




Article

Morphology-Dependent Electrochemical Sensing Properties of Iron Oxide-Graphene Oxide Nanohybrids for Dopamine and Uric Acid

Zhaotian Cai ^{1,†}, Yabing Ye ^{1,†}, Xuan Wan ¹, Jun Liu ¹, Shihui Yang ¹, Yonghui Xia ²,
Guangli Li ^{1,*}  and Quanguo He ^{1,*}

¹ Hunan Key Laboratory of Biomedical Nanomaterials and Devices, College of Life Sciences and Chemistry, Hunan University of Technology, Zhuzhou 412007, China; caizhaotian1998@163.com (Z.C.); yyb980501@163.com (Y.Y.); wanxuan1111@163.com (X.W.); liu.jun.1015@163.com (J.L.); yangshihui0522@163.com (S.Y.)

² Zhuzhou Institute for Food and Drug Control, Zhuzhou 412000, China; Sunnyxia0710@163.com

* Correspondence: guangli010@hut.edu.cn (G.L.); hequanguo@hut.edu.cn (Q.H.);
Tel.: +86-0731-2218-3382 (G.L. & Q.H.)

† These authors contributed equally to this work.

Received: 4 May 2019; Accepted: 20 May 2019; Published: 1 June 2019



Abstract: Various morphologies of iron oxide nanoparticles (Fe₂O₃ NPs), including cubic, rhombohedral and discal shapes were synthesized by a facile meta-ion mediated hydrothermal route. To further improve the electrochemical sensing properties, discal Fe₂O₃ NPs with the highest electrocatalytic activity were coupled with graphene oxide (GO) nanosheets. The surface morphology, microstructures and electrochemical properties of the obtained Fe₂O₃ NPs and Fe₂O₃/GO nanohybrids were characterized by scanning electron microscopy (SEM), X-ray diffraction (XRD), cyclic voltammetry (CV) and electrochemical impedance spectroscopy (EIS) techniques. As expected, the electrochemical performances were found to be highly related to morphology. The discal Fe₂O₃ NPs coupled with GO showed remarkable electrocatalytic activity toward the oxidation of dopamine (DA) and uric acid (UA), due to their excellent synergistic effect. The electrochemical responses of both DA and UA were linear to their concentrations in the ranges of 0.02–10 μM and 10–100 μM, with very low limits of detection (LOD) of 3.2 nM and 2.5 nM for DA and UA, respectively. Moreover, the d-Fe₂O₃/GO nanohybrids showed good selectivity and reproducibility. The proposed d-Fe₂O₃/GO/GCE realized the simultaneous detection of DA and UA in human serum and urine samples with satisfactory recoveries.

Keywords: morphology-dependent; α-Fe₂O₃ nanoparticles; GO; uric acid; dopamine; voltammetric detection

1. Introduction

Dopamine (DA) and uric acid (UA) usually coexist in the serum and extracellular fluids of the central nervous system and play a significant role in regulating human metabolism activity [1]. As an indispensable catecholamine neurotransmitter, DA plays critical roles in regulating the function of the cardiovascular and central nervous systems, as well as maintaining emotional control and hormonal balance [2]. Abnormal levels of DA can lead to various neurological disorders such as schizophrenia, Parkinson's and Alzheimer's disease [3–5]. Therefore, the precise detection of the DA level in physiological fluids is essential for the early diagnosis of these neurological disorders. However, the rapid and reliable detection of DA in physiological samples remains critical and challenging due to the low DA concentration in the extracellular matrix (usually in the range of 0.01–1 μM) and its susceptibility to interference from endogenous substances such as UA and ascorbic acid (AA). Uric

acid is another crucial biomolecule in physiological fluids and is often regarded as the end-product of purine metabolism in the human body [6]. For a healthy individual, the UA concentration is generally in the range of 4.1 ± 8.8 mg/100 mL [7]. The dysfunction of UA in bodily fluids likely causes several diseases, including gout, pneumonia and hyperuricemia [8]. As stated, both DA and UA are regarded as important biomolecules for the regulation of human metabolic activity. Thus, determining the concentration of DA and UA in biological matrices (i.e., human urine, serum) can provide valuable clues for healthcare and disease diagnosis. Since DA and UA usually coexist in physiological fluids, it is of the utmost importance to propose a highly efficient technique for the simultaneous determination of DA and UA.

To date, several analytical techniques have been proposed for the detection of DA and UA, including, but not limited to, high performance liquid chromatography [9,10], fluorescent [11], spectrophotometry [12], electrogenerated chemiluminescent [13] and surface plasmon resonance [14] etc. Although quite reliable, these techniques usually involve tedious and time-consuming analytical procedures that require expensive equipment, well-trained technical personnel or a large quantity of toxic solvents [15]. Compared with other techniques, the electroanalytical techniques are more suitable for sensing DA and UA because of their low price, fast response, facile operation and excellent anti-interfering ability [16–18]. Owing to the considerable superiorities including cost-effectiveness, rapidness, convenience and high efficiency, electroanalytical methods have drawn increasing attention for the detection of small biomolecules, food additives and contaminants [19–24]. DA and UA are electroactive species whose redox processes can be quantitatively detected by electroanalytical techniques. However, it becomes a great challenge to simultaneously detect DA and UA on bare electrodes due to the fouling effect that occurs during the oxidation [7] and cross-interferences as a result of similar oxidation potentials [25]. To resolve this problem, nanostructured materials were employed to achieve high sensitivity and prevent overlapping of the oxidation peaks [25]. In recent years, much effort has been devoted to developing promising alternatives as sensing materials for the simultaneous detection of DA and UA, including noble metal nanoparticles [25], metal oxides nanocomposites [26], alloyed nanoparticles [27], polymer films [28,29], and nanocarbon materials [30–32] etc.

Iron oxide (Fe_2O_3) has become one of the most versatile transition metal oxides not only due to low cost, more abundant, good biocompatibility and excellent electrochemical performances, but also for its widespread applications [33–38]. In particular, $\alpha\text{-Fe}_2\text{O}_3$ nanoparticles ($\alpha\text{-Fe}_2\text{O}_3$ NPs) have been considered as the most promising modifying material, because of the variable valence state of iron oxides that can be recovered in situ via electrochemical reducing or oxidizing during the sensing process, thus triggering the heterogeneous redox of the target analytes [39]. As far as we know, various morphologies of $\alpha\text{-Fe}_2\text{O}_3$ NPs have been made available in previous reports, including wire [40], rod [41,42], tube [41], sphere [43,44], flower [45], spindle [44], cubic [44,46–49], rhombohedral [46–48], discal [47], and shuttle [50]. Many studies demonstrate that the morphologies of nanostructured $\alpha\text{-Fe}_2\text{O}_3$ have a significant impact on optical, magnetic, photocatalytic and electrochemical properties [46,47,51,52]. However, the morphology-dependent electrochemical sensing performances with respect to small biomolecules have rarely been investigated. Hence, it is essential to explore the morphology-dependent sensing properties of different $\alpha\text{-Fe}_2\text{O}_3$ NPs. Unfortunately, the electrochemical sensing performances of pure $\alpha\text{-Fe}_2\text{O}_3$ NPs modified electrodes are relatively poor probably because of their poor electrical conductivity and dispersibility [37,53,54]. To address this issue, iron oxides were often used in a composite with graphene for the detection of DA. For example, nitrogen and sulfur dual doped graphene-supported Fe_2O_3 (NSG- Fe_2O_3) has been utilized for the electrochemical detection of DA in the presence of AA, with a wide linear response range (0.3–210 μM) and low LOD (0.035 μM) [55]. However, the procedure for the doping of nitrogen and sulfur is very complicated. Moreover, the simultaneous detection of DA and UA is not clear for this nanocomposite. As an important derivant of graphene, graphene oxide (GO) usually works as a conductive component to enhance the electron transfer between electrode surface and target analytes [18,19]. Indeed, there are abundant hydrophilic oxygen-containing functional groups (OxFGs) presented on the hydrophobic basal planes of GO, which

can behave like an amphiphilic surfactant to improve the dispersion of α -Fe₂O₃ NPs [56]. As far as we know, α -Fe₂O₃/GO nanocomposites have rarely reported for the simultaneous detection of DA and UA.

Herein, α -Fe₂O₃ NPs with various morphologies including cubic, thorhombic and discal shapes were synthesized by a facile meta-ion mediated hydrothermal route then composite with GO nanosheets. The electrocatalytic activities of DA and UA at Fe₂O₃/GO nanohybrids decorated glassy carbon electrodes (Fe₂O₃/GO/GCE) were measured in this work. The electrochemical measurements exhibited that the discal Fe₂O₃ NPs had the most remarkable electrochemical response toward the simultaneous detection of DA and UA, attributing to the more surface defects and rougher surface. After further coupled with GO, the discal α -Fe₂O₃ NPs/GO nanohybrids (d-Fe₂O₃/GO) showed superior electrochemical sensing performances toward DA and UA, due to the notable synergistic effect from d-Fe₂O₃ and GO. Therefore, a novel and ultrasensitive electrochemical sensor based on d-Fe₂O₃/GO nanohybrids was proposed for the simultaneous detection of DA and UA.

2. Materials and Methods

2.1. Chemicals and Solutions

Dopamine (DA), uric acid (UA), Iron (III) nitrate nonahydrate (Fe(NO₃)₃·9H₂O), cupric acetate anhydrous (Cu(Ac)₂), Zinc acetate (Zn(Ac)₂·2H₂O), aluminum acetate (Al(Ac)₃), disodium hydrogen phosphate dodecahydrate (Na₂HPO₄·12H₂O) and Sodium dihydrogen phosphate dihydrate (NaH₂PO₄·2H₂O) were purchased from Aladdin Reagents Co., Ltd. (Shanghai, China). Graphite powder, potassium permanganate (KMnO₄), hydrogen peroxide (H₂O₂, 30%), sodium nitrate (NaNO₃), potassium ferricyanide (K₃[Fe(CN)₆]), potassium ferrocyanide (K₄[Fe(CN)₆]), ammonia (NH₃·H₂O), sodium hydrate (NaOH), concentrated hydrochloric acid (HCl, 37%), concentrated sulfuric acid (H₂SO₄, 98%) and absolute ethanol (CH₃CH₂OH) were supplied by Sinopharm Chemical Reagent Co. Ltd. (Shanghai, China). All chemicals were analytically pure and directly used as received. Human serum samples were provided by Zhuzhou People's Hospital (Zhuzhou, China). The stock solutions of DA and UA (1 mM) were prepared by dissolving appropriate amount of DA and UA in 500 mL 0.1 M PBS. Then lower concentration series of the standard solution were obtained by appropriately diluting the stock solution with 0.1 M PBS. Deionized water (DI water, 18.2 M Ω) was used in all the experiments.

