

1 **Title**

2 Learning to use landmarks for navigation amplifies their representation in retrosplenial
3 cortex.

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5 **Authors and Affiliations**

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14

15 **Abstract**

16 Visual landmarks provide powerful reference signals for efficient navigation by altering
17 the activity of spatially tuned neurons, such as place cells, head direction cells, and grid
18 cells. To understand the neural mechanism by which landmarks exert such strong
19 influence, it is necessary to identify how these visual features gain spatial meaning. In
20 this study, we characterized visual landmark representations in mouse retrosplenial
21 cortex (RSC) using chronic two-photon imaging of the same neuronal ensembles over
22 the course of spatial learning. We found a pronounced increase in landmark-referenced
23 activity in RSC neurons that, once established, remained stable across days. Changing
24 behavioral context by uncoupling treadmill motion from visual feedback systematically
25 altered neuronal responses associated with the coherence between visual scene flow
26 speed and self-motion. To explore potential underlying mechanisms, we modeled how
27 burst firing, mediated by supralinear somatodendritic interactions, could efficiently
28 mediate context- and coherence-dependent integration of landmark information. Our
29 results show that visual encoding shifts to landmark-referenced and context-dependent
30 codes as these cues take on spatial meaning during learning.

31

32 **Introduction**

33 Precise and reliable spatial navigation is critical for the survival of most mammals
34 and has an accordingly prominent representation in the brain, spread across multiple
35 areas (Vann, Aggleton, and Maguire 2009; Fischer et al. 2020). Spatial navigation is
36 guided by self-localization based on internal movement estimates combined with sensory
37 inputs that allow animals to locate themselves in the environment. Landmarks are sensory
38 cues that can be used to inform an agent about its location within a given spatial context
39 (E Save and Poucet 2000; Etienne et al. 2000; Biro et al. 2007; Julian et al. 2018). For a
40 sensory stimulus to act as a landmark, it must first be associated with spatial meaning
41 (Epstein et al. 2017; Gothard and Skaggs 1996; Chan et al. 2012; Taube and Burton
42 1995; Jeffery 1998). Once the spatial meaning of a landmark in a given environment has
43 been learned, subsequent exposures to the landmark allow current self-localization
44 estimates to be corrected (Etienne, Maurer, and Séguinot 1996; Campbell et al. 2018;
45 Knierim, Kudrimoti, and McNaughton 1998; Gothard, Skaggs, and McNaughton 1996).
46 How environmental cues are integrated into neural codes of space is an important but
47 poorly understood process that remains a key unanswered question for the field of
48 navigation, and which could shed light on the mechanisms underlying navigational deficits
49 in Alzheimer's disease and dementia.

50 Converging evidence points to retrosplenial cortex (RSC) as an important locus for
51 landmark processing (Vann, Aggleton, and Maguire 2009; Etienne, Maurer, and Séguinot
52 1996; Gothard and Skaggs 1996; Jeffery 1998; Auger, Mullally, and Maguire 2012; Jacob
53 et al. 2017; Fischer et al. 2020; Mao et al. 2020). Neurons in RSC have been shown to
54 encode a range of egocentric and allocentric encoding properties, making it an ideal locus
55 for landmark processing (Alexander and Nitz 2017; 2015; Vedder et al. 2016; Mao et al.
56 2020; 2017). During spatial navigation, RSC neurons represent visual landmarks via
57 nonlinear integration of self-motion and visual inputs (Fischer et al. 2020). Recordings in
58 freely moving rats have shown that individual RSC neurons conjunctively encode space
59 in egocentric and allocentric spatial reference frames (Alexander and Nitz 2015).
60 Complementary evidence from freely rotating head-fixed mice indicate that top-down
61 dendritic computations are engaged in this process (Voigts and Harnett 2020). These

62 properties suggest that RSC is a key node in processing sensory inputs for effective
63 landmark-mediated self-localization.

64 However, a physiologically plausible mechanistic understanding of how neurons
65 learn the spatial meaning of landmarks over the course of exploring an environment is
66 missing. Previous studies show an interplay between primary visual cortex and RSC
67 during landmark-dependent navigation (Fischer et al. 2020; Campbell et al. 2018). Other
68 experiments indicate that RSC encodes self-motion information (e.g. how many steps
69 have I taken?), as well as world-referenced inputs (e.g. where in my field of vision is a
70 wall?) (Mao et al. 2020; 2017; Julian et al. 2018). To effectively utilize landmarks, RSC
71 must generate accurate self-localization estimates by combining these two sources of
72 information. Neural networks in RSC are therefore subject to conflicting demands in order
73 to reconcile self-localization estimates with sensory inputs. Internal location
74 representations need to be continuous and resist sudden jumps to provide reliable
75 estimates, even during times of scarce external information, such as low-light conditions
76 (McNaughton et al. 1996; Moser, Kropff, and Moser 2008). Sensory processing, in
77 contrast, must rapidly encode inputs to allow quick responses to novel or unexpected
78 stimuli (D. A. Evans et al. 2018; Carandini and Churchland 2013). How these different
79 coding regimes interact to provide continuous and accurate position estimates is currently
80 poorly understood (T. Evans et al. 2016; Angelaki and Laurens 2020). We hypothesized
81 that neurons in RSC alter the balance of self-referenced or world-reference codes
82 depending on which source of information provides a more accurate self-localization
83 signal in the current environment.

84 To address this question, we recorded longitudinally from the same RSC neurons
85 as mice learned a landmark-dependent navigation task using 2-photon imaging. We used
86 a generalized linear model (GLM) to evaluate the contribution(s) of self-referenced versus
87 world-referenced factors to the activity of individual neurons over the course of learning.
88 We then assessed neuronal activity in different behavioral contexts to characterize the
89 properties of landmark signals in RSC. Based on our experimental data we developed a
90 proof-of-principle model that uses a putative cellular mechanism for landmark-mediated
91 error correction during navigation. Our results show that individual neurons in RSC shift
92 their activity patterns to allow efficient landmark-mediated self-localization.

93 **Results**

94 *RSC neurons transition from self-referenced to landmark-referenced spatial codes while*
95 *learning a visual landmark navigation task.*

96 We trained mice to perform a virtual landmark navigation task (Fischer et al. 2020). Briefly,
97 head-fixed mice learned to lick for water rewards at one of two different unmarked reward
98 locations associated with two distinct visual landmarks along a virtual corridor (Fig. 1A,
99 Fig. S1A-C). The virtual corridor consisted of a floor and two walls that contained non-
100 location-specific patterns that provided optic flow but no other spatial information. Each
101 trial started at a randomized location between 50 to 150 cm before a landmark. By licking
102 within the (unindicated) reward zone, mice could trigger water delivery. In-between trials,
103 mice spent at least 3 seconds in a featureless ‘black box.’

