



Skeletal Muscle O₂ Diffusion and the Limitation of Aerobic Capacity in Heart Failure: A Clarification

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INTRODUCTION

The capacity to convey oxygen (O₂) from the atmosphere in to mitochondria essentially determines maximal aerobic metabolism in humans (1–6). The inherent constitution of the O₂ transport and utilization chain is asymmetrical, not all steps have the same importance (7, 8). Intracellular biochemical mechanisms that could in theory limit O₂ utilization are overbuilt in relation to the potential delivery of O₂ through the circulatory system (2, 3, 9). Peak oxygen consumption (VO_{2peak}), a hallmark of aerobic capacity elicited by incremental exercise involving more than half of total muscle mass, is mainly determined by the circulatory capacity to deliver O₂ to working muscle even in the presence of compromised muscle oxidative capacity (5, 7, 8). Glaring evidence of the impact of the circulatory system on VO_{2peak} includes conditions such as heart failure (HF), intrinsically linked with impaired cardiac output and thus limited convective O₂ delivery (2, 6). VO_{2peak} is a strong and independent predictor of survival in HF patients used to determine eligibility for cardiac transplantation (6, 10, 11). After diagnosis of HF, survival estimates do not exceed 50% at 5 years (12, 13).

Understanding the physiology of O₂ delivery and thereby VO_{2peak} in HF may facilitate the identification of target mechanisms and the advent of effective treatments. While classic empirical studies in HF patients support the primary role of impaired cardiac pumping capacity in the limitation of VO_{2peak} (14, 15), a recent paradigm based on theoretical assumptions attribute the main importance to skeletal muscle abnormalities in O₂ diffusion from capillaries in to mitochondria (16). Given the radical change of rehabilitation programs implicit in the “skeletal muscle” paradigm, herein we sought to shed light on the foundation of this relatively new tenet in the HF field. In particular, a fundamental aspect will be clarified: the measurement and calculation of O₂ diffusion in skeletal muscle.

O₂ TRANSPORT ASSESSMENT: DE FACTO MEASUREMENT OF O₂ DIFFUSION IN SKELETAL MUSCLE

The transport of O₂ in living organisms follows well-known physical phenomena. O₂ molecules move via (i) convection, due to the bulk motion of fluids, and (ii) diffusion, spontaneously spreading out from a region of high concentration to a region of low concentration. Along the O₂ cascade, convection is the mode of O₂ transport between the atmosphere and the lungs, and between pulmonary capillary blood and tissue microvascular beds, respectively determined by the bulk motion of air and circulating blood. Diffusion of O₂ mainly occurs from alveoli in to pulmonary capillaries, and from tissue microvascular beds in to mitochondria. With respect to the measurement of O₂ transport, both convection steps (air-to-lung, blood circulation) can be measured with relatively high accuracy in humans by means of spirometers, air/blood gas analyzers,

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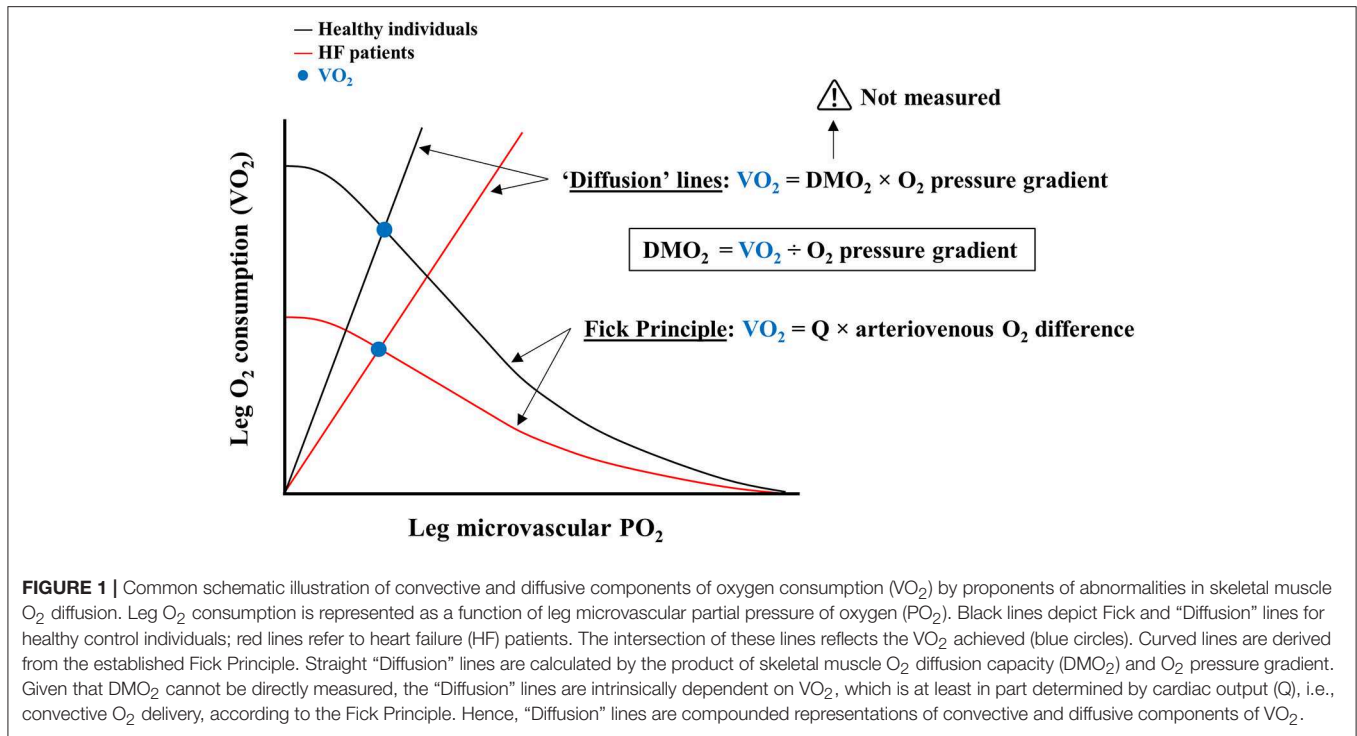
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arterial/venous blood samples and indicator-dilution/ultrasound techniques (17, 18). These well-established research methods may also be used to assess lung O₂ diffusion. The final O₂ diffusion step in the skeletal muscle microcirculation, however, cannot yet be directly measured. The level of resolution required to capture O₂ extraction in microvessels supplying active muscle fibers is beyond reach owing to technical limitations including temporal and spatial constraints (8, 19).

