Original Article

Assessment and comparison of retention of zirconia copings luted with different cements onto zirconia and titanium abutments: An *in vitro* study

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Abstract

Aim: The purpose of this *in vitro* study was to assess and compare the retention of zirconia copings luted with different luting agents onto zirconia and titanium abutments.

Materials and Methods: Titanium and zirconia abutments were torqued at 35 N/cm onto implant analogs. The samples were divided into two groups: Group A consisted of four titanium abutments and 32 zirconia copings and Group B consisted of four zirconia abutments and 32 zirconia copings and four luting agents were used. The cemented copings were subjected to tensile dislodgement forces and subjected to ANOVA test.

Results: Zirconia abutments recorded a higher mean force compared to titanium. Among the luting agents, resin cement recorded the highest mean force followed by zinc phosphate, glass ionomer, and noneugenol zinc oxide cement, respectively.

Conclusion: Highest mean retention was recorded for zirconia implant abutments compared to titanium abutments when luted with zirconia copings.

Key Words: Titanium abutment, zirconia abutment, zirconia copings

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INTRODUCTION

Main goals of restorations in modern dentistry are optimal function and esthetics.[1] The options for restoring edentulous areas have changed dramatically with the introduction of endosseous dental implants. Clinical decisions are not only limited to the selection of the type of implant but also the type of abutment and cement used.[2] Initially, implant-supported prostheses were exclusively retained by screws, but with the development of new implant systems and rehabilitation techniques cement retained prostheses have become popular treatment option. Cement-retained superstructures over the implant abutments assure passive fit because of the cement layer between the framework and abutment. Other advantages of cement-retained implant restorations include improved direction of load, enhanced esthetics, easy access, reduced fabrication cost and time, simplified restorative procedures, and optimum occlusion excluding the interference of screw access openings.

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Limitations associated with the cement-retained implant restorations include low profile retention, when there is limited interarch space, retrievability, and presence of cement in the sulcus.[3] Commercially, pure titanium has been widely used as an abutment material in implant therapy because of its well-documented biocompatibility and mechanical properties. Recently, zirconia implant abutment materials have gained popularity because of their better fracture resistance and superior optical properties over titanium.[2] Selection of luting agent is very important for cement-retained implant prostheses and it is largely dependent on operator preference, convenience, and manufacturer recommendations. Ideal luting agent should be strong enough to retain the restorations yet weak enough so that restorations can be removed easily if required.[4] The aim of this study was to assess and compare the retentive strengths of different classes of luting agents used to cement zirconia copings to titanium and zirconia implant abutments.

MATERIALS AND METHODS

Materials

Materials used in the present study included eight implant analogs (Collagen Meniscus Implant [CMI]), four titanium [Figure 1] abutments (CMI, hexed abutment), four zirconia abutments [Figure 2], and 64 zirconia copings (Lava, Zirconia 3M ESPE) [Figures 3 and 4]. The luting agents used were resin cement (Calibra-Densply), glass ionomer (GC gold label luting and lining cement), zinc phosphate (Harvard Cement), and zinc oxide noneugenol (Rely X™ Temp NE) cements.

Methodology

Fabrication of resin blocks and emdedding specimen

Eight implant analogs (CMI) were embedded in acrylic resin blocks, titanium and zirconia abutments were torqued into implant analogs. Acrylic resin blocks were fabricated to facilitate mounting the specimen on tensile strength testing machine. Implant analogs were embedded into acrylic block. Abutments were torqued onto implant analogs. An 8 mm diameter hole was drilled at the end of acrylic block to facilitate mounting the specimen on tensile testing machine. A single operator prepared all eight resin blocks and implant analogs were embedded, and abutments were torqued at 35 N/cm. Both zirconia and titanium abutments used in the study were of 7.4 mm in height with 8° convergence angle and 5.8 mm in diameter.[5]

Fabrication of zirconia copings

Samples were divided into two groups. Group A consisted of four titanium abutments and 32 zirconia copings. Group B consisted of four zirconia abutments and 32 copings. Resin pattern were made for zirconia copings; an extension was made on the occlusal surface of each coping parallel to long axis of the tooth to serve as a connector to the tensile strength testing machine. zirconia copings thus designed were milled with computer aided designing – computer aided manufacturing unit.