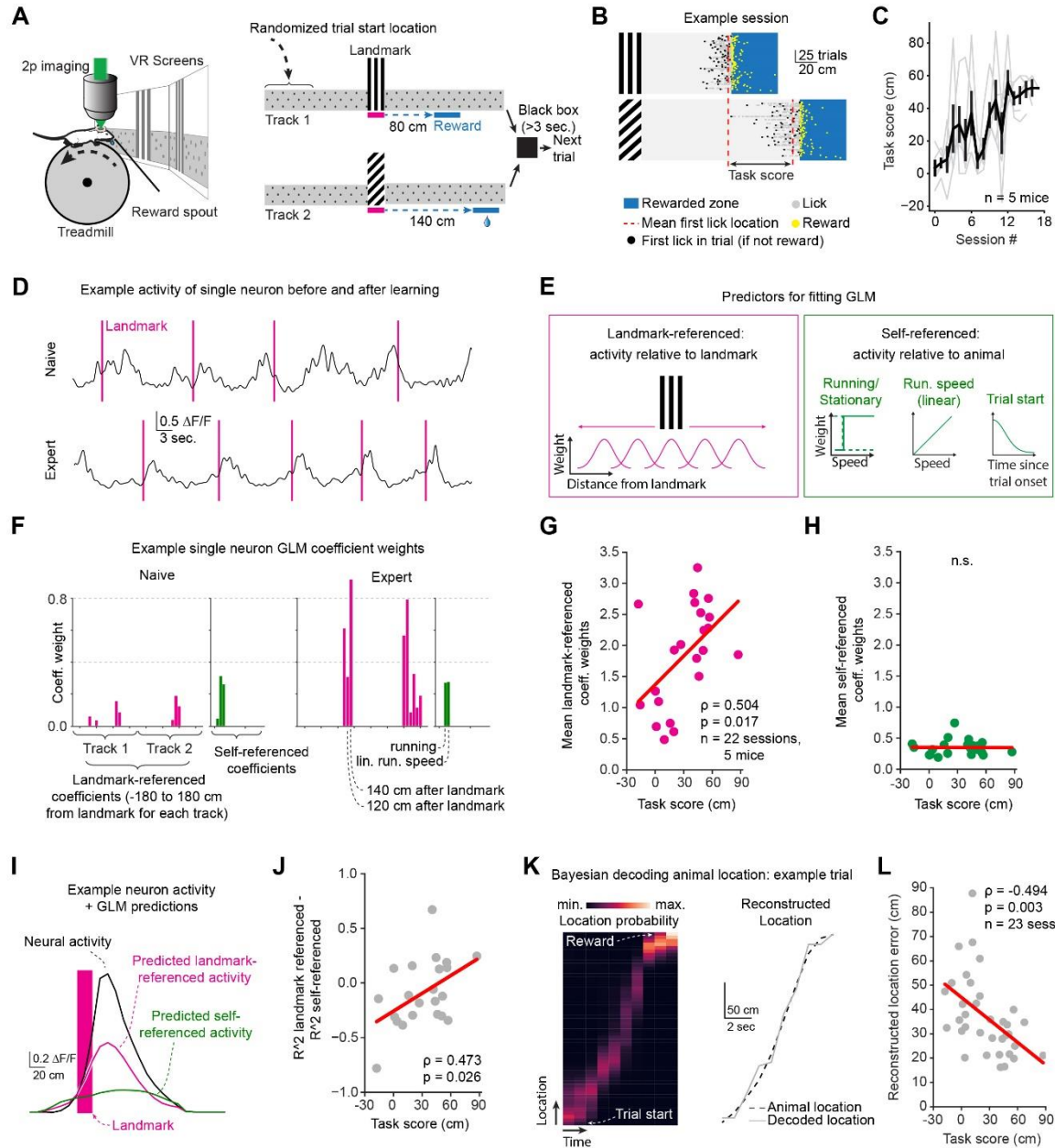
104 The mean distance between the first lick location on each track in a given session
105 was used as a behavioral readout for task proficiency (Fig. 1B, C, Fig. S1B). Two-photon
106 GCaMP6f imaging of layer 2/3 (L2/3) RSC neurons was carried out on 35/85 interspersed
107 sessions (n=5 mice) sessions: the other 50/85 sessions were behavior only training
108 sessions (Fig. 1D). A subset of individual neurons were tracked 22 of the 35 sessions
109 (mean \pm SEM: 35.14 \pm 1.86 tracked cells/session). To do so, we matched the spatial
110 footprints of neurons between a reference session and a second session using the
111 CellReg algorithm (Sheintuch et al. 2017) in conjunction with manual curation (see
112 Methods and Fig. S2A-C).

113 We applied a generalized linear model (GLM) to quantify which behavioral
114 variables each neuron encoded in each session as animals learned the task. The GLM
115 included two categories of predictors: landmark-referenced and self-referenced. Self-
116 referenced predictors captured behavioral variables relative to the animal, while
117 landmark-referenced predictors related to locations relative to the landmark (Fig. 1E, Fig.
118 S1F). The GLM was fit to the GCaMP fluorescence signals using elastic net regularization
119 (Friedman, Hastie, and Tibshirani 2010) ($\alpha=0.5$, see Methods for details, Fig. S3A).
120 Coefficient weights showed an increase in the weight of landmark-referenced predictors
121 over the course of learning (Fig. 1F-H, Fig. S1D, E; Pearson correlation $\rho=0.504$,
122 $p=0.017$, n=22 sessions, 5 animals, mean \pm SEM: 35.1 \pm 1.9 tracked neurons/session).
123 These results were in line with previously reported results (Fischer et al. 2020). Further

124 analysis showed that neither the number of non-zero coefficients, peak fluorescence
125 signal, nor trial-by-trial robustness of responses changed over the course of learning.
126 However, neuron activity increased overall (Fig. S3E-H). Predicting neural activity using
127 only landmark-referenced or only self-referenced predictors showed small but significant
128 increases in model fit (explained variance R^2 ; Fig. 1I,J, Pearson correlation $\rho=0.473$,
129 $p=0.026$), despite the overall explained variance not changing significantly (Fig. S3D) and
130 running speeds remaining largely similar (Fig. S3L). The same relationships held true
131 when all neurons in all recorded sessions, rather than just neurons that were tracked
132 across sessions, were included in this analysis (Fig. S3B, C).

133 We next evaluated how well RSC neurons encoded space by decoding the
134 animal's location relative to the landmark using population activity. For this analysis we
135 used all recorded neurons in a given session (mean \pm SEM: 75.51 ± 3 neurons/session).
136 We found a significant decrease in reconstruction error as task proficiency increased,
137 suggesting that landmark-anchored spatial codes increase with the animal's ability to use
138 landmarks for navigation (Fig. 1K, L, Fig. S2I-K; Pearson correlation $\rho=-0.494$, $p=0.003$).
139 Together, our results show a significant correlation in RSC neurons between the
140 representation of landmark-referenced activity and proficiency in using landmarks for
141 navigation. This indicates that RSC neurons shift their encoding priorities as a function of
142 task demands.

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145 **Figure 1: RSC neurons transition from self-referenced to landmark-referenced spatial**
 146 **codes while learning a visual landmark navigation task.**

147 (A) Experimental setup (left) and task schematic (right). Animals had to traverse a virtual linear
 148 corridor and locate an unmarked reward zone relative to one of two visual landmarks that were
 149 randomized on a trial-to-trial basis ('Track 1' and 'Track 2'). Animals were then "teleported" to a
 150 black box for >3 seconds and subsequently to a randomized start location for the next trial. (B)
 151 Raster plot of licking behavior relative to the respective landmarks. (C) The performance metric
 152 (task score) was calculated as the median distance between licking onset on Track 1 and Track
 153 2. (D) GCaMP fluorescence of an example neuron over multiple trials before and after learning
 154 the task (task score > 20 cm). Purple vertical lines indicate when the animal passed the landmark.
 155 (E) Predictors used to fit a generalized linear model (GLM). Predictors were categorized into two
 156 groups: 1) landmark-referenced (anchored to spatial locations relative to the landmark) and 2)

157 self-referenced to the animal. **(F)** Coefficient weights of the example neuron shown in (D) before
158 and after learning. **(G)** Mean landmark-referenced coefficient weights over the course of learning.
159 **(H)** Same as (G) but for self-referenced coefficients. **(I)** Average activity of an example neuron as
160 a function of location relative to the landmark (black trace) as well as activity predicted by GLM
161 using either landmark (purple) or self-referenced (green) coefficients only. **(J)** Variance explained
162 (R^2) by prediction of neural activity using only landmark-referenced coefficients and self-
163 referenced coefficients as a function of task score. **(K)** Example trial using a Bayesian decoder to
164 estimate animal position based on neural activity. Left: Probability density function of location
165 estimate for each time bin. Right: Reconstructed location (grey) versus actual location (black). **(L)**
166 Mean position reconstruction error as a function of task score across all animals and sessions.

167 *Visual inputs stabilize spatial codes in RSC.*

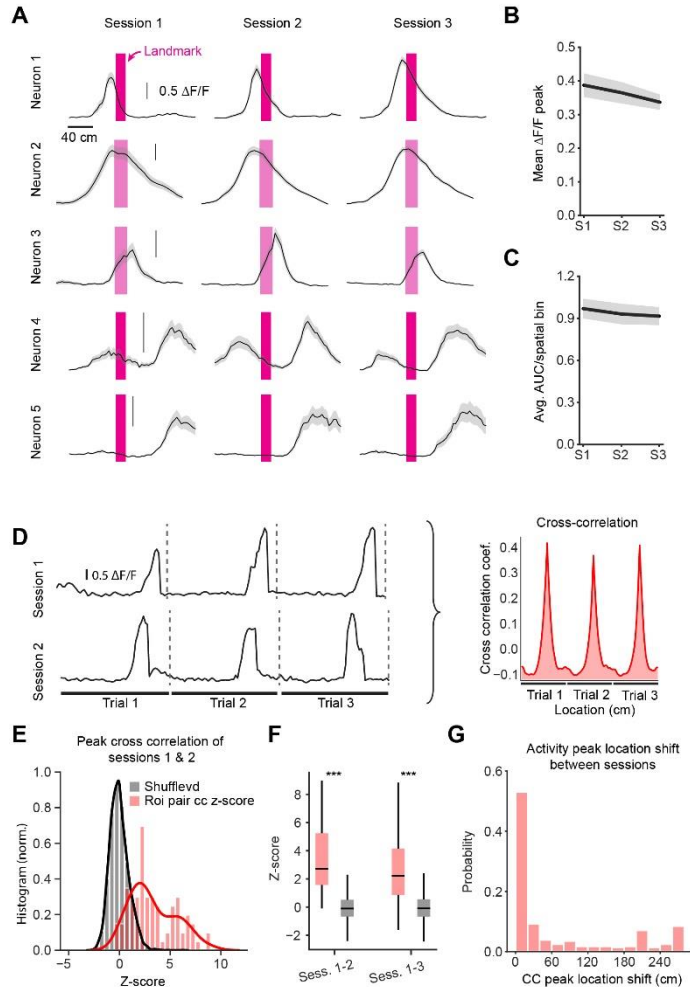
168 We next asked how stable landmark representations in RSC are over time. Persistent
169 codes allow for stable output to downstream structures, while variable population activity
170 indicates that organizational principles are embedded in higher-order network dynamics
171 (Quiari Quiroga and Panzeri 2009; Haider et al. 2016; Ujfalussy et al. 2015; Remington
172 et al. 2018). Previous work has shown that spatial codes of individual RSC neurons vary
173 day-by-day in the absence of location-specific visual inputs (Mao et al. 2018). We
174 therefore asked whether learning visual landmark cues can stabilize neuronal
175 representations across days. We tested the persistence of landmark-referenced codes in
176 RSC by tracking the same neurons over three expert sessions (task score > 20 cm; Fig.
177 2A & Fig. S2A-C). The task score threshold of 20 cm was empirically chosen to indicate
178 when mice began reliably using landmarks to locate rewards. These sessions constitute
179 a subset of the sessions shown in Fig. 1. Peak responses (calculated as the peak average
180 $\Delta F/F$ across all trials along the track) and the area under the curve of all tracked neurons
181 ($n = 169$ neurons from 5 animals) did not change significantly across days (Fig. 2B, C;
182 One-way ANOVA, $p=0.5$ for $\Delta F/F$ peak, $p = 0.8$ for AUC/spatial bin).

