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A novel fluorescein-bisphosphonate based diagnostic tool for the detection of hydroxyapatite in both cell and tissue models

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A rapid and efficient method for the detection of hydroxyapatite (HAP) has been developed which shows superiority to existing well-established methods. This fluorescein-bisphosphonate probe is highly selective for HAP over other calcium minerals and is capable of detecting lower levels of calcification in cellular models than either hydrochloric acid-based calcium leaching assays or the Alizarin S stain. The probe has been shown to be effective in both *in vitro* vascular calcification models and *in vitro* bone calcification models. Moreover we have demonstrated binding of this probe to vascular calcification in rat aorta and to areas of microcalcification, in human vascular tissue, beyond the resolution of computed tomography in human atherosclerotic plaques. Fluorescein-BP is therefore a highly sensitive and specific imaging probe for the detection of vascular calcification, with the potential to improve not only *ex vivo* assessments of HAP deposition but also the detection of vascular microcalcification in humans.

Calcium is a crucial intracellular element that is responsible for regulating many cellular processes across every cell type in biological organisms¹. Calcium is found in either the free ion form or as a mineral phase, for example in the form of hydroxyapatite (HAP) that makes up bone and teeth. However mineralisation is also a critical component of a wide range of diseases such as cancer, arthritis and cardiovascular disease (CVD)^{2–4}. In atherosclerosis the presence of microscopic deposits of HAP can weaken the fibrous cap of an atherosclerotic plaque, leading to rupture of the plaque and vessel occlusion^{5–9}. In aortic stenosis the progressive accumulation of HAP in the valve leads to increasing obstruction to the flow of blood out of the heart, whilst in abdominal aortic aneurysm disease microcalcification is associated with aneurysms that expand more quickly and are at increased risk of rupture or requiring repair. Thus the development of a calcium assay which is able to selectively detect HAP with high sensitivity and specificity could both improve understanding of disease pathophysiology and aid the diagnosis of a range of clinical disorders including vascular calcification.

The most common assays for calcium phosphate mineralisation are calcium leaching by hydrochloric acid (HCl); and staining with Alizarin S and von Kossa stains^{10,11}. Each comes with their own limitations. The calcium leaching assay is used in laboratory settings to determine the presence of calcification in vascular and bone cell models. The assay involves incubating cell monolayers in the presence of HCl which allows the extraction of free calcium ions from the cells. The calcium content is then detected using a colourimetric assay and normalised against the total number of cells per sample¹². Given the timeframe of the calcium leaching assay (24–48 h) it is not suitable for high-throughput applications. The colourimetric stain Alizarin S detects calcium, and not phosphate, thus it can also bind to calcium-binding proteins and proteoglycans without discriminating for the presence of HAP¹³. Finally, the colourimetric von Kossa stain detects phosphates but only in acidic environments, even though the presence of phosphate does not necessarily imply the presence of calcium or even HAP^{10,13}. Both Alizarin S and von Kossa stains are used to indicate calcium depositions but at best give only semi-quantitative calcium readings¹⁴. In this study, the fluorescein-bisphosphonate conjugate **1** (Fluorescein-BP, Fig. 1)¹⁵ was

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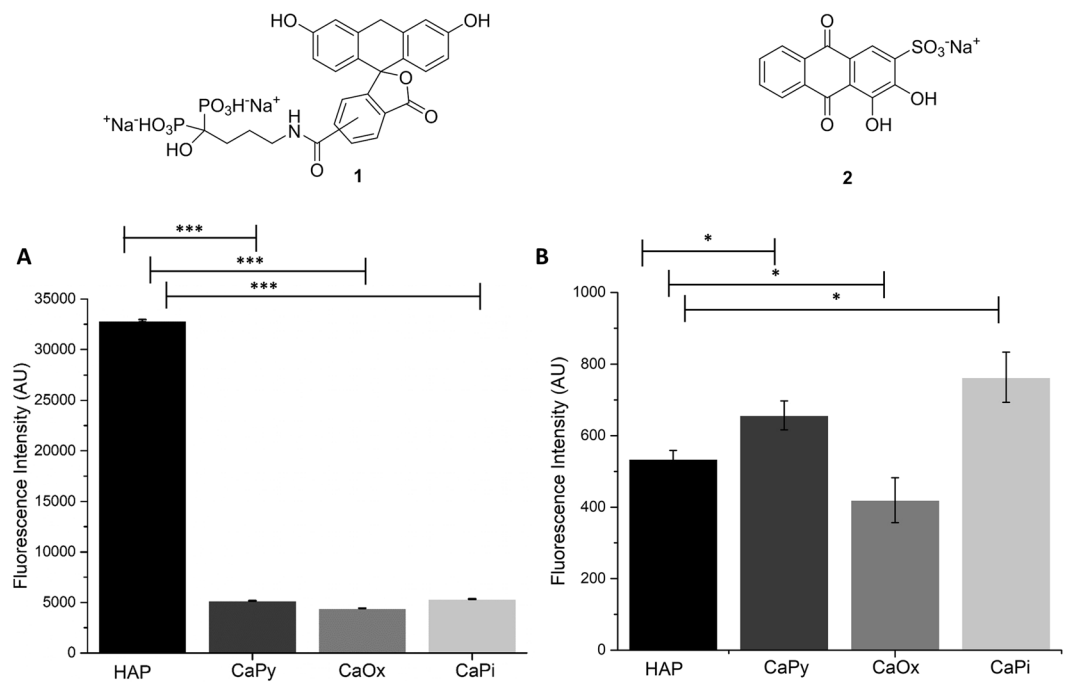


Figure 1. Selectivity towards calcium minerals of Fluorescein-BP (1) in comparison to Alizarin S stain (2). Calcium minerals were incubated with Fluorescein-BP (5 μ M) (A) or 1% w/w Alizarin S (B) in water for 2 hours and the un-bound probe was removed and quantified. The histograms show the relative amounts of bound fluorophore for each of the calcium minerals. Data shown are representative of at least 3 independent experiments yielding comparable results. * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$ compared to HAP, $n = 6$.

repurposed to allow for a rapid and inexpensive method of studying calcification and its use was investigated in a range of cell based models as well as mouse and human vascular tissue.

Results

Fluorescein-BP synthesis and specificity. The bisphosphonate, alendronate is recognised as a bone targeting reagent due to its striking ability to bind to HAP^{16,17}. Previous experiments have shown that alendronate is readily able to bind to bulk calcium mineral even in the presence of free calcium ions; and it is approved for clinical use for Paget's disease and osteoporosis^{16,18,19}. The ready availability of the FDA-approved probe components makes the alendronate-based Fluorescein-BP conjugate 1 particularly attractive for development and human translation as a method for the detection of calcification. Recently the Leong group reported the use of Fluorescein-BP 1 for the study of urinary calculi¹⁵; although the fluorescence intensity of the probe in the presence of macroscopic calcium oxalate (CaOx) was found to be relatively moderate.

Fluorescein-BP was synthesised following the procedure reported by the Leong group¹⁵. Specificity of the probe towards HAP was shown by incubating Fluorescein-BP with a range of calcium minerals including HAP, calcium pyrophosphate (CaPy), CaOx and calcium phosphate (CaPi). Aqueous suspensions of these minerals at fixed weight per volume were incubated with probe 1 for 2 hours, and un-bound probe was removed from the solids through a series of centrifugation and washing steps. Fluorescence analysis of the combined aqueous extracts allowed the levels of un-bound probe to be quantified and hence a direct comparison of the levels of Fluorescein-BP binding to each of the different calcium-containing minerals was enabled. These experiments showed that Fluorescein-BP demonstrated almost an order of magnitude higher selectivity towards HAP than any other calcium species tested (Fig. 1A). In contrast, when Alizarin S (2, Fig. 1) the most common histological stain for calcium, was incubated with the different calcium minerals it showed a very similar fluorescent intensity for each indicating non-specific binding (Fig. 1B). In order to achieve effective visualisation of the Alizarin S stain by fluorescence, millimolar concentrations of the stain were required which is in sharp contrast to the low micromolar concentrations required of probe 1. This reflects the relative brightness of the signal for each fluorophore which is proportional to its quantum yield ($\Phi = 0.79$ for fluorescein^{20–22}, and $\Phi = 0.001$ for Alizarin S^{22,23}).

Use of Fluorescein-BP in cell-based models of vascular calcification. A series of experiments were designed to probe the ability of the Fluorescein-BP probe 1 to define the location of HAP in cellular calcification assays, exploiting both the selectivity and sensitivity which was demonstrated in the mineral-based assays. Vascular smooth muscle cells (VSMCs), the principal cell type involved in vascular calcification, can undergo a phenotypic transition under specific environmental conditions to calcifying osteoblastic cells²⁴. The mouse VSMC line MOVAS-1 exhibits a smooth muscle cell phenotype and has been previously employed to investigate the VSMC cell cycle²⁵. Validation of the Fluorescein-BP probe 1 was carried out using MOVAS-1 and primary mouse VSMCs.