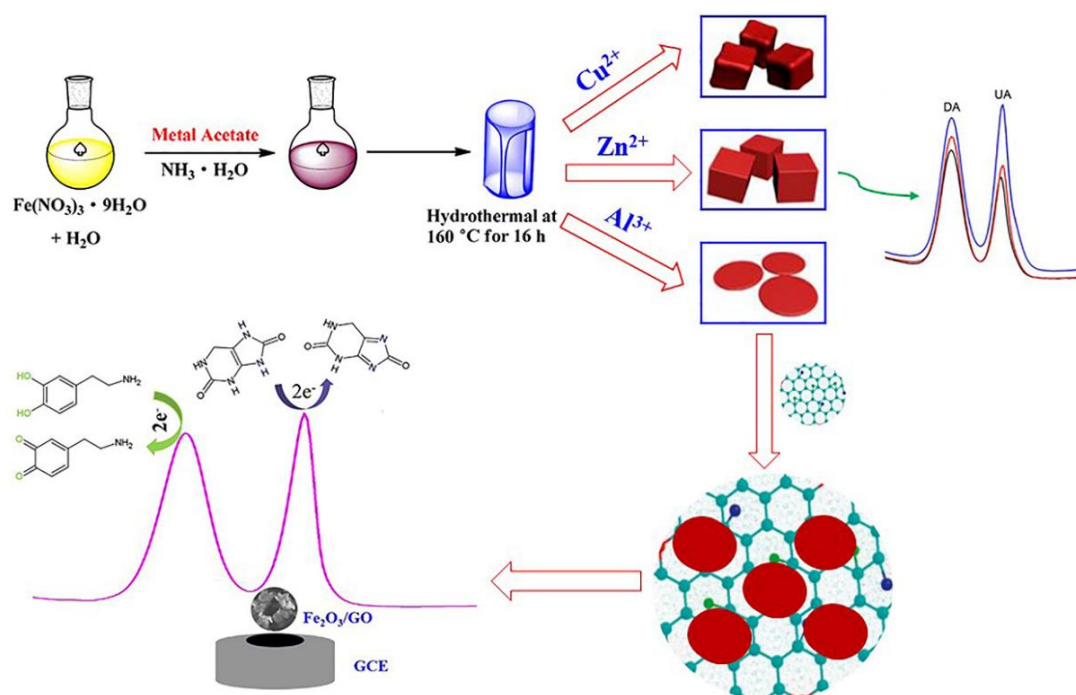
2.2. Apparatus

All the electrochemical measurements were performed on a CHI 760E electrochemical workstation (Chenhua Instrument Inc., Shanghai, China). Surface morphologies and crystalline structure of α -Fe₂O₃ NPs, and Fe₂O₃/GO were investigated by scanning electron microscopy (SEM) and powder X-ray diffractometry (XRD), respectively. SEM images were recorded on a cold field-emission SEM (Hitachi S-4800, Tokyo, Japan) at an accelerating voltage of 5.0 kV. The XRD patterns of α -Fe₂O₃ NPs was recorded using a powder X-ray diffractometer system (PANalytical, Holland) with monochromatized Cu K α radiation ($\lambda = 0.1542$ nm) operating at 40 kV and 40 mA. The patterns were collected in a 2 θ range from 10° to 80° with a scanning step of 0.02° 2 θ s⁻¹. A digital precision pH meter (Leici instrument Inc., Shanghai, China) was used to measure solution pH.

2.3. Synthesis of Discal, Thorhombic, and Cubic α -Fe₂O₃ NPs

Referring to previous reports [46–48], three types of α -Fe₂O₃ NP_S were synthesized by a meta-ion mediated hydrothermal route (Scheme 1). In briefly, 0.808 g of Fe(NO₃)₃·9H₂O was adequately dissolved into 10 mL of DI water under magnetic stirring, and then 1 mM of acetate precursor was added to the above solution. After 15 min of stirring, 10 mL NH₃·H₂O was added and continuously stirring for another 15 min. Next, the mixture was poured into a 50 mL Teflon-lined stainless-steel autoclave and reacted at 160 °C for 16 h. Subsequently, the autoclave was naturally cooled down to room temperature. Finally, the resultant α -Fe₂O₃ product was alternately washed three times

with absolute alcohol and DI water, and allowed to dry under vacuum at 60 °C for 12 h. Herein, cupric acetate, zinc acetate, and aluminum acetate were separately used as acetate precursor to obtain thorhombic, cubic and discal α - Fe_2O_3 NPs.



Scheme 1. The schematic illustration of meta-ion mediated hydrothermal route for the synthesis of discal, thorhombic, and cubic α - Fe_2O_3 NPs and possible mechanism for the electrochemical sensing of DA and UA at the d- Fe_2O_3 /GO/GCE.

2.4. Preparation of Fe_2O_3 /GO Composite

GO was synthesized by a slightly modified Hummer's method according to our earlier reports [20,23,24]. 10 mg GO was delaminated and dispersed in the 10 mL DI water under ultrasonication for 2 h to form 1 mg/mL GO dispersion. Then one aliquot of as-obtained α - Fe_2O_3 products was added into five aliquots of GO dispersion (1 mg/mL), and then ultrasonicated for 0.5 h to form uniform α - Fe_2O_3 /GO dispersion.

2.5. Fabrication of Fe_2O_3 /GO/GCE

At first, bare GCE (ca. 0.0707 cm^2) was carefully polished to mirror-like with 0.3 μm and 0.05 μm fine alumina slurry. Then the polished GCE was alternately washed by absolute ethanol and DI water several times and allowed to dry under an infrared lamp. The Fe_2O_3 /GO/GCE was prepared by a simple drop-casting method. More specifically, 5 μL Fe_2O_3 /GO dispersion was carefully dropped and coated on the GCE surface with a micropipette, then dried with an infrared lamp to form sensing film. For comparison, the discal, thorhombic, and cubic α - Fe_2O_3 NPs decorated GCEs (d- Fe_2O_3 /GCE, t- Fe_2O_3 /GCE, c- Fe_2O_3 /GCE) and GO decorated GCE (GO/GCE) were also fabricated by similar procedure.

2.6. Electrochemical Measurements

The electrochemical behaviors of various decorated electrodes were measured by cyclic voltammetry (CV) and electrochemical impedance spectroscopy (EIS) in the 0.1 M PBS (pH 7.0) containing 0.5 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ as redox probe solution. EIS was measured at the frequency range from 100 kHz to 0.1 Hz at open circuit potential with 5 mV amplitude, using a redox couple of 0.5 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ (1:1) in 0.1 M KCl as an electrochemical probe. The electrochemical responses

of 10 μM DA and UA (1:1) mixture standard solution at different electrodes were recorded by CV. Differential pulse voltammetry (DPV) was used for the individual and simultaneous detection of DA and UA. A conventional three-electrode assembly was immersed into a 10 mL electrochemical cell for electrochemical measurements and detections, consisting of a bare or modified GCE as the working electrode, a saturated calomel electrode (SCE) as the reference electrode, and a platinum wire as auxiliary electrode, respectively. To increase response peak current, a suitable accumulation period was applied before CV and DPV measurements. DPV was performed from 0 V to 0.8 V, with step potential of 4 mV, the amplitude of 50 mV and pulse width of 0.06 s and pulse period of 0.5 s, respectively. 0.1 M PBS was used as the supporting electrolytes unless otherwise specified. All the electrochemical measurements were performed at 25 $^{\circ}\text{C}$.

3. Results and Discussions

3.1. Morphology-Dependent Electrochemical Sensing of $\alpha\text{-Fe}_2\text{O}_3$ NPs

The schematic diagram of the preparation of the $\alpha\text{-Fe}_2\text{O}_3$ NPs is shown in Scheme 1. The $\alpha\text{-Fe}_2\text{O}_3$ NPs with cubic ($c\text{-Fe}_2\text{O}_3$ NPs), discal ($d\text{-Fe}_2\text{O}_3$ NPs), and throrhombic ($t\text{-Fe}_2\text{O}_3$ NPs) shapes were prepared via different metal-ion mediated hydrothermal treatment [46–48]. The $\alpha\text{-Fe}_2\text{O}_3$ NPs are produced as cubic, discal and throrhombic shapes, due to the addition of Zn^{2+} , Al^{3+} , and Cu^{2+} ions, respectively. Figure 1A–C shows the SEM images of as-obtained $\alpha\text{-Fe}_2\text{O}_3$ NPs. Clearly, three $\alpha\text{-Fe}_2\text{O}_3$ NPs with uniform cubic, throrhombic and discal shapes are observed, suggesting uniform cubic, throrhombic and discal shapes were successfully prepared. The crystalline structures of $\alpha\text{-Fe}_2\text{O}_3$ NPs with three distinct morphologies were further investigated by XRD. As presented in Figure 2, the diffraction peaks in all the patterns can be well assigned to the rhombohedral phase of hematite (JCPDS PDF# 33-0664) [46]. Moreover, no apparent diffraction peaks relating to CuFe_2O_4 , ZnFe_2O_4 and AlFeO_3 can be found, demonstrating the crystalline structures of the $\alpha\text{-Fe}_2\text{O}_3$ NPs are not altered by the addition of Cu^{2+} , Zn^{2+} and Al^{3+} ions.

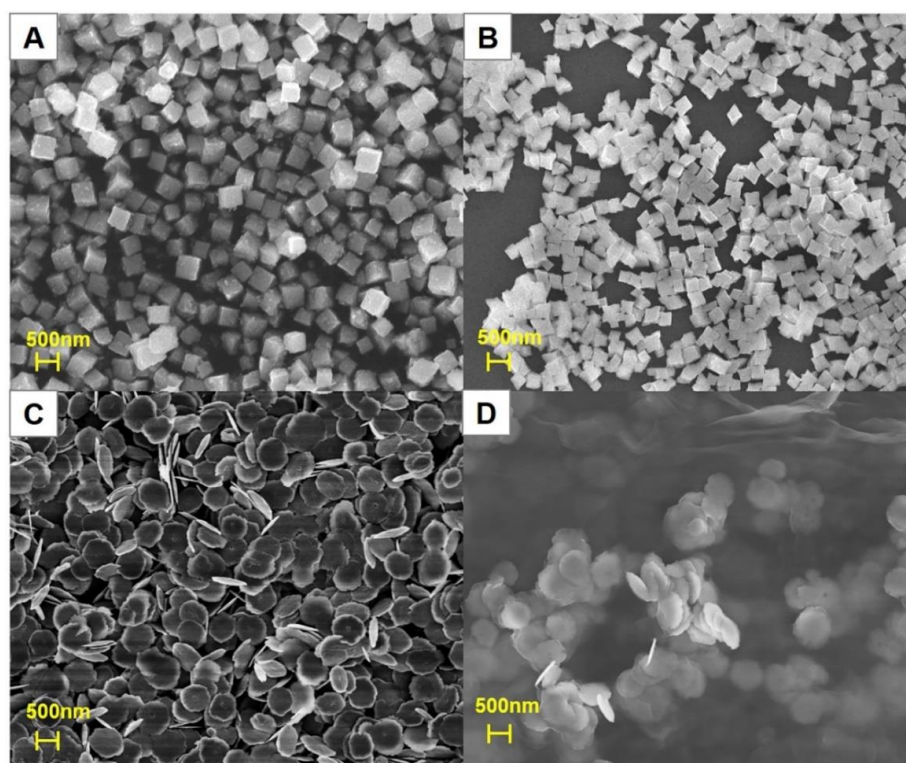


Figure 1. Scanning electron microscopy (SEM) images of $\alpha\text{-Fe}_2\text{O}_3$ NPs with cubic (A), throrhombic (B) and discal (C) morphology, discal $\alpha\text{-Fe}_2\text{O}_3$ NPs/GO nano hybrid (D).

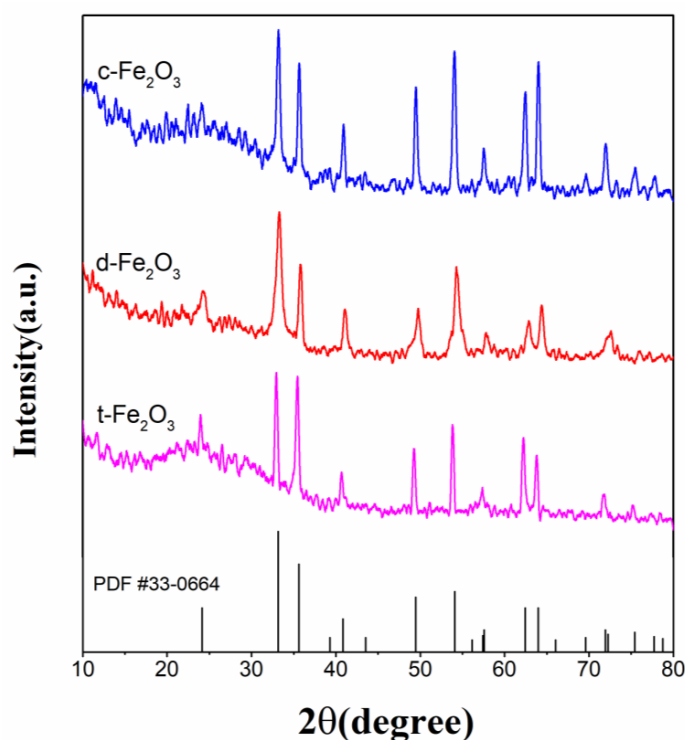


Figure 2. X-ray diffraction (XRD) patterns of α -Fe₂O₃ NPs with cubic (c-Fe₂O₃), discal (d-Fe₂O₃), and thorhombic (t-Fe₂O₃) morphologies.

