# **Original Article**

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# **Does the flatting of the curve of spee affect the chewing force distribution in the mandible? (3D finite element study)**

**Lamiaa A. Hasan, Sarmad S. Salih Al Qassar, Mohammad N. Alrawi and Emad H. Alhajar**

# **Abstract:**

**OBJECTIVE:** To search the effects of Curve of Spee (COS) flatting on the stresses and displacement on the different mandible landmarks and lower teeth during posterior teeth loading using three-dimensional (3D) finite element analysis.

**MATERIALS AND METHODS:** Three‑dimensional hemi mandibular model was created from real selected mandible. The lower teeth was aligned originally in a curved form with 2.4 mm depth at the cusp tip of the second premolar. Another replica with flat aligned teeth was formed to confirm the analysis by up righting premolars and molars. A load was applied at mesio-buccal cusp of the lower first molar on both models, and the resultant stresses and displacements on the mandibular landmarks and the lower teeth were tested.

**RESULTS:** Von mises over the mandible was higher in flat than in curve model. The highest stress levels were detected at the Mesio‑buccal cusp tip of first molar for flat and curved simulation (5053, 3304) Mpa respectively. Mesio-distally, the teeth displacement was higher in curve model than in flat one. The maximum distal displacement, in flat model, was seen in central and lateral incisors. While, in curve model, the maximum distal displacement was grasped within first and second premolars.

**CONCLUSIONS:** Flatting the COS magnify the stresses over whole mandible and reduce lower teeth displacement mesio‑distally. We speculated that the readjustment of the COS after orthodontic treatment could reduce the stress and displacements on the lower anterior teeth and decrease the lower anterior teeth crowding relapse.

#### **Keywords:**

Chewing force, curve of Spee, finite element, lower anterior crowding

# **Introduction**

*Collage of Dentistry, University of Mosul, Mosul, Iraq*

# **Address for**

**correspondence:** Dr. Sarmad S. Salih Al **Qassar** Department of Orthodontics, Prevention and Pedodontics, Collage of Dentistry, Mosul University, Mosul, Iraq. Email: sarmadsobhi@ yahoo.com; sarmadsobhi@uomosul. edu.iq.

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 $\blacksquare$  he Curve of Spee (COS) is an identifying characteristic of normal alignment of the lower teeth which had been observed in the sagittal profile view of the human skulls,[1] It was first noted by Graf Von Spee in 1890.[2] Recent studies described it, as a curvature extended from disto‑buccal cusps of the most posterior teeth to the incisor edge of the central's incisors.[3] The Literatures

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stated that COS developed as a result of the mesial tilting of the long axis of the lower molar teeth incompetence to the efficiency of muscles of mastication.[4‑6] COS improves food chewing throughout preserving upper and lower teeth contacts during function as it enhances free lower jaw movements.[2] Also, COS has a role in facial aesthetic through its enterprise of an esthetical smile.[7]

COS was evaluated by two main techniques; the first one: as a radius of inferior portion of circle that extended from anterior border of the Condyle to the buccal cusps of second and

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first molar, and pass to contact the cusp tips of premolars and canine respectively, and terminated on the incisor edge of the two central incisors.[8] The second technique of COS evaluation was depending on the arch length and depth of the posterior teeth according to the occlusal plane.[9]

However, there is a disagreement about the measurement methodology for COS. Some authors excluded lower incisors during measurements of Spee's curve. As, they are (sometimes) super‑erupted, and a raised COS depth was obtained.<sup>[10]</sup>

Recently, with advance technology improvements and the used of three-dimensional (3D) scanner, COS measurement became more easy and accurate by using a digital cast analysis. While, previously all the measurements were obtained from hard study models or their photographs, using a divider, calliper, and a coordinate apparatus.<sup>[11]</sup>

During comprehensive orthodontic treatment, leveling of COS of the mandibular teeth is imperative step to establish proper incisors relation and posterior teeth occlusion, especially for deep bite correction<sup>[12,13]</sup>; however, there are disagreements according to COS leveling techniques used to improve the stability of the orthodontic outcomes.[14] Since 1972, Andrews[15] advised leveling the COS to a flat plane to assist the construction of an optimal occlusion, regardless of its effects on the mandible or Tempro‑mandibular joint (TMJ) or even the lower teeth. As, Kanavakis and Mehta<sup>[16]</sup>found a correlation between the sound in TMJ with the COS flatting.<sup>[16]</sup>

The finite element analysis (FEA) technique has been wildly used to study the dynamics of the stomatognathic system.<sup>[17]</sup>It has a capacity for analyzing the frequency, intensity, direction, duration, and of occlusal forces, also it unable to study mandibular biomechanics and to evaluate deformations, tensions, and displacements that may occur throughout the mandible.<sup>[18,19]</sup> The amazing advantage of this FEA is the study of areas that are impossible to access without any risks to the human.<sup>[17,19]</sup>

Stability of the COS as well as orthodontic outcomes after orthodontic treatment is a matter of arguments.[1] As there are no clear clarifications for such relapse. The role of the light continuous force which is produced during daily chewing could be a factor for such deterioration. So, this study was aimed to find out the variations in stresses and displacements after flatting COS, on the mandible and lower teeth during posterior teeth biting, using the FEA.