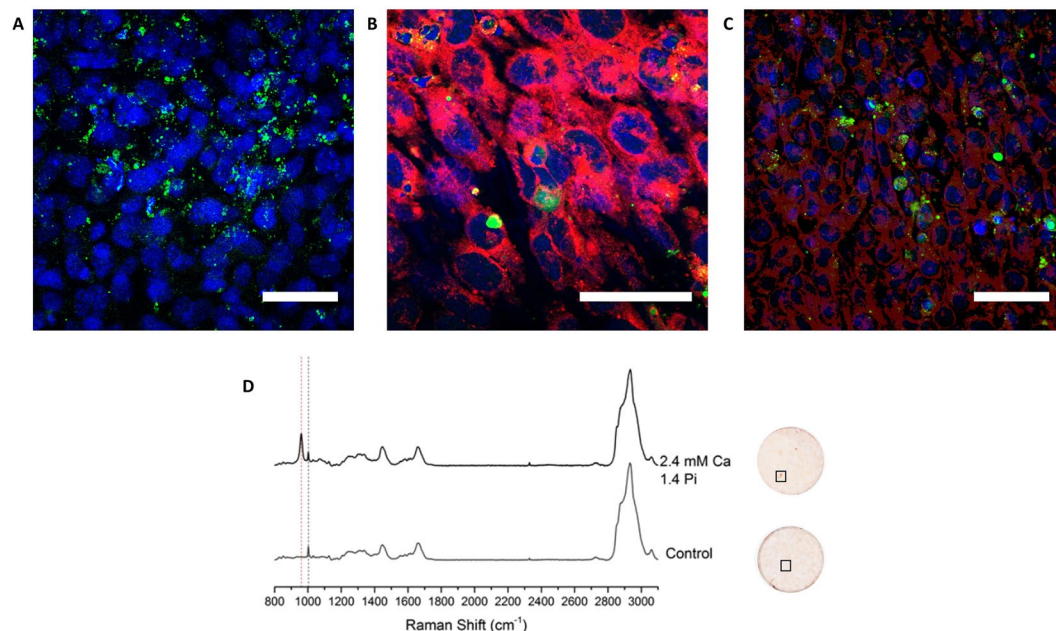


Figure 2. Confocal Images showing dual staining and Raman spectra of MOVAS-1 monolayers. Monolayers of MOVAS-1 cells were grown to confluence (day 0) and then switched to calcification media (2.4 mM Ca and 1.4 mM Pi) for 7 days, changing media on alternate days. The cell monolayers were treated sequentially with Fluorescein-BP (1 μ M, 2 hours; green); CellMask Orange (500 nM, 10 minutes, pink); NBF (10%, 15 minutes); Triton X (0.05%, 3 \times 5 minutes); DAPI (300 nM, 5 minutes, blue); then imaged on an Zeiss Confocal LSM710 microscope (λ_{ex} = 488 nm, 554 nm and 350 nm). Images are representative of at least 3 repeats. Scale bars = 100 μ m. (A) Incubation with Fluorescein-BP and DAPI. (B,C) Incubation with Fluorescein-BP, CellMask Orange and DAPI. (D) Monolayers of MOVAS-1 cells were grown to confluence (day 0) on CaF₂ slides and then switched to either control media or calcification media (2.4 mM Ca and 1.4 mM Pi) for 7 days, changing media on alternate days. The cell monolayers were fixed with NBF (10%, 15 minutes); and imaged using an InVia Renishaw Raman instrument (785 nm, 30 s, 50%). Following imaging, the cell monolayers were incubated with Alizarin S (2%, 10 minutes). Red dashed line indicates peak at 960 cm^{-1} for HAP while the black dashed line indicates the inherent cellular peak at 1003 cm^{-1} for phenylalanine. Images shown are representative of at least 3 independent experiments yielding comparable results.

Monolayers of MOVAS-1 cells were incubated with 2.4 mM Ca and 1.4 mM Pi for 7 days; then treated with Fluorescein-BP **1** for 2 h prior to imaging. Confocal microscopy (Fig. 2A–C) shows extracellular localisation of probe **1** (in green); indicative of the presence of HAP in the extracellular matrix in accord with previous reports^{26–29}. In contrast, no signal was observed when the same cells were incubated with a fluorescein-amino-1-pentanol conjugate (SI Fig. 1); giving a clear indication that the bisphosphonate motif is responsible for Fluorescein-BP binding to HAP in a cellular environment. Raman spectroscopic analysis of the observed mineral deposits confirmed the presence of HAP, with its distinctive peak at 960 cm^{-1} (Fig. 2D)³⁰.

To probe the range of conditions under which the Fluorescein-BP probe **1** can be used, and compare its efficacy with the hydrochloric acid-based calcium leaching assay and Alizarin S stain, a further series of calcification assays were conducted using the MOVAS-1 cell line and primary mouse VSMCs. Monolayers of MOVAS-1 cells were incubated in both phosphate-enriched (3.0 mM Pi; 5.0 mM Pi), and phosphate and calcium-enriched (2.4 mM Ca and 1.4 mM Pi; 2.7 mM Ca and 2.5 mM Pi), growth media. Both the hydrochloric acid-based calcium leaching assay (4-fold, $p < 0.001$) (Fig. 3A) and the Fluorescein-BP **1** fluorescence assay (4-fold, $p < 0.001$) (Fig. 3B) show significant levels of calcium deposition in the presence of calcium-enriched media. The fluorescence assay (LOD 0.0065 $\mu\text{mol/L}$, SI Fig. 2) is able to detect the presence of HAP when using media enriched with only phosphate in comparison to the calcium leaching assay (LOD 225 $\mu\text{mol/L}$)³¹ demonstrating the greater sensitivity of Fluorescein-BP **1**. A comparison of the fluorescence images obtained for well plates with images of Alizarin S staining of equivalent plates (Fig. 3C), shows that both fail to detect calcification in media only enriched with phosphate. However, when cells are incubated in the presence of both calcium and phosphate, the fluorescent probe is able to detect the deposition of microcrystalline HAP with greater sensitivity than the Alizarin S stain. This is particularly notable when the incubation media have been enriched with 2.4 mM Ca and 1.4 mM Pi, as commonly used in vascular calcification models³².

When comparable studies were performed using primary mouse VSMCs (Fig. 4A–C), incubating the monolayers with increasing levels of phosphate to induce calcification (1.8 mM Pi, 2.6 mM Pi and 3.0 mM Pi), the fluorescent probe (5-fold, $p < 0.001$) was also shown to be more sensitive than either the Alizarin S or calcium leaching assays (1.2-fold, $p < 0.001$).

In further experiments, MOVAS-1 cells (SI Fig. 3) and primary mouse VSMCs (SI Fig. 4) were incubated under standard calcification conditions (2.4 mM Ca and 1.4 mM Pi) and the calcification on days 3, 5 and 7

