Combined culture experiment of mouse bone marrow mesenchymal stem cells and bioceramic scaffolds

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Abstract. Articular cartilage injuries are common orthopedic conditions that severely affect the quality of life of patients. Tissue engineering can facilitate cartilage repair and the key points involve scaffolding and seed cell selection. Pre-experiments found a range of microstructures of bioceramic scaffolds suitable for chondrocyte adhesion and proliferation, and maintaining chondrocyte phenotype. Three-dimensional cultures of bone marrow mesenchymal stem cell (BMSC) scaffolds were implanted into mice. According to the shape of the bioceramic scaffolds and the implantation time in vivo, RNA sequencing was performed on the removed scaffolds to explore the molecular mechanism. The in vitro bone plate culture can induce differentiation of chondrocytes, making culture different to that produced in vitro. Implantation of scaffolds in vivo increases the expression of bone-related genes. The ceramic rod-like material was found to be superior to the disc shape, and the bone repair effect was more marked with longer implantation times. Gene Ontology analysis revealed that 'cell chemotaxis', 'negative regulation of ossification' and 'bone development' pathways were involved in recovery. It was further confirmed that BMSCs were suitable as seed cells for cartilage tissue engineering, and that the β -tricalcium phosphate scaffold maybe ideal as cartilage tissue engineering scaffold material. The present research provided new insights into the molecular mechanism of cartilage repair by BMSCs and bioceramic scaffolds. Bioinformatics analysis revealed that AMMECR1L-like protein, tumor necrosis factor-induced protein 2, inhibitor of nuclear factor-B kinase subunit and protein kinase C type and 'negative regulation of ossification'

and 'bone development' pathways may be involved in osteoblast maturation and bone regeneration.

Introduction

Articular cartilage injury is a common and frequent disease-related orthopedic condition (1). Inadequate and improper treatment can lead to osteoarthritis, pain and dysfunctional walking, which affect the quality of life of patients (2). Due to poor self-repairing ability of the articular cartilage, the current clinical treatment of articular cartilage defects is not satisfactory; in particular, repair of the damage to the full-thickness articular cartilage is a challenge for clinicians (3). Tissue engineering can facilitate cartilage repair, with numerous successful reports based on animal experiments (4,5). Scaffold and seed cell selection are important factors affecting cartilage repair.

Bone marrow mesenchymal stem cells (BMSCs) are suitable cellular materials for articular cartilage repair. Cartilage differentiation is an intrinsic property of mesenchymal stem cells (6). Most in vitro and in vivo studies suggest that BMSCs have the potential to increase osteoinduction and osteogenesis (7-11). A study has demonstrated that seeding BMSCs on biocompatible scaffolds may be an effective method for treating nonunion fractures (12). Mesenchymal stem cells have the potential to home to damaged areas, which may enhance repair in two respects: i) Differentiation of tissue cells, specifically, the recovery of lost morphology and function; and ii) secretion of various biologically active factors, which have antiapoptotic effects and immunoregulatory functions, thereby creating an environment that stimulates the proliferation of endothelial progenitor cells and leads to subsequent repair (13). A clinical study has demonstrated the effectiveness of direct local BMSC delivery by injection in promoting bone regeneration (14). However, in large bone defects where a significant amount of bony tissue has been lost, the direct injection method was found to be ineffective for BMSC delivery and the commensurate acceleration of the bone healing process (15). Cartilage repair without a scaffold or soft support does not provide sufficient mechanical support, leading to insufficient cell enrichment in the repair area, hindering early weight bearing and an environment with insufficient pressure and nutritional support to induce cartilage repair (16). The bioceramic hard scaffold is prepared using a controlled microporous structure of β-tricalcium

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phosphate (β -TCP) as the raw material (17). β -TCP is capable of triggering proliferation, migration and differentiation of the bone cells required for bone regeneration (18,19). Porous ceramics have good biocompatibility and high mechanical strength, and their porous structure and degradation rate can be controlled according to the growth of the tissue (20). Physical microstructures, such as the bore and internal junction, can be regulated to facilitate cell adsorption and proliferation (15). High-porosity scaffolds facilitate the migration and proliferation of bone marrow cells in the scaffold, which is essential for the repair of osteochondral injury (21).

