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Does the flatting of the curve of spee affect the chewing force distribution in the mandible? (3D finite element study)

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Abstract:

OBJECTIVE: To search the effects of Curve of Spee (COS) flatting on the stresses and displacement on the different mandible landmarks and lower teeth during posterior teeth loading using three-dimensional (3D) finite element analysis.

MATERIALS AND METHODS: Three-dimensional hemi mandibular model was created from real selected mandible. The lower teeth was aligned originally in a curved form with 2.4 mm depth at the cusp tip of the second premolar. Another replica with flat aligned teeth was formed to confirm the analysis by up righting premolars and molars. A load was applied at mesio-buccal cusp of the lower first molar on both models, and the resultant stresses and displacements on the mandibular landmarks and the lower teeth were tested.

RESULTS: Von mises over the mandible was higher in flat than in curve model. The highest stress levels were detected at the Mesio-buccal cusp tip of first molar for flat and curved simulation (5053, 3304) Mpa respectively. Mesio-distally, the teeth displacement was higher in curve model than in flat one. The maximum distal displacement, in flat model, was seen in central and lateral incisors. While, in curve model, the maximum distal displacement was grasped within first and second premolars.

CONCLUSIONS: Flatting the COS magnify the stresses over whole mandible and reduce lower teeth displacement mesio-distally. We speculated that the readjustment of the COS after orthodontic treatment could reduce the stress and displacements on the lower anterior teeth and decrease the lower anterior teeth crowding relapse.

Keywords:

Chewing force, curve of Spee, finite element, lower anterior crowding

Introduction

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Submitted: 17-Jul-2020 Revised: 25-Jul-2020 Accepted: 31-Jul-2020 Published: 19-Feb-2021 The Curve of Spee (COS) is an identifying characteristic of normal alignment of the lower teeth which had been observed in the sagittal profile view of the human skulls,^[1] It was first noted by Graf Von Spee in 1890.^[2] Recent studies described it, as a curvature extended from disto-buccal cusps of the most posterior teeth to the incisor edge of the central's incisors.^[3] The Literatures

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stated that COS developed as a result of the mesial tilting of the long axis of the lower molar teeth incompetence to the efficiency of muscles of mastication.^[4-6] COS improves food chewing throughout preserving upper and lower teeth contacts during function as it enhances free lower jaw movements.^[2] Also, COS has a role in facial aesthetic through its enterprise of an esthetical smile.^[7]

COS was evaluated by two main techniques; the first one: as a radius of inferior portion of circle that extended from anterior border of the Condyle to the buccal cusps of second and

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first molar, and pass to contact the cusp tips of premolars and canine respectively, and terminated on the incisor edge of the two central incisors.^[8] The second technique of COS evaluation was depending on the arch length and depth of the posterior teeth according to the occlusal plane.^[9]

However, there is a disagreement about the measurement methodology for COS. Some authors excluded lower incisors during measurements of Spee's curve. As, they are (sometimes) super-erupted, and a raised COS depth was obtained.^[10]

Recently, with advance technology improvements and the used of three-dimensional (3D) scanner, COS measurement became more easy and accurate by using a digital cast analysis. While, previously all the measurements were obtained from hard study models or their photographs, using a divider, calliper, and a coordinate apparatus.^[11]

During comprehensive orthodontic treatment, leveling of COS of the mandibular teeth is imperative step to establish proper incisors relation and posterior teeth occlusion, especially for deep bite correction^[12,13]; however, there are disagreements according to COS leveling techniques used to improve the stability of the orthodontic outcomes.^[14] Since 1972, Andrews^[15] advised leveling the COS to a flat plane to assist the construction of an optimal occlusion, regardless of its effects on the mandible or Tempro-mandibular joint (TMJ) or even the lower teeth. As, Kanavakis and Mehta^[16]found a correlation between the sound in TMJ with the COS flatting.^[16]

The finite element analysis (FEA) technique has been wildly used to study the dynamics of the stomatognathic system.^[17]It has a capacity for analyzing the frequency, intensity, direction, duration, and of occlusal forces, also it unable to study mandibular biomechanics and to evaluate deformations, tensions, and displacements that may occur throughout the mandible.^[18,19] The amazing advantage of this FEA is the study of areas that are impossible to access without any risks to the human.^[17,19]

Stability of the COS as well as orthodontic outcomes after orthodontic treatment is a matter of arguments.^[1] As there are no clear clarifications for such relapse. The role of the light continuous force which is produced during daily chewing could be a factor for such deterioration. So, this study was aimed to find out the variations in stresses and displacements after flatting COS, on the mandible and lower teeth during posterior teeth biting, using the FEA.

