

RESEARCH ARTICLE

Modeling the Cellular Mechanisms and Olfactory Input Underlying the Triphasic Response of Moth Pheromone-Sensitive Projection Neurons

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Abstract

In the antennal lobe of the noctuid moth *Agrotis ipsilon*, most pheromone-sensitive projection neurons (PNs) exhibit a triphasic firing pattern of excitation (E_1)-inhibition (I)-excitation (E_2) in response to a pulse of the sex pheromone. To understand the mechanisms underlying this stereotypical discharge, we developed a biophysical model of a PN receiving inputs from olfactory receptor neurons (ORNs) via nicotinic cholinergic synapses. The ORN is modeled as an inhomogeneous Poisson process whose firing rate is a function of time and is fitted to extracellular data recorded in response to pheromone stimulations at various concentrations and durations. The PN model is based on the Hodgkin-Huxley formalism with realistic ionic currents whose parameters were derived from previous studies. Simulations revealed that the inhibitory phase I can be produced by a SK current (Ca^{2+} -gated small conductance K^+ current) and that the excitatory phase E_2 can result from the long-lasting response of the ORNs. Parameter analysis further revealed that the ending time of E_1 depends on some parameters of SK, Ca^{2+} , nACh and Na^+ currents; I duration mainly depends on the time constant of intracellular Ca^{2+} dynamics, conductance of Ca^{2+} currents and some parameters of nACh currents; The mean firing frequency of E_1 and E_2 depends differentially on the interaction of various currents. Thus it is likely that the interplay between PN intrinsic currents and feedforward synaptic currents are sufficient to generate the triphasic firing patterns observed in the noctuid moth *A. ipsilon*.

Introduction

Odor coding by the olfactory system has been studied by various experimental and modeling approaches. Natural odor stimuli can be characterized not only by their molecular features but also by properties such as concentration, spatial and temporal change of chemical components. Behavioral experiments on vertebrates [1], terrestrial [2–5] and aquatic invertebrates [6–7] showed that the physical characteristics of odor stimuli condition the behavioral

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response to an odorant. In moths, for example, intermittent and continuous stimulation with the same odor (the sex pheromone) evokes two distinct flight behaviors of upwind zig-zagging flight towards the odor source and cast/counter turn across the wind line, respectively [8]. The stimulation features are encoded and analyzed by individual neurons and neural networks of the olfactory system involving the antennae, the antennal lobes (ALs), the mushroom bodies (MBs) and the lateral horn in insects. Odorants are first detected and encoded by different types of olfactory receptor neurons (ORNs) situated in the antenna. Features of odorant stimuli are further analyzed in the AL, the first-order processing center. ORNs of the same type project to the same glomerulus [9] where they establish synaptic connections with multiglomerular local neurons (LNs), intrinsic to the AL, and uniglomerular projection neurons (PNs) [9]. The stimulation features/parameters influence the spatial and temporal activity patterns throughout the glomerular array and the response characteristics of individual PNs [10]. However, the neural basis of the differential response to the different physical odor stimulation features of the same odorant is poorly known. Neurons at different processing stages show different response patterns in response to the same stimulus [11–13]. Recordings in mitral/tufted cells in vertebrates and PNs in insects revealed that the odor-evoked responses of these second-order neurons are generally complex, consisting of both depolarizing and hyperpolarizing phases [12–19]. Remarkably, the temporal patterns of spike activity observed in some vertebrate mitral/tufted cells and insect PNs are very similar [12–20], suggesting common principles of cellular and/or synaptic mechanisms. In the macroglomerular complex (MGC) of the moth *A. ipsilon*, i.e. the specialist system processing pheromone information in the insect AL, a large majority of pheromone-sensitive PNs exhibit a triphasic firing pattern when the antenna is stimulated with pulses of the sex pheromone [12, 21]. Patch-clamp experiments revealed that several types of Na^+ , Ca^{2+} , and K^+ ionic currents are expressed in PNs [22–25] suggesting that they may play roles in shaping the activity patterns of PNs. Especially, it was recently found that SK channels are expressed in AL PNs both in *Drosophila* [24] and in *Agrotis* [25].

A number of biophysical models of neuron and network have been developed to investigate the cellular, synaptic, network structure and dynamical mechanisms underlying PN firing patterns and odor coding in the MGC or the AL of insects. First, a simplified Hodgkin–Huxley (HH) type neuron model and a neural network model with disinhibition mechanism were developed to simulate the low-frequency (< 10 Hz) background activity and the high-frequency (> 100 Hz) bursting capacity of pheromone-sensitive PNs in moth MGC [26–27]. In the absence of stimulation, the modeled PN is inhibited by a LN (denoted LN2), the model exhibits about 3Hz spontaneous oscillations. During odor stimulation, LN2 is inhibited by another LN (denoted LN1), the PN is released from inhibition and exhibits a burst response at frequency higher than 100 Hz. I_{Ca} and $I_{\text{K}(\text{Ca})}$ are responsible for burst and quiescent period generation whereas I_{A} reduces the firing frequency. However, in this model the activation and inactivation of the ionic channels of I_{Na} , I_{K} , I_{A} , I_{Ca} and $I_{\text{K}(\text{Ca})}$ are simplified and not biophysically realistic. Second, to simulate the temporal activity patterns induced by odor stimuli in the locust AL, neural networks with randomly connected neurons based on HH type models of PNs and LNs were developed [28–29]. In these models, I_{Ca} and $I_{\text{K}(\text{Ca})}$ for slow patterning generation were in non-spiking LNs, but not in PNs. The temporal patterns of PNs were generated through strong GABA_B -mediated slow inhibition. Third, in another small neural network model of AL consisting of identical PNs and LNs of HH type, the I_{Na} , I_{K} , I_{Ca} and $I_{\text{K}(\text{Ca})}$ were located in both PNs and LNs [30]. It was found that I_{Ca} and $I_{\text{K}(\text{Ca})}$ in PNs are sufficient to account for the slow patterning. The authors showed that the major effect of network inhibition is to redistribute the action potentials of the PNs from bursting to one action potential per cycle of oscillation. Fourth, based on morphological and physiological data from glomerular circuitry of insect AL

and using models of PNs and LNs developed in [28–29], a cross-scale neurodynamical model of the AL was developed [31]. This model demonstrates the effects of connectivity and complex dynamics in amplifying weak odor signals, in discriminating signals, and in detecting odor similarity, difference and specialty. Simulation results also showed that the spatiotemporal patterns of the odor information emerging in the glomeruli of the AL rely on the glomerular morphology, the connectivity and the complex dynamics of the AL circuits. Fifth, a model of the MGC in the moth *Manduca sexta* with HH type neuronal models and two types of inhibitory LNs, LNs-IIa, and LNs-IIb was proposed [32]. It was shown that synaptic inhibition, intrinsic currents I_A and I_{SK} in PNs can account for the first and second inhibitory phases and contribute to a rapid encoding of pheromone information. Sixth, recently, using a model of AL with PNs and LNs developed in [28–29], the relationship between a structural property of a network—its colorings, Ca^{2+} dynamics and the spatiotemporal activity and synchronization properties of PNs were explored [33]. Seventh, an inhibitory neural network model of MGC, which was quantitatively reduced from a HH conductance-based model to a mean field one, was recently developed [34]. It was analytically shown that the network's ability to operate on signal amplitudes across several orders of magnitude is optimal when a disinhibitory model is close to losing stability and the network dynamics are close to bifurcation.

However, most of the previous modeling work oversimplified the ORN inputs as an input current to PN. Moreover the ionic currents and parameters of the PN and LN models were not taken from insect neurons. In this work, the ORN was modeled from the experimental data recorded in the noctuid moth *A. ipsilon* from our lab [12]. In light of the availability of patch-clamp data of some ionic currents in PNs or other types of insect neurons [22, 36–38], we developed a biophysical model of PN. In a recent work, using a similar PN model with SK currents we reproduced the E_1 phase and I phase [21]. In the present paper, we describe the PN model and its parameters in detail and we consider a realistic ORN input modeled from experimental data. Based on the convergence rate in the moth pheromone system [35], we connected 100 ORNs to 1 PN by fast nicotinic cholinergic synapses to form a simple model of the MGC. Our model was built based on three types of experimental data: intracellular, extracellular and patch-clamp data recorded from ORNs, PNs and other neurons in insects obtained from our lab and other labs. Because ORNs do not show triphasic patterns we simply modeled each ORN firing by an inhomogeneous Poisson process. The firing frequency of the ORN model is a function of time and is fitted to the extracellular recorded data in response to pheromone stimulations varying in concentration and duration [12]. In order to better understand the cellular and synaptic mechanisms underlying the triphasic response patterns of PNs, we made a biophysical PN model taking into account the nicotinic cholinergic currents resulting from ORN synapses onto PNs and various intrinsic ionic currents found in PNs. The parameters in the voltage-dependent steady state and time-dependent functions were fitted to patch-clamp data [22, 36]. When no data were available on PN currents we utilized data from other neuron types in insects [37–38] or even vertebrates [39]. We hypothesize that the multiphasic firing patterns of PNs may be generated by the ionic currents in PNs and ORN inputs, the cholinergic synaptic currents from ORNs to PN may affect the PN response characteristics. Using this model we reproduced the recorded triphasic response patterns of PNs. Then, we investigated the ionic current mechanisms underlying these patterns. We further performed thorough analysis on how the response characteristics change with stimulation parameters and how the ORN inputs, the intrinsic and synaptic currents affect the response characteristics. In addition, we also reconstructed a model of LN and explored possible influences of LNs on the PN response characteristics through $GABA_A$ - and $GABA_B$ -mediated inhibition. Finally, we draw some conclusions based on our modeling study.

