

Estimation of maximum lower limb muscle strength from vertical jumps

Chuan-Fang Hou^{1‡}, Chin-Wei Hsu², Philip X. Fuchs₆, Tzyy-Yuang Shiang₆^{2*}

- 1 Department of Physical Education and Sport Sciences, National Taiwan Normal University, Taipei, Taiwan, 2 Department of Sport and Kinesiology, National Taiwan Normal University, Taipei, Taiwan
- ‡ These author share first authorship on this work.
- * tyshiang@gmail.com (TYS); philip.fuchs@ntnu.edu.tw (PHF)





Citation: Hou C-F, Hsu C-W, Fuchs PX, Shiang T-Y (2025) Estimation of maximum lower limb muscle strength from vertical jumps. PLoS ONE 20(2): e0316636. https://doi.org/10.1371/journal.pone.0316636

Editor: Mário Espada, Instituto Politecnico de Setubal, PORTUGAL

Received: March 30, 2024

Accepted: December 13, 2024

Published: February 27, 2025

Copyright: © 2025 Hou et al. This is an open access article distributed under the terms of the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original author and source are credited.

Data availability statement: All relevant data are within the manuscript and its <u>Supporting</u> <u>Information</u> files.

Funding: This work was financially supported by the National Taiwan Normal University (NTNU) within the framework of the Higher Education Sprout Project by the Ministry of Education (MOE) in Taiwan. This funding was received by Drs. Tzyy-Yuang Shiang and Philip X. Fuchs.

Abstract

Determining the one-repetition maximum (1RM) is crucial for organizing training loads, but it also is time-consuming, physically demanding, and poses a risk of injury. Vertical jumps are a less demanding and well-established method to test the ability of the lower limbs to generate great forces over a short time, which may allow for the estimation of 1RM in squatting. The purpose of this study was to develop a model for estimating 1RM back squat from ground reaction forces during vertical jumps. Thirteen healthy participants completed a 1RM back squat test, countermovement jumps, and squat jumps. Five kinematic and kinetic variables (e.g., peak and mean power, relative net impulse, jump height, and peak kinetic energy during various phases) were derived from ground reaction forces collected via a Kistler force plate (1000 Hz). Five out of 5 variables correlated with 1RM in countermovement jump and squat jump (ICC = .96-.98, r = .88-.95, p < .001 and ICC = .97-.99, r = .76-.90, p = .76-.90< .05, respectively). The most accurate stepwise regression model (adjusted $R^2 = .90$, SEE =13.24 kg, mean error = 7.4% of mean $1RM_m$, p < .001) estimated 1RM back squat based on peak kinetic energy during countermovement jumps. Estimation errors ranged from 7.4% to 10.7% of mean measured 1RM, with no differences between estimated and measured values (d < 0.01, p = .96-1.00). Estimating 1RM via jump tests may offer a practical alternative to traditional methods, reducing injury risks, testing intervals, and effort. Our study proposes a new possible approach for estimating 1RM back squat from jump forces, providing coaches and sports professionals with a more efficient tool to monitor and adjust training loads.

Introduction

Muscle strength is crucial for both general physical fitness and athletic performance. Maintaining muscle strength is essential for functional health throughout various life stages, including childhood, youth, adolescence, and old age [1-3]. In children, youth, and adolescents, lower extremity muscle strength is key to motor skill development and physical fitness [4]. For the elderly, a decline in lower extremity muscle strength increases the risk of falls, frailty, and functional impairments [5,6]. In athletes, the scientific analysis and monitoring of lower extremity muscle strength are integral to their training regimes. High-quality muscle strength contributes to muscle power, rate of force development, jump height, dynamic changes of direction, and overall sports performance economy [7-10]. Additionally, functional muscle

Competing interests: The authors have declared that no competing interests exist.

strength plays a critical role in absorbing impacts and distributing forces, which helps in preventing sports-related overuse injuries [11].

Resistance training encompassing free weights, weight machines, medicine balls, elastic tubing devices, and one's own body weight is widely regarded as the optimal approach for enhancing muscle strength [12]. Assessing muscle strength is crucial for evaluating muscular capabilities and the designing effective strength training programs. The one-repetition maximum (1RM) back squat test serves as the traditional gold standard for assessing lower limb maximal muscle strength performance, known for its high validity and reliability [13-15]. The 1RM is also well-established in training practices as many training protocols define training loads relative to the 1RM. However, determining the 1RM can be time-consuming, physically demanding, and carries a risk of overload injuries [5,16]. Additionally, the 1RM back squat needs to be repeated frequently for monitoring purposes, which may not only increase the time and physical demands but also require adjustments to regular strength training regimens and the associated effort. Finally, 1RM testing is also associated with injury risks that can be avoided through a single jump test. The vertical jump, involving explosive extension of the hips, knees, and ankles, closely resembles the back squat movement [17]. Consequently, the vertical jump test, including the countermovement jump (CMJ) and squat jump (SJ), has been used for decades as an alternative method to assess lower limb dynamic performance. Compared to the 1RM back squat test, jump tests are more convenient, less time-intensive, impose less physical strain, and entail a lower risk of injury.