Method and Materials

This study is coordinating with the roles of the ethics committee of the college of Dentistry/University of Mosul/Iraq no. 4S/475 in 25/3/2019.

All the necessary procedures for FEA and model constriction were carried out as model creations, definitions of the elements form and the properties of the material under load application as well as boundary condition and load application.^[20-23]

In the current study, 30 skulls for males (judged by three orthodontists to be normal by visual inspections) were examined. Only 10 skulls followed our inclusion criteria, which include: full dentition excluding third molar, class I molar and canine relationships, and without any sever crino-facial abnormalities. The COS of the lower teeth of the 10 selected skulls were measured according to previously authorized methods.[24-26] The depth of the bottom of COS was calculated using a Mitutoyo electronic caliper (Mitutoyo, Kawasaki, Japan) as the vertical distance between the deepest cusp tip and occlusal flat plane (a flat metal ruler was seated over the teeth for COS evaluation). The COS line was passed over the mandibular dental teeth extending from the incisal edge of the centrals, passing over the cusp tips of the canine and premolars to touch the mesio-buccal cusp of the lower first molar to the distal cusp tips of the lower second molar [Figure 1]. The average depth of COS for the 10 selected mandibles was $2.4 (\pm 0.24)$ mm. The mandible which have a COS depth value near the average (2.4 mm) was selected to be our target model to be use for FEA (The deepest point of it was on the cusp tip of the second premolar). However, this depth value is compatible with previous study.^[27] Auto cad (2010) Program was used for drawing 3D model of one half of mandible^[23,28] which was analog to the selected mandible. The previous authorized methods were used to create our 3D model.^[29,30] All the linear measurements were taken using a Mitutoyo electronic caliper from the selected mandible. The periodontal ligaments were excluded in this study, because of the difficulties in mechanical modeling as well as the complexity of its mesh mathematical calculations.^[31,32] The first model was



Figure 1: Schematic the curve of Spee extension and its bottom on the cusp tip of the lower second premolar

duplicated to create the second one. The teeth in second model were aligned with a flat plane, in order to simulate flatting of COS after orthodontic treatment, by upright the lower first and second premolars.

The two models were transported to finite element program (Autodesk Inventor Professional Computer Program (version 2012)), the mechanical properties of the materials were considered to be homogenous, isotropic, and linear elastic as in most reported studies^[23,28,30];only two independent material properties, Young's modulus and Poisson's ratio were present in an isotropic material. Cancellous bone network ignored in most FEA studies.^[21,23]Therefore, it was assumed that cancellous bone has a solid design inside the inner cortical bone shell.^[23] The Young's modulus and Poisson's ratio for cortical and cancellous bone were considered according to the ultrasound study of Rho *et al.*^[33], while teeth properties were identified according to Boccaccio *et al.*^[34], as in Table 1.

The mandible was supported by restraining all the movements at the top of the Condyle^[23,32]resembling Glenoid fossa, as the boundary conditions. The models were discredited to many elements; each element containing numbers of apexes called nodes; the organization of elements and nodes called the finite element mesh. Finite element results are very critical to the number of elements included in the model. Our final mesh was consisted of 922,592 nodes, 637,262 elements. The force applied was (560N) perpendicular on the mesio-buccal cusp of the first permanent molar for both replicas which represent 75% of the maximum chewing force to simulate natural chewing^[35], as shown in Figure 2.

Table 1: Material mechanical properties for FEA usedin this study

Material	Young's modulus (GPa*)	Poisson's ratio		
Cortical bone	20.7**	0.3		
Cancellous bone	14.8 **	0.3		
Teeth	18.6***	0.31		

*GPaGega Pascal, **Rho et al., 1993^[33], ***Boccaccio et al., 2008^[34]



Figure 2: Schematic of the three-dimensional model of hemi mandible after meshing and the site of force application

In order to detect the amount of teeth displacements, the mesial and distal contact points of each tooth were observed in both models after load application.