Previous experiments were conducted to determine a preliminary range of bioceramic scaffold microstructures suitable for promoting chondrocyte adhesion and proliferation and for maintaining the chondrocyte phenotype. The present study implanted a three-dimensional culture of BMSC scaffolds into mice and used RNA sequencing to explore the molecular mechanism of the bioceramic scaffolds on the basis of their shape and duration of implantation.

Materials and methods

Cell culture and flow cytometry. The 3rd generation BMSCs (CinoAsia Co., Ltd.) were digested using trypsin, after which $1x10^5/ml$ cell suspensions in DMEM/F12 (Gibco; Thermo Fisher Scientific, Inc.) were generated in an eppendorf tube. A total of 10 μ l fluorescently-labelled CD34 (cat. no. ab8158), CD45 (cat. no. ab33923) and CD44 (cat. no. ab119348) antibodies (all, Abcam; all, 1:100) were added to 100 μ l of the cell suspension and incubated for 1 h at 37°C. Flow cytometry was performed to detect individual cell markers (FACSMelody; Becton, Dickinson and Company). BMSCs were counted and resuspended in complete DMEM/F12 supplemented with 10% fetal bovine serum and 1% senicillin-streptomycin solution (all, Gibco; Thermo Fisher Scientific, Inc.). Samples were cultured at 37°C and cell density was adjusted to 1x10⁶ cells/ml.

Combined culture of BMSCs and bioceramic scaffolds. The β -TCP bioceramic material (purchased from Shanghai Bio-lu Biomaterials Co., Ltd.) was prepared and placed in a 24-well plate. First, 200 μ l of BMSCs suspended in DMEM/F12 (Gibco; Thermo Fisher Scientific, Inc.) were added to one side of the ceramic plate and incubated for 1 h at 37°C. Subsequently, 200 μ l of the cell suspension was added to the reverse side, where it was incubated for another 1 h at 37°C. DMEM/F12 was added to a total volume of 1 ml/well and scaffolded cells were placed into medium for routine culture.

Bioceramic scaffolds implanted in mice. After 3 days of culture, the bioceramic scaffolds were planted into the femoral trochlea of the mice, where they remained for 3 or 6 days. The scaffolds were removed from the mice and crushed with small tweezers. A total of 40, six-week-old male mice (weight, 22-26g, Shanghai SLAC Laboratory Animal Co., Ltd.) were randomly divided into 5 groups (each, n=8). Animals were maintained at 25°C, with a relative humidity of 40-70%, under specific-pathogen free conditions. Animals were housed under a 12 h light/dark cycle with free access to food and water. Mice anaesthetized by intraperitoneal injection of 1%

sodium pentobarbital (50 mg/kg). Following implantation of the ceramic material, the health and behavior of the mice were observed every day. Following removal of the ceramic material after 3 or 6 days, mice were intraperitoneally injected with an overdose (1%; 150 mg/kg) of sodium pentobarbital for euthanasia. Mice with no breathing for 3 min and no corneal reflex were considered to be successfully euthanized.

Sequencing. Several small particles were placed in cell lysates (0.2% triton X-100+5% RNase inhibitor), and stored at -80°C for *in vitro* sequencing. The cultured ceramic material was digested with trypsin, and the library was sequenced. The sequences were grouped into controls (untreated mice; CONT); ceramic disc *in vitro* (MAT1); ceramic rod *in vitro* (MAT2); ceramic rod, 3 days *in vivo* (DAY3) and ceramic rod, 6 days *in vivo* (DAY6). Experiments in each group were performed in triplicate.

Ethical approval. All experiments were performed according to the principles outlined in the Guide for the Care and Use of Laboratory Animals and approved by the Ethics Committee of Huashan Hospital Affiliated to Fudan University (approval no. 2018 Huashan Hospital JS-098).

RNA database and sequencing. The cells cultured as described above were subjected to RNA sequencing, and each group was replicated three times. Cellular RNA was extracted and reverse transcribed into cDNA for PCR amplification. The PCR amplification reaction product was purified and subjected to quality control in a 96-well plate. The samples described above were measured by molar conversion, and each 2 nM sample was diluted to 1:1. After dilution, 10 μ l of the sample was removed from the main tube and sent to the sequencing company for quality control with a 2100 QC bioanalyzer (Agilent Technologies, Inc.) before sequencing. The Hiseq2500 sequencer(Illumina, USA) was used, and the sequencing mode was set to a 2x150 bp read length with a 250 M read number.

