

# Modulation of Voltage-dependent Sodium and Potassium Currents by Charged Amphiphiles in Cardiac Ventricular Myocytes

## *Effects via Modification of Surface Potential*

SEN JI, JAMES N. WEISS, and GLENN A. LANGER

From the Cardiovascular Research Laboratories, Departments of Physiology and Medicine, UCLA School of Medicine, Los Angeles, California 90024-1760

**ABSTRACT** Modulation of voltage-dependent sodium and potassium currents by charged amphiphiles was investigated in cardiac ventricular myocytes using the patch-clamp technique. Negatively charged sodium dodecylsulfate (SDS) increased amplitude of  $I_{Na}$ , whereas positively charged dodecyltrimethylammonium (DDTMA) decreased  $I_{Na}$ . Furthermore, SDS shifted the steady-state activation and inactivation of  $I_{Na}$  in the negative direction, whereas DDTMA shifted the curves in the opposite direction. These shifts provided an explanation for the changes in current amplitude. Activation and inactivation kinetics of  $I_{Na}$  were accelerated by SDS but slowed by DDTMA. These changes in both steady-state gating and kinetics of  $I_{Na}$  are consistent with a decrease of the intramembrane field by SDS and an increase of the field by DDTMA due to an alteration of surface potential after their insertion into the outer monolayer of the sarcolemma. The effect of SDS on the steady-state inactivation of  $I_{Na}$  was concentration dependent and partially reversed by screening surface charges with increased extracellular  $[Ca^{2+}]$ . These amphiphiles also altered the activation of the delayed rectifier  $K^+$  current ( $I_{K,del}$ ), producing a shift in the negative direction by SDS but in the positive direction by DDTMA. These results suggest that the insertion of charged amphiphiles into the cell membrane alters the behavior of voltage-dependent  $I_{Na}$  and  $I_{K,del}$  by changing the surface charge density, and consequently the surface potential and implies, although indirectly, that the lipid surface charges are important to the voltage-dependent gating of these channels.

### INTRODUCTION

Since A. F. Huxley suggested to Frankenhauser and Hodgkin that there is probably a localized potential on the surface of the cell membrane (Frankenhauser and

Address reprint requests to Dr. Sen Ji, Cardiovascular Research Laboratories, 3645 MRL Bldg., 675 Circle Drive South, UCLA School of Medicine, Los Angeles, CA 90024-1670. Dr. Sen Ji's present address is Department of Neuroscience, University of Pennsylvania, Philadelphia, PA 19104-6074.

Hodgkin, 1957), surface potential theory has been widely used to explain many phenomena involving electrostatic interactions in the membrane. The theory is significant because such a potential can establish an intramembrane electric field, which might then affect the function of many molecules residing in the membranes, particularly the gating mechanisms of voltage-dependent ion channels (McLaughlin, 1977; Green and Andersen, 1991). The consequences of the effect can be very important in terms of its influence on cellular functions such as excitability.

The chemical identity of the surface potential has been attributed to several different components in the membrane (Green and Andersen, 1991). (1) Membrane proteins contribute a significant amount of charges, carried by charged amino acids and other hydrophilic residues located at or near the aqueous surface of protein due to their hydrophilicity (Kyte and Doolittle, 1982; Catterall, 1988). (2) Charged lipids are also an important source contributing to the surface potential, especially phospholipids (Storch and Kleinfeld, 1985; Mato, 1990). At physiological pH, phospholipids exist as charged zwitterions, among which phosphatidylserine and phosphatidylinositol carry net negative charges. (3) Negatively charged sialic acid residues attached to asparagine-linked oligosaccharide chains (Kornfeld and Kornfeld, 1985) are normally added to the extracellular domain of membrane proteins during the glycosylation of membrane proteins (Catterall, 1988; Levinson, Thornhill, Duch, Recio-Pinto, and Urban, 1990). (4) Negatively charged phosphates can also be attached to membrane proteins following the phosphorylation of proteins by protein kinases, e.g., phosphorylation of the delayed rectifier  $K^+$  channels (Perozo, Bezanilla, and Dipolo, 1989).

The possible role of surface potential in the modulation of ion channel function has been extensively investigated. Various approaches have been used to alter this potential (for review, see Green and Andersen, 1991). (1) Changing ionic strength in the extracellular solution, particularly with divalent cations, is the classical way to modify (screen) surface potential. Following the leading work by Frankenhauser and Hodgkin (1957), many laboratories have observed the screening effects of divalent cations on the surface potential and the consequences on the behavior of different ion channels (McLaughlin, Szabo, and Eisenman, 1971; Hille, Woodhull, and Shapiro, 1975; Gilly and Armstrong, 1982; Hahin and Campbell, 1983; Armstrong and Matterson, 1986; Cukierman, Zinkand, French, and Krueger, 1988; Armstrong and Cota, 1990); (2) Changing pH is also an effective method to alter the surface charges (Campbell and Hahin, 1984; Zhang and Siegelbaum, 1991); (3) Various enzymes have been used as well in an attempt to modify the density of the surface charges; for example, the removal of sialic acid residues by neuraminidase (Yee, Weiss, and Langer, 1989; Levinson et al., 1990).

In this study, we have examined the effects of altering charge density on the surface membrane by introduction of charged lipid-like amphiphiles (Helenius, McCaslin, Fries, and Tanford, 1979) such as sodium dodecylsulfate (SDS) and dodecyltrimethylammonium (DDTMA). These amphiphiles can insert into the outer monolayer of the membrane, and, based on thermodynamic considerations, are unlikely to move through the hydrophobic center of the membrane to the inner monolayer over a short time period (several minutes), even if their movements are facilitated by a so-called endogenous "flip-pass." This approach has been used

previously to examine the effects of these agents on the voltage-gated  $\text{Ca}^{2+}$  currents, contractile function, and  $\text{Ca}^{2+}$  uptake and binding in single cardiac myocytes (Burt and Langer, 1983; Philipson, Langer, and Rich, 1985; Langer and Rich, 1986; Post, Ji, Leonards, and Langer, 1991). After the exposure of myocytes to SDS and DDTMA, negatively charged amphiphile SDS increased L-type  $\text{Ca}^{2+}$  current ( $I_{\text{Ca,L}}$ ), cell contraction, and  $\text{Ca}^{2+}$  uptake and binding, whereas positively charged amphiphile DDTMA had opposite effects (Post et al., 1991). The observed changes in both the amplitude and steady-state gating of the L-type  $\text{Ca}^{2+}$  current were in good agreement with the alterations of surface potential, assuming that the charged amphiphiles inserted into the outer monolayer of the sarcolemma (Ji, Weiss, and Langer, 1990; Post et al., 1991). These previous studies raised significant questions: (1) Are these effects specific to L-type  $\text{Ca}^{2+}$  channels? In other words, does the insertion also occur around other channels? If so, do other voltage-gated channels, e.g.,  $\text{Na}^+$  and  $\text{K}^+$  channels, show similar alterations in terms of their voltage-dependent steady-state gating and macroscopic current? Can these alterations be interpreted as the results of modification of surface potential? (2) Besides the effects on the surface potential, is there a direct interaction between the charged amphiphiles and ion channels? Such an interaction may cause a conformational change of the channel protein with consequent changes of single channel properties, e.g., single channel conductance, contributing to the changes of macroscopic current. In this study, we further investigate the effects of these agents on voltage-dependent  $\text{Na}^+$  ( $I_{\text{Na}}$ ) and delayed rectifier  $\text{K}^+$  current ( $I_{\text{K,del}}$ ) in cardiac ventricular myocytes in order to address these questions and further characterize the effects of these amphiphiles.

Part of the work was reported previously in an abstract (Ji, Weiss, and Langer, 1992).

## MATERIALS AND METHODS

### *Isolation of Cardiac Ventricular Myocytes*

Adult rabbit or guinea pig ventricular myocytes were isolated by retrograde perfusion of the aortic artery with modified Tyrode's solution containing collagenase (class II; Worthington Biochemical Corp., Freehold, NJ) and protease or hyaluronidase (Sigma Immunochemicals, St. Louis, MO) (Mitra and Morad, 1985). The isolated rabbit ventricular myocytes were suspended in modified Eagle's medium (S-MEM; Irvine Scientific, Santa Ana, CA) and incubated overnight at  $37^\circ\text{C}$  to use on day 2. The guinea pig ventricular myocytes were used immediately after isolation.

### *Whole-Cell Current Recording*

The patch-clamp technique was used to study the effects of the charged amphiphiles on voltage-dependent sodium and delayed rectifier potassium currents in the whole-cell recording configuration (Hamill, Marty, Neher, Sakmann, and Sigworth, 1981). The currents were recorded using an Axopatch 200 or Axopatch 1D patch-clamp amplifier (Axon Instruments, Inc., Foster City, CA) and digitized and stored in a PC computer interfaced to the amplifier through a 40-kHz Labmaster board (Scientific Solutions Inc., Solon, OH). The recording electrodes had a resistance of  $\sim 1\text{--}2\text{ M}\Omega$  when filled with our pipette solutions (Table I). Standard procedures of capacitance and series resistance compensation were used (Hamill et

al., 1981; Cota and Armstrong, 1989). Programming of voltage-clamp commands and data acquisition and analysis were performed utilizing the pCLAMP software package (Axon Instruments, Inc.). The experimental chamber (0.5 ml) containing the myocytes was continuously perfused at a flow rate of 3–4 ml/min. All experiments were done at room temperature, 22°C.