Results

The results in term of Von mises and displacement in three dimensions (X, Y, and Z) were studied. A color scale (12 colors scale and 13 values) was used for quantitative visualization of the stress distribution and displacement of our models as shown in Figure 3. The maximum values for Von mises stress and displacement for both models were labeled in Table 2.

The von mises stress and X, Y, and Z displacement, for different anatomical landmarks plotted through the mandible for flat and curve conditions are labeled in Table 3 and displayed in Figures 4-11.

Von mises stresses of Mandibular landmarks

When the teeth simulated to be flattened the maximum value for von mises stress were higher than the maximum von mises value within curved plane. The highest stress levels were detected in the mesio-buccal cusp tip of first molar for both simulation (flat and curved plane) (5053, 3304) Mpa respectively. High stress values for both simulations (flat and curved plane) were seen within Anterior mandibular condylar (ACo) (2135, 1370) Mpa, respectively. While, Moderate stress level observed in posterior mandibular Condyle (PCo) in both simulation (1478, 912) Mpa respectively, and these values decrease gradually to the posterior border of mandible (119,41) Mpa. Low stress level was seen in the Superior mandibular condylar (SCo) (26,19) Mpa, Anterior border of ramus (Ab) (41,23) Mpa, Jlat (30,18) Mpa, Jmed (15,2) Mpa, Gonion posterior (Go_{post}) (10,2) Mpa, Gonion (Go) (5,3) Mpa and Gonioninferius (Go_{inf}) (17,4) Mpa for both imitation flat and curve one-to-one. Zero stress values seen in Menton (Me), Pogonion (Pog), Supramemtale (B), Infradental (Id), Central incisor edge and Coronoid, as in Figures 4 and 5.



Figure 3: Schematic probe command in Autodesk Inventor Professional Computer Program

Mandiblular anatomical landmarks Displacement

Maximum displacement seems to be nearly the same for both models in all three directions. Zero movement was detected in Posterior mandibular condylar (PCo), Anterior mandibular condylar (ACo), and Superior mandibular condylar (SCo). The presentation of X, Y, and Z for displacement depend on how you set your model according to these global coordinate.

X-displacement

X-displacement was illustrated as anterio-posterior (sagittal) movement of mandible, positive value indicate back ward (distally) displacement, negative value specify mesial (forward) displacement. The highest positive X-displacement was seen in the Gonioninferius (Go_{inf}) (+0.117, +0.110) mm, Gonion (Go) (+0.112,+0.110)) mm for flat and curve simulation respectively, and extended along the inferior border of the mandible. The high value for distal X-movement were observed in Gonion posterior (Go_{post}) (+0.099, +0.104) mm and Menton (Me) (+0.078,+0.082) mm for both flat and curve simulations respectively. Moderate positive X-displacements for both models were detected within Posterior border of ramus (Pb) (+0.057, +0.086) mm,

Table 2: Maximum Von Mises stress and displacement values for flat and curve models

Flat model	Curve model					
5411	3452					
0.119	0.1187					
0.2579	0.26					
0.4548	0.4561					
	Flat model 5411 0.119 0.2579 0.4548					

Coronoid (Cor) (+0.052,+0.057) mm, Anterior border of ramus (Ab) (+0.024, +0.046) mm, Pogonion (Pog) (+0.037, +0.065) mm and Central incisor edge (+0.042, +0.026) mm respectively. Less positive X-displacement was noted Supramentale (B) and Infradental (Id). While, negative (mesial) X-displacement was noted in mesio-buccal cusp tip of first molar, J_{lat} and $J_{med'}$ as shown in Figures 6 and 7.