# **Method and Materials**

This study is coordinating with the roles of the ethics committee of the college of Dentistry/University of Mosul/Iraq no. 4S/475 in 25/3/2019.

All the necessary procedures for FEA and model constriction were carried out as model creations, definitions of the elements form and the properties of the material under load application as well as boundary condition and load application.<sup>[20-23]</sup>

In the current study, 30 skulls for males (judged by three orthodontists to be normal by visual inspections) were examined. Only 10 skulls followed our inclusion criteria, which include: full dentition excluding third molar, class I molar and canine relationships, and without any sever crino-facial abnormalities. The COS of the lower teeth of the 10 selected skulls were measured according to previously authorized methods.<sup>[24-26]</sup> The depth of the bottom of COS was calculated using a Mitutoyo electronic caliper (Mitutoyo, Kawasaki, Japan) as the vertical distance between the deepest cusp tip and occlusal flat plane (a flat metal ruler was seated over the teeth for COS evaluation). The COS line was passed over the mandibular dental teeth extending from the incisal edge of the centrals, passing over the cusp tips of the canine and premolars to touch the mesio‑buccal cusp of the lower first molar to the distal cusp tips of the lower second molar [Figure 1]. The average depth of COS for the 10 selected mandibles was  $2.4$  ( $\pm$  0.24) mm. The mandible which have a COS depth value near the average (2.4 mm) was selected to be our target model to be use for FEA (The deepest point of it was on the cusp tip of the second premolar). However, this depth value is compatible with previous study.[27] Auto cad (2010) Program was used for drawing 3D model of one half of mandible<sup>[23,28]</sup> which was analog to the selected mandible. The previous authorized methods were used to create our 3D model.[29,30] All the linear measurements were taken using a Mitutoyo electronic caliper from the selected mandible. The periodontal ligaments were excluded in this study, because of the difficulties in mechanical modeling as well as the complexity of its mesh mathematical calculations.[31,32] The first model was



**Figure 1:** Schematic the curve of Spee extension and its bottom on the cusp tip of the lower second premolar

duplicated to create the second one. The teeth in second model were aligned with a flat plane, in order to simulate flatting of COS after orthodontic treatment, by upright the lower first and second premolars.

The two models were transported to finite element program (Autodesk Inventor Professional Computer Program (version 2012)), the mechanical properties of the materials were considered to be homogenous, isotropic, and linear elastic as in most reported studies<sup>[23,28,30]</sup>;only two independent material properties, Young's modulus and Poisson's ratio were present in an isotropic material. Cancellous bone network ignored in most FEA studies.[21,23]Therefore, it was assumed that cancellous bone has a solid design inside the inner cortical bone shell.<sup>[23]</sup> The Young's modulus and Poisson's ratio for cortical and cancellous bone were considered according to the ultrasound study of Rho *et al.*[33], while teeth properties were identified according to Boccaccio *et al.*[34], as in Table 1.

The mandible was supported by restraining all the movements at the top of the Condyle<sup>[23,32]</sup>resembling Glenoid fossa, as the boundary conditions. The models were discredited to many elements; each element containing numbers of apexes called nodes; the organization of elements and nodes called the finite element mesh. Finite element results are very critical to the number of elements included in the model. Our final mesh was consisted of 922,592 nodes, 637,262 elements. The force applied was (560N) perpendicular on the mesio‑buccal cusp of the first permanent molar for both replicas which represent 75% of the maximum chewing force to simulate natural chewing<sup>[35]</sup>, as shown in Figure 2.

#### **Table 1: Material mechanical properties for FEA used in this study**



\*GPaGega Pascal, \*\*Rho *et al*., 1993[33], \*\*\*Boccaccio *et al*., 2008[34]



**Figure 2:** Schematic of the three-dimensional model of hemi mandible after meshing and the site of force application

In order to detect the amount of teeth displacements, the mesial and distal contact points of each tooth were observed in both models after load application.

#### **Results**

The results in term of Von mises and displacement in three dimensions (X, Y, and Z) were studied. A color scale (12 colors scale and 13 values) was used for quantitative visualization of the stress distribution and displacement of our models as shown in Figure 3. The maximum values for Von mises stress and displacement for both models were labeled in Table 2.

The von mises stress and  $X$ ,  $Y$ , and  $Z$  displacement, for different anatomical landmarks plotted through the mandible for flat and curve conditions are labeled in Table 3 and displayed in Figures 4-11.