### Solutions

Pipette and extracellular solutions used for isolation of  $I_{Na}$  current ( $I_{Na}$ ) and delayed rectifier  $K^+$  ( $I_{K,del}$ ) are listed in Table I.

The charged amphiphiles we used were SDS and DDTMA (both from Sigma Immunochemicals). They are oppositely charged at the headgroup, negative for SDS but positive for DDTMA, and have an identical 12-carbon backbone. The concentration of the amphiphiles used was 20  $\mu$ M, which was >40-fold below the critical micellar concentration of  $\sim$ 8.13 mM for

TABLE I  
Solutions for Isolation of  $I_{Na}$  and  $I_{K,del}$

	$I_{Na}$		$I_{K,del}$	
	Internal	External	Internal	External
NaCl	5.0	5.3	—	—
NaOH	—	4.7	—	—
CsCl	133.5	—	—	—
CsOH	11.5	—	—	—
TEA-Cl	—	135.0	—	—
Choline-Cl	—	(135.0)	—	140.0
K-glutamate	—	—	108.2	—
KCl	—	—	20.0	0.6
KOH	—	—	16.8	4.8
MgCl <sub>2</sub>	1.0	1.0	1.0	1.0
CaCl <sub>2</sub>	—	1.0	—	1.0
EGTA	5.0	—	5.0	—
HEPES	10.0	10.0	10.0	10.0
pH	7.2	7.4	7.2	7.4
Glucose	—	10.0	—	10.0
MgATP	5.0	—	5.0	—

SDS and  $\sim$ 14.6 mM for DDTMA. At this concentration, the detergents exist in the form of monomers (Helenius et al., 1979).

### Data Analysis

All results in both figures and text are expressed as mean  $\pm$  SEM.

## RESULTS

### Isolation of $I_{Na}$

The voltage-dependent  $I_{Na}$  was isolated by blocking  $I_{Ca,L}$  with 2  $\mu$ M nifedipine and blocking  $K^+$  currents with tetraethylammonium (TEA) from the extracellular side and  $Cs^+$  from the intracellular side in overnight-incubated or freshly dissociated rabbit ventricular myocytes. To minimize the potential errors in the accuracy of clamp

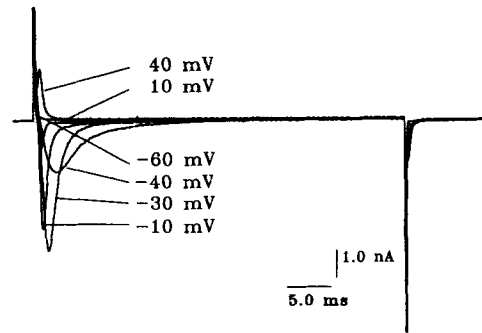


FIGURE 1. Isolation of  $I_{Na}$ .  $I_{Na}$  was recorded in the whole-cell recording configuration using the patch-clamp technique. Amplitude of the current was reduced by lowering extracellular  $[Na^+]$  to 10 mM, with substitution of  $Na^+$  with choline or TEA. The intracellular  $[Na^+]$  was 5 mM. The holding potential was  $-110$  mV.

pulses by series resistance, the magnitude of the macroscopic  $Na^+$  current was reduced by lowering extracellular  $[Na^+]$  to 10 mM with substitution of choline, TEA, or *N*-methyl-D-glutamine and keeping intracellular  $[Na^+]$  at 5 mM (Table I). The typical recording of the isolated  $I_{Na}$  under these conditions is shown in Fig. 1. The current was elicited by 55-ms test pulses to different membrane potentials ( $-70$  to  $30$  mV) in 10-mV steps from a holding potential of  $-110$  mV.

#### *Effects of the Charged Amphiphiles on $I_{Na}$*

The amplitude of  $I_{Na}$  was significantly affected by both charged amphiphiles (Fig. 2). As shown in Fig. 2A, the maximal peak current increased by  $\sim 20\%$  after exposure to SDS. From the plot of the peak  $Na^+$  current–voltage ( $I$ - $V$ ) relationships (Fig. 2B), it was found that after exposure to SDS (1) the maximal peak  $I_{Na}$  was increased by  $\sim 20\%$ ; (2)  $I_{Na}$  was activated at a membrane potential 10 mV more negative ( $-60$  mV as compared with  $-50$  mV); (3) the maximal peak  $I_{Na}$  occurred at  $-40$  mV instead of

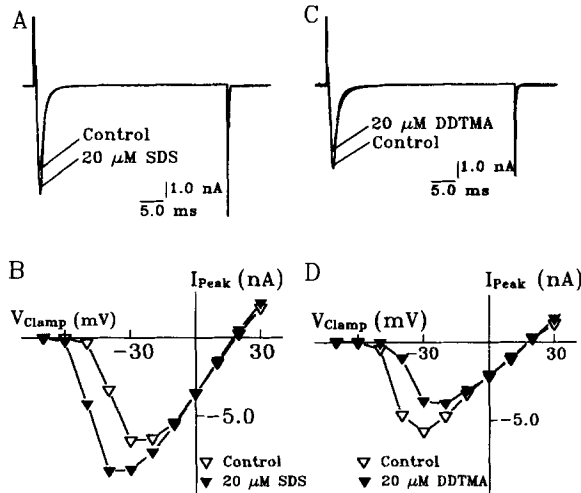


FIGURE 2. Effects of the charged amphiphiles on  $I_{Na}$ . (A) The effects of negatively charged SDS on the maximal peak  $I_{Na}$ . The current was elicited at a test membrane potential of  $-30$  mV from a holding potential of  $-110$  mV under control conditions and at a test membrane potential of  $-40$  mV from a holding potential of  $-120$  mV after exposure to  $20 \mu M$  SDS. (B) The  $I$ - $V$  plots before and after SDS treatment. (C) The effects of positively charged DDTMA on the maximal peak  $I_{Na}$ . The current was recorded at a test membrane

potential of  $-30$  mV from a holding potential of  $-110$  mV under control conditions and at a test membrane potential of  $-20$  mV from the same holding potential after exposure to  $20 \mu M$  DDTMA. (D) The  $I$ - $V$  relations before and after  $20 \mu M$  DDTMA superfusion.

-30 mV. In six cells, the maximal peak  $I_{Na}$  was increased by  $19.6 \pm 11.7\%$  ( $n = 6$ ;  $P < 0.05$ , paired  $t$  test) after exposure to  $20 \mu\text{M}$  SDS. After SDS treatment, a holding potential of  $-120$  mV was applied to maintain channels fully available for opening because of the possibility that the channels would be partially inactivated due to a shift of the steady-state inactivation of the current in the negative direction (see Fig. 3).

On the other hand, the exposure of myocytes to  $20 \mu\text{M}$  DDTMA produced opposite effects (Fig. 2 C). The maximal peak current was decreased and there was a shift of the peak and the activation threshold of the current in the positive direction

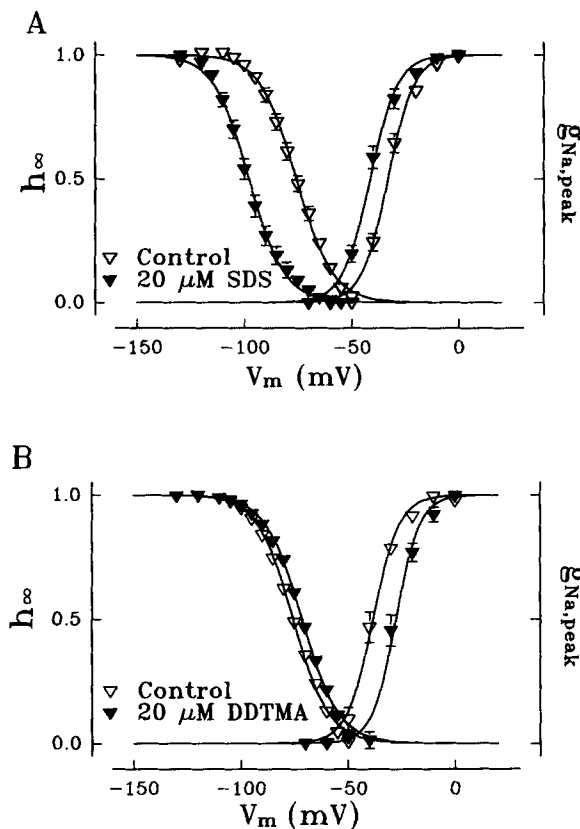


FIGURE 3. Effects of the charged amphiphiles on the steady-state activation and inactivation of  $I_{Na}$ . Open symbols represent the controls and filled symbols are experimental data points after treatment with SDS or DDTMA. Experimental data points are expressed as mean  $\pm$  SEM. The solid lines are the best fits to the Boltzmann relation (see Results). (A) The effects of  $20 \mu\text{M}$  SDS ( $n = 7$ ). (B) The effects of  $20 \mu\text{M}$  DDTMA ( $n = 5$ ).