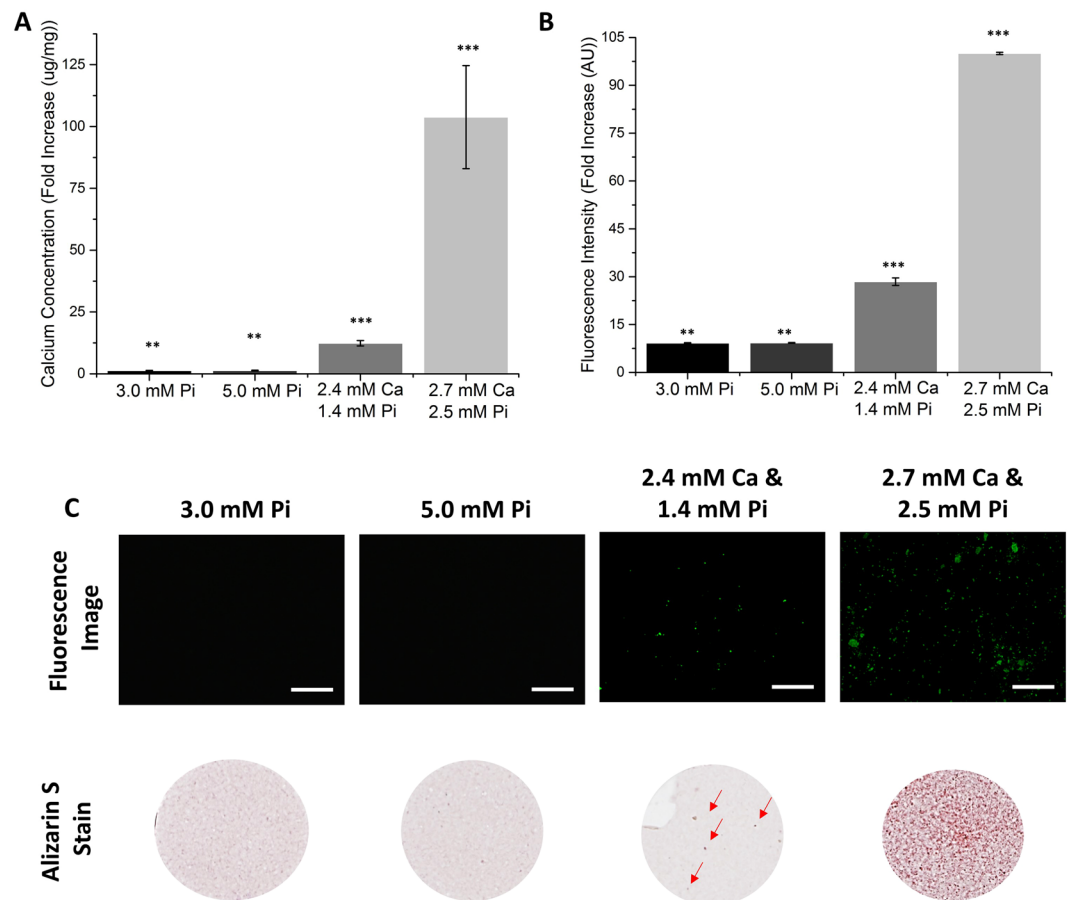


Figure 3. Determination of calcification in the MOVAS-1 cell line at various concentrations (3.0 mM Pi, 5.0 mM Pi, 2.4 mM Ca and 1.4 mM Pi, 2.7 mM Ca and 2.5 mM Pi). Monolayers of MOVAS-1 cells were grown to confluence (day 0) and then switched to calcification media. The monolayers were incubated in calcification media (3.0 mM Pi, 5.0 mM Pi, 2.4 mM Ca and 1.4 mM Pi, 2.7 mM Ca and 2.5 mM Pi) for 7 days, changing media on alternate days. **(A)** Calcium leaching assay: o-cresolphthalein complexone. **(B)** Fluorescence assay: cell monolayers were incubated with Fluorescein-BP (1 μ M, 2 hours); NBF (10%, 15 minutes). **(C)** Fluorescence images and Alizarin S stain images: cell monolayers were either incubated with Fluorescein-BP (1 μ M, 2 hours) and then fixed with NBF (10%, 15 minutes), or fixed with NBF (10%, 15 minutes) and then incubated with Alizarin S (2%, 500 μ L, 10 minutes). Data shown in **(A)** and **(B)** are from at least 6 repeats and shown as the mean \pm S.E.M., * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$ compared to control, $n = 6$. Images shown in **(C)** are representative of at least 3 independent experiments yielding comparable results. Arrows indicate the location of calcium deposits within the well. Scale bars = 250 μ m.

was detected using Fluorescein-BP probe **1** (2.5-fold, $p < 0.001$ for MOVAS-1; 2.5-fold, $p < 0.001$ for VSMCs) and compared with calcium leaching using the hydrochloric acid-based assay (5-fold, $p < 0.001$ for MOVAS-1; 2.5-fold, $p < 0.001$ for VSMCs) and staining by Alizarin S. The fluorescent probe was shown to be more sensitive than both the other assays. Similarly, when MC3T3 cells (SI Fig. 5), an osteoblast derived cell line which is commonly used for studies in the field of bone and skeletal mineralisation^{33,34}, were incubated with Fluorescein-BP, calcium mineralisation was readily detected (2-fold, $p < 0.001$).

Ex vivo rat aorta and human tissue study. VSMC monolayer cultures are of only limited use in the study of calcification in CVD: they lack the architecture and matrix of normal vessels; they reach confluence over a short timeframe; they rapidly convert to a proliferative, secretory phenotype³⁵; morphological variations have been seen at high passage numbers; and variations in the gene phenotype can also occur. Cultured aortae can provide complementary information that bridges the gap between traditional cell culture and animal models, under almost *in vivo* conditions^{35,36}. Previous studies have cultured sectioned thoracic aortas dissected from mice and estimated the status of calcification under Pi stimulation at 2.6–3.0 mM Pi³⁶; these phosphate concentrations correlate with myocardial infarction in human studies³⁶.

Ex vivo aortic rings from rats were incubated under different calcification conditions (1.8 mM Pi, 2.6 mM Pi and 3.0 mM Pi) for 7 days and subsequently incubated with Fluorescein-BP **1** followed by Alizarin S (Fig. 5, SI Fig. 6). From both staining methods, it is apparent that with increasing calcification conditions there is an increase in signal in both the Alizarin S and Fluorescein channel. When the two channels are merged, it is clear

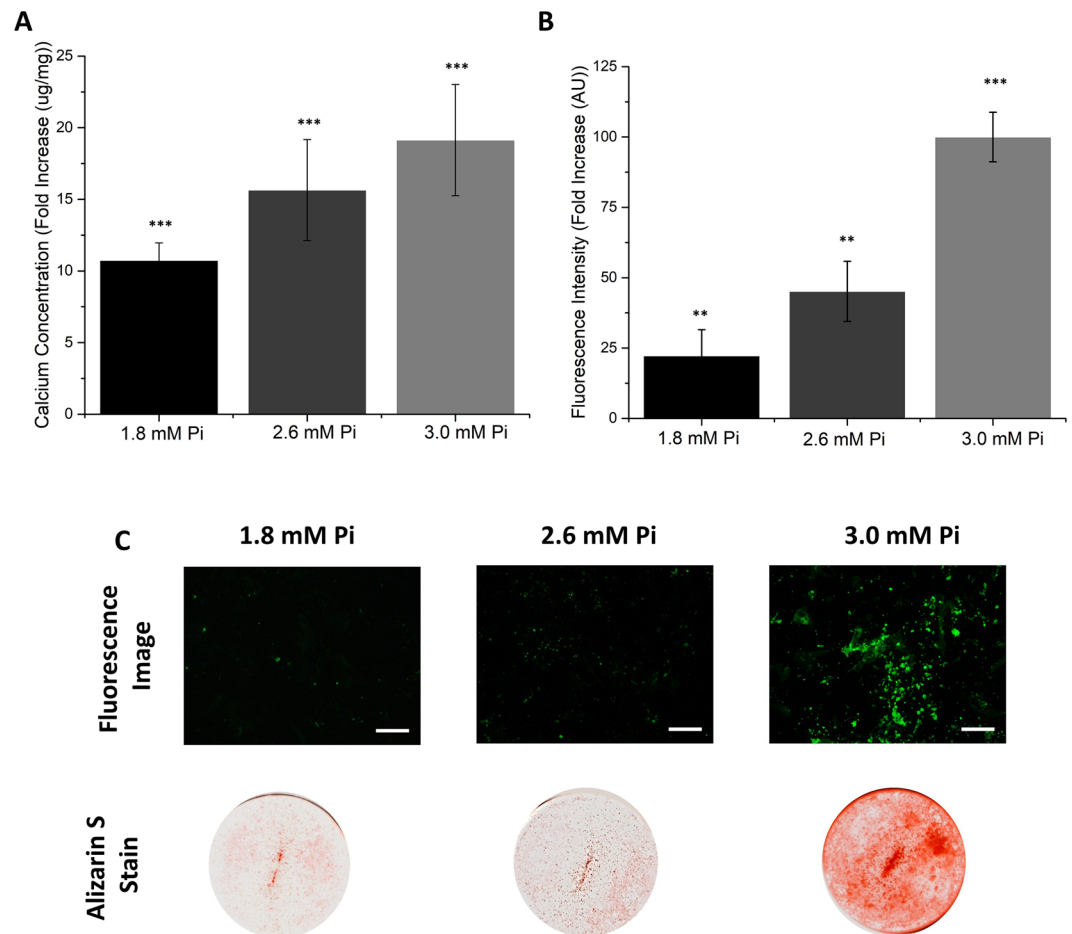


Figure 4. Determination of calcification in primary mouse VSMCs at various concentrations (1.8 mM Pi, 2.6 mM Pi, 3.0 mM Pi). Monolayers of primary mouse VSMCs were grown to confluence (day 0) and then switched to calcification media. The monolayers were incubated in calcification media (1.8 mM Pi, 2.6 mM Pi, 3.0 mM Pi) for 7 days, changing media on alternate days. **(A)** Calcium leaching assay: o-cresolphthalein complexone. **(B)** Fluorescence assay: cell monolayers were incubated with Fluorescein-BP (1 μ M, 2 hours); NBF (10%, 15 minutes). **(C)** Fluorescence images and Alizarin S stain images: cell monolayers were either incubated with Fluorescein-BP (1 μ M, 2 hours) and then fixed with NBF (10%, 15 minutes) or fixed with NBF (10%, 15 minutes) and then incubated with Alizarin S (2%, 500 μ L, 10 minutes). Data shown in **(A)** and **(B)** are from at least 6 repeats and shown as the mean \pm S.E.M., * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$ compared to control, $n = 6$. Images shown in **(C)** are representative of at least 3 independent experiments yielding comparable results. * $P < 0.05$, ** $P < 0.01$, *** $P < 0.001$ compared to control, $n = 6$. Scale bars = 250 μ m.

that the Alizarin S and Fluorescein-BP stains colocalize in most areas. No fluorescence signal is observed when the rings are cultured with control media confirming that the Fluorescein-BP probe is selective for HAP.

Next, a more detailed analysis of calcification in aortic rings was conducted using 5 μ m sections (Fig. 6). Calcified rat aortic rings were fixed and cryosectioned on day 7; the sections were then incubated with Fluorescein-BP probe 1 followed by Alizarin S. Fluorescent microscopy of these sections confirms differences in calcification between the control and 3.0 mM Pi specimens. This also allows the location of the calcification to be determined; which in this rat model occurs in the medial layer of the aorta³⁵.