Results

Reproducing the triphasic pattern and frequency of PN responses

To understand the cellular mechanisms underlying the triphasic firing patterns ($E_1/I/E_2$) of MGC neurons in *A. ipsilon* in response to pheromone stimuli, we developed a simple biophysical MGC network model. This model (see [Methods](#)) consists of 100 Poisson ORNs connected to one PN through cholinergic synapses. The outline of the model is shown in [S1 Fig](#) and its parameter values are given in [Tables 1–4](#). Using this model we reproduced the triphasic PN response pattern to high concentration pheromone stimuli. Results are shown in [Fig 1A–1D](#). In the simulations, the stimulation onset is 5000ms and the ORN response latency is 140ms. The pheromone stimulus duration and dose are 500ms and 10ng respectively. Since the parameter values of various intrinsic currents were taken from different types of neurons, in order to produce the firing pattern shown in [Fig 1A–1D](#) we have modified the values of some parameters from the experimental data. The modified values are also shown in [Tables 2–4](#) (denoted by modified value). Comparing [Fig 1A](#) and [1C](#) shows that the spontaneous frequency of PN is higher than that of ORN; the E_1 phase in PN corresponds to the initial response of ORNs where their firing frequency is the highest; the E_2 phase in PN corresponds to the late response of ORNs where their firing rate is lower. Since the PN receives convergent inputs from 100 ORNs, the frequency of the spontaneous activity and those of E_1 and E_2 phases are higher in PN than in ORN. These results agree with the experimental findings in [\[12–13\]](#). [Fig 1B](#) and [1D](#) indicate that the I phase corresponds to the falling phase of intracellular Ca^{2+} of PN (shown by the green rectangle in [Fig 1B](#) and [1D](#)). In order to see how the intrinsic current I_A affects the PN firing pattern in [Fig 1E](#) and [1F](#), we turned off I_A . The frequency of the PN spontaneous activity and that of the second excitatory phase E_2 in [Fig 1E](#) and [1F](#) are reduced compared with [Fig 1B](#) and [1C](#). By contrast, in [Fig 1G](#) and [1H](#) we reduced the half-activation voltage $V_{0.5act}$ of I_A from -32.7 to -40.0 mV. The frequency of the second excitatory phase E_2 was significantly increased, whereas the PN spontaneous activity was further reduced. This means that the A current affects the PN firing frequency of various phases in a parameter-dependent way. We

Table 1. Parameter values of ORN model fitted to extracellular recorded data.

Dose (ng)	Period (ms)	f_{sp} (Hz)	f_{pe} (Hz)	f_{pl} (Hz)	T_{lat} (ms)	T_{d2pe} (ms)	T_{pl} (ms)	τ_{rise} (ms)	τ_{fall1} (ms)	τ_{fall2} (s)	τ_{fall3} (s)	q
0.1	200	1.5	16	—	250	150	—	180	130	20	—	0.9
1.0	200	1.5	35	—	250	115	—	128.6	170	10	—	0.9
10.0	200	1.5	154	—	150	115	—	155	115	5	—	0.9
10.0	500	1.5	125	30	140	160	330	150	40	0.2	10.5	0.72
10.0	1000	1.5	130	30	170	110	870	140	70	0.3	11.791	0.72

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Table 2. Parameter values of Ca dynamics and passive parameters of the PN model.

	Name	Value	Modified value	Reference
Passive parameters	C_m (pF)	22.9	—	[22]
	E_L (mV)	-61.4	—	[22]
	g_L (nS)	11.16 ^a	—	[22]
Parameters of Ca dynamics	f_{Ca}	1.6	1.7	[39]
	τ_{Ca} (ms)	656	2000	[39]
	Ca_{∞} (nM)	113.0	—	[39]

^aCalculated by $g_L = 1/R_M = 1/(89.6 \text{ M}\Omega) = 11.16 \text{ nS}$.

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Table 3. Parameter values of the ionic currents of the PN model given or calculated from data.

Steady-state functions of I_{Na}	\bar{g}_{Na} (nS)	$V_{0.5act}$ (mV)	S_m	$V_{0.5inact}$ (mV)	S_h	E_{Na} (mV)	Ref.
	206 modified2500	-25.8	9.32	-41.1 modified43.0	9.75	+48.2(RP)+47.9(EP)	[38]
Time constant functions of I_{Na}	$a_{\tau m,up}$	$V_{\tau m,0.5up}$ (mV)	$S_{\tau m,up}$	$a_{\tau m,dn}$	$V_{\tau m,0.5dn}$	$S_{\tau m,dn}$	Ref.
	0.5	-30	3.7	0.5	-15	13.7	Fitted
	$a_{\tau h,up}$	$V_{\tau h,0.5up}$	$S_{\tau h,up}$	$a_{\tau h,dn}$	$V_{\tau h,0.5dn}$	$S_{\tau h,dn}$	to
	2.1	-55	5	0.7	-10	11	[38]
Steady-state functions of I_{Ca}	\bar{g}_{Ca} (nS)	$V_{0.5act}$ (mV)	S_m	$V_{0.5inact}$ (mV)	S_h	E_{Ca} (mV)	Ref.
	16.1 modified45	-10.6	8.5	-29.6	8.4	160	[22]
Time constant functions of I_{Ca}	$a_{\tau m,up}$	$S_{\tau m,up}$	$a_{\tau m,dn}$	$V_{\tau m,dn}$	$S_{\tau m,dn}$	—	Ref.
	0.046	20.73	0.19	19.8	10	—	[39]
Steady-state functions of I_{sk}	a_{msk}	b_{msk}	S_{msk}	—	—	—	Ref.
	1.120	2.508	1000	—	—	—	[39]
Steady-state functions of I_{Kd}	\bar{g}_{Kd} (nS)	$V_{0.5act}$ (mV)	S_m	E_K (mV)	—	—	Ref.
	8.17 ^a modified700	-18.5	22.5 modified 20.0	-91.6	—	—	[36]
Time constant functions of I_{Kd}	$a_{\tau m,up}$	$V_{\tau m,0.5up}$	$S_{\tau m,up}$	—	—	—	Ref.
	0.125	-40	11.0	—	—	—	Fitted
	$a_{\tau m,dn}$	$V_{\tau m,0.5dn}$	$S_{\tau m,dn}$	—	—	—	to
	0.15	25	45.7	—	—	—	[37]
Steady-state functions of I_A	\bar{g}_A (nS)	$V_{0.5act}$ (mV)	S_m	$V_{0.5inact}$ (mV)	S_h	E_K (mV)	Ref.
	17.35 ^b modified 500	-32.69	17.5	-53.3	7.23	-91.6	[36]
Time constant functions of I_A	$a_{\tau m,up}$	$V_{\tau m,0.5up}$	$S_{\tau m,up}$	$a_{\tau m,dn}$	$V_{\tau m,0.5dn}$	$S_{\tau m,dn}$	Ref.
	0.5	-30	13.7	0.42	-15	46	Fitted
	$a_{\tau h,up}$	$V_{\tau h,0.5up}$	$S_{\tau h,up}$	$a_{\tau h,dn}$	$V_{\tau h,0.5dn}$	$S_{\tau h,dn}$	to
	0.04	-55	25	0.045	40	55	[37]

^{a,b}Calculated from Kloppenburg et al.,1999.

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Table 4. Parameter values of nACh synaptic current.

Name	\bar{g}_{nACh} (μ S)	E_{nACh} (mV)	α (ms^{-1})	β (ms^{-1})	A	t_{max} (ms)
Value	0.3	0.0	10	0.2	0.5	0.3
Reference	[28]	[28]	[28]	[28]	[28]	[28]
Modified value	0.017	—	—	2.0	0.8	—

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further checked the influence of I_{Ca} on the firing pattern. We found that decreasing \bar{g}_{Ca} , on the one hand, enhances the firing frequency during spontaneous activity, as well as the E_1 and E_2 phases; on the other hand, it decreases the duration of the I phase. One of the results is shown in Fig 1I and 1J. In the subsection “Effects of intrinsic PN parameters on the response characteristics”, the influence of PN intrinsic currents is detailed.

In order to further reveal the mechanisms underlying the generation of the $E_1/I/E_2$ pattern, we analyzed the PN depolarizing and repolarizing currents in our simulation (Fig 1A–1D). Employing the low-pass (cut-off frequency: 5Hz) and high-pass (cut-off frequency: 5Hz) Butterworth filters (see Methods), we extracted the slow and fast components of the depolarizing currents I_{nACh} , I_{Na} , I_{Ca} and the repolarizing currents I_{SK} , I_A and I_{Kd} (Fig 2). During E_1 and I, the kinetics of the slow component of the repolarizing Ca^{2+} -dependent K^+ current I_{SK} are similar to those of the depolarizing synaptic current I_{nACh} (Fig 2A). Similarly, during E_1 , the kinetics of the slow components of I_A and I_{Kd} are similar to those of the I_{Na} and I_{Ca} , respectively (Fig 2C and