The CMJ involves a downward movement of the center of mass (COM) followed by a maximal vertical upward movement of the COM. This process, known as the stretch-shortening cycle (SSC), enhances the storage and release of elastic energy during the transition from eccentric to concentric contractions in the lower limb muscles [18]. In contrast, the SJ consists solely of an upward concentric movement of the COM, emphasizing the capacity of the lower limb muscles to produce force during a concentric-only action [19]. The CMJ includes phases of weighting, unweighting, braking, propulsion, flight, and landing. In comparison, SJ involves only the propulsion, flight, and landing phases. Additionally, ground reaction force (GRF) variables derived from these different phases of vertical jumps provide valuable insights into the characteristics of lower extremity strength, power, and fatigue [20–24]. The main categories of variables include force, velocity, power, impulse, work, kinetic energy, jump height, and countermovement depth. Previous studies have developed prediction equations that incorporate body mass alongside vertical jump height to estimate peak power in the lower extremities across diverse populations [4,25–31,]. To date, no research has investigated the estimation of 1RM back squat based on GRF variables during vertical jumps.

Power, impulse, jump height, and kinetic energy derived from GRF variables are regarded as essential metrics representing kinetics and kinematics in vertical jumps [32,33]. These metrics reflect the combined characteristics of force production, velocity optimization, and energy utilization in the lower limb muscles, which are crucial for explosive movements [34–41]. Peak power and jump height have been found to strongly correlate with 1RM back squat performance and maximal strength improvements, underscoring their relevance for assessing lower body strength, as they represent the explosive force and displacement capacity required for heavy lifts [38,40]. Additionally, mean power has been proposed as a metric for monitoring neuromuscular performance, as it directly reflects explosive strength capabilities over a sustained period, which is necessary for consistent power output during a 1RM back squat [36,41]. Relative net impulse and peak kinetic energy play essential roles in determining vertical jump performance, capturing the force exerted over time and energetic capacity during movement, which are fundamental for effective force transfer during strength exercises like the back squat [33,39]. In summary, these variables from vertical jumps represent maximal and explosive lower extremity neuromuscular capacity and may have the potential to estimate 1RM back squat performance.

Therefore, the purpose of this study was to estimate the 1RM back squat based on GRF variables (peak and mean power, relative net impulse, jump height, and peak kinetic energy) measured during CMJ and SJ. The hypotheses were as follows: 1) There will be correlations between the GRF variables of vertical jumps and 1RM back squat; 2) A predictive formula can be developed to estimate 1RM back squat from the GRF variables measured during a maximum vertical jump test.

Materials and methods

Participants

An a-priori power analysis (G*Power 3.1, Düsseldorf, Germany) indicated that a sample size of 11 participants would achieve the desired power of 0.80 at alpha = 0.05 to detect F-test effect sizes f^2 of 1.50 and higher for the main test of this study involving two predictors. The effect size $f^2 = 1.50$ is the equivalent of $R^2 = 0.60$, explaining 60% of the variance. This effect size is generally considered large, which means that smaller effects may remain undetected. However, this threshold is below the expected and acceptable results reported in previous studies that developed similar estimation equations with also two predicators for related context, namely lower body power in vertical jumping (R²: 0.74–0.93; 2 predictors) [28,29,42,43]. Therefore, although this sample size may miss detecting small and moderate effects, it was sufficient to reliably detect the expected and practically relevant effects. The current sample size also meets the recommended requirement of a minimum sample of n = 8 for regression estimations based on low-variance samples [44], which is the case in our study. Thirteen healthy adults, actively involved in frequent strength training (2-6 times/week), participated in this study (age: 23.4 ± 0.7 years, body height: 171.6 ± 5.7 cm, body mass: 70.8 ± 10.2 kg, 1RM back squat: 1.7 ± 0.4 BW, ten males and three females, recruitment period: 2018/08/15– 2018/12/15). None of the participants had engaged in weight training within 24 hours before the experiment as per the protocol by Wang et al. [45]. All participants were provided with detailed information regarding the risks and benefits associated with their involvement. The Human Research Ethics Committee of National Taiwan Normal University provided written approval of the study (approval number: 201803HM001) in accordance with the Declaration of Helsinki. All participants signed a written consent before the experiment and declared to be free of injuries.

Data collection

A cross-sectional study was designed to estimate the 1RM back squat based on GRF-derived variables during CMJ and SJ. The study comprised two parts: first, a 1RM back squat test; second, maximal vertical CMJ and SJ tests (randomized order) on a force plate. The maximal vertical jump tests were conducted within 2–7 days after the 1RM back squat test. Subsequently, the data were analyzed using stepwise linear regression models to develop estimation equations for the 1RM back squat based on CMJ and SJ performance. And the researcher was blinded to which participant the estimation was for.

Each participant initiated the study with a 1RM back squat test, using a barbell. This test followed a familiarization session and a standardized warm-up protocol that included both general warm-up and dynamic stretching routines. The test procedure adhered to the National Strength and Conditioning Association (NSCA) guidelines [46]: (1) commence with a light resistance, allowing participants to perform 5–10 repetitions easily, (2) rest for one minute, (3) gradually increase the weight by 10–20% and assess the participant's 3–5RM, (4) rest for two minutes, (5) gradually increase the weight by 10–20% and assess the participant's 2–3RM, (6) rest for 2–4 minutes, (7) gradually increase the weight

by 10–20%, (8) instruct participants to aim for a 1RM, (9) if the attempt was successful, rest for 2–4 minutes and return to step 7; otherwise, rest for 2–4 minutes, reduce the weight by 5–10%, and repeat step 8, (10) continue adjusting the load until participants can successfully complete one repetition with proper technique within a maximum of five trials.