PET/CT imaging using Na¹⁸F has been reported as a novel tool for vascular disease diagnosis^{9,37}. Na¹⁸F is able to identify areas of micro-calcification that are associated with unstable plaque phenotype and which are beyond the resolution of CT. Indeed Na¹⁸F PET is currently being explored as a method for detecting high risk coronary plaques and improving cardiovascular risk prediction (clinicaltrials.gov NCT02278211)^{9,37,38}. We next compared Fluorescein-BP binding to the detection of vascular calcification by computed tomography and Na¹⁸F PET in 8 samples of human arterial tissues (7 affected by calcific atherosclerotic disease and 1 control tissue which was free of atherosclerosis). All the tissue samples were assessed initially using PET/CT scans followed by sectioning of the tissue as required to allow appropriate fluorescence images to be obtained (as depicted for a representative sample in Fig. 7, additional examples shown in SI Fig. 7). PET/CT imaging (Fig. 7A–C) showed both areas of macrocalcification, as detected by CT, and areas of microcalcification, as detected by PET using a Na¹⁸F tracer. Samples from both areas were sectioned and stained (Fig. 7D–K). The images show that Fluorescein-BP probe 1 binds to both macro- and micro-calcification and colocalizes with Alizarin S staining (Fig. 7D,E). The control

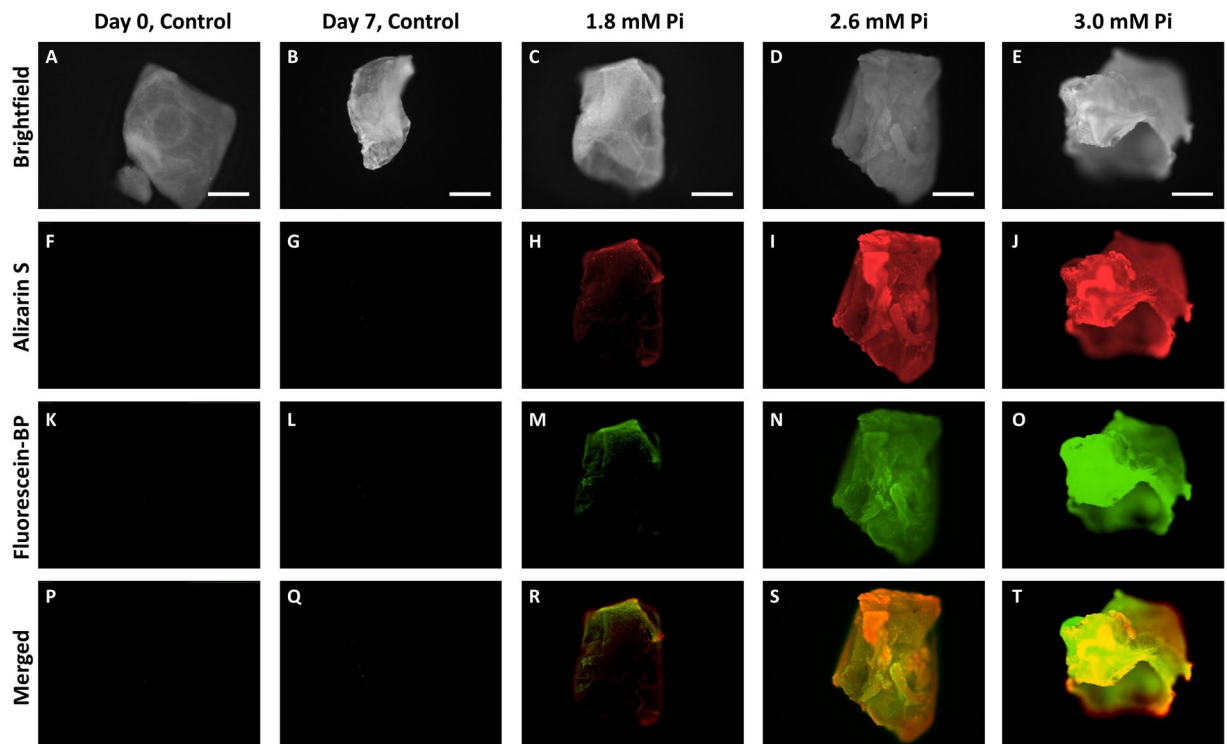


Figure 5. Determination of calcification in rat aorta incubated under different calcification conditions (1.8 mM Pi, 2.6 mM Pi and 3.0 mM Pi). Rat aortic rings were incubated for 2 days in fresh control media followed by calcification media (1.8 mM Pi, 2.6 mM Pi and 3.0 mM Pi) for 7 days. The rings were subsequently incubated with Fluorescein-BP (1 μ M, 2 hours), fixed with NBF (10%, 15 minutes), permeabilised in KOH (1%, 1 hour) and then incubated with Alizarin S (0.00005% Alizarin S in 1% KOH, 24 hours). Brightfield (A–E) Fluorescence (K–O) Alizarin S (F–J). Merged images (P–T) recorded using both Alizarin S and Fluorescein-BP channels. Images shown are representative of at least 3 independent experiments yielding comparable results. Scale bars = 250 μ m.

tissue sample (Fig. 7L,M), where there was no clinical history of coronary disease, showed neither PET/CT signal nor fluorescence staining.

Discussion

Here, we demonstrate that Fluorescein-BP is a highly sensitivity and specific marker of HAP in vascular tissue. Fluorescein-BP has been compared to the current gold standard techniques for identifying calcification, the Alizarin S and HCl decalcification assays, and in both instances shows greater sensitivity and selectivity for HAP. Moreover we have confirmed its binding to HAP in both *in vitro* cell models of vascular and bone calcification, *ex vivo* rat aorta tissue and human coronary atherosclerotic plaques. Given that its component parts are already FDA approved, Fluorescein-BP holds great translational potential for the detection of crystalline HAP in humans.

Vascular mineralisation in atherosclerotic plaques contains high concentrations of crystalline HAP³⁹. Within the arterial walls, extracellular vesicles containing HAP are extruded from lipid-rich macrophages and apoptotic smooth muscle cells which increase the plaque structural stress and risk of fibroatheromatous cap fracture⁴⁰. The inflammatory milieu driving the production of HAP deposition is associated with a greater propensity to destabilise plaques and results in clinical cardiovascular events^{41,42}. Recent clinical trials have focused attention on the vital role that early calcification plays in carotid, aortic aneurysmal and coronary artery disease and hence there is a clinical imperative to better understand the mechanisms governing early calcification in the vascular wall^{41–43}. The ability to differentiate calcium derivatives in regions of calcification, specifically by detecting HAP, will facilitate the dichotomisation of unstable and stable cardiovascular phenotypes in future clinical trials.

The detection of HAP deposition has been a field that has gained a lot of attention in the past 20 years^{1,44–46}. Histological stains such as Alizarin S and von Kossa are widely used to study calcium deposits but their effectiveness has been disputed since their binding modes are somewhat indiscriminate⁴⁵. Additionally, calcein is a routinely used tool for imaging calcium, however, not only does it bind across a range of calcium species, but it is also non-specific for calcium and interacts with a range of other metals including aluminium and zinc^{47,48}. Another recently reported probe used in animal based models of both bone and vascular disease is Osteosense (680 and 750), a commercially available, near infrared (NIR) probe conjugated to a bisphosphonate^{49–51}. However, the benefits offered by a NIR probe for *in vivo* studies, are off-set by the need for non-standard filters for plate readers and microscopes in laboratory based experiments which limited our capacity to directly compare the two probes.