Y-displacement

Y-displacement specify transverse (in–out) movement, positive value means inward twisting of the mandible. The mandible under masticatory force simulation was bended in inward direction, the highest value in both flat and curve models were noticed inMenton (Me)(+0.257, +0.259) mm and Pogonion (Pog) (+0.237,+0.254) mm respectively. High inward bending was seen in Supramentale (B) (+0.227, +0.230) mm, Infra-dental (Id)(+0.2134,+0.225) mm and central incisor edge (+0.206,+0.213) mm respectively. Moderate Y-displacement for both simulation were detected within mesio-buccal cusp tip of



Figure 4: Schematic the magnitude and distribution of Von mises stress in flat model

*(MPa) Mega Pascal, ** (mm) millimeter

Table 3: Von Mises stress and displacement in different anatomical landmarks

Land marks	Flat von	Curve von	Flat	Curve	Flat	Curve	Flat	Curve
	mises	mises	X-displace	X-displace	Y-displace	Y-displace	Z-displace	Z-displace
	(Mpa)	(Mpa)	(mm)	(mm)	(mm)	(mm)	(mm)	(mm)
Posterior mandibular condylar (PCo)	1478	912	0	0	0	0	0	0
Anterior mandibular condylar (ACo)	2135	1370	0	0	0	0	0	0
Superior mandibular condylar (SCo)	26	19	0	0	0	0	0	0
Coronoid (Cor)	0	0	+0.052	+0.057	+0.003	+0.002	0.083	-0.090
Anterior border of ramus (Ab)	41	23	+0.024	+0.046	+0.073	+0.091	0.151	-0.164
Posterior border of ramus (Pb)	119	41	+0.057	+0.086	+0.021	+0.040	+0.006	+0.020
Jlat	30	18	0.050	0.056	+0.100	+0.116	+0.176	+0.198
Jmed	15	2	0.013	0.009	+0.095	+0.086	+0.199	+0.187
Gonion posterior (Go _{post})	10	2	+0.099	+0.104	+0.058	+0.074	+0.048	+0.073
Gonion (Go)	5	3	+0.112	+0.110	+0.080	+0.084	+0.080	+0.088
Gonioninferius (Go _{inf})	17	4	+0.117	+0.110	+0.088	+0.089	+0.092	+0.098
Menton (Me)	0	0	+0.078	+0.082	+0.257	+0.259	+0.446	+0.443
Pogonion (Pog)	0	0	+0.037	+0.065	+0.237	+0.254	+0.442	+0.447
Supramemtale (B)	0	0	+0.005	+0.016	+0.227	+0.230	+0.447	+0.445
Infradental (Id)	0	0	+0.019	+0.005	+0.213	+0.225	+0.444	+0.445
Central incisor edge	0	0	+0.042	+0.026	+0.206	+0.213	+0.450	+0.451
Mesio-buccal cusp tip of first molar	5053	3304	0.007	0.049	+0.147	+0.155	0.300	-0.300

(MP) Mega Pascal, (mm) millimeter

first molar(+0.147,+0.155) mm, J_{lat} (+0.100, +0.116) mm, and J_{med} (+0.095,+0.086) mm, Gonioninferius (Go_{inf}) (+0.088,+ 0.089) mm, Gonion (Go)(+0.080,+0.084) mm, Anterior border of ramus (Ab)(+0.073,+0.091) mm, and Gonion posterior (Go_{post}) (+0.058,+0.074) mm in sequence. Low Y-displacement was seen in Coronoid (Cor) and Posterior border of ramus (Pb), see Figures 8 and 9.

Z-displacement

Z-displacement identify vertical (up–down) movement, positive values pointed to upward movement of the mandible negative values indicate downward displacement. Maximum positive values (upward movement) seen within central incisor edge (+0.450,+0.451) mm, Supramentale (+0.447,+0.445) mm, Infradental (+0.444,+0.445) mm, Pogonion (+0.442,+0.447)



Figure 5: Schematic the magnitude and distribution of Von mises stress in curve plane



Figure 7: Schematic the magnitude and distribution of X-displacement incurve plane



Figure 9:Schematic the magnitude and distribution of Y-displacement in curve plane

mm and Menton (+0.446,+0.443) mm for both flat and curved models respectively. Highest positive z-displacement seen in Jmed (+0.199, +0.187) mm and Jlat(+0.176,+0.198) mm, the high positive displacement detected within Goinf(+0.092,+0.098) and Go(+0.080,+0.088) mm, moderate upward movement seen in Gopost(+0.048,+0.073) mm, low values noted within Pb(+0.006,+0.02) mm respectively for flat and curve simulations. While, negative (downward) Z-movement noted within Coronoid (Cor), Anterior border of ramus (Ab), mesio-buccal cusp tip of first molar. High downward displacement grasped in mesio-buccal cusp tip of first molar (0.300, 0.3) mm for both models correspondingly. Moderate negative Z-movement values observed in Ab (0.151, 0.164) mm while Lowest values noted in Cor (0.083, 0.090) mm for both simulations respectively. See Figures 10 and 11.