During the maximal vertical jump test, all participants underwent a standardized warm-up procedure that included stretching, dynamic lower limb exercises, and jumps. Each participant completed three CMJ and three SJ in a random order, as outlined by Bender [18,19,47]. Participants were allowed to rest for three minutes between jumps. Before initiating each jump, participants were instructed to stand still for five seconds to prepare for the jump. During the jumps, participants were directed to keep their hands on their hips, jump as high as possible, and maintain a stationary stance for at least five seconds after landing, following previous guidelines [47]. GRF data were recorded and processed via a Kistler force plate model 9827 (Kistler Holding AG, Winterthur, Switzerland) (90x60 cm) at a sampling frequency of 1000 Hz (Figs 1 and 2) with BioWare software (Kistler Instruments Inc., Type 2812A, Version 5.4.3.0, Winterthur, Switzerland). The GRF-time profiles were analyzed to ensure compliance with the instructions. Trials were repeated if deviations from the instructions were observed. The highest CMJ and SJ values were selected for subsequent statistical analysis.

Data processing

<u>Figs 1</u> and <u>2</u> illustrate the phases and GRF variables and COM position of CMJ and SJ based on prior research [<u>33,35,36,48</u>–<u>54</u>]. These phases included:

- 1. Weighting phase: from beginning of the GRF data collection to the initial start of the vertical jump movement (CMJ and SJ: from the start of GRF data collection to point A)
- 2. Unweighting phase: from the initial start of the vertical jump movement through to the instant at which force returns to BW (CMJ: points A to C)

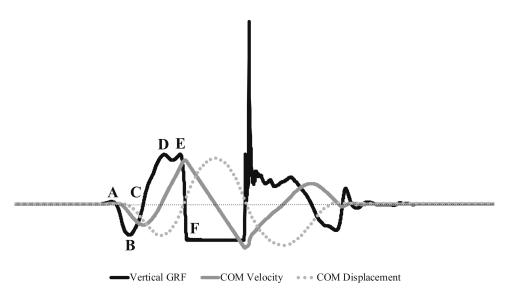


Fig 1. Vertical GRF force-time curve, COM vertical velocity, and COM vertical displacement of CMJ. Beginning to point A: weighting phase. Points A to C: unweighting phase. Points C to point D: braking phase. Points D to F: propulsion phase.

https://doi.org/10.1371/journal.pone.0316636.g001

- 3. Braking phase: from the instant of peak negative COM velocity through to when COM velocity increases to zero (CMJ: points C to D)
- 4. Propulsion phase: starts when a positive COM velocity is achieved and continues through to the instant of take-off (CMJ: points D to F; SJ: points A to C)

Body weight was determined during the first 500 data points of vertical GRF during the weighting phase [35]. The start of the jump was defined as the time point 30 ms before the vertical GRF exceeded the threshold (the total system weight \pm 5 SD). Take-off was identified as the moment when the vertical GRF decreased to < 20 N after the start of the propulsion phase [40]. The selected GRF variables included peak and mean power, relative net impulse, jump height, and peak kinetic energy.

The following definitions clarify the variables:

- Peak power: The maximum power from the unweighting to the propulsion phases in CMJ and during the propulsion phase in SJ
- Mean power: The average power from the unweighting to the propulsion phases in CMJ and during the propulsion phase in SJ
- Relative net impulse: The total impulse from the unweighting to the propulsion phases/ jumper's body mass in CMJ and during the propulsion phase/ jumper's body mass in SJ
- Jump height: Calculated using the equation: $JH = V_{TO}^2 / 2g$ (where $V_{TO} = COM$ vertical velocity at take-off and g is the acceleration due to gravity)
- Peak kinetic energy: Calculated as PKE = 1/2 mv²_{Peak} (where m = body mass and V_{Peak} = Peak COM vertical velocity: The maximum vertical velocity of the COM from the unweighting to the propulsion phases in CMJ and during the propulsion phase in SJ)

Previous studies showed that these variables respond to training interventions $[\underline{17,55-58}]$, which underlines the practical relevance of including those variables in the current investigation.

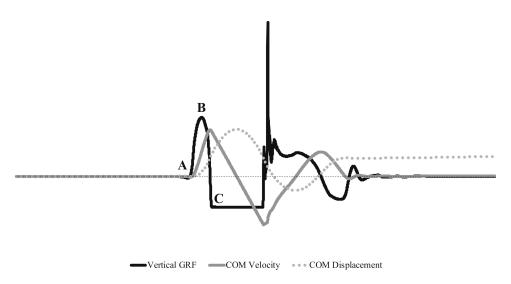


Fig 2. Vertical GRF force-time curve, COM vertical velocity, and COM vertical displacement of SJ. Beginning to Point A: weighting phase. Points A to C: propulsion phase.

