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The Anatomic Study of Anterior Transdiscal Axial Screw Fixation for Subaxial Cervical Spine Injuries

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Abstract: Anterior transdiscal axial screw (ATAS) fixation is an alternative or supplement to the plate and screw constructs for the upper cervical spine injury. However, no existing literatures clarified the anatomic feasibility of this technique for subaxial cervical spine. Therefore, the objective of this study was to evaluate the anatomical feasibility and to establish guidelines for the use of the ATAS fixation for the subaxial cervical spine injury

Fifty normal cervical spines had radiographs to determine the proposed screw trajectory (the screw length and insertion angle) and the interbody graft-related parameters (the disc height and depth, and the distance between anterior vertebral margin and the screw) for all levels of the subaxial cervical spine. Following screw insertion in 8 preserved human cadaver specimens, surgical simulation and dissection verified the feasibility and safety of the ATAS fixation.

Radiographic measurements showed the mean axial screw length and cephalic incline angle of all levels were 41.2 mm and 25.2°, respectively. The suitable depth of the interbody graft was >11.7 mm (the distance between anterior vertebral margin and the screw), but <17.1 mm (disc depth). Except the axial screw length, increase in all the measurements was seen with level up to C5-C6 segment. Simulated procedure in the preserved specimens demonstrated that ATAS fixation could be successfully performed at C2-C3, C3-C4, C4-C5, and C5-C6 levels, but impossible at C6-C7 due to the obstacle of the sternum. All screws were placed accurately. None of the screws penetrated into the spinal canal and caused fractures determined by dissecting the specimens.

The anterior transdiscal axial screw fixation, as an alternative or supplementary instrumentation for subaxial cervical spine injuries, is feasible and safe with meticulous surgical planning.

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Abbreviations: ACDF = anterior cervical decompression and fusion, ATAS = anterior transdiscal axial screw, AxiaLIF = axial lumbosacral interbody fusion.

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INTRODUCTION

ervical flexion distraction injuries account for about 10% of all injuries to the subaxial cervical spine and mainly caused by traffic accidents.^{1,2} The injuries involve not only the intervertebral disc and anterior ligament, but also posterior complex ligament, which may further result in subluxation or dislocation of the facet joint.³⁻⁷ The instability associated with cervical flexion distraction injury is emphasized due to those circumferential injuries affecting both anterior and posterior structures.

Although some surgeons proposed conservative treatment for the patients suffered mild flexion distraction injury,⁸⁻¹⁰ more authors recommend aggressive surgical treatment would be one choice.^{11–13} In most cases, anterior cervical decompression and fusion (ACDF) plus plate instrumentation was carried out according to the injury mechanism and pathology. But Johnson et al^{14} reported that 13% of cases received anterior cervical procedure alone would result in cervical deformity healing. It was considered that only anterior cervical plate fixation could not supply sufficient biomechanical stability in those cases with severe facet fracture and posterior complex injury.¹⁵ More authors recommended that the combined anterior and posterior approach should be applied, that means, on the basis of ACDF and anterior plate, the posterior screw-rods instrumentation should also be added.^{16–18} However, the complications associated with those combined procedures were also

noted with high risks of surgical trauma. In 2006, Defino et al¹⁹ put forward a procedure for anterior C2/3 screw fixation and performed a biomechanical study in swine cervical spine. The results showed that anterior 2 axial screws for C2/3 fixation could achieve similar biomechanical stability compared to anterior cervical plate fixation. Therefore, the author suggested that anterior transdiscal axial screw fixation (ATAS) of C2-3 could be considered as an alternative procedure if some difficulty of exposing or instrumenting occurred when performing the anterior plate fixation.

Given these potential uses for anterior transdiscal axial screw fixation, we believe that this technique should be included in the armamentarium of subaxial cervical spine fixation methods. And yet, to the best of our knowledge, there are no literatures that have document the detailed and relative anatomical data for ATAS. In this study, the authors proposed the ATAS fixation technique as a supplementary instrumentation for the subaxial cervical spine injury. The anatomic feasibility was assessed through a radiographic study of patients and an evaluation of human cadaveric spine specimens.

MATERIALS AND METHODS

Radiographic Measurements

This was an institutional review board-approved, retrospective analysis of patients of East Asian ancestry who presented to the emergency department at Nanfang hospital between January 1, 2015, and July 30, 2015, requiring standard lateral x-ray films

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of the cervical spine. To be included, the films have to be with normal cervical curve and alignment, to be negative for the presence of endplate sclerosis, osteophytes, and narrowing of disc spaces or segmental instability. Fifty patients (32 males/18 females, range 22–48 years) with mean age of 28 ± 4 years were available for analysis. The lateral films of the cervical spine were obtained from a 500-mA x-ray machine (Siemens, Erlangen, Germany) and the lines and angles were drawn and measured using PACS (INFINIFF, Seoul, South Korea).