Raw data processing. The raw data were first processed using Trimmomatic (http://www.usadellab.org/cms/) to remove sequencing linker sequences and low quality read lengths. The remaining high-quality reads were aligned with the 25,014 genes of the Mus musculus genome using HiSat2 (http://daehwankimlab.github.io/hisat2/main/). The expression levels of each gene were quantified using featureCounts software, which produced raw count values for each sample. For raw data analysis, the counts of the sample genes were defined as >1, which was used as the base count value for the expressed genes. The read count was then normalized to the transcripts per kilobase million value for the log2 conversion with the 'newSCESet' function of the 'scater' package in R (https://www.r-project. org/). Principal component (PC) analysis, one-way ANOVA and hierarchical cluster analysis (HCA) using the 'prcomp', 'cor', 't.test' and 'cluster' functions were performed using the R 'cluster stats' package. Following analysis, a heatmap was generated with the R 'ComplexHeatmap' package and the PC analysis results were visualized using 'ggplot'.

Analysis of differentially expressed genes (DEGs). DEGs were identified by calculating the fold-change and P-values



Figure 1. Expression of surface markers CD44 (95.3%), CD34 (1.39%) and CD45 (0.22%) in bone marrow mesenchymal stem cells as determined by flow cytometry.

of the experimental and control groups. The multiples were modified to be >two-fold; P<0.05 was used as the standard for DEG selection and the 'stat' package in R was used. DEG intersections were determined with a 'Venn diagram' online tool (http://bioinformatics.psb.ugent.be/webtools/Venn/). Pathway analysis was performed using and Gene Ontology (GO; http://geneontology.org/) analysis was performed using the Database for Annotation, Visualization and Integrated Discovery (version 6.7; https://david.ncifcrf.gov/).

mRNA sequencing analysis. The quality of the sequencing data was evaluated prior to data analysis using FastQC.

Results

Cell identification. The cell surface antigens were detected by flow cytometry. The BMSC marker CD44 (95.3%) was expressed, but not CD34 (1.39%) or CD45 (0.22%), indicating that the cells were BMSCs (Fig. 1).

RNA sequencing analysis. PC1 level analysis showed a good sample repeatability within the group, and the ceramic scaffold culture was superior compared with the CONT group. The degree of differentiation in three groups was measured by diffusion pseudotime analysis. Compared with MAT1 group, MAT2 group was farther from the CONT group in terms of the evolutionary trajectory, MAT2 was exhibited with a more differentiated state. Compared with the CONT group, the MAT2 group was superior to the MAT1 group (Fig. 2A). HCA revealed the characteristic genes of each group (Fig. 2B). Characteristic genes of the CONT group included transcription factor HES-1, ferritin light chain 2 and serine/threonine-protein phosphatase PP1-a catalytic subunit. Characteristic genes of the MAT1 group included neutrophil gelatinase-associated lipocalin (Lcn2), decorin (Dcn) and thrombospondin 2 (Thbs2). Characteristic genes of the MAT2 group included Lcn2, Dcn, Thbs2 and C-C motif chemokine ligand 7 (Ccl7).

Comparison between the top 10 upregulated and downregulated genes in the MAT1 and MAT2 groups compared with the CONT group found that the shared genes were serum amyloid A-3 protein (Saa3), Lcn2, nitric oxide synthase (Nos2) and nuclear receptor subfamily 4 group A member 1 (Tables I and II).

The DEGs between the MAT1 and MAT2 groups were compared, and the top 10 upregulated and downregulated genes are listed in Table III. Functional and pathway analysis of the DEGs was further performed (Fig. 3A). Three bone-related genes, NADH: Ubiquinone oxidoreductase subunit B6 (Ndufb6), ribosomal protein L17, pseudogene 9 (Rpl17-ps9) and Ccl7, were selected for comparison (Fig. 3B).