#### **Von mises stresses of Mandibular landmarks**

When the teeth simulated to be flattened the maximum value for von mises stress were higher than the maximum von mises value within curved plane. The highest stress levels were detected in the mesio‑buccal cusp tip of first molar for both simulation (flat and curved plane) (5053, 3304) Mpa respectively. High stress values for both simulations (flat and curved plane) were seen within Anterior mandibular condylar (ACo) (2135, 1370) Mpa, respectively. While, Moderate stress level observed in posterior mandibular Condyle (PCo) in both simulation (1478, 912) Mpa respectively, and these values decrease gradually to the posterior border of mandible (119,41) Mpa. Low stress level was seen in the Superior mandibular condylar (SCo) (26,19) Mpa, Anterior border of ramus (Ab) (41,23) Mpa, Jlat (30,18) Mpa, Jmed (15,2) Mpa, Gonion posterior (Go<sub>post</sub>) (10,2) Mpa, Gonion (Go) (5,3) Mpa and Gonioninferius (Go<sub>inf</sub>) (17,4) Mpa for both imitation flat and curve one-to-one. Zero stress values seen in Menton (Me), Pogonion (Pog), Supramemtale (B), Infradental (Id), Central incisor edge and Coronoid, as in Figures 4 and 5.



**Figure 3:** Schematic probe command in Autodesk Inventor Professional Computer Program

#### *Mandiblular anatomical landmarks Displacement*

Maximum displacement seems to be nearly the same for both models in all three directions. Zero movement was detected in Posterior mandibular condylar (PCo), Anterior mandibular condylar (ACo), and Superior mandibular condylar (SCo). The presentation of X, Y, and Z for displacement depend on how you set your model according to these global coordinate.

# *X‑displacement*

X‑displacement was illustrated as anterio‑posterior (sagittal) movement of mandible, positive value indicate back ward (distally) displacement, negative value specify mesial (forward) displacement. The highest positive X-displacement was seen in the Gonioninferius (Go<sub>inf</sub>) (+0.117, +0.110) mm, Gonion (Go) (+0.112,+0.110)) mm for flat and curve simulation respectively, and extended along the inferior border of the mandible. The high value for distal X‑movement were observed in Gonion posterior  $(G_{\rho_{\text{post}}})$  (+0.099, +0.104) mm and Menton (Me)  $(+0.078,+0.082)$  mm for both flat and curve simulations respectively. Moderate positive X‑displacements for both models were detected within Posterior border of ramus (Pb) (+0.057, +0.086) mm,

**Table 2: Maximum Von Mises stress and displacement values for flat and curve models**



Coronoid (Cor) (+0.052,+0.057) mm, Anterior border of ramus (Ab) (+0.024, +0.046) mm, Pogonion (Pog) (+0.037, +0.065) mm and Central incisor edge (+0.042, +0.026) mm respectively. Less positive X-displacement was noted Supramemtale (B) and Infradental (Id). While, negative (mesial) X-displacement was noted in mesio-buccal cusp tip of first molar,  $J<sub>lat</sub>$  and  $J<sub>med</sub>$  as shown in Figures 6 and 7.

# *Y‑displacement*

Y‑displacement specify transverse (in–out) movement, positive value means inward twisting of the mandible. The mandible under masticatory force simulation was bended in inward direction, the highest value in both flat and curve models were noticed inMenton (Me)(+0.257, +0.259) mm and Pogonion (Pog) (+0.237,+0.254) mm respectively. High inward bending was seen in Supramemtale (B) (+0.227, +0.230) mm, Infra‑dental (Id)(+0.2134,+0.225) mm and central incisor edge (+0.206,+0.213) mm respectively. Moderate Y‑displacement for both simulation were detected within mesio‑buccal cusp tip of



**Figure 4:** Schematic the magnitude and distribution of Von mises stress in flat model

\*(MPa) Mega Pascal, \*\* (mm) millimeter

# **Table 3: Von Mises stress and displacement in different anatomical landmarks**



(MP) Mega Pascal, (mm) millimeter

first molar(+0.147,+0.155) mm,  $J_{\text{lat}}$ (+0.100, +0.116) mm, and J<sub>med</sub> (+0.095,+0.086) mm, Gonioninferius (Go<sub>inf</sub>) (+0.088,+ 0.089) mm, Gonion (Go)(+0.080,+0.084) mm, Anterior border of ramus (Ab)(+0.073,+0.091) mm, and Gonion posterior  $(G_{O_{post}})$  (+0.058,+0.074) mm in sequence. Low Y-displacement was seen in Coronoid (Cor) and Posterior border of ramus (Pb), see Figures 8 and 9.

# *Z‑displacement*

Z‑displacement identify vertical (up–down) movement, positive values pointed to upward movement of the mandible negative values indicate downward displacement. Maximum positive values (upward movement) seen within central incisor edge (+0.450,+0.451) mm, Supramemtale (+0.447,+0.445) mm, Infradental (+0.444, +0.445) mm, Pogonion(+0.442,+0.447)



**Figure 5:** Schematic the magnitude and distribution of Von mises stress in curve plane



**Figure 7:** Schematic the magnitude and distribution of X-displacement incurve plane



**Figure 9:**Schematic the magnitude and distribution of Y-displacement in curve plane

mm and Menton (+0.446,+0.443) mm for both flat and curved models respectively. Highest positive z‑displacement seen in Jmed (+0.199, +0.187) mm and  $\text{flat}(+0.176,+0.198)$  mm, the high positive displacement detected within Goinf(+0.092,+0.098) and Go(+0.080,+0.088) mm, moderate upward movement seen in Gopost(+0.048,+0.073) mm, low values noted within Pb(+0.006,+0.02) mm respectively for flat and curve simulations. While, negative (downward) Z‑movement noted within Coronoid (Cor), Anterior border of ramus (Ab), mesio‑buccal cusp tip of first molar. High downward displacement grasped in mesio‑buccal cusp tip of first molar (0.300, 0.3) mm for both models correspondingly. Moderate negative Z‑movement values observed in Ab (0.151, 0.164) mm while Lowest values noted in Cor (0.083, 0.090) mm for both simulations respectively. See Figures 10 and 11.