183 To test if neurons retained their spatial tuning, we quantified the cross correlation
184 of each neuron's activity as a function of location on the track. The cross-day cross-
185 correlation was calculated by concatenating the activity of a given neuron on all trials
186 where a given landmark was shown and finding the highest peak in the cross-correlogram
187 (Fig. 2D). Neural activity in the black box between trials and after reward delivery was
188 removed from this analysis. Neurons with an R^2 value smaller than 0.25 were not included

189 in this analysis to remove neurons with little-to-no landmark- or self-referenced activity.
190 In total, 156 neurons (out of 169 tracked neurons) from 5 mice were used in this analysis.

191 To test whether individual neurons were significantly cross-correlated across days,
192 a shuffled distribution of cross-correlation values was calculated for each neuron by
193 rotating its neural activity by a random amount for each trial and re-calculating the cross-
194 correlation. We used this shuffled null distribution to compare trial-by-trial activity
195 correlations of individual neurons to spatially-randomized activity. The z-score relative to
196 the shuffled distribution was then calculated (Fig. 2E). We found that landmark-referenced
197 codes across three consecutive sessions were stable (Fig. 2F; median z-score for
198 correlation between sessions 1-2: 2.72, IQR: 3.67; session 1-3: 2.21, IQR: 3.29, unpaired
199 two-tailed T-test: $p < 0.0001$ for all comparisons, see Fig. S4A for non-z-scored cross
200 correlation values). Finally, we analyzed the peak-shift in cross correlation (Fig. 2G). The
201 peak-shift analysis revealed a median shift of 15 cm (IQR: 135 cm), suggesting that the
202 vast majority of neurons retain their spatial tuning. These results indicate that
203 behaviorally-relevant anchoring visual cues can stabilize spatial codes in the cortex.

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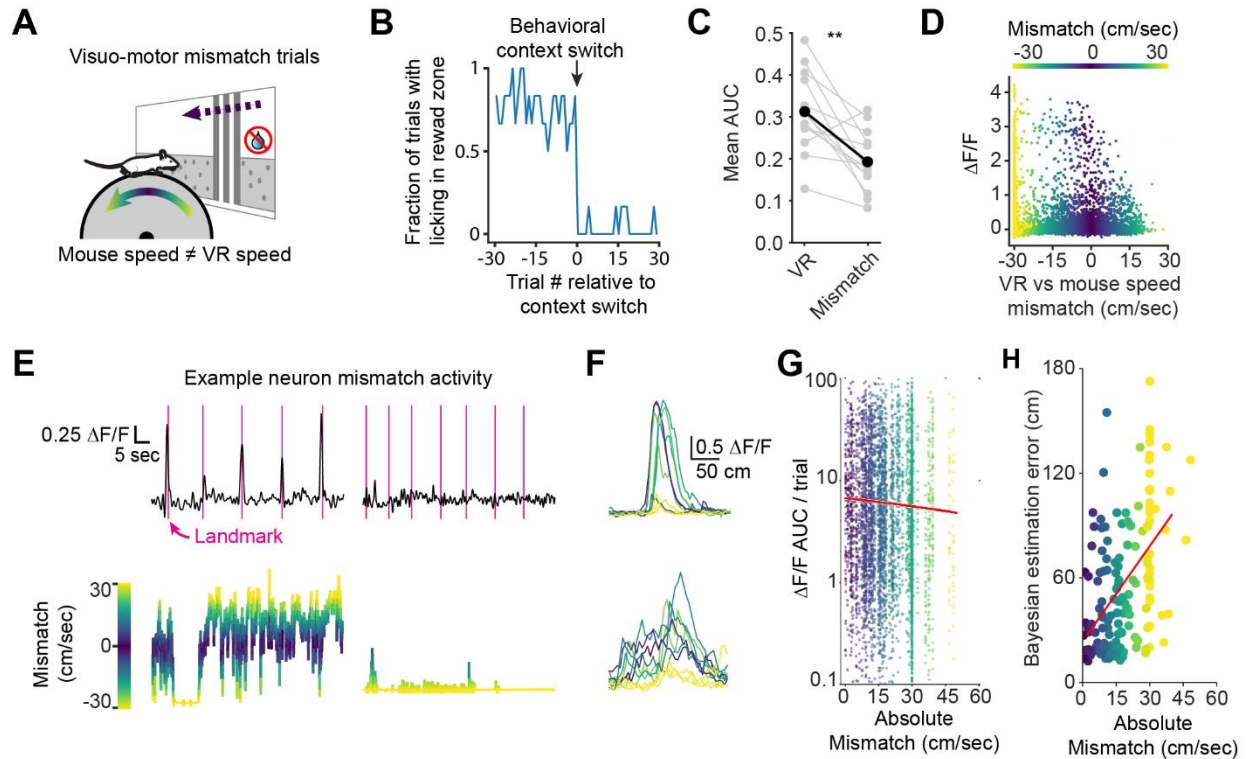
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 207 **Figure 2: RSC neuron spatial codes stabilize after learning in the presence of visual cues.**
 208 (A) Trial-averaged activity of five example neurons as a function of location on the track. All
 209 vertical scale bars indicate 0.5 $\Delta F/F$. (B) Mean peak $\Delta F/F$ for all tracked neurons across three
 210 sessions. (C) Same as (B) but for area under the curve (AUC) calculation. One-way ANOVA
 211 indicates no significant difference between days. (D) Schematic of cross-correlation calculation
 212 between sessions. For each neuron, the cross correlation between sessions was calculated
 213 from spatially binned activity with periods in-between trials removed. (E) Histogram of the z-
 214 score of each neuron's cross-correlation value relative to a shuffled distribution. (F) Z-score
 215 boxplot for first vs. second and first vs. third session. (G) Probability of cross-correlation peak
 216 location shift.
 217

218 *RSC neurons are most active when visual flow and self-motion signals are coherent.*

219 Context-dependent processing of sensory inputs is a cornerstone of cortical function
220 (Mante et al. 2013; Smith, Barredo, and Mizumori 2012; Mao et al. 2017). A number of
221 studies have reported a general decrease in activity and spatial specificity during visuo-
222 motor mismatch conditions in cortex (Harvey, Coen, and Tank 2012; Fischer et al. 2020;
223 Diamanti et al. 2019; Mao et al. 2020). However, a more detailed understanding of the
224 patterns of activity changes can provide clues as to how visual and motor information is
225 integrated. We hypothesized that RSC neurons implement context-sensitive codes by
226 associating self-motion with visual motion cues in a given environment. This allows
227 sensory cues to be differentially encoded depending on the behavioral context in which
228 they are encountered. To test this hypothesis, we introduced visuo-motor mismatch trials
229 in which virtual movement was uncoupled from animal running (Fig. 3A). During these
230 mismatch trials, the virtual corridor moved at a constant speed of 30 cm/sec, independent
231 of running behavior. The reward zone was in the same virtual location and, though licking
232 behavior was still recorded, no rewards were dispensed. A brief trial break (approx. 30
233 sec.) between VR and visuo-motor mismatch sessions signaled the behavioral context
234 switch. Mice ceased to lick in the rewarded zone soon after the switch to the visuo-motor
235 mismatch session (Fig. 3B), behavioral confirmation that they recognized the change.
236 Congruent with previous data (Fischer et al. 2020), neural activity overall was lower during
237 the visuo-motor mismatch session compared to when the animal was actively executing
238 the task (Fig. 3C; mean \pm SEM VR: 0.31 ± 0.03 , visuo-motor mismatch: 0.19 ± 0.02 ,
239 paired, two-tailed T-test: $p=0.001$, $n=13$ sessions, 5 naïve and 8 expert with a task score
240 >20 cm, $n=5$ mice).