For comparison purposes, α -Fe₂O₃ NPs with various morphologies were utilized for the simultaneous detection of 10 μ M DA and UA in 0.1 M PBS through CV and DPV technique, and the results are shown in Figure 3A,B, respectively. On all the electrodes, two anodic peaks for DA and UA are independent and evident (Figure 3A), suggesting high selectivity. However, a very small cathodic peaks relating to UA are observed on all the electrode at reverse scanning, demonstrating the reversibility of UA redox is very poor. Note that a pair of redox peaks can be observed on all the electrodes with I_{pa}/I_{pc} ranging from 1.08 to 1.39, indicating that DA undergoes a quasi-reversible electrode process. The increased anodic peak heights in the CVs indicates enhanced electrocatalytic activity. Among the three morphologies of α -Fe₂O₃ NPs modified electrodes, d-Fe₂O₃/GCE exhibits highest electrocatalytic activity toward DA and UA, with well-shaped anodic peaks ($I_{pa(DA)} = 0.1764 \mu\text{A}$, $I_{pc(UA)} = 0.6626 \mu\text{A}$) appear at 0.238 and 0.395 V for DA and UA, respectively. Compared to c-Fe₂O₃/GCE and t-Fe₂O₃/GCE, the anodic peak current for DA at d-Fe₂O₃/GCE increases by 65.8% and 30.0% and the anodic peak current for UA increases by 177% and 73.1%, respectively. Liu et al. systematically compared the photocatalytic activity among cubic, discal and thorhombic α -Fe₂O₃ NPs, d-Fe₂O₃ NPs were found to have more surface defects and rougher surface which result in highest photocatalytic activity [47]. Generally, the electrochemical active sites will be more accessible on the more defective surface, which can greatly facilitate the electrocatalytic oxidation of target analysts. Moreover, the rougher surface means a larger specific surface area, which is also favorable for electrochemical sensing. These facts explain well the remarkable electrocatalytic activity for d-Fe₂O₃. For the DPVs in Figure 3B further confirmed discal α -Fe₂O₃ NPs have the strongest electrocatalytic ability for the oxidation of DA and UA. Therefore, there is solid proof that the electrochemical activity of α -Fe₂O₃ NPs can be tailored by their morphologies. Considering the excellent sensitivity for the simultaneous determination of DA and UA, high electrocatalytic active discal α -Fe₂O₃ NPs were chosen as sensing materials in subsequent experiments. To further enhance the sensitivity, discal α -Fe₂O₃ NPs were coupled with GO (d-Fe₂O₃/GO) aiming to yield synergistic effect toward the electrooxidation of DA and UA. The SEM image of d-Fe₂O₃/GO is shown in Figure 1D. Evidently, discal α -Fe₂O₃ NPs are warped by silky graphene oxide sheets.

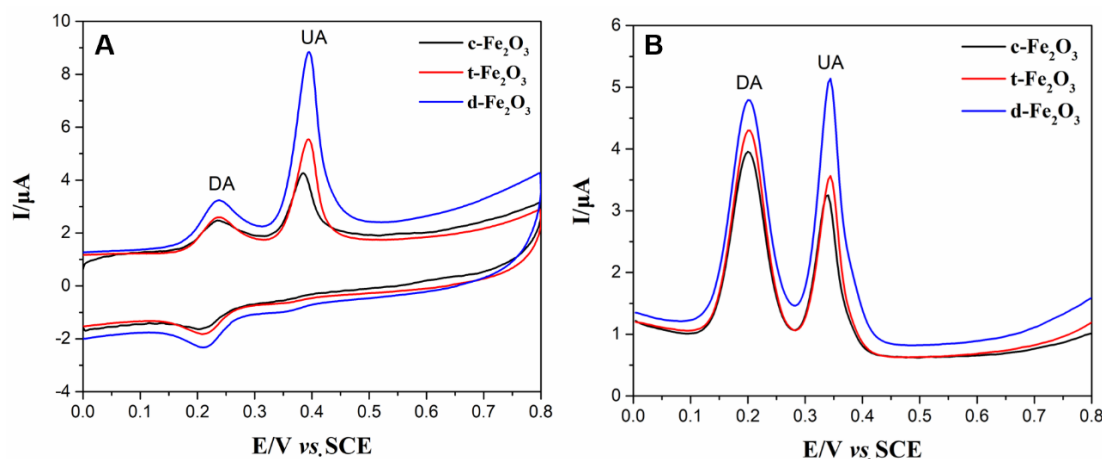


Figure 3. Cyclic voltammetry (CV) (A) and differential pulse voltammetry (DPV) (B) curves of c-Fe₂O₃, t-Fe₂O₃, and d-Fe₂O₃ NPs modified GCEs in 0.1 M PBS (pH = 7) containing 10 μM DA and UA.

3.2. Electrochemical Performance of d-Fe₂O₃/GO/GCE

The electrochemical performance of different modified GCEs were investigated by CV using 0.5 mM [Fe(CN)₆]^{3-/4-} as probe solution. The corresponding CV curves are plotted in Figure 4. A pair of weak redox peaks ($I_{pa} = 12.73 \mu\text{A}$, $I_{pc} = 12.16 \mu\text{A}$) are observed on the bare GCE with peak potential separation (ΔE_p) of 0.156 V, suggesting that the electron transfer rate is very slow. At the GO/GCE, a pair of wide and weak redox peak occurs with the lowest redox peak currents ($I_{pa} = 3.942 \mu\text{A}$, $I_{pc} = 3.768 \mu\text{A}$) and maximum ΔE_p ($\Delta E_p = 0.182 \text{ V}$). It was mainly due to the presence of poor electrical conductivity of GO. At the d-Fe₂O₃/GCE, a pair of well-shaped and sharp redox peak appears. Both anodic peak current (I_{pa}) and cathodic peak current (I_{pc}) increase greatly ($I_{pa} = 3.942 \mu\text{A}$, $I_{pc} = 3.768 \mu\text{A}$) while the ΔE_p decreases to 0.136 V, indicating d-Fe₂O₃ can effectively promote the redox process due to its high electrocatalytic activity. As expected, d-Fe₂O₃/GO/GCE displays remarkable electrochemical properties with the highest redox peak currents ($I_{pa} = 47.45 \mu\text{A}$, $I_{pc} = 46.8 \mu\text{A}$) and minimum potential separation ($\Delta E_p = 0.104 \text{ V}$), attributing to the synergistic effect from d-Fe₂O₃ NPs and GO nanosheets. As well known, electrochemical active area is highly related to the electrochemical sensing properties. The electrochemical active areas of various electrodes were also estimated using the Randles-Sevcik equation [20,21,24]. The electrochemical active areas of bare GCE, GO/GCE, d-Fe₂O₃/GCE and d-Fe₂O₃/GO/GCE are estimated as 0.1037, 0.0321, 0.3991 and 1.1181 cm², respectively. The electrochemical active area of d-Fe₂O₃/GO/GCE is approximately 2-fold and 10-fold higher than that of d-Fe₂O₃/GCE and bare GCE, respectively.

EIS is a valuable tool to acquire interfacial properties, which has extensively used in the various electrochemical sensors [20,21,57–59]. Nyquist plots for bare GCE, d-Fe₂O₃/GCE, GO/GCE and d-Fe₂O₃/GO/GCE are presented in Figure 4B. The Nyquist plots reveals electron transfer kinetics and diffusion characteristic. Typically, Nyquist plots include two portions, namely semicircular and linear portions. The semicircular at the higher frequency domain and linear part at the lower frequency domain represents the electron transfer limited and diffusion limited electrode processes, respectively. The semicircle diameter indicates the charge transfer resistance (R_{ct}). Obviously, the largest semicircle diameters (4500 ohm) are obtained at GO/GCE, indicating the poor electrical conductivity of GO retard electron transfer process. Compared to bare GCE (948 ohm), the R_{ct} values for d-Fe₂O₃/GCE and d-Fe₂O₃/GO/GCE decrease to 64 ohm and 35 ohm, respectively. The lowest R_{ct} value is obtained at d-Fe₂O₃/GO/GCE since numerous electrocatalytic active sites occurred, demonstrating that an obvious acceleration of redox kinetics of [Fe(CN)₆]^{3-/4-} happened on the surface of d-Fe₂O₃/GO nanohybrids. The results verify that the d-Fe₂O₃/GO nanohybrids can effectively lower the R_{ct} .

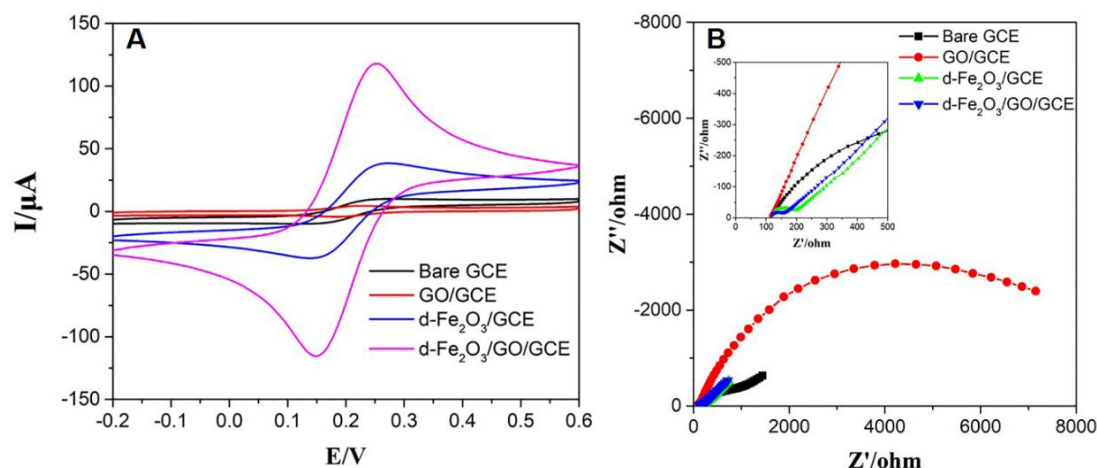


Figure 4. (A) CVs curves of bare GCE, GO/GCE, $d\text{-Fe}_2\text{O}_3/\text{GCE}$ and $d\text{-Fe}_2\text{O}_3/\text{GO}/\text{GCE}$ in the 0.5 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$; (B) Nyquist plots of different electrodes for the EIS measurements in the presence of 0.5 mM $[\text{Fe}(\text{CN})_6]^{3-/4-}$ (1:1) in 0.1 M KCl. The inset is the magnification of Nyquist plots at the higher frequency region.