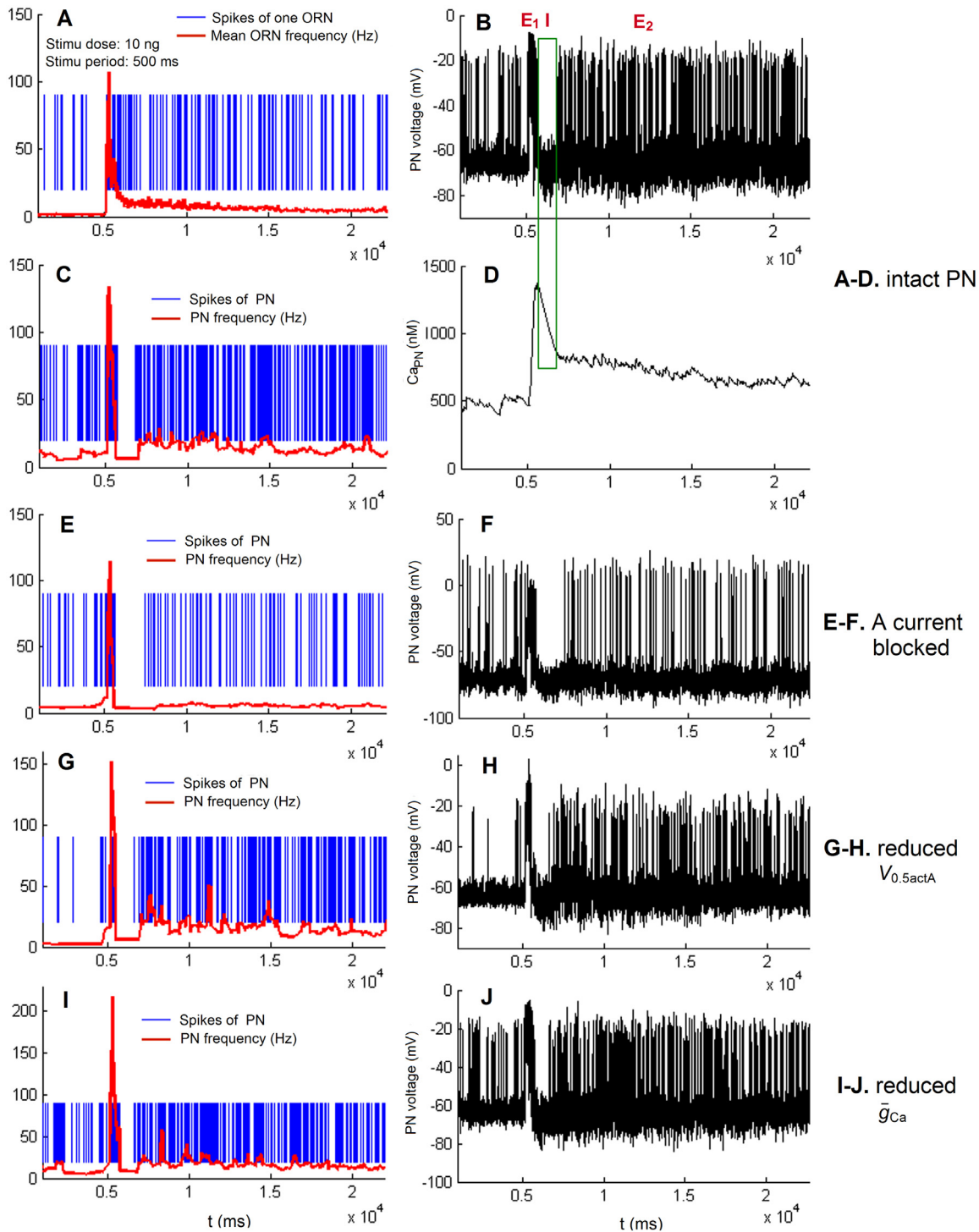


Fig 1. Triphasic response pattern reproduced by the MGC model in response to a pheromone stimulus (500 ms, 10ng). In the results shown in A to D, for most parameters in Eqs (4–14), we used the original values from literature given in Tables 2–4 except for some values that were modified (modified values in Tables 2–4). A. Spikes of one ORN (blue lines) and mean firing frequency curve of ORNs (red line). B. Dynamics of the PN membrane potential V . C. Spikes of the PN (blue lines) and PN firing frequency (red line). D. Kinetics of intracellular Ca^{2+} concentration of the PN. E. Spikes of the PN (blue lines) and PN firing frequency (red line) ($\bar{g}_A = 0 \mu S$, $\bar{g}_{Ca} = 0.045 \mu S$). F. Dynamics of the PN membrane potential V ($\bar{g}_A = 0 \mu S$, $\bar{g}_{Ca} = 0.045 \mu S$). G. Spikes of the PN (blue lines) and PN firing frequency (red line) ($\bar{g}_A = 0.5 \mu S$, $V_{0.5actA} = -40.0$ mV, $\bar{g}_{Ca} = 0.045 \mu S$). H. Dynamics of the PN membrane potential V ($\bar{g}_A = 0.5 \mu S$, $V_{0.5actA} = -40.0$ mV, $\bar{g}_{Ca} = 0.045 \mu S$). I. Spikes of the PN (blue lines) and PN firing frequency (red line) ($\bar{g}_A = 0.5 \mu S$, $V_{0.5actA} = -37.0$ mV, $\bar{g}_{Ca} = 0.035 \mu S$). J. Dynamics of the PN membrane potential V ($\bar{g}_A = 0.5 \mu S$, $V_{0.5actA} = -37.0$ mV, $\bar{g}_{Ca} = 0.035 \mu S$).

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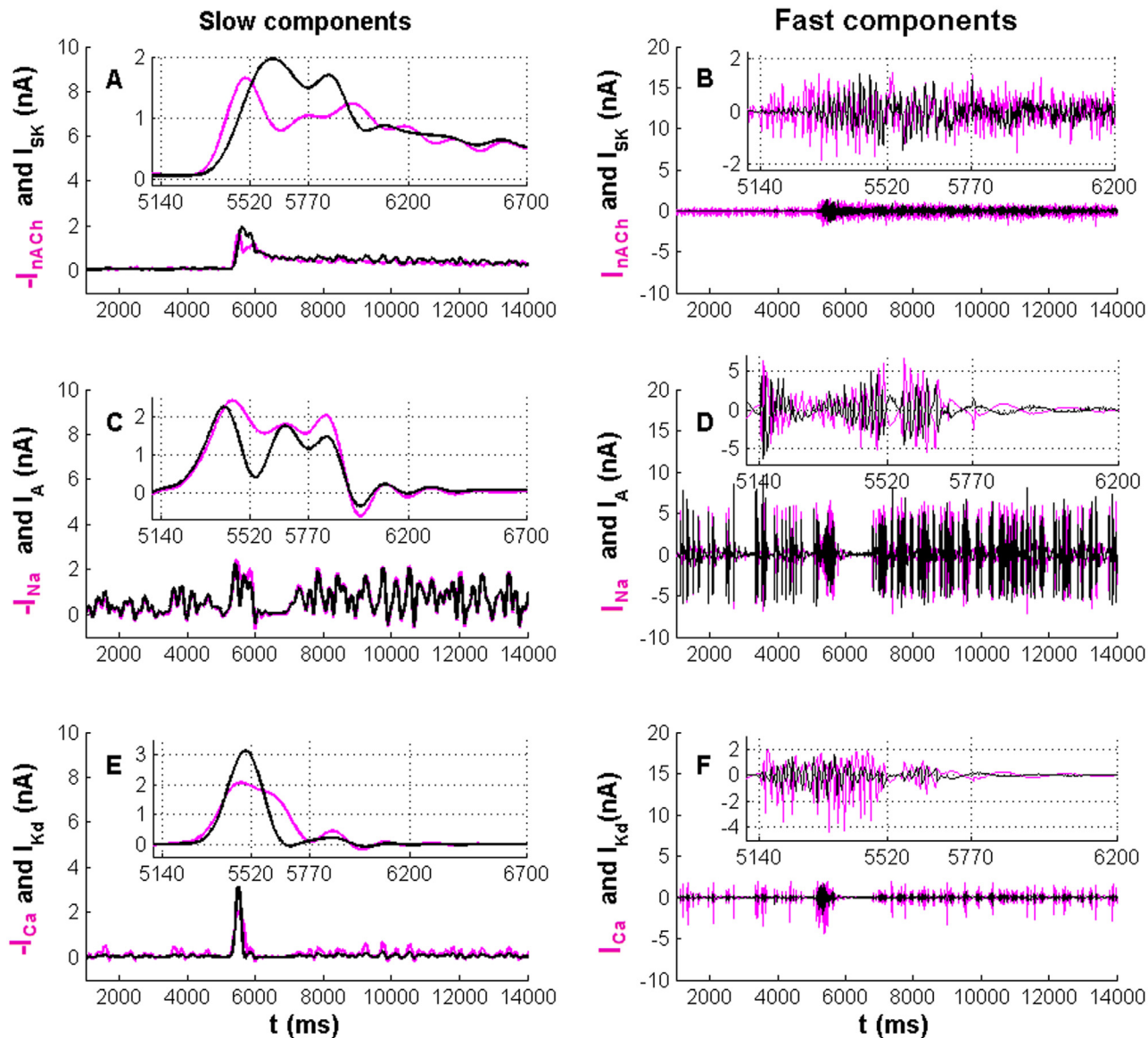


Fig 2. Synaptic and intrinsic currents in a PN from the simulation results shown in Fig 1. Left panel: the slow components of the repolarizing currents (black lines) and depolarizing currents (magenta lines); I_{SK} and $-I_{nACh}$ (A), I_A and $-I_{Na}$ (C) and I_{Kd} and $-I_{Ca}$ (E). Right panel: Fast components of the repolarizing (black lines) and depolarizing currents (magenta lines); I_{SK} and I_{nACh} (B), I_A and I_{Na} (D) and I_{Kd} and I_{Ca} (F). Note that in the left panel we draw the minus values of I_{nACh} , I_{Na} , I_{Ca} for comparing their amplitudes, while in the right panel we draw the values of I_{nACh} , I_{Na} , I_{Ca} directly for comparing their depolarizing and repolarizing effects). The slow components of E_1 (from 5140 to 5770ms) and I (from 5770 to 6700ms) are enlarged in the insets in A, C and E; and the fast components of E_1 and the period transiting from E_1 to I (from 5770 to 6200ms) are enlarged in the insets in B, D and F.

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2E). In the beginning of E_1 (from 5140 to 5520ms) the amplitudes of the slow and fast components of the depolarizing synaptic current I_{nACh} from ORNs are higher than those of the repolarizing current I_{SK} (insets in Fig 2A and 2B). With depolarization I_{SK} increases because of the accumulation of intracellular Ca^{2+} . At 5520ms the amplitude of the slow component of I_{SK} exceeds that of I_{nACh} (inset in Fig 2A). From 5520ms onwards I_{SK} competes with I_{nACh} and slows down the PN firing. At 5770ms the PN stops spiking and transits to the I phase. During I, I_{SK} flows out against I_{nACh} to create a hyperpolarization phase until the intracellular Ca^{2+} concentration falls. During this hyperpolarization phase, the voltage-gated currents (I_A , I_{Kd} , I_{Na} and I_{Ca})

cannot be activated due to the low membrane potential (Fig 2C–2F). Interestingly, both the slow and fast components of I_A have the same kinetics as I_{Na} and the amplitude of I_A is slightly smaller than that of I_{Na} , especially during E_1 and E_2 phases (Fig 2C and 2D and the insets). Whenever I_{Na} depolarizes the membrane to make a spike, I_A flows out and repolarizes the membrane, so that the amplitude of each spike is reduced and the firing frequency is increased.