241 We analyzed neural activity in visuo-motor mismatch sessions as a function of the
242 difference between the visual flow speed and the animal's running speed on the treadmill
243 in expert animals (Fig. 3D). To account for linear speed modulation of neural activity, we
244 fit a linear regression to the activity of each neuron as a function of speed and subtracted
245 the corresponding linear factor (see Methods). We found a tendency for neurons to be
246 most strongly activated when the movement speed of the displayed corridor matched the
247 animal's own running speed (Fig. 3E,F, Fig. S5A). To quantify the relationship between
248 visuo-motor mismatch and neural activity, we calculated the integrated calcium activity of

249 each neuron on each trial as a function of the absolute visuo-motor mismatch. This
250 revealed a modest negative correlation, suggesting that neurons are most active when
251 visuo-motor mismatch was smallest (Fig. 3G, Spearman rank correlation: $\rho=-0.036$,
252 $p=0.0017$; the same relationship held true when we did not correct for linear speed, Fig.
253 S5C). No relationship between running speed and neural activity was found while animals
254 were in the black box in-between trials (Fig. S5B). We reasoned that the relationship
255 between mismatch and neural activity should translate into improved spatial coding when
256 running and visual flow speed match, and vice versa, if the mismatch is large, spatial
257 coding should be disrupted. To test this, we trained a Bayesian decoder on neural data
258 collected during virtual navigation in trained animals (task score > 20 cm) and used it to
259 estimate the mouse's location during visuo-motor mismatch trials. Reconstruction error
260 was smallest when the difference in animal running speed and visual flow speed was
261 around zero (Fig. 3H, Spearman rank correlation: $\rho=-0.474$, $p<0.001$). These results
262 indicate that RSC neurons are functionally organized to most strongly represent visual
263 feedback when coordinated with self-motion, thus providing evidence for behavioral-
264 context representation that is based on reconciling internal and external cues for self-
265 localization.
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Figure 3: Behavioral context modulates RSC neuronal response strength and spatial coding.

(A) Visuo-motor mismatch experiment schematic: virtual corridor flow speed (30 cm/sec) versus animal running speed was measured in relation to neuronal responses. (B) Fraction of trials with at least one lick in the reward zone. (C) Mean GCaMP6f $\Delta F/F$ signal area under the curve (AUC) per 5 cm spatial bin during VR and visuo-motor mismatch periods. (D) $\Delta F/F$ of an example neuron as a function of mismatch. Each dot represents the signal of one recorded frame. Color code indicates speed mismatch. (E) Example GCaMP6f $\Delta F/F$ traces of one neuron (top) and the difference in animal running and virtual corridor flow speed (Δ Speed; below) during two sets of trials (left: 5 trials where the animal was locomoting, right: 7 trials where the animal was quiescent). (F) GCaMP6f activity of two example neurons during visuo-motor mismatch session. Each trace represents one trial with the color code indicating the difference in average running and virtual corridor flow speed for that trial. (G) Integrated $\Delta F/F$ of each trial as a function of speed mismatch for all neurons and all trials of $n=8$ expert sessions. Each trial of a given neuron is represented by one dot. Red line: linear fit. (H) Location reconstruction error using a Bayesian decoder that was trained on virtual navigation data and applied to visuo-motor mismatch trials ($n=8$ expert sessions). Red line: linear fit.

286 *Bursting firing mediated by dendrites can accurately correct self-localization estimates.*

287 Our experimental results show that RSC neurons develop stable, landmark-referenced
288 codes over learning that are modulated by behavioral context. We hypothesized that
289 individual neurons could generate these landmark codes by integrating visual bottom-up
290 inputs with contextual top-down signals. Recent work has shown that RSC receives
291 spatially segregated inputs from thalamic, primary visual, and associative cortices
292 (Lafourcade et al. 2022). We reasoned that the generation of bursts of action potentials
293 generated by coincident bottom-up somatic and top-down dendritic inputs (Naud and
294 Sprekeler 2018; Payeur et al. 2021; Xu et al. 2012; Ranganathan et al. 2018; Bicknell and
295 Häusser 2021; Takahashi et al. 2016; Francioni and Harnett 2021; London and Häusser
296 2005; Larkum, Kaiser, and Sakmann 1999; Larkum 2013; Greedy et al. 2022; Fişek et al.
297 2023) could underlie the amplification of sensory inputs by behavioral context we have
298 observed in our data. We therefore created a model to explore how somatodendritic
299 interactions in pyramidal neurons could potentially be utilized to provide context-
300 dependent self-localization.

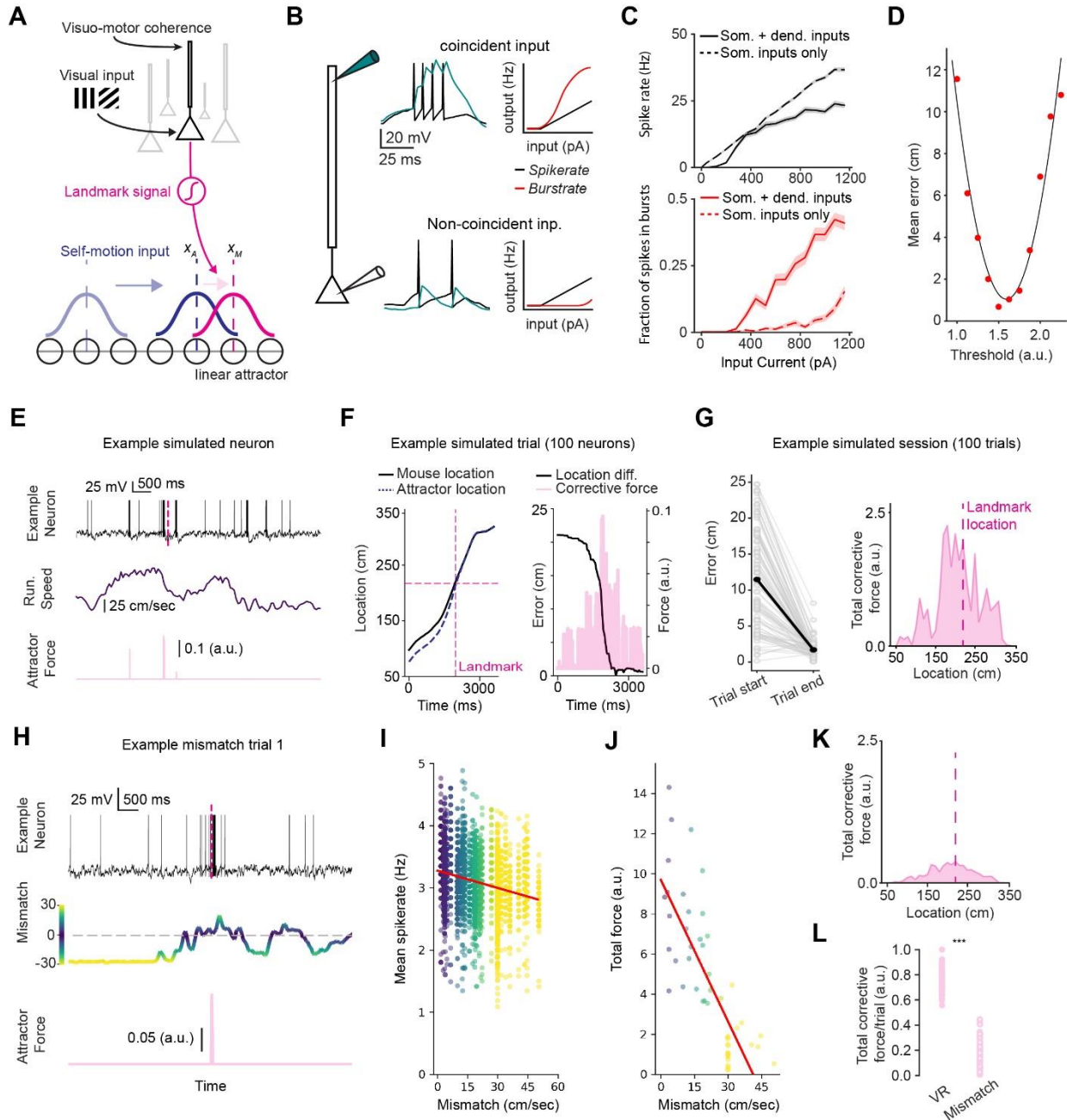
301 Our model combined multi-compartment spiking neurons developed by Naud and
302 Sprekeler (2018) with an attractor model representing an agent's self-localization
303 estimate (Ocko et al. 2018). We adjusted the parameters of neurons compared to (Naud
304 and Sprekeler 2018), which consisted of a somatic and a dendritic compartment (Fig.
305 4A,B). The biophysical properties of each compartment endowed these neurons with the
306 ability to generate bursts of action potentials, but only when somatic and dendritic inputs
307 coincided (Fig. 4B,C) (Naud and Sprekeler 2018). The multi-compartment neurons sent
308 output to a linear attractor (Fig. 4A, Fig. S6A), which represented the agent's self-
309 localization estimate by a Gaussian activity bump centered at the best current location
310 estimate (Zhang 1996; Campbell et al. 2018; Ocko et al. 2018). Each neuron received
311 visual inputs at a location relative to the landmark. The location relative to the landmark
312 was drawn from a Gaussian distribution (Fig. S8A). Even though visual landmark inputs
313 cease after the animal has passed the landmark, in this model some visual inputs indeed
314 have their receptive field center after the landmark. This is consistent with previous
315 findings (Fischer et al. 2020) and is further supported by the rich responses primary visual
316 cortex is known to generate (Saleem et al. 2018; Niell and Stryker 2010; Musall et al.