Figure 1: Titanium abutment mounted on acrylic resin blocks

Figure 2: Zirconia abutment mounted on acrylic resin blocks

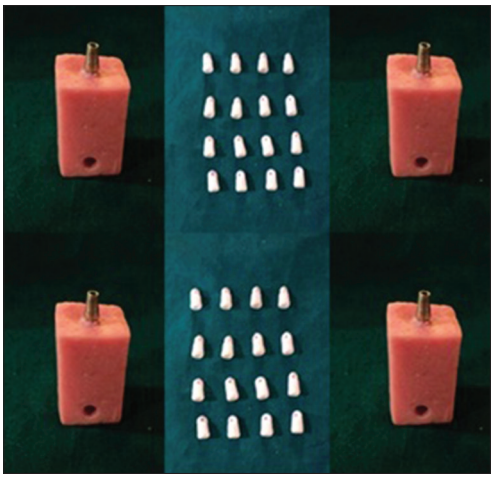


Figure 3: Group A consisting of four titanium abutments and 32 zirconia copings

Cementation of copings

Both Groups A and B were randomly divided into four groups each comprising specimens Groups 1-4. Zirconia copings in Groups A1 and B1 were cemented with glass ionomer (GC gold label luting and lining cement) cement, Groups A2 and B2 were cemented with resin cement (Calibra-Densply), Groups A3 and B3 were cemented with zinc oxide noneugenol cement (Rely X™ Temp NE), and Groups A4 and B4 were cemented with zinc phosphate cement (Harvard Cement). Each coping of all groups was sandblasted with 50 μm aluminum oxide before cementation. Cements were mixed according to the manufacturer's instructions and were applied in a thin layer to the inner axial walls of the crown. Each coping was seated on its perspective abutment with firm finger pressure and then placed under a 10 kg weight for 5 min and cementation was carried out [Figure 5]. Excess cement was removed with an explorer.

Thermocycling and tensile testing

Specimens were stored at room temperature for 24 h and immersed in artificial saliva for 7 days, after which specimens were thermo cycled 100 times between 5°C and 55°C with a dwell time of 10 s, dried and subjected to retention test.[6] The cemented copings were subjected to tensile dislodgement forces using crosshead speed of 0.5 mm/min until cement failure occurred[4] [Figures 6-8]. The same abutment was used with each of the coping and four cements were evaluated. Abutments were cleaned with a plastic explorer. Abutments were immersed in an ultrasonic cleaner for 15 min and re-used.