3.3. Electrochemical Behaviors of DA and UA on the $d\text{-Fe}_2\text{O}_3/\text{GO}/\text{GCE}$

Electrochemical responses of 10 μM DA and UA (1:1) at different electrodes were recorded by DPV in 0.1 M PBS (pH = 5.65). As presented in Figure 5A, the anodic peaks of DA and UA are well separated, indicating simultaneous detection of DA and UA is very feasible. On the bare GCE, the I_{pa} of DA and UA is 0.2724 μA and 0.1555 μA , respectively. After the modification of GO nanosheets, the I_{pa} of DA and UA increased a little ($I_{\text{pa}(\text{DA})} = 0.2915 \mu\text{A}$, $I_{\text{pa}(\text{UA})} = 0.2356 \mu\text{A}$). The large specific area of GO could provide abundant adsorption sites for target analytes, which enhances the electrochemical response signals. But the poor electrical conductivity of GO severely retards the redox process, which impedes electrochemical oxidation of DA and UA. When $d\text{-Fe}_2\text{O}_3$ NPs were modified on the GCE, the I_{pa} of both DA and UA boosts greatly ($I_{\text{pa}(\text{DA})} = 0.5519 \mu\text{A}$, $I_{\text{pa}(\text{UA})} = 0.4770 \mu\text{A}$), suggesting $d\text{-Fe}_2\text{O}_3$ NPs have high electrocatalytic activity toward DA and UA. Among all the electrodes, $d\text{-Fe}_2\text{O}_3/\text{GO}$ nanohybrids show a remarkable electrocatalytic capacity toward the electrochemical oxidation of DA and UA, with the highest I_{pa} of 1.077 and 1.234 μA for DA and UA, respectively. The synergistic effect from $d\text{-Fe}_2\text{O}_3$ NPs and GO nanosheets contributed to the significant enhancement in the response currents. Specifically, abundant active sites presented in the GO surface greatly facilitates the adsorption of target analytes; $d\text{-Fe}_2\text{O}_3$ can efficiently catalyze the electrooxidation of DA and UA. Besides, the $d\text{-Fe}_2\text{O}_3$ NPs/GO nanohybrids remarkably decrease the electron transfer resistant (confirmed by EIS, Figure 4B), which greatly accelerates the redox kinetics. Moreover, the peak-to-peak separations of bare GCE, GO/GCE, $d\text{-Fe}_2\text{O}_3/\text{GCE}$ and $d\text{-Fe}_2\text{O}_3/\text{GO}/\text{GCE}$ are 0.132, 0.140, 0.144, and 0.148 V, respectively. The maximum ΔE_p is obtained at $d\text{-Fe}_2\text{O}_3/\text{GO}/\text{GCE}$, demonstrating good distinguish capacity.

The electrochemical responses of various electrodes were also measured by CV. As shown in Figure 5B, two anodic peaks belonging to DA and UA are observed at all the electrodes. However, a negligible cathodic peak corresponding to the reduction of UA appears at reverse scanning, implying a poor reversible electrode reaction for UA. The ratio of $I_{\text{pa}}/I_{\text{pc}}$ approaches 1 for all the electrodes, meaning the electrode undergoes a quasi-reversible process. Among all electrodes, $d\text{-Fe}_2\text{O}_3/\text{GO}$ nanohybrids also have the largest response peak currents for DA and UA. The CV result is in good agreement with the results obtained by DPVs. It is worth pointing out that DPV is more sensitive than CV, which is very suitable for multiple analytes detection. Therefore, DPV was used for the quantitative analysis of DA and UA.

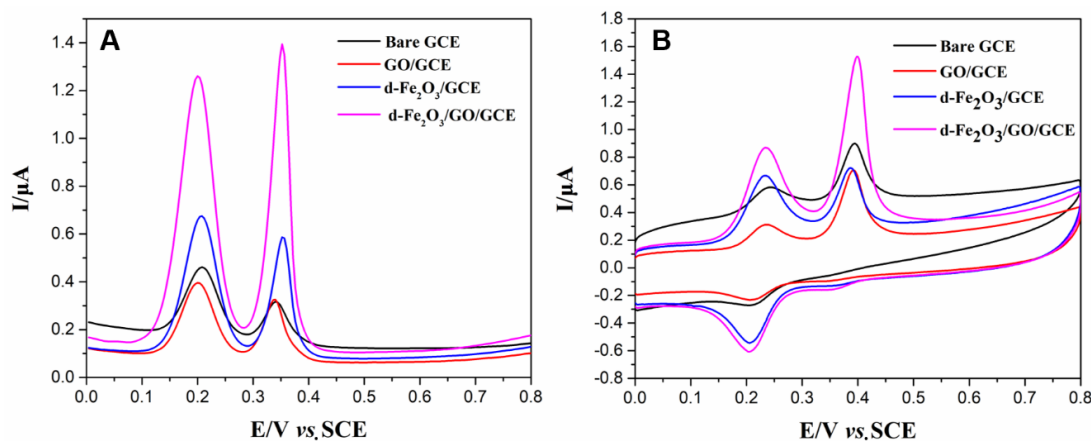


Figure 5. CVs (A) and DPVs (B) of 10 μM DA and UA (1:1) mixture solution at the bare GCE, GO/GCE, $\text{d-Fe}_2\text{O}_3/\text{GCE}$ and $\text{d-Fe}_2\text{O}_3/\text{GO/GCE}$.

3.4. Optimization of Voltammetric Parameters

3.4.1. Influence of pH

It is well known that pH is a vital parameter that directly influences the electrochemical responses. The DPVs of 10 μM DA and UA mixture solution (1:1) at different pH are depicted in Figure 6A. Notably, the anodic peaks shift to the negative direction as the increasing of pH. The influence of pH on the response peak currents of DA and UA is shown in Figure 6B. In the pH range of 3.10 to 6.90, the anodic peak currents always increase with the increase of pH. The anodic peak currents of UA slowly increase when pH varied from 3.10 to 4.56, then gradually decrease with the further increase of pH. The highest response anodic peak is obtained at pH = 4.56. Trading off the oxidation peak current of DA and UA, pH 5.65 is selected as optimum pH in the following measurements. Moreover, the anodic peak potentials linearly decrease with the increase of pH (Figure 6C). The linear plots of peak potential versus pH can be expressed as $E_{\text{DA}} = -0.06079 \text{ pH} + 0.5762$ ($R^2 = 0.9988$) and $E_{\text{UA}} = -0.06130 \text{ pH} + 0.7184$ ($R^2 = 0.9986$). The slopes of these linear plots (-60.8 mV/pH and -61.3 mV/pH for DA and UA, respectively) are very close to the theoretical value from the Nernst equation (-59 mV/pH), indicating that the equal numbers of protons (H^+) and electrons (e^-) participate in the electrooxidation process of DA and UA, which is in good agreement with previous works.

3.4.2. Influence of Accumulation Parameters

To enhance the response electrochemical peak currents, accumulation was applied before electrochemical measurements. The influence of accumulation time on the response anodic peak currents of DA and UA was explored (Figure 7A). The response peak currents of DA and UA slowly increase during the first 60 s, then gradually attenuate with further extending of accumulation time. The highest response peaks are obtained at 60 s. Furthermore, the dependence of the anodic peak currents on the accumulation potential was also investigated (Figure 7B). When accumulation potentials vary from -0.4 to -0.3 V , the anodic peak currents of DA and UA enhance gradually. However, the anodic peak currents decline with accumulation potential varying from -0.3 to 0 V . The maximum anodic peaks are obtained at -0.3 V . Therefore, 60 s and -0.3 V were chosen as the optimum accumulation parameters.

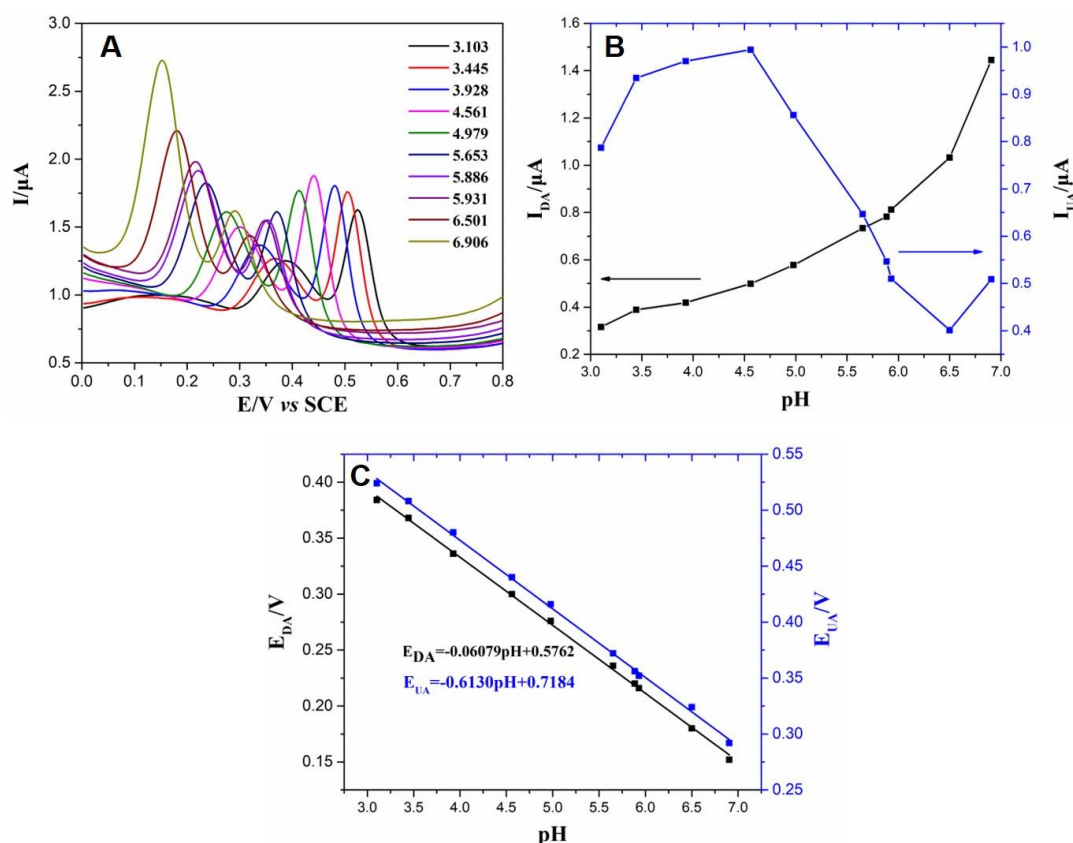


Figure 6. (A) DPVs of 10 μM DA and UA (1:1) mixture solution recorded at different pH; (B) Effect of pH on the response anodic peak current of DA and UA; (C) Linear plots of the anodic peak potential of DA and UA against pH.

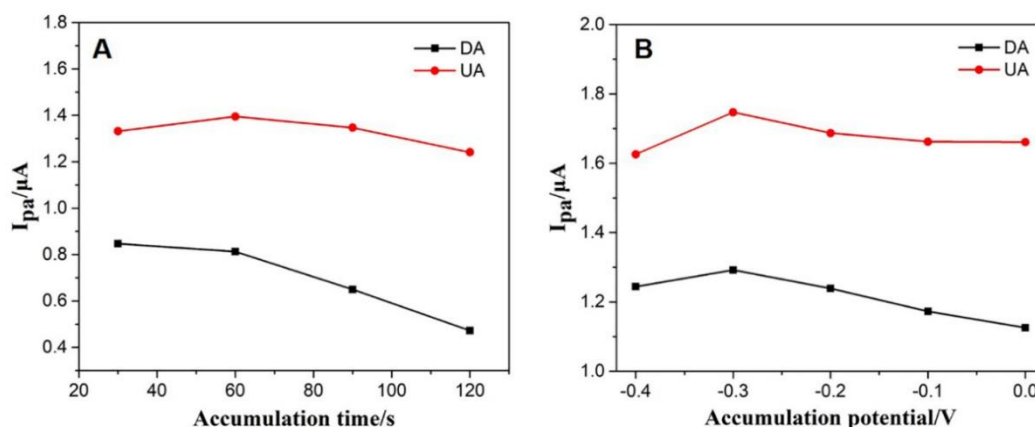


Figure 7. Influence of accumulation time (A) and accumulation potential (B) on the response anodic peak currents of DA and UA.