317 2019; Pakan et al. 2018). Visual landmark inputs were modeled as somatic input currents
318 that scaled as a function of distance to its respective receptive field center.

319 Each neuron also received input into its dendritic compartment as a function of
320 coherence between self-motion and visual flow feedback (visuo-motor coherence; Fig.
321 4A). Both compartments received constant noise inputs (see Methods) that resulted in
322 stochastic background spiking. The combination of bottom-up feedforward and top-down
323 feedback inputs resulted in an increased propensity for neurons to burst. In contrast,
324 neurons receiving an equivalent total amount of current injected into the somatic
325 compartment alone emitted significantly fewer bursts (Fig. S6B). Each spike emitted by a
326 landmark neuron exerted a rapidly decaying force on the attractor via a sigmoidal
327 activation function that incorporated a gating threshold (Fig. 4A; Methods) that corrected
328 the self-localization estimate towards its respective receptive field center. This rapid
329 decay acted as a filter that prevented the self-localization estimate from erroneously
330 changing due to background noise. To test this, we ran a series of simulations with
331 increasing gating threshold values (Fig. 4D). While a low threshold value meant single
332 spikes pull the attractor away from the agent's actual location, higher thresholds
333 prevented any error correction altogether. Our fit showed an optimal range between 1.4
334 and 1.8. We used 1.75 for all subsequent simulations.

335 We then used behavioral data from our experimental recording sessions to
336 simulate 100 trials of the landmark navigation task (from Fig. 1) with 100 simulated
337 neurons whose activity was anchored by the landmark ("landmark neurons"). Each trial
338 started with a random initial offset between the self-localization estimate and the agent's
339 actual location. As the agent traversed the linear corridor, the combined force generated
340 by neurons corrected the self-localization estimate (Fig. 4E-G, Fig. S8B; mean final error:
341 1.7 ± 0.11 cm. Paired t-test: $p < 0.001$; mean corrective force AUC \pm SEM: 225.11 ± 2.62).
342 In contrast, running the same simulation without coincident somatodendritic inputs
343 resulted in significantly worse error correction (Fig. S6C-E, Fig. S8C). These simulations
344 show that bursts of actional potentials generated by somatodendritic interactions are a
345 robust way to generate corrective inputs for self-localization estimates.

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349 **Figure 4: Somatodendritic bursting in a hybrid simulated neural network enables**
350 **accurate location error correction.**
351 (A) Simulation components. Each landmark neuron is connected onto the attractor at its
352 respective spatial receptive field center. (B) Schematic of spikes and bursts generated as a
353 function of somatic and dendritic inputs. Bursts are defined as 2 or more spikes with an
354 interspike interval <10 ms. (C) Spike and burst rates in response to increasing current inputs.
355 (D) Agent self-localization error correction during simulated trials as a function of threshold
356 between neurons and attractor. Each red dot represents a set of simulated trials at a given
357 threshold value, black line is a 2nd order polynomial fit. (E) Example simulated trial. Top:
358 example neuron activity. The landmark is indicated by the dashed lines. Middle: running speed
359 in simulated trial. Bottom: force applied to attractor by example neuron. (F) Left: Actual location

360 (solid line) and self-localization estimate of attractor (dashed line). Right: Self-localization error
361 (calculated as actual location minus attractor activity bump location) and corrective force applied
362 to the attractor by 100 landmark neurons. **(G)** Left: Error at the beginning and at the end of 100
363 simulated trials. Right: Total force applied to the attractor by all landmark neurons combined. **(H)**
364 Activity traces of an example neuron during visuo-motor mismatch. Neural activity is shown
365 above the respective speed mismatch (color coded) and the force exerted by that neuron on the
366 attractor (pink). **(I)** Mean spike rate per trial as a function of visuo-motor mismatch speed. Each
367 dot represents one trial of one neuron. **(J)** Force exerted on attractor. **(K)** Total force exerted by
368 landmark neurons on the attractor during mismatch trial simulation. **(L)** Force exerted onto
369 attractor during simulated virtual navigation (“VR”) and visuo-motor mismatch trials
370 (“Mismatch”).

371 *Somatodendritic interactions can support context-dependent computations.*

372 Our experimental data indicate that mouse RSC exhibits different sensory cue integration
373 regimes during virtual navigation and visuo-motor mismatch sessions. We tested if our
374 model could recapitulate these findings by simulating 100 visuo-motor mismatch trials.
375 Consistent with our virtual navigation simulation, we used behavioral data from our mouse
376 experiments. We reasoned that visual landmark inputs do not influence downstream
377 neural representations during visuo-motor mismatch, as they are not relevant to ongoing
378 behavior, and they should therefore exert minimal force. We modeled dendritic inputs as
379 a visuo-motor coherence signal which was dependent on the difference in agent running
380 and VR flow speed. The virtual environment was shown at a constant flow speed of 30
381 cm/sec while mice were free to sit or run on the treadmill. Similar to observations made
382 in biological neurons during this task (Fig. 3), the activity of model neurons was highest
383 when animal running speed approximately matched visual flow speed leading to
384 increased force exerted on the attractor (Fig. 4H-J, Spearman rank correlation for spike
385 rate: $\rho = -0.263$, $p < 0.001$, for force exerted: $\rho = -0.799$, $p < 0.001$). Overall, the total force
386 exerted on the attractor was significantly lower compared to virtual navigation during
387 visuo-motor mismatch trials (Fig. 4K,L; mean \pm SEM VR: 225.11 ± 2.62 , Mismatch: 42.25
388 ± 3.43 , Two-tailed T-Test for related samples: $p < 0.001$). By modeling dendritic inputs as
389 visuo-motor coherence, we were thus able to implement a biophysically-plausible
390 mechanism for context-dependent sensory cue integration switching.

391 Finally, we tested if supralinear somatodendritic interactions in our model were
392 necessary for context-dependent landmark computations. We ran two simulations using
393 linearly or supralinearly integrating single-compartment variants of the previously

394 described artificial neurons (Fig. S6A,B). Both models had an otherwise identical
395 architecture. Supralinear single-compartment neurons transformed current input into
396 spiking in such a way that it mirrored that of 2-compartment neurons with coincident
397 somatodendritic inputs (Fig. S6C, top). This is achieved by multiplying input currents by
398 a factor that is dependent on the membrane potential (see Methods). Vice-versa, linear
399 single-compartment neurons matched the firing properties of 2-compartment neurons
400 without coincident inputs (Fig. S6C, bottom). The supralinear model reliably corrected the
401 agent's self-localization estimate (Fig. S6D). In contrast, the linear model did not (Fig.
402 S6E). The lack of correction in the linearly integrating model is the result of the landmark
403 neuron's inability to exert any meaningful force on the attractor (Fig. S6F; mean corrective
404 force AUC \pm SEM supralinear model: 711.05 ± 11.63 ; linear model: 0.001 ± 0.0008). This
405 is reflected in the overall correction performance over 100 trials (Fig. S6G). Importantly,
406 neither model was able to respond appropriately to the behavioral context switch. The
407 supralinear single-compartment model fired bursts consistently, regardless of behavioral
408 context (Fig. S6H; Fig. S9A,B; mean corrective force AUC \pm SEM during VR: $711.05 \pm$
409 11.63 ; during visuo-motor mismatch: 225.11 ± 2.62). In contrast, the linear model was
410 never able to correct the agent's self-localization estimate (Fig. S6I; Fig. S9C,D; mean
411 corrective force AUC \pm SEM during VR: 0.001 ± 0.0008 ; during visuo-motor mismatch:
412 $2.59 \pm 4.3 \times 10^{-6}$). Together, these results provide evidence that supralinear dendritic
413 integration in 2-compartment cortical neurons can facilitate cortical computations across
414 behavioral contexts (Tran-Van-Minh et al. 2015; Francioni and Harnett 2021; Poirazi and
415 Papoutsis 2020; Greedy et al. 2022; B. A. Richards and Lillicrap 2019; Payeur et al. 2021).
416

417 **Discussion**

418 We provide evidence for a learned, persistent, and context-dependent landmark code in
419 RSC. This code is evident in a significant increase in the encoding of landmark-referenced
420 variables over the course of task acquisition (Fig. 1) that remains stable over days (Fig.
421 2). The landmark codes are significantly attenuated when landmarks are irrelevant to
422 behavior, but appear to increase activity if external visual cues and animal behavior are
423 similar to the context in which landmark signals are important (Fig. 3). Based on our data,
424 we combined a multi-compartmental neuron model with an attractor network to evaluate
425 the plausibility of a somatodendritic mechanism in which burst firing of cortical neurons
426 mediates a corrective signal.