(Fig. 2 D). The decrease in peak  $I_{Na}$  in five cells averaged  $18.1 \pm 6.37\%$  ( $P < 0.01$ , paired  $t$  test).

The reversal potential of  $I_{Na}$ , however, was not significantly changed by either agent (Fig. 2, B and D).

#### *Effects of the Amphiphiles on the Steady-State Inactivation and Activation of $I_{Na}$*

As shown by the  $I$ - $V$  relations (Fig. 2, B and D), the peak and the activation threshold of  $I_{Na}$  were shifted along the voltage axis by the amphiphiles, suggesting that the

voltage dependence of the steady-state inactivation and activation might be altered also. Fig. 3 *A* shows the effects of SDS on the steady-state inactivation and activation of  $I_{Na}$ . The steady-state inactivation was measured by recording the peak  $I_{Na}$  during a voltage clamp to  $-30$  mV after a 500-ms conditioning pulse to various membrane potentials ranging from  $-150$  to  $0$  mV and normalizing the currents to the maximum. The normalized peak currents were fit to a Boltzmann relationship:

$$h_{\infty} = 1 / \{1 + \exp[ze(V - V_{1/2})/kT]\} \quad (1)$$

where  $z$  is the apparent valence of the inactivation gate,  $e$  is the electric charge,  $k$  is the Boltzmann constant,  $T$  is the absolute temperature,  $V$  is the conditioning membrane potential, and  $V_{1/2}$  is the membrane potential corresponding to 50% inactivation. The inactivation curve (or  $h_{\infty}$  curve, by Hodgkin and Huxley's convention [Hodgkin and Huxley, 1952]) was shifted in the hyperpolarizing direction after exposure to SDS with  $V_{1/2}$  shifted by  $-22.1$  mV ( $n = 7$ ). However, the slope of the curve did not show a significant change (Fig. 3 *A*).

TABLE II  
*Effects of the Charged Amphiphiles on  $V_{1/2}$ 's and the Apparent Valences of Steady-State Inactivation and Activation of  $I_{Na}$*

	Control ( $n = 7$ )	20 $\mu$ M SDS ( $n = 7$ )	Control ( $n = 5$ )	20 $\mu$ M DDTMA ( $n = 5$ )
Activation				
$V_{1/2}$ (mV)	$-32.9 \pm 1.0$	$-41.1 \pm 1.3$	$-38.5 \pm 1.6$	$-28.4 \pm 1.6$
$z$	$3.9 \pm 0.3$	$3.8 \pm 0.4$	$4.1 \pm 0.2$	$3.7 \pm 0.4$
Inactivation				
$V_{1/2}$ (mV)	$-75.7 \pm 1.2$	$-97.8 \pm 1.5$	$-75.6 \pm 0.4$	$-71.5 \pm 0.9$
$z$	$2.9 \pm 0.3$	$3.0 \pm 0.3$	$2.8 \pm 0.4$	$2.7 \pm 0.3$

The activation of  $I_{Na}$  was measured by clamping the membrane potential to various levels ranging from  $-70$  to  $0$  mV from a holding potential of  $-110$  mV. The whole-cell  $Na^+$  channel conductance ( $g_{Na}$ ) was calculated by dividing the peak  $I_{Na}$  by the driving force ( $V_m - E_{Na}$ ) assuming that  $E_{Na} = 18$  mV for  $[Na^+]_o = 10$  mM and  $[Na^+]_i = 5$  mM.  $g_{Na}$  was normalized to the maximal value ( $g_{max}$ ) and fit to a Boltzmann relationship:

$$g/g_{max} = 1 / \{1 + \exp[ze(V_{1/2} - V)/kT]\} \quad (2)$$

to obtain the 50% activation point and the valence of the activation gate.  $V_{1/2}$  of the activation was shifted in the hyperpolarizing direction by  $-8.2$  mV ( $n = 7$ ), which was less than the shift in the steady-state inactivation caused by SDS (Fig. 3 *A* and Table II).

Mean values of  $V_{1/2}$ 's and the calculated apparent valences of the activation and inactivation gates from individual cells before and after exposure of the myocytes to SDS are summarized in Table II.

Conversely, positively charged DDTMA had opposite effects on the voltage dependence of  $I_{Na}$  inactivation and activation (Fig. 3 *B*).  $V_{1/2}$  of the activation curve was shifted in the depolarizing direction by  $10.1$  mV ( $n = 5$ ).  $V_{1/2}$  of the steady-state

inactivation curve was shifted by 4.5 mV ( $n = 5$ ) in the same direction. The averaged values of  $V_{1/2}$ 's and the calculated valences of the activation and inactivation gates before and after exposure of the cells to DDTMA are listed in Table II.

*No Significant Change of the Peak Whole-Cell Conductance*

As shown in Fig. 4, neither SDS nor DDTMA significantly altered the maximal whole-cell conductance, suggesting that the changes in the magnitude of  $I_{Na}$  caused by the amphiphiles resulted from the shifts in the voltage dependence of the current gating and not from the direct effects on channel conductance.

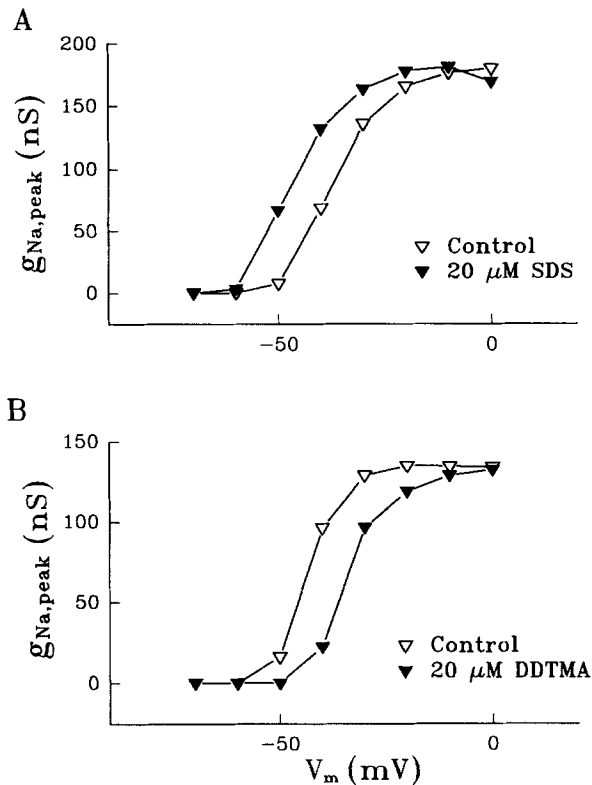


FIGURE 4. Effects of amphiphiles on the whole-cell Na<sup>+</sup> conductance. The whole-cell Na<sup>+</sup> channel conductance was calculated from the maximal peak  $I_{Na}$  recorded at various membrane potentials by assuming a reversal potential of 18 mV. (A) The whole-cell Na<sup>+</sup> conductance before and after 20  $\mu$ M SDS and (B) before and after 20  $\mu$ M DDTMA. Note that the maximal conductance was not affected by either amphiphile.

*No Open Channel Facilitation of the Effect of SDS on the Steady-State Inactivation*

To determine whether the ability of SDS to alter the steady-state inactivation of  $I_{Na}$  was affected by the state of the Na<sup>+</sup> channel (closed, open, or inactivated), a train of depolarizing pulses was delivered before the conventional double-pulse protocol in order to drive Na<sup>+</sup> channels into the open or inactivated state for a greater percentage of time. Fig. 5 shows that the steady-state inactivation curve was not significantly altered by the train of depolarization pulses either before or after SDS treatment, suggesting that the effect of SDS was not dependent on the state of the Na<sup>+</sup> channel.



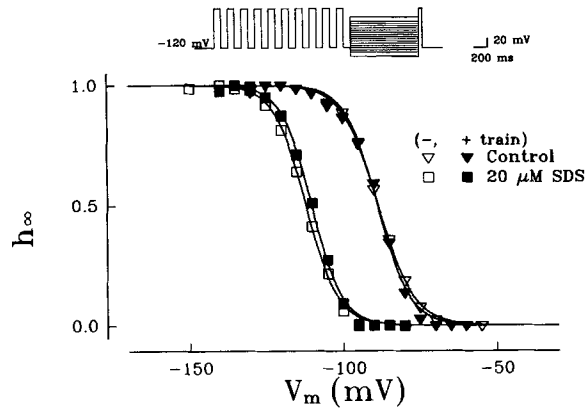


FIGURE 5. No open channel facilitation of the effects of SDS on the steady-state inactivation. Steady-state inactivation was examined using conventional double-pulse protocol (*open symbols*) and a double-pulse protocol preceded by a train of five depolarizing pulses to  $-30$  mV for 100 ms from a holding potential of  $-120$  mV delivered at 10 Hz (*filled symbols*). The protocol is shown in the upper panel. The  $V_{1/2}$  and slope of the steady-state inactivation curves were not significantly altered by the train either before or after exposure to SDS.

