

Research Article

A Novel Domperidone Hydrogel: Preparation, Characterization, Pharmacokinetic, and Pharmacodynamic Properties

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Received 11 September 2010; Accepted 29 November 2010

Academic Editor: Yellela S. R. Krishnaiah

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The purpose of the present study was to prepare a novel domperidone hydrogel. The domperidone dispersion was prepared by the solvent evaporation method. The characteristics of domperidone dispersion were measured by dynamic light scattering (DLS), scanning electronic microscopy (SEM), differential scanning calorimetry (DSC), X-ray diffractometry, and solubility test, respectively. Domperidone hydrogel was prepared by directly incorporating the domperidone dispersion in Carbopol hydrogel to increase its mucoadhesive properties to gastrointestinal tract (GIT). The *in vivo* pharmacokinetic and pharmacodynamic studies were investigated to evaluate the relative oral bioavailability and the propulsion efficacy of domperidone hydrogel as compared with market domperidone tablet (Motilium tablet). The particle size of domperidone dispersion in distilled water was 454.0 nm. The results of DSC and X-ray indicated that domperidone in dispersion was in amorphous state. The solubility of domperidone in the dispersion in distilled water, pH of 1, 5, and 7 buffer solution was 45.7-, 63.9-, 13.1-, and 3.7-fold higher than that of raw domperidone, respectively. The area under the plasma concentration curve (AUC₀₋₂₄) in domperidone hydrogel was 2.2-fold higher than that of tablet. The prolonged propulsion efficacy in the domperidone hydrogel group compared to that in tablet group was observed in the pharmacodynamic test.

1. Introduction

Domperidone, a dopamine D₂ receptor antagonist, is used as a prokinetic and antiemetic agent for the treatment of gastroparesis, nausea, and vomiting [1]. Domperidone is a weak base with good solubility in acidic pH but in alkaline pH, its solubility is significantly reduced [2]. The oral bioavailability of domperidone has been reported at the range of 13–17% [3]. The poor aqueous solubility may be one possible reason for its low bioavailability. In order to increase the bioavailability of domperidone, a controlled release dosage form has been prepared to increase the solubility of domperidone in the alkaline medium [2]. Recently, the domperidone gastric floating matrix tablet has been demonstrated to prolong the presence of the dosage form in the stomach or the upper small intestine and increase the amount of dissolved domperidone in

gastric medium [4]. Therefore, it may play a key role of enhancing the solubility of domperidone in the aqueous medium.

The oral bioavailability of amorphous drugs can be improved because of the increase of apparent solubility [5–7]. In addition, supersaturation of the drug in the gastrointestinal tract, particularly in the upper intestine, may lead to faster permeation rates through biomembranes and thus, enhance absorption [8–10]. Many polymers have been used as crystallization inhibitors to form amorphous solid dispersion in order to avoid forming lower energy crystalline states. These polymeric crystallization inhibitors orient preferentially to the water/drug particle interface to stabilize the particles. Recently, itraconazole amorphous nanoparticles and amorphous compositions have been reported to increase the supersaturation of itraconazole [11–19]. In addition, felodipine amorphous nanoparticles were investigated by

an evaporation method using PVP as a hydrophilic polymeric carrier [20]. The author indicated that the interaction at the molecular level of drug with the polymer carrier would control the physical state and the particle size of drug-carrier system. Being controlled by the relatively strong interaction of felodipine with PVP, the drug forms amorphous particles in the nanometer size range. Otherwise, for felodipine/PEG system, the drug is dispersed as crystals having sizes in the microrange.

Mucoadhesive hydrogel prepared by bioadhesive polymer has the property of increasing the time of retention in GIT when it orally administrated. Carbopol is one of the currently most widely used mucoadhesive hydrogel polymers. Now, a relevant amount of work has been done on its bioadhesive properties [21–24]. In particular, Carbopols may be used in oral preparations to improve GIT retention time. It has been reported that the combination of nanosized drug particles with Carbopol hydrogel would increase mucoadhesive properties of the drug particles, and then achieve a sufficiently high bioavailability [25]. When nanosized drug particles are directly dispersed in the hydrogel, the mucoadhesive polymer will be absorbed onto the particle surface and the contact time of drug particles with GIT mucous membranes will further increase.

The aim of the present study was to prepare a novel domperidone hydrogel and evaluate its *in vivo* properties. The domperidone dispersion was prepared by a solvent evaporation method using polyvinylpyrrolidone K30 as a hydrophilic polymer. The dynamic light scattering (DLS) technique was used to measure the particle size of the domperidone dispersion in distilled water. Morphological and thermal behaviors of the domperidone dispersion were examined by scanning electronic microscopy (SEM) and differential scanning calorimetry (DSC), respectively. Also, X-rays were used to investigate the characteristic of drug crystallinity. The solubility of domperidone in dispersion was tested. Domperidone hydrogel was prepared by directly incorporating the domperidone dispersion in Carbopol hydrogel. The *in vivo* pharmacokinetic and pharmacodynamic studies were investigated to evaluate the relative oral bioavailability and propulsion efficacy of domperidone hydrogel compared with market domperidone tablet (Motilium tablet).

2. Materials and Methods

2.1. Materials. Domperidone (the purity more than 99.5%) was purchased from the Baotai Pharmaceutical Co. of Shanxi, China. Polyvinylpyrrolidone K₃₀ (PVP K₃₀) was obtained from ISP Technologies, INC. (A local agent in Beijing, China). Carbopol 974 P was kindly provided by BF Goodrich Specialty Chemicals (a local agent in Beijing, China). The market domperidone tablet, Motilium tablet (10 mg/per tablet, Lot: 0611211114, Xian Janssen Co. China) was purchased from Beijing pharmacy. Absolute alcohol was obtained from the Beijing Chemical Factory. All other chemicals were of analytical grade or HPLC grade.