427 While numerous studies have shown that RSC is involved in landmark processing
428 (Fischer et al. 2020; Epstein 2008; Maguire 2001), how individual neurons adapt their
429 encoding properties while learning the spatial meaning of a landmark is unknown. We
430 show that individual RSC neurons significantly increase their encoding self-referenced
431 variables over the course of learning. Interestingly, our GLM results further indicate that
432 neurons retain some encoding of self-referenced information. This result is consistent
433 with the demands of our task, which requires animals to use landmark-referenced
434 information during self-localization as well as self-referenced information during the
435 localization of the reward after they have passed the landmark. Our results are congruent
436 with previous studies that point to conjunctive encoding of ego- and allocentric variables
437 in RSC (Alexander and Nitz 2015; Mao et al. 2020; Jacob et al. 2017). It is worth noting
438 that residual encoding of self-referenced variables may account for path-integration
439 deficits found in lesion studies of RSC (Cooper and Mizumori 2001; 1999; Elduayen and
440 Save 2014). An exciting direction for future inquiries is to gain a deeper understanding of
441 how task structure affects encoding priorities in RSC.

442 Landmark codes were stable across days in our paradigm. This contrasts with
443 previous observations of variation across days in the spatial tuning of RSC cells (Mao et
444 al. 2018). We posit that the presence of visual landmarks in our experimental design
445 underlies the cross-day stability that we have observed. This result could be related to
446 instability of other cell types that are tuned either to the environment or oneself, such as
447 place cells (Etienne Save, Nerad, and Poucet 2000; Muller and Kubie 1987), head-

448 direction cells (Taube, Muller, and Ranck 1990; Knight et al. 2014) and even grid cells
449 (Campbell et al. 2018). This speaks to the importance of visual landmarks in spatial
450 navigation. However, the exact topological organization of spatially tuned brain structures,
451 and how visual inputs are integrated during navigation, remains unknown. Our work
452 suggests that RSC is a key node in receiving and parsing behaviorally relevant visual
453 stimuli during navigation.

454 Context-dependent modulation of neural activity is a critical aspect of cortical
455 computation and has been found in nearly every region where it has been investigated
456 (Harris and Mrsic-Flogel 2013; Pakan et al. 2016; Zipser, Lamme, and Schiller 1996;
457 Ferguson and Cardin 2020). In line with previous reports in RSC (Fischer et al. 2020; Mao
458 et al. 2017; 2020; Harvey, Coen, and Tank 2012), we found a decrease in overall neural
459 activity when animals are not actively navigating. Such an overall decrease could be
460 attributed to a number of factors including overall decreased engagement or lack of
461 reward. While we cannot entirely rule out other contributing factors, our previous work
462 (Fischer et al. 2020) and our analyses here suggest that general attenuation of neural
463 activity is not the most likely explanation. Our data further showed that neuronal activity
464 increases as the mismatch between visual flow and self-motion feedback decreases. One
465 possible mechanism underlying such a context-dependent modulation could be predictive
466 coding, which may be dendrite-mediated (Rao and Ballard 1999; Leinweber et al. 2017;
467 Keller and Mrsic-flogel 2018). While previous studies investigating dendritic mechanisms
468 of nonlinear integration have mostly focused on primary sensory areas (Xu et al. 2012;
469 Ranganathan et al. 2018; Francioni, Padamsey, and Rochefort 2019; Beaulieu-Laroche
470 et al. 2019; Palmer et al. 2014; Manita et al. 2015; Ayaz et al. 2019), associative areas
471 may implement similar computations (Lafourcade et al. 2022).

472 We have posited that visuo-motor coherence could provide a top-down signal for
473 when a cue is encountered in a familiar location. This enables correct encoding of
474 landmarks in two ways: 1) A visual cue passes through the visual field at different rates,
475 depending on its distance from the observer. Visuo-motor coherence thus allows correct
476 encoding of visual cue distance; 2) When a cue is encountered but the animal is not
477 actively navigating, as is the case in mismatch sessions, the same cue does not generate
478 bursts and thus does not affect downstream change in positional codes. Our simulations

479 predict a dendrite-localized signal that varies as a function of the learned association
480 between a given, familiar environment and self-motion. Future studies may address this
481 mechanistic hypothesis resulting from our work.

482 We simulated a population of multi-compartment neurons (Naud and Sprekeler
483 2018) to explore how the computational capabilities of cortical neurons add flexibility to
484 the way visual landmark inputs update self-localization estimates. Previous studies have
485 investigated how corrective inputs to attractor networks can offset errors that either
486 accumulate over time or are introduced through environmental manipulations (Campbell
487 et al. 2018; Hardcastle, Ganguli, and Giocomo 2015; Bicanski and Burgess 2016; Burak
488 and Fiete 2009; Page and Jeffery 2018). Most of these models are designed to work in a
489 single behavioral context and are therefore unable to account for more complex demands
490 in real world scenarios. We explicitly modeled the source of landmark and context signals
491 to show how neuronal output can be efficiently modulated by a simple somatodendritic
492 mechanism. We note that our experimental paradigm does not capture the complexities
493 of freely moving mice in their natural habitats. However, we contend that our proposed
494 mechanism can generalize to natural environments in which a given landmark,
495 encountered from the same viewing angle under similar self-motion aspects, should still
496 elicit a stronger response compared to the same landmark being seen from completely
497 different vantage point, as self-localization errors can be most efficiently corrected if a
498 landmark is seen from a familiar location.

499 An important future avenue of inquiry will be to investigate how individual neurons
500 bind their code to a certain location relative to the landmark. A number of studies have
501 looked into this dynamic (Widloski and Fiete 2014; Ocko et al. 2018; Campbell et al.
502 2018). Our previous work (Fischer et al. 2020) has shown that primary visual cortex sends
503 spatially tuned inputs to RSC which could act as an initially context-free
504 feedforward/bottom-up signal. Over the course of learning, top-down context signals,
505 such as we suggest in this study, could trigger AP bursts which in turn strengthen synaptic
506 connections between RSC neurons and downstream brain structures. Future work is
507 needed to illuminate how burst-dependent synaptic plasticity can play the dual role of
508 controlling synaptic plasticity (Payeur et al. 2021; Greedy et al. 2022; N. A. Richards et
509 al. 2019) while also acting as a form of efficient, context-depending communication

510 between brain structures as we show here (Krahe and Gabbiani 2004; Bialek et al. 1991;
511 Bair et al. 1994).

512 Investigating dendritic computation in awake behaving animals is currently limited
513 by a number of serious technical and experimental challenges (Francioni and Harnett
514 2021). The modeling approach we used here has successfully demonstrated complex
515 encoding schemes in the past (Kaifosh and Losonczy 2016; Williams et al. 2021; Payeur
516 et al. 2021; Bicknell and Häusser 2021) and may prove an advantageous complementary
517 avenue to investigate the contribution of dendritic computations during behavior.

518 Overall, we demonstrate how individual neurons shift their encoding priorities from
519 self-centered to world-centered in our landmark navigation task. These codes remain
520 stable while animals repeatedly execute the same task over multiple days but significantly
521 change their activity patterns in a different behavioral context. However, when behavioral
522 and sensory inputs matched in this alternative context, we observed activity reminiscent
523 of that recorded during active navigation. We formulated a mechanistic hypothesis of how
524 sensory information could be integrated by multi-compartment cortical neurons to update
525 downstream internal state representations through bursting. These bursts were critical for
526 output to downstream neurons while being robust to background noise. Our proposed
527 mechanism therefore combines the advantages afforded by rapid and flexible integration
528 sensory stimuli with the robustness of attractor dynamics for the internal representation
529 of behavioral state.