https://doi.org/10.1371/journal.pone.0316636.g002

Statistical analyses

After obtaining and processing GRF via BioWare software, data were merged and organized via Microsoft Excel for further analysis. Statistical analysis was conducted via SPSS software version 23 (IBM Corp., Armonk, NY, USA). The Shapiro-Wilk test was conducted to assess the normality of each variable. To determine the reliability of the vertical jumps, a test-retest reliability analysis was performed using a 2-way random (type, absolute agreement) intraclass correlation coefficient (ICC) calculated for variables recorded during the separate testing sessions. ICC values of (ICC < 0.5), $(0.5 \le ICC < 0.75)$, $(0.75 \le ICC < 0.9)$ and $(ICC \ge ICC < 0.9)$ 0.9) were interpreted as poor, moderate, good and excellent respectively, based on the lower bound of the 95% confidence interval [59]. The standard error of measurement (SEM) was also calculated as SEM = SD $\times \sqrt{1-ICC}$ [60]. The percentage of SEM (%) was calculated as SEM (%) = $(SEM / Mean) \times 100$ [61]. The mean represents the average GRF variable values across three trials. Pearson product-moment correlations were calculated between the GRF variables and 1RM back squat derived from the vertical jumps including CMJ and SJ. Correlation coefficients were considered trivial (r < 0.1), small $(0.1 \le r < 0.3)$, moderate (0.3) $\leq r < 0.5$), high $(0.5 \leq r < 0.7)$, very high $(0.7 \leq r < 0.9)$, or extremely high $(r \geq 0.9)$ [62]. GRF-derived variables were used to develop the estimation equation for 1RM back squat via stepwise linear regression analysis. Collinearity among predictors was assessed, and cocorrelating GRF-derived variables have been removed from the regression analysis. Paired samples t-test was used to examine the differences between the estimated 1RM back squat (1RM₂) and the measured 1RM back squat (1RM₂₂). The effect size of the differences between the 1RM_a and the 1RM_m was calculated as Cohen's d. The magnitude of Cohen's d was interpreted as negligible (d < 0.2), small ($0.2 \le d < 0.5$), moderate $(0.5 \le d < 0.8)$, or large $(d \ge 0.8)$ [63,64]. Standard error of estimate was calculated as SEE = $\sqrt{\sum (1RMe - 1RMm)^2}/(N-2)$, where N represented the number of the participants. Bland-Altman plots depicted the agreement between 1RM and 1RM [45]. Effect sizes for correlation, regression, and t-tests were presented as r, adjusted R^2 , and d, respectively. Statistical significance level was set at p < .05. Post-hoc Bonferroni correction was applied to correlation analysis to avoid the accumulation of family-wise error rates due to multiple correlation tests.

Results

Reliability of CMJ and SJ measurements

<u>Table 1</u> displays ICC and *SEM* values calculated for the entire sample size to quantify the relationship between the GRF variables achieved during three CMJ and SJ trials.

Table 1. Reliability statistics for the GRF variables derived from CMJ and SJ.

GRF variables	CMJ		SJ	sj		
	ICC (95% CI)	SEM	ICC (95% CI)	SEM		
Peak power (W)	.97 (.9399)	219.64 (5%)	.99 (.97-1.00)	129.36 (3%)		
Mean power (W)	.96 (.9199)	29.08 (7%)	.98 (.9699)	61.29 (5%)		
Relative net impulse (N·s·kg-1)	.98 (.9499)	0.06 (2%)	.97 (.9199)	0.07 (3%)		
Jump height (cm)	.97 (.9399)	1.77 (5%)	.97 (.9399)	1.63 (6%)		
Peak kinetic energy (J)	.96 (.8999)	22.15 (7%)	.98 (.9599)	12.31 (5%)		

ICC = intraclass correlation coefficient; CI = confidence interval

https://doi.org/10.1371/journal.pone.0316636.t001

Correlation between GRF-derived variables and measured 1RM back squat

The mean 1RM_{m} across all participants was 1.7 ± 0.4 times their body weight (BW). Table 2 shows the results of the correlation between GRF-derived variables and 1RM_{m} for all participants. Five out of 5 variables in CMJ and SJ showed significant and very high correlations with 1 RM (r = .88 - .95, p < .001 and r = .76 - .90, p < .05, respectively).

1RM back squat estimation equation using GRF-derived variables from CMJ

The following estimation equations were derived from GRF during CMJ: $1RM = 0.352 \times peak$ kinetic energy + 12.775 (adjusted $R^2 = .90$, p < .001, standard error of the estimate [SEE] = 13.24 kg, mean error = 7.4% of mean $1RM_m$). Paired samples t-tests on the validation sample showed no significant (p = 1.00, d < 0.01) difference between the $1RM_e$ (123.9 ± 39.8 kg) and $1RM_m$ (123.9 ± 41.8 kg) (Tables 3 and 4). The Bland-Altman plot showing 95% limits of agreement (LOA) between $1RM_e$ and $1RM_m$ was depicted in Fig 3A. The 95% LOA ranged from -24.87 to 24.82 kg between the $1RM_e$ and $1RM_m$ in CMJ. The post-hoc analysis revealed that the power of the estimation model derived from CMJ for 1RM was 1.

1RM back squat estimation equation using GRF-derived variables from SJ

The following estimation equations were derived from GRF during SJ: 1RM = $0.078 \times \text{mean power} + 12.254$ (adjusted $R^2 = .80$, p < .001, SEE = 18.72 kg, mean error = 10.7% of mean 1RM $_{\rm m}$). Paired samples t-tests on the validation sample showed no significant (p = .96, d = -0.02) difference between the 1RM $_{\rm e}$ (124.2 ± 37.8 kg) and 1RM $_{\rm m}$ (123.9 ± 41.8 kg) (Tables 3 and 4). The Bland-Altman plot, which includes the 95%, is depicted in Fig. 3B. LOA ranged from -34.9 to 35.4 kg between the 1RM $_{\rm e}$ and 1RM $_{\rm m}$ in SJ. The posthoc analysis revealed that the power of the estimation model derived from SJ for 1RM was 1.

Table 2. Correlation between GRF-derived variables and 1RM back squat in CMJ and SJ.