Based on the DEG analysis, there were 1,274 DEGs in the MAT2 and CONT groups, 2,659 DEGs in the DAY3 and CONT groups and 1,785 DEGs in the DAY6 and DAY3 groups. With additional searches for genes with consistently changed expression compared with the CONT, MAT2 and the DAY3 and DAY6 groups, 10 genes were found to have increased expression levels: AMMECR1L-like protein (Ammecr11), tumor necrosis factor a-induced protein 2 (Tnfaip2), La Ribonucleoprotein 4B, Zinc Finger ZZ-Type And EF-Hand Domain Containing 1, Acid Phosphatase 2, inhibitor of nuclear factor κ-B kinase subunit ε (Ikbke), protein kinase C δ type (Prkcd), ATP Binding Cassette Subfamily A Member 1, CD44 Molecule and HIVEP Zinc Finger 2. A total of nine genes were found to have decreased expression levels:, including ferredoxin-1 (Fdx1), Eukaryotic Translation Initiation Factor 4E Binding Protein 1 (Eif4ebp1), insulin-like growth factor-binding protein 6 (Igfbp6), Solute Carrier Family 25 Member 4 (Slc25a4), Ribosomal Protein L14 (Rpl14), Actin Alpha 2, Smooth Muscle (Acta2), barrier-to-autointegration factor 1 (Banf1), Cytochrome C Oxidase Subunit 4I1 (Cox4i1) and elongation factor 2 (Eef2) (Fig. 4A). The heatmaps of these 19 common upregulated and downregulated genes were generated, with Table I. Top 10 differentially expressed genes of the MAT1 group compared with the CONT group.

A, Upregulated genes			
Gene name	FC	P-value	
Saa3	2847.6775	0.0012	
Lcn2	304.3738	0.0109	
RP23-459L15.8	47.7720	0.0012	
Egfros	46.0328	0.0021	
RP23-380F8.2	44.2728	0.0194	
Nos2	43.0737	0.0023	
Fam71f2	40.7737	0.0026	
Gtf2a11	39.3699	0.0043	
RP24-111C16.1	37.2839	0.0125	

B, Downregulated genes

Gene name	FC	P-value
Yif1b	0.0348	0.0173
Rpl23a-ps1	0.0295	0.0053
Rps2-ps13	0.0284	0.0299
RP24-574O8.7	0.0264	0.0023
Hes1	0.0247	0.0043
Ftl2	0.0199	0.0376
Ppp1ca	0.0193	0.0307
Nme2	0.0165	0.0051
Nr4a1	0.0246	0.0215

FC, fold-change; CONT, control group; MAT1, ceramic disc *in vitro* group.

blue indicating lower expression (TPM \leq 5) and red indicating higher expression (TPM >5) (Fig. 4B). The top 10 continuously elevated genes were included in a trend graph (Fig. 4C).

Further GO analysis of trend genes revealed that the main enriched pathways were 'cell chemotaxis', 'negative regulation of ossification' and 'bone development pathway' (Fig. 5).

Discussion

Articular cartilage repair is a prominent focus of current research and represents a problem that needs to be resolved in clinical practice. The current experiments involve seed cells cultured *in vitro* and conventional soft scaffold structures that cannot be regulated and have biomechanical problems, which hinder the transformation of experimental results into clinical applications. It is crucial to prepare biodegradable scaffolds with osteoinductive properties; their application can provide a 3D environment for BMSCs at the site of the defect, where they can promote angiogenesis and thus contribute to the healing process (22). The biological materials currently used for bone repair include medical bioceramics, medical polymer materials, medical composite materials and artificial nanobone (23). Table II. Top 10 differentially expressed genes of the MAT2 group compared with the CONT group.

A, Upregulated genes

Gene name	FC	P-value	
Saa3	2584.2307	0.0037	
Lcn2	158.9995	0.0130	
Saa1	66.5714	0.0167	
Saa2	62.8477	0.0043	
Ср	48.7990	0.0084	
Nos2	44.6269	0.0083	
Cxcl5	41.3231	0.0220	
Dcn	38.1207	0.0004	
Mmp3	37.9426	0.0004	

B, Downregulated genes

Gene name	FC	P-value
Slc34a2	0.0675	0.0263
Fos	0.0660	0.0003
Rps2	0.0643	0.0067
Hist1h2af	0.0479	0.0461
Cdsn	0.0439	0.0147
Spon2	0.0368	0.0040
Wnt4	0.0287	0.0097
Dlk2	0.0234	0.0099
Nr4a1	0.0221	0.0243
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FC, fold-change; CONT, control group; MAT2, ceramic rod *in vitro* group.