**Figure 6:** Schematic the magnitude and distribution of X-displacement in flat plane



**Figure 8:** Schematic the magnitude and distribution of Y-displacement in flat plane



**Figure 10:**Schematic the magnitude and distribution of Z-displacement in flat plane

#### **Teeth displacement and contact points stresses** *Teeth Von miss stresses*

Table 4 shows the von miss stresses of all the contact points between the lower teeth.

# *Teeth X‑displacement*

For central, lateral, canine, first and second premolars, mesial, and distal contact point were founded to displace distally. In flat model, maximum distal movement seen within central mesial, distal, and lateral mesial contact point. While in curve model, the maximum distal movement grasped within first and second premolars, in mesial and distal contact points. In first and second molars, the mesial and distal contact points seem to move mesially for both simulations, this movement was higher in curve model than flat one, as in Table 4.

# *Teeth Y‑displacement*

All teeth seem to move lingually in both models with high value seen in central teeth and decrease gradually to the lowest value in second molar distal contact point, please see Table 4.



**Figure 11:** Schematic the magnitude and distribution of Z-displacement in curve plane

# *Teeth Z‑displacement*

Table 4 shows the teeth contact points displacements and stress. Central, lateral, canine, first premolar and second molar founded to move in upward direction with nearly the same value for both simulations. Second premolar and first molar moved in downward direction with nearly the same value for both simulations.

# **Discussion**

This 3D finite element study was conducted to find out the effects of the simulation of the flatting of the curve of Spee during orthodontic treatment over the force distribution on the lower jaw and lower teeth after tip‑back of premolars teeth. The instability of the COS flatting after orthodontic treatment is unheralded [36,37] and the role of long term of chewing force over its steadiness is unidentified. FEA is an estimated method to study both the stress distribution and the deformation consequential with forced bodies. Thus, the FEA has been broadly used in medical and dental sciences during the last decade in assessment the biomechanical effects of different treatment modalities.<sup>[30]</sup>

One of the dependable methods used for flatting of the COS—that recommended by Andrews 1972[15] is the extrusion of the infra erupted premolars to be in a flat plane with the incisors by the straight wire appliance,<sup>[38]</sup>this method was used to acquire a more stable orthodontic outcome.[1,39,40]

The amount of occlusal load during biting is different from subject to another depending on different factors. One of these factors is the thickness of the transducer used for testing, the thinner transducer the more reliable results. In order to simulate normal chewing function with a limited mouth opening, 2/3 of maximum bite

#### **Table 4: Von Mises stress and X, Y, and Z displacements of the teeth contact points**



\*(MP) Mega Pascal, \*\* (mm) millimeter

force (560 N) over the mesio-buccal cusp of lower first molar was applied.[35] In our FE model, the deepest point of the COS was (2.4 mm) which consider normal according to Bayadas *et al.*[9] and Ahmad *et al.*[27] Although, some authors considered up to 2 mm is normal Spee curve.<sup>[1]</sup>According to Koyama,<sup>[36]</sup>the deepest point of the COS located in the second premolar at the midpoint of the COS, compared with Shannon and Nanda<sup>[1]</sup>which claimed that high percentage of COS bottom located on the mesio‑buccal cusp of lower first molar. However, it's positioned moved distally during treatment and retain-back to their mesial position.<sup>[26,41]</sup>

Our hemi mandible model geometry was derived from real physical dimensions taken from the selected desiccated mandible and introduced to the FE program with 922592 nodes and 637,262 elements for more fine details on stress and strain distribution over the jaw.<sup>[42-44]</sup>

In the first curved model, with 2.4mm depth of the COS, the von mises stress was distributed throughout the mandible. The most stress concentration point was predetermined on the mesio‑buccal cusp tip of first permanent molar, this consider theoretically true as, this is the point of force application. While, high stress value was observed in the anterior mandibular condylar(ACo) and the posterior mandibular Condylar (PCo), because these are adjacent to our fixation area (mandibular Condyle), as the reaction force appeared in higher stress level, this agree with Basciftci *et al*. [45]and Wan *et al.*, [46] as they found that the stress accumulation appear at mandibular Condyle, as a result of the mandibular Condyle restraining in the simulation. This considers being representative finding, because the mandibular Condyle is connected to the cranium by several ligaments and muscles that limit the mandible movements during function.