On the lateral x-ray film, the following parameters related with ATAS were measured (Figure 1): (L) axial screw length, made from anteroinferior point of inferior vertebral body to the posterosuperior point of superior vertebral body (the diagonal line of the adjoining cervical vertebral bodies); (α) cephalic incline angle of axial screw, made between the simulated trajectory of the screw and the front edge of the vertebral body; (DH) disc height, the height of the intervertebral space; (DD) disc depth, the distance between the anterior edge and posterior edge of the cervical disc; (A) graft depth A, the length between the intersection of the trajectory of the axial screw with the inferior endplate of superior vertebral body and its anterior inferior border, representing the depth of the superior border of the graft; (B) graft depth B, the length between the intersection of the trajectory of the axial screw with the superior endplate of inferior vertebral body and its anterior inferior border, representing the depth of the inferior border of the graft. The parameters measurement of the ATAS were performed at



FIGURE 1. Measurement of the parameters related with ATAS fixation. α = the angle between the simulated trajectory of the axial screw and the anterior edge of the vertebral body, A = the depth of the superior border of the graft, ATAS = anterior transdiscal axial screw, B = the depth of the inferior border of the graft, DD = disc depth, DH = disc height, L = axial screw length.

C2–C3, C3–C4, C4–C5, and C5–C6 levels, but the C6–C7 level in all patients, due to the obstruction of the sternum.

Cadaveric Simulation

Eight preserved human cadaver specimens (5 males/3 females) of East Asian ancestry with unknown age were obtained from the Department of Anatomy. The specimen was confirmed by x-ray to have a normal cervical spine. The cadaver heads were secured with pins in a head-holder (Figure 2), avoiding flexion-extension and rotation. The tools necessary to facilitate insertion of a screw include the following equipment seen in Figure 3.

The surgical procedure of ATAS fixation was carried out as follows. The midline of vertebral body was confirmed and used as guidance for axial screw insertion. Under the lateral C-arm x-ray fluoroscope, guiding wire was inserted from the anteroinferior portion of the inferior cervical vertebral body, pointing to the posterosuperior portion of the superior cervical vertebral body. After the guiding wire positioned successfully, the trajectory length of the wire was measured on the surplus distance by a second identical K-wire placed parallel with the initial guiding wire. The screw length was determined based on the length of the wire trajectory. A cannulated drill bit was used to make a recess for the screw insertion. Then, a partially threaded self-tapping cannulated screw (diameter in 3.5 or 4.0 mm) was inserted over the guiding wire. Once the axial screw was successfully positioned, the wire was then removed. The 8 specimens were dissected to observe the incidence of violation to the spinal canal and vertebral fracture after the ATAS fixation.

STATISTICAL ANALYSIS

All collected data were further processed with SPSS software (SPSS Inc, Chicago, IL), and expressed in mean \pm stanstandard deviation. A 1-way analysis of variance was used to compare all parameters among levels. The significance level was set at 95%.

RESULTS

Radiographic Measurements

Given that no significant difference was observed (P < 0.05) in the measurements for sexes, the results presented



FIGURE 2. Photograph of anatomical preparation of a cadaveric head on a head holder.



FIGURE 3. Photograph showing the system of tools to facilitate insertion of screw.

here correspond to averages obtained without considering the sexes (Tables 1 and 2). Except the axial screw length, increase in all the measurements was seen with level up to the C5-C6 segment.

The mean screw length and angle for all patients were 41.2 mm and 25.2° , respectively. The C2–C3 segment has the longest axial screw, but with a smallest screw inclination angle. The mean graft depth A and B for all patients were 11.7 mm and 7.9 mm, respectively. Increase in the both measurements was seen with level up to the C5–C6 segment. There was a significant difference between levels in graft depth A, except for C4–C5 and C5–C6 levels. In contrast, in graft depth B, no significant difference was observed between levels except for C2–C3 and the other levels. The mean disc height and disc depth for all patients were 6.6 mm and 17.4 mm, respectively. The above both parameters also appear to be a growing trend with level up. There were no significance differences between the levels for the disc height or disc depth (Table 2).

Simulation Procedure

ATAS fixation was performed successfully at C2–C3, C3–C4, C4–C5, and C5–C6 segments in all specimens (Figure 4). Due to the obstruction of the sternum, however, it could not be conducted in the C6–C7 segment. On gross examination, all 32 screws met the criteria for viable positioning. Based on dissection of the specimens, none of screws penetrated into the spinal canal and caused vertebral fracture.

