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# Immunoaffinity biosensors for the detection of SARS-CoV-1 using screened Fv-antibodies from an autodisplayed Fv-antibody library

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#### ABSTRACT

The detection of severe acute respiratory syndrome coronavirus (SARS-CoV-1) was demonstrated using screened Fv-antibodies for SPR biosensor and impedance spectrometry. The Fv-antibody library was first prepared on the outer membrane of E. coli using autodisplay technology and the Fv-variants (clones) with a specific affinity toward the SARS-CoV-1 spike protein (SP) were screened using magnetic beads immobilized with the SP. Upon screening the Fv-antibody library, two target Fv-variants (clones) with a specific binding affinity toward the SARS-CoV-1 SP were determined and the Fv-antibodies on two clones were named "Anti-SP1" (with CDR3 amino acid sequence: <sup>1</sup>GRTTG<sup>5</sup>NDRPD<sup>11</sup>Y) and "Anti-SP2" (with CDR3 amino acid sequence: <sup>1</sup>CLRQA<sup>5</sup>GTADD<sup>11</sup>V). The binding affinities of the two screened Fv-variants (clones) were analyzed using flow cytometry and the binding constants (K<sub>D</sub>) were estimated to be  $80.5\pm3.6$  nM for Anti-SP1 and  $45.6\pm8.9$  nM for Anti-SP2 (n = 3). In addition, the Fv-antibody including three CDR regions (CDR1, CDR2, and CDR3) and frame regions (FRs) between the CDR regions was expressed as a fusion protein (Mw. 40.6 kDa) with a green fluorescent protein (GFP) and the  $K_D$  values of the expressed Fv-antibodies toward the SP estimated to be 15.3  $\pm$  1.5 nM for Anti-SP1 (n =3) and 16.3  $\pm$  1.7 nM for Anti-SP2 (n = 3). Finally, the expressed Fv-antibodies screened against SARS-CoV-1 SP (Anti-SP1 and Anti-SP2) were applied for the detection of SARS-CoV-1. Consequently, the detection of SARS-CoV-1 was demonstrated to be feasible using the SPR biosensor and impedance spectrometry utilizing the immobilized Fv-antibodies against the SARS-CoV-1 SP.

# 1. Introduction

Human coronaviruses (CoVs), such as CoV strains OC43, HKU1, NL63, and CoV-229E, are known to be among the most common etiologic agents for seasonal common colds and also pneumonia (Jain et al., 2015; Sariol and Perlman, 2020; Jung et al., 2021b). In particular, severe acute respiratory syndrome (SARS) has been reported to be caused by beta-CoV, as in the case of MERS and COVID-19 (Belouzard et al., 2012; Bong et al., 2020, 2021a; Chen et al., 2020; Elfiky, 2020; Jung et al., 2021a; Wuertz et al., 2021). SARS-associated coronavirus (SARS-CoV-1) infection has been reported to occur through binding of SARS-CoV-1 spike protein (SP) to the angiotensin-converting enzyme 2 (ACE2) receptor of the host cell (Lan et al., 2020; Sun et al., 2020). The receptor binding domain (RBD) of homotrimer spike glycoprotein is known to be the core region for the interaction between SP and ACE2,

and the binding affinity of SP to ACE2 is known to be in the range of ~31–100 nM (Lan et al., 2020; Walls et al., 2020; Wrapp et al., 2020; Zahradník et al., 2021). Consequently, antibodies against the RBD region of the SP have been studied as potential therapeutic targets that can block viral entry to the host cell, and many research groups have reported the development of multiple high-affinity neutralizing antibodies against CoVs (He et al., 2006; Liu et al., 2020). For the detection of SARS-CoV-1 in medical samples, various kinds of detection methods have been used, such as PCR methods, immunoassays and so on. As summarized in Table 1, PCR methods have been used as a confirmatory test of infection because of its high sensitivity and the lateral flow immunoassay based on antibodies against SARS-CoV-1 SP have been widely used for the ease of detection without any instruments and rapid analysis time with a compromised sensitivity (Poon et al., 2004; Tahamtan and Ardebili, 2020; Oishee et al., 2021). For the development

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**Table 1**Detection technologies for SARS-CoVs.

| Detection<br>method                          | Limit of detection                                    | Sensitivity       | Analysis<br>time  | Reference   |
|--|---|-------------------|-------------------|---|
| Cell culture and microscopy                  | N/A   | +++               | 1–2 days          | (Farkash et al., 2020;<br>Oishee et al., 2021)  |
| Radiology-based<br>detection                 | N/A   | $\leftrightarrow$ | 10 min            | (Peiris et al., 2003;<br>Cozzi et al., 2020;<br>Oishee et al., 2021)  |
| Real-time RT-<br>PCR                         | 0.3-100<br>copies/ $\mu$ L<br>Cut-off = 34-35<br>(Ct) | +++               | 1–2 h             | (Lau et al., 2003;<br>Tahamtan and<br>Ardebili, 2020;<br>Engelmann et al.,<br>2021; Oishee et al.,<br>2021)                   |
| RT-LAMP                                      | 5 copies/<br>μL                                       | +++               | 40 min            | (Poon et al., 2004;<br>Park et al., 2020;<br>Oishee et al., 2021;<br>Lino et al., 2022)                                       |
| CRISPR-based<br>diagnosis                    | 10<br>copies/μL                                       | +++               | 30–40<br>min      | (Broughton et al.,<br>2020; Oishee et al.,<br>2021; Lee et al.,<br>2022b; Lino et al.,<br>2022)                               |
| ELISA/CLIA                                   | $\leftrightarrow$                                     | ++                | $\leftrightarrow$ | (Bundschuh et al., 2020; Oishee et al., 2021)   |
| Lateral flow<br>immunoassay                  | $\leftrightarrow$                                     | +                 | <20 min           | (Quesada-González<br>and Merkoçi, 2015;<br>Oishee et al., 2021;<br>Lino et al., 2022)   |
| Electrochemical<br>impedance<br>spectroscopy | 6 pg/mL   | +++               | <10 min           | (Drobysh et al., 2022;<br>Lino et al., 2022;<br>Liustrovaite et al.,<br>2022; Ong et al.,<br>2023; Zukauskas<br>et al., 2023) |
| Total internal<br>reflection<br>ellipsometry | 0.3 nM<br>(K <sub>D</sub> )                           | +++               | $\leftrightarrow$ | (Qi et al., 2006;<br>Drobysh et al., 2022;<br>Plikusiene et al.,<br>2022a, 2022b)   |
| Field effect<br>transistor                   | 242<br>copies/μL                                      | +++               | $\leftrightarrow$ | (Lino et al., 2022;<br>Novodchuk et al.,<br>2022)   |
| Surface plasmon resonance                    | 38.7 (Ct)<br>(using<br>Anti-SP2)                      | +++               | <20 min           | This work   |
| Electrochemical impedance spectroscopy       | 38.2 (Ct)<br>(using<br>Anti-SP2)                      | +++               | <10 min           | This work   |

<sup>&</sup>quot;+" Positive/Good; "++" Better; "+++" High; "↔" Variable; "-" Negative.

of a sensitive immunoassays including the lateral flow immunoassay, the screening of antibodies against SARS-CoV-1 with a high affinity to ACE2 has been a critical process (Lan et al., 2020; Sun et al., 2020).