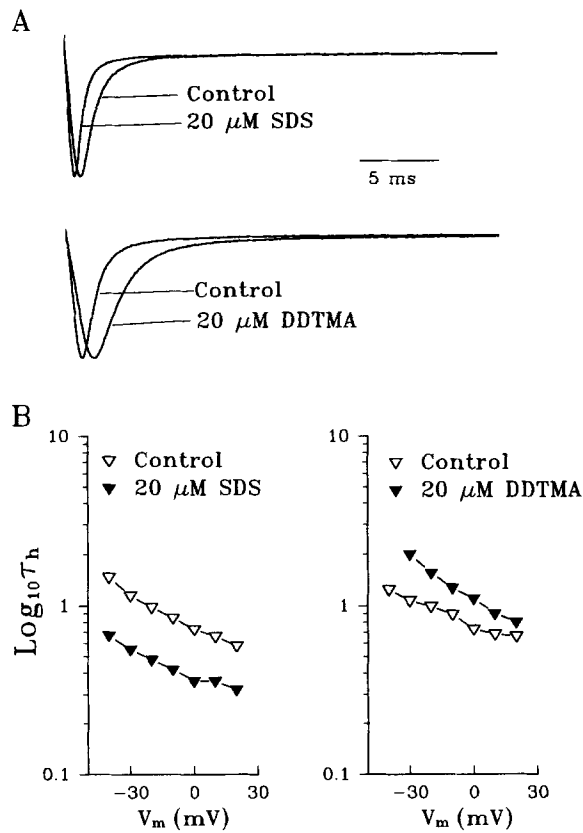


FIGURE 6. The effects of the amphiphiles on the activation and inactivation kinetics of  $I_{Na}$ . (A)  $I_{Na}$  normalized to the same peak amplitude before and after amphiphile treatment with SDS (*upper traces*) and DDTMA (*lower traces*). (B) The inactivation time constants ( $\tau_h$ ) of  $I_{Na}$  before (*open symbols*) and after (*filled symbols*) amphiphile treatment.  $\tau_h$  was obtained by fitting the inactivating phase of  $I_{Na}$  to a single exponential.

*Effects of the Amphiphiles on the Activation and Inactivation Kinetics of  $I_{Na}$* 

In addition to the effects on  $I_{Na}$  amplitude and steady-state activation and inactivation, the charged amphiphiles also altered the kinetics of  $I_{Na}$  activation and inactivation. When  $I_{Na}$  before and after exposure to the amphiphiles was scaled to the same peak amplitude, alterations in both the activation and inactivation phases of the currents were quite obvious (Fig. 6A). Both activation and inactivation were accelerated by SDS and slowed by DDTMA. Activation was too rapid to fit accurately, but the inactivation phase was well fit to a single exponential, yielding the inactivation time

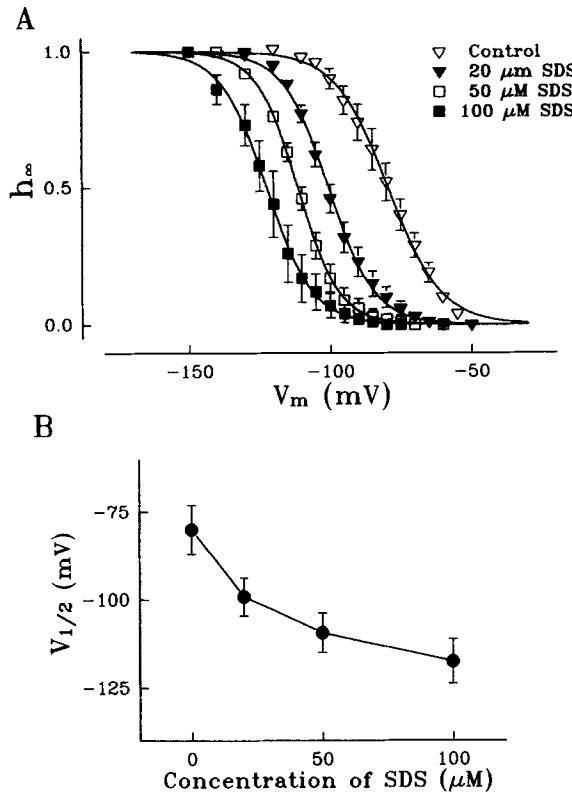


FIGURE 7. Concentration dependence of the effects of SDS on the steady-state inactivation of  $I_{Na}$ . (A) After recording the control curve ( $\nabla$ ), [SDS] was raised from 20  $\mu$ M ( $\blacktriangledown$ ) to 50  $\mu$ M ( $\square$ ) and 100  $\mu$ M ( $\blacksquare$ ). The solid lines are the best fits to the Boltzmann relation.  $V_{1/2}$  was progressively shifted in the negative direction as the concentration of SDS was increased. (B) Summary of  $V_{1/2}$ 's at different SDS concentrations ( $n = 6$ ).

constants (Fig. 6B). The time constants ( $\tau_h$ ) were decreased by SDS, but increased by DDTMA (Fig. 6B). In both cases,  $\tau_h$  was shifted along the voltage axis in a parallel fashion. However, the magnitude of the shift along the voltage axis produced by either amphiphile was considerably greater than the corresponding shift in steady-state inactivation and activation (Fig. 3).

*Concentration Dependence of the Effects on Steady-State Inactivation of  $I_{Na}$  by SDS*

The effects of SDS on the steady-state inactivation of  $I_{Na}$  occurred in a concentration-dependent fashion. Fig. 7A shows that the voltage dependence of the steady-state

inactivation was shifted progressively in the negative direction as the concentration of SDS was increased from 20 to 100  $\mu\text{M}$ . As shown in Fig. 7 B,  $V_{1/2}$  was shifted by  $-21.1$  mV with 20  $\mu\text{M}$  SDS, by  $-32.0$  mV with 50  $\mu\text{M}$  SDS, and by  $-43.1$  mV with 100  $\mu\text{M}$  SDS ( $n = 6$ ).

*Screening the Effects of SDS on the Steady-State Inactivation by Increasing Extracellular  $[\text{Ca}^{2+}]$*

$\text{Ca}^{2+}$  is one of the most widely used divalent cations to screen the negative surface charges, although it may also block sodium channel in a voltage-dependent manner

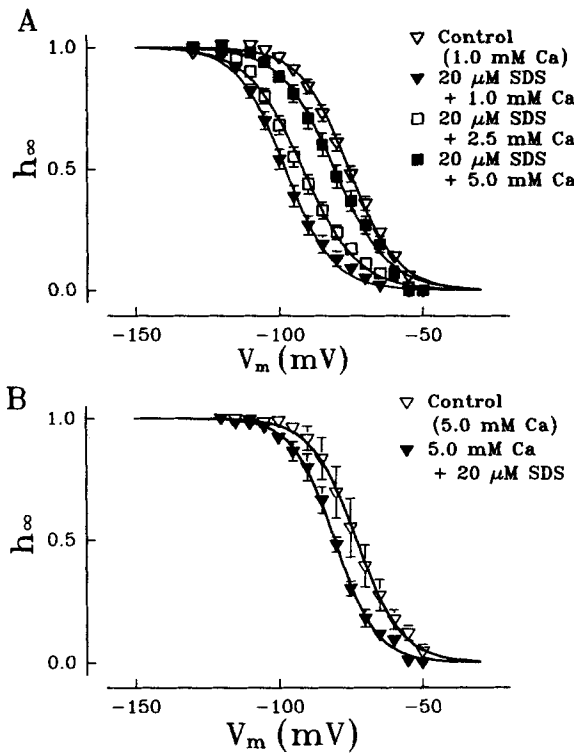


FIGURE 8. (A) Partial reversal of the effects of SDS on the steady-state inactivation of  $I_{\text{Na}}$  by raising extracellular  $[\text{Ca}^{2+}]$  from 1.0 mM ( $\blacktriangledown$ ) to 2.5 mM ( $\square$ ) and 5.0 mM ( $\blacksquare$ ) in the presence of 20  $\mu\text{M}$  SDS. The control curve before exposure to SDS is also shown ( $\nabla$ ). The solid lines are the best fits to the Boltzmann relation ( $n = 7$ ). (B) Dependence of SDS insertion on extracellular  $[\text{Ca}^{2+}]$ . The shift of the steady-state inactivation curve by SDS was less in the presence of 5.0 mM  $\text{Ca}^{2+}$  in the perfusate ( $n = 4$ ) than in the presence of 1.0 mM  $\text{Ca}^{2+}$  (compare with A).