Zero stress values was noted in Menton, Pogonion, Supramentale, Infradental, Central incisor edge and Coronoid, this is again accepted hypothetically because they were far from the point of force application and restriction area (the Condyle), this is once more coordinate with Basciftci *et al*. [45] findings; who mentioned that there was no stress accumulation occur in symphysis region as they located away from fixation and stress application points.

It seems that, the flatting of COS is a causative factor for increasing the values of von mises stress all through the mandible, as the PCo, ACo, and SCo stressed higher in flat model than in the curved. This could be related to facts that, the force acts along the long axis of the lower first molar. And according to the geometry of the mandible and the Condyle, the fixed area is subjected to higher stress, unlike in curve case, the force act on the first molar, which tilted mesially, that could lead to dissipation of the applied force and decrease the amount of stress over the Condyle (fixed area).

Baragar and Osborn<sup>[5]</sup> found a correlation between the Condyle angel (angle formed between the occlusal plane and Condyle slop) with biting angle (which represent the angle between the long axes of the tooth and the direction of the biting force). The biting angle increased in curve condition than in flat COS. As, the first permanent molar tend to tilt mesaily. Such mesial inclination is highly increased the efficiency of the biting force. After the flatting of the COS during orthodontic treatment, this biting angle will changed without compensatory changes in the Condyle angle. This could leads to high stress on the Condyle, especially at maximum bite force, as it is correlated to most posterior position of the Condyle to form zero Condyle angles. The continuous over load of the Condyle could lead to bone destruction and damage for the entire joint,[44] because the slope of two Condyles are related to occlusal plane in the frontal plane. In the same context, Kanavakis and Mahta<sup>[16]</sup>proclaimed that flatting of COS is a predisposing factor for TMJ sound as Condyle is more posteriorly positioned specially during growth as the posterior teeth less dis‑occluded during function, this will increase the load on TMJ during chewing leading to more sounds on it.

This could be explain the high percentage (60%) of recurrence of COS flatting noted by Shannon and Nanda[1] and Bayades *et al.*[9] as the teeth and mandible tend to establish the most suitable position with less amount of force distributed all around the mandible and lower teeth (see later).

In the same context, the deciduous teeth aligned parallel in flat level. During mandible growth and the permanent teeth eruption, the occlusal plane move downward and posteriorly away from the Condyle and the lower permanent molars teeth erupted with mesial inclination to form the COS.<sup>[47,48]</sup>So, we speculated that the high stress incorporated at the Condylein primary dentition (flat COS) could be correlated to stimulation of the growth at the Condyle in the early childhood.

#### **Von mises stress over the lower teeth**

The stress over the posterior teeth after COS flatting increased in posterior teeth than in anterior teeth[Table 4]. It is range from 32%, 26%, and 27% in second premolar, first molar and second molar respectively. This high stress over the first molar consider logical as they receive the applied load. The small size of the second premolar as well as its position near the point of applied force could be the responsible for the high stress value act over it. The second molar receive high stress, this could be related to its position related to site of force application and

the bending response of the mandible (see later).<sup>[49]</sup>This finding coordinate with previous conclusions concerning with high percentage of COS relapse and was related mainly to the second molar.<sup>[1]</sup>

While in the anterior teeth, and after the COS flatting, the von mises stress increased to 25%, 23% for central and lateral correspondingly. This could consider as a factor lead to relapse of the mandibular teeth crowding, this could be clarifying by the bending response of the mandible during chewing to overcome the biting force.<sup>[49]</sup> This finding agree with Shannon and Nada<sup>[1]</sup>results, as they conclude a parallel correlation between the COS relapse after flatting and the irregularity index of the lower anterior teeth. In another hand, this finding disagree with Kumara *et al.* conclusions,[50]as they found a weak negative correlation between the flat COS and the lower anterior teeth crowding. However, their sample was already present with flat COS. The canine represents the less stressed tooth at 22% to act as a stable guard for the integrity of the lower teeth.

These results are high light the role of the biting force on the relapse of COS after orthodontic treatment. This coordinates with Rozzi *et al*. [39] argument on the role of biting force on COS relapse.

Alignment of the teeth in flat plane increased the amount of the von miss stresses distribution over the contact points between each other. The whole, anatomy of the mandible with the Condyle, level of the occlusal plane as well as the angulations of the teeth in sagital plane are set in a harmony of coordination for biting force distribution. As, the COF is the inferior portion of the radius, that connect the Condyle with the occlusal surface of the posterior teeth and the incisor edge of the anterior teeth.[41] So, any changes in this harmony will leads to change in force distribution over the mandible.[49] As in our model, the mandible is originally incorporated with mesialy tilting of the posterior teeth. After re alignment of the teeth by tip back of the posterior teeth (changes the biting angle) with zero COS depth, it looks that this harmony is interrupted and the amount of stresses applied over the whole mandible is increased with raise in the amount of stresses and displacements with the same quantity of applied force. The mandibular Condyle takes the big responsibility for such alteration, as it consider the joining points that connecting the mandible with the cranial base.