2.2. Animals. Healthy adult male beagle dogs weighting 9–11 kg and male Kunming mice weighing 18–21 g were supplied by the Department of Experimental Animals (Peking University Health Science Center) and maintained under natural light/dark conditions. Animals were acclimatized for 7 days prior to experiment and were allowed free access to standard food and water. Temperature and relative humidity were maintained at 25°C and 50%, respectively. All care and handling of animals were performed with the approval of Institutional Authority for Laboratory Animal Care of Peking University.

2.3. Preparation of Domperidone Dispersion and Physical Mixture. Domperidone dispersion was prepared by dissolving accurately weighed amounts of domperidone (50 mg) and PVP K₃₀ (500 mg) (1:10 w/w) in dehydrated ethanol in a closed glass receiver. After complete dissolution, the solvent was evaporated under reduced pressure at 50°C to form a uniform film. Desiccation was completed in a vacuum oven until constant weight was achieved. After adding distilled water, the mixture was sonicated for five minutes and then lyophilized to form a pulverous domperidone dispersion using an FD-2B Lyophilizer (Boyikang Co., Beijing, China).

Physical mixture was prepared by simple intensive mixing of domperidone and PVP K₃₀ previously grinded for 1–2 min in a mortar until a homogeneous mixture was obtained. The resulting mixture was sieved through grade 60 and then stored in a desiccator at room temperature until use.

2.4. Particle Size Analysis. The particle size of domperidone dispersion in distilled water (1 mg domperidone dispersion suspended in 10 mL distilled water) was determined by dynamic light scattering (DLS) using a Zetasizer Nano-Instrument (Malvern Instruments, Nano ZS, ZEN3600, UK).

2.5. Scanning Electron Microscopy (SEM). SEM analysis was carried out using a Jeol JSM-5600LV scanning electron microscope (Japan). Prior to examination, samples were gold sputter-coated to render them electrically conductive.

2.6. Differential Scanning Calorimetry (DSC). The DSC studies were conducted using a Thermal Analysis DSC-Q100 differential scanning calorimeter (USA). About 5 mg of samples including raw domperidone, raw PVP, physical mixture, and domperidone dispersion were encapsulated in flat-bottomed aluminum pans. The thermograms were recorded at a heating rate of 10°C · min⁻¹ from 30 to 280°C using nitrogen as the purging gas.

2.7. Powder X-Ray Diffraction (PXRD). The powder X-ray diffraction patterns were obtained with a Rigaku Dmax/2400 apparatus (Japan) using Cu-K α radiation ($\lambda = 1.541$ nm), a voltage of 40 kV and a 100 mA current. Samples were scanned from 5–30° 2 θ for qualitative studies and the scanning rate was 4° · min⁻¹.

2.8. Solubility Determination. Excess amounts of raw domperidone or domperidone dispersion were added into 50 mL polypropylene conical tubes with suitable volume of buffer solution (pH 1.0, 5.0, and 7.0) or distilled water, respectively. Then, the capped tubes were agitated at 37°C in a thermostatically controlled water bath for 48 hours. After equilibrium had been attained, the solutions were immediately and rapidly filtered through a 0.22 μm Millipore filter (supplied by Jingteng Science China Corp.) and the filtrate was diluted with buffer solutions or distilled water. The amount of domperidone in each diluted sample was analyzed by the HPLC system (Waters Co. Inc., Westerville, OH, USA), which was equipped with a 1525-pump, 2487-ultraviolet detector, and a Phenomenex ODS3 (250 \times 4.60 mm, 5 μm) chromatographic column. The mobile phase, composed of methanol-0.06 M ammonium acetate (70:30), was delivered at 1.0 mL/min. The injection volume was 20 μL . The drug was detected at 287 nm and the retention time of the drug was \sim 10 min. The drug concentration in the filtrate represented its saturation solubility. The experiment was conducted in triplicate.

2.9. Preparation of Domperidone Hydrogel. Carbopol 974 P was dispersed in distilled water. After equilibrated for 24 h, the Carbopol 974 P suspension was neutralised by addition of triethanolamine (adjusted to pH 7.0–7.5) to obtain the hydrogel (0.25% w/w). The domperidone dispersion was directly incorporated into the hydrogel with stirring to obtain the domperidone hydrogel. The content of domperidone in hydrogel was 1 mg per mL hydrogel.

2.10. Pharmacokinetic Studies of Domperidone Hydrogel in Beagle Dogs. Three adult male beagle dogs weighting 9–11 kg, after denied food overnight for at least 12 hours but had access to water ad libitum, were orally received marketed domperidone tablet or domperidone hydrogel at 8:00 a.m. with 30 mL of distilled water in a crossover manner with one week washout period, respectively. The dose of domperidone administered to each dog was 10 mg/body. All the experiments were carried out at the same time of the day to exclude the influence of circadian rhythms. After oral administration of domperidone formulations, blood sample (about 0.8 mL) was collected with glass vials containing lyophilized sodium heparin from the jugular vein at 0, 0.17, 0.33, 0.5, 1, 1.5, 2, 2.5, 3, 4, 6, 8, 12, 18, and 24 hours intervals. After centrifugation at 3000 g for 5 min, the plasma samples were obtained and stored at -20°C until analysis. The measurement method of domperidone in plasma was modified according to the previous report [26]. Briefly, an aliquot of 400 μL plasma samples, 100 μL propranolol solution (25 $\mu\text{g}/\text{mL}$, as an internal standard, the purity was 99.22%), 100 μL NaOH (0.1 M), 0.5 mL acetonitrile, and 4 mL absolute ether were mixed by a vortex mixer for 1 min. The mixture was centrifuged at 5000 g for 10 min. Then, a volume of 4.0 mL of supernatant was collected, and dried under a low flow of nitrogen gas at 50°C in a water bath. The residue was reconstituted using