Figure 6: Schematic the magnitude and distribution of X-displacement in flat plane



Figure 8: Schematic the magnitude and distribution of Y-displacement in flat plane



Figure 10:Schematic the magnitude and distribution of Z-displacement in flat plane

Teeth displacement and contact points stresses *Teeth Von miss stresses*

Table 4 shows the von miss stresses of all the contact points between the lower teeth.

Teeth X-displacement

For central, lateral, canine, first and second premolars, mesial, and distal contact point were founded to displace distally. In flat model, maximum distal movement seen within central mesial, distal, and lateral mesial contact point. While in curve model, the maximum distal movement grasped within first and second premolars, in mesial and distal contact points. In first and second molars, the mesial and distal contact points seem to move mesially for both simulations, this movement was higher in curve model than flat one, as in Table 4.

Teeth Y-displacement

All teeth seem to move lingually in both models with high value seen in central teeth and decrease gradually to the lowest value in second molar distal contact point, please see Table 4.



Figure 11: Schematic the magnitude and distribution of Z-displacement in curve plane

Teeth Z-displacement

Table 4 shows the teeth contact points displacements and stress. Central, lateral, canine, first premolar and second molar founded to move in upward direction with nearly the same value for both simulations. Second premolar and first molar moved in downward direction with nearly the same value for both simulations.

Discussion

This 3D finite element study was conducted to find out the effects of the simulation of the flatting of the curve of Spee during orthodontic treatment over the force distribution on the lower jaw and lower teeth after tip-back of premolars teeth. The instability of the COS flatting after orthodontic treatment is unheralded ^[36,37] and the role of long term of chewing force over its steadiness is unidentified. FEA is an estimated method to study both the stress distribution and the deformation consequential with forced bodies. Thus, the FEA has been broadly used in medical and dental sciences during the last decade in assessment the biomechanical effects of different treatment modalities.^[30]

One of the dependable methods used for flatting of the COS—that recommended by Andrews 1972^[15] is the extrusion of the infra erupted premolars to be in a flat plane with the incisors by the straight wire appliance,^[38]this method was used to acquire a more stable orthodontic outcome.^[1,39,40]

The amount of occlusal load during biting is different from subject to another depending on different factors. One of these factors is the thickness of the transducer used for testing, the thinner transducer the more reliable results. In order to simulate normal chewing function with a limited mouth opening, 2/3 of maximum bite

Table 4: Von Mises stress and X, Y, and Z displacements of the teeth contact points

Land marks	Flat von mises (Mpa)*	Curve von mises (Mpa)*	Flat X- dis place (mm)**	Curve X-dis place (mm)**	Flat Y-dis place (mm)	Curve Y-dis place (mm)**	Flat Z-dis place (mm)**	Curve Z-dis place (mm)**
Central mesial contact point	156	112	+0.036	+0.019	+0.206	+0.218	+0.445	+0.454
Central distal contact point	180	125	+0.028	+0.009	+0.203	+0.216	+0.430	+0.437
Lateral mesial contact point	193	146	+0.020	+0.011	+0.200	+0.217	+0.430	+0.435
Lateral distal contact point	214	168	+0.014	+0.016	+0.194	+0.204	+0.400	+0.403
Canine mesial contact point	248	189	+0.006	+0.011	+0.197	+0.206	+0.400	+0.402
Canine distal contact point	277	218	+0.008	+0.017	+0.190	+0.194	+0.377	+0.377
First premolar mesial contact point	300	223	+0.010	+0.021	+0.186	+0.196	+0.370	+0.375
First premolar distal contact point	357	259	+0.010	+0.022	+0.170	+0.178	+0.342	+0.340
Second premolar mesial contact point	400	270	+0.014	+0.029	+0.175	+0.180	0.340	0.339
Second premolar distal contact point	429	301	+0.015	+0.033	+0.155	+0.161	0.300	0.301
First molar mesial contact point	450	330	0.016	0.031	+0.150	+0.162	0.300	0.300
First molar distal contact point	432	314	0.019	0.038	+0.137	+0.139	0.260	0.260
Second molar mesial contact point	421	308	0.028	-0.033	+0.138	+0.141	+0.260	+0.260
Second molar distal contact point	400	285	0.030	0.035	+0.117	+0.118	+0.220	+0.222