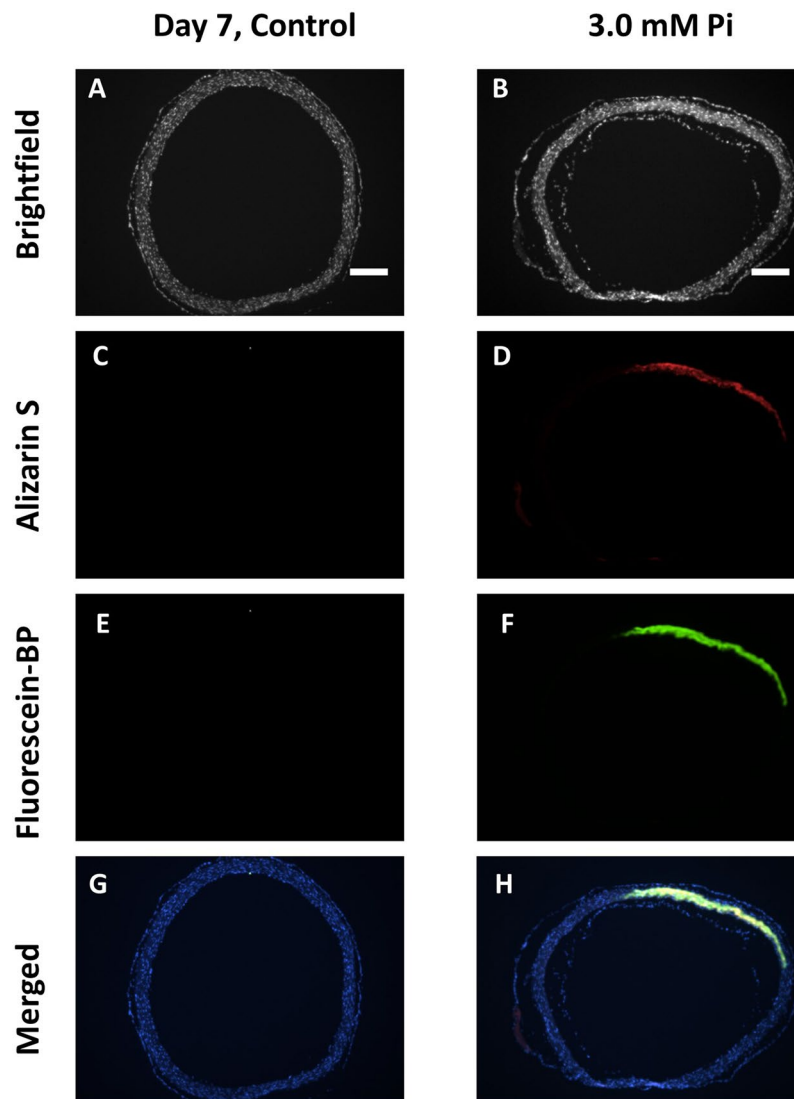


Figure 6. Determination of calcification in rat aortic ring sections. Rat aortic rings were incubated for 2 days in fresh control media followed by calcification media 3.0 mM Pi for 7 days and fixed with NBF (10%, 15 minutes). Rings were cryosectioned into 5 μ m sections. Sections were incubated with Fluorescein-BP (1 μ M, 2 hours), permeabilised in KOH (1%, 1 hour), incubated with Alizarin S (0.00005% Alizarin S in 1% KOH, 24 hours), followed by DAPI (500 nM, 5 minutes). Brightfield (A,B) Fluorescence (E,F) Alizarin S (C,D). Merged images (G,H) recorded using Alizarin S, Fluorescein-BP and DAPI channels. Images shown are representative of at least 3 independent experiments yielding comparable results. Scale bars = 250 μ m.

Fluorescein-BP probe **1**, in comparison to Calcein and Osteosense, presents a more selective, sensitive and widely-applicable method of detecting calcification in vascular and bone models. In addition, the two low-cost reagents required for the synthesis of the probe are both commercially available, ensuring a wider user base for the new probe. Future *in vivo* studies might be enabled by intravascular administration of probe **1** using catheters fitted with a confocal endomicroscope probe, thus negating the need for conjugation to a costly NIR dye.

Conclusions

Fluorescein-BP probe **1** gives a dramatically improved signal output over more conventional imaging methods such as Alizarin S and von Kossa stains for the detection of calcium phosphate in a range of *in vitro* studies. It has been shown to be mineral-specific giving a markedly increased signal in the presence of HAP over other calcium species, and can be used in both condition-specific and temporal studies of calcification in cell-based models of CVD and bone disease. Staining with probe **1** is rapid, allowing high-throughput assays in multi-well format which are not possible with comparable assays such as the hydrochloric acid-based quantification method typically used in the field. When applied to *ex vivo* aortic sections and to human tissue presenting both macro- and micro-calcification, Fluorescein-BP **1** shows binding to both types of vascular calcification which are not readily detectable using one stand-alone technique. The employment of this probe may enable the elucidation of key mechanisms underpinning these pathological processes.

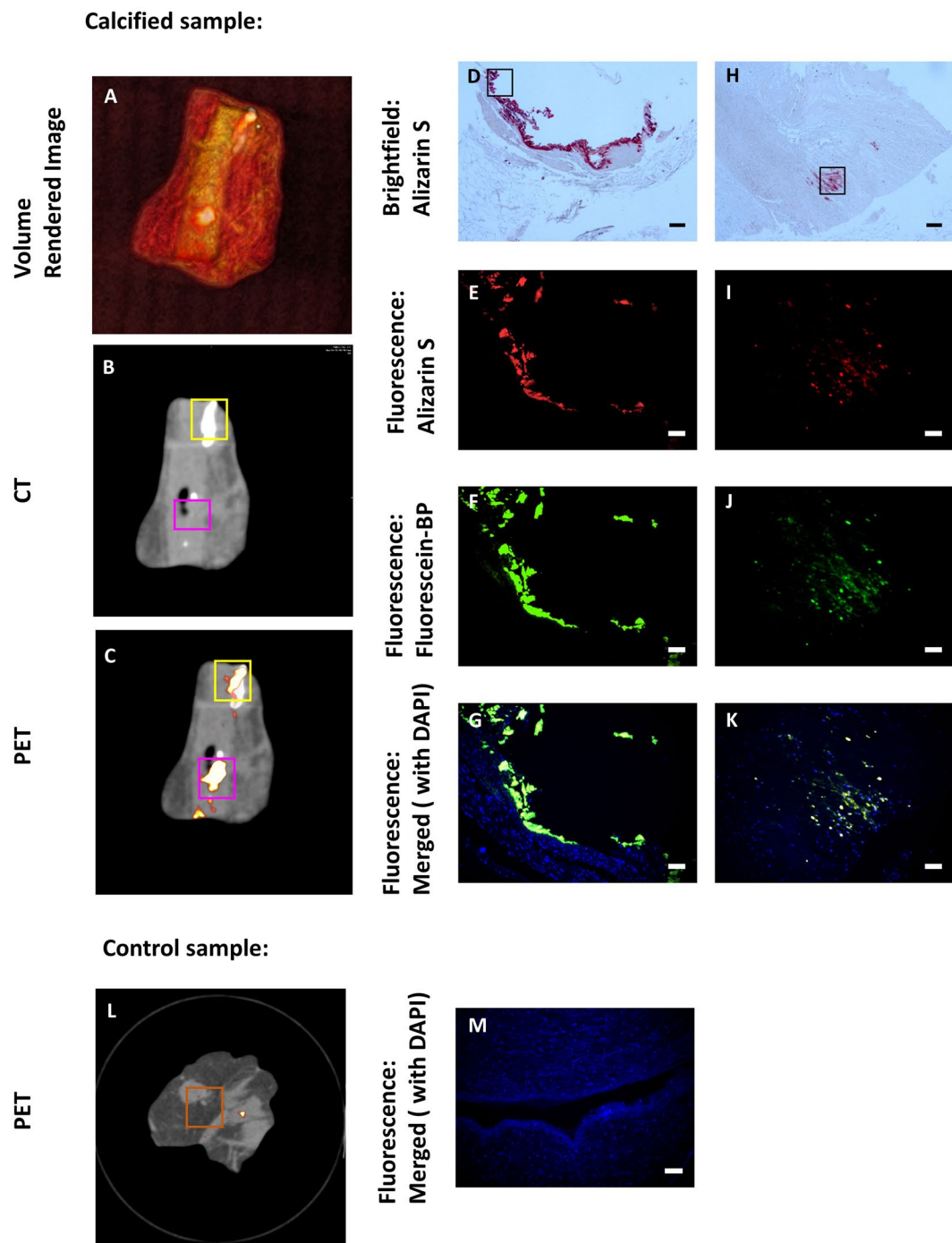


Figure 7. Determination of calcification in human vascular tissue (calcified and control). (A) Volume rendered image; (B) CT image; (C) PET image, with NaF tracer, of vascular tissue. Yellow, purple and orange boxes indicate the areas selected for tissue sectioning where Brightfield and Fluorescence images of calcification were taken. (D–G) Brightfield and Fluorescence (Alizarin S, Fluorescein-BP, DAPI) images of tissue in the yellow box which show high CT activity. (H–K) Brightfield and Fluorescence (Alizarin S, Fluorescein-BP, DAPI) images of tissue in the purple box which show high PET activity. Sections were incubated with Fluorescein-BP (1 μ M, 2 hours), Alizarin S (2%, 10 minutes) and DAPI (500 nM, 5 minutes) and subsequently imaged. Black boxes indicate region of Brightfield image where Fluorescence images were taken. Control sample, PET image (L) and Fluorescence (Alizarin S, Fluorescein-BP and DAPI, M). Scale bars = 2.0 mm for Brightfield and 100 μ m for Fluorescence.

Methods

Unless otherwise noted, starting materials and reagents were obtained from Sigma-Aldrich and were used without further purification. Saturated aqueous solutions of inorganic salts are represented as (volume, sat. aq.).

Semi-preparative RP-HPLC was performed using a Waters 600E pump, a Waters 486 tuneable absorbance detector controlled by Water Empower software which was equipped with a Phenomenex Luna C18(2), 5 μ m particle size, 250 \times 21.2 mm column at a flow rate of 18 mL min⁻¹.