the mobile phase (100 μL), then, an aliquot of this solution (50 μL) was injected onto and assayed by Agilent 1100 HPLC system consisting of a G1321A spectrofluorometric detector (Agilent Co. Inc., USA). Mobile phase was consisted of methanol-0.02 M KH_2PO_4 (48:52, v/v), and delivered at a flow rate of 1 mL/min. Chromatographic separation was performed on a Phenomenex ODS₃ column (250 \times 4.6 mm, 5 μm , Torrance, CA, USA), and maintained at 30°C by a column oven. The detector was set at 282 nm for excitation and 328 nm for emission wavelength. The peak area of domperidone (Ad) and propranolol (Ap) were recorded, and the concentration of domperidone was calculated according to the ratio of Ad/Ap. The limit of quantification (LOQ) of the assay was 1 ng/mL, and linearity was obtained for domperidone concentrations ranging from 5 to 100 ng/mL ($R^2 = 0.9978$). The coefficients of variation of the interday and intraday precision of the quality control samples ranged from 6.4% to 11.4% and accuracy ranged from 101 to 117%.

The pharmacokinetic parameters were calculated from the plasma levels by noncompartmental pharmacokinetic analysis using the software package WinNonLin v 5.2 (Pharsight Corporation, Mountain View, CA). The peak plasma concentration (C_{max}) and time to reach peak plasma concentration (T_{max}) was obtained from the visual inspection of the plasma concentration-time curves. The area under the plasma concentration curve (AUC_{0-t}) was determined using the trapezoidal rule up to 24 hours after drug administration.

2.11. The Propulsion Efficacy of Domperidone Hydrogel in Mice. Kunming mice—after 12 hours of fasting—were divided into a Motilium tablet group and a domperidone hydrogel group ($n = 8$). Mice in this two domperidone preparation groups received Motilium tablet (the Motilium tablet was grinded and suspended in distilled water) or domperidone hydrogel by intragastric administration. The dose of domperidone administered to each animal was 5 mg/kg. After 0.5, 1.0, 1.50, 2.0, 2.5, 3.0, 4.0, and 6.0 h administrations, mice received 0.1 mL ink [27]. After 10 min, the mice were killed by cervical vertebral dislocation with their stomachs cut open to collect their intestines. The propulsion efficacy of domperidone in preparations was presented by ink propulsion rate. The ink propulsion rate was calculated by using the formula: ink propulsion rate % = migration distance of ink/the distance from pylorus-duodenum junction to ileocecum \times 100%. The mice ($n = 8$) in control group intragastrically received 0.5 mL physiological saline. The ink propulsion rate was determined according to the procedures outlined above.

2.12. Statistics. Data was presented as the mean \pm standard deviation (SD). One-way analysis of variance (ANOVA) was used to determine significance among groups, after which post hoc tests with the Bonferroni correction were used for comparisons between individual groups. Statistical significance was established at $P < .05$.

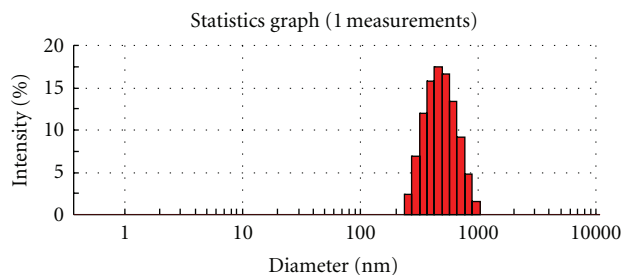


FIGURE 1: The particle size and distribution of domperidone dispersion. The particle size of domperidone dispersion in distilled water (1 mg domperidone dispersion suspended in 10 mL distilled water) was determined by dynamic light scattering (DLS).

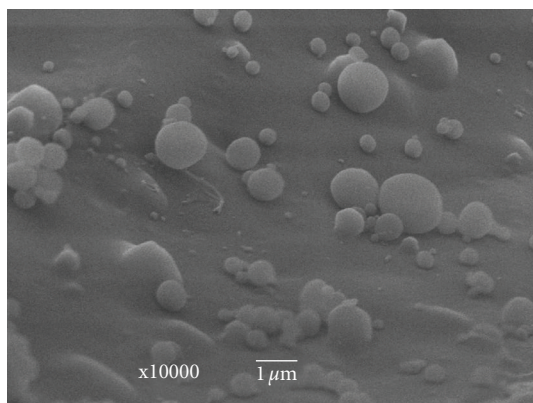


FIGURE 2: Scanning electron micrographs (SEM) photograph of domperidone dispersion.

3. Results

3.1. Particle Size Analysis. The particle size of domperidone dispersion in distilled water was found to be 454.0 nm, as shown in Figure 1. The polydispersity index was 0.115.

3.2. Scanning Electron Microscopy (SEM). The result of SEM imaging of domperidone dispersion, which is shown in Figure 2, indicated that the particles had nanometer-size spherical shapes with a rounded surface appearance and also that no drug crystal was visible.

3.3. Differential Scanning Calorimetry (DSC). The DSC thermograms of raw domperidone, raw PVP, physical mixture, and domperidone dispersion are shown in Figure 3. The curve of raw domperidone showed an endothermic peak at 251.9°C. In case of the physical mixture, the endothermic peak of domperidone was broadened, shrunk, and shifted to 125°C. The complete disappearance of the drug endothermic peak was observed in the domperidone dispersion. This phenomenon can therefore assume that the domperidone in the dispersion was in an amorphous form.