*(MP) Mega Pascal, ** (mm) millimeter

force (560 N) over the mesio-buccal cusp of lower first molar was applied.^[35] In our FE model, the deepest point of the COS was (2.4 mm) which consider normal according to Bayadas *et al.*^[9] and Ahmad *et al.*^[27] Although, some authors considered up to 2 mm is normal Spee curve.^[1]According to Koyama,^[36]the deepest point of the COS located in the second premolar at the midpoint of the COS, compared with Shannon and Nanda^[1]which claimed that high percentage of COS bottom located on the mesio-buccal cusp of lower first molar. However, it's positioned moved distally during treatment and retain-back to their mesial position.^[26,41]

Our hemi mandible model geometry was derived from real physical dimensions taken from the selected desiccated mandible and introduced to the FE program with 922592 nodes and 637,262 elements for more fine details on stress and strain distribution over the jaw.^[42-44]

In the first curved model, with 2.4mm depth of the COS, the von mises stress was distributed throughout the mandible. The most stress concentration point was predetermined on the mesio-buccal cusp tip of first permanent molar, this consider theoretically true as, this is the point of force application. While, high stress value was observed in the anterior mandibular condylar (ACo) and the posterior mandibular Condylar (PCo), because these are adjacent to our fixation area (mandibular Condyle), as the reaction force appeared in higher stress level, this agree with Basciftci et al.^[45] and Wan et al.,^[46] as they found that the stress accumulation appear at mandibular Condyle, as a result of the mandibular Condyle restraining in the simulation. This considers being representative finding, because the mandibular Condyle is connected to the cranium by several ligaments and muscles that limit the mandible movements during function.

Zero stress values was noted in Menton, Pogonion, Supramentale, Infradental, Central incisor edge and Coronoid, this is again accepted hypothetically because they were far from the point of force application and restriction area (the Condyle), this is once more coordinate with Basciftci *et al.*^[45] findings; who mentioned that there was no stress accumulation occur in symphysis region as they located away from fixation and stress application points.

It seems that, the flatting of COS is a causative factor for increasing the values of von mises stress all through the mandible, as the PCo, ACo, and SCo stressed higher in flat model than in the curved. This could be related to facts that, the force acts along the long axis of the lower first molar. And according to the geometry of the mandible and the Condyle, the fixed area is subjected to higher stress, unlike in curve case, the force act on the first molar, which tilted mesially, that could lead to dissipation of the applied force and decrease the amount of stress over the Condyle (fixed area).

Baragar and Osborn^[5] found a correlation between the Condyle angel (angle formed between the occlusal plane and Condyle slop) with biting angle (which represent the angle between the long axes of the tooth and the direction of the biting force). The biting angle increased in curve condition than in flat COS. As, the first permanent molar tend to tilt mesaily. Such mesial inclination is highly increased the efficiency of the biting force. After the flatting of the COS during orthodontic treatment, this biting angle will changed without compensatory changes in the Condyle angle. This could leads to high stress on the Condyle, especially at maximum bite force, as it is correlated to most posterior position of the Condyle to form zero Condyle angles. The continuous over load of the Condyle could lead to bone destruction and damage for the entire joint,^[44] because the slope of two Condyles are related to occlusal plane in the frontal plane. In the same context, Kanavakis and Mahta^[16]proclaimed that flatting of COS is a predisposing factor for TMJ sound as Condyle is more posteriorly positioned specially during growth as the posterior teeth less dis-occluded during function, this will increase the load on TMJ during chewing leading to more sounds on it.