3.5. Reaction Mechanism of DA and UA

In order to provide a deeper insight into the electrochemical oxidation mechanism, CVs of 10 μM DA and UA (1:1) mixture solution were recorded at various scanning rates using d-Fe₂O₃/GO/GCE. CVs at different scanning rates are plotted in Figure 8A. Notably, the redox peaks increase with the increasing of scanning rate. Meanwhile the background currents also increased, probably because high scanning rates can increase the charging current of double layer. Moreover, the anodic peaks for DA and UA shift positivity as the increase of scanning rate while the cathodic peaks for UA shift to negative direction. As shown in Figure 8B, the anodic and cathodic peak currents of DA are highly correlated

with the square root of scanning rate ($v^{1/2}$), suggesting the electrooxidation of DA is a diffusion-limited process. The linear regression equations are $I_{pa(DA)} = 13.6968 v^{1/2} - 0.5756$ and $I_{pc(DA)} = -8.7663 v^{1/2} + 0.0129$, with the correlation coefficient (R^2) of 0.985. The anodic peak currents of UA are in positive proportion to the square root of scanning rate ($v^{1/2}$), indicating the oxidation of UA limited by the diffusion in bulk solution. The linear regression equation is $I_{pa(UA)} = 11.9383 v^{1/2} - 0.7370$ with the correlation coefficient (R^2) of 0.999 (Figure 8C). Since the electrooxidation of DA and UA is an equal number of electrons (e^-) coupled with protons (H^+) process, a two electron and two proton ($2H^+$, $2e^-$) mechanism was proposed for the oxidation of DA and UA (Scheme 1).

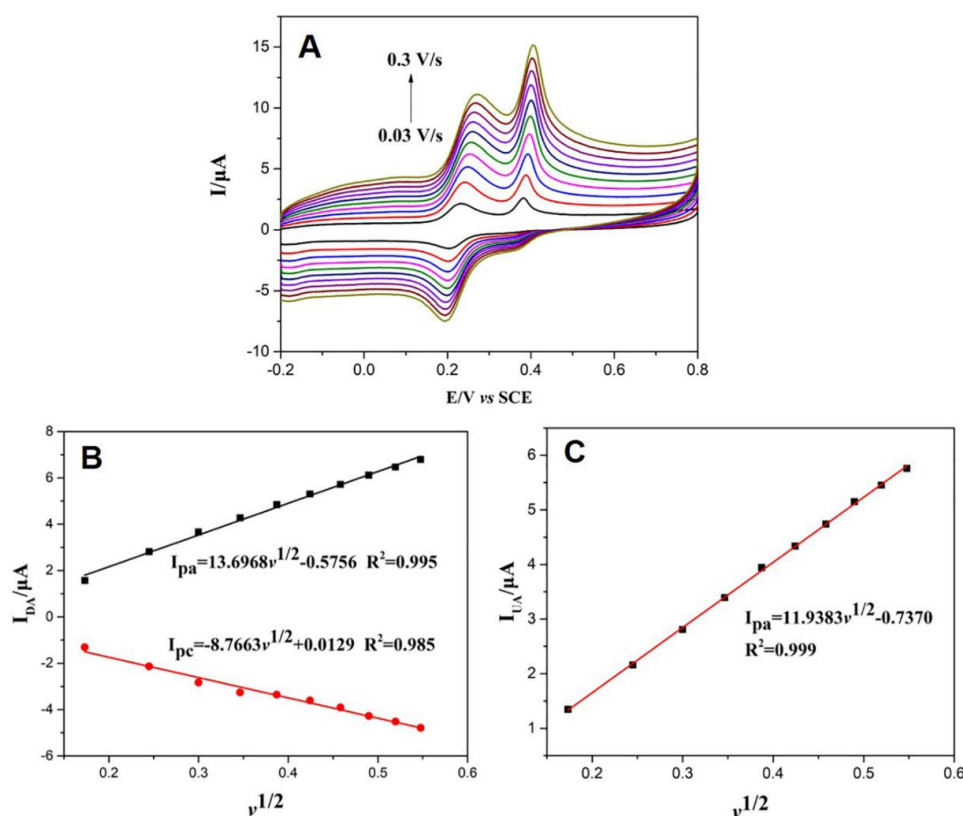


Figure 8. (A) CVs of 10 μM DA and UA (1:1) mixture solution recorded at various scanning rates; (B) Linear relationship between the redox peak current of DA and the square root of scanning rate ($v^{1/2}$); (C) Linear relationship between the anodic peak current of UA and the square root of scanning rate ($v^{1/2}$).

3.6. Individual and Simultaneous Detection of DA and UA

For the individual detection of DA and UA on the d- $\text{Fe}_2\text{O}_3/\text{GO}/\text{GCE}$, DPVs were performed in the potential range from 0–0.8 V in 0.1 M PBS (pH 5.65). In this case, only the concentrations of the target species were changed, while the concentrations of the other species remained unaltered. As plotted in Figure 9, the response anodic peak currents of DA increases linearly with the DA concentrations increasing from 0.04 to 4 μM . However, the response anodic peak currents of DA are highly correlation to Napierian logarithm of DA concentrations ($\ln C_{DA}$) at higher concentration domain (4–100 μM). For individual detection of UA, the response anodic peak currents of UA are in proportion to the all working concentrations from 0.1 to 100 μM (Figure 10). The limit of detection (LOD) for the individual detection of DA and UA are estimated to 4.8 and 12 nM at $S/N = 3$, respectively. It is noteworthy that addition of the target species does not have obvious interference on the electrochemical responses (i.e., the anodic peak current and potential) of the other species. The results strongly imply that DA and UA can be sensitively and selectively detected on d- $\text{Fe}_2\text{O}_3/\text{GO}/\text{GCE}$ in the DA and UA mixture (specific concentrations (C_{DA}/C_{UA}) range of 0.01–100).

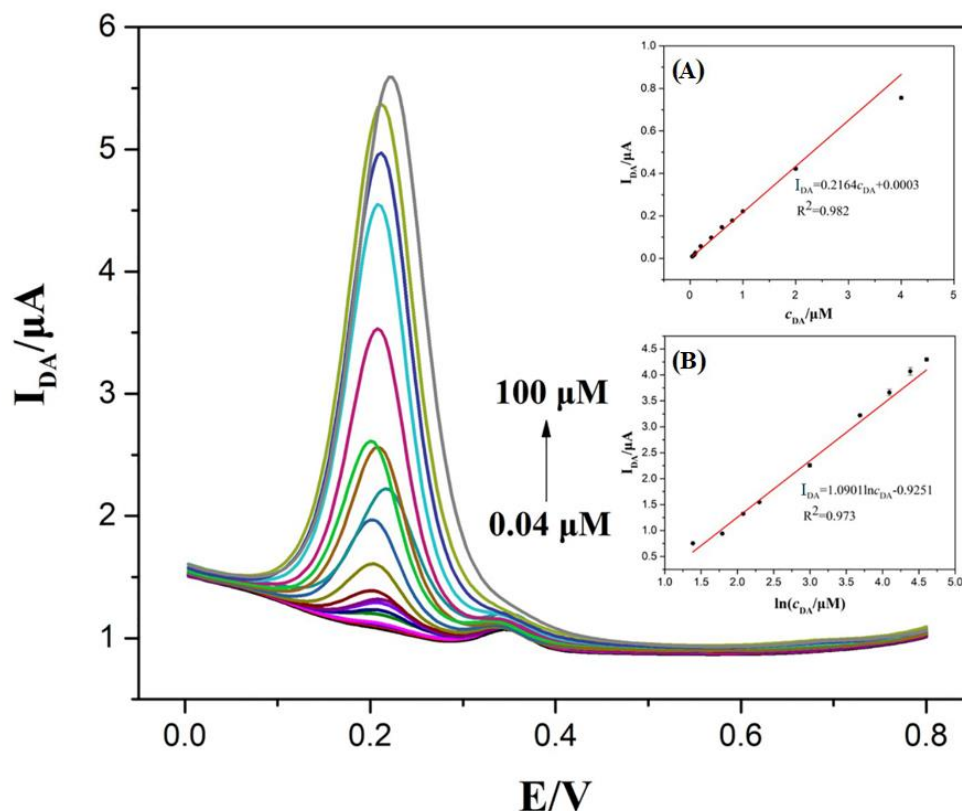


Figure 9. DPVs on the d-Fe₂O₃/GO/GCE in 0.1 M PBS (pH 5.65) containing 1 μM UA and various concentrations of DA from 0.04 to 100 μM; The inset (A) represents the linear plot of the anodic peak currents versus the DA concentrations varying from 0.04 to 4 μM; The inset (B) represents the linear plot of the anodic peak currents versus the Napierian logarithm of DA concentrations with DA concentration ranging from 4 to 100 μM.

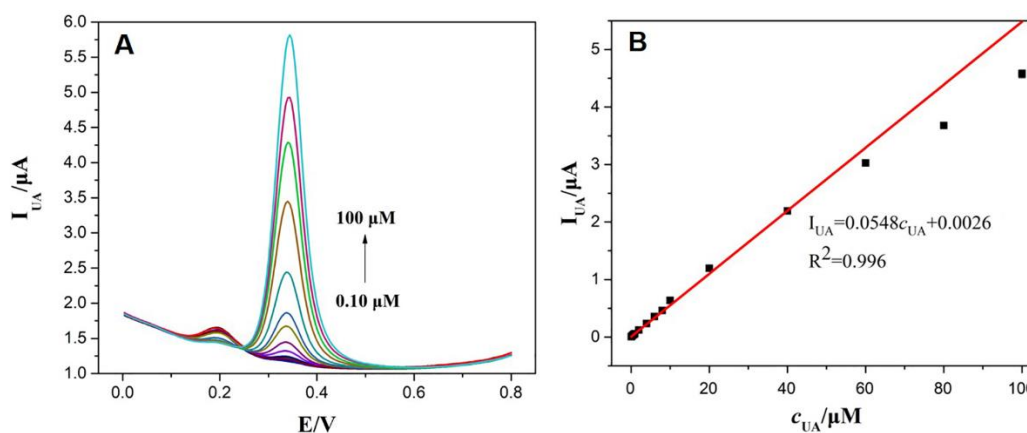


Figure 10. (A) DPVs on the d-Fe₂O₃/GO/GCE in 0.1 M PBS (pH 5.65) containing 1 μM DA and various concentrations of UA from 0.1 to 100 μM; (B) The linear plot of the anodic peak currents of UA versus the UA concentrations varying from 0.1 to 100 μM.

Superior electrocatalytic activity of d-Fe₂O₃/GO also showed simultaneous detection of DA and UA using DPV technique in 0.1 M PBS (pH 5.65) (Figure 11). Two well-separated anodic peaks relating to the electrooxidation of DA and UA occur on DPV curves using d-Fe₂O₃/GO/GCE. Moreover, DPV responses are resolved into two peaks at 0.22 and 0.36 V, which can be attributed to the oxidations of DA and UA, respectively. These results indicating that simultaneous distinguish from the two substances is feasible in mixture solutions. As expected, all anodic peak currents increase linearly

with increasing concentrations of DA and UA. Two linear response regions for both DA and UA are obtained within concentration ranges of 0.02–10 μM and 10–100 μM , respectively (Figure 11B–E). The linear regression equations for DA can be expressed as $I_{\text{DA}}(\mu\text{M}) = 0.1062C_{\text{DA}}(\mu\text{M}) + 0.0122$ ($R^2 = 0.975$) and $I_{\text{DA}}(\mu\text{M}) = 0.0186C_{\text{DA}}(\mu\text{M}) + 0.7835$ ($R^2 = 0.985$). The linear regression equations for UA are $I_{\text{UA}}(\mu\text{M}) = 0.0862C_{\text{UA}}(\mu\text{M}) + 0.0036$ and $I_{\text{UA}}(\mu\text{M}) = 0.0320C_{\text{UA}}(\mu\text{M}) + 0.4804$, with correlation coefficient of 0.995 and 0.990, respectively. The LODs are calculated as 3.2 and 2.5 nM for DA and UA, respectively. All results demonstrate that the proposed d-Fe₂O₃/GO/GCEs feature wider linear response ranges and lower LOD for the electrochemical oxidation of DA and UA. Hence, the simultaneous detection of DA and UA can be realized on d-Fe₂O₃/GO/GCE with high sensitivity and good selectivity. The sensing performances are compared to those in previous reports (Table 1). Clearly, the sensing parameters (i.e., linear response ranges and LOD) of the proposed sensor are comparable to, or even better than most previous reported modified electrodes [7,55,60–70]. The high sensitivity of our proposed sensor is closely related to the synergistic electrocatalytic effect from the d-Fe₂O₃ and GO.