(Yamamoto, Yeh, and Narahashi, 1984, 1985; Nilius, 1988). We therefore investigated whether the effects of SDS on  $I_{\text{Na}}$  could be reversed by increasing extracellular  $[\text{Ca}^{2+}]$  to screen the negative charges of amphiphiles inserted in the outer monolayer of the membrane. After exposure to 20  $\mu\text{M}$  SDS, the steady-state inactivation of  $I_{\text{Na}}$  was shifted in the hyperpolarizing direction by  $-22.1$  mV when extracellular  $[\text{Ca}^{2+}]$  was 1 mM. Increasing extracellular  $[\text{Ca}^{2+}]$  to 2.5 and 5.0 mM returned the inactivation curve toward the pre-SDS value by 6.1 and 17.0 mV, respectively (Fig. 8 A;  $n = 7$ ). A summary of  $V_{1/2}$ 's and the calculated valences of the inactivation gate under these conditions is shown in Table III. This effect of increasing extracellular  $[\text{Ca}^{2+}]$  was due to the screening of the inserted surface charges as well as the fixed,

TABLE III  
 Screening the Effects of SDS on Steady-State Inactivation of  $I_{Na}$  by Raising  
 Extracellular  $[Ca^{2+}]_o$  ( $n = 7$ )

	Control	20 $\mu$ M SDS	+2.5 mM $Ca^{2+}$	+5.0 mM $Ca^{2+}$
$V_{1/2}$ (mV)	$-75.7 \pm 1.2$	$-97.8 \pm 1.5$	$-91.8 \pm 1.6$	$-80.7 \pm 1.8$
$z$	$2.8 \pm 0.3$	$3.0 \pm 0.3$	$2.6 \pm 0.2$	$2.5 \pm 0.2$

“native” negative surface charges, since in the presence of 5.0 mM  $Ca^{2+}$ , 20  $\mu$ M SDS produced a significantly smaller shift in  $V_{1/2}$  of the steady-state inactivation curve ( $h_\infty$  curve) ( $\Delta V_{1/2} = -7.6$  mV,  $n = 4$ ) (Fig. 8 B) than in the presence of 1.0 mM  $Ca^{2+}$  ( $\Delta V_{1/2} = -22.1$  mV) (Fig. 8 A). It should be noted that increasing  $[Ca^{2+}]_o$  caused progressive voltage-dependent block of  $I_{Na}$ . In construction of the  $h_\infty$  curves,  $I_{Na}$  was therefore normalized to the maximal  $I_{Na}$  at each  $[Ca^{2+}]_o$ , respectively. Since the magnitude of  $I_{Na}$  was elicited at a constant test potential,  $Ca^{2+}$ -dependent block of  $I_{Na}$  would be expected to have little effect on the intrinsic shape of the  $h_\infty$  curves at different  $[Ca^{2+}]_o$ .

*Effects of the Amphiphiles on the Activation of  $I_{K,del}$*

Guinea pig ventricular myocytes were used to examine the effects of the amphiphiles on the delayed rectifier potassium current ( $I_{K,del}$ ) (Matsuura, Ehara, and Imoto, 1987; Balsler, Bennett, and Roden, 1990), since  $I_{K,del}$  is larger in this species (Sanguinetti and Jurkiewicz, 1990).  $I_{K,del}$  was isolated by blocking  $I_{Na}$  with  $1 \times 10^{-5}$  M tetrodotoxin and  $I_{Ca,L}$  with  $2 \times 10^{-6}$  M nifedipine (Fig. 9 A).  $I_{K,del}$  elicited by voltage pulses to positive potentials from a holding potential of  $-30$  mV, activated very slowly and was not fully activated at the end of a 7.2-s pulse. Tail currents were recorded after

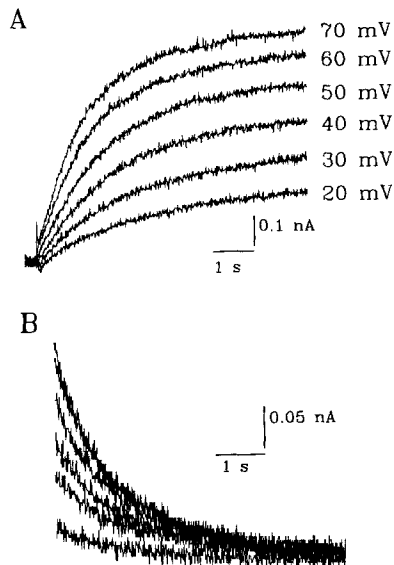


FIGURE 9. Recording of the delayed rectifier potassium current. (A) The delayed rectifier potassium current elicited by depolarizing the myocytes to various membrane potentials (as indicated) positive to the holding potential of  $-30$  mV in guinea pig ventricular myocytes. (B) Tail currents of the delayed rectifier potassium current recorded when the myocytes were clamped back to  $-30$  mV.

clamping the myocytes back to a holding potential of  $-30$  mV (Fig. 9 B) and plotted against the test potentials to obtain the activation curve of  $I_{K,del}$  (Fig. 10).

After exposing myocytes to the amphiphiles, the activation curves of  $I_{K,del}$  were shifted in the negative direction by SDS and in the positive direction by DDTMA (Fig. 10, A and B), similar to the shifts of  $I_{Na}$ . The shifts in the  $V_{1/2}$  were  $-7.1 \pm 1.7$  ( $n = 7$ ) for SDS and  $10.2 \pm 3.0$  ( $n = 4$ ) for DDTMA, respectively. Without amphi-

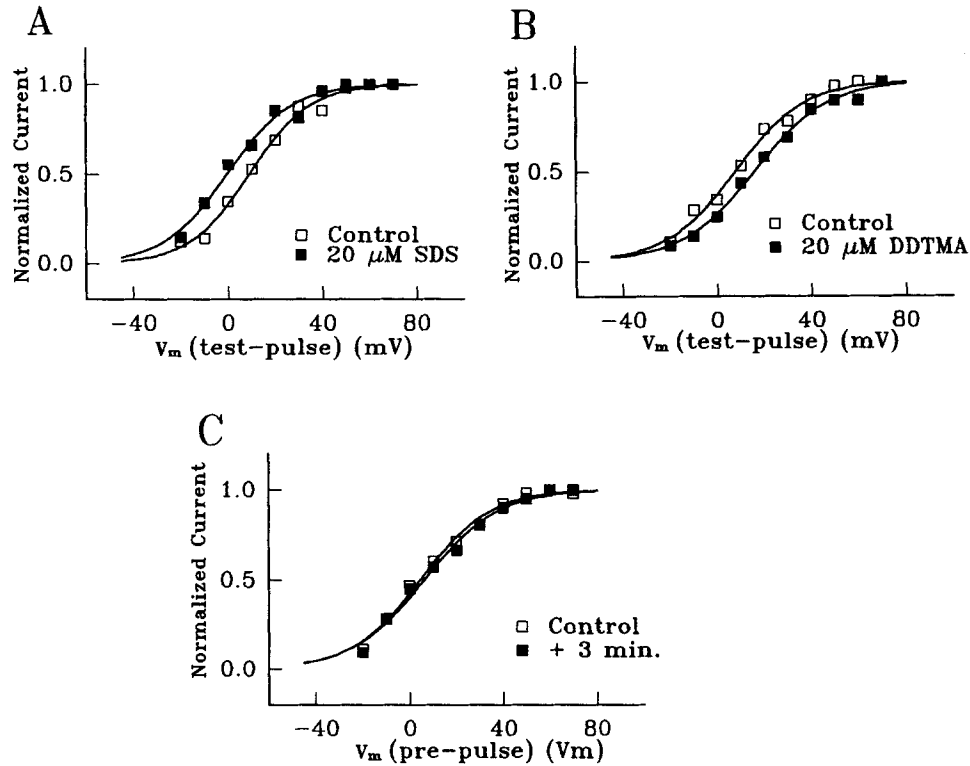


FIGURE 10. The effects of the amphiphiles on the normalized tail currents of the delayed rectifier potassium current. The tail currents were normalized to the maximal value and plotted against the test potentials. Open symbols ( $\square$ ) are the recordings under control conditions and solid symbols ( $\blacksquare$ ) are the experimental data points 3 min after exposure to either 20  $\mu$ M SDS (A), 20  $\mu$ M DDTMA (B), or no amphiphile (C). The solid lines are the best fits to the Boltzmann relation.

phile treatment, no significant shift in  $V_{1/2}$  was observed over a comparable time period after the control recording (Fig. 10 C). Fig. 11 shows the  $I$ - $V$  relations of  $I_{K,del}$ . Under control conditions,  $I_{K,del}$  showed a notable rundown after breaking into the cell (Fig. 11 A), which is believed to be due to inadequate phosphorylation of channel proteins (Giles, Nakajima, Ono, and Shibata, 1989). However, the rundown of the current was not obviously altered by either amphiphile (Fig. 11, B and C). Consistent with the shifts in the voltage dependence of current activation, SDS increased and