Effects of the pheromone stimulus parameters on the response characteristics

To see how the stimulation parameters affect the PN response characteristics (such as duration and frequency) whose calculation is described in Methods section, we varied the concentration and duration of the pheromone pulses. For each parameter value, the computer simulation was repeated ten times and the mean and standard deviation of the response characteristics were calculated over the ten trials. The results are shown in Fig 3. The parameter values are the same as those in Fig 1A–1D). The duration of E_1 nearly linearly increases with the stimulus duration and the duration of I for 200ms stimulus duration is slightly lower than that for 500 and 1000ms stimulus duration (Fig 3A). The mean response frequency of E_1 decreases with stimulus duration (this is due to frequency adaptation during E_1) (Fig 3B). E_1 and I durations are independent of stimulation doses (Fig 3C). These relationships between E_1 duration and stimulation duration and dose agree with the experimental findings described in [12]. The mean response frequency of E_1 increases with stimulus concentration while that of E_2 does not (Fig 3D).

Effects of intrinsic PN parameters on the response characteristics

We examined how the intracellular Ca^{2+} dynamics and intrinsic currents in the PN affect its dynamic response characteristics. To this end we varied the value of each parameter from low to high in a range while keeping the values of other parameters the same as in Fig 1A–1D. At a given value of each parameter the computer simulation was repeated ten times and the mean and standard deviation of each response characteristics were calculated over the ten trials.

Effects of Ca^{2+} dynamics, I_{Ca} and I_{SK} . The simulation results indicate that the inhibitory phase following E_1 is generated by the slow component of the repolarizing current I_{SK} that exceeds the slow component of the depolarizing synaptic current I_{nACh} . I_{SK} depends on Ca^{2+} concentration which in turn depends on I_{Ca} . In addition, I_{Ca} also affects the triphasic response pattern (Fig 1I–1J). Therefore we further analyzed the effects of the parameters of the Ca^{2+} dynamics, I_{Ca} and I_{SK} on the PN response characteristics. Fig 4 shows that the duration of the E_1 phase exponentially decreases with \bar{g}_{SK} (A) while the duration of the I phase linearly increases with \bar{g}_{Ca} (C) and τ_{Ca} (E). The mean frequency of the E_1 phase linearly decreases with \bar{g}_{Ca} (D) and that of the E_2 phase exponentially decreases with \bar{g}_{Ca} (D) and τ_{Ca} (F). Some parameters for the steady-state activation m_∞ , the time constant τ_m of I_{Ca} and for the steady-state function of the gating variable $m_{sk\infty}$ of I_{SK} have also clear influences on the PN response duration, especially the duration of the I phase. These effects are illustrated in S2 Fig. The I duration decreases with $a_{\tau m, up}$ and S_{msk} while it increases with $S_{\tau m, up}$ and a_{msk} .

Effects of I_{Na} , I_A and I_{kd} . In this section, by varying the parameter values of I_{Na} , I_{kd} and I_A , we quantitatively investigated how the PN response characteristics depend on these parameters. The major influences of I_{Na} on the response characteristics are illustrated in Fig 5. The maximal conductance and parameters for steady-state activation and inactivation function of I_{Na} strongly affect the response frequency of E_1 phase: E_1 frequency increases with the half-activation parameter $V_{0.5act}$ (Fig 5D) and decreases with \bar{g}_{Na} (Fig 5B) and the slope factor S_h (Fig 5H); both E_1 and E_2 frequencies increase with the slope factor S_m (Fig 5F). Parameters $V_{0.5act}$, S_m and S_h of I_{Na} have also some influences on E_1 and I duration (Fig 5C, 5E and 5G). Other parameters of I_{Na}

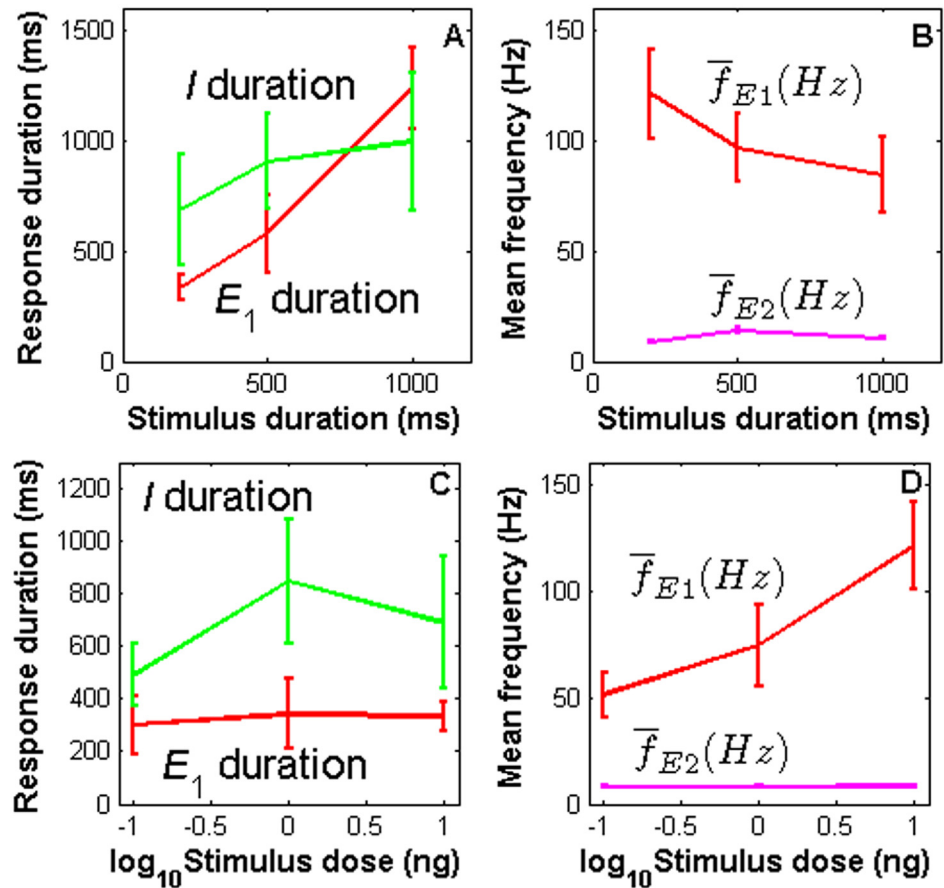


Fig 3. Effects of stimulation parameters on PN response characteristics. Top panel: effects of stimulus duration on E₁ and I duration (A) and mean firing frequency of E₁ and E₂ (B). Bottom panel: effects of stimulus concentration on E₁ and I durations (C) and mean firing frequency of E₁ and E₂ phases (D).

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affect one or two PN response characteristics as shown in S3 Fig. I_{Kd} has also some influences on the PN response characteristics as shown in S4 Fig. As illustrated in Fig 1 the transient potassium current I_A affects the firing frequency of E₁, E₂. Here we further investigated the influences of I_A . We found that the mean maximal conductance, the half activation, and the slope factor S_m of I_A have strong effects on PN response frequency. Increasing the maximal mean conductance \bar{g}_A and decreasing the voltage of half activation $V_{0.5act}$ and the slope factor S_m increase the mean firing frequency of both E₁ and E₂ phases (Fig 6B, 6D and 6F). The increased frequency of spontaneous activity of the PN is also due to the higher conductance and lower voltage of half activation and smaller slope factor s_m of this current (data not shown). In addition, increasing \bar{g}_A has a small effect of decreasing the duration of the I phase at low \bar{g}_A values (Fig 6A); increasing $V_{0.5act}$ clearly decreases the duration of the I phase and increases the duration of the E₁ phase (Fig 6C). Moreover, decreasing S_m clearly decreases I duration whereas increases E₁ duration. Some parameters in time constant functions of I_A have slight influences on PN response characteristics (data not shown): I duration increases with $a_{\tau m \uparrow}$, $a_{\tau h \downarrow}$ and $V_{\tau m \uparrow 0.5 \downarrow}$ when it is less than -10 mV while decreases with $S_{\tau m \uparrow}$, $a_{\tau h \uparrow}$ and $V_{\tau h \uparrow 0.5 \downarrow}$ when it is less than -40 mV; E₁ duration decreases with $a_{\tau m \uparrow}$ and E₁ frequency decreases with $V_{\tau m \uparrow 0.5 \uparrow}$, $S_{\tau m \downarrow}$, $a_{\tau h \uparrow}$, $S_{\tau h \uparrow}$ and $a_{\tau h \downarrow}$; E₂ frequency increases with $S_{\tau m \uparrow}$ and $a_{\tau m \downarrow}$ when it is less than 0.7.