# **Teeth displacement**

All the teeth were displaced lingually, and this could be due their alignment with lingual inclination in the space to coordinate the upper teeth following the fencing theory.[51]

The central and lateral incisors displaced lingually, distally, and superiorly. It seems that the lower anterior teeth were retroclined and compressed to each other during biting in the two models; this could be elucidating by the bending theory of the mandible during biting to overcome the biting force.[49] In spite of our model not incorporated the roots of the teeth, our result showed the role of the canine in supporting the teeth alignment as it the less tooth displace distally, this could be related to its position between the centrals and premolars to support the lower teeth alignments as well as in the angle of the hemi lower jaw. The first premolar also followed the anterior teeth in the manner of displacement. Also, the second premolar expressed higher distal displacements with downward shift, as it nearest point of force application (mesio‑buccal cusp of the lower first molar). The lower first molar (receptor of the applied force) displaced mesially and downwards. Finally the second molar displace mesially and upwards. This finding support the mandible bending theory, as the lateral ends of the bended object elevated and the nearest points are squeezed and move down ward. This finding agree with previous finding<sup>[49]</sup>as they stated that the teeth is displace under occlusal load. The amount of displacement found by our results differs from their results; however their model was used the upper teeth and lower teeth in occlusal form that could limit free movement of the teeth as in our model.

The range of mesial displacement of the anterior central and mesial surface of lateral was less than in curved plane than in flat one, this could be specified to our model that already has slight crowding in the anterior teeth.

One of the interesting results was that, in the curve model the amount of mesio‑distal displacements of the canine, premolars and molars were higher than in the flat one, this could be related the slope of posterior teeth alignment that could permit easily smooth teeth displacement over each other rather than in flat case, to overcome the masticatory forces.

# **Limitation of the study**

The main limitation of any FEA study could be the incorporation of the roots of the teeth as well as the PDL, which is highly, affects the reliability of the results. As, we dealt only with the crowns of the teeth that were already aligned in curve form and then we altered them in a flat arrangement. The additional limitation of this study is the used of the hemi mandible for force analysis. The use for whole mandible will complicated our mathematical calculations due to the inadequacy the software used in correlations with the numbers of the nodes included in the model. The other limitation could be the fixation of the mandibular Condyle in the FE model that is not harmonizes perfectly with the

normal situation, where it is attached to the cranial base with the ligaments and muscles that permit specific movements during function. The further limitation of this FE study could be the depending on the geometry of the specific mandible, as it is differing from subject to another. Finally, this study excludes the effect of occlusion of the teeth during function on the direction of teeth displacement.

#### **Clinical implication**

This study could be giving us an idea about the importance of the COS on force distribution over the mandible as well as the significance of the re-adjustments of the COS after finishing the comprehension orthodontic treatments. Re‑adjustment of the COS after orthodontic treatments play a role on the eliminations of the stresses over the Condyle and the lower anterior teeth as well as whole the mandible. Other researches could be conducted to search out the most suitable site and depth of COS along with the coordinate of force distributions throughout the mandible to increase the stability of our orthodontic out comes. Also, the alignments of the teeth in a curve form should be considered during posterior teeth implant, complete denture, and fixed prosthesis constructions.

# **Conclusions**

- 1. Flatting the COS by leveling of the premolars and tip back of molars is increasing the stresses over the Condyle, the teeth and the whole mandible.
- 2. The point of force application (mesio-buccal cusp of lower first molar) stressed 35% less in case of teeth aligned in curve form than in flat situation.
- 3. Posterior mandibular Condylar (PCo), anterior mandibular Condylar (ACo), and Superior mandibular Condylar (SCo) are stressed about 38%, 36%, 27% more in flat case than in curved model, respectively.
- 4. The canine is the less displaced and stressed tooth and has a role on the stability of the dental arch weather if the teeth are aligned in flat or curved planes.
- 5. The mandible is bending under occlusal load.
- 6. When the force applied on the mesio‑buccal cusp of the lower first molar, the second premolar and first molar displace inferiorly while all the other teeth are superiorly displaced.
- 7. All the mandibular teeth are displaced lingually during function.
- 8. The premolars and molars are more displaced than anterior teeth, when the teeth aligned in curved than in flat manner in the mesio‑distal direction.
- 9. The central, lateral, canine and first and second premolars displace distally under loading, while the first and second molars displace mesially under the same load for both models.
- 10.In flat model, maximum distal movement seen within central and lateral contact points. While in curve model, the maximum distal movement grasped within first and second premolars, in mesial and distal contact points.
- 11. All the lower teeth are displaced mesio‑distally in curve model, more than in flat replica.

#### **Abbreviations**

COS: Curve of Spee; TMJ: Tempro‑Mandibuler Joint; 3D: Three-dimensional; FEA: Finite Element Analysis; ACo: Anterior mandibular condylar; PCo Posterior Mandibular Condyle; SCo: Superior mandibular condylar; Ab: Anterior border of ramus (Ab);  $Go_{post}$ : Gonion posterior; Go: Gonion; Go<sub>ini</sub>: Gonioninferius; Me: Menton; Pog: Pogonion; B: Supramemtale; Id: Infradental; Cor: Coronoid.