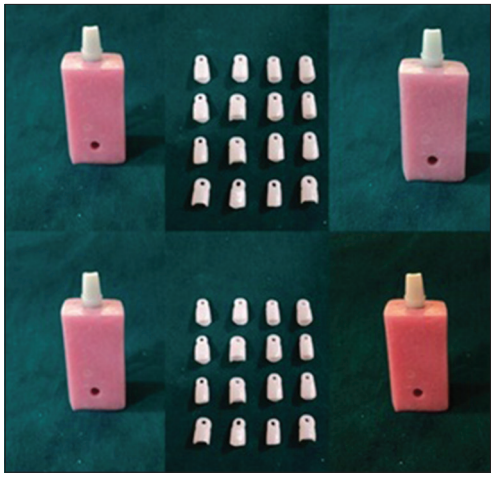


Figure 4: Group B consisting of four zirconia abutments and 32 zirconia copings

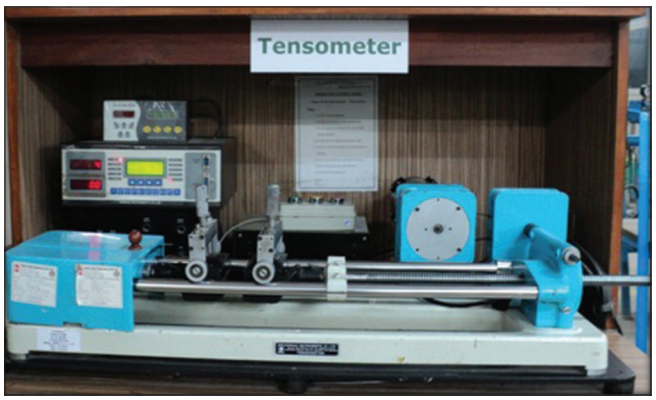


Figure 6: Tensometer

RESULTS

Results obtained from the retention test were statistically analyzed using factorial ANOVA test.

Among the cements, the highest mean force was recorded in resin cement followed by zinc phosphate, glass ionomer, and noneugenol zinc oxide, respectively. The difference in mean force recorded between them was found to be statistically significant ($P < 0.001$) [Table 1].

Between the two abutments, the higher mean force was recorded in zirconia and the difference in mean force between zirconia and titanium was found to be statistically significant ($P < 0.001$) [Table 2].

Figure 5: Device used to apply load on coping during cementation

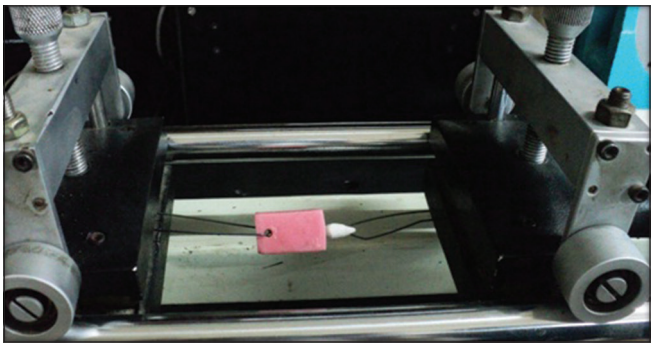


Figure 7: Specimens mounted on tensometer

Table 1: Depicts the mean tensile force recorded for all the four cements

Cement	Mean	SD	SE of mean	Median	Minimum	Maximum
Glass ionomer	99.38	27.46	6.86	102.0	49	139
Noneugenol zinc oxide	16.31	5.79	1.45	16.0	6	29
Resin cement	552.63	118.39	29.60	575.5	370	720
Zinc phosphate	251.44	49.36	12.34	258.5	176	327

SD: Standard deviation, SE: Standard error

Table 2: Depicts the mean tensile force recorded for the two abutments

Abutment	Mean	SD	SE of mean	Median	Minimum	Maximum
Zirconia	271.50	246.26	43.53	200.0	13	720
Titanium	188.38	174.55	30.86	139.0	6	556

SD: Standard deviation, SE: Standard error

The interaction (joint effect) of cement and abutment on force was also found to be statistically significant ($P < 0.001$) [Table 3 and Graph 1].

Noneugenol zinc oxide cement always had a lower mean force when used with titanium or zirconia abutments. Resin cement always has a higher mean force compared to other cements when used either with titanium or zirconia abutment. All the cements yield a higher mean force when used with zirconia abutment compared to titanium abutment.

After resin cement, the higher mean force was recorded in zinc phosphate and glass ionomer, respectively [Table 4 and Graph 2].