This could be explain the high percentage (60%) of recurrence of COS flatting noted by Shannon and Nanda^[1] and Bayades *et al.*^[9] as the teeth and mandible tend to establish the most suitable position with less amount of force distributed all around the mandible and lower teeth (see later).

In the same context, the deciduous teeth aligned parallel in flat level. During mandible growth and the permanent teeth eruption, the occlusal plane move downward and posteriorly away from the Condyle and the lower permanent molars teeth erupted with mesial inclination to form the COS.^[47,48]So, we speculated that the high stress incorporated at the Condylein primary dentition (flat COS) could be correlated to stimulation of the growth at the Condyle in the early childhood.

Von mises stress over the lower teeth

The stress over the posterior teeth after COS flatting increased in posterior teeth than in anterior teeth [Table 4]. It is range from 32%, 26%, and 27% in second premolar, first molar and second molar respectively. This high stress over the first molar consider logical as they receive the applied load. The small size of the second premolar as well as its position near the point of applied force could be the responsible for the high stress value act over it. The second molar receive high stress, this could be related to its position related to site of force application and

the bending response of the mandible (see later).^[49]This finding coordinate with previous conclusions concerning with high percentage of COS relapse and was related mainly to the second molar.^[1]

While in the anterior teeth, and after the COS flatting, the von mises stress increased to 25%, 23% for central and lateral correspondingly. This could consider as a factor lead to relapse of the mandibular teeth crowding, this could be clarifying by the bending response of the mandible during chewing to overcome the biting force.^[49] This finding agree with Shannon and Nada^[1]results, as they conclude a parallel correlation between the COS relapse after flatting and the irregularity index of the lower anterior teeth. In another hand, this finding disagree with Kumara et al. conclusions,^[50]as they found a weak negative correlation between the flat COS and the lower anterior teeth crowding. However, their sample was already present with flat COS. The canine represents the less stressed tooth at 22% to act as a stable guard for the integrity of the lower teeth.

These results are high light the role of the biting force on the relapse of COS after orthodontic treatment. This coordinates with Rozzi *et al.*^[39] argument on the role of biting force on COS relapse.

Alignment of the teeth in flat plane increased the amount of the von miss stresses distribution over the contact points between each other. The whole, anatomy of the mandible with the Condyle, level of the occlusal plane as well as the angulations of the teeth in sagital plane are set in a harmony of coordination for biting force distribution. As, the COF is the inferior portion of the radius, that connect the Condyle with the occlusal surface of the posterior teeth and the incisor edge of the anterior teeth.^[41] So, any changes in this harmony will leads to change in force distribution over the mandible.^[49] As in our model, the mandible is originally incorporated with mesialy tilting of the posterior teeth. After re alignment of the teeth by tip back of the posterior teeth (changes the biting angle) with zero COS depth, it looks that this harmony is interrupted and the amount of stresses applied over the whole mandible is increased with raise in the amount of stresses and displacements with the same quantity of applied force. The mandibular Condyle takes the big responsibility for such alteration, as it consider the joining points that connecting the mandible with the cranial base.

Teeth displacement

All the teeth were displaced lingually, and this could be due their alignment with lingual inclination in the space to coordinate the upper teeth following the fencing theory.^[51] The central and lateral incisors displaced lingually, distally, and superiorly. It seems that the lower anterior teeth were retroclined and compressed to each other during biting in the two models; this could be elucidating by the bending theory of the mandible during biting to overcome the biting force.^[49] In spite of our model not incorporated the roots of the teeth, our result showed the role of the canine in supporting the teeth alignment as it the less tooth displace distally, this could be related to its position between the centrals and premolars to support the lower teeth alignments as well as in the angle of the hemi lower jaw. The first premolar also followed the anterior teeth in the manner of displacement. Also, the second premolar expressed higher distal displacements with downward shift, as it nearest point of force application (mesio-buccal cusp of the lower first molar). The lower first molar (receptor of the applied force) displaced mesially and downwards. Finally the second molar displace mesially and upwards. This finding support the mandible bending theory, as the lateral ends of the bended object elevated and the nearest points are squeezed and move down ward. This finding agree with previous finding^[49]as they stated that the teeth is displace under occlusal load. The amount of displacement found by our results differs from their results; however their model was used the upper teeth and lower teeth in occlusal form that could limit free movement of the teeth as in our model.