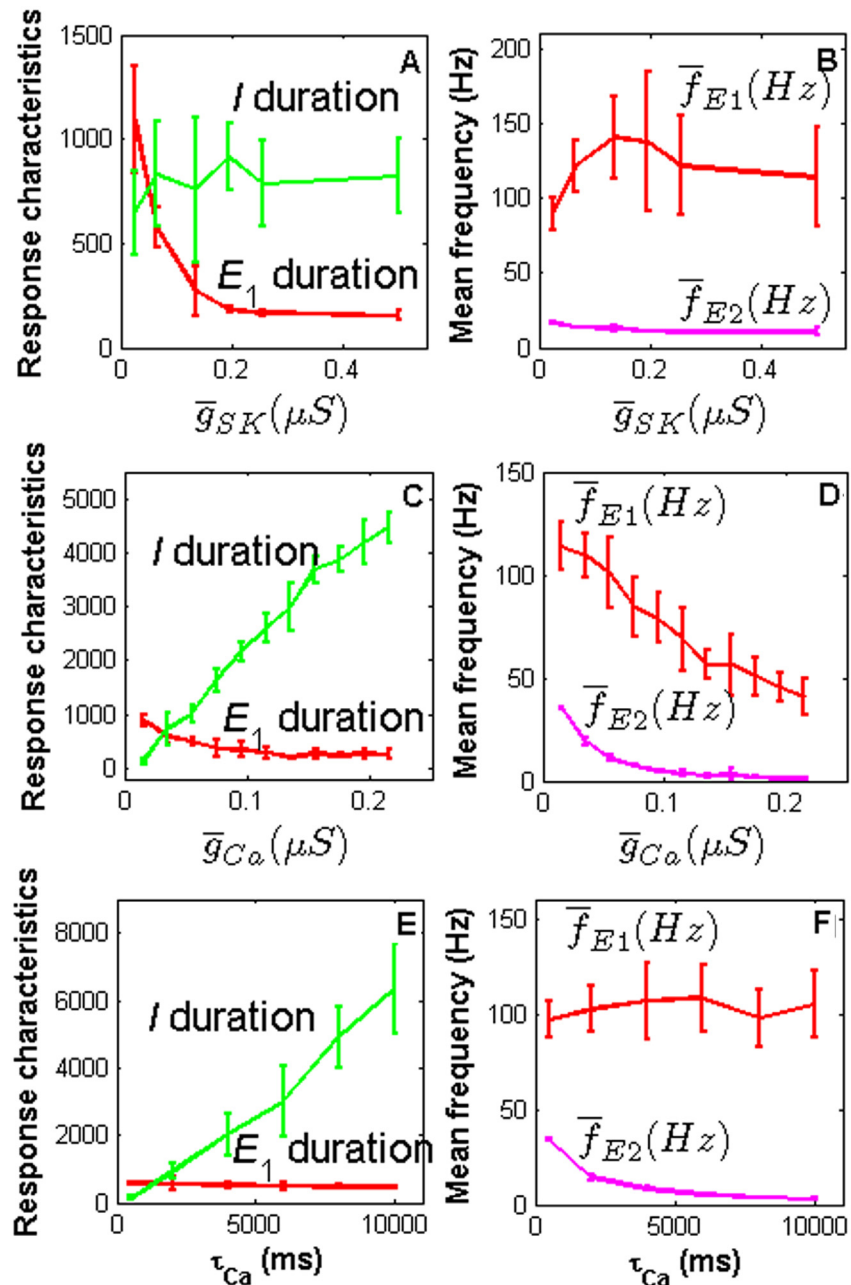


Fig 4. Effects of I_{Ca} , I_{SK} and dynamics of intracellular Ca^{2+} on PN response characteristics. Top panel: effects of the mean maximal conductance \bar{g}_{SK} of I_{SK} on E_1 and I durations (A) and mean firing frequency of E_1 and E_2 (B). Intermediate panel: effects of the mean maximal conductance \bar{g}_{Ca} of I_{Ca} on E_1 and I duration (C) and mean firing frequency of E_1 and E_2 (D). Bottom panel: effects of time constant τ_{Ca} of Ca^{2+} dynamics on E_1 and I duration (E) and mean firing frequency of E_1 and E_2 phases (F).

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Effect of nACh synaptic parameters on PN firing patterns

In the presence or absence of pheromone stimulation, PN dendrites receive feedforward cholinergic synaptic inputs from ORNs through nicotinic receptors. Hence, the nACh synaptic currents are the stimulation inputs of PNs. We studied how the parameters of I_{nACh} affect the PN response characteristics.

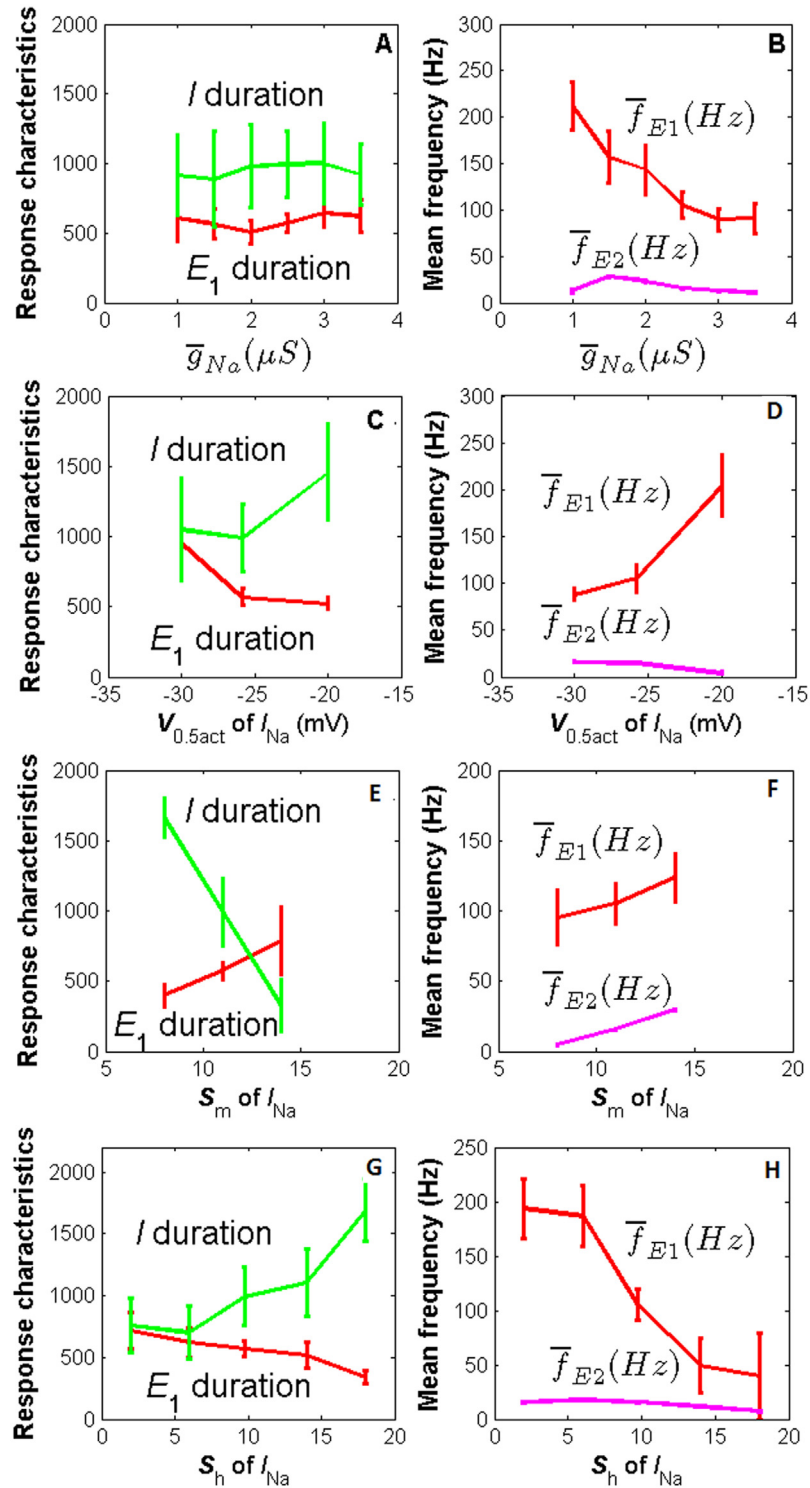


Fig 5. Major effects of I_{Na} on PN response characteristics. Effects of \bar{g}_{Na} , $V_{0.5act}$, S_m and S_h on E₁ and I duration (left panel) and mean firing frequency of E₁ and E₂ (right panel).

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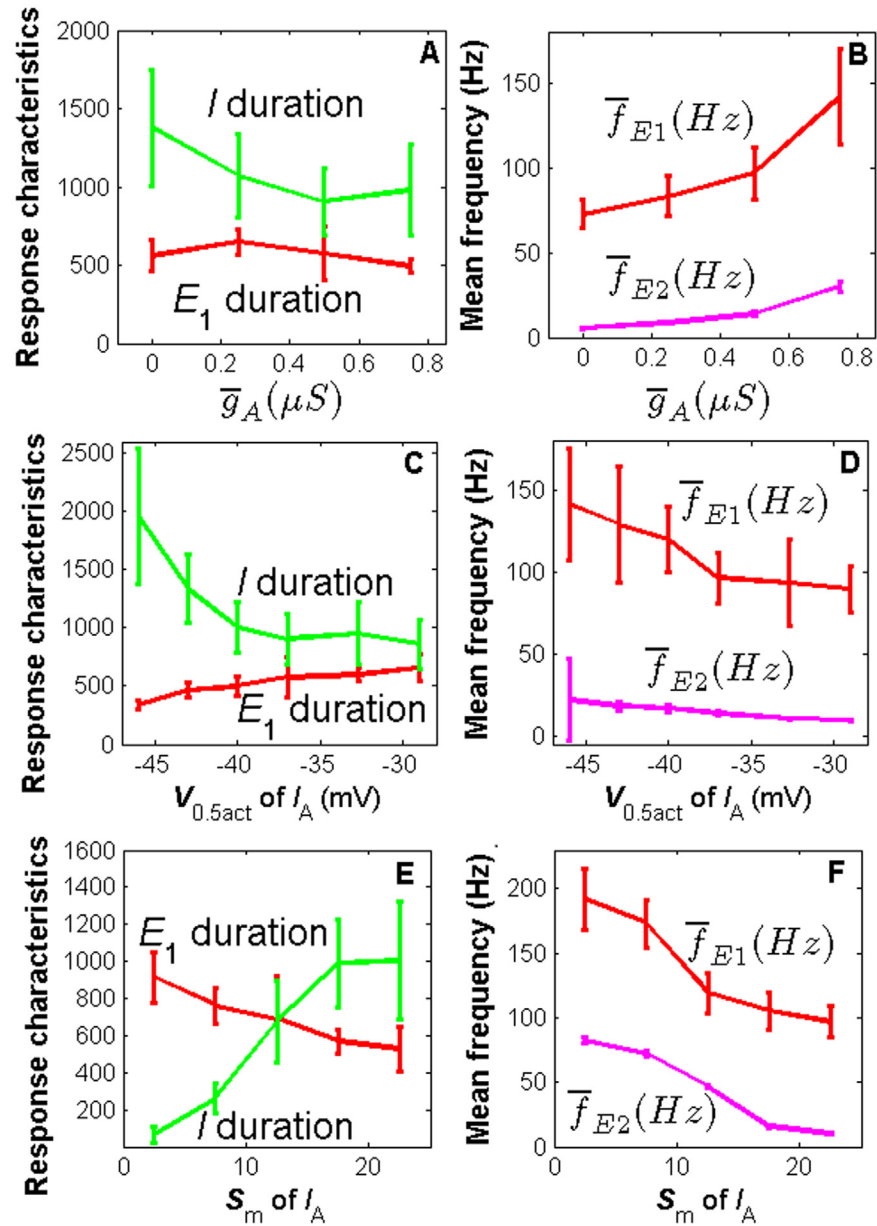


Fig 6. Major effects of I_A on PN response characteristics. Top panel: effects of \bar{g}_A on E_1 and I duration (A) and mean firing frequency of E_1 and E_2 (B). Intermediate panel: effects of $V_{0.5act}$ on E_1 and I duration (C) and mean firing frequency of E_1 and E_2 phases (D). Bottom panel: effects of S_m on E_1 and I duration (E) and mean firing frequency of E_1 and E_2 phases (F).