This work presents the screening of Fv-antibodies against the SARS-CoV-1 SP from an Fv-antibody library, which was expressed on the outer membrane of E. coli. As shown in Fig. 1(a), Fv-antibody in this work represented the variable region of V<sub>H</sub>-region which was composed of three CDR regions (CDR1, CDR2, and CDR3) and frame regions (FRs) in between the CDR regions (Xu and Davis, 2000). To prepare the Fy-antibody library, the amino acid sequence of the CDR3 region was randomized using site-directed mutagenesis, as shown in Fig. 1(b) (Xie et al., 2020). As previously reported (Jung et al., 2021c, 2021d; Lee et al., 2021; Sung et al., 2022a, 2022b), the Fv-antibody library plasmid was prepared based on anti-thyroid peroxidase (TPO) antibodies as a template sequence and the amino acid sequence of the CDR3 region (composed of eleven amino acids) was randomized and Fv-antibody library plasmids were prepared. As shown in Fig. 1(c), so-prepared Fv-antibody library plasmid was inserted into an authodisplay vector which expressed the Fv-antibody library on the outer membrane of E. coli (Jose and Meyer, 2007; Gratz et al., 2015). The control strain with the Fv-variant bearing the CDR1 and CDR2 regions was also prepared as

the control. The efficiency of autodisplayed proteins have been reported to be as high as 10<sup>5</sup> proteins/E. coli (Jose and Meyer, 2007). And, the transformation was estimated to be occurred for more than 90% of total E. coli population (Yoo et al., 2015). Because of such a high expression efficiency of autodisplay technology, the target Fv-variants with a high affinity toward target antigens could be achieved without the need to perform the repeated biopanning process. So far various kinds of antibody libraries have been reported based on site-directed mutagenesis of IgG as summarized in Table 2. For example, the bacteriophage based antibody library has been the most frequently used among various libraries. In the case of the bacteriophage based antibody library was reported to have a transformation efficiency of <10 proteins/bacteriophage and <10% of total bacteriophage population (Pande et al., 2010). From such a low expression efficiency, the repeated biopanning process was inevitably required for the screening of target variants. Using the autodisplayed Fv-antibody library, several kinds of target Fv-variants have been screened against various antigens, such as biotin, dopamine, fluorescein, rhodamine B, and monosodium urate crystal, using an autodisplayed Fv-antibody library (Jung et al., 2021c, 2021d; Lee et al., 2021; Sung et al., 2022a, 2022b).

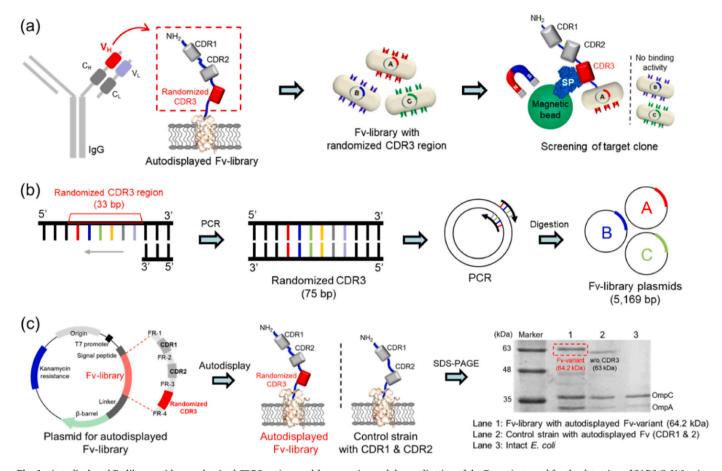
In comparison with the conventional IgG, the size of Fv-antibody (13.6 kDa) is far smaller than IgG (150 kDa). Such small antibodies or antibody fragments have been reported to have serval advantages for biosensor applications: (1) the small antibodies have a relatively high physico-chemial stability, such as high solubility, solvent-resistance and thermal tolerance (Kolkman and Law, 2010); (2) the small antibodies could be effectively used for transducers with a limited sensitive layer thickness, such as surface plasmon resonance (SPR) with the evanescence field in the range of 100-400 nm (Roper, 2007), field effect transistor (FET) with a Debye length of 0.7 nm (Chu et al., 2017), and electrochemical impedance spectroscopy (EIS) with an outer helmholtz plane (OHP) distance of <1.0 nm (Nakamura et al., 2011; Zhao et al., 2022); (3) the small antibodies could be effectively screened from antibody libraries for the antigens with a molecular weight of less than 5 kDa which had a low immunogenicity (Andorko et al., 2017; Jung et al., 2021d). As previously reported, the autodisplayed Fv-antibody library presented the feasibility of screening Fv-antibodies against various small antigens and biomarkers, such as dopamine for Parkinson's disease (Sung et al., 2022b), food allergens (Sung et al., 2022a), and monosodium urate crystal for gout (Jung et al., 2021c); (4) the small antibodies could be screened and produced in a short time in comparison with the antibody production using animal immunization (Fridy et al.,

In this work, Fv-variants (clones) with a high affinity toward the SARS-CoV-1 SP were screened from the Fv-antibody library and the binding affinities of the two screened clones were analyzed using flow cytometry. And the, the screened Fv-antibodies against SARS-CoV-1 SP (Anti-SP1 and Anti-SP2) were expressed as a fusion protein with green fluorescence protein (GFP). Finally, the detection of SARS-CoV-1 was demonstrated for viral cultures of SARS-CoV-1 using the SPR biosensor and impedance spectrometry utilizing the immobilized Fv-antibodies obtained from the two screened clones against SARS-CoV-1 SP.