DISCUSSION

Prosthetic rehabilitation of edentulous areas using implants has become a popular treatment modality. All ceramic crowns are used in implants more often than metal ceramic crowns to enhance esthetics. The most commonly used material in all ceramic being zirconia due to its high flexibility, fracture toughness, biocompatibility, and excellent esthetics. Zirconia abutments in comparison with titanium abutments enhance the esthetic effect especially in case of maxillary anterior implants, since they do not allow display of metal, unlike titanium abutments.[7] Mansour *et al.* found that the rank order of cement retentiveness differed when tested on implants rather than on natural teeth.[8] Among the four types of cements used to lute Zirconia copings, resin cement showed the highest mean force when used with zirconia as well as titanium abutments. The higher mean retention of resin cement, when used along with Zirconia abutments, is due to the presence of adhesive phosphate monomer in the resin cement that enhances the bonding between them. Sandblasting of zirconia copings also enhances the retention by increasing the microroughness of the surface.[9,10] Studies conducted by Barbosa *et al.* have proved that resin cements bond with the titanium alloy by reacting with metal oxides. The phosphate ester group of acidic monomer

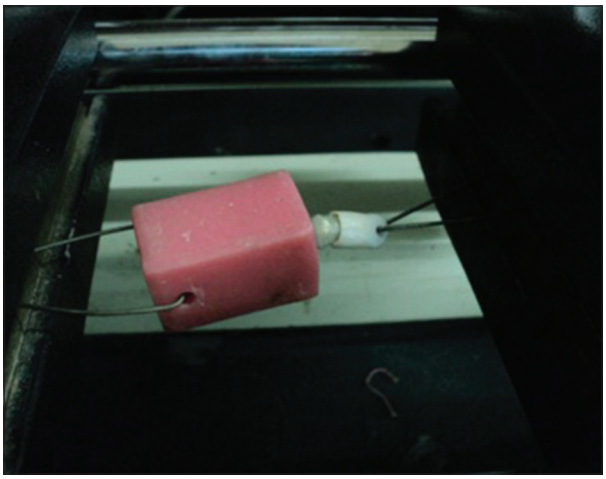
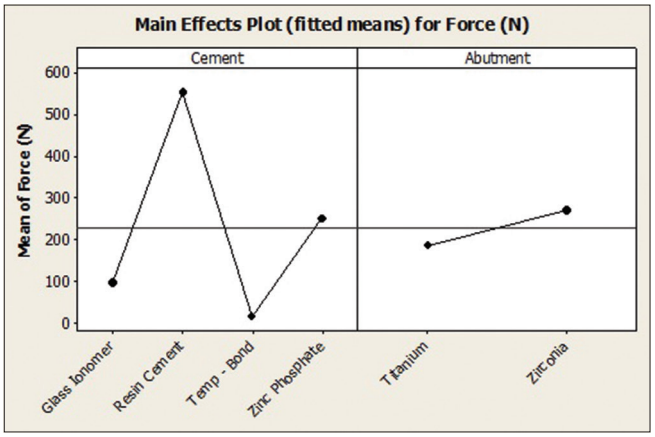
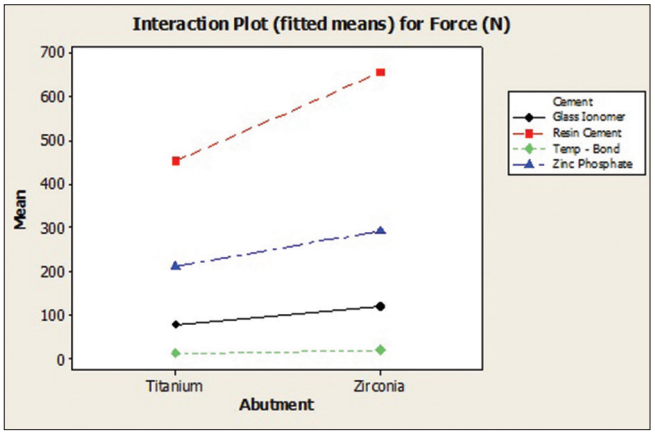


Figure 8: Samples subjected to dislodging forces



Graph 1: Main effects plot depicting the mean tensile force recorded with four cements and zirconia and titanium abutments



Graph 2: Interaction plot depicting the mean tensile force recorded with four cements and zirconia and titanium abutments