530

531

532

533 **Methods**

534

535 *Animals and surgeries*

536 All animal procedures were carried out in accordance with NIH and Massachusetts
537 Institute of Technology Committee on Animal care guidelines. Male and female mice were
538 singly housed on a 12/12 hr (lights on at 7 am) cycle. Surgical procedures were identical
539 to those in Fischer et.al. 2020. Briefly, C57BL/6 mice aged 7-10 weeks were
540 anaesthetized. A 3.0 mm diameter craniotomy was drilled on the dorsal surface of the
541 skull. AAV1.Syn.GCaMP6f.WPRE.SV40 was injected into the exposed retrosplenial
542 cortex at 4-6 injection sites 1800 - 3400 μm caudal of bregma and 350-600 μm lateral to
543 the midline. Recordings were taken directly over the injection sites adjacent to the central
544 sinus. 50-100 nl were injected at each site. After successful injection, a cranial window
545 was placed over RSC and a headplate implanted on the skull.

546

547 *Virtual reality setup and behavioral training*

548 The same virtual reality setup as described in Fischer et.al. 2020 was used for this study.
549 Mice were head fixed atop a 20 cm polystyrene disc. Two 23.8" computer screens
550 covered the majority of the mouse's field of view. During virtual navigation, animal
551 movement was translated into visual flow through the virtual environment that was shown
552 on the screens. A lick spout was placed close to the mouse's mouth such that it could
553 easily touch it by extending its tongue. Recordings were obtained from mouse from day
554 0 of exposure to the landmark navigation task. Prior to behavioral training/recording mice
555 were habituated to head-restraint on the treadmill and with a linear corridor without
556 landmarks.

557

558 *Image Registration, ROI detection and ROI matching across days*

559 Two-photon imaging was carried as described in Fischer et.al. 2020. In brief, a
560 NeuroLabware 2-photon microscope with a 16x objective was used to collect all imaging
561 data. Images were acquired either at 15.5 or 31.0 Hz using an excitation wavelength
562 between 920 and 980 nm. Frames of the raw video data were registered, and putative
563 neurons (regions of interest or ROIs) were detected using the CalmAn software package

564 (Giovannucci et al. 2019). ROIs were subsequently manually curated to remove dendrites
565 or other, non-soma ROIs. Individual neurons from a subset of recorded fields of view
566 (FOV) were tracked across sessions to analyze their activity patterns over the course of
567 learning. In order to do so, one FOV from each animal after it had robustly learned the
568 task (Task score > 20 cm) was used as a reference session. The mask of detected ROIs
569 for any two sessions was then overlaid and coarsely aligned if necessary. This was
570 followed by applying the CellReg algorithm to determine if two ROIs are the same neuron
571 base on centroid distance and spatial footprint (Sheintuch et al. 2017). Supplementary
572 figure 2 shows this process for three FOVs. This process was repeated until each session
573 of a given animal was matched to the reference session. Neurons considered ‘tracked
574 neurons’ are those that have been matched between any given session and the reference
575 session. For the analyses shown in figure 2, the same neurons were tracked over three
576 sessions. This was done by overlaying the ROI masks and selecting ROIs that could be
577 matched across all three sessions.

578

579 *GLM*

580 We used a generalized linear model to identify which variables each neuron was encoding
581 throughout training. We created two broad categories of predictors: self-centered and
582 landmark-centered. Self-centered predictors consisted of: Running speed (linear) and
583 categorical (running/not running) with a threshold of 1 cm/sec. Trials starts were captured
584 by 3 Gaussians (standard deviation of 0.25 sec.) offset from the trial start to capture neural
585 activity that is related to the trial start but delayed in terms of fluorescence increase.
586 Landmark-referenced predictors consisted of a series of Gaussians covering the entire
587 virtual corridor. Each landmark had its own set of landmark-referenced predictors. We fit
588 the model on calcium fluorescent data using elastic net regression using the glmnet
589 package (Friedman, Hastie, and Tibshirani 2010) with $\alpha=0.5$. Only neurons that our model
590 fit reasonably well (explained variance > 25%) were included for GLM analyses in Fig. 1.
591 For cross-validation we held out 1 trial and fit to the others. We repeated this until each
592 trial was held out once. We calculated an R^2 value (explained variance) to evaluate the
593 fit quality of our GLM model by calculating the difference between the predicted and true
594 calcium signal on held out data:

595

$$D_{model} = 2 * \sum df * \log\left(\frac{df}{df_{pred}}\right) - (df - df_{pred}) \quad (1)$$

$$D_{null} = 2 * \sum df * \log\left(\frac{df}{df_{null}}\right) - (df - df_{null}) \quad (2)$$

$$r^2 = 1 - \frac{D_{model}}{D_{null}} \quad (3)$$

599

600 Where df is the average activity of the neuron on the held out trial, df_{pred} is the predicted
601 activity and df_{null} is the average activity of that neuron on that trial. R^2 was calculated only
602 on activity in-between trial start and reward delivery. We determined the fraction of
603 landmark-referenced vs. self-referenced encoding by calculating the sum of all absolute
604 landmark-referenced coefficient weights divided by the sum of absolute landmark-
605 referenced and self-referenced coefficient weights.

606 We quantified the explained variance of landmark-referenced of self-referenced
607 coefficients by first fitting the full model but predict activity with either one or the other set
608 of predictors set to 0. This way, only activity captured by the respective coefficients was
609 used for the prediction. Explained variance was calculated as described above.

610

611 *Bayesian location decoding*

612 We used a Bayesian decoder to estimate the animal's position on the track based on
613 neural data alone (Davidson, Kloosterman, and Wilson 2009; Mao et al. 2018). Briefly,
614 spatial tuning curves for each neuron were constructed using one of two methods: 1) In
615 experiments where we analyzed precision of the spatial code during virtual navigation
616 (Fig. 1) every other trial in a session was used to construct the tuning curves. Activity on
617 the other half of trials was used to decode animal position. 2) In experiments that analyzed
618 how well we could reconstruct animal position during visuo-motor mismatch trials, all trials
619 during virtual navigation were used to construct tuning curves while trials during visuo-
620 motor mismatch were used for location estimation.

621 Location and activity data were binned into 2.5 cm and 0.25 sec. bins, respectively. For
622 each time bin, the probability density function across all location bins on the track was
623 calculated. The reconstructed position was defined as the location with the highest

624 probability in a given time bin. The overall decoding error for a trial was calculated as the
625 median difference between the decoded location and the animal's actual location. The
626 probability density functions were calculated as described in (Mao et al. 2018):

$$627 \quad P\left(\text{loc} \mid \left(\frac{\Delta F}{F}\right)_{pop}\right) = C(\prod_{i=1}^N f_i(\text{loc})^{n_i})e^{-\tau \sum_{i=1}^N f_i(\text{loc})}$$

628 Where f_i is the spatial tuning for neuron i , N is the total number of neurons, n_i is the
629 activity of neuron i at the respective time bin (calculated as the average value of all
630 datapoints within that time bin) and τ is the time bin size.

631

632 *Cross-day cross-correlation analysis*

633 To evaluate the stability of landmark-referenced codes we cross correlated activity over
634 subsequent recording sessions. To do so, we excised neural activity in the black-box
635 between trials and concatenated the remaining calcium fluorescence trace. The resulting
636 traces, one from each recording session, were then shifted relative to each other with a
637 maximum lag of 800 seconds. The maximum cross correlation value was used for further
638 analysis. To create null-distributions for each neuron, we randomly rotated neural activity
639 in one of the sessions for each trial independently. The cross correlation for the null
640 distribution was thus calculated from a non-rotated first session, and a rotated second
641 session.

642

643 *Visuo-motor mismatch analysis*

644 We calculated visuo-motor mismatch by subtracting the visual flow speed of 30 cm/sec
645 from the animal running speed. Each visuo-motor mismatch session consisted of 10
646 cm/sec and 30 cm/sec flow speed sessions. However, here we only used 30 cm/sec trials
647 as these were closer to the animals average running speed and thus gave us better
648 sampling of a range above and below that speed. Before relating flow speed to neural
649 activity, we removed the linear speed component. We did this by fitting a robust linear
650 regression (`scipy.stats.siegel slopes`) to fluorescence data as a function of running speed.
651 We then subtracted the corresponding amount from each datapoint. For the following
652 analysis we calculated the average running speed on a trial and subtracted the visual flow
653 speed to determine ΔSpeed . To determine the maximum response across all neurons

654 and trials, we evaluated dF/F for each trial as a function of ΔSpeed and fit a 2nd order
655 polynomial (numpy.polyfit).