3.4. Powder X-Ray Diffraction (PXRD). The PXRD patterns for raw domperidone, raw PVP, domperidone dispersion,

TABLE 1: Solubility of domperidone in buffer solutions and distilled water (mean \pm SD, $n = 3$). The drug concentration ($\mu\text{g/mL}$) represents its solubility.

pH	Raw domperidone	Domperidone dispersion
1.0	566.8 \pm 50.9	36211.8 \pm 1.3
5.0	243.3 \pm 4.2	3198.4 \pm 21.7
7.0	2.9 \pm 0.33	10.6 \pm 0.27
Distilled water	4.5 \pm 0.3	205.5 \pm 3.7

and the corresponding physical mixture are shown in Figure 4. In the X-ray diffraction spectrum, domperidone exhibited several strong characteristic crystalline peaks at $2\theta = 9.28^\circ, 13.94^\circ, 15.58^\circ, 19.80^\circ,$ and 24.80° in raw domperidone, suggesting that the drug was present as a crystalline material. Some domperidone crystal peaks were still detected in the physical mixtures. In contrast, there were no sharp peaks attributable to the crystalline form in domperidone dispersion, suggesting that domperidone in this dispersion was in an amorphous state. This result confirmed the result obtained from DSC.

3.5. Solubility. The solubility of domperidone in raw domperidone and domperidone dispersion is presented in Table 1. In distilled water, the solubility of domperidone in the dispersion was $205.5 \pm 3.7 \mu\text{g/mL}$, 45.7-fold higher than that of raw domperidone ($4.5 \pm 0.3 \mu\text{g/mL}$). In pH 1, 5 and 7 buffer solution, the solubility of domperidone in dispersion were $36211.8 \pm 1.3, 3198.4 \pm 21.7$ and $10.6 \pm 0.27 \mu\text{g/mL}$, 63.9-, 13.1- and 3.7-fold higher than that of raw domperidone ($566.8 \pm 50.9, 243.3 \pm 4.2,$ and $2.9 \pm 0.33 \mu\text{g/mL}$), respectively.

3.6. Pharmacokinetic Studies of Domperidone Hydrogel in Beagle Dogs. The *in vivo* pharmacokinetic results obtained for the formulation based on domperidone hydrogel were compared with Motilium tablet. Figure 5 showed the average plasma concentration versus time curves of domperidone after oral administration of preparations to beagle dogs at a dose of 10 mg/body. The concentrations of domperidone in hydrogel treatment group, especially in last time points, were remarkable higher than that in tablet treatment group ($P < .05$).

As shown in Table 2, administration of Motilium tablet resulted in AUC_{0-24} values of $382.11 \pm 52.71 \text{ h} \cdot \text{ng/mL}$. When the same dose of domperidone was formulated in hydrogel, the systemic exposure to domperidone was raised significantly as reflected in an AUC_{0-24} of $829.64 \pm 105.09 \text{ h} \cdot \text{ng/mL}$ higher than that from tablet ($P < .01$). In terms of C_{max} , the values from hydrogel group ($70.05 \pm 12.27 \text{ ng/mL}$) were higher than those from tablet group ($56.95 \pm 6.63 \text{ ng/mL}$), however, there was no significant difference between these two groups. Based on a comparison of the T_{max} values, the C_{max} reached time in hydrogel group ($1.17 \pm 0.29 \text{ h}$) was significantly longer as compared to tablet group ($0.44 \pm 0.10 \text{ h}$) ($P < .01$). In addition, the differences