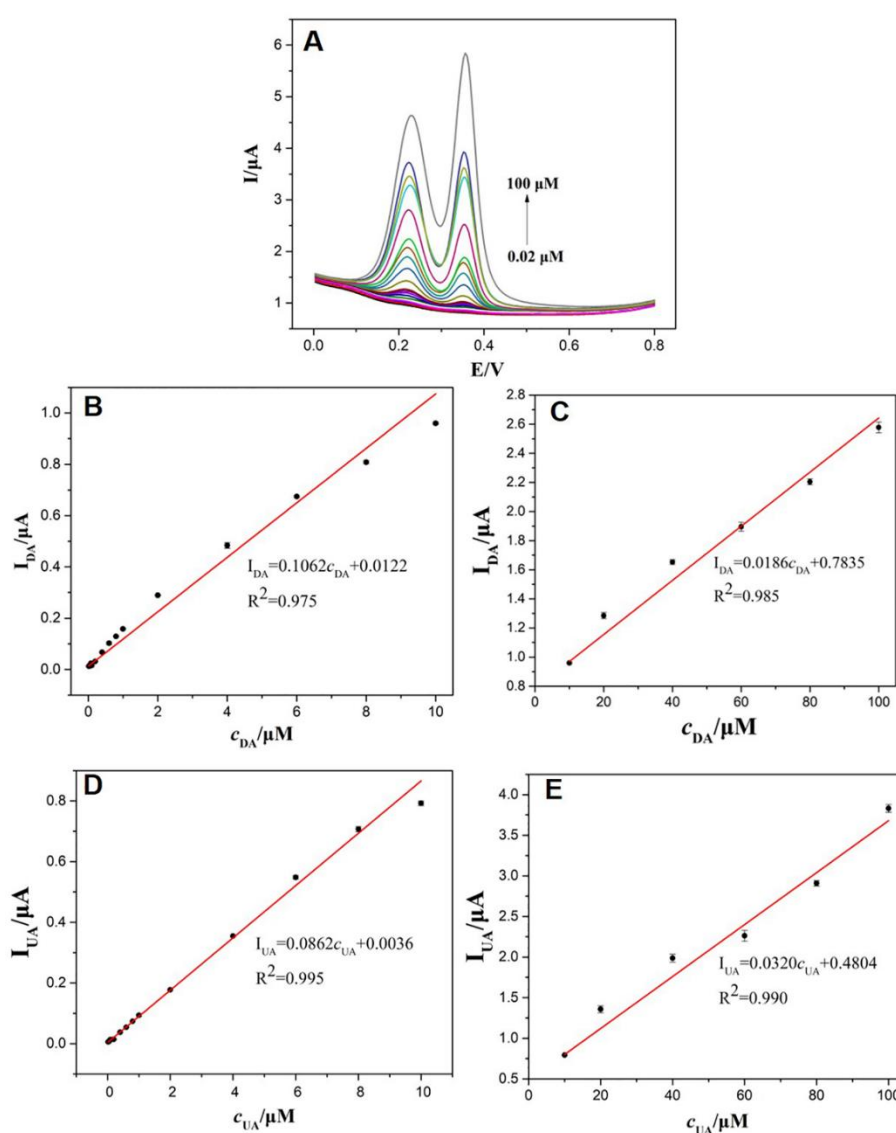


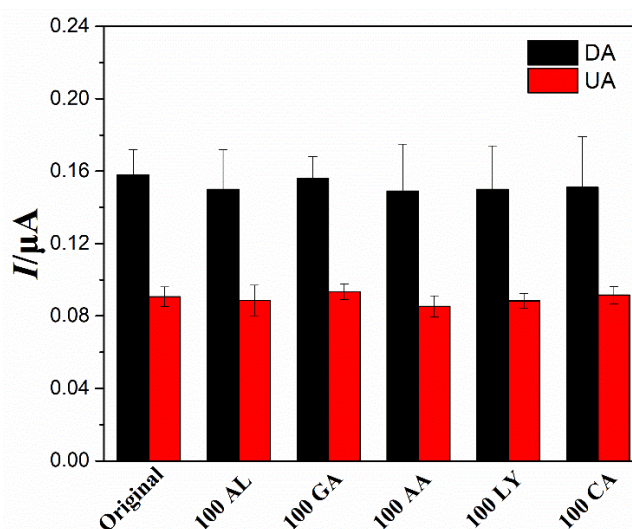
Figure 11. (A) DPVs on the d-Fe₂O₃/GO/GCE in 0.1 M PBS (pH 5.65) containing different concentrations of DA and UA ranging from 0.02–100 μM ; Plots of the anodic peak currents as the function of DA concentrations in the range of 0.02–10 μM (B) and 10–100 μM (C); Plots of the anodic peak currents as the function of UA concentrations in the range of 0.02–10 μM (D) and 10–100 μM (E).

Table 1. Comparison analytical performance between previous reports and the proposed d-Fe₂O₃/GO/GCE for the simultaneous detection of DA and UA.

Electrodes	Methods	Detection Range (μM)		LOD (μM)		Ref.
		DA	UA	DA	UA	
Au/Cu ₂ O/rGO/GCE	DPV	10–90	100–900	3.9	6.5	[7]
NSG-Fe ₂ O ₃ /GCE	DPV	0.3–210		0.035		[55]
Pd/RGO/GCE	DPV	0.45–71	6–469.5	0.18	1.6	[60]
Pt/RGO/GCE	DPV	10–170	10–130	0.25	0.45	[61]
ZnO/SPCE	DPV	0.1–374	0.1–169	0.004	0.00849	[62]
Fe ₃ O ₄ /rGO/GCE	DPV	0.5–100		0.12		[63]
AuPtNPs/S-NS-GR/GCE	DPV	0.01–400	1–1000	0.006	0.0038	[64]
Au-Pt/GO-ERGO	DPV	0.0682–49,800	0.125–82,800	0.0207	0.0407	[65]
Fe ₂ O ₃ /NrGO/GCE	Amperometry	0.5–340		0.49		[66]
ZnO/PANI/rGO/GCE	DPV	0.1–90	0.5–90	0.017	0.12	[67]
pCu ₂ O NS-rGO/GCE	DPV	0.05–109	1–138	0.015	0.112	[68]
Zn-NiAl LDH/rGO/GCE	DPV	0.0001–1	0.0011–0.95	0.0001	0.0009	[69]
α-Fe ₂ O ₃ @Au-Pd/GCE	SWV	0.1–1000	1–1000	0.0000138	0.97	[70]
d-Fe ₂ O ₃ /GO/GCE	DPV	0.02–10; 10–100	0.02–10; 10–100	0.0032	0.0025	This work

3.7. Practical Application

Prior to the simultaneous determination of DA and UA in actual samples, the selectivity, repeatability, stability and reproducibility were also investigated. In order to assess the anti-interference of the proposed d-Fe₂O₃/GO/GCE toward the DA and UA, the DPV responses of the DA and UA in the presence of potential interfering species were recorded. Negligible interference with accepted relative error (less than 5.70%) even in the presence of 100-fold ascorbic acid, citric acid, alanine, glutamic acid, and lysine (Figure 12). To assess electrode reproducibility, the variation on anodic peak currents in the 1 μM DA and UA (1:1) mixture solution was measured at room temperature using five d-Fe₂O₃/GO/GCE, which were fabricated by the same procedure. The relative standard deviations (RSD) for the anodic peak current are 4.56% and 3.03%, respectively, indicating that the electrode fabrication has high reproducibility. To evaluate the repeatability, seven successive measurements for detection of 1 μM DA and UA (1:1) were carried out. The RSD for DA and UA are 5.07% and 4.81%, respectively, suggesting good repeatability.

**Figure 12.** The anodic peak currents of 1 μM DA and UA in the presence of 100-fold alanine (AL), glutamic acid (GA), ascorbic acid (AA), lysine (LY) and citric acid (CA).

To verify applicability, the concentrations of DA and UA in actual samples were also detected on d-Fe₂O₃/GO/GCE. Since DA and UA always coexist in most biological fluids, the practicability of

d-Fe₂O₃/GO/GCE in actual sample detection was assessed with human urine and serum samples. The determined results listed in Table 2 were carefully estimated from the standard curves. To further validate the accuracy and precision of the proposed sensor, a series of known concentration solutions of DA and UA were spiked to the actual samples to calculate the recovery. The recoveries of 94.1–106.4% and 95.2–108.2% are obtained for DA and UA, respectively. DPVs for the analysis of human serum samples with 100-fold dilution are presented in Figure S1. Notably, the shape and position of the DPVs are not affected when using real samples. These results confirm that the biological matrixes such as human urine and serum does not affect the simultaneous determination of DA and UA.

Table 2. Detection results of DA and UA in human serum and urine samples using d-Fe₂O₃/GO/GCE.

Samples ^a	Detected (μM)	Added (μM)	Found (μM)	RSD (%)	Recovery (%)	
Serum	DA	ND ^b	20	18.82	3.75	94.1
			40	38.26	2.86	95.7
	UA	20.6	20	41.76	2.75	105.8
			40	63.86	2.21	108.2
Urine	DA	ND ^b	20	21.06	4.98	105.3
			40	42.56	3.67	106.4
	UA	35.24	20	54.27	2.62	95.2
			40	74.52	1.39	98.2

^a The human urine and serum samples were detected at 100-fold and 10-fold dilution, respectively. ^b Not detected.

4. Conclusions

In summary, the influence of Fe₂O₃/GO morphologies on electrochemical sensing performances was studied systematically. Cubic, thorhombic and discal Fe₂O₃ NPs with a uniform size and controllable structure were successfully prepared by a facile meta-ion mediated hydrothermal route. When coupled with GO nanosheets and then worked as sensing films for the simultaneous detection of DA and UA, the α-Fe₂O₃ NPs with discal morphology displayed the highest electrocatalytic activity. This remarkable electrocatalytic behavior was highly correlated with the discal shapes with more surface defects and a rougher surface. The synergistic effect from d-Fe₂O₃ NPs and GO nanosheets contributed to a significant enhancement in the response currents. As a consequence, two wide detection ranges (0.02–10 μM and 10–100 μM) were obtained for DA and UA, with very low limit of detection (LOD) of 3.2 and 2.5 nM for DA and UA, respectively. Moreover, the d-Fe₂O₃/GO nanohybrids showed good selectivity and reproducibility. The proposed d-Fe₂O₃/GO nanohybrids have become one of the most competitive candidates as sensing materials for the simultaneous determination of DA and UA in various real samples.

Supplementary Materials: The following are available online at <http://www.mdpi.com/2079-4991/9/6/835/s1>, Figure S1: DPVs for the analysis of human serum samples with 100-fold dilution.

Author Contributions: Conceptualization, Z.C., Y.Y. and G.L.; methodology, Z.C., Y.Y. and X.W.; experiment, Z.C., Y.Y., X.W., and S.Y.; data analysis, Z.C., Y.Y., and Y.X.; writing—original draft preparation, Z.C., Y.Y.; writing—review and editing, G.L. and Q.H.; supervision, G.L. and Q.H.; funding acquisition, G.L., J.L. and Q.H.