¹H and ¹³C NMR spectra were obtained on Bruker AVA600 instrument at the stated frequency using TMS as a reference and residual solvent as an internal standard. Infra-red spectra were recorded neat on a Shimadzu IRAffinity-1. Electrospray (ESI) mass spectra were obtained on a Bruker micrOTOF II instrument. UV/VIS absorption spectra were measured using a Shimadzu UV-1800 spectrometer. Melting points were determined on a Gallenkamp Electrothermal Melting Point apparatus and are uncorrected. Fluorescence data was obtained using SPEX Fluoromax-3.

Fluorescein-BP conjugate (1). Sodium alendronate (34 mg, 1 mmol, 5 eq; Alfa Aesar) was dissolved in NaHCO₃ (1 mL, sat. aq.). Fluorescein (5/6) NHS ester (10 mg, 0.2 mmol, 1 eq; Thermo Fisher) dissolved in DMF (0.1 mL) was added to the solution and the reaction mixture was stirred for 2 days at room temperature in the dark. The solution was acidified with TFA (10% v/v aq.) and purified by RP HPLC [isocratic 80/20 H₂O (+0.1% v/v TFA)/MeCN (+0.1% v/v TFA)] to yield the fluorescein-BP conjugate as an orange solid (34 mg, 50%).

$\lambda_{\text{abs}}/\lambda_{\text{em}}$ 491/515; Φ 0.83; ϵ 41,400 M⁻¹cm⁻¹; MP 240 °C; IR (solid, cm⁻¹) 1700 (C=O), 1635 (C=O), 1538 (N-H), 1271 (P=O), 1116 (C-N); ¹H NMR (601 MHz, DMSO-*d*₆) δ 10.13 (2H, br s, *OH isomer 1 + 2*) 8.85 (0.6H, t, *J* = 5.7 Hz, *NH isomer 1*), 8.72 (0.4H, t, *J* = 5.9 Hz, *NH isomer 2*), 8.47 (0.6H, d, *J* = 1.5 Hz, *ArH isomer 1*), 8.26 (0.6H, dd, *J* = 8.0, 1.5 Hz, *ArH isomer 1*), 8.19 (0.4H, dd, *J* = 8.1, 1.4 Hz, *ArH isomer 2*), 8.07 (0.4H, d, *J* = 8.1 Hz, *ArH isomer 2*), 7.70 (0.4H, s, *ArH isomer 2*), 7.37 (0.6H, d, *J* = 8.0 Hz, *ArH isomer 1*), 6.69 (2H, dd, *J* = 5.3, 2.3 Hz, *ArH isomer 1 + 2*), 6.63 – 6.53 (4H, m, *ArH isomer 1 + 2*) 3.30 (1.2H, q, *J* = 6.5 Hz, *NCH₂ isomer 1*), 3.17 (0.8H, q, *J* = 6.4 Hz, *NCH₂ isomer 2*), 2.01–1.70 (4H, m, *CH₂CH₂ isomer 1 + 2*); ¹³C NMR (151 MHz, DMSO-*d*₆) δ 168.69 (C=O), 168.55 (C=O), 164.86 (C=O), 164.67 (C=O), 160.06 (2 \times Ar C), 155.02 (Ar C), 153.17 (Ar C), 152.32 (2 \times Ar C), 152.30 (2 \times Ar C), 141.35 (Ar C), 136.96 (Ar C), 135.16 (Ar CH), 129.85 (Ar CH), 129.74 (2 \times Ar CH), 129.66 (2 \times Ar CH), 128.55 (Ar C), 126.92 (Ar C), 125.27 (Ar CH), 124.66 (Ar CH), 123.72 (Ar CH), 122.73 (Ar CH), 113.21 (2 \times Ar CH), 113.16 (2 \times Ar CH), 109.67 (2 \times Ar C), 109.60 (2 \times Ar C), 102.73 (2 \times Ar CH), 83.75 (C), 83.72 (C), 72.60 (t, ¹*J*_{CP} = 148 Hz, C), 41.99 (t, ²*J*_{CP} = 21 Hz, CH₂), 41.65 (t, ²*J*_{CP} = 21 Hz, CH₂), 31.13 (CH₂), 24.06 (CH₂); *m/z* (ESI+, H₂O:MeOH): 630 ([M+Na]⁺, 10%), 608 ([M+H]⁺, 100); ³¹P NMR (202 MHz, DMSO-*d*₆) δ 20.21.

Fluorescein-BP and Alizarin S incorporation in Calcium minerals. Aqueous suspensions of calcium species (HAP, CaOx, CaPi, CaPyr, Sigma and Fisher Scientific) (50 mg) were incubated with Fluorescein-BP **1** (5 μ M) for 2 hours. Unbound probe was removed by centrifugation of the suspension at 670 g for 5 minutes, the supernatant was removed and the precipitated solid was resuspended in water with continuous agitation for 15 minutes. This process of centrifugation and resuspension was repeated three times, until there was no further fluorescence in the supernatant after centrifugation. Fluorescence analysis of the combined aqueous extracts was performed using a Synergy HT Multi Mode Microplate reader at 488 nm.

VSMC isolation and culture. Primary aortic VSMCs were isolated from five week old C57BL/6 mice (Charles River Laboratories) as previously described^{1,32,53}. Mice were euthanized by cervical dislocation, the aorta was then dissected and the adventitia removed. After washing with Hanks' balanced salt solution (HBSS; Life Technologies), the aorta was cut longitudinally to expose the endothelial layer. Eight aortae were pooled together and incubated for 10 minutes at 37 °C in 1 mg/mL trypsin (Life Technologies) to remove any remaining adventitia and endothelium. Aortae were washed and incubated overnight at 37 °C in VSMC growth medium containing Minimum Essential Medium Eagle alpha modification (α -MEM; Life Technologies), 10% foetal bovine serum (FBS; Life Technologies) and 1% gentamicin (Life Technologies) in a humidified 5% CO₂ incubator. Tissues were then washed and incubated in 425 UI/mL collagenase type II (Worthington Biochemical Corporation) for 4 hours at 37 °C. The resulting cell suspension was centrifuged at 320 g for 5 minutes. VSMC pellets were resuspended in culture medium and cultured for two passages in T25 tissue culture flasks (Corning) coated with 0.25 μ g/cm² laminin (Sigma) to promote maintenance of the contractile differentiation state⁵⁴.

MOVAS-1 culture. MOVAS-1 cells (ATCC) were suspended in growth media consisting of Dulbecco's Modified Eagle Media (DMEM)-Formula 12 (Life Technologies) supplemented with 10% FBS and 1% gentamicin and cultured at 37 °C, in the presence of 5% CO₂. Before experimentation, MOVAS-1 were expanded in growth media and cells were then used for experiments.

Induction of calcification in MOVAS-1 and VSMCs. Calcification was introduced as previously described^{1,32,53}. In brief, for MOVAS-1, cells were grown to confluence (day 0) and switched to calcification medium, which was prepared by adding 1 M inorganic phosphate (mixture of NaH₂PO₄ and Na₂HPO₄, pH = 7.4) and 1 M CaCl₂ to reach a final concentrations of 3.0 mM Pi, 5.0 mM Pi, 2.4 mM Ca and 1.4 mM Pi or 2.7 mM Ca and 2.5 mM Pi. For VSMCs, cells were grown to confluence (day 0) and switched to calcification medium, which was prepared by adding 1 M inorganic phosphate to reach a final concentrations of 1.8 mM Pi, 2.6 mM Pi and 3.0 mM Pi. Cells were incubated for 7 days in 95% air/5% CO₂, changing media on alternate days.

Fluorescence staining of fixed cells using Fluorescein-BP and CellMask Orange Plasma Membrane Stain. MOVAS-1 cells were grown on glass coverslips and calcified as described above. After incubation with Fluorescein-BP probe **1** (1 μ M) for 2 hours, the media was changed, the monolayer was washed twice with HBSS and fresh HBSS containing 500 nM CellMask Orange Plasma Membrane Stain (Thermo Fisher) was added for 10 minutes. The monolayer was washed with phosphate buffered saline (PBS, 2 \times) and water (1 \times), fixed with 10% neutral buffered formalin (NBF) for 15 minutes and washed with PBS (2 \times) and water (1 \times). The cell monolayers were

permeabilised with Triton X-100 (0.05%, 3×) for 5 minutes and incubated with DAPI (300 nM; Life Technologies) for 5 minutes. Excess DAPI was removed by washing with water (1×). Glass coverslips were mounted onto slides with Prolong Gold Anti-Fade Reagent (Life Technologies). Fluorescence signal was detected under a Zeiss Axiovert 25 inverted microscope and/or Zeiss Confocal LSM 710 at 488 nm (Fluorescein-BP), 554 nm (CellMask Orange) and 350 nm (DAPI).

Raman microscopy. MOVAS-1 were grown and calcified (2.4 mM Ca and 1.4 mM Pi) on CaF₂ slides. After 7 days, the monolayer was fixed with 10% NBF for 15 minutes. Raman imaging was carried out using an InVia Renishaw Microscope with laser excitation at 785 nm and a 50, N.A. 0.75 objective. The total data acquisition was performed during 30 s for spectra with a 50% laser power using the WiRE software. All of the spectra acquired were background subtracted using a background correction algorithm in the WiRE software.