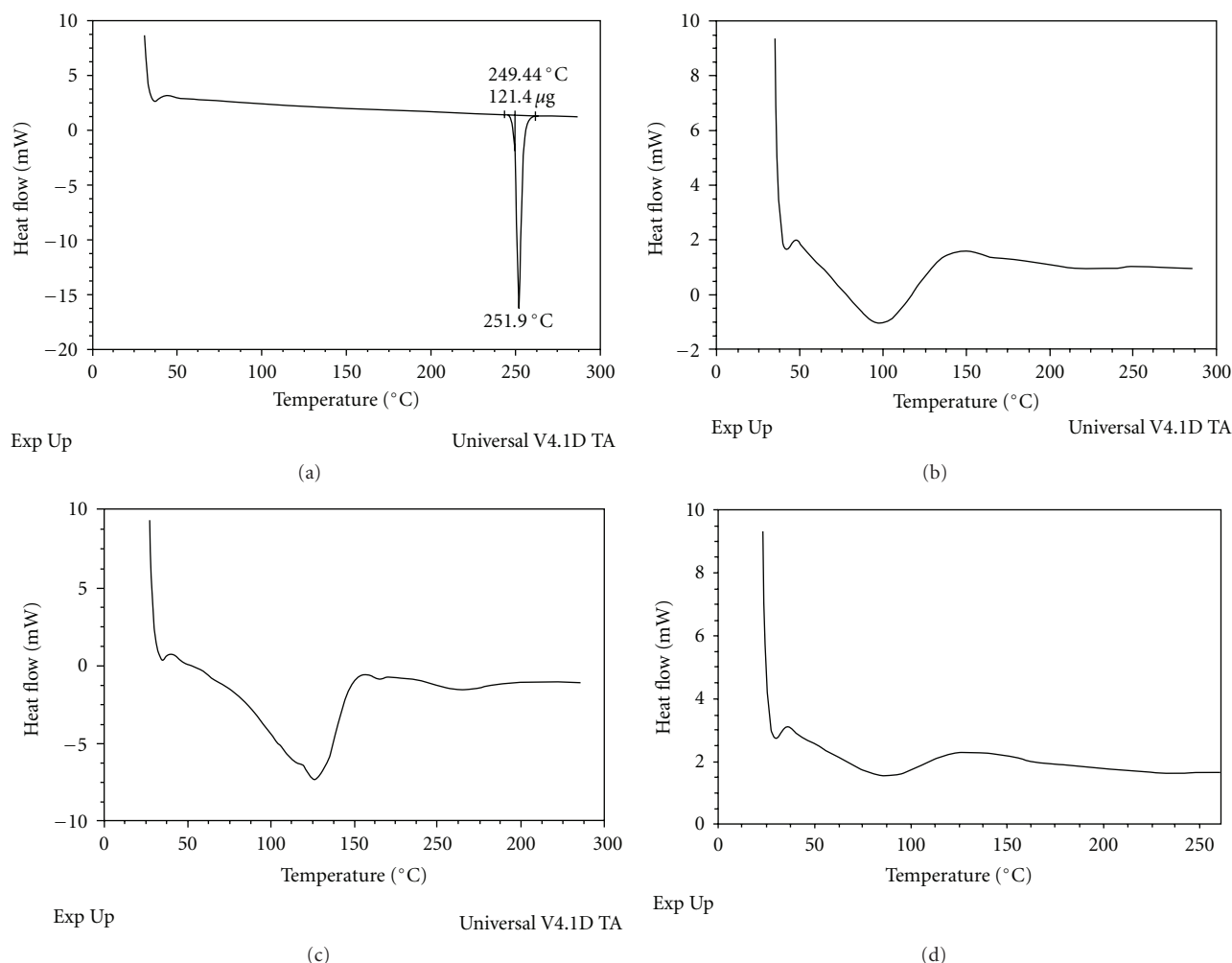


FIGURE 3: Differential scanning calorimetry (DSC) of raw domperidone (1), raw PVP K30 (2), physical mixture of domperidone and PVP K₃₀ (3), and domperidone dispersion (4).

TABLE 2: Selected pharmacokinetic parameters of domperidone after a single administration of Motilium tablet or domperidone hydrogel to beagle dogs at a dose of 10 mg/body ($n = 3$).

Parameter	Units	Motilium tablet	Domperidone hydrogel
T _{max}	h	0.44 ± 0.10	1.17 ± 0.29**
C _{max}	ng/mL	56.95 ± 6.63	70.05 ± 12.27
AUC ₀₋₂₄	h · ng/mL	382.11 ± 52.71	829.64 ± 105.09**
V _z	l/kg	35.16 ± 2.06	17.49 ± 2.17*
Cl	l/h/kg	2.04 ± 0.26	0.93 ± 0.08**
MRT	h	10.04 ± 1.05	10.85 ± 0.49

* $P < .05$ or ** $P < .01$ versus tablet group.

in the values of V_z and Cl between hydrogel group and tablet group ($P < .05$ or $P < .01$) could also be noted.

3.7. The Propulsion Efficacy of Domperidone Hydrogel in Mice. Figure 6 shows the ink propulsion rates of small intestine in mice after they were administered intragastric Motilium tablet, domperidone hydrogel, or physiological

TABLE 3: The ink propulsion rate of the small intestine at peak time or 6 h time point after an intragastric given Motilium tablet or domperidone hydrogel to mice at a dose of 5 mg/kg and the average ink propulsion rate of the small intestine after intragastric given physiological saline to mice. Each point represents mean ± S.D. ($n = 8$).

Ink propulsion rate (%)	Average	Peak time	6 h time point
Physiological saline group	41.9 ± 9.9	/	/
Motilium tablet group	/	57.1 ± 11.5*	38.3 ± 13.2
Domperidone hydrogel group	/	71.5 ± 13.3** ^Δ	58.0 ± 9.1* ^Δ

* $P < .05$, ** $P < .01$ versus physiological saline group.

^Δ $P < .05$ versus tablet group.

saline. The ink propulsion rates in domperidone preparation groups at peak time were significantly higher than that in tablet or physiological saline group ($P < .05$ or $P < .01$),

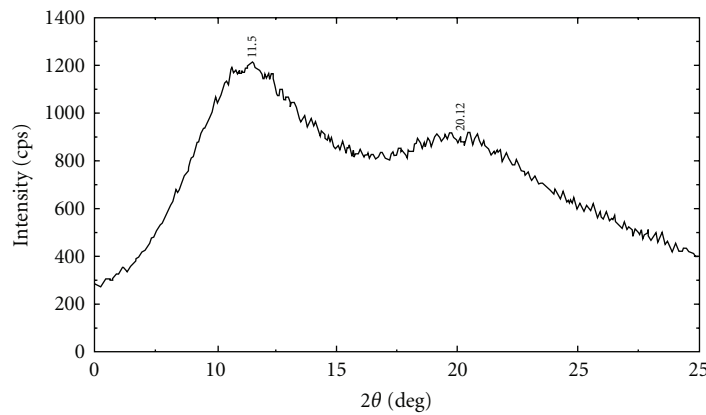
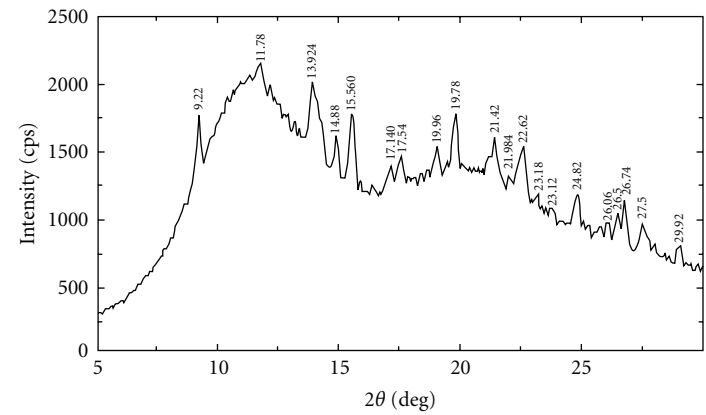
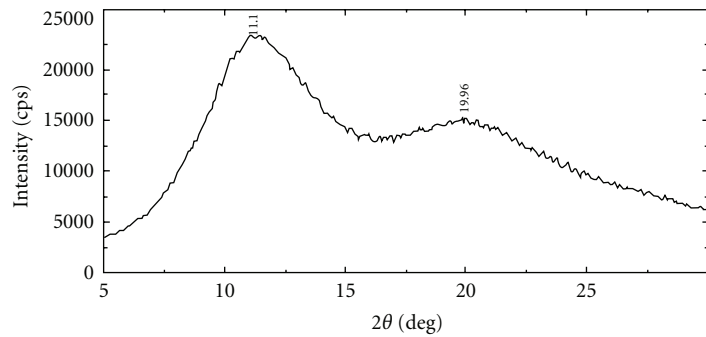
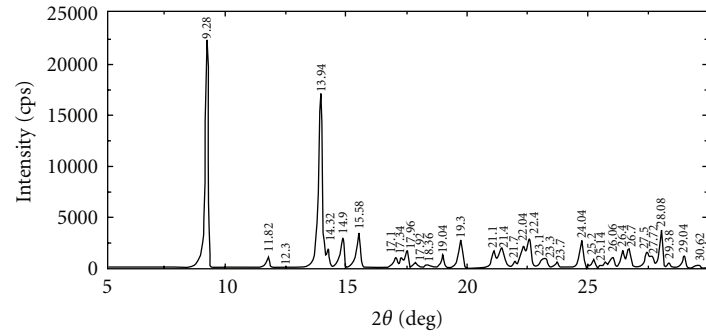