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First, the effects of presynaptic ACh transmitter delivered as square pulses of duration t_{max} and concentration A were investigated (S5 Fig). E_1 duration increases while I duration decreases with Ach pulse duration t_{max} (S5A Fig). The mean frequency of the E_2 phase \bar{f}_{E2} significantly increases with t_{max} , whereas the influence of this parameter on the average frequency of the E_1 phase \bar{f}_{E1} is not monotonic (S5B Fig). This result is interesting because this parameter has a different effect on the average frequency of the E_1 and E_2 phases. The \bar{f}_{E1} increases at values of t_{max} smaller than 0.3ms then decreases with t_{max} . This is due to the fact that the firing frequency adaptation induced by SK currents takes effect when the E_1 duration increases with

t_{\max} . The ACh concentration parameter A has a very different effect on the duration of E_1 and I phase and the average frequency of E_1 phase \bar{f}_{E_1} . The duration of E_1 phase increases and that of I phase decreases with A when A is less than 1, then the duration of E_1 and I phases reaches saturation (S5C Fig). The clearest effect of A is that it can significantly increase the average frequency of E_1 phase \bar{f}_{E_1} (S5D Fig).

Second, we investigated the effects of the opening and closing rates of nACh postsynaptic channels on PN response characteristics (S6A–S6D Fig). Increasing the opening rate α slightly increases E_1 duration and decreases I duration (S6A Fig) and significantly increases the mean frequency of E_2 phase (S6B Fig purple line). Increasing the closing rate β has exactly opposite effects (S6C and S6D Fig purple line). Interestingly, increasing α and β has the same clear effect of increasing the average frequency of the E_1 phase (S6B and S6D Fig red lines). The increasing effect of β on \bar{f}_{E_1} can be explained by its decreasing effect on E_1 duration. When the value of β is small, the E_1 duration is quite long (S6C Fig). Thus the frequency adaptation mediated by SK currents is strong. As a result of frequency adaptation, the mean frequency of E_1 phase is low.

Finally, the effects of the mean maximal conductance \bar{g}_{nACh} on PN response characteristics were studied. Increasing \bar{g}_{nACh} clearly increases the duration of the E_1 phase and strongly decreases that of the I phase (S6E Fig) and significantly increases the mean frequency of both phases (S6F Fig).

Exploring possible effects of LNs on PN response patterns

In order to investigate possible network mechanisms, particularly the influences from LNs we have developed a model of type I LNs (LNIs), that generate Na^+ -driven action potentials [22–23]. The mathematical description of the LNI model and its parameter values are given in S1 Text. We have done some exploratory simulations by connecting 80 ORNs and 20 LNI with one PN. The LNI receives inputs from ORNs and PN through fast nicotinic cholinergic synapses, while the PN receives fast nicotinic cholinergic synaptic inputs from ORNs and fast GABAergic inhibitory inputs from LNI mediated by GABA_A receptors or slow GABAergic inhibitory inputs from LNI mediated by metabotropic GABA_B receptors. Preliminary results revealed that the synaptic interactions between PN and LNI affect the synchronization among the PN and LNI, PN response pattern and PN response characteristics. Synchronization and I duration changes with fast GABAergic inhibition. S7 Fig qualitatively shows how the closing rate β of the GABA_A synaptic currents from LNI to PN affects the response characteristics and synchronization. Decreasing β decreases the synchronization of PN and LNI and also decreases the duration of I phase. As for the influence of slow GABAergic inhibition, we found that in the parameter range of the slow GABAergic inhibition given in S1 Text (Eq S3) the PN maintained the triphasic response pattern (S8A Fig). Decreasing the rate parameter r_3 in Eq S3 prolonged the I duration (S8E Fig). In these cases the rising kinetics of G protein concentration is close to that of the intracellular Ca^{2+} concentration in PN (S8C and S8F Fig). The LNI showed synchronized triphasic response pattern (S8B and S8D Fig). When increasing r_3 and decreasing r_4 in Eq S3 the rising kinetics of GABA_B receptor-coupled G protein concentration became faster than that of the intracellular Ca^{2+} concentration in PN. In this case the E_1 phase of PN may become an I phase (data not shown) or terminate early due to the GABAergic inhibition (S8G Fig). The shortened or disappeared E_1 is at odds with the experimental findings in [12] and S9 Fig showing that the E_1 duration lasts approximately as long as the stimulus and increases with the duration of pheromone stimuli. After an I phase, another excitatory phase appeared (S8G Fig) which corresponds to the rising period of intracellular Ca^{2+} concentration (S8H Fig). The second excitatory phase in turn is followed by another short I phase corresponding to the early falling phase of Ca^{2+} concentration. After the short I phase, the late excitatory phase of PN appeared.

Discussion

In this work, using a simple MGC model with ORNs based on the recorded frequency curves under different pheromone stimuli, PN based on patch-clamp data from PN and other neurons and a biophysical model of nACh synapses, we reproduced the triphasic response pattern of PNs at high pheromone stimulation concentrations. We investigated mechanisms generating this triphasic response pattern. Our results show that it can be shaped by intrinsic mechanisms in ORNs and PNs: in our model Ca^{2+} -dependent SK current in PN is responsible for the I phase following the E_1 phase and the E_2 phase is due to the long-lasting excitatory response of ORNs. We further investigated how the external stimulation parameters and the parameters of the internal ionic currents in PN and the nACh synaptic currents from ORNs to PN affect the duration of E_1 and I, the firing frequency of E_1 and E_2 and other response characteristics of PN. In our model E_1 duration significantly increases with stimulation duration. The ending time of E_1 clearly depends on parameters: \bar{g}_{SK} ; \bar{g}_{Ca} ; $V_{0.5\text{act}}$, S_m and S_h of I_{Na} ; t_{max} , A , β and \bar{g}_{nACh} of I_{nACh} . The external stimulation parameters have no significant influence on I duration. This implies that I phase is an intrinsic property of the network. Our results revealed that I duration linearly increases with the time constant of intracellular Ca^{2+} (τ_{Ca}) and \bar{g}_{Ca} , decreases with t_{max} and \bar{g}_{nACh} of I_{nACh} . I duration is also influenced by some other parameters such as S_m , $S_{\text{tm,up}}$ of I_{Na} ; $a_{\text{tm,up}}$, $S_{\text{tm,up}}$ of I_{Ca} ; a_{msk} and S_{msk} of I_{SK} ; \bar{g}_A and $V_{0.5\text{act}}$ of I_A ; and the concentration of the pulse of ACh transmitter delivered. The mean firing frequency of E_1 phase \bar{f}_{E_1} increases with stimulation concentration and decreases with stimulation duration. \bar{f}_{E_1} and \bar{f}_{E_2} are also strongly affected by some intrinsic parameters. Both of \bar{f}_{E_1} and \bar{f}_{E_2} increase with S_m of I_{Na} . \bar{f}_{E_1} increases with $V_{0.5\text{act}}$ of I_{Na} ; \bar{g}_A ; \bar{g}_{nACh} , A , α and β of I_{nACh} ; while decreases with \bar{g}_{Na} , S_h and $V_{0.5\text{inact}}$ of I_{Na} ; $V_{0.5\text{act}}$ and S_m of I_{Kd} ; \bar{g}_{Ca} ; and $V_{0.5\text{act}}$ of I_A . Besides, \bar{g}_{SK} and t_{max} have non monotonic effects on \bar{f}_{E_1} . \bar{f}_{E_2} increases with \bar{g}_A , t_{max} , A , α and \bar{g}_{nACh} , while it decreases with \bar{g}_{Ca} , τ_{Ca} and β .

The aim of this study is to show that it is possible to explain the triphasic PN responses with intrinsic mechanisms only (and realistic parameter values) without denying the possible implication of extrinsic mechanisms and influences. We have also explored possible network effects on the PN response characteristics, particularly the influences from LNs. Preliminary results show that I duration and synchronization between PN and LNs change with GABAergic inhibition. Slow GABAergic inhibition does not affect the triphasic PN response pattern in the parameter range given in [S1](#) and [S2](#) Texts. When the rising kinetics of GABA_B receptor-coupled G protein concentration became faster than that of the intracellular Ca^{2+} concentration in PN, GABA_B mediated inhibition may change the triphasic pattern and result in a much reduced E_1 duration which is at odds with the experimental data. This might indicate that in the MGC of *A. ipsilon* moths if GABA_B receptor mediated slow inhibitory synapses exist GABA_B receptor may couple to Ca^{2+} activated SK channel via G protein as reviewed in [\[41\]](#). Previously we have found that applying bicuculline (BIC), an antagonist of GABA_A and a SK channel blocker, to *A. ipsilon* moths abolished the inhibitory phase in all tested neurons [\[21\]](#). However, applying picrotoxin (PTX), another GABA_A antagonist, to *A. ipsilon* led to different effects. This experimental result together with our modeling results indicate that the Ca^{2+} -activated SK channel is likely responsible for the generation of I phase while interactions between LNs and PNs might affect the PN response characteristics. These are very preliminary qualitative results showing the influences of LNs on PN response pattern. The network structure of MGC may also affect the PN response characteristics. Further experimental and modeling investigations are needed to study how the intrinsic property of LNs, various synaptic mechanisms and network structure of MGC affect PN response. Besides, the functional roles of PN response patterns in the dynamical representation, classification and discrimination of pheromone stimuli and in guiding the moths tracking in turbulent and intermittent pheromone plumes to be elucidated.

In conclusion, our modeling study revealed that I_{SK} and the long-lasting excitatory response of ORNs can be intrinsic mechanisms for the generation of triphasic response patterns of pheromone-sensitive PN. The parameters of Ca^{2+} , nACh synaptic, Na^+ and A currents have strong influence on the response patterns and the response characteristics. Preliminary results show that network interactions between PN and LNIs can also affect the PN response. Although SK channels can be responsible for the generations of I phase, parameters of I_{Ca} , I_{Na} and I_A , as well as the synaptic currents can also affect the I phase. Therefore, experimentally blockers that affect any of these parameters might block the I phase.