Fluorescence microscopy. MOVAS-1 and VSMCs were grown on plates and calcified as described above. Media was removed and the cell monolayer was subsequently washed with HBSS then incubated with DMEM/F12 (MOVAS-1) and α -MEM (VSMCs) containing Fluorescein-BP probe 1 (1 μ M) for 2 hours. The media was then extracted and the cell monolayer was washed twice with HBSS, fixed with 10% NBF for 15 minutes and washed with PBS (PBS, 2×) and water (1×). Fluorescence images were captured using a Leica DMBL-2 upright fluorescent microscope and on Synergy HT Multi Mode Microplate reader at 488 nm (Fluorescein-BP).

Calcium leaching assay. Calcium deposition was quantified as previously described^{32,52}. Briefly, cells were rinsed with phosphate buffered saline (PBS) and decalcified with 0.6N HCl at room temperature for 24 hours. Free calcium was determined calorimetrically by a stable interaction with *o*-cresolphthalein complexone using a commercially available kit (Randox Laboratories Ltd.) and corrected for total protein concentration (Bio-Rad Laboratories Ltd).

Alizarin S staining of cell monolayers. Cells were grown in plates and calcified as described above. Media was removed and the cell monolayer was subsequently washed with HBSS. Cells were fixed in 10% NBF for 15 minutes before washing twice with PBS. The cells were then stained with Alizarin S (2%, pH 4.2; 500 μ L) for 10 minutes at rt. The supernatant was discarded and the cell monolayer was washed with water (3×) and then imaged at 530 nm (Alizarin S).

Ex vivo aorta isolation and culture. Aortic rings were dissected from eight week old Fischer male rats. Rats were euthanized by cervical dislocation, the aorta was then dissected and the adventitia removed. After washing with HBSS the aortae were cut into ~4 mm thick rings and cultured in α -MEM supplemented with 10% FBS and 1% gentamicin at 37 °C in 95% air/5% CO₂. After 1 day, the media was changed to calcifying media (1.8 mM Pi, 2.6 mM Pi, 3.0 mM Pi) for 7 days, changing media on alternate days. On day 7, aortas were incubated with Fluorescein-BP (1 μ M) for 2 hours. Aortas were washed with PBS (2×) and fixed with 10% NBF for 15 minutes. Residual NBF was removed by washing with PBS (2×) and water (1×). For Alizarin S staining, the fixed aortas were permeabilised with 1% KOH for 1 hour followed by overnight staining with 0.00005% Alizarin S in 1% KOH. Residual Alizarin S was removed by washing with water (3×). Rings were then imaged under a Zeiss Axiovert 25 inverted microscope at 488 nm (Fluorescein-BP) and 530 nm (Alizarin S).

Aortic sections. Aortic rings were dissected and calcified following the standard protocol. Once calcified, the rings were fixed in 10% NBF for 15 minutes and then cryosectioned into 5 μ m thick sections. Sections were then imaged under a Leica DMBL-2 upright fluorescent microscope at 488 nm (Fluorescein-BP), 530 nm (Alizarin S) and 350 nm (DAPI).

Human tissue. Atherosclerotic layers of left main coronary arteries were analysed from a range of patients, both male and female between the age of 48–71, for which main cause of death was either haemopericardium or ischaemic and hypertensive heart disease. Upon approval, the tissue was frozen at –80 °C.

PET/CT analysis of human tissue. Thawed non-decalcified coronary artery specimens were incubated for 20 minutes in ¹⁸F-sodium fluoride 100 kBq/mL solution (10.5 MBq 18F-NaF in 99.5 mL 0.9% NaCl). Samples were twice washed in 10 mL 0.9% NaCl for 5 minutes to remove unbound ¹⁸F-fluoride. Coronary artery specimens were scanned using high-resolution micro-positron emission tomography and non-contrast computed tomography [50 kV p tube voltage, 300 ms exposure time] (Mediso nanoScan PET/CT). After whole specimen imaging, the coronary arteries were fixed in 10% buffered formaldehyde before being dehydrated, embedded in paraffin wax and sectioned (5 μ m thickness).

Alizarin S Staining of human tissue. Sections were de-waxed in xylene and stained with 2% Alizarin S for 5 minutes, washed three times with water and dehydrated to visualize calcium deposition. Images were obtained using a Nikon Ni1 Brightfield microscope.

Fluorescein-BP and Alizarin S Staining of human tissue. Sections were de-waxed in xylene and incubated with Fluorescein-BP probe 1 (1 μ M) for 2 hours, washed in water (2×) followed by incubation with 2% Alizarin S (250 μ L) for 5 minutes. Sections were washed in water (3×) and subsequently incubated with DAPI (500 nM) for 5 minutes. Sections were washed with water (1×) and then mounted using ProLong Gold Antifade. Fluorescence signal was detected using a Leica DMRB fluorescence microscope at 488 nm (Fluorescein-BP), 530 nm (Alizarin S) and 350 nm (DAPI).

Statistical analysis. Two-sample Student's *t*-test was used to analyse the significance between data sets. Data are presented as mean \pm standard error of the mean (S.E.M.). All statistical analysis was performed using Minitab 17 (Minitab Inc.). $p < 0.05$ was considered to be significant, and *p*-values are represented as: * $p < 0.05$; ** $p < 0.01$; *** $p < 0.001$.

Ethical approval. All animal experiments were approved by The Roslin Institute's Animal Users Committee and the animals were maintained in accordance with Home Office guidelines for the care and use of laboratory animals. Atherosclerotic layers of left main coronary arteries were obtained from victims of sudden death at autopsy with written informed relative authorisation from the next of kin. Ethical approval was granted by National Health Service Research Ethics Committee South East Scotland (14/SS/1090). The retention, storage and use of tissue sections were compliant with the United Kingdom Human Tissue Act of 2004 and in accordance with the relevant guidelines and regulations approved by National Health Service Research Ethics Committee South East Scotland (14/SS/1090).

Data Availability

All data generated and analysed during this study are available as Supplementary Data online. Primary data files are available at <https://doi.org/10.7488/ds/2467>.