Funding: This research was funded by the Undergraduates' Innovation Experiment Program of Hunan Province (No. 2018649), National Natural Science Foundation of China (No. 61703152), Natural Science Foundation of Hunan Province (No. 2019JJ50127, 2018JJ3134), Scientific Research Foundation of Hunan Provincial Education Department (18A273, 18C0522), Project of Science and Technology Plan of Zhuzhou (201707201806), and the Doctoral Program Construction of Hunan University of Technology.

Acknowledgments: We sincerely express our thanks to Zhuzhou People's Hospital for offering human serum samples.

Conflicts of Interest: The authors declare no conflict of interest.

References

1. He, Q.; Liu, J.; Liang, J.; Liu, X.; Li, W.; Liu, Z.; Ding, Z.; Tuo, D. Towards improvements for penetrating the blood–brain barrier—recent progress from a material and pharmaceutical perspective. *Cells* **2018**, *7*, 24. [[CrossRef](#)] [[PubMed](#)]
2. Dalley, J.W.; Roiser, J.P. Dopamine, serotonin and impulsivity. *Neuroscience* **2012**, *215*, 42–58. [[CrossRef](#)] [[PubMed](#)]
3. Carlsson, A. Does dopamine play a role in schizophrenia? *Psychol. Med.* **1977**, *7*, 583–597. [[CrossRef](#)]
4. Zhang, M.; Liao, C.; Yao, Y.; Liu, Z.; Gong, F.; Yan, F. High-Performance Dopamine Sensors Based on Whole-Graphene Solution-Gated Transistors. *Adv. Funct. Mater.* **2014**, *24*, 978–985. [[CrossRef](#)]
5. Wightman, R.M.; May, L.J.; Michael, A.C. Detection of Dopamine Dynamics in the Brain. *Anal. Chem.* **1988**, *60*, 769A–793A. [[CrossRef](#)] [[PubMed](#)]
6. Jindal, K.; Tomar, M.; Gupta, V. Nitrogen-doped zinc oxide thin films biosensor for determination of uric acid. *Analyst* **2013**, *138*, 4353–4362. [[CrossRef](#)]
7. Aparna, T.K.; Sivasubramanian, R.; Dar, M.A. One-pot synthesis of Au-Cu₂O/rGO nanocomposite based electrochemical sensor for selective and simultaneous detection of dopamine and uric acid. *J. Alloys Compd.* **2018**, *741*, 1130–1141. [[CrossRef](#)]
8. Sharaf El Din, U.A.A.; Salem, M.M.; Abdulazim, D.O. Uric acid in the pathogenesis of metabolic, renal, and cardiovascular diseases: A review. *J. Adv. Res.* **2017**, *8*, 537–548. [[CrossRef](#)]
9. Xiang, L.W.; Li, J.; Lin, J.M.; Li, H.F. Determination of gouty arthritis' biomarkers in human urine using reversed-phase high-performance liquid chromatography. *J. Pharm. Anal.* **2014**, *4*, 153–158. [[CrossRef](#)]
10. Lin, L.; Qiu, P.; Yang, L.; Cao, X.; Jin, L. Determination of dopamine in rat striatum by microdialysis and high-performance liquid chromatography with electrochemical detection on a functionalized multi-wall carbon nanotube electrode. *Anal. Bioanal. Chem.* **2006**, *384*, 1308–1313. [[CrossRef](#)]
11. Zhao, D.; Song, H.; Hao, L.; Liu, X.; Zhang, L.; Lv, Y. Luminescent ZnO quantum dots for sensitive and selective detection of dopamine. *Talanta* **2013**, *107*, 133–139. [[CrossRef](#)]
12. Moghadam, M.R.; Dadfarnia, S.; Shabani, A.M.H.; Shahbazikhah, P. Chemometric-assisted kinetic–spectrophotometric method for simultaneous determination of ascorbic acid, uric acid, and dopamine. *Anal. Biochem.* **2011**, *410*, 289–295. [[CrossRef](#)]
13. Huang, C.; Chen, X.; Lu, Y.; Yang, H.; Yang, W. Electrogenerated chemiluminescence behavior of peptide nanovesicle and its application in sensing dopamine. *Biosens. Bioelectron.* **2015**, *63*, 478–482. [[CrossRef](#)]
14. Kumbhat, S.; Shankaran, D.R.; Kim, S.J.; Gobi, K.V.; Joshi, V.; Miura, N. Surface plasmon resonance biosensor for dopamine using D3 dopamine receptor as a biorecognition molecule. *Biosens. Bioelectron.* **2007**, *23*, 421–427. [[CrossRef](#)]
15. Liu, S.; Yan, J.; He, G.; Zhong, D.; Chen, J.; Shi, L.; Zhou, X.; Jiang, H. Layer-by-layer assembled multilayer films of reduced graphene oxide/gold nanoparticles for the electrochemical detection of dopamine. *J. Electroanal. Chem.* **2012**, *672*, 40–44. [[CrossRef](#)]
16. Qi, S.; Zhao, B.; Tang, H.; Jiang, X. Determination of ascorbic acid, dopamine, and uric acid by a novel electrochemical sensor based on pristine graphene. *Electrochim. Acta* **2015**, *161*, 395–402. [[CrossRef](#)]
17. Lian, Q.; He, Z.; He, Q.; Luo, A.; Yan, K.; Zhang, D.; Lu, X.; Zhou, X. Simultaneous determination of ascorbic acid, dopamine and uric acid based on tryptophan functionalized graphene. *Anal. Chim. Acta* **2014**, *823*, 32–39. [[CrossRef](#)]
18. Hou, J.; Xu, C.; Zhao, D.; Zhou, J. Facile fabrication of hierarchical nanoporous AuAg alloy and its highly sensitive detection towards dopamine and uric acid. *Sens. Actuators B Chem.* **2016**, *225*, 241–248. [[CrossRef](#)]
19. He, Q.; Liu, J.; Liu, X.; Xia, Y.; Li, G.; Deng, P.; Chen, D. Novel Electrochemical Sensors Based on Cuprous Oxide-Electrochemically Reduced Graphene Oxide Nanocomposites Modified Electrode toward Sensitive Detection of Sunset Yellow. *Molecules* **2018**, *23*, 2130. [[CrossRef](#)]
20. He, Q.; Liu, J.; Liu, X.; Li, G.; Chen, D.; Deng, P.; Liang, J. A promising sensing platform toward dopamine using MnO₂ nanowires/electro-reduced graphene oxide composites. *Electrochim. Acta* **2019**, *296*, 683–692. [[CrossRef](#)]
21. He, Q.; Liu, J.; Liu, X.; Li, G.; Deng, P.; Liang, J. Manganese dioxide Nanorods/electrochemically reduced graphene oxide nanocomposites modified electrodes for cost-effective and ultrasensitive detection of Amaranth. *Colloids Surf. B* **2018**, *172*, 565–572. [[CrossRef](#)] [[PubMed](#)]

22. He, Q.; Liu, J.; Liu, X.; Li, G.; Deng, P.; Liang, J.; Chen, D. Sensitive and Selective Detection of Tartrazine Based on TiO₂-Electrochemically Reduced Graphene Oxide Composite-Modified Electrodes. *Sensors* **2018**, *18*, 1911. [[CrossRef](#)]
23. He, Q.; Liu, J.; Liu, X.; Li, G.; Chen, D.; Deng, P.; Liang, J. Fabrication of Amine-Modified Magnetite-Electrochemically Reduced Graphene Oxide Nanocomposite Modified Glassy Carbon Electrode for Sensitive Dopamine Determination. *Nanomaterials* **2018**, *8*, 194. [[CrossRef](#)]
24. He, Q.; Liu, J.; Liu, X.; Li, G.; Deng, P.; Liang, J. Preparation of Cu₂O-Reduced Graphene Nanocomposite Modified Electrodes towards Ultrasensitive Dopamine Detection. *Sensors* **2018**, *18*, 199. [[CrossRef](#)] [[PubMed](#)]
25. Chen, L.X.; Zheng, J.-N.; Wang, A.J.; Wu, L.J.; Chen, J.R.; Feng, J.J. Facile synthesis of porous bimetallic alloyed PdAg nanoflowers supported on reduced graphene oxide for simultaneous detection of ascorbic acid, dopamine, and uric acid. *Analyst* **2015**, *140*, 3183–3192. [[CrossRef](#)]
26. Zhao, L.; Li, H.; Gao, S.; Li, M.; Xu, S.; Li, C.; Guo, W.; Qu, C.; Yang, B. MgO nanobelt-modified graphene-tantalum wire electrode for the simultaneous determination of ascorbic acid, dopamine and uric acid. *Electrochim. Acta* **2015**, *168*, 191–198. [[CrossRef](#)]
27. Zhang, X.; Yan, W.; Zhang, J.; Li, Y.; Tang, W.; Xu, Q. NiCo-embedded in hierarchically structured N-doped carbon nanoplates for the efficient electrochemical determination of ascorbic acid, dopamine, and uric acid. *RSC Adv.* **2015**, *5*, 65532–65539. [[CrossRef](#)]
28. Chen, J.; Zhang, J.; Lin, X.; Wan, H.; Zhang, S. Electrocatalytic Oxidation and Determination of Dopamine in the Presence of Ascorbic Acid and Uric Acid at a Poly (4-(2-Pyridylazo)-Resorcinol) Modified Glassy Carbon Electrode. *Electroanalysis* **2007**, *19*, 612–615. [[CrossRef](#)]
29. Li, Y.; Lin, X. Simultaneous electroanalysis of dopamine, ascorbic acid and uric acid by poly (vinyl alcohol) covalently modified glassy carbon electrode. *Sens. Actuators B* **2006**, *115*, 134–139. [[CrossRef](#)]
30. Sheng, Z.H.; Zheng, X.-Q.; Xu, J.Y.; Bao, W.J.; Wang, F.B.; Xia, X.H. Electrochemical sensor based on nitrogen doped graphene: Simultaneous determination of ascorbic acid, dopamine and uric acid. *Biosens. Bioelectron.* **2012**, *34*, 125–131. [[CrossRef](#)]
31. Liu, Y.; Huang, J.; Hou, H.; You, T. Simultaneous determination of dopamine, ascorbic acid and uric acid with electrospun carbon nanofibers modified electrode. *Electrochem. Commun.* **2008**, *10*, 1431–1434. [[CrossRef](#)]
32. Cui, R.; Wang, X.; Zhang, G.; Wang, C. Simultaneous determination of dopamine, ascorbic acid, and uric acid using helical carbon nanotubes modified electrode. *Sens. Actuators B Chem.* **2012**, *161*, 1139–1143. [[CrossRef](#)]
33. Harraz, F.A.; Ismail, A.A.; Al-Sayari, S.A.; Al-Hajry, A.; Al-Assiri, M.S. Highly sensitive amperometric hydrazine sensor based on novel α -Fe₂O₃/crosslinked polyaniline nanocomposite modified glassy carbon electrode. *Sens. Actuators B Chem.* **2016**, *234*, 573–582. [[CrossRef](#)]
34. Ahmad, R.; Ahn, M.A.; Hahn, Y. A Highly Sensitive Nonenzymatic Sensor Based on Fe₂O₃ Nanoparticle Coated ZnO Nanorods for Electrochemical Detection of Nitrite. *Adv. Mater. Interfaces* **2017**, *4*, 1700491. [[CrossRef](#)]
35. Larsen, G.K.; Farr, W.; Murph, S.E.H. Multifunctional Fe₂O₃-Au Nanoparticles with Different Shapes: Enhanced Catalysis, Photothermal Effects, and Magnetic Recyclability. *J. Phys. Chem. C* **2016**, *120*, 15162–15172. [[CrossRef](#)]
36. Quan, H.; Cheng, B.; Xiao, Y.; Lei, S. One-pot synthesis of α -Fe₂O₃ nanoplates-reduced graphene oxide composites for supercapacitor application. *Chem. Eng. J.* **2016**, *286*, 165–173. [[CrossRef](#)]
37. Zhang, Z.J.; Wang, Y.X.; Chou, S.L.; Li, H.J.; Liu, H.K.; Wang, J.Z. Rapid synthesis of α -Fe₂O₃/rGO nanocomposites by microwave autoclave as superior anodes for sodium-ion batteries. *J. Power Sources* **2015**, *280*, 107–113. [[CrossRef](#)]
38. Wang, H.; Xu, Z.; Yi, H.; Wei, H.; Guo, Z.; Wang, X. One-step preparation of single-crystalline Fe₂O₃ particles/graphene composite hydrogels as high performance anode materials for supercapacitors. *Nano Energy* **2014**, *7*, 86–96. [[CrossRef](#)]
39. Cummings, C.Y.; Bonn e, M.J.; Edler, K.J.; Helton, M.; Mckee, A.; Marken, F. Direct reversible voltammetry and electrocatalysis with surface-stabilised Fe₂O₃ redox states. *Electrochem. Commun.* **2008**, *10*, 1773–1776. [[CrossRef](#)]
40. Fu, Y.; Wang, R.; Xu, J.; Chen, J.; Yan, Y.; Narlikar, A.; Zhang, H. Synthesis of large arrays of aligned α -Fe₂O₃ nanowires. *Chem. Phys. Lett.* **2003**, *379*, 373–379. [[CrossRef](#)]
41. Liu, L.; Kou, H.-Z.; Mo, W.; Liu, H.; Wang, Y. Surfactant-assisted synthesis of α -Fe₂O₃ nanotubes and nanorods with shape-dependent magnetic properties. *J. Phys. Chem. B* **2006**, *110*, 15218–15223. [[CrossRef](#)]