Table 3: Depicts the mean tensile force recorded for both cement and abutment

Cement	Abutment	Mean	SD	SE of mean	Median	Minimum	Maximum
Glass ionomer	Zirconia	120.13	12.29	4.34	120.0	102	139
	Titanium	78.63	21.92	7.75	84.0	49	102
Noneugenol zinc oxide	Zirconia	20.00	4.99	1.76	19.0	13	29
	Titanium	12.63	4.00	1.41	13.5	6	18
Resin cement	Zirconia	654.25	39.31	13.90	649.5	595	720
	Titanium	451.00	69.87	24.70	439.5	370	556
Zinc phosphate	Zirconia	291.63	21.76	7.69	290.5	261	327
	Titanium	211.25	32.50	11.49	208.0	176	256

SD: Standard deviation, SE: Standard error

Table 4: Depicts the statistical significance

Source	df	SS	Mean SS	*F*	*P*
Cement	3	2,676,346.875	892,115.625	827.080	<0.001*
Abutment	1	110,556.250	110,556.250	102.500	<0.001*
Cement × abutment	3	87,633.125	29,211.042	27.080	<0.001*
Error	56	60,403.500	1078.634	-	-
Total	63	2,934,939.750	-		

SS: Sum of square, The difference in mean force recorded between the cements, between the abutments and interaction between cement and abutment on force were found to be statistically significant. ($P<0.001$)

results in chemical bonding with metal oxides. Studies have also proved that sandblasting the titanium abutment surface with alumina also enhances the bonding between resin cement and titanium abutment.[11] D'Amario *et al*.[3] noted that bond strength of resin cement decreased when subjected to thermocycling, which resulted in weakening the bond between zirconia and resin cement leading to bond failure.

Following resin cement second highest mean retention was recorded for zinc phosphate cement. Zinc phosphate cement provides retention by micromechanical bonding. The surface irregularities on the abutment/coping improve the retention. In this study, machined abutment (zirconia and titanium) surface was not modified with any preparation or surface treatments and therefore relatively smooth.[12] This could have decreased the cement abutment micromechanical interlocking leading to debonding of zirconia copings from the respective abutments. Bond failure may also be affected by thermocycling process since zinc phosphate cement exhibit solubility in water. Following zinc phosphate cement, the next highest mean retentive force recorded was for glass ionomer cement. Adhesion in glass ionomer is as a result of molecular interactions of an ionic/polar nature. It does not adhere to the inert surfaces of metal and metal oxides, unlike resin cements where phosphate ester groups directly bonds with the metal oxides. Studies have revealed that the solubility of glass ionomer cement is more than that of zinc phosphate and is very susceptible to early water contact and desiccation which can dramatically reduce the mechanical properties of cement.[13] The least retentive force was recorded with noneugenol zinc oxide cement. It may be due to its poor marginal seal and high solubility in water. Temp-Bond has higher solubility in direct contact with water and also requires sufficient time for complete setting reaction in order to maximize retention.[12]

CONCLUSION

Within the limitations of this study, following conclusions were drawn:

Highest mean retention was recorded for zirconia copings cemented on to zirconia abutments when compared to titanium abutments. Zirconia copings when luted onto zirconia abutments, highest mean retention were recorded with resin cement followed by zinc phosphate cement and glass ionomer cement. Least mean retention was recorded with noneugenol zinc oxide cement. Zirconia copings when luted onto titanium abutments highest mean retention was recorded with resin cement followed by zinc phosphate cement and glass ionomer cement. Least mean retention was recorded with noneugenol zinc oxide cement. The above study provides a superficial idea about the retention of zirconia copings with four different types of lutings on to zirconia as well as titanium abutments, which will help the clinician in deciding during prosthetic rehabilitation with implant-supported restorations. The study also highlights the chemical and mechanical factors that influence retention of cements onto the abutments. Scanning electron microscopic analysis must be required to provide a more accurate analysis on the bonding mechanisms, which is a limitation of the present study.

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Nil.

Conflicts of interest
There are no conflicts of interest.

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