DISCUSSION

Anterior axial fixation was first introduced in the lumbosacral zone with a fibular strut or direct screw fixation, which was introduced in the midline from the anterior superior border of L5, obliquely down through the vertebral body of L5 and the disk space L5/S1, into the vertebral body of S1.^{20,21} The procedure was recommended for the treatment of lumbosacral spondylolisthesis. Recently, some reports presented a posterior axial fixation technique by using the transpedicle-disc-vertebral body screw for the lumbosacral junction.^{22–24} Furthermore, this procedure also can achieve a delta fixation combined with other pedicle screw and rod application. Aebi et al²¹ noted that the procedure was simple and easy to perform, and the overall satisfaction of the patients was >80%. It was anticipated that the instant stability supported by the axial screw would be superior to the vertebral cancellous screw fixation such as the anterior plate-screw system. But all these fixation methods are not the mainstream spinal instrumentation techniques clinically.

In 2004, Cragg et al²⁵ first introduced a new procedure of percutaneous axial lumbosacral interbody fusion (AxiaLIF). With a presacral working tunnel through a small incision in paracoccyx, 1 specially designed screw was introduced from anterior S1 to L5, or L4 for the lumbosacral fixation. Erkan et al²⁶ conducted a biomechanical study of 2-level fusion of L4-S1 AxiaLIF in 6 lumbosacral cadaveric specimens. Three states including the AxiaLIF alone, AxiaLIF with posterior facet screws, and AxiaLIF with pedicle screws and rods fixation were evaluated, respectively. The result indicated that at the L4-L5 level, there was no statistical significance in rotation or flexion-extension movement among the 3 different AxiaLIF procedures, and the AxiaLIF with pedicle screws and rods fixation shows a significantly higher stability than the other 2 fixation methods in lateral bending movement; at the L5-S1 level, there was no significance difference in rotation and lateral bending movement among the 3 fixation methods, and the AxiaLIF alone showed a larger range of motion in flexionextension, the AxiaLIF with posterior constructs fixation had an increased stiffness in this level. Ledet et al²⁷ reported that the

TABLE 1. Measurement Parameters Related With Anterior Transdiscal Axial Screw Fixation (Patients N = 50)						
	C2-C3	C3-C4	C4-C5	C5-C6		
L (mm)	44.3 ± 3.6 (38.5–52.6)	40.8±3.4 (34.7-49.3)	39.9±3.5 (34.3-49.4)	39.7±3.4 (33.9–48.3)		
α (°)	$22.5 \pm 3.1 \ (13.5 - 28.9)$	25.5 ± 3.7 (19.2–38.6)	26.1 ± 2.9 (19.9-34.3)	$26.8 \pm 3.1 \ (20.6 - 33.4)$		
A (mm)	10.4 ± 1.4 (7.7–14.3)	$11.7 \pm 1.4 \ (8.4 - 15.4)$	$12.3 \pm 1.5 \ (9.6 - 16.0)$	$12.4 \pm 1.5 \ (9.5 - 16.4)$		
B (mm)	7.1 ± 1.1 (4.7–9.6)	8.1 ± 1.1 (5.9–10.7)	8.3 ± 1.3 (5.5–11.8)	8.2 ± 1.4 (6.1–12.5)		
DH (mm)	6.6 ± 0.8 (5.0–8.4)	6.5 ± 0.7 (3.9–8.0)	6.6 ± 0.7 (4.9–8.1)	6.7 ± 0.8 (5.0–8.9)		
DD (mm)	17.1 ± 1.50 (15.0–20.6)	$17.3 \pm 1.5 \; (15.0 - 20.9)$	$17.5 \pm 1.7 \ (15.0 - 21.2)$	17.8 ± 1.8 (14.4-21.8)		

Data are presented as mean and standard deviation. α = screw angle, A = the depth of the superior border of the graft, B = the depth of the inferior border of the graft, DD = disc depth, DH = disc height, L = screw length, N = number.

		* P		+	P	$\frac{{}^{\ddagger}P}{C5-C6}$
	C3-C4	C4-C5	C5-C6	C4-C5	C5-C6	
L (mm)	< 0.001	< 0.001	< 0.001	0.231	0.334	0.453
α (°)	0.032	< 0.001	< 0.001	0.090	0.005	0.567
A (mm)	0.043	0.012	0.003	0.021	0.007	0.642
B (mm)	0.036	0.026	0.009	0.205	0.134	0.089
DH (mm)	0.541	0.317	0.203	0.125	0.087	0.636
DD (mm)	0.462	0.221	0.461	0.231	0.132	0.532

TABLE 2. P Values of Post Hoc Ana	lysis Between Levels for all Measurements
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 α = screw angle, A = the depth of the superior border of the graft, B = the depth of the inferior border of the graft, DD = disc depth, DH = disc height, L = screw length.

*Indicates comparison with the C2–C3 level.

[†]Indicates comparison with the C3–C4 level.