Methods

Based on various experimental findings (see [S2 text](#), Experimental findings in ORNs and PNs), we developed models of ORN and PN and of the MGC neural network. The model parameters were fitted to the experimental data.

The Poisson model of ORNs

To construct the Poisson model of ORNs, we fitted the extracellular recorded data [12] about the rise and fall of the mean instantaneous response frequency as a function of time following different concentrations and durations of the pheromone stimulus. At any concentration the rising phase of the frequency curve can be fitted by a single exponential function. However, the dynamics of the falling phase depend on the stimulation parameters. For short stimulation periods of 100 and 200 ms at any concentration, the falling phase can be fitted by the sum of two exponential functions, one fast with a small time constant τ_{fall1} and one slow with a larger time constant τ_{fall2} as shown in [Fig 7A](#). The fitting function used in this case is given by [Eq 1](#). The fitted curves are shown in [Fig 7B](#) and the blue (stimulation period: 100 ms, stimulation dose: 10 ng) and purple curves (stimulation period: 200 ms, stimulation dose: 10 ng) in [Fig 7D](#). The fitted falling time constants decrease with pheromone concentration ([Table 1](#)). For stimulation concentration at 10 ng with long stimulation periods of 500 ms and 1000 ms, the falling phase of frequency undergoes two stages: a rapid falling stage to a plateau and a slow falling stage. The rapid falling stage can be fitted by one exponential function with a small time constant τ_{fall1} and the slow falling stage can be fitted by two exponential functions with one intermediate time constant τ_{fall2} and one larger time constant τ_{fall3} as shown in [Fig 7C](#). The fitting function used in this case is given by [Eq 2](#). The fitted curves are shown by the green and red curves in [Fig 7D](#). The fitted parameter values of [Eqs 1](#) and [2](#) are given in [Table 1](#).

$$\bar{f}(t) = \begin{cases} f_{sp}, & \text{if } t \leq t_{sti} + T_{lat} \\ f_{sp} + (f_{pe} - f_{sp}) \cdot \left(1 - e^{-\frac{t - t_{sti} - T_{lat}}{\tau_{rise}}}\right), & \text{else if } (t_{sti} + T_{lat}) \leq t \leq t_{sti} + T_{lat} + T_{d2pe} \\ f_{sp} + (f_{pe} - f_{sp}) \cdot \left(1 - e^{-\frac{T_{d2pe}}{\tau_{rise}}}\right) \cdot \left(qe^{-\frac{t - (t_{sti} + T_{lat} + T_{d2pe})}{\tau_{fall1}}} + (1 - q)e^{-\frac{t - (t_{sti} + T_{lat} + T_{d2pe})}{\tau_{fall2}}}\right), & \text{otherwise} \end{cases} \quad (1)$$

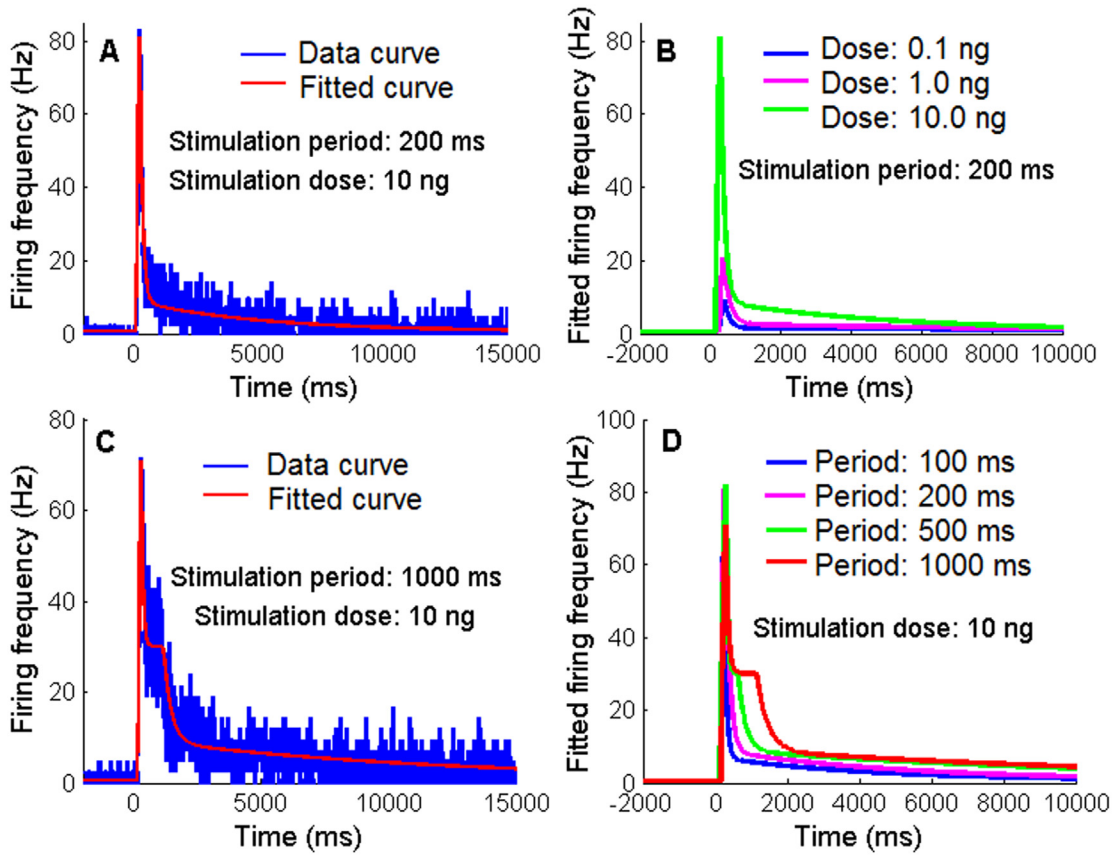


Fig 7. Mean frequency response curves of the ORN population in response to different concentrations and durations of the pheromone stimulation. A. Response data curve (blue) and fitted curve (red) to stimulus: 10 ng and 200 ms. B. Fitted response curves to the same stimulation period 200 ms and different stimulation doses from 0.1 to 10 ng. C. Response data curve (blue) and fitted curve (red) to stimulus: 10 ng and 1000 ms. D. Fitted response curves to the same stimulation dose 10 ng and different stimulation periods from 100 to 1000 ms.

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$$\bar{f}(t) = \begin{cases} f_{sp}, & \text{if } t \leq t_{sti} + T_{lat} \\ f_{sp} + (f_{pe} - f_{sp}) \cdot \left(1 - e^{-\frac{t - t_{sti} - T_{lat}}{\tau_{rise}}} \right), & \text{else if } (t_{sti} + T_{lat}) \leq t \leq t_{pe} \\ f_{pl} + \left(f_{sp} + (f_{pe} - f_{sp}) \cdot \left(1 - e^{-\frac{T_{d2pe}}{\tau_{rise}}} \right) - f_{pl} \right) e^{-\frac{t - (t_{sti} + T_{lat} + T_{d2pe})}{\tau_{fall1}}}, & \\ f_{sp} + (f_{pl} - f_{sp}) \cdot \left(qe^{-\frac{t - (t_{sti} + T_{lat} + T_{d2pe} + T_{pl})}{\tau_{fall2}}} + (1 - q)e^{-\frac{t - (t_{sti} + T_{lat} + T_{d2pe} + T_{pl})}{\tau_{fall3}}} \right), & \text{otherwise} \end{cases} \quad (2)$$

where, f_{sp} , f_{pe} and f_{pl} are the mean spontaneous frequency of the ORN, peak frequency and plateau frequency in response to stimulation; t_{sti} the time of stimulation onset; T_{lat} , T_{d2pe} and T_{pl} the response latency of the ORN population, the duration to peak frequency from $t_{sti} + T_{lat}$ and duration of the plateau; τ_{rise} , τ_{fall1} , τ_{fall2} and τ_{fall3} the rising and falling time constants respectively; q coefficient of the fast falling component.

We modelled the ORN spike train by a Poisson process characterized by a single parameter, the mean firing rate $\bar{f}(t)$ given by Eqs (1) and (2). For sufficiently short interval δt , and a mean frequency $\bar{f}(t)$ varying slowly with respect to δt , the probability of a spike occurring during δt is equal to the value of the instantaneous firing frequency during this time interval times the length of the interval

$$P\{1 \text{ spike during } \delta t\} \approx \bar{f}(t) \cdot \delta t. \tag{3}$$

At iteration time t , a random number $R[t]$, uniformly distributed between 0 and 1 is generated. If $R[t] \leq \bar{f}(t) \cdot \delta t$ where δt is the time step used in simulations, the membrane potential of ORNs is set to $V_{ORNS} = 50 \text{ mV}$. Otherwise, $V_{ORNS} = -62 \text{ mV}$ (resting potential).

The biophysical model of PN

The model is mathematically described by Hodgkin—Huxley type equations (Eqs (4–14)). The membrane activity of PN satisfies the following differential equation:

$$C_m \frac{dV}{dt} = -I_{Na} - I_{Ca} - I_{Kd} - g_L(V - E_L) - I_A - I_{SK} - I_{nAch}, \tag{4}$$

where V is the membrane potential, C_m the membrane capacitance, g_L and E_L the conductance and reversal potential of the leak current, respectively. The values of these passive parameters are given in Table 2.