The range of mesial displacement of the anterior central and mesial surface of lateral was less than in curved plane than in flat one, this could be specified to our model that already has slight crowding in the anterior teeth.

One of the interesting results was that, in the curve model the amount of mesio-distal displacements of the canine, premolars and molars were higher than in the flat one, this could be related the slope of posterior teeth alignment that could permit easily smooth teeth displacement over each other rather than in flat case, to overcome the masticatory forces.

Limitation of the study

The main limitation of any FEA study could be the incorporation of the roots of the teeth as well as the PDL, which is highly, affects the reliability of the results. As, we dealt only with the crowns of the teeth that were already aligned in curve form and then we altered them in a flat arrangement. The additional limitation of this study is the used of the hemi mandible for force analysis. The use for whole mandible will complicated our mathematical calculations due to the inadequacy the software used in correlations with the numbers of the nodes included in the model. The other limitation could be the fixation of the mandibular Condyle in the FE model that is not harmonizes perfectly with the

normal situation, where it is attached to the cranial base with the ligaments and muscles that permit specific movements during function. The further limitation of this FE study could be the depending on the geometry of the specific mandible, as it is differing from subject to another. Finally, this study excludes the effect of occlusion of the teeth during function on the direction of teeth displacement.

Clinical implication

This study could be giving us an idea about the importance of the COS on force distribution over the mandible as well as the significance of the re-adjustments of the COS after finishing the comprehension orthodontic treatments. Re-adjustment of the COS after orthodontic treatments play a role on the eliminations of the stresses over the Condyle and the lower anterior teeth as well as whole the mandible. Other researches could be conducted to search out the most suitable site and depth of COS along with the coordinate of force distributions throughout the mandible to increase the stability of our orthodontic out comes. Also, the alignments of the teeth in a curve form should be considered during posterior teeth implant, complete denture, and fixed prosthesis constructions.

Conclusions

- 1. Flatting the COS by leveling of the premolars and tip back of molars is increasing the stresses over the Condyle, the teeth and the whole mandible.
- 2. The point of force application (mesio-buccal cusp of lower first molar) stressed 35% less in case of teeth aligned in curve form than in flat situation.
- 3. Posterior mandibular Condylar (PCo), anterior mandibular Condylar (ACo), and Superior mandibular Condylar (SCo) are stressed about 38%, 36%, 27% more in flat case than in curved model, respectively.
- 4. The canine is the less displaced and stressed tooth and has a role on the stability of the dental arch weather if the teeth are aligned in flat or curved planes.
- 5. The mandible is bending under occlusal load.
- 6. When the force applied on the mesio-buccal cusp of the lower first molar, the second premolar and first molar displace inferiorly while all the other teeth are superiorly displaced.
- 7. All the mandibular teeth are displaced lingually during function.
- 8. The premolars and molars are more displaced than anterior teeth, when the teeth aligned in curved than in flat manner in the mesio-distal direction.
- 9. The central, lateral, canine and first and second premolars displace distally under loading, while the first and second molars displace mesially under the same load for both models.

- 10. In flat model, maximum distal movement seen within central and lateral contact points. While in curve model, the maximum distal movement grasped within first and second premolars, in mesial and distal contact points.
- 11. All the lower teeth are displaced mesio-distally in curve model, more than in flat replica.

Abbreviations

COS: Curve of Spee; TMJ: Tempro-Mandibuler Joint; 3D: Three-dimensional; FEA: Finite Element Analysis; ACo: Anterior mandibular condylar; PCo Posterior Mandibular Condyle; SCo: Superior mandibular condylar; Ab: Anterior border of ramus (Ab); Go_{post}: Gonion posterior; Go: Gonion; Go_{inf}: Gonioninferius; Me: Menton; Pog: Pogonion; B: Supramemtale; Id: Infradental; Cor: Coronoid.

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Conflicts of interest

There are no conflicts of interest.

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