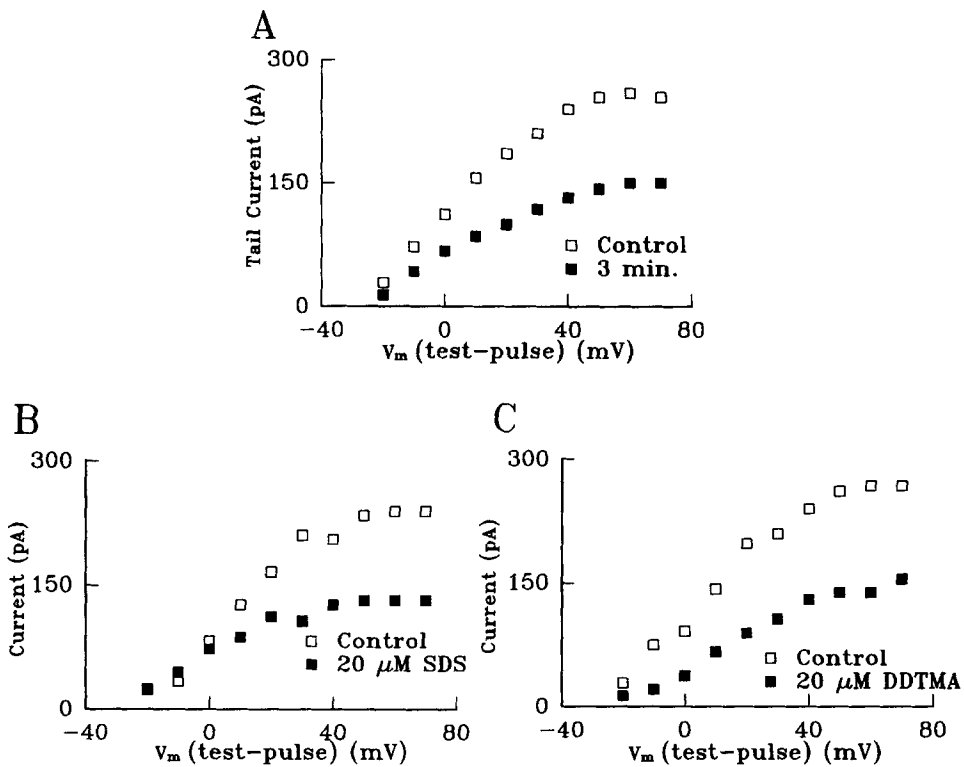


FIGURE 11. Effects of the amphiphiles on the magnitude of the tail currents of the delayed rectifier potassium current. The tail currents were measured arbitrarily at 6.9 ms after the end of the test pulse when the myocyte was clamped back to  $-30$  mV and plotted against the test potentials. Open symbols ( $\square$ ) are the recordings under initial control conditions and solid symbols ( $\blacksquare$ ) are the recordings 3 min later under the same control condition (A) or with exposure to  $20 \mu\text{M}$  SDS (B) or  $20 \mu\text{M}$  DDTMA (C).

DDTMA decreased the magnitude of  $I_{K,\text{tail}}$  over the membrane potential range from  $-20$  to  $20$  mV.

#### DISCUSSION

The importance of the surface potential in the modulation of voltage-dependent ionic currents has been long recognized (Frankenhauser and Hodgkin, 1957; Hille, 1992). In our previous studies (Ji et al., 1990; Post et al., 1991), we found that the steady-state kinetics of voltage-gated L-type  $\text{Ca}^{2+}$  current, and consequently the amplitude of the current, were altered by charged amphiphiles. We hypothesized that the changes in the steady-state gating were probably the consequence of the modification of surface potential by the charged amphiphiles inserting into the outer monolayer of the cell membrane. In this study, we have found that the charged amphiphiles also altered the amplitude and the voltage dependence of steady-state gating of both voltage-gated  $\text{Na}^+$  and delayed rectifier  $\text{K}^+$  currents in a manner

consistent with altered surface potential. This study therefore supports the idea that insertion of the amphiphiles occurs in the lipid environment surrounding  $\text{Na}^+$  and  $\text{K}^+$  channels, and is not just specific to the L-type  $\text{Ca}^{2+}$  channels. At this point, however, it cannot be concluded whether the insertion occurs in an evenly smeared or an uneven discrete manner. Finally, our study suggests that direct channel protein–amphiphile interactions are also likely to be present.

#### *Effects of the Amphiphiles on $I_{\text{Na}}$ and Surface Potential*

Similar to the effects on  $I_{\text{Ca,L}}$  (Ji et al., 1990; Post et al., 1991), the maximal peak  $I_{\text{Na}}$  was increased after superfusion of myocytes with negatively charged SDS, but decreased with positively charged DDTMA. These changes in the amplitude of the maximal peak current could be adequately explained by the shifts of the voltage dependence of current activation along the voltage axis (Fig. 3). In the case of SDS, a shift in the negative direction of the  $I_{\text{Na}}$  activation curve caused a larger fraction of channels to open at an equivalent membrane potential, increasing the whole-cell  $\text{Na}^+$  conductance at that membrane potential. As a consequence, the macroscopic current increased, according to the relation:  $I = G \times (V_m - E_{\text{ion}})$ , in which  $G$  is the whole-cell conductance (product of  $N$  [number of total functioning channels],  $\gamma$  [single channel conductance], and  $P_o$  [open probability of channels, or fraction of open channels]),  $V_m$  is the membrane potential, and  $E_{\text{ion}}$  is the reversal potential for the ion. The positively charged DDTMA, on the other hand, shifted the activation curve in the depolarizing direction and therefore produced an opposite effect: decrease of macroscopic current due to a decrease of  $P_o$ . The possibility that the amphiphiles affected the magnitude of macroscopic  $I_{\text{Na}}$  by altering  $\gamma$  and  $N$  is unlikely since the maximal whole-cell conductance was similar before and after exposure to SDS or DDTMA (Fig. 4). This is consistent with the observation that the  $I$ - $V$  plots before and after amphiphile treatment were closely superimposed once the current was fully activated above 0 mV (Fig. 2). The estimation that the extracellular mouth of the  $\text{Na}^+$  channel may protrude well beyond the diffuse double layer (Green, Weiss, and Andersen, 1987) would also make it unlikely that changes of  $[\text{Na}^+]$  in the diffuse double layer after the insertion of the amphiphiles might affect  $\gamma$ .

The shifts of the activation and inactivation of  $I_{\text{Na}}$  can be explained by a change of surface potential due to the intercalation of the charged amphiphiles into the outer monolayer of the sarcolemma. Under physiologic conditions, fixed negative surface charges at the aqueous faces of the membrane, carried by integral membrane proteins, sugar moieties, and phospholipids (see Introduction) are believed to produce local potentials (surface potentials) which construct an intramembrane field, electrostatically affecting the operation of voltage-sensitive membrane proteins. This is described by the following relation:

$$V_{\text{eff}} = V_m + (\psi_i - \psi_o) \quad (3)$$

in which  $V_{\text{eff}}$  is the overall effective potential across the membrane,  $V_m$  is the membrane potential measured in the bulk solutions inside and outside of the sarcolemma, and  $\psi_i$  and  $\psi_o$  are the surface potentials at the inner and outer surfaces of the membrane. After intercalation into the outer monolayer, negatively charged SDS should increase the negativity of  $\psi_o$  and reduce the difference between  $\psi_o$  and  $\psi_i$ ,

causing a partial depolarization of  $V_{\text{eff}}$  and consequently shifting the steady-state inactivation and activation in the hyperpolarizing direction. Positively charged DDTMA, on the other hand, is expected to produce opposite effects: a decrease in the negativity of  $\psi_0$  causing a partial hyperpolarization of  $V_{\text{eff}}$  and therefore a shift of the activation and inactivation curves in the depolarizing direction.

The effects of SDS on steady-state inactivation of  $I_{\text{Na}}$  were concentration dependent. This is consistent with the Gouy-Chapman-Stern surface potential theory (McLaughlin, 1977; Cevc, 1990), which predicts that the concentration of anions at the membrane surface ( $[A^-]_{x=0}$ ) is a function of the concentration of anionic amphiphiles in the bulk solution ( $[A^-]_{x=\infty}$ ), before reaching the maximum capacity of insertion. According to the theory, the surface charge density is related to surface potential by the relation (Graham, 1947):

$$\sigma^2 = 2\epsilon\epsilon_0RT \sum c_i[\exp(-z_i\psi_0F/RT) - 1] \quad (4)$$

where  $\sigma$  is the surface charge density,  $\psi_0$  is the surface potential,  $\epsilon$  is the dielectric constant for aqueous solution,  $\epsilon_0$  is the permittivity of free space,  $c_i$  is the concentration of the  $i$ th ion in the bulk solution, and  $z_i$  is the valence of the  $i$ th ion. When an anionic amphiphile is added,  $\sigma$  will be changed after the absorption of the anion to the membrane according to:

$$\sigma' = (1/K)(\sigma'_{\text{max}} - \sigma')[A^-]_{x=0} \quad (5)$$

where  $\sigma'$  is the charge density of the amphiphiles absorbed per unit area,  $\sigma'_{\text{max}}$  is the maximum absorption,  $K$  is the dissociation constant, and  $[A^-]_{x=0}$  is a function of  $[A^-]_{x=\infty}$  expressed via the Boltzmann relationship:

$$[A^-]_{x=0} = [A^-]_{x=\infty} \exp(\psi_0F/RT) \quad (6)$$

It is clear from Eqs. 5 and 6 that the total density of surface charges ( $\sigma + \sigma'$ ), and therefore the magnitude of surface potential, is dependent on the  $[A^-]_{x=\infty}$ . In our case,  $V_{1/2}$  of the steady-state inactivation of  $I_{\text{Na}}$  was progressively shifted in the negative direction as the concentration of SDS was increased from 20 to 100  $\mu\text{M}$ , consistent with a continuous absorption of anionic amphiphiles over this concentration range.