FIGURE 4: Powder X-ray diffractogram (PXRD) of raw domperidone (1); raw PVP K30 (2); physical mixture of domperidone and PVP K30 (3); domperidone dispersion (4).

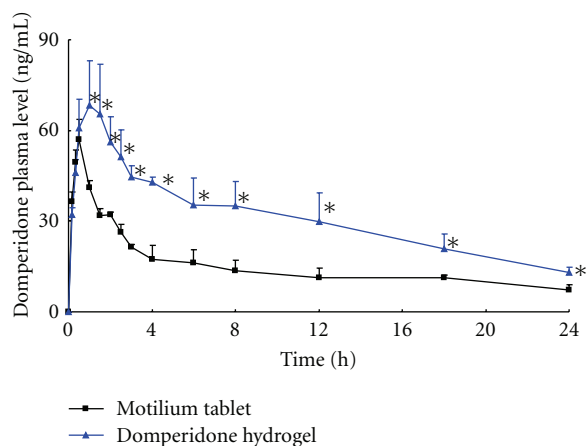


FIGURE 5: Concentration-time profiles of domperidone in plasma after a single oral administration of domperidone hydrogel or Motilium tablet to beagle dogs at a dose of 10 mg/body. Each point represents mean \pm S.D. ($n = 3$). The asterisks indicate a statistically significant difference between domperidone hydrogel group and Motilium tablet group ($P < .05$).

as shown in Table 3. The difference in ink propulsion rates at peak time point between the hydrogel group and tablet group were significant ($P < .05$). The values of ink propulsion rates at 6 h time point in hydrogel group compared with the tablet or physiological saline group were significant higher ($P < .05$), whereas there was no significant difference between the physiological saline group and tablet group (Table 3).

The peak time of ink propulsion rates in domperidone hydrogel group and tablet group was 1.5 and 1 h, respectively. In fact, the values of ink propulsion rates in domperidone hydrogel group at 0.5 h time points, ($60.1 \pm 14.0\%$), was similar with those in tablets group in 1 h time point (at peak time point, ($57.1 \pm 11.5\%$)), indicating that the onset time of propulsion efficacy in hydrogel group was faster than that in tablet group. The propulsion efficacy in the domperidone hydrogel group was sustained at least 6 h; however, it was sustained only 3 h in tablet group, indicating the prolonged propulsion efficacy in hydrogel group compared to that in tablet group.

4. Discussion

In the present study, we prepared domperidone dispersion by evaporation method using PVP as a polymeric crystallization inhibitor. The amorphous domperidone in dispersion was confirmed by DSC and X-ray tests. The particle size of domperidone dispersion in distilled water and the morphology of domperidone dispersion indicated that the domperidone dispersion was in the nanometer size range. The solubility of domperidone in the dispersion in distilled water was found to be 45.7-fold higher than that of raw domperidone. Similar results were also found in pH 1 and 5 buffer solution, 63.9- and 13.1-fold higher than that of raw domperidone. The higher solubility of domperidone in the dispersion would provide a guarantee of enhancing the absorption of domperidone in GIT.

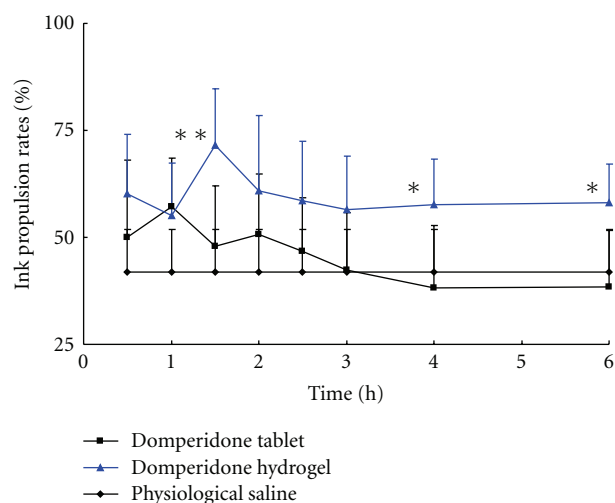


FIGURE 6: Profiles of the ink propulsion rates of the small intestine after intragastric administered Motilium tablet, domperidone hydrogel, or physiological saline to mice. Each point represents mean \pm S.D. ($n = 8$). The dose of domperidone was 5 mg/kg. The asterisks indicate a statistically significant difference between domperidone hydrogel group and physiological saline group ($*P < .05$; $**P < .01$).

The solubility of domperidone in dispersion in pH 7.0 buffer solution was $10.6 \mu\text{g/mL}$. According to the calculation, about 99.9% domperidone dispersion existed as solid nanosized particles in this solution. Therefore, we suggest that almost all of the domperidone dispersion in the Carbopol hydrogels would exist as solid nanosized particles.