The possibility seemingly exists, nonetheless, to make use of partial measurements and multiple assumptions to deliver a quantitative value for skeletal muscle O₂ diffusion capacity (DMO₂) (20–22). Notably, in the field of HF (16), some clinical researchers are currently applying a method for estimating DMO₂ conceived almost 3 decades ago (20–22). Herein, DMO₂ is portrayed as the ratio of skeletal muscle O₂ consumption (VO₂) and O₂ pressure gradient between microvessels and mitochondria (21, 23, 24).

$$DMO_2 = \frac{\text{skeletal muscle } VO_2}{O_2 \text{ pressure gradient}}$$

At first sight the notion of DMO₂ appears consistent, albeit a close scrutiny of the actual measurements reveals salient incongruences. Skeletal muscle O₂ consumption—calculated by the product of leg blood flow (LBF) and the difference between femoral arterial and venous O₂ content (16, 21)—is primarily determined by convective O₂ delivery, since LBF is substantially impaired (up to –40%) in HF conforming to the reduced pumping capacity of the failing heart (6, 25). Moreover, femoral vein O₂ content is close to zero in HF patients at VO_{2peak} (2). Therefore, the first component (numerator) of

the DMO₂ equation, i.e., skeletal muscle VO₂, is essentially a function of convective O₂ delivery (LBF × arterial O₂ content) a fundamental mathematical flaw for a variable claimed to represent diffusive O₂ transport (Figure 1).

The O₂ pressure gradient between skeletal muscle microvessels and mitochondria is also estimated from femoral arterial and venous O₂ content measurements, both pertaining to the macro- instead of microcirculation (16, 21). A myriad of assumptions are thus necessary to infer the postulated denominator of the DMO₂ equation (20). For instance, the inherent heterogeneity of leg microvascular blood flow (26, 27), which even at VO_{2peak} perfuses tissues (e.g., adipose tissue, bone, inactive muscle) not demanding a high VO₂, is neglected (20, 21). Similarly, altered capillarization as well as anatomical and/or functional shunting within the lower limb, which may have a substantial influence in HF patients at VO_{2peak} (28, 29), is ignored (16, 21). Taken together, the estimation of the O₂ pressure gradient entails as a necessary premise that all blood flow downstream of the femoral artery perfuses active muscle fibers, in a perfect match between O₂ delivery and metabolic demand, an untenable shortcoming (26–28).

Considering the actual measurements underpinning the concept of DMO₂, its mathematical equation would be more accurately expressed as:

$$DMO_2 = \frac{LBF \times \text{arteriovenous } O_2 \text{ difference}}{\text{Blood flow distribution} \times O_2 \text{ pressure gradient}}$$

Hence, the numerator and denominator of DMO₂ comprise variables reflecting convective O₂ delivery, LBF and blood flow distribution, respectively. The observation of reduced DMO₂

in HF patients is therefore not surprising (16, 23, 24). To conclude from these studies that mechanisms underlying skeletal muscle O₂ diffusion should be primarily targeted for therapy is questionable (30). Caution should be taken in the interpretation of lower DMO₂ in HF patients, which can be largely attributed to abnormalities in convective O₂ delivery, let alone presenting DMO₂ results as the main buttress of a new paradigm (31, 32). Further research taking advantage of technological developments

in measurement accuracy and resolution of O₂ dynamics in skeletal muscle will have to elucidate its role in the limitation of VO_{2peak} in HF populations.

AUTHOR CONTRIBUTIONS

DM and CD-C contributed to study design, interpretation, and manuscript writing.

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