Table III. Top 10 differentially expressed genes in the MAT1 and MAT2 groups.

A, Upregulated genes			
Gene name	FC	P-value	
Ndufb6	36.7160	0.0245	
RP24-574O8.7	22.5928	0.0039	
Rpl17-ps9	20.2378	0.0356	
Rpl23a-ps1	18.4759	0.0090	
Mrpl24	14.4720	0.0260	
Hspe1-ps2	14.2868	0.0333	
Ccl7	13.0649	0.0221	
Mrps36-ps2	12.4257	0.0297	
RP24-272N10.4	11.2402	0.0132	
Fth-ps2	10.6130	0.0475	

B, Downregulated genes

FC	P-value
0.0797	0.0383
0.0792	0.0152
0.0691	0.0005
0.0649	0.0065
0.0643	0.0427
0.0625	0.0050
0.0545	0.0071
0.0454	0.0198
0.0427	0.0045
0.0376	0.0353
	FC 0.0797 0.0792 0.0691 0.0649 0.0643 0.0625 0.0545 0.0545 0.0454 0.0427 0.0376

FC, fold-change; MAT1, ceramic disc *in vitro* group; MAT2, ceramic rod *in vitro* group.

In the present study, based on the microstructure characteristics of the hard bioceramic scaffold, the bioceramic scaffold was used to implant into the articular cartilage defect in mice. The scaffold suitable for microstructure absorbs autologous bone marrow cells and proliferates in the scaffold to repair articular cartilage. Seed cells do not need to be cultured in vitro, and the experimental results may provide a basis for clinical application. Since BMSCs and their differentiation during remodeling processes have essential roles in bone regeneration, it is thought that understanding the molecular signaling pathways involved is crucial to the development of bone implants, bone substitute materials and cell-based scaffolds for bone regeneration (24). The present study cultured and implanted BMSC scaffolds into mice and used RNA sequencing to explore the molecular mechanism of the bioceramic scaffolds according to the scaffold shape and duration of implantation.

PC1 level analysis showed that the measurements were reproducible, and the ceramic scaffold culture was better compared with the CONT group. The outcome for the MAT2 group was better compared with the MAT1 group; HCA results revealed the DEGs of each group. The MAT2 rod material is easier to implant compared with the MAT1 disc and has a high degree of surface smoothness; this result can be used to optimize the clinical choices of bioceramics. By comparing the top 10 upregulated genes in the MAT1 group compared with the CONT group and in the MAT2 group compared with the CONT group, the intersection genes were found to be Saa3, Lcn2 and Nos2. Saa3 is a secreted protein that is prominently expressed in bone cells and affects bone metabolism by regulating genes expressed during inflammation, apoptosis and bone matrix remodeling (25). Saa3 may have a number of different biological functions related to extracellular matrix repair, bone remodeling, bone resorption and bone development (25). LCN2 is secreted by osteoblasts and is involved in bone metabolism, which is essential for bone health (26). Nos2 is elevated in osteoblasts and chondroblasts in bones during the early stages of fracture healing (27). Therefore, the bioinformatics analysis performed in the current study suggests that ceramic materials may be beneficial for bone formation.

Further comparison of the DEGs in the MAT2 and MAT1 groups revealed that the expression levels of osteogenesis-related genes, such as Ndufb6, Rpl17-ps9 and Ccl7, were upregulated. Ndufb6 is a component of the human skeletal



Figure 2. Principal components analysis and characteristic gene analysis. (A) Principal component 1 level analysis showed that the samples in each experimental group were reproducible, and the ceramic scaffold culture was superior to that of the control group. The MAT2 group had better reproducibility compared with the MAT1 group. (B) Hierarchal clustering analysis map showing the characteristic genes in each group. CONT, control group; MAT1, ceramic disc *in vitro* group; MAT2, ceramic rod *in vitro* group.