Carbopol is a very useful polymer for hydrogel delivery system [28, 29]. The incorporation of nanoparticles with hydrogel would increase its adhesive properties to GIT. This is a benefit for enhancing drug oral bioavailability. In addition, Carbopol hydrogel has the characteristic of a higher viscosity, which could limit the sedimentation of the contained particles. Excellent long-term stability of the hydrogel/drug nanoparticles system has been observed by Müller and Jacobs [25]. Even so, the stability of domperidone dispersion existed as nanosize particles in the Carbopol hydrogel should be further investigate in future.

The physical properties of the Carbopol hydrogels are extremely sensitive to the presence and concentration of additives [30]. It has been reported that for Carbopol hydrogels with 0.05 and 0.1% of PVP, the behavior is similar to that of single Carbopol formulation, their pseudoplastic non-Newtonian character being maintained [21]. Therefore, in the present research, the addition of PVP does not substantially modify the rheological behavior of the Carbopol hydrogels.

Considering the advantages of amorphous dispersion and adhesive properties of hydrogel to the GIT wall, we incorporated domperidone dispersion with Carbopol hydrogel to prepare a novel domperidone hydrogel. The *in vivo* pharmacokinetic evaluation of domperidone hydrogel in dogs was investigated. The positive pharmacokinetic results

showed that the AUC in domperidone hydrogel was 2.2-fold higher than that in Motilium tablet. The concentrations of domperidone in hydrogel treatment group, especially in last time points, were remarkable higher than that in tablet treatment group ($P < .01$). The results of *in vivo* pharmacodynamic evaluation in mice indicated that the higher and prolonged propulsion efficacy was observed in the domperidone hydrogel group compared to that in tablet group. We suggested that the particle size of domperidone reduction to a nanometer range and the conversion of crystalline drug to amorphous state in dispersion resulted in an increase of dissolution velocity and degree of the drug in the GIT, especially in gastric fluid. Therefore, the rapid and complete absorption from the gastrointestinal tract would lead to improving the bioavailability and the propulsion efficacy of domperidone in hydrogel group. Another reason for the *in vivo* results was the role of Carbopol hydrogel which prolonged the residence and the contact time of domperidone in GIT. The sustained release behavior in domperidone hydrogel group was confirmed by our pharmacokinetic and pharmacodynamic results.

5. Conclusion

The characterization of domperidone dispersion demonstrated that the prepared domperidone dispersion were amorphous and in the nanometer size range. Solubility of domperidone in the dispersion showed a marked increase. The domperidone hydrogel was prepared by directly incorporating the domperidone dispersion in Carbopol hydrogel. As a result of the mucoadhesive properties and improved solubility, a statistically significant improvement in bioavailability and prolonged propulsion efficacy of domperidone in hydrogel group were observed compared to that in Motilium tablet group in beagle dogs and mice. In addition, these results indicate that dispersion incorporating with hydrogel can be an effective tool to improve the bioavailability of poor water soluble drugs.

Acknowledgment

The authors gratefully acknowledge the financial support from the National Basic Research Program of China (973 Program), and the project number is 2009CB930300.

References

- [1] N. Ahmad, J. Keith-Ferris, E. Gooden, and T. Abell, "Making a case for domperidone in the treatment of gastrointestinal motility disorders," *Current Opinion in Pharmacology*, vol. 6, no. 6, pp. 571–576, 2006.
- [2] M. S. Nagarsenker, S. D. Garad, and G. Ramprakash, "Design, optimization and evaluation of domperidone coevaporates," *Journal of Controlled Release*, vol. 63, no. 1-2, pp. 31–39, 2000.
- [3] S. C. Reddymasu, I. Soykan, and R. W. McCallum, "Domperidone: review of pharmacology and clinical applications in gastroenterology," *American Journal of Gastroenterology*, vol. 102, no. 9, pp. 2036–2045, 2007.
- [4] S. T. Prajapati, L. D. Patel, and D. M. Patel, "Gastric floating matrix tablets: design and optimization using combination of polymers," *Acta Pharmaceutica*, vol. 58, no. 2, pp. 221–229, 2008.
- [5] B. C. Hancock and M. Parks, "What is the true solubility advantage for amorphous pharmaceuticals?" *Pharmaceutical Research*, vol. 17, no. 4, pp. 397–404, 2000.
- [6] S. B. Murdande, M. J. Pikal, R. M. Shanker, and R. H. Bogner, "Solubility advantage of amorphous pharmaceuticals: I. a thermodynamic analysis," *Journal of Pharmaceutical Sciences*, vol. 99, no. 3, pp. 1254–1264, 2010.
- [7] P. Gupta, G. Chawla, and A. K. Bansal, "Physical stability and solubility advantage from amorphous celecoxib: the role of thermodynamic quantities and molecular mobility," *Mol Pharm*, vol. 1, no. 6, pp. 406–413, 2004.
- [8] K. A. Overhoff, J. T. McConville, W. Yang, K. P. Johnston, J. I. Peters, and R. O. Williams III, "Effect of stabilizer on the maximum degree and extent of supersaturation and oral absorption of tacrolimus made by ultra-rapid freezing," *Pharmaceutical Research*, vol. 25, no. 1, pp. 167–175, 2008.
- [9] S. L. Raghavan, A. Trividic, A. F. Davis, and J. Hadgraft, "Effect of cellulose polymers on supersaturation and *in vitro* membrane transport of hydrocortisone acetate," *International Journal of Pharmaceutics*, vol. 193, no. 2, pp. 231–237, 2000.
- [10] D. Hörter and J. B. Dressman, "Influence of physicochemical properties on dissolution of drugs in the gastrointestinal tract," *Advanced Drug Delivery Reviews*, vol. 46, no. 1-3, pp. 75–87, 2001.
- [11] J. C. DiNunzio, D. A. Miller, W. Yang, J. W. McGinity, and R. O. Williams III, "Amorphous compositions using concentration enhancing polymers for improved bioavailability of itraconazole," *Molecular Pharmaceutics*, vol. 5, no. 6, pp. 968–980, 2008.
- [12] D. A. Miller, J. C. DiNunzio, W. Yang, J. W. McGinity, and R. O. Williams III, "Enhanced *in vivo* absorption of itraconazole via stabilization of supersaturation following acidic-to-neutral pH transition," *Drug Development and Industrial Pharmacy*, vol. 34, no. 8, pp. 890–902, 2008.
- [13] D. A. Miller, J. C. DiNunzio, W. Yang, J. W. McGinity, and R. O. Williams III, "Targeted intestinal delivery of supersaturated itraconazole for improved oral absorption," *Pharmaceutical Research*, vol. 25, no. 6, pp. 1450–1459, 2008.
- [14] K. A. Overhoff, A. Moreno, D. A. Miller, K. P. Johnston, and R. O. Williams III, "Solid dispersions of itraconazole and enteric polymers made by ultra-rapid freezing," *International Journal of Pharmaceutics*, vol. 336, no. 1, pp. 122–132, 2007.
- [15] J. M. Vaughn, J. T. McConville, D. Burgess et al., "Single dose and multiple dose studies of itraconazole nanoparticles," *European Journal of Pharmaceutics and Biopharmaceutics*, vol. 63, no. 2, pp. 95–102, 2006.
- [16] M. E. Matteucci, B. K. Brettmann, T. L. Rogers, E. J. Elder, R. O. Williams III, and K. P. Johnston, "Design of potent amorphous drug nanoparticles for rapid generation of highly supersaturated media," *Molecular Pharmaceutics*, vol. 4, no. 5, pp. 782–793, 2007.
- [17] M. E. Matteucci, J. C. Paguio, M. A. Miller, R. O. Williams III, and K. P. Johnston, "Flocculated amorphous nanoparticles for highly supersaturated solutions," *Pharmaceutical Research*, vol. 25, no. 11, pp. 2477–2487, 2008.
- [18] M. E. Matteucci, J. C. Paguio, M. A. Miller, R. O. Williams III, and K. P. Johnston, "Highly supersaturated solutions from dissolution of amorphous itraconazole microparticles at pH 6.8," *Molecular Pharmaceutics*, vol. 6, no. 2, pp. 375–385, 2009.