GRF variables	CMJ		SJ			
	Mean ± SD	r	p	Mean ± SD	r	p
Peak power (W)	4336.2 ± 1341.9	.93	神神	4006.3 ± 1307.6	.90	**
Mean power (W)	433.9 ± 164.7	.88	alcak:	1435 ± 485	.90	**
Relative net impulse (N·s·kg-1)	2.9 ± 0.4	.90	***	2.6 ± 0.4	.77	*
Jump height (cm)	39.9 ± 11.5	.89	**	30.6 ± 9.8	.76	*
Peak kinetic energy (J)	315.7 ± 113.1	.95	**	245 ± 92.9	.86	**

CMJ=countermovement jump; SJ=squat jump;

p < .05

**p<.001

https://doi.org/10.1371/journal.pone.0316636.t002

Table 3. Mean, standard deviations, and correlations of 1RM, 1RM, of CMJ, and 1RM, of SJ.

Mean ± SD			Mean SE			r; p		
1RMm	1RMeC	1RMeS	1RMm	1RMeC	1RMeS	1RMm - 1RMeC	1RMm - 1RMeS	
123.9 ± 41.8	123.9 ± 39.8	124.2 ± 37.8	11.6	11	10.5	.95; < .001	.90; < .001	

 $1RM_m = 1RM$ actually measured; $1RM_e^{\ C} = 1RM$ estimated from CMJ; $1RM_e^{\ S} = 1RM$ estimated from SJ.

https://doi.org/10.1371/journal.pone.0316636.t003

Table 4	Paired samples	t tests of 1RM	1RM of CMI	and 1RM of SI.

	95% CI							
	Mean	SD	Mean SE	Lower	Upper	p	d	
1RM _m - 1RM _e ^C								
1RM = 0.352 peak kinetic energy + 12.775	.02	12.68	3.52	-7.64	7.68	1.00	< 0.01	
1RM _m - 1RM _e ^S								
1RM = 0.078 mean power + 12.254	26	17.93	4.97	-11.1	10.57	.96	-0.02	

 $1RM_m = 1RM$ actually measured; $1RM_a^C = 1RM$ estimated from CMJ; $1RM_a^S = 1RM$ estimated from SJ.

https://doi.org/10.1371/journal.pone.0316636.t004

Discussion

The objective of this study was to develop equations for estimating 1RM back squat based on GRF during CMJ and SJ. Key findings were: (1) Measurements of GRF variables during vertical jumps, including CMJ and SJ, are both reliable assessments; (2) the GRF variables derived from vertical jumps were significantly correlated with the 1RM back squat; (3) the estimation models of 1RM back squat based on GRF variables were developed across two jump types explaining 80%-90% of the total variance in the 1RM back squat, with an error range of 7.4–10.7% of the mean $1RM_{\rm m}$.

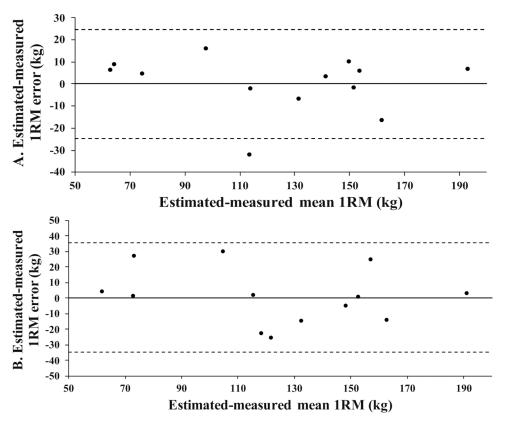


Fig 3. A. Bland-Altman plots between the 1RMe and 1RMm using GRF variables from CMJ. B. Bland-Altman plots between the 1RM_e and 1RM_m using GRF variables from SJ. Dashed line represents 95% confidence interval.

https://doi.org/10.1371/journal.pone.0316636.g003

All of the GRF variables in our study, derived from healthy adults with regular exercise habits during vertical jumps, showed good to excellent reliability (<u>Table 1</u>). This indicates that the measurement error is limited, being less than the individual variability. Our ICC results (i.e., 0.96–0.98 in CMJ and 0.97–0.99 in SJ) were within previously reported ranges of ICC values (i.e., 0.65–0.99) in vertical jump kinetics and back squat performance [<u>14,15,65–67</u>]. In summary, the investigation of the GRF variables during vertical jump tests provides a reliable assessment tool for sports scientists, sports medicine professionals, coaches, and athletes.

Another current finding was the strong correlation between GRF-related variables during vertical jumps and the 1RM back squat, suggesting vertical jump performance as an indicator of maximal back squat strength. Specifically, the study highlighted peak kinetic energy, peak power, and relative net impulse in the CMJ, as well as peak power and mean power in the SJ. The previously documented relevance of peak movement velocity [68] and body mass [69] for 1RM back squat performance may explain the currently observed, strongest correlation between 1RM back squat and peak kinetic energy derived from body mass multiplied by the square of peak velocity. Supported by the previous reports on the role of relative net impulse in determining jump performance [39], impulse contributed to the current predictions. Notably, limited research explored the relationship between the 1RM back squat and GRF variables during CMJ and SJ. This study contributed to filling this gap and demonstrated that vertical jump kinetics can effectively reflect an individual's maximal strength capabilities.

The estimation models for 1RM back squat based on GRF variables were developed using data from CMJ and SJ. The CMJ-based model demonstrated a higher R^2 and smaller error range of the mean $1RM_m$ compared to the SJ-based model. These findings suggested that CMJ may be a more reliable predictor of 1RM back squat performance. The higher R^2 value implied that the CMJ-based model explained more of the variance in 1RM back squat performance, while the smaller error range indicated greater precision and consistency. One potential explanation for the superior performance of the CMJ-based model could be the involvement of the SSC in CMJ, which was less pronounced in SJ. The SSC is a natural muscle function that enhances force production and efficiency [18,70], potentially leading to better predictive validity for dynamic movements like the back squat. The elastic energy stored during the eccentric phase of the CMJ and released during the concentric phase is similar to that utilized in the back squat and might contribute to the higher predictive accuracy observed.