42. Mou, X.; Zhang, B.; Li, Y.; Yao, L.; Wei, X.; Su, D.S.; Shen, W.J. Rod-shaped Fe₂O₃ as an efficient catalyst for the selective reduction of nitrogen oxide by ammonia. *Angew. Chem. Int. Ed.* **2012**, *51*, 2989–2993. [[CrossRef](#)] [[PubMed](#)]
43. Liu, X.; Wang, H.; Su, C.; Zhang, P.; Bai, J. Controlled fabrication and characterization of microspherical FeCO₃ and α-Fe₂O₃. *J. Colloid Interface Sci.* **2010**, *351*, 427–432. [[CrossRef](#)]
44. Fu, X.; Bei, F.; Wang, X.; Yang, X.; Lu, L. Surface-enhanced Raman scattering of 4-mercaptopyridine on sub-monolayers of α-Fe₂O₃ nanocrystals (sphere, spindle, cube). *J. Raman Spectrosc.* **2009**, *40*, 1290–1295. [[CrossRef](#)]
45. Yan, W.; Fan, H.; Zhai, Y.; Yang, C.; Ren, P.; Huang, L. Low temperature solution-based synthesis of porous flower-like α-Fe₂O₃ superstructures and their excellent gas-sensing properties. *Sens. Actuators B* **2011**, *160*, 1372–1379. [[CrossRef](#)]
46. Yang, S.; Zhou, B.; Ding, Z.; Zheng, H.; Huang, L.; Pan, J.; Wu, W.; Zhang, H. Tetragonal hematite single crystals as anode materials for high performance lithium ion batteries. *J. Power Sources* **2015**, *286*, 124–129. [[CrossRef](#)]
47. Liu, J.; Yang, S.; Wu, W.; Tian, Q.; Cui, S.; Dai, Z.; Ren, F.; Xiao, X.; Jiang, C. 3D Flowerlike α-Fe₂O₃@TiO₂ Core–Shell Nanostructures: General Synthesis and Enhanced Photocatalytic Performance. *ACS Sustain. Chem. Eng.* **2015**, *3*, 2975–2984. [[CrossRef](#)]
48. Wu, W.; Yang, S.; Pan, J.; Sun, L.; Zhou, J.; Dai, Z.; Xiao, X.; Zhang, H.; Jiang, C. Metal ion-mediated synthesis and shape-dependent magnetic properties of single-crystalline α-Fe₂O₃ nanoparticles. *CrystEngComm* **2014**, *16*, 5566–5572. [[CrossRef](#)]
49. Yin, C.Y.; Minakshi, M.; Ralph, D.E.; Jiang, Z.T.; Xie, Z.; Guo, H.J. Hydrothermal synthesis of cubic α-Fe₂O₃ microparticles using glycine: Surface characterization, reaction mechanism and electrochemical activity. *J. Alloys Compd.* **2011**, *509*, 9821–9825. [[CrossRef](#)]
50. Chen, A.; Liang, X.; Zhang, X.; Yang, Z.; Yang, S. Improving Surface Adsorption via Shape Control of Hematite α-Fe₂O₃ Nanoparticle for Sensitive Dopamine Sensors. *ACS Appl. Mater. Interfaces* **2016**, *8*, 33765–33774. [[CrossRef](#)]
51. Mitra, S.; Das, S.; Mandal, K.; Chaudhuri, S. Synthesis of a α-Fe₂O₃ nanocrystal in its different morphological attributes: growth mechanism, optical and magnetic properties. *Nanotechnology* **2007**, *18*, 275608. [[CrossRef](#)]
52. Jagadeesan, D.; Mansoori, U.; Mandal, P.; Sundaresan, A.; Eswaramoorthy, M. Hollow Spheres to Nanocups: Tuning the Morphology and Magnetic Properties of Single-Crystalline α-Fe₂O₃ Nanostructures. *Angew. Chem. Int. Ed.* **2008**, *47*, 7685–7688. [[CrossRef](#)]
53. Liu, X.; Chen, T.; Chu, H.; Niu, L.; Sun, Z.; Pan, L.; Sun, C.Q. Fe₂O₃-reduced graphene oxide composites synthesized via microwave-assisted method for sodium ion batteries. *Electrochim. Acta* **2015**, *166*, 12–16. [[CrossRef](#)]
54. Zhang, Y.; Gao, W.; Zuo, L.; Zhang, L.; Huang, Y.; Lu, H.; Fan, W.; Liu, T. In situ growth of Fe₂O₃ nanoparticles on highly porous graphene/polyimide-based carbon aerogel nanocomposites for Effectively selective detection of dopamine. *Adv. Mater. Interfaces* **2016**, *3*, 1600137. [[CrossRef](#)]
55. Yasmin, S.; Ahmed, M.S.; Jeon, S. Determination of dopamine by dual doped graphene-Fe₂O₃ in Presence of Ascorbic Acid. *J. Electrochem. Soc.* **2015**, *162*, B363–B369. [[CrossRef](#)]
56. Gan, T.; Shi, Z.; Deng, Y.; Sun, J.; Wang, H. Morphology-dependent electrochemical sensing properties of manganese dioxide–graphene oxide hybrid for guaiacol and vanillin. *Electrochim. Acta* **2014**, *147*, 157–166. [[CrossRef](#)]
57. Li, G.; Wang, S.; Duan, Y.Y. Towards conductive-gel-free electrodes: Understanding the wet electrode, semi-dry electrode and dry electrode-skin interface impedance using electrochemical impedance spectroscopy fitting. *Sens. Actuators B Chem.* **2018**, *277*, 250–260. [[CrossRef](#)]
58. Li, G.; Wang, S.; Duan, Y.Y. Towards gel-free electrodes: A systematic study of electrode-skin impedance. *Sens. Actuators B Chem.* **2017**, *241*, 1244–1255. [[CrossRef](#)]
59. Li, G.; Zhang, D.; Wang, S.; Duan, Y.Y. Novel passive ceramic based semi-dry electrodes for recording electroencephalography signals from the hairy scalp. *Sens. Actuators B Chem.* **2016**, *237*, 167–178. [[CrossRef](#)]
60. Wang, J.; Yang, B.; Zhong, J.; Yan, B.; Zhang, K.; Zhai, C.; Shiraishi, Y.; Du, Y.; Yang, P. Dopamine and uric acid electrochemical sensor based on a glassy carbon electrode modified with cubic Pd and reduced graphene oxide nanocomposite. *J. Colloid Interface Sci.* **2017**, *497*, 172–180. [[CrossRef](#)] [[PubMed](#)]

61. Xu, T.Q.; Zhang, Q.L.; Zheng, J.N.; Lv, Z.Y.; Wei, J.; Wang, A.J.; Feng, J.J. Simultaneous determination of dopamine and uric acid in the presence of ascorbic acid using Pt nanoparticles supported on reduced graphene oxide. *Electrochim. Acta* **2014**, *115*, 109–115. [[CrossRef](#)]
62. Kogularasu, S.; Akilarasan, M.; Chen, S.-M.; Chen, T.W.; Lou, B.S. Urea-based morphological engineering of ZnO; for the biosensing enhancement towards dopamine and uric acid in food and biological samples. *Mater. Chem. Phys.* **2019**, *227*, 5–11. [[CrossRef](#)]
63. Teo, P.S.; Alagarsamy, P.; Huang, N.M.; Lim, H.N.; Yusran, S. Simultaneous electrochemical detection of dopamine and ascorbic acid using an iron oxide/reduced graphene oxide modified glassy carbon electrode. *Sensors* **2014**, *14*, 15227–15243.
64. Zhang, K.; Chen, X.; Li, Z.; Wang, Y.; Sun, S.; Wang, L.N.; Guo, T.; Zhang, D.; Xue, Z.; Zhou, X. Au-Pt bimetallic nanoparticles decorated on sulfonated nitrogen sulfur co-doped graphene for simultaneous determination of dopamine and uric acid. *Talanta* **2018**, *178*, 315–323. [[CrossRef](#)] [[PubMed](#)]
65. Liu, Y.; She, P.; Gong, J.; Wu, W.; Xu, S.; Li, J.; Zhao, K.; Deng, A. A novel sensor based on electrodeposited Au-Pt bimetallic nano-clusters decorated on graphene oxide (GO)-electrochemically reduced GO for sensitive detection of dopamine and uric acid. *Sens. Actuators B Chem.* **2015**, *221*, 1542–1553. [[CrossRef](#)]
66. Yang, Z.; Zheng, X.; Zheng, J. A facile one-step synthesis of Fe₂O₃/nitrogen-doped reduced graphene oxide nanocomposite for enhanced electrochemical determination of dopamine. *J. Alloys Compd.* **2017**, *709*, 581–587. [[CrossRef](#)]
67. Ghanbari, K.; Moloudi, M. Flower-like ZnO decorated polyaniline/reduced graphene oxide nanocomposites for simultaneous determination of dopamine and uric acid. *Anal. Biochem.* **2016**, *512*, 91–102. [[CrossRef](#)] [[PubMed](#)]
68. Mei, L.P.; Feng, J.J.; Wu, L.; Chen, J.R.; Shen, L.; Xie, Y.; Wang, A.J. A glassy carbon electrode modified with porous Cu₂O nanospheres on reduced graphene oxide support for simultaneous sensing of uric acid and dopamine with high selectivity over ascorbic acid. *Microchim. Acta* **2016**, *183*, 2039–2046. [[CrossRef](#)]
69. Asif, M.; Aziz, A.; Wang, H.; Wang, Z.; Wang, W.; Ajmal, M.; Xiao, F.; Chen, X.; Liu, H. Superlattice stacking by hybridizing layered double hydroxide nanosheets with layers of reduced graphene oxide for electrochemical simultaneous determination of dopamine, uric acid and ascorbic acid. *Microchim. Acta* **2019**, *186*, 61. [[CrossRef](#)]
70. Sumathi, C.; Venkateswara Raju, C.; Muthukumaran, P.; Wilson, J.; Ravi, G. Au-Pd bimetallic nanoparticles anchored on α -Fe₂O₃ nonenzymatic hybrid nanoelectrocatalyst for simultaneous electrochemical detection of dopamine and uric acid in the presence of ascorbic acid. *J. Mater. Chem. B* **2016**, *4*, 2561–2569. [[CrossRef](#)]



© 2019 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<http://creativecommons.org/licenses/by/4.0/>).