[‡]Indicates comparison with the C4–C5 level.

axial screw fixation had more segmental stability than the traditional implants such as intervertebral cage, thus promoting bony fusion. Initial clinical experience on AxiaLIF showed this procedure had good effects on lumbosacral fusion in early stage.²⁸

For upper cervical spine, axial screw fixation was commonly used as posterior or anterior atlantoaxial transarticular fixation. Magerl and Seemann²⁹ first introduced the posterior transarticular screw fixation for atlantoaxial instability. More authors supported this procedure can apply sufficient biomechanical stability, and >90% of fusion rate can be achieved by this procedure. Anterior atlantoaxial transarticular fixation was introduced by Barbour,³⁰ and the clinical results confirming the superior efficacy of this technique.



FIGURE 4. X-ray image of ATAS fixation. A partially threaded selftapping cannulated screw with an upper oblique angle, passing through the lower vertebral body and the intervertebral space into the upper adjacent vertebral body. ATAS = anterior transdiscal axial screw.

To our knowledge, the ATAS fixation is not yet reported as the normal surgical procedure for the subaxial cervical spine injury in the literature. Argenson et al³¹ showed us some figures of fixation by 1 anterior screw and graft between C3 and C2 in the case with severe sprain injury. In 2006, Defino et al¹⁹ put forward a procedure for anterior C2–C3 screw fixation and performed a biomechanical study in swine cervical spine. The results showed that anterior 2 axial screws for C2/3 fixation could achieve similar biomechanical stability compared to anterior cervical plate fixation. Therefore, the author suggested that the axial screw fixation of C2–C3 could be considered as an alternative procedure if some difficulty of exposing or instrumenting occurred when performing the anterior plate fixation.

The present study was the first anatomical analysis of the ATAS fixation. The important parameters related to this fixation were collected from this study. For adult, about 41-mm length cancellous screw was adapted for most cases, and the preferable inclination angle was nearly 25° . Simulation surgery showed that the axial screw fixation can be carried out for C2– C3, C3–C4, C4–C5, and C5–C6 levels. For the C6–C7 level, cephalically axial screw was not possible due to the obstruction of the sternum. Therefore, the ATAS fixation was feasible and safe to perform.

Theoretically, biomechanical advantages of ATAS fixation were noted as following aspects. First, the length of the anterior cervical axial screw (41 mm) was remarkable longer than that of the commercially designed cervical plate screw (12-18 mm), which should favor resistance to screw pull-out. Second, ATAS as a fixation procedure of vertebral body-discbody could penetrate at least 2 endplate structures and achieved more biomechanical benefits compared to the simple cancellous screw. Luk et al³² evaluated biomechanically the insertion torque and maximal pull-out strength between conventional sacral pedicle screw and the bicortical sacral pedicle screw through the S1 endplate and confirmed the superiority of the screw fixation with the trajectory through the S1 endplate. Third, anterior cervical plate fixation only had the tension-band effect anteriorly, and the flexion stability was insufficient under complete destruction of the posterior elements. Supplementary anterior axial screw could add the beneficial synergistic effect with anterior plate instrumentation for the treatment of the cervical instability. With ATAS, the adjoining vertebral bodies and in-between graft were hold together as a whole, which can be seen as a biomechanical fusion.

ATAS fixation is recommended for the cervical flexion distraction or rotational injury, which results in transdisc fracture or dislocation. Although this fixation technique has the same dissection plane as the anterior plate and screw fixation system, the exposure area for ATAS placement is smaller compared to the standard technique, involving a lower risk of injury to adjacent structures. When the anterior plate and screw fixation system could not provide sufficient stability or the procedure is impossible to perform in the cervical spine, the availability of the ATAS fixation technique may add stable fixation to further attempts at obtaining an anterior spinal fusion. The possible disadvantage of this technique would be the degeneration of the adjacent disc that is sometimes seen in anterior odontoid fixation. As a supplementary anterior instrumentation procedure, the ATAS fixation technique is not suitable for the cases with serious vertebral body fracture.

Some limitations of this study must be acknowledged. For the radiographic study, the sternum cannot be observed on the standard lateral x-ray films of the cervical spine even on the computed tomographic images, and the parameters related to the ATAS fixation were just measured in C2–C3, C3–C4, C4– C5, and C5–C6 segments. Next, for the cadaveric simulation and evaluation, it cannot represent the situation in vivo absolutely. Extending backward of the neck in vivo, the ATAS fixation would be successfully performed in the C6–C7 level in some cases. Finally, this study mainly focused on bony structures and gave less consideration to soft tissue such as a thick fat layer cover the sternum.

CONCLUSION

The anterior transdiscal axial screw fixation, as an alternative or supplementary instrumentation for the subaxial cervical spine injury, is feasible and safe with meticulous surgical planning. However, further biomechanical studies are required to compare its reliability to other more established techniques.

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