No studies have established estimation equations for lower body maximum strength through vertical jumping. However, several previous studies have developed estimation equations for lower body average and maximum power in vertical jumping [28,29,42,43]. These studies selected body mass and jump height to develop the estimation equations and the R^2 values reported range from 0.74 to 0.93. Our results revealed adjusted R^2 values of 0.90 and 0.80 for the estimation equations of 1RM back squat based on CMJ and SJ, respectively. This suggested that GRF variables from vertical jumps can be highly effective in estimating 1RM back squat strength. Furthermore, the observed error range in predicting 1RM back squat (13.2 to 18.7 kg) in our study aligned with the error ranges reported for estimating 1RM bench press (2 to 19 kg) using GRF data during a ballistic push-off [45,71]. This comparison indicates that the estimation equations we developed for back squat strength have comparable predictive accuracy to those used for bench press strength. In addition, the measurement error in other 1RM back squat estimations via individual load-velocity profiles during the back squat ranged from below 5 kg to 17.2 kg [72,73]. Therefore, the load-velocity methods may exhibit lower measurement errors than those reported in this study. However, these studies estimated 1RM based on load-velocity profiles from participants squatting at least 1.5 BW as their 1RM, which was 50% higher than in the current study. Therefore, it was unclear if estimation approaches were applicable across samples with different strength levels. In summary,

these findings underscored the validity of using vertical jump metrics for estimating lower body strength and suggested that the errors in our predictions fall within a range similar to those observed in established methods. This alignment supports the reliability of our estimation equations and highlights their potential utility in accurately assessing lower body strength through vertical jump performance.

The current findings were limited to physically active participants who integrated the loaded back squats in their frequent training and were capable of squatting an extra weight of 1 BW or more. To generalize the estimation model, future research may recruit individuals with a larger variability regarding strength and skill levels. Second, although the sample size was sufficient to detect the desired effect sizes in the current study and aligned with recommendations from the literature [44,74], smaller effects may have been undetected. Studies that aim for assessing a larger range of effects in more diverse samples are recommended to recruite a larger sample. In the current study, as expected, effect sizes were so large that the acual observed power of $1-\beta = 1$ was achieved via post-hoc analysis, suggesting a sufficient sample size for the current effects. Third, the small age range (22-25 years) and the underrepresentation of females (23%) in the current sample. A previous study showed no significant impact of age and sex on the estimation of peak muscle power from the CMJ [28]. In addition, the current study did not attempt to investigate the effect of age and sex or to derive age- and sex-specific prediction models. Therefore, the limitation in sample characteristics was not considered consequential for practical implication. Another limitation was that the SEE rates reported in this study were based on a single assessment without cross-validation after a period of prescribed training. However, the accuracy of the estimation model still needs to be further improved in the future. Considering the current error rates, the proposed model may be more suitable for providing a general fitness assessment of lower limb strength than for prescribing exact training loads.

Conclusion

This study presents evidence that GRF-derived variables obtained during CMJ and SJ may provide alternative methods for assessing the 1RM back squat. CMJ has been demonstrated to be a more accurate predictor of 1RM back squat compared to the SJ. This study developed a general equation using peak kinetic energy from CMJ data applicable to healthy young adults (r = .95, adjusted R^2 = .90, mean error = 7.4% of the mean 1RM $_{\rm m}$). The proposed equations could be implemented to enhance their potential impact and relevance for practical monitoring in strength training. Incorporating lower body maximum strength assessment through GRF variables from vertical jumps has the potential to improve general fitness programs and serve as a valuable component of periodized strength and conditioning protocols for both general populations and athletes. Furthermore, the developed estimation models for 1RM back squat based on GRF-derived variables from vertical jumps could be utilized to create a force assessment algorithm for sports technology companies.

Supporting information

S1 Table. Raw data from all participants. (XLSX)

Author contributions

Conceptualization: Chuan-Fang Hou, Chin-Wei Hsu, Tzyy-Yuang Shiang.

Data curation: Chuan-Fang Hou, Chin-Wei Hsu.

Formal analysis: Chuan-Fang Hou, Chin-Wei Hsu.

Investigation: Chuan-Fang Hou, Chin-Wei Hsu, Tzyy-Yuang Shiang. **Methodology:** Chuan-Fang Hou, Chin-Wei Hsu, Philip X. Fuchs.

Project administration: Tzyy-Yuang Shiang.

Resources: Tzyy-Yuang Shiang.

Supervision: Philip X. Fuchs, Tzyy-Yuang Shiang. **Validation:** Chuan-Fang Hou, Chin-Wei Hsu.

Visualization: Chuan-Fang Hou, Chin-Wei Hsu, Philip X. Fuchs.

Writing - original draft: Chuan-Fang Hou.

Writing - review & editing: Chuan-Fang Hou, Philip X. Fuchs, Tzyy-Yuang Shiang.