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#### **References**

- 1. ShannonR, Nanda S. Changes in the curve of Spee with treatments and at 2 years post treatment. Am J OrthodDentofacOrthop 2004;125:589‑96.
- 2. Spee G, Biedenbach A, Hotz M, Hitchcock P. The gliding path of the mandible along the skull. J Am Dent Assoc 1890;100:670-5.
- 3. Hitchcock P. The curve of Spee in Stone Age man. Am J Orthod 1983;84:248‑53.
- 4. Osborn W. Orientation of the masseter muscle and the curve of Spee in relation to crushing forces on the molar teeth of primates. Am J PhysAnthropol1993;92:99-106.
- 5. Baragar FA, Osborn JW. Efficiency as a predictor of human jawdesign in the sagittal plane. JBiomech 1987;20:447‑57.
- 6. Marshall D, Caspursen M, Hardinger R, Franciscus G, Aquilino A, Southard E. Development of curve of Spee. Am J OrthodDentofacOrthop 2008;134:344‑52.
- 7. Dawson E. Functional Occlusion: From TMJ to Smile Design. 1st ed. St. Louis, Mo: Elsevier; 2006.p. 450.
- 8. Xu H, Suzuki T, Muronoi M, Okoya K. An evaluation of the curve of Spee in the maxilla and mandible of human permanent healthy dentitions. J Prosthet Dent 2008;92:344‑52.
- 9. Bayadas B, Yavus I, Atasaral N, Ceylan I, Dagsuyu M. Investigations of the changes in the positions of upper and lower incisors, overjet, overbite an irregularity index in subject with different depths of curve of Spee. Angle Orthod 2008;74:349‑55.
- 10. Harris F, Corruccini E. Quantification of dental occlusal variation: A review of methods. Dental Anthrop 2008;21:1‑11.
- 11. Adaškevičius R, Švalkauskienė V. Measurement of the depth of spee's curve using digital 3D dental models. Electronics and Electrical Engineering – Kaunas: Technologija 2011;3:53-6.
- 12. Burstone R. Deep overbite correction by intrusion. Am J Orthod 1977;72:1‑22.
- 13. Schudy F. The control of vertical overbite in clinical orthodontics. Angle Orthod 1968;38:19‑38.
- 14. Cordon NE. Post-treatment stability of deep bite malocclusions [thesis]. Oklahoma City: The University of Oklahoma; 1996.
- 15. Andrews L. The six keys to normal occlusion. Am J Orthod 1972;62:296‑309.
- 16. Kanavakis G, Mehta N. The role of occlusal curvatures and maxillary arch dimensions in patients with signs and symptoms of tempromandibular disorder. Angle Orthod 2014;84:96‑101.
- 17. Jeon D, Turley K, Moon B, Ting K. Analysis of stress in the periodontium of the maxillary first molar with a three-dimensional finite element model. Am J OrthodDentofacOrthop 1999;115:267‑74.
- 18. Nagahara K, Murata S, Nakamura S, TsuchiyaT. Displacementand stress distribution in the temporomandibular joint clenching. Angle Orthod 1999;69:372‑9.
- 19. Korioth P, Romilly P, Hannam G. Three‑dimensionalfinite element analysis of the dentate human mandible. Am J Phys Anthro 1992;88:69‑96.
- 20. Mohammed D, Desai H. Basic concepts of finite element analysis and its applications in dentistry. J Oral Hyg Health 2014;2:156.
- 21. Pritam M, Priyam M, Nivedita S, Sah S, Debapreeti M. Finite element method: A research tool in orthodontics. J Res Advanc Dent 2015;4:58‑63.
- 22. Şteţiu A, Oleksik V,Şteţiu M, Burlibaşa M, Trăistaru V, Oancea L, *et al*. Modelling and finite element method in dentistry. Rom Biotech Lett 2015;20:10579‑84.
- 23. Hsu M, Chang C. Application of finite element analysis in dentistry, finite element analysis. David Moratal, IntechOpen. 2010;3:43.
- 24. Braun L, Schmidt G. A cephalometric appraisal of the curve of Spee in Class I and Class II, Division 1 occlusions for males and females. Am J Orthod 1956;42:255‑78.
- 25. Braun S, Hnat P, Johnson E. The curve of Spee revisited. Am J OrthodDentofacOrthop1996;110:206-10.
- 26. Lie F, Kuitert R, Zentner A. Post-treatment development of the curve of Spee. Eur J Orthod 2006;28:262-8.
- 27. Ahmed I, Nazir R, Erum G, Ahsan T. Influence of malocclusion on the depth of curve of Spee. JPak Med Assoc 2011;61:1056‑9.
- 28. Kim K, ChaK, ChoiS, Jang I, YiJ, Jost‑BrinkmannG. Afinite element study on the effects of mid symphyseal distraction osteogenesis on the mandible and articular disc.Angle Orthod 2012;82:464‑71.
- 29. Katada H, Arakawa T, Ichimora K, Sueishi K, Samishima T. Stress distribution in the mandible and tempromandibular joint by mandibular distraction: A 3‑dimentional finite‑element analysis. Bull Tokyo Dent Coll 2009;50:161‑8.
- 30. Choi H, Ben‑ Nissan B, Conway C. Three‑dimensional modeling and finite element analysis of the human mandible during clenching.Aust Dent J 2006;50:42‑8.
- 31. Rees JS. An investigation into the importance of periodontal ligament and alveolar bone as supporting structures in finite element studies. J Oral Rehabil 2001;28:425–32.
- 32. Gei M, Genna F, Bigoni D. An interface model for the periodontal ligament. JBiomechEng 2002;124:538‑46.
- 33. Rho Y, Ashman B, Turner H. Young's modulus of trabecular and cortical bone material: Ultrasonic and micro tensile measurements. J Biomech 1993;26:111‑9.
- 34. Boccaccio A, Lamberti L, Pappalettere C, Cozzani M, Siciliani G.