656

657 *2-compartment model*

658 Variables and parameters are defined in the tables below.

659

660 Landmark cells are simulated with a two-compartment model developed by Naud and
661 Sprekeler 2018). The dynamics of the somatic compartment are

662

$$663 \quad \frac{dV_i^{(s)}}{dt} = -\frac{V_i^{(s)} - E_L}{\tau_s} + \frac{g_s f(V_i^{(d)}) + I_i^{(s)} + w_i^{(s)}}{C_s} \quad (5)$$

$$664 \quad \frac{dw_i^{(s)}}{dt} = -\frac{w_i^{(s)}}{\tau_w^{(s)}} + b_w^{(s)} S_i^{(s)} \quad (6)$$

665

666 whereas the dynamics of the dendritic compartment are

667

$$668 \quad \frac{dV_i^{(d)}}{dt} = -\frac{V_i^{(d)} - E_L}{\tau_d} + \frac{g_d f(V_i^{(d)}) + c_d K(t - \widehat{t}_i^{(s)}) + I_i^{(d)} + w_i^{(d)}}{C_d} \quad (7)$$

$$669 \quad \frac{dw_i^{(d)}}{dt} = \frac{-w_i^{(d)} + a_w^{(d)}(V_i^{(d)} - E_L)}{\tau_w^{(d)}} \quad (8)$$

670

671 The voltages $V_i^{(s)}$ and $V_i^{(d)}$ are initialized to -70mV, whereas $w_i^{(s)}$ and $w_i^{(d)}$ are initialized
672 to 0. The function f is defined as $f(x) = \frac{1}{1 + e^{-\frac{x - E_d}{D_d}}}$ and K is a rectangular kernel with an

673 amplitude of 1 between 0.5 ms and 2.5 ms. The neuron spikes when $V_i^{(s)}$ reaches $V_T =$
674 -50mV , after which $V_i^{(s)}$ is reset to -70mV .

675

676 The input current to the somatic compartment of a landmark neuron is given by $I_i^{(s)} =$

677 $I_{base} + I_{max} e^{-\frac{1}{2} \left(\frac{x_m - \mu_i}{\sigma(I)} \right)^2} + I_i^{(s,bg)}$. The locations μ_i where $I_i^{(s)} - I_i^{(s,bg)}$ is maximized are

678 selected from a Gaussian distribution centered at 220 cm with a standard deviation of 30
 679 cm. The input current to the dendritic compartment of a landmark neuron is $I_i^{(d)} =$
 680 $I^{(d,coh)} + I_i^{(d,bg)}$. The current $I^{(d,coh)}$ is calculated as $I^{(d,coh)} = \max(1 - |(v_{mouse} -$
 681 $v_{VR})/v_{VR}|, 0) * I_{max}^d$. Both background currents $I_i^{(s,bg)}$ and $I_i^{(d,bg)}$ are modelled with an
 682 Ornstein-Uhlenbeck process with a mean of 0: $\frac{dI_i^{(bg)}}{dt} = -\frac{I_i^{(bg)}}{\tau_{bg}} + \sigma^{(bg)}\eta$, where η is white
 683 noise.

684
 685 In the somatic inputs only condition (no inputs to dendrites), the somatic compartment
 686 receives an input of $I_i^{(s)} = I_{base} + I_{max}e^{-\frac{1}{2}\left(\frac{x_m - \mu_i}{\sigma(I)}\right)^2} + I_i^{(s,bg)} + I_i^{(d,coh)}$ and the dendritic
 687 compartment has an input of $I_i^{(d)} = I_i^{(d,bg)}$.

688
 689 The continuous attractor is modeled as a reduced, low-dimensional model of a line
 690 attractor (Ocko et al. 2018). Velocity inputs move the peak of the activity bump x_{att} in
 691 proportion to the mouse's velocity $v(t)$:

$$692 \quad \frac{dx_{att}}{dt} = v(t) \quad (9)$$

693
 694
 695 Spiking from landmark neurons can also move x_{att} . Spikes from landmark neurons are
 696 convoluted with an exponential filter:

$$697 \quad s_i = \sum_{t_i^{(s)}} e^{-\frac{t - t_i^{(s)}}{10}} \quad (10)$$

698
 699 The resulting aggregated value generated by spiking multiplied by a sigmoidal function
 700 as follows:

$$701 \quad s_i^f = s_i * \frac{2.5}{1 + e^{-(30 * s_i - s_T)}} \quad (11)$$

702

703 The resulting force s_i^f moves the activity bump moves towards the landmark cell's
704 receptive field center:

705
$$\frac{dx_{att}}{dt} = \omega s_i^f (\mu_i - x_{att}) \quad (12)$$

706 The initial location of x_{att} is determined by averaging the mouse's starting location over
707 the trials. ω is a normalization factor calculated as 1/number of simulated neurons. For
708 each trial, the mouse's velocity $v(t)$ is determined by cutting out timesteps where the
709 mouse's recorded velocity exceeds 1 m/s and fitting a function to the data with linear
710 interpolation. Unless otherwise stated, each simulation consists of 100 trials using 100
711 neurons.
712

713

Variable	Description
$V_i^{(s)}$	Voltage of somatic compartment for the i^{th} landmark cell
$w_i^{(s)}$	Adaptive current for somatic compartment of the i^{th} landmark cell
$S_i^{(s)}$	Spike train of the i^{th} landmark cell
$V_i^{(d)}$	Voltage of dendritic compartment for the i^{th} landmark cell
$\widehat{t}_i^{(s)}$	Spike times of the i^{th} landmark cell
$w_i^{(d)}$	Adaptive current for dendritic compartment of the i^{th} landmark cell
$I_i^{(s)}$	Input current to somatic compartment of the i^{th} landmark cell
$I_i^{(d)}$	Input current to dendritic compartment of the i^{th} landmark cell
x_m	Mouse location
μ_i	Location of peak current of i^{th} landmark cell
$I_i^{(s,bg)}$	Background input to somatic compartment of i^{th} landmark cell
$I_i^{(d,coh)}$	Input to the dendritic compartment of i^{th} landmark cell from the coherence signal
$I_i^{(d,bg)}$	Background input to dendritic compartment of i^{th} landmark cell
$\sigma^{(bg)}$	Parameter for Ornstein-Uhlenbeck process for background noise
x_{att}	Location of the peak of the steady state activity bump on the attractor
$v(t)$	Mouse velocity
s_i	Activity of i^{th} landmark cell
s_T	Threshold value for gating force from landmark neurons to attractor
f_i	Force applied to attractor

714 **Table 1:** Variable descriptions for model and simulations.

715

Parameter	Value
E_L	-70 mV
g_s	1300 pA
τ_s	16 ms
C_s	370 pF
$\tau_w^{(s)}$	100 ms
$b_w^{(s)}$	-200 pA
g_d	1200 pA
c_d	2600 pA
τ_d	7 ms
C_d	170 pF
$a_w^{(d)}$	-13 nS
$\tau_w^{(d)}$	30 ms
E_d	-38 mV
D_d	6 mV
V_T	-50 mV
I_{base}	250 pA
I_{max}	800 pA
$\sigma^{(l)}$	5
I_{max}^d	150 pA
S_T	1.75 a.u.

716 **Table 2:** Model parameters and set values.

717

718

719 *Single compartment model*

720 The single compartment model was based on the 2-compartment model but without the
721 dendritic compartment. The dynamics of the compartment are:

722

$$723 \quad \frac{dV_i^{(s)}}{dt} = -\frac{V_i^{(s)} - E_L}{\tau_s} + \frac{F(I_i^{(s)}) + w_i^{(s)}}{C_s} \quad (13)$$

$$724 \quad \frac{dw_i^{(s)}}{dt} = -\frac{w_i^{(s)}}{\tau_w^{(s)}} + b_w^{(s)} S_i^{(s)} \quad (14)$$

725 where the function F is defined to be

726

$$727 \quad F(x) = x + \frac{S_C}{1 + e^{-(x-S_T)/S_0}} \quad (15)$$

728

729 in the supralinear case, and $F(x) = x$ otherwise. The somatic compartment receives an

730 input of $I_i^{(s)} = I_{base} + I_{max} e^{-\frac{1}{2}\left(\frac{x_m - \mu_i}{\sigma(I)}\right)^2} + I_i^{(s,bg)} + I_i^{(d,bg)} + I_i^{(d,coh)}$.

731

732 The variables are as described in Table 1, with the addition of parameters S_C , S_T and S_0
733 describing the supralinear integration. For the simulations in supplementary figure 7, the
734 following parameter values were used:

S_C	2000 pA
S_T	1000 pA
S_0	10

735 **Table 3:** Model parameters and set values for single compartment models.

736

737

738 Reference

739

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1068 **Author Contributions**

1069 L.F.F. performed experiments, analyzed data, designed and helped build the model,
1070 made figures, and wrote the manuscript. L.X. helped design and built the model and
1071 also analyzed model data. K.T.M. collected experimental data and assisted with
1072 analysis. M.T.H supervised all aspects of the project and helped write the manuscript.

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1075 **Competing interests**

1076 The authors declare that they have no competing interests.

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1078 **Data availability**

1079 All data needed to evaluate the conclusions in the paper are present in the paper and/or
1080 the Supplementary Materials. Additional data will be deposited in Zenodo upon
1081 acceptance.

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1083 **Supplementary materials**

1084 Supplementary figures 1-9.

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