# 2. Experimental

# 2.1. Materials

SARS-CoV-1 SP (recombinant with amino acid residues of 14–667, 72.9 kDa) was supplied from Optolane Inc. (Seongnam, Korea). Luria-Bertani (LB) medium was purchased from Duchefa (Haarlem, Netherlands). M-280 tosyl-activated dynabead (diameter: 2.8 µm) was purchased from Invitrogen Co. (Carlsbad, CA, USA). Bovine serum albumin was purchased from Sigma-Aldrich Korea Seoul, Korea). Primers were custom-synthesized by Bionics (Seoul, Korea). Klenow DNA polymerase was purchaed from New England BioLabs (Ipswich, MA, USA). A PCR purification mini kit was purchased from Favorgen (Pingtug,



**Fig. 1.** Autodisplayed Fv-library with a randomized CDR3 region used for screening and the application of the Fv-variant used for the detection of SARS-CoV-1 using immunoaffinity biosensors. (a) Procedure for the screening of the Fv-variants from Fv-antibody library with randomized amino acid sequence at CDR3 region. (b) Preparation of the Fv-library with a randomized CDR3 region at V<sub>H</sub> using site-directed mutagenesis. (c) Expression of the Fv-library on the outer membrane of *E. coli* using an autodisplay vector (SDS-PAGE of the autodisplayed Fv-variant, a control strain with CDR1 & CDR2, and intact *E. coli*).

**Table 2** Antibody libraries based on protein engineering technologies.

| Screening technology                      | Anchor<br>protein | Surface density                                     | Expression efficiency | Diversity of<br>library  | Screening method        | Reference                                 |
|---|-------------------|---|-----------------------|--------------------------|-------------------------|---|
| E. coli autodisplayed library (This work) | AIDA-1            | > 10 <sup>5</sup> proteins/<br>E. coli              | > 95%                 | $> 10^6 - 10^7$ clones   | FACS (no<br>biopanning) | Jose and Meyer (2007)                     |
| Anchored periplasmic expression           | APEX              | > 10 <sup>5</sup> proteins/<br>E. coli              | > 95%                 | $> 10^6 - 10^7$ clones   | Biopanning (2–5 times)  | Harvey et al. (2004)                      |
| Phage library                             | M13 gene III      | < 10 proteins/<br>phage                             | > 10%                 | > 10 <sup>7</sup> clones | Biopanning (2–5 times)  | Pande et al. (2010)                       |
| Yeast library                             | Aga1-Aga2         | 10 <sup>4</sup> -10 <sup>5</sup> proteins/<br>yeast | > 40%                 | > 10 <sup>7</sup> clones | FACS (no<br>biopanning) | (Linciano et al., 2019; Mei et al., 2019) |

Taiwan). Phusion high-fidelity DNA polymerase was purchased from Thermo Fisher Scientific (Waltham, MA, USA). Plasmids for Fv-antibody labeled with green fluorescence protein (Superfolder GFP) (Liu et al., 2019; Kim et al., 2021) were custom-synthesized by Cosmogenetech (Seoul, Korea). Viral cultures were purchased from Zeptometrix (Buffalo, NY, USA): NATtrol<sup>TM</sup> SARS-CoV-1 (Ct = 25–28), MERS-CoV (Ct = 25–28), CoV-229E strain reagent (Ct = 25–28) and NATtrol<sup>TM</sup> negative control reagent (A-549 cells, 50,000 cells/mL) (; Jung et al., 2021a, 2021b; Wei et al., 2021; Park et al., 2022).

# 2.2. Autodisplay of the Fv-variants library

The Fv-antibody library was prepared and autodisplayed as previously reported (Jung et al., 2021c, 2021d; Lee et al., 2021; Sung et al., 2022a, 2022b). To prepare the Fv-antibody library with site-directed

mutagenesis at the CDR3 region, the single-stranded forward primer with a randomized sequence of CDR3 (75 bp) was mixed with the corresponding reverse primer (22 bp), as shown in Fig. 1(b). The primer sequences for the Fv-antibody library are summarized in Table S1.

Subsequently, annealing of the primers (2  $\mu L$ , respectively) was performed upon heating at 95 °C for 5 min, followed by cooling at 36 °C with NEB buffer (4  $\mu L$ ) and DW (32  $\mu L$ ) in a total volume of 40  $\mu L$ . For the extension reaction, Klenow (exo-) DNA polymerase (3  $\mu L$ ), NEB buffer (16  $\mu L$ ), 10 mM dNTPs (8  $\mu L$ ), and distilled water (DW, 133  $\mu L$ ) were added to obtain a total volume of 200  $\mu L$ .

Thereafter, the extension reaction was performed at 37  $^{\circ}\text{C}$  for 15 min. After inactivation of the enzyme reaction at 75  $^{\circ}\text{C}$  for 20 min, the PCP products (double-stranded primers of Fv-antibody library with a randomized CDR3 region) were filtered using a PCR purification mini kit. The Fv-antibody library plasmid with a randomized CDR3 sequence

was prepared using anti-thyroid peroxidase (TPO) antibodies as a template sequence. Fv-antibody library plasmids were synthesized using a template plasmid (pST009, 150 ng), double-stranded Fv-antibody library primer mixture (150 ng), HF buffer (10 µL), 10 mM dNTPs (1 µL), and Phusion high-fidelity DNA polymerase (0.5  $\mu$ L) in a total volume of 50 µL. PCR was performed using the following steps: (1) Initial denaturation (98 °C for 1 min), (2) denaturation (98 °C for 30 s), (3) annealing (68 °C for 1 min), (4) elongation (72 °C for 5 min), (5) repetition of (2)-(4) for 30 cycles, and (6) termination (72 °C for 10 min). Finally, the template plasmids were digested using DpnI restriction enzyme (37  $^{\circ}$ C for 16 h). The digested Fv-antibody library plasmids were filtered using a 100 K Amicon filter (Millipore, Billerica, MA, USA). The autodisplay of the Fv-antibody library on the outer membrane of E. coli BL21(DE3) was performed by transforming the prepared Fv-antibody library plasmid into competent intact cells via electroporation, as shown in Fig. 1(c) (Dower et al., 1988). The transformed E. coli cells were cultured in LB broth containing 50  $\mu g/mL$  kanamycin at 37 °C for 16 h. The cultured E. coli cells (100 μL) were then cultured again in LB medium (10 mL) containing 99% β-mercaptoethanol (8 μL), kanamycin (50 μg/mL), and ethylenediaminetetraacetic acid (5 μM) at 37 °C with shaking (150 rpm) until it reached an OD<sub>600nm</sub> of 0.6. To induce Fv-antibody library expression, the cultured E. coli cells (10 mL,  $OD_{600nm} = 0.6$ ) were incubated with 1 mM isopropylthio- $\beta$ -galactoside (IPTG) at 30 °C with shaking (120 rpm) for 3 h.