Comparison of different orthodontic devices for mandibular symphyseal distraction osteogenesis: A finite element study. Am J OrthodDentofacOrthop 2008;134:260‑9.

- 35. Al Qassar SS, Mavragani M, Psarras V, Halazonetis DJ. The anterior component of occlusal force revisited: Direct measurement and theoretical considerations. Eur J Orthod2016;38:190-6.
- 36. Koyama T. A comparative analysis of the curve of Spee (lateral aspect) before and after orthodontic treatment‑with particular reference to overbite patients. J Nihon UnivSch Dent 1997;21:25‑34.
- 37. Garcia R. Leveling the curve of Spee: A new prediction formula. J Charles H Tweed Int Found1985;13:65‑72.
- 38. Pandis N, Polychoronopoulou A, Sifakakis I, Makou M, Eliades T. Effects of leveling of the curve of spee on the proclination of the mandibuler incisors and expansion of the dental arch: A prospective clinical trial. Austral Orthod J 2010;26:61-5.
- 39. Rozzi M, Mucedero M, Pezzuto C, Cozza P. Leveling the curve of spee with continuous arch wire appliances in different vertical skeletal patterns: A retrospective study. Am J OrthodDentofacOrthop 2017;151:758‑66.
- 40. Rozzi M, Mucedero M, Pezzuto C, Lione R. Cozza P. Long term stability of the curve of the spee leveled by continuous archwires in subjects with different vertical patterns: A retrospective study. Eur J Orthod 2019;41:286-93.
- 41. Surendran SV, Hussain S, Bhoominthan S, Nayar S, Jayesh R. Analysis of the curve of Spee and the curve of Wilson in adult Indian population: A three-dimensional measurement study. J Indian Prosthodont Soc 2016;16:335‑9.
- 42. Magne P, Bulser UC. Rationalization of shape and related stress distribution in posterior teeth: A finite element study using nonlinear contact analysis. Int J Periodontics Restorative Dent 2002;22:3‑11.
- 43. Gupta K, Knoell C, Grenoble E. Mathematical modeling and structural analysis of the mandible. Med DevucesArtif Organs 1973;1:469‑79.
- 44. Knoell C. A mathematical model of an *in vitro* human mandible. J Biomech 1977;10:159‑66.
- 45. Basciftci A, Korkmaz H, Iseri H, Malkoc S. Biomechanical evaluation of Mandibular midline distraction osteogensis by using the finite element method. Am J Orthod Dento fac Orthop 2004;125:706‑15.
- 46. Wan M, Bi M, Han H, WangY. A three‑ dimensional finite element study of the tempromandibular joint with different curve of Spee. (Zhonghua Kou Qiang Yi XueZaZhi) 2012;47:277. (abs).
- Orthlieb D. The curve of Spee: Understanding the sagittal organization of mandibular teeth. Cranio 1997;15:333‑40.
- 48. Fukoe H, Basilli C, Slavicek R, Sato S, Akimoto S. Three dimentional analysis of the mandible and occlusla architecture of mandibuler dentition. J Stomat Occ Med 2012;5:119‑29.
- 49. Gomes De Oliveira S, Seraidarianp I, landrejrj J, Oliveira D, Cavalcanti N. Tooth displacement due to occlusal contacts: A three dimensional finite element study. J Oral Rehabil 2006;33:874‑80.
- 50. Kumara N, Fida M, Shaikh A. Exploration of variation in positions of upper and lower incisors, over jet, overbite, and irregularity index in orthodontic patients with dissimilar depth of Curve of Spee. J AyoubMedColl Abbottabad 2016;28:766‑72.
- 51. Mehta N, Abdallah E, Lobo-Lobo S, Ceneviz C, Correa L. Three dimensional assessment of dental occlusion (occlusal fencing): A clinical technique. Head, Face, and Neck Pain Science, Evaluation, and Management. 1<sup>st</sup> ed. Hoboken, New Jersey: John Wiley & Sons Inc.; 2009.p. 435–55.