The intrinsic currents of PN. The intrinsic inward (I_{Na} and I_{Ca}) and outward (I_A , I_{Kd} and I_{SK}) ionic currents in PN are described by

$$I_j = \bar{g}_j m^M h^N (V - E_j), \tag{5}$$

where \bar{g}_j and E_j are the maximal mean conductance and reversal potential for the ionic current j . The values of these two parameters of each current are given in Table 3. $M = 3$, $N = 1$ for I_{Na} and I_A ; $M = 1$, $N = 1$ for I_{Ca} ; $M = 3$, $N = 0$ for I_{Kd} ; $M = 2$, $N = 0$ for I_{SK} . The gating variables m and h in Eq (5) satisfy Eqs (6) and (7) except that $h = h_\infty$ for I_{Ca} .

$$\dot{m} = (m_\infty - m) / \tau_m, \tag{6}$$

$$\dot{h} = (h_\infty - h) / \tau_h, \tag{7}$$

where the steady-state activation m_∞ and inactivation h_∞ of the voltage-activated currents are described by Boltzmann equations as Eqs (8) and (9)

$$m_\infty = 1 / \{1 + \exp[(V_{0.5act} - V) / S_m]\}, \tag{8}$$

$$h_\infty = 1 / \{1 + \exp[(V - V_{0.5inact}) / S_h]\} \tag{9}$$

The voltage dependency of the time constants of m and h of the voltage-activated currents is described by functions as Eqs (10) and (11) except that the τ_m of Ca^{2+} current takes the form of

Eq (10')

$$\tau_m(V) = \frac{1}{a_{\tau m, up} e^{(V_{\tau m, 0.5up} - V)/S_{\tau m, up}} + a_{\tau m, dn} e^{(V - V_{\tau m, 0.5dn})/S_{\tau m, dn}}}, \quad (10)$$

$$\tau_{mCa}(V) = (a_{(\tau m, up)} \exp\left(\frac{-V}{S_{\tau m, up}}\right) + a_{(\tau m, dn)} \left(\frac{-V + V_{\tau m, dn}}{\exp\left(\frac{-V + V_{\tau m, dn}}{S_{\tau m, dn}} - 1\right)} + 1\right))^{-1}, \quad (10)$$

$$\tau_h(V) = \frac{1}{a_{\tau h, up} e^{(V_{\tau h, 0.5up} - V)/S_{\tau h, up}} + a_{\tau h, dn} e^{(V - V_{\tau h, 0.5dn})/S_{\tau h, dn}}}, \quad (11)$$

For Na⁺ currents I_{Na} , value of parameter $V_{0.5act}$ in Eq (8) was taken from [38] (DUM cells of the cockroach *Periplaneta americana*), values of parameter S_m , $V_{0.5inact}$ and S_h were modified from [38] and values of parameters in Eqs (10) and (11) were fitted to the data given in [38]. For Ca²⁺ currents I_{Ca} , values of parameters in Eqs (8) and (9) were taken from [22] (PN in *P. americana*), time constant for activation takes the form of Eq (10') described in [39], $h = h_{\infty}$. For the sustained and transient voltage-gated K⁺ currents I_{kd} and I_A , values of parameters in Eqs (8) and (9) were taken from [36] (MGC PN in male sphinx moth *Manduca sexta*), and values of parameters in Eqs (10) and (11) were fitted to the data given in [37] (in *M. sexta*). The values of various parameters in the voltage dependent steady-state and time constant function of I_{Na} , I_{Ca} , I_{Kd} and I_A are given in Table 3.

The mathematical description of m_{∞} and current of the Ca²⁺-dependent K⁺ currents I_{SK} and that of the Ca²⁺ dynamics were borrowed directly from [39] as Eqs (12–14)

$$\frac{dCa}{dt} = -f_{Ca} I_{Ca} - (Ca - Ca_{\infty})/\tau_{Ca}, \quad (12)$$

$$m_{SK\infty} = 1 / \left(1 + e^{-a_{msk} - b_{msk} \log \frac{Ca - Ca_{\infty}}{S_{msk}}} \right), \quad (13)$$

$$I_{SK} = \bar{g}_{SK} \cdot m_{SK\infty}^2 (V - E_K), \quad (14)$$

where the values of parameters of Ca²⁺ dynamics are given in Table 2 and those of I_{SK} are given in Table 3.

The cholinergic synaptic current from ORNs to PN. The fast nicotinic cholinergic synaptic currents calculated according to

$$I_{nACh} = \sum_{i=1}^N \bar{g}_{nACh} \cdot [O]_i(t) \cdot (V - E_{nACh}), \quad (15)$$

where N is the number of ORNs, \bar{g}_{nACh} the mean peak conductance, and $E_{nACh} = 0$ mV the reversal potential of the current respectively. The fraction of open channels $[O]_i$ is modeled by first-order activation scheme (see review in [40])

$$\frac{d[O]_i}{dt} = \alpha(1 - [O]_i)[T]_i - \beta[O]_i \quad (16)$$

The release of cholinergic transmitter $[T]_i$ from i th ORN was modeled by a square pulse

$$[T]_i = A\theta(t_0 + t_{max} - t)\theta(t - t_0) \quad (17)$$

Parameter values of the nACh synaptic current are given in Table 4.

The MGC network model

We constructed a MGC network model by connecting 100 ORNs to one PN as shown in [S1 Fig](#). No LNs were included in the MGC model in order to test the hypothesis that the triphasic firing patterns of PN can be generated by the ionic currents in PN and ORN inputs. Computer simulations of the model were performed in Microsoft visual studio 2008. The simulation results were analyzed with Matlab 7.5. The total computer simulation time is 25s and the pheromone stimulation started at 5s.

Low-pass and high-pass Butterworth filters

In order to better understand how different ionic currents contribute to the generation of the PN firing pattern we separated the slow and fast components of the depolarizing and repolarizing currents in PN. We designed 10th-order lowpass and highpass Butterworth filters with cut-off frequency 5 Hz using the Matlab function "butter". By applying the designed lowpass and highpass filters the slow and fast components of each ionic currents were extracted.

Analysis of the PN response characteristics

The PN response pattern is quantitatively characterized by duration of E_1 and I phases and frequency of E_1 and E_2 phases. These features were defined in [S9 Fig](#) and were calculated as follows and expressed as means \pm standard error of the mean.

Duration. The E_1 durations were measured from the first spike of the PN response to the spike just preceding the inhibitory phase. The I durations were measured from the last spike of E_1 to the first spike of E_2 .

Frequency. We first calculated the interspike intervals (ISIs) between successive spikes. Then the ISIs were averaged in 10 spikes around each spike using Matlab function smooth. The frequencies are the inverse of the ISIs.

Supporting Information

S1 Fig. Simplified model of moth MGC. The model is composed of 100 Poisson ORNs and one biophysical PN. ORNs receive pheromone stimuli and the PN receive Ach synaptic inputs from ORNs through nicotinic receptors at the dendrites.

(TIF)

S2 Fig. Effects of parameters for m_∞ , τ_m function of I_{Ca} and for $m_{sk\infty}$ function of I_{SK} on PN response duration.

(TIF)

S3 Fig. Effects of parameters for τ_m , τ_h and h_∞ function of I_{Na} on PN response characteristics. I duration clearly increases with $S_{tm,up}$ (A) and $V_{th>0.5dn}$ (G), while it decreases with $a_{th>dn}$ (C). E_1 frequency linearly decreases with $V_{0.5inact}$ (F); E_2 frequency increases with $a_{th,dn}$ (D), $S_{th,dn}$ (B) and $V_{th>0.5up}$ (E) while it decreases with $V_{0.5inact}$ (F) and $V_{th>0.5dn}$ (H).

(TIF)

S4 Fig. Effects of parameters of I_{Kd} on PN response characteristics. I_{Kd} clearly affects E_1 frequency which increases with \bar{g}_{Kd} when \bar{g}_{Kd} is below $0.7 \mu S$ then decreases (B) while it decreases with $V_{0.5act}$ (E) and S_m of I_{Kd} (H).

(TIF)

S5 Fig. Effects of Ach pulse duration t_{max} and concentration A on PN response characteristics. Top panel: effects of t_{max} on E_1 and I duration (A) and mean firing frequency of E_1 and E_2

(B). Bottom panel: effects of A on E_1 and I duration (C) and mean firing frequency of E_1 and E_2 phases (D).

(TIF)

S6 Fig. Effects of nACh postsynaptic channel opening rate α , closing rate β and \bar{g}_{nACh} on PN response characteristics. Top panel: effects of α on E_1 and I duration (A) and mean firing frequency of E_1 and E_2 (B). Middle panel: effects of β on E_1 and I duration (C) and mean firing frequency of E_1 and E_2 phases (D). Bottom panel: effects of \bar{g}_{nACh} on E_1 and I duration (E) and mean firing frequency of E_1 and E_2 (F).

(TIF)

S7 Fig. Effects of inhibition mediated by fast GABA_A receptors on the activity patterns of PN and three LNIs in a network with 80 ORNs, 1 PN and 20 LNIs. The postsynaptic channel closing rate β of the GABA synapses from LNI to PN is 0.1 (left panel), 2.0 (middle panel) and 3.0 (right panel) respectively.

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S8 Fig. Effects of slow inhibition mediated by metabotropic GABA_B receptors on the response activity of PN and three LNIs in a network with 80 ORNs, 1 PN and 20 LNIs. Panel A-D show that the GABA_B mediated synaptic inhibition did not alter the triphasic response pattern of PN in the normal parameter range: A. PN potential, spikes and frequency; B. potentials of LNI8; C. normalized concentration of intracellular Ca in PN and of GABA_B receptor-coupled G protein; D. potentials of LNI17. Panel E-F show that the I duration is prolonged when r_3 is decreased: E. PN potential, spikes and frequency; F. normalized concentration of intracellular Ca in PN and of GABA_B receptor-coupled G protein. Panel G-H show that the GABA_B mediated synaptic inhibition changed the triphasic response pattern when r_3 is increased and r_4 is decreased: G. PN potential, spikes and frequency; H. normalized concentration of intracellular Ca in PN and of GABA_B receptor-coupled G protein.

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S9 Fig. Extracellularly recorded response patterns of the moth pheromone sensitive PN in MGC. Left panel: top trace, response pattern to low dose pheromone stimulus; bottom trace, response pattern to high dose pheromone stimulus. Right panel: from top to bottom trace the duration of pheromone stimuli were increased at a given stimulation concentration.

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S1 Text. Model of type I LNs with sodium spikes.

(PDF)

S2 Text. Experimental findings in ORNs, PNs and type I LNs.

(PDF)

Author Contributions

Conceived and designed the experiments: YG. Performed the experiments: YG. Analyzed the data: YG. Contributed reagents/materials/analysis tools: YG. Wrote the paper: YG.

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