#### 2.3. Screening of the target Fv-variants (clones)

Screening of the targeted *E. coli* with Fv-antibodies (Fv-variants) from the autodisplayed Fv-antibody library was performed using the following steps: (1) Fv-antibody library (500  $\mu L$ , OD $_{600}=0.5)$  was reacted with M-280 tosyl-activated dynabeads (5 mg) coated with SARS-CoV-1 SP (20  $\mu g$ ) at 37 °C and 10 rpm for 1 h, (2) the target *E. coli*-bound

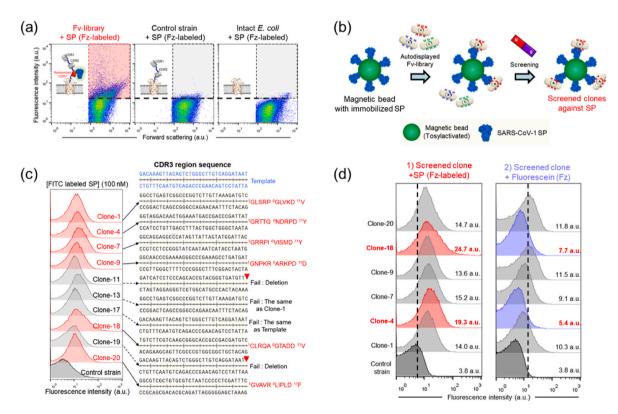
magnetic beads were sorted using a magnet and the unbound *E. coli* were removed by rinsing the beads five times with 0.01% PBST and PBS, (3) the separated magnetic beads with bound *E. coli* against SARS-CoV-1 SP were resuspended in PBS (100  $\mu$ L), and (4) the separated magnetic beads in PBS were spread on agar plates to obtain the screened *E. coli* clones, as shown in Fig. 2(b) (Jung et al., 2021b; Lamaiphan et al., 2021).

The binding properties of the screened *E. coli* clones against SARS-CoV-1 SP were estimated by mixing with FITC-labeled SARS-CoV-1 SP (Vira et al., 2010).

The screened *E. coli* (150  $\mu$ L, OD<sub>600</sub> = 0.5) were mixed with the FITC-labeled SARS-CoV-1 SP (3.1–100.0 nM) for 1 h. After centrifugation (3000×g, 2 min), the screened *E. coli* clones were washed with 0.01% PBST and PBS. After resuspension in PBS, the fluorescence intensity of screened clones was recorded using a FACSCalibur flow cytometer (Becton–Dickinson, Franklin Lakes, NJ, USA) operated at an excitation wavelength of 488 nm, as shown in Fig. 3.

#### 2.4. Expression of the Fv-antibodies

The plasmids (pJY003 and pJY004), encoding an open reading frame of the Fv-antibody with binding activity toward the SARS-CoV-1 SP, fusion proteins were custom-synthesized by Cosmogenetech (Seoul, Korea), as shown in Fig. 4(a). The amino acid sequences of Fv-antibody consisted of CDRs and FRs were summarized in Table S2. The Fv-antibody was expressed intracellularly in *E. coli* by transforming the customized plasmid into competent cells. The transformed *E. coli* were cultured in 20 mL high-salt LB medium containing 1 mM IPTG and 30  $\mu$ g/mL carbenicillin for 16 h at 30 °C. *E. coli* pellet was collected via centrifugation (3000×g, 3 min) and then resuspended in 50 mL of binding buffer (5 mM Tris-HCl, 0.5 mM EDTA, and 1 M NaCl) with 3 M urea. And then, the resuspended *E. coli* was sonicated using a sonic reactor (Vibra cell VCX-130, Sonics, USA). The lysate was centrifuged at



**Fig. 2.** Screening of the Fv-variants (clones) with affinity toward the spike SP of SARS-CoV-1. (a) Flow cytometric analysis after treatment of the fluorescence labeled SP to the Fv-antibody library, the control strain with CDR1, CDR2, and intact *E. coli*. (b) Screening procedure for the target clones using magnetic beads with immobilized SP. (c) Selection of the target clones using flow cytometry and genetic sequencing of the CDR3 region. (d) A comparison of the binding affinity of the screened clones to SP and fluorescence dye (fluorescein).

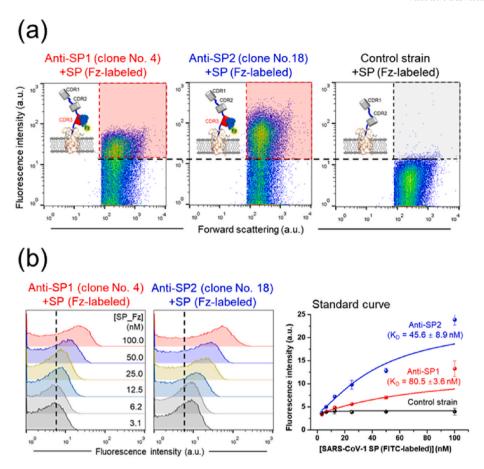


Fig. 3. Estimation of binding affinity of the screened clones. (a) Flow cytometric analysis after treatment of the fluorescence labeled SP with the screened clones compared with the control strain with CDR1 and CDR2. (b) Determination of the binding constant  $(K_D)$  using a quantitative binding assay with flow cytometry.

 $25,000\times g$  for 10 min. The Fv-antibody in the supernatant was then purified on a His-tag purification column from Roche (Bassel, Switzerland) using elution buffer (binding buffer with 3 M urea and 500 mM imidazole) (Spriestersbach et al., 2015). The purified proteins were dialyzed for 16 h at 100 rpm and 4 °C to remove urea and imidazole.

