an acceptable substitute for P_aCO_2 to calculate V_d/V_t .

Thus, we propose that substituting $P_{tc}CO_2$ for P_aCO_2 may be clinically useful and provide a noninvasive means for estimating V_d/V_t . Using a noninvasive CO₂ measurement to calculate V_d/V_t potentially could permit more frequent estimates of V_d/V_t when multiple samples of arterial blood are unavailable or invasive procedures are not desired. For example, it is plausible that following the V_d/V_t over the course of a spontaneous breathing trial could be useful at identifying patients at high risk for requiring continued mechanical ventilator support, as has been shown in pediatric patients with respiratory failure [11]. Future work incorporating noninvasive CO_2 measurements into V_d/V_t calculations should focus on whether these estimates are valid in a broader population of critically ill patients and whether V_d/V_t measurements can be incorporated into treatment strategies to yield improved patient-centered outcomes.

5. Conclusion

 $P_{tc}CO_2$ may be a useful substitute for P_aCO_2 to calculate the dead space fraction. $P_{tc}CO_2$ measurements can provide a noninvasive means to measure the dead space fraction, thus allowing us to obtain important physiologic information and prognostic assessment in critically ill patients on mechanical ventilation.

Competing Interests

The authors declare that they have no competing interests.

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