References

- Suchomel TJ, Nimphius S, Bellon CR, Hornsby WG, Stone MH. Training for muscular strength: methods for monitoring and adjusting training intensity. Sports Med. 2021;51(10):2051–66. https://doi.org/10.1007/s40279-021-01488-9 PMID:34101157
- García-Hermoso A, Ramírez-Campillo R, Izquierdo M. Is muscular fitness associated with future health benefits in children and adolescents? A systematic review and meta-analysis of longitudinal studies. Sports Med. 2019;49(7):1079–94. https://doi.org/10.1007/s40279-019-01098-6 PMID:30953308
- Grgic J, Garofolini A, Orazem J, Sabol F, Schoenfeld BJ, Pedisic Z, et al. Effects of resistance training on muscle size and strength in very elderly adults: a systematic review and meta-analysis of randomized controlled trials. Sports Med. 2020;50(11):1983–99. https://doi.org/10.1007/s40279-020-01331-7 PMID:32740889
- Güçlüöver A, Gülü M. Developing a new muscle power prediction equation through vertical jump power output in adolescent women. Medicine (Baltim). 2020;99(25):e20882. https://doi.org/10.1097/MD.0000000000000000882 PMID:32569237
- Mazur LJ, Yetman RJ, Risser WL. Weight-training injuries. Common injuries and preventative methods. Sports Med. 1993;16(1):57–63. https://doi.org/10.2165/00007256-199316010-00005 PMID:8356377
- Marini M, Sarchielli E, Brogi L, Lazzeri R, Salerno R, Sgambati E, et al. Role of adapted physical activity to prevent the adverse effects of the sarcopenia. a pilot study. Ital J Anat Embryol. 2008;113(4):217–25. PMID:19507462
- 7. Wing CE, Turner AN, Bishop CJ. Importance of strength and power on key performance indicators in elite youth soccer. J Strength Cond Res. 2020;34(7):2006–14. https://doi.org/10.1519/JSC.0000000000002446 PMID:29373431
- 8. Suchomel TJ, Nimphius S, Stone MH. The Importance of muscular strength in athletic performance. Sports Med. 2016;46(10):1419–49. https://doi.org/10.1007/s40279-016-0486-0 PMID:26838985
- Seitz LB, Reyes A, Tran TT, Saez de Villarreal E, Haff GG. Increases in lower-body strength transfer positively to sprint performance: a systematic review with meta-analysis. Sports Med. 2014;44(12):1693–702. https://doi.org/10.1007/s40279-014-0227-1 PMID:25059334
- Støren O, Helgerud J, Støa EM, Hoff J. Maximal strength training improves running economy in distance runners. Med Sci Sports Exerc. 2008;40(6):1087–92. https://doi.org/10.1249/MSS.0b013e-318168da2f PMID:18460997
- Lauersen JB, Bertelsen DM, Andersen LB. The effectiveness of exercise interventions to prevent sports injuries: a systematic review and meta-analysis of randomised controlled trials. Br J Sports Med. 2014;48(11):871–7. https://doi.org/10.1136/bjsports-2013-092538 PMID:24100287
- Rhodes RE, Lubans DR, Karunamuni N, Kennedy S, Plotnikoff R. Factors associated with participation in resistance training: a systematic review. Br J Sports Med. 2017;51(20):1466–72. https://doi.org/10.1136/bjsports-2016-096950 PMID:28404558
- Grgic J, Lazinica B, Schoenfeld BJ, Pedisic Z. Test-retest reliability of the one-repetition maximum (1RM) strength assessment: a systematic review. Sports Med Open. 2020;6(1):31. https://doi.org/10.1186/s40798-020-00260-z PMID:32681399