# 2.5. SPR biosensor and impedance spectrometry utilizing the expressed Fv-antibodies

SPR measurements of the expressed Fv-antibodies obtained from Anti-SP1 and Anti-SP2 were estimated using an SPR biosensor from i-Cluebio (Seongnam, Korea). The assay configuration was prepared using the immobilized expressed Fv-antibodies or SARS-CoV-1 SP on the gold surface of the SPR biosensor. SPR chips for SPR measurements were prepared using the following steps: BK-7 glass  $(1 \times 1 \text{ cm}^2)$  was sputter coated with titanium, (thickness: 2 nm) as the adhesive layer, and gold (thickness: 48 nm). Fig. 4(b) and (c) show the SPR chips were incubated with the Fv-antibodies or SARS-CoV-1 SP (20 μg/mL, respectively) at 4 °C for 16 h. After washing with PBS, incubation for non-specific blocking with BSA (1 mg/mL) was performed for 1 h. After the washing step, a solution of the SARS-CoV-1 SP (3.8-30.0 nM) or Fvantibodies (15.0-120.0 nM) solution was injected into the flow cell for 10 min (15 μL/min) as the association step. Finally, PBS was injected into the flow cell for 10 min (15  $\mu L/min$ ) as the dissociation step. The diluted  $NATtrol^{TM}$  SARS-CoV-1, MERS-CoV, CoV-229E strain and negative samples in the dilution range of 100-fold (Ct value = 33.1) to 8000-fold (Ct value = 39.4) were analyzed in the same way as described using the SPR biosensor, as shown in Fig. 5(b). The SPR measurements were carried out by treating the samples under the flow conditions and the SPR signal according to the amount of bound analytes was recorded

after the dissociation step (Jung et al., 2021d). The SPR signal was calculated as the dose-response curve for the samples with solution protein was carried out by the isotherm model:

$$R = \frac{R_{MAX}.[Ag]}{K_d + [Ag]}$$

where R represented the SPR signal (Rmax = maximum SPR signal), [Ag] represented the solution protein concentration and K  $_{\rm d}$  represented affinity constant (Bong et al., 2020).

The results of SPR signals and impedance signals were fitted using Hill's equation.

$$y = \frac{a-d}{1 + \left(x/c\right)^2} + d$$

Where a and d were the maximum and minimum signals, respectively; c was the concentration of the solution protein; and b was the Hill's slope of the curve (Oshannessy et al., 1993; Saleviter et al., 2019; Lee et al., 2022a).

Impedance spectroscopy was carried out using a three-electrode system and commercial potentiostat from IVIUM Technologies (Eindhoven, Netherlands) (Bong et al., 2019; Patel et al., 2021; Jeong et al., 2022; Park et al., 2022). A gold electrode was prepared by sputtering a titanium layer (10 nm) as an adhesive layer and a gold layer (200 nm) on an  $SiO_2$  wafer as a working electrode. Pt wire was used as a counter electrode for impedance spectroscopy. The reaction vessel was attached with a UV-curing glue to expose the working electrode area of 30 mm<sup>2</sup> (Bong et al., 2021b; Park et al., 2021; Song et al., 2022). The expressed Fv-antibodies (20 µg/mL) were immobilized on the electrode for 2 h. Incubation for non-specific blocking with BSA (1 mg/mL) was

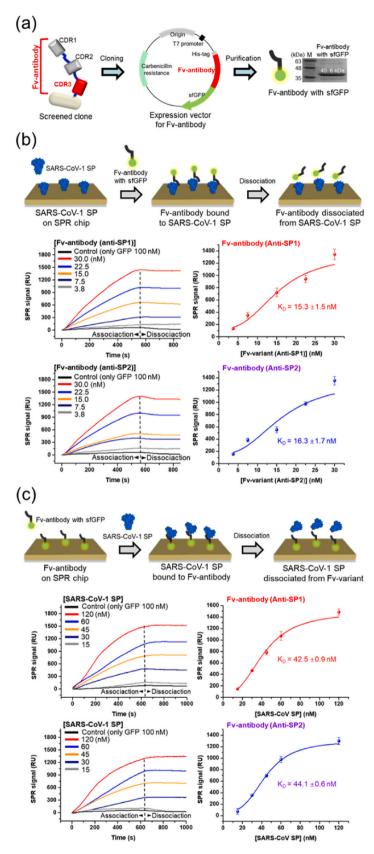


Fig. 4. Expression of the screened Fv-antibodies and estimation of the binding affinity. (a) Expression procedure for the screened Fv-antibodies. (b) Estimation of the binding constant ( $K_D$ ) of the Fv-antibodies (Anti-SP1 and Anti-SP2) from two screened clones toward the immobilized SARS-CoV-1 SP using the SPR biosensor. (c) Estimation of the binding constant ( $K_D$ ) of SARS-CoV-1 SP toward the immobilized Fv-antibodies using the SPR biosensor.

(a)

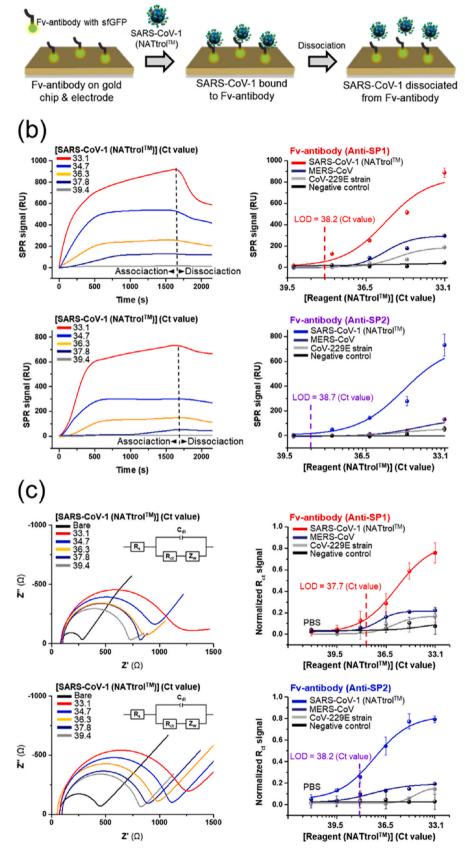


Fig. 5. Detection of SARS-CoV-1 using the SPR biosensor and impedance spectrometry. (a) Assay configuration of the SPR biosensor and impedance spectrometry with the immobilized Fv-antibodies (Anti-SP1 and Anti-SP2). (b) Detection of SARS-CoV-1 using the SPR biosensor with two kinds of immobilized Fv-antibodies (Anti-SP1 and Anti-SP2) from two screened clones. (c) Detection of SARS-CoV-1 using impedance spectrometry with two kinds of the screened Fv-antibodies (Anti-SP1 and Anti-SP2) from two screened clones.