The ability of increased extracellular  $[\text{Ca}^{2+}]$  to partially reverse the shift in  $V_{1/2}$  of the steady-state inactivation of  $I_{\text{Na}}$  by SDS is also consistent with the idea that the effects of SDS on  $I_{\text{Na}}$  are mediated via changes in surface potential (Fig. 8A) since it is well known that  $\text{Ca}^{2+}$  screens negative surface charges (Hille et al., 1975). The screening effects of  $\text{Ca}^{2+}$  on the inserted anions (and the fixed surface charges as well) may only be fractional. This is due to the insertion of more SDS when  $\psi_0$  is reduced by the screening effects of  $\text{Ca}^{2+}$  since the insertion of SDS is also a function of  $\psi_0$  (Eq. 6). However, in Gouy-Chapman-Stern theory, the lipophilicity of negatively charged amphiphiles was not considered. The insertion of anionic amphiphiles may be dependent on this property as well as on  $\psi_0$ . This seems to be the case in this study because: (1) the shift of  $I_{\text{Na}}$  inactivation curve by SDS showed strong concentration dependence despite an increase of  $\psi_0$  in the negative direction resulted from the continuous insertion of SDS (Fig. 7); and (2) the shift was at least partially removed



by raising extracellular  $[Ca^{2+}]$  despite a decrease in the negativity of  $\psi_0$  due to the screening effect of  $Ca^{2+}$ , which would be expected to facilitate SDS insertion.

Besides the effects on the amplitude and steady-state gating of  $I_{Na}$ , the activation and inactivation kinetics of the current were also changed by the amphiphiles. Currents recorded at the same testing potential showed that both activation and inactivation were accelerated by SDS but slowed by DDTMA (Fig. 6 A).  $\tau_h$  was shifted in the hyperpolarizing direction by SDS but in the depolarizing direction by DDTMA (Fig. 6 B). The changes of both activation and inactivation kinetics of  $I_{Na}$  are consistent with the result of alterations of surface potential following amphiphile treatment. However, as shown by Fig. 6 B, the magnitude of shift in the time constants of inactivation was much greater than the shifts in the steady-state activation and inactivation. It is, therefore, tempting to speculate about the possibility that additional effects by the amphiphiles on the inactivation mechanism of the sodium channels were present (see below).

#### *Asymmetry of the Shifts by SDS and DDTMA*

Although shifts of steady-state activation and inactivation of  $I_{Na}$  can be attributed to surface potential alterations by the amphiphiles, the asymmetry between the effects of two compounds is inconsistent with the assumption that the amphiphiles exert their effects exclusively by modifying surface potential. In our previous work, both the steady-state activation and inactivation of  $I_{Ca,L}$  were similarly shifted by SDS and DDTMA by  $\sim 10$  mV (Ji et al., 1990; Post et al., 1991). This study shows that the shift in  $V_{1/2}$  of the  $I_{Na}$  activation curve ( $\sim 10$  mV) was less pronounced than that of the steady-state inactivation ( $\sim 20$  mV) or the time constants of the current inactivation ( $\sim 40$  mV; Figs. 3 A and 6 B) in the case of SDS, but more pronounced in the case of DDTMA. Similar asymmetrical shifts in  $I_{Na}$  activation and inactivation were also observed previously in several studies involving modification of surface potential by different agents ( $La^{3+}$ , Armstrong and Cota, 1990; trinitrobenzene sulphonic acid, Cahalan and Pappone, 1981;  $Ca^{2+}$ , Frankenhauser and Hodgkin, 1957;  $Zn^{2+}$ , Gilly and Armstrong, 1982), and may suggest that the electrical field sensed by the protein is very complex. One could also argue that these phenomena may reflect a different sensitivity of steady-state activation and inactivation of  $I_{Na}$  to surface potential alteration. However, this seems inconsistent with the substantial evidence that  $I_{Na}$  inactivation is not intrinsically voltage dependent, and that its apparent voltage dependence is related to the voltage dependence of  $I_{Na}$  activation (Armstrong and Bezanilla, 1977; Armstrong, 1981; Cota and Armstrong, 1989). Thus, to explain this asymmetry, it seems likely that the charged amphiphiles must interact directly with the charges borne by channel proteins, possibly via a mechanism involving electrostatic attraction or repulsion. One possibility is that the amphiphiles interact with fatty acids covalently linked to the Na channel protein. It is conceivable that the portion of the channel protein with which SDS interacts to influence the voltage dependence of steady-state inactivation is more positively charged than the site at which it interacts to influence activation. Then, because of electrostatic interaction, negatively charged SDS might accumulate to a greater extent at the site influencing inactivation than at the site influencing activation, causing a greater shift in the

voltage dependence of inactivation than activation. Since DDTMA is positively charged, it would be expected to have opposite effects, as was observed experimentally (Fig. 3). This hypothesis is consistent with the notion that activation and inactivation gates of voltage-dependent ion channels contain charged amino acid residues, such as lysines and arginines located in the S4 segment and the intracellular loop between domains 3 and 4 of the channel primary structure (Barchi, 1988; Catterall, 1988; Stühmer, Conti, Suzuki, Wang, Noda, Yahagi, Kubo, and Numa, 1989). Whether the amphiphiles could interact with the inactivation mechanism directly through the hydrophilic, pore-forming portion of the channel when it is open, or through the lipoprotein interface is speculative. It seems unlikely that the charged amphiphiles may gain access to the sodium channel when the voltage sensors are exposed to extracellular side during depolarization (Sammar, Spira, and Meiri, 1992) since the effects on the steady-state inactivation were not facilitated by a depolarizing train (Fig. 5).

#### *Effects on the Delayed Rectifier K<sup>+</sup> Current*

Effects of amphiphiles on the delayed rectifier K<sup>+</sup> current were studied in single ventricular myocytes from guinea pig since  $I_{K,del}$  is generally larger in this species than in rabbit ventricular myocytes (Sanguinetti and Jurkiewicz, 1990). Due to the slow activation and a rapid rundown of the current after the rupture of patch membrane, it was difficult to precisely quantitate the effects of amphiphiles on the current. However, as shown in Fig. 11, neither SDS nor DDTMA seemed to alter the rundown of  $I_{K,del}$ . Despite this,  $I_{K,del}$  was increased by SDS and decreased by DDTMA in a voltage-dependent manner over the range of membrane potentials from -20 to 20 mV. The changes of  $I_{K,del}$  over this membrane potential range could be explained by the shift of  $I_{K,del}$  activation along the voltage axis, in the hyperpolarizing direction in the case of SDS and in the depolarizing direction in the case of DDTMA, similar to the effects on  $I_{Na}$  activation produced by the amphiphiles. This is consistent with our hypothesis of an alteration of surface potential due to the insertion of charged amphiphiles around ion channels.

In summary, our observations demonstrate that the effects of the charged amphiphiles on the amplitude of  $I_{Na}$  and  $I_{K,del}$  can be largely explained by the alterations in their voltage-dependent steady-state gating due to a modification of surface potential after the insertion of amphiphiles into the outer monolayer of the membrane in the myocytes, which is consistent with the notion that the voltage-dependent gating mechanisms of these channels are located within the electrical field established by surface potential. It is therefore indicated, although indirectly, that the charges carried by membrane lipids are of significance in the modulation of channel gating. This agrees well with experiments in lipid planar bilayers, which have shown that channel gating mechanisms, unlike ion permeation properties, are influenced by lipid charges (Green et al., 1987; Cukierman et al., 1988). These charged amphiphiles may be useful as a tool to modify the density of surface charges in order to observe the interaction between surface charges and channel proteins. Besides the effects on surface potential, however, in the case of  $I_{Na}$ , a direct electrostatic interaction between the amphiphiles and channel gating mechanisms appears highly likely. Finally, the marked effects of these amphiphiles on cardiac excitation-

contraction coupling (Post et al., 1991) demonstrate that modification of surface charge can markedly influence physiological function. It is intriguing to speculate that alterations of surface potential under pathophysiological conditions, such as cardiac ischemia, in which dramatic changes in membrane phospholipid content occur, may contribute to altered cardiac function in these settings.

This work was supported by USPHS grant HL-28539-10 and the Castera Endowment (to G. A. Langer), by NIH grants RO1 HL-37629 and RO1 HL-88440, and Research Career Development Award KO4 HL-01890 and the Chizuko Kawata Endowment (to J. N. Weiss), and by the Laubisch Cardiovascular Research Fund.