References

- Berridge, M. J., Lipp, P. & Bootman, M. D. The versatility and universality of calcium signalling. *Nat. Rev. Mol. Cell Biol.* **1**, 11–21 (2000).
- Moe, S. M. Disorders involving calcium, phosphorus, and magnesium. *Prim. Care* **35**, 215–37, v–vi (2008).
- Zaheer, A. *et al.* Optical imaging of hydroxyapatite in the calcified vasculature of transgenic animals. *Arter. Thromb. Vasc. Biol.* **26**, 1132–1136 (2006).
- Lee, J. S., Morrisett, J. D. & Tung, C.-H. Detection of hydroxyapatite in calcified cardiovascular tissues. *Atherosclerosis* **224**, 340–7 (2012).
- Hutcheson, J. D., Maldonado, N. & Aikawa, E. Small entities with large impact: microcalcifications and atherosclerotic plaque vulnerability. *Curr. Opin. Lipidol.* **25**, 327–32 (2014).
- Sakaguchi, M. *et al.* New insights into spotty calcification and plaque rupture in acute coronary syndrome: an optical coherence tomography study. *Heart Vessels* **31**, 1915–1922 (2016).
- Otsuka, F., Sakakura, K., Yahagi, K., Joner, M. & Virmani, R. Has our understanding of calcification in human coronary atherosclerosis progressed? *Arter. Thromb. Vasc. Biol.* **34**, 724–736 (2014).
- Wu, B., Pei, X. & Li, Z.-Y. How does calcification influence plaque vulnerability? Insights from fatigue analysis. *Sci. World J.* **2014**, 417324 (2014).
- Irkle, A. *et al.* Identifying active vascular microcalcification by 18F-sodium fluoride positron emission tomography. *Nat. Commun.* **6**, 7495 (2015).
- Rungby, J., Kassem, M., Eriksen, E. F. & Danscher, G. The von Kossa reaction for calcium deposits: silver lactate staining increases sensitivity and reduces background. *Histochem. J.* **25**, 446–451 (1993).
- Paul, H., Reginato, A. J. & Schumacher, H. R. Alizarin red S staining as a screening test to detect calcium compounds in synovial fluid. *Arthritis Rheum.* **26**, 191–200 (1983).
- Jono, S., Nishizawa, Y., Shioi, A. & Morii, H. Parathyroid hormone-related peptide as a local regulator of vascular calcification. Its inhibitory action on *in vitro* calcification by bovine vascular smooth muscle cells. *Arter. Thromb. Vasc. Biol.* **17**, 1135–42 (1997).
- Bonewald, L. F. *et al.* Von Kossa staining alone is not sufficient to confirm that mineralization *in vitro* represents bone formation. *Calcif. Tissue Int.* **72**, 537–547 (2003).
- Hale, L. V., Ma, Y. F. & Santerre, R. F. Semi-quantitative fluorescence analysis of calcein binding as a measurement of *in vitro* mineralization. *Calcif. Tissue Int.* **67**, 80–4 (2000).
- Gavin, C. T. *et al.* Novel methods of determining urinary calculi composition: Petrographic thin sectioning of calculi and nanoscale flow cytometry urinalysis. *Sci. Rep.* **6**, 19328 (2016).
- Li, N., Song, J., Zhu, G., Shi, X. & Wang, Y. Alendronate conjugated nanoparticles for calcification targeting. *Colloids Surfaces B Biointerfaces* **142**, 344–350 (2016).
- Coxon, F. P., Thompson, K., Roelofs, A. J., Ebetino, F. H. & Rogers, M. J. Visualizing mineral binding and uptake of bisphosphonate by osteoclasts and non-resorbing cells. *Bone* **42**, 848–860 (2008).
- Swami, A. *et al.* Engineered nanomedicine for myeloma and bone microenvironment targeting. *Proc. Natl. Acad. Sci.* **111**, 10287–10292 (2014).
- Kowada, T. *et al.* *In vivo* fluorescence imaging of bone-resorbing osteoclasts. *J. Am. Chem. Soc.* **133**, 17772–17776 (2011).
- Sjöback, R., Nygren, J. & Kubista, M. Absorption and fluorescence properties of fluorescein. *Spectrochim. Acta Part A Mol. Biomol. Spectrosc.* **51**, L7–L21 (1995).
- Zhang, X. F., Zhang, J. & Liu, L. Fluorescence properties of twenty fluorescein derivatives: Lifetime, quantum yield, absorption and emission spectra. *J. Fluoresc.* **24**, 819–826 (2014).
- Neumann, M., Fuldner, S., König, B. & Zeitler, K. Metal-free, cooperative asymmetric organophotoredox catalysis with visible light. *Angew. Chem. Int. Ed.* **50**, 951–954 (2011).
- Zhang, L., Dong, S. & Zhu, L. Fluorescent dyes of the esculetin and alizarin families respond to zinc ions ratiometrically. *Chem. Commun.* 1891–3 (2007).
- Mackenzie, N. C. W. *et al.* MOVAS-1 cell line: A new *in vitro* model of vascular calcification. *Int. J. Mol. Med.* **27**, 663–8 (2011).
- Afroz, T. *et al.* Calcineurin-independent regulation of plasma membrane Ca²⁺ ATPase-4 in the vascular smooth muscle cell cycle. *Am. J. Physiol.* **285**, C88–C95 (2003).
- Murshed, M. & McKee, M. D. Molecular determinants of extracellular matrix mineralization in bone and blood vessels. *Curr. Opin. Nephrol. Hypertens.* **19**, 359–365 (2010).
- Abedin, M., Tintut, Y. & Demer, L. L. Vascular calcification: Mechanisms and clinical ramifications. *Arter. Thromb. Vasc. Biol.* **24**, 1161–1170 (2004).
- Zhu, D., Mackenzie, N. C. W., Millan, J. L., Farquharson, C. & Macrae, V. E. Upregulation of IGF2 expression during vascular calcification. *J. Mol. Endocrinol.* **52**, 77–85 (2014).
- Cui, L., Houston, D. A., Farquharson, C. & MacRae, V. E. Characterisation of matrix vesicles in skeletal and soft tissue mineralisation. *Bone* **87**, 147–158 (2016).
- Liu, C. *et al.* Vulnerable atherosclerotic plaque detection by resonance Raman spectroscopy. *J. Biomed. Opt.* **21**, 127006 (2016).
- Hokazono, E. *et al.* Development of a new measurement method for serum calcium with chlorophosphonazo-III. *Annal. Clin. Biochem.* **46**, 296–301 (2009).

32. Cui, L. *et al.* End stage renal disease-induced hypercalcemia may promote aortic valve calcification via Annexin VI enrichment of valve interstitial cell derived-matrix vesicles. *J. Cell. Physiol.* **232**, 2985–2995 (2017).
33. Lee, Y.-K. *et al.* Proliferation, differentiation, and calcification of preosteoblast-like MC3T3-E1 cells cultured onto noncrystalline calcium phosphate glass. *J. Biomed. Mater. Res.* **69A**, 188–195 (2004).
34. Hiura, K. *et al.* Mouse osteoblastic cells (Mc3t3-e1) at different stages of differentiation have opposite effects on osteoclastic cell formation. *Endocrinology* **128**, 1630–1637 (1991).
35. Akiyoshi, T. *et al.* A novel organ culture model of aorta for vascular calcification. *Atherosclerosis* **244**, 51–58 (2016).
36. Lomashvili, K. A., Cobbs, S., Hennigar, R. A., Hardcastle, K. I. & O'Neill, W. C. Phosphate-induced vascular calcification: Role of pyrophosphate and osteopontin. *J. Am. Soc. Nephrol.* **15**, 1392–1401 (2004).
37. Dweck, M. R. *et al.* Imaging of coronary atherosclerosis — evolution towards new treatment strategies. *Nat. Rev. Cardiol.* **13**, 533–548 (2016).
38. Adamson, P. D., Vesey, A. T., Joshi, N. V., Newby, D. E. & Dweck, M. R. Salt in the wound: 18 F-fluoride positron emission tomography for identification of vulnerable coronary plaques. *Cardiovasc. Diagn. Ther.* **5**, 150–155 (2015).
39. Carlstorm, D., Engfeldt, B., Engstrom, A. & Ringertz, N. Studies on the chemical composition of normal and abnormal blood vessel walls. I. Chemical nature of vascular calcified deposits. *Lab. Invest.* **2**, 325–35 (1953).
40. Kelly-Arnold, A. *et al.* Revised microcalcification hypothesis for fibrous cap rupture in human coronary arteries. *Proc. Natl. Acad. Sci.* **110**, 10741–10746 (2013).
41. Vesey, A. T. *et al.* 18 F-Fluoride and 18 F-fluorodeoxyglucose positron emission tomography after transient ischemic attack or minor ischemic stroke: Case-control study. *Circ Cardiovasc. Imaging* **10**, e004976 (2017).
42. Joshi, N. *et al.* Systemic atherosclerotic inflammation following acute myocardial infarction: Myocardial infarction begets myocardial infarction. *J. Am. Heart Assoc.* **4**, e001956 (2015).
43. Forsythe, R. O. *et al.* 18 F-Sodium fluoride uptake in abdominal aortic aneurysms. *J. Am. Coll. Cardiol.* **71**, 513–523 (2018).
44. Bratosin, D., Mitrofan, L., Paliu, C., Estaquier, J. & Montreuil, J. Novel fluorescence assay using calcein-AM for the determination of human erythrocyte viability and aging. *Cytom. Part A* **66**, 78–84 (2005).
45. Hernandez-Santana, A., Yavorsky, A., Loughran, S. T., McCarthy, G. M. & McMahon, G. P. New approaches in the detection of calcium-containing microcrystals in synovial fluid. *Bioanalysis* **3**, 1085–1091 (2011).
46. Russell, J. T. Imaging calcium signals *in vivo*: A powerful tool in physiology and pharmacology. *Br. J. Pharmacol.* **163**, 1605–1625 (2011).
47. Furry, J. Preparation, properties and applications of Calcein in a highly pure form. *Retrospective Theses and Dissertations* (1985).
48. Diehl, H. & Ellingboe, J. L. Indicator for titration of calcium in presence of magnesium using disodium dihydrogen ethylenediamine tetraacetate. *Anal. Chem.* **28**, 882 (1956).
49. Garland, M., Yim, J. J. & Bogyo, M. A bright future for precision medicine: Advances in fluorescent chemical probe design and their clinical application. *Cell Chem. Biol.* **23**, 122–136 (2016).
50. Vonwil, D., Christensen, J., Fischer, S., Ronneberger, O. & Shastri, V. P. Validation of fluorescence molecular tomography/micro-CT multimodal imaging *in vivo* in rats. *Mol. Imaging Biol.* **16**, 350–61 (2014).
51. Harmatys, K. M., Cole, E. L. & Smith, B. D. *In vivo* imaging of bone using a deep-red fluorescent molecular probe bearing multiple iminodiacetate groups. *Mol. Pharmacol.* **10**, 4263–71 (2013).
52. Zhu, D., Mackenzie, N. C. W., Millán, J. L., Farquharson, C. & MacRae, V. E. The appearance and modulation of osteocyte marker expression during calcification of vascular smooth muscle cells. *PLoS One* **6**, e19595 (2011).
53. Zhu, D., Rashdan, N. A., Chapman, K. E., Hadoko, P. W. & MacRae, V. E. A novel role for the mineralocorticoid receptor in glucocorticoid driven vascular calcification. *Vascul. Pharmacol.* **86**, 87–93 (2016).
54. Johnson, K. A., Polewski, M. & Terkeltaub, R. A. Transglutaminase 2 is central to induction of the arterial calcification program by smooth muscle cells. *Circ. Res.* **102**, 529–537 (2008).

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Author Contributions

A.M.S., N.R., L.C., V.E.M., A.N.H., F.N. and M.D. designed the experiments; A.M.S. performed all the experiments apart from VSMCs isolation (N.R.) and PET/CT (AJM). The paper was written by A.M.S., N.R., A.J.M., M.D., F.N., V.E.M. and A.N.H.

Additional Information

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