performed on the electrode for 1 h. Diluted NATtrol<sup>TM</sup> SARS-CoV-1, MERS-CoV, CoV-229E strain and negative samples were added to the electrode and incubated for 30 min in the dilution range of 100-fold (Ct value = 33.1) to 8000-fold (Ct value = 39.4). Each detection was performed after a washing step with 0.01% PBST and PBS. Impedance spectroscopy was carried out in the frequency range of 0.1 Hz-1 MHz (amplitude: 10 mV) versus the Ag/AgCl reference electrode (amplitude: 50 mV) in potassium ferricyanide (50 mM), as shown in Fig. 5(c). The measured impedance value was performed using the Randles equivalent circuit model consisting of the parallel charge transfer resistance (Rct) and a combination of double-layer capacitance (C<sub>dl</sub>) with series medium resistance (R<sub>s</sub>). The normalized charge transfer resistance (R<sub>ct</sub>) signal was calculated by normalizing the change in R<sub>ct</sub> after absorbing analyte on the electrode with the initial R<sub>ct</sub> value of electrode. The calculation was performed as following equation: Normalized  $R_{ct}$  signal =  $[R_{ct}$  - $R_{ct0}$ ]/ $R_{ct0}$ , where  $R_{ct}$  was the value after the adsorption of analyte on the electrode and R<sub>ct0</sub> was the initial R<sub>ct</sub> value of the electrode (Bong et al., 2021b; Park et al., 2021)

#### 3. Results and discussion

#### 3.1. Screening of the Fv-antibodies against the SARS-CoV-1 SP

The Fv-antibody library with three CDR regions was prepared as previously reported by randomizing the CDR3 region (Jung et al., 2021c, 2021d; Lee et al., 2021; Sung et al., 2022a, 2022b). In addition, the control strain was also prepared with only CDR1 and CDR2 regions (without CDR3 region). After the fluorescence labeled SARS-CoV-1 SP was reacted to the Fv-antibody library, the control strain (with only CDR1 and CDR2), and intact *E. coli* (without autodisplayed Fv-antibodies), flow cytometric analysis was carried out and the resulting dot plots were compared with the Fv-antibody library. Fig. 2(a) showed that the Fv-antibody library exhibited a high fluorescence region on the dot plot when compared with that of the control strain (with only CDR1 and CDR2) and intact *E. coli* (without the autodisplayed Fv-antibodies) over the cut-off value (displayed as a dashed line in the graphs). In the case of the control strain and the intact *E. coli* only showed a fluorescence signal under the cut-off value.

Therefore, the high fluorescence region of the Fv-antibody library indicated that the CDR3 regions of some of the Fv-variants (clones) could bind to the fluorescence labeled SP with a high affinity. The Fv-variants (clones) with a specific affinity toward SP were screened from the autodisplayed Fv-antibody library on the outer membrane of *E. coli*. Fig. 2(b) showed that the SP was covalently immobilized on the tosylactivated magnetic beads. Magnetic beads with the immobilized SP were incubated with the Fv-antibody library to screen Fv-variants (clones) with a binding affinity toward the SP. The magnetic beads with bound *E. coli* were isolated using an external magnet and then cultured on an agar plate. These clones were further analyzed to confirm that (1) the Fv-variants (clones) had a variated genetic sequence for the CDR3 region when compared with the template sequence, and (2) the Fv-variants (clones) had a specific affinity to the SP using the fluorescence labeled SP.

Among the cultured colonies on the agar plate, twenty colonies were randomly selected from the Fv-antibody library. Fig. 2(c) showed that the nucleotide sequences were analyzed for the randomized CDR3 region and six clones (Clone No. 1, 4, 7, 9, 18, and 20) were determined to have a binding affinity toward the fluorescence labeled SP, which had appropriate nucleotide sequences from the site-directed mutagenesis when compared with the template sequence. The other fourteen clones had inappropriate nucleotide sequences: Two clones were found to have deleted nucleotides, two clones had a repeated nucleotide sequence, and ten clones had the same nucleotide sequence as the template plasmid before site-directed mutagenesis. To investigate whether the binding of the fluorescence-labeled SP occurred at the fluorescence dye (fluorescein), the six selected clones (Clone No. 1, 4, 7, 9, 18, and 20) were

reacted with the fluorescence-labeled SP as well as fluorescein dye. When the fluorescence dye (fluorescein) was reacted with the six selected clones, a remarkable fluorescence signal was observed for four clones (Clone No. 1, 7, 9, and 20), which indicated the non-specific binding of the fluorescence-labeled SP to these clones via the labeled fluorescence dye (fluorescein), as shown in Fig. 2(d). Two target clones with a specific binding affinity toward the SP were determined (Clone No. 4 and 18) and Fv-antibodies on two clones were named "Anti-SP1" for Clone No. 4 (amino acid sequence of CDR3 region: \(^1\)GRTTG^5NDRPD^\(^1\)Y) and "Anti-SP2" for Clone No. 18 (amino acid sequence of CDR3 region: \(^1\)CLRQA^5GTADD^\(^1\)V). The nucleotide sequences and corresponding amino acid sequences of the screened CDR3 regions were summarized in Table 3.

# 3.2. Binding properties of screened Fv-antibodies

The binding affinity of two screened Fv-variants (clones) was analyzed using flow cytometry. Initially, the fluorescence signals from the two screened clones were compared with the control strain (with only CDR1 and CDR2) after treatment with SARS-CoV-1 SP labeled with fluorescein. Fig. 3(a) showed the dot plots obtained for the two screened clones (Anti-SP1 and Anti-SP2) showed a far higher fluorescence signals when compared with the control strain. These results showed that the two screened clones had Fv-variants with a far higher affinity toward the SP via CDR3 regions.