*Original version received 4 May 1992 and accepted version received 25 November 1992.*

#### REFERENCES

- Armstrong, C. M. 1981. Sodium channels and gating currents. *Physiological Reviews*. 61:644–683.
- Armstrong, C. M., and F. Bezanilla. 1977. Inactivation of the sodium channel. II. Gating current experiments. *Journal of General Physiology*. 70:567–590.
- Armstrong, C. M., and G. Cota. 1990. Modification of sodium channel gating by lanthanum. Some effects that cannot be explained by surface charge theory. *Journal of General Physiology*. 96:1129–1140.
- Armstrong, C. M., and D. R. Matterson. 1986. The role of calcium ions in the closing of K channels. *Journal of General Physiology*. 87:817–832.
- Balsler, J. R., P. B. Bennett, and D. M. Roden. 1990. Time-dependent outward current in guinea pig ventricular myocytes. Gating kinetics of the delayed rectifier. *Journal of General Physiology*. 96:835–863.
- Barchi, R. L. 1988. Probing the molecular structure of the voltage-dependent sodium channel. *Annual Review of Neuroscience*. 11:455–495.
- Burt, J. M., and G. A. Langer. 1983. Ca<sup>2+</sup> displacement by polymyxin B from sarcolemma isolated by 'gas-dissection' from cultured neonatal rat myocardial cells. *Biochimica et Biophysica Acta*. 729:44–52.
- Cahalan, M. D., and P. A. Pappone. 1981. Chemical modification of sodium channel surface charges in frog skeletal muscle by trinitrobenzene sulphonic acid. *Journal of Physiology*. 321:127–139.
- Campbell, D. T., and R. Hahin. 1984. Altered sodium and gating current kinetics in frog skeletal muscle caused by low external pH. *Journal of General Physiology*. 84:771–788.
- Catterall, W. A. 1988. Structure and function of voltage-sensitive ion channels. *Science*. 242:50–61.
- Cevc, G. 1990. Membrane electrostatics. *Biochimica et Biophysica Acta*. 1031:311–382.
- Cota, G., and C. M. Armstrong. 1989. Sodium channel gating in clonal pituitary cells. The inactivation step is not voltage-dependent. *Journal of General Physiology*. 94:213–232.
- Cukierman, S., W. C. Zinkand, R. J. French, and B. K. Krueger. 1988. Effects of membrane surface charge and calcium on the gating of rat brain sodium channels in planar bilayers. *Journal of General Physiology*. 92:431–447.
- Frankenhauser, B., and A. L. Hodgkin. 1957. The action of calcium on the electrical properties of squid axons. *Journal of Physiology*. 137:218–244.
- Giles, W., T. Nakajima, K. Ono, and E. F. Shibata. 1989. Modulation of the delayed rectifier K<sup>+</sup> current by isoprenaline in bull-frog atrial myocytes. *Journal of Physiology*. 415:233–249.
- Gilly, W. F., and C. M. Armstrong. 1982. Slowing of sodium channel opening kinetics in squid axon by extracellular zinc. *Journal of General Physiology*. 79:935–964.
- Graham, D. C. 1947. The electrical double layer and the theory of electrocapillarity. *Chemical Reviews*. 41:441–501.

- Green, W. N., and O. S. Andersen. 1991. Surface charges and ion channel function. *Annual Review of Physiology*. 53:341–359.
- Green, W. N., L. B. Weiss, and O. S. Andersen. 1987. Batrachotoxin-modified sodium channels in planar lipid bilayers. Ion permeation and block. *Journal of General Physiology*. 89:841–872.
- Hahin, R., and D. T. Campbell. 1983. Simple shifts in the voltage dependence of sodium channel gating caused by divalent cations. *Journal of General Physiology*. 82:785–805.
- Hamill, O. P., A. Marty, E. Neher, B. Sakmann, and F. J. Sigworth. 1981. Improved patch-clamp techniques for high-resolution current recording from cells and cell-free membrane patches. *Pflügers Archiv*. 391:85–100.
- Helenius, A., D. R. McCaslin, E. Fries, and C. Tanford. 1979. Properties of detergents. *Methods in Enzymology*. 56:734–749.
- Hille, B. 1992. *Ionic Channels of Excitable Membranes*. 2nd ed. Sinauer Associates, Inc., Sunderland, MA. 607 pp.
- Hille, B., A. M. Woodhull, and B. I. Shapiro. 1975. Negative surface charge near the sodium channels of nerve: divalent ions, monovalent ions, and pH. *Philosophical Transactions of the Royal Society of London, Series B*. 270:301–318.
- Hodgkin, A. L., and A. F. Huxley. 1952. A quantitative description of membrane current and its application to conduction and excitation in nerve. *Journal of Physiology*. 117:500–544.
- Ji, S., J. N. Weiss, and G. A. Langer. 1990. Effect of amphiphiles on calcium currents in rabbit ventricular myocytes. *Biophysical Journal*. 57:526a. (Abstr.)
- Ji, S., J. N. Weiss, and G. A. Langer. 1992. Charged amphiphiles alter steady-state gating of ionic currents in cardiac ventricular myocytes. *Biophysical Journal*. 61:394a. (Abstr.)
- Kornfeld, R., and S. Kornfeld. 1985. Assembly of asparagine-linked oligosaccharides. *Annual Review of Biochemistry*. 54:631–664.
- Kyte, J., and R. F. Doolittle. 1982. A simple method for displaying the hydropathic character of protein. *Journal of Molecular Biology*. 157:105–132.
- Langer, G. A., and T. L. Rich. 1986. Augmentation of sarcolemmal  $\text{Ca}^{2+}$  by anionic amphiphile: contractile responses of three ventricular tissues. *American Journal of Physiology*. 250 (*Heart and Circulatory Physiology* 19):H247–H254.
- Levinson, S. R., W. B. Thornhill, D. S. Duch, E. Recio-Pinto, and B. W. Urban. 1990. The role of nonprotein domains in the function and synthesis of voltage-gated sodium channels. In *Ion Channels*. T. Narahashi, editor. Plenum Publishing Corp., New York. 33–64.
- Mato, J. M. 1990. *Phospholipid Metabolism in Cellular Signalling*. CRC Press, Inc., Boca Raton, FL. 145 pp.
- Matsuura, H., T. Ehara, and Y. Imoto. 1987. An analysis of the delayed outward current in single ventricular cells of the guinea pig. *Pflügers Archiv*. 410:596–603.
- McLaughlin, S. 1977. Electrostatic potentials at membrane-solution interfaces. *Current Topics in Membranes and Transport*. 9:71–144.
- McLaughlin, S., G. Szabo, and G. Eisenman. 1971. Divalent ions and the surface potential of charged phospholipid membrane. *Journal of General Physiology*. 58:667–687.
- Mitra, R., and M. Morad. 1985. A uniform enzymatic method for dissociation of myocytes from hearts and stomachs of vertebrates. *American Journal of Physiology*. 249 (*Heart and Circulatory Physiology* 18):H1056–H1060.
- Nillius, B. 1988. Calcium block of guinea pig heart sodium channels with and without modification by the piperazinyllindole DPI 201-106. *Journal of Physiology*. 399:537–558.
- Perozo, E., F. Bezanilla, and R. Dipolo. 1989. Modulation of K channels in dialyzed squid axons. ATP-mediated phosphorylation. *Journal of General Physiology*. 93:1195–1218.

- Philipson, K. D., G. A. Langer, and T. L. Rich. 1985. Charged amphiphiles regulate heart contractility and sarcolemma- $\text{Ca}^{2+}$  interactions. *American Journal of Physiology*. 248(*Heart and Circulatory Physiology* 17):H147–H150.
- Post, J. A., S. Ji, K. S. Leonards, and G. A. Langer. 1991. Effects of charged amphiphiles on cardiac cell contractility are mediated via effects on  $\text{Ca}^{2+}$  current. *American Journal of Physiology*. 260(*Heart and Circulatory Physiology* 29):H759–H769.
- Sammar, M., G. Spira, and H. Meiri. 1992. Depolarization exposes the voltage sensor of the sodium channels to the extracellular region. *Journal of Membrane Biology*. 125:1–11.
- Sanguinetti, M. C., and N. K. Jurkiewicz. 1990. Lanthanum blocks a specific component of  $I_K$  and screens surface charge in cardiac cells. *American Journal of Physiology*. 259(*Heart and Circulatory Physiology* 28):H1881–H1889.
- Storch, J., and A. M. Kleinfeld. 1985. The lipid structure of biological membrane. *Trends in Biological Science*. 10:418–421.
- Stühmer, W., F. Conti, H. Suzuki, X. Wang, M. Noda, N. Yahagi, H. Kubo, and S. Numa. 1989. Structural parts involved in activation and inactivation of the sodium channel. *Nature*. 339:597–603.
- Yamamoto, D., J. Z. Yeh, and T. Narahashi. 1984. Voltage-dependent calcium block of normal and tetramethrin-modified single sodium channels. *Biophysical Journal*. 45:337–344.
- Yamamoto, D., J. Z. Yeh, and T. Narahashi. 1985. Interactions of permeant cations with sodium channels of squid axon membranes. *Biophysical Journal*. 48:361–368.
- Yee, H. F., J. N. Weiss, and G. A. Langer. 1989. Neuraminidase selectively enhances transient  $\text{Ca}^{2+}$  current in cardiac myocytes. *American Journal of Physiology*. 256(*Cell Physiology* 25):C1267–C1272.
- Zhang, J.-F., and S. A. Siegelbaum. 1991. Effects of external protons on single cardiac sodium channels from guinea pig ventricular myocytes. *Journal of General Physiology*. 98:1065–1083.