Figure 3. MAT2-MAT1 differentially expressed gene analysis. (A) GO analysis of differentially expressed genes between the MAT1 and MAT2 groups. (B) Comparison of Ndufb6, Rpl17-ps9 and Ccl7 gene expression in the MAT1 and MAT2 groups. *P<0.05 and ***P<0.001. GO, Gene Ontology; MAT1, ceramic disc *in vitro* group; MAT2, ceramic rod *in vitro* group; Ndufb6, NADH: Ubiquinone oxidoreductase subunit B6; Rpl17-ps9, ribosomal protein L17, psudogene 9; Ccl7, C-C motif chemokine ligand 7.

muscle respiratory chain (28). Rpl17 can be used in the early stages of osteogenic differentiation in mouse bone marrow mesenchymal stem cells (29). CCL7 increases the mRNA levels of a number of genes involved in metastasis and osteolysis (30). Therefore, it was hypothesized that the material used in the MAT2 group may be superior to that used in the MAT1 group. Therefore, rod-shaped ceramic implants used in the MAT2 group were selected for subsequent *in vivo* experiments.

The ceramic rods were implanted into mice for 3 or 6 days. By comparing the DEGs of each group, it was found that there were 10 genes with increased expression levels, such as Ammecr11, Tnfaip2, Ikbke and Prkcd. Nine genes, including Fdx1, Igfbp6, Banf1 and Eef2 showed decreased expression levels. Further GO analysis of the 19 DEG expression trends revealed that the main pathways involved were 'cell chemotaxis', 'negative regulation of ossification' pathway and 'bone development'. The involvement of the important signaling pathways associated with the bone development during embryogenesis, as well as during fracture healing and repair has been demonstrated by various studies. These include the Wnt/ β -catenin, Notch, bone morphogenic protein/transforming growth factor- β , PI3K/Akt/mTOR, mitogen-activated protein kinase, platelet-derived growth factor, insulin-like growth factor, fibroblast growth factor and Ca²⁺ pathways (24). It has been suggested that BMSCs and their differentiation during the remodeling processes, as well as specific signaling pathways and their activated downstream networks, are implicated in bone regeneration (31). The present study indicated that the BMSC ceramic rod was successfully implanted into the mouse and played a role in repairing bone damage. The bone repair effect was more obvious as the implantation time was increased. Numerous treatment strategies can improve bone repair, which opens up new avenues for bone regeneration therapies. One of the strategies is based on the study of molecular signaling pathways. Changing gene expression levels to increase the number of osteoblasts or promote their maturity is expected to stimulate bone regeneration. The experimental limitation of the present study is the lack of quantitative PCR and western blot validation data, which will be performed in subsequent studies.

The present study successfully performed three-dimensional culture of mesenchymal stem cell composite scaffolds in mice and used RNA sequencing to explore its molecular mechanism based on the shape of bioceramic scaffold and the duration of implantation *in vivo*. Molecular studies found that rod-shaped ceramic materials were superior to the disc shape.



Figure 4. Gene expression trend analysis. (A) Venn diagram showing upregulated and downregulated differentially expressed genes of MAT2 vs. CONT, DAY3 vs. CONT and DAY6 vs. DAY3. (B) Heat map showing trend changes in CONT-MAT2-DAY3-DAY6 genes. (C) Trend chart of top 10 genes with continually increased expression.



Figure 5. GO analysis and interaction network of the gene trends (upregulated and downregulated differentially expressed genes of CONT, DAY3 vs. CONT and DAY6 vs. DAY3.). GO, Gene Ontology. (A) GO analysis of trend genes revealed the main enriched pathways. (B) Trend gene interaction network.

This conclusion may be used to optimize clinical choices for bioceramics. By comparing the DEGs of each group, it was further confirmed that BMSCs were suitable as seed cells for cartilage tissue engineering, and the β -TCP scaffold may be ideal cartilage tissue engineering scaffold material. The present research provided new insights into the molecular mechanism of cartilage repair by BMSCs and bioceramic scaffolds.

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Availability of data and materials

The datasets used and/or analyzed during the present study are available from the corresponding author on reasonable request.

Authors' contributions

XH and ZC conceptualized the study, designed the research and performed the experiments. GZ and JS performed the experiments. GH, FC, YW and JX analyzed and interpreted the data. JC and SW designed the experiments, analyzed and interpreted the data, wrote and edited the manuscript, and supervised the project. All authors read and approved the final manuscript.

Ethics approval and consent to participate

All experiments were performed according to the principles outlined in the Guide for the Care and Use of Laboratory Animals and the current study was approved by the Ethics Committee of Huashan Hospital Affiliated to Fudan University (approval no. 2018 Huashan Hospital JS-098).

Patient consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

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