To evaluate the binding constants (K D) of the screened Fv-variants (clones), the fluorescence signal observed from the two screened clones were analyzed upon treatment with different concentrations of the fluorescein labeled SP. Fig. 3(b) showed the fluorescence signal was observed to quantitatively increase in the concentration range studied, and the signal observed for the control strain was maintained at the baseline level. To evaluate the K<sub>D</sub> values of the Fv-variants (clones), the peak value was taken as the fluorescence signal. The dose-response curve was obtained by plotting the fluorescence signal with respect to the concentration of the fluorescence labeled SP. By fitting the doseresponse curve using an isotherm model (Oshannessy et al., 1993; Saleviter et al., 2019; Bong et al., 2020), the K<sub>D</sub> value was estimated to be 80.5  $\pm$  3.6 nM for Anti-SP1 and 45.6  $\pm$  8.9 nM for Anti-SP2 (n = 3) on the Fv-variants (clones). According to the literature, the K<sub>D</sub> of SARS-CoV-1 SP toward the ACE2 receptor of the host was in the range of 31-100 nM (Lan et al., 2020; Walls et al., 2020; Wrapp et al., 2020; Zahradník et al., 2021). These results showed that the two screened Fv-variants (clones) had comparably high binding affinities toward the SARS-CoV-1 SP.

The Fv-antibodies including three CDR regions (CDR1, CDR2, and CDR3) and frame regions in-between the CDR regions were expressed as a fusion protein of GFP, as shown in Fig. 4(a). The GFP-fusion protein was carried out for the following reasons: (1) the Fv-antibody had a limited solubility and the fusion protein with GFP has a far improved solubility (Pédelacq et al., 2006; Liu et al., 2019) and (2) the GFP could be used effectively for the immobilization to the metal surface of biosensors. The immobilization efficiency of GFP was estimated to be similar to BSA which were frequently used as a blocking protein for immunoassays.

The binding of the expressed Fv-antibodies to the SP was monitored using the SPR sensor, which were associated and dissociated under

**Table 3**Comparison of the amino acid sequence of the screened CDR3 regions.

| Screened Fv-<br>antibody | Sequence (11-amino acid)                                   | Oligonucleotide sequence (33 base pairs)            |
|--------------------------|--|---|
| Anti-SP1                 | N- <sup>1</sup> GRTTG <sup>5</sup> NDRPD <sup>11</sup> Y-C | 5'-GGT AGG ACA ACT GGAAAT<br>GAC CGA CCC GAT TAT-3' |
| Anti-SP2                 | N- <sup>1</sup> CLRQA <sup>5</sup> GTADD <sup>11</sup> V-C | 5'-TGT CTT CGT CAA GCGGGC ACC<br>GCC GAC GAT GTC-3' |

continuous flow conditions. After the SP was immobilized on the SPR-chip, different concentrations of the expressed Fv-antibodies in the range of 3.8–30.0 nM were added, as shown in Fig. 4(b). The  $K_D$  values of the expressed Fv-antibodies toward the SP were estimated to be 15.3  $\pm$  1.5 nM for the expressed Anti-SP1 and 16.3  $\pm$  1.7 nM for the expressed Anti-SP2 (n = 3).

As the next step, the K D values of the immobilized Fv-antibodies toward the SARS-CoV-1 SP were also estimated using the SPR biosensor for the application of the expressed Fv-antibodies to detect SARS-CoV-1. The expressed Fv-antibodies were immobilized on the SPR biosensor and different concentrations of the SARS-CoV-1 SP in the range of 15.0-120.0 nM were added, as shown in Fig. 4(c). The binding of the SP toward the expressed Fv-antibodies was monitored using the SPR sensor under the same continuous flow conditions and the K<sub>D</sub> values of the expressed Fv-antibodies toward the SP were estimated to be 42.5  $\pm$  0.9 nM for the expressed Anti-SP1 and 44.1  $\pm$  0.6 nM for the expressed Anti-SP2 (n = 3). These results show that: (1) The binding constants for the immobilized Fv-antibodies to SPR were estimated to be in the nanomolar range and (2) the immobilized Fv-antibodies could be used for the detection of SARS-CoV-1. Additionally, the comparable binding constants (K<sub>D</sub> values) of Fv-antibodies in comparison with those of native virus indicated that the Fv-antibody library could be effectively used for the screening of Fv-antibodies against various antigens related to other viral diseases.

#### 3.3. Detection of SARS-CoV-1 using the expressed Fv-antibodies

The expressed Fv-antibodies (Anti-SP1 and Anti-SP2) obtained from the two screened clones against SARS-CoV-1 SP were used for the detection of SARS-CoV-1 using the SPR biosensor and impedance spectrometry. As a real sample of SARS-CoV-1, the  $NATtrol^{TM}$  reagent of SARS-CoV-1 from Zeptometrix (Buffalo, NY, USA) was used, which was prepared with a similar composition to medical samples (Jung et al., 2021a, 2021b; Wei et al., 2021; Park et al., 2022). The cycle threshold (Ct) value of the NATtrol  $^{\text{TM}}$  reagent was in the average range of 26.5 for SARS-CoV-1 (Wei et al., 2021; Park et al., 2022); the cut-off Ct value for the conventional diagnosis of SARS-CoV-1 using RT-PCR was reported to be 35 (Lau et al., 2003; Poon et al., 2003). In this work, standard samples for diagnosis using the SPR biosensor and impedance spectrometry were prepared upon serial dilution of the NATtrol<sup>TM</sup> reagent. As a negative control, NATtrol<sup>TM</sup> negative reagent without SARS-CoV-1 from Zeptometrix (Buffalo, NY, USA) was used in the SPR biosensor and impedance spectrometry.

Fig. 5(a) showed that the assay configuration for the detection of SARS-CoV-1 was prepared by immobilizing the expressed Fv-antibodies on the sensor surfaces of the SPR biosensor and gold electrode in the impedance spectrometer. SPR measurements were carried out upon treating the diluted SARS-CoV-1 samples obtained from the NATtrol TM SARS-CoV-1 reagent in the average Ct range of 26.5 diluted in the range of 100-fold (Ct value = 33.1) to 8000-fold (Ct value = 39.4). Fig. 5(b) showed that the SPR measurements were carried out by treating the samples under flow conditions and the SPR signal according to the amount of bound analytes was recorded after the dissociation step. The detection of SARS-CoV-1 was possible in the dilution range of 100-fold (Ct value = 33.1) to 8000-fold (Ct value = 39.4); the SPR signal from the negative samples was maintained at the baseline level. The limit of detection was estimated to be the dilution factor of 3300-fold (Ct value = 38.2) for the Fv-antibodies (Anti-SP1) and 5000-fold (Ct value = 38.7) for the Fv-antibodies (Anti-SP2). These results show that the medical diagnosis of SARS-CoV-1 was feasible using the SPR biosensor with the screened antibodies (Anti-SP1 and Anti-SP2) against the SARS-CoV-1 SP.