- [19] S. Janssens, S. Nagels, H. N. D. Armas, W. D'Autry, A. Van Schepdael, and G. Van den Mooter, "Formulation and characterization of ternary solid dispersions made up of Itraconazole and two excipients, TPGS 1000 and PVPVA 64, that were selected based on a supersaturation screening study," *European Journal of Pharmaceutics and Biopharmaceutics*, vol. 69, no. 1, pp. 158–166, 2008.
- [20] E. Karavas, E. Georganakakis, M. P. Sigalas, K. Avgoustakis, and D. Bikiaris, "Investigation of the release mechanism of a sparingly water-soluble drug from solid dispersions in hydrophilic carriers based on physical state of drug, particle size distribution and drug-polymer interactions," *European Journal of Pharmaceutics and Biopharmaceutics*, vol. 66, no. 3, pp. 334–347, 2007.
- [21] T. Sanz Taberner, A. Martín-Villodre, J. M. Pla-Delfina, and J. V. Herráez, "Consistency of Carbopol 971-P NF gels and influence of soluble and cross-linked PVP," *International Journal of Pharmaceutics*, vol. 233, no. 1-2, pp. 43–50, 2002.
- [22] G. Bonacucina, S. Martelli, and G. F. Palmieri, "Rheological, mucoadhesive and release properties of Carbopol gels in hydrophilic cosolvents," *International Journal of Pharmaceutics*, vol. 282, no. 1-2, pp. 115–130, 2004.
- [23] G. Bonacucina, M. Cespi, M. Misici-Falzi, and G. F. Palmieri, "Rheological, adhesive and release characterisation of semisolid Carbopol/tetraglycol systems," *International Journal of Pharmaceutics*, vol. 307, no. 2, pp. 129–140, 2006.
- [24] R. A-sasutjarit, A. Sirivat, and P. Vayumhasuwan, "Viscoelastic properties of Carbopol 940 gels and their relationships to piroxicam diffusion coefficients in gel bases," *Pharmaceutical Research*, vol. 22, no. 12, pp. 2134–2140, 2005.
- [25] R. H. Müller and C. Jacobs, "Buparvaquone mucoadhesive nanosuspension: preparation, optimisation and long-term stability," *International Journal of Pharmaceutics*, vol. 237, no. 1-2, pp. 151–161, 2002.
- [26] M. Kobylińska and K. Kobylińska, "High-performance liquid chromatographic analysis for the determination of domperidone in human plasma," *Journal of Chromatography B*, vol. 744, no. 1, pp. 207–212, 2000.
- [27] J. Liu, R. Wan, X. F. Xu et al., "Effect of Lianshu preparation on lipopolysaccharide-induced diarrhea in rats," *World Journal of Gastroenterology*, vol. 15, no. 16, pp. 2009–2015, 2009.
- [28] A. K. Singla, M. Chawla, and A. Singh, "Potential applications of carbomer in oral mucoadhesive controlled drug delivery system: a review," *Drug Development and Industrial Pharmacy*, vol. 26, no. 9, pp. 913–924, 2000.
- [29] R. Barreiro-Iglesias, C. Alvarez-Lorenzo, and A. Concheiro, "Incorporation of small quantities of surfactants as a way to improve the rheological and diffusional behavior of carbopol gels," *Journal of Controlled Release*, vol. 77, no. 1-2, pp. 59–75, 2001.
- [30] T. Ozeki, H. Yuasa, and Y. Kanaya, "Controlled release from solid dispersion composed of poly(ethylene oxide)-Carbopol interpolymers complex with various cross-linking degrees of Carbopol," *Journal of Controlled Release*, vol. 63, no. 3, pp. 287–295, 2000.