Impedance spectrometry was carried out by treating the diluted SARS-CoV-1 samples in the same dilution range of 100-fold (Ct value = 33.1) to 8000-fold (Ct value = 39.4). Impedance spectrometry was carried out upon treating the samples under flow conditions and the impedance signal according to the amount of bound analytes was taken

at the x-cut of the impedance spectrum after the washing step, as shown in Fig. 5(c). From the Nyquist plot (Fig. 5(c)), the signal of the charge transfer resistance (R ct) was taken from the fitting based on the Randles equivalent circuit model, which consisted of a parallel combination of double layer capacitance (Cdl) and charge transfer resistance (Rct) with a series medium resistance (R<sub>s</sub>). As previously reported (Park et al., 2021), the x-cut value represented the charge transfer resistance (Rct), which indicated the resistance required for charge transfer to the electrode. Upon binding SARS-CoV-1, the R<sub>ct</sub> value was observed to quantitatively increase, which indicated the specific binding of SARS-CoV-1 to the immobilized Fv-antibodies. The normalized charge transfer resistance (Rct) signal was calculated by normalizing the change in Rct after absorbing analyte on the electrode with the initial R<sub>ct</sub> value of electrode. The calculation was performed as following equation: Normalized R<sub>ct</sub>  $signal = [R_{ct} - R_{ct0}]/R_{ct0}$ , where  $R_{ct}$  was the value after the adsorption of analyte on the electrode and R<sub>ct0</sub> was the initial R<sub>ct</sub> value of the electrode (Bong et al., 2021b; Park et al., 2021). The detection of SARS-CoV-1 was possible in the range of 100-fold (Ct value = 33.1) to 8000-fold (Ct value = 39.4) and the impedance signal from the negative samples was maintained at the baseline level. The limit of detection was estimated to be 2500-fold (Ct value = 37.7) for the expressed Anti-SP1 and 3300-fold (Ct value = 38.2) for the expressed Anti-SP2. These results showed that the feasibility of medical diagnosis of SARS-CoV-1 using impedance spectrometry utilizing two screened Fv-antibodies (Anti-SP1 and Anti-SP2) against the SARS-CoV-1 SP. As summarized in Table 1, the LOD of this work was estimated to be Ct = 38.7 (with Anti-SP2) using SPR biosensor and Ct = 38.2 (with Anti-SP2) using impedance spectrometry. These results indicated that the LOD of this work was comparable to conventional real-time PCR methods which had the gold standard method for the diagnosis of SARS-CoVs with cutoff value of Ct = 34–35. Such a high level of LOD was estimated to be the high binding affinity (K<sub>D</sub>) of the screened Fv-antibodies of Anti-SP1 (K<sub>D</sub> = 15.3 nM) and Anti-SP2 ( $K_D = 16.3 \text{ nM}$ ) in comparison with the  $K_D$  of SARS-CoV-1 SP toward the ACE2 receptor of the host was in the range of 31-100 nM (Lan et al., 2020; Walls et al., 2020; Wrapp et al., 2020; Zahradník et al., 2021).

# 4. Conclusions

An Fv-antibody library was prepared on the outer membrane of E. coli using autodisplay technology. The Fv-variants with a specific affinity toward the SARS-CoV-1 SP were screened using paramagnetic beads immobilized with the SP. From the screening of the Fv-antibody library, two target clones with a specific binding affinity toward the SP were determined (Clone No. 4, and No. 18) and the screened Fvantibodies were named "Anti-SP1" for Clone No. 4 (CDR3 amino acid sequence: <sup>1</sup>GRTTG<sup>5</sup>NDRPD<sup>11</sup>Y) and "Anti-SP2" for Clone No. 18 (CDR3 amino acid sequence: <sup>1</sup>CLRQA<sup>5</sup>GTADD<sup>11</sup>V). The binding affinities of the two screened clones were analyzed using flow cytometry. The fluorescence signal observed from these two screened clones were compared with the control strain with CDR1 and CDR2 only after treatment with SARS-CoV-1 SP labeled with fluorescein and the KD value was estimated to be 80.5  $\pm$  3.6 nM for Anti-SP1 and 45.6  $\pm$  8.9 nM for Anti-SP2. From the literature, the binding affinity of SARS-CoV-1 SP to the ACE2 receptor of the host has been reported to be 31-100 nM. These results show that the two screened Fv-variants have a comparably high binding affinity toward the SARS-CoV-1 SP. And, the small size of Fv-antibodies indicated the feasibility of effective applications to transducers with a limited sensitive layer thickness, such as surface plasmon resonance (SPR), field effect transistor (FET) and electrochemical impedance spectroscopy (EIS). In addition, the Fv-antibodies including three CDR regions (CDR1, CDR2, and CDR3) and frame regions in-between the CDR regions were expressed as a fusion protein of sfGFP. The binding of the expressed Fv-antibodies toward the SP was monitored using the SPR sensor and the KD values of the expressed Fv-antibodies toward the SP were estimated to be 15.3  $\pm$  1.5 nM for the expressed Fv-antibodies

(Anti-SP1) and  $16.3\pm1.7$  nM for the expressed Fv-antibodies (Anti-SP2) (n = 3). For the application of the expressed Fv-antibodies to detect SARS-CoV-1, the  $K_D$  values of the immobilized Fv-antibodies toward the SARS-CoV-1 SP were also estimated using the SPR biosensor. The assay results showed that: (1) The binding constants for the immobilized SARS-CoV-1 SP to the SPR were estimated to be in the nanomolar range and (2) the immobilized Fv-antibodies can be used for the detection of SARS-CoV-1. Finally, the expressed Fv-antibodies from the two screened clones against SARS-CoV-1 SP (Anti-SP1 and Anti-SP2) were applied for SARS-CoV-1 detection using the NATtrol TM reagent of SARS-CoV-1. The medical diagnosis of SARS-CoV-1 has been demonstrated to be feasible using the SPR biosensor as well as impedance spectrometry utilizing the immobilized Fv-antibodies obtained from the two clones screened against the SARS-CoV-1 SP.

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The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

# Data availability

Data will be made available on request.

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#### Appendix A. Supplementary data

Supplementary data to this article can be found online at https://doi.org/10.1016/j.bios.2023.115439.

#### **Abbreviations**

SARS-CoV-1 severe acute respiratory syndrome coronavirus

SP spike protein

CDR complementarity determining region ACE2 angiotensin-converting enzyme 2

RBD receptor binding domain

FRs frame regions

GFP green fluorescence protein

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