- 14. Ryman Augustsson S, Svantesson U. Reliability of the 1 RM bench press and squat in young women. Eur J Physiother. 2013:15(3):118–26. https://doi.org/10.3109/21679169.2013.810305
- Comfort P, McMahon JJ. Reliability of maximal back squat and power clean performances in inexperienced athletes. J Strength Cond Res. 2015;29(11):3089–96. https://doi.org/10.1519/JSC.0000000000000815 PMID:25559912
- Willardson JM, Burkett LN. The effect of rest interval length on bench press performance with heavy vs. light loads. J Strength Cond Res. 2006;20(2):396–9. https://doi.org/10.1519/R-17735.1 PMID:16686570
- Watkins CM, Barillas SR, Wong MA, Archer DC, Dobbs IJ, Lockie RG, et al. Determination of vertical jump as a measure of neuromuscular readiness and fatigue. J Strength Cond Res. 2017;31(12):3305– 10. https://doi.org/10.1519/JSC.0000000000002231 PMID:28902119
- Gillen ZM, Shoemaker ME, McKay BD, Bohannon NA, Gibson SM, Cramer JT. Influences of the stretch-shortening cycle and arm swing on vertical jump performance in children and adolescents. J Strength Cond Res. 2022;36(5):1245–56. https://doi.org/10.1519/JSC.000000000000003647 PMID:32483060
- Petronijevic MS, Ramos AG, Mirkov DM, Jaric S, Valdevit Z, Knezevic OM. Self-preferred initial position could be a viable alternative to the standard squat jump testing procedure. J Strength Cond Res. 2018;32(11):3267–75. https://doi.org/10.1519/JSC.0000000000002385 PMID: 30540284
- Claudino JG, Cronin J, Mezêncio B, McMaster DT, McGuigan M, Tricoli V, et al. The countermovement jump to monitor neuromuscular status: a meta-analysis. J Sci Med Sport. 2017;20(4):397–402. https://doi.org/10.1016/j.jsams.2016.08.011 PMID:27663764
- Marques MC, Izquierdo M, Marinho DA, Barbosa TM, Ferraz R, González-Badillo JJ. Association between force-time curve characteristics and vertical jump performance in trained athletes. J Strength Cond Res. 2015;29(7):2045–9. https://doi.org/10.1519/JSC.0000000000000739 PMID:26098568
- 22. Fransz DP, Huurnink A, de Boode VA, Kingma I, van Dieën JH. Time series of ground reaction forces following a single leg drop jump landing in elite youth soccer players consist of four distinct phases. Gait Posture. 2016;50:137–44. https://doi.org/10.1016/j.gaitpost.2016.09.002 PMID:27611061; PMID:27611061
- 23. Hovey S, Wang H, Judge LW, Avedesian JM, Dickin DC. The effect of landing type on kinematics and kinetics during single-leg landings. Sports Biomech. 2021;20(5):543–59. https://doi.org/10.1080/14763 141.2019.1582690 PMID:30882276
- 24. Taylor K, Chapman D, Cronin J, Newton MJ, Gill N. Fatigue monitoring in high performance sport: a survey of current trends. J Aust Strength Cond. 2012;20(1):12–23.
- Quagliarella L, Sasanelli N, Belgiovine G, Moretti L, Moretti B. Power output estimation in vertical jump performed by young male soccer players. J Strength Cond Res. 2011;25(6):1638–46. https://doi.org/10.1519/JSC.0b013e3181d85a99 PMID:21358432
- Mahar MT, Welk GJ, Janz KF, Laurson K, Zhu W, Baptista F. Estimation of lower body muscle power from vertical jump in youth. Meas Phys Educ Exercise Sci. 2022;26(4):324–34. https://doi.org/10.1080/1091367x.2022.2041420
- Gülü M, Akalan C. A new peak-power estimation equations in 12 to 14 years-old soccer players. Medicine (Baltim). 2021;100(39):e27383. https://doi.org/10.1097/MD.000000000027383 PMID:34596159
- 28. Gomez-Bruton A, Gabel L, Nettlefold L, Macdonald H, Race D, McKay H. Estimation of peak muscle power from a countermovement vertical jump in children and adolescents. J Strength Cond Res. 2019;33(2):390–8. https://doi.org/10.1519/JSC.0000000000002002 PMID:28570492
- Duncan MJ, Hankey J, Nevill AM. Peak-power estimation equations in 12- to 16-year old children: comparing linear with allometric models. Pediatr Exerc Sci. 2013;25(3):385–93. https://doi.org/10.1123/pes.25.3.385 PMID:23881526
- 30. Markovic S, Mirkov DM, Nedeljkovic A, Jaric S. Body size and countermovement depth confound relationship between muscle power output and jumping performance. Hum Mov Sci. 2014;33:203–10. https://doi.org/10.1016/j.humov.2013.11.004 PMID:24280557
- Samozino P, Rabita G, Dorel S, Slawinski J, Peyrot N, Saez de Villarreal E, et al. A simple method for measuring power, force, velocity properties, and mechanical effectiveness in sprint running. Scand J Med Sci Sports. 2016;26(6):648–58. https://doi.org/10.1111/sms.12490 PMID:25996964
- 32. Gillett J, De Witt J, Stahl CA, Martinez D, Dawes JJ. Descriptive and kinetic analysis of two different vertical jump tests among youth and adolescent male basketball athletes using a supervised machine learning approach. J Strength Cond Res. 2021;35(10):2762–8. https://doi.org/10.1519/JSC.000000000000000100 PMID:34417401

- Barker LA, Harry JR, Mercer JA. Relationships between countermovement jump ground reaction forces and jump height, reactive strength index, and jump time. J Strength Cond Res. 2018;32(1):248–54. https://doi.org/10.1519/JSC.000000000002160 PMID:28746248
- Merrigan JJ, Rentz LE, Hornsby WG, Wagle JP, Stone JD, Smith HT, et al. Comparisons of countermovement jump force-time characteristics among national collegiate athletic association division i american football athletes: use of principal component analysis. J Strength Cond Res. 2022;36(2):411–9. https://doi.org/10.1519/JSC.0000000000004173 PMID:34798642
- Krzyszkowski J, Chowning LD, Harry JR. Phase-specific predictors of countermovement jump performance that distinguish good from poor jumpers. J Strength Cond Res. 2022;36(5):1257–63. https://doi.org/10.1519/JSC.00000000000003645 PMID:32412965
- 36. Linthorne NP. The correlation between jump height and mechanical power in a countermovement jump is artificially inflated. Sports Biomech. 2021;20(1):3–21. https://doi.org/10.1080/14763141.2020.1721737 PMID:32200754
- Daugherty HJ, Weiss LW, Paquette MR, Powell DW, Allison LE. Potential predictors of vertical jump performance: lower extremity dimensions and alignment, relative body fat, and kinetic variables. J Strength Cond Res. 2021;35(3):616–25. https://doi.org/10.1519/JSC.0000000000000003962 PMID:33587546
- **38.** Thomas C, Jones PA, Rothwell J, Chiang CY, Comfort P. An investigation into the relationship between maximum isometric strength and vertical jump performance. J Strength Cond Res. 2015;29(8):2176–85. https://doi.org/10.1519/JSC.0000000000000866 PMID:25647649
- Kirby TJ, McBride JM, Haines TL, Dayne AM. Relative net vertical impulse determines jumping performance. J Appl Biomech. 2011;27(3):207–14. https://doi.org/10.1123/jab.27.3.207 PMID:21844609
- Nishioka T, Okada J. Associations of maximum and reactive strength indicators with force-velocity profiles obtained from squat jump and countermovement jump. PLoS One. 2022;17(10):e0276681. https://doi.org/10.1371/journal.pone.0276681 PMID:36269787
- Zemková E, Vilman T, Cepková A, Uvaček M, Olej P, Šimonek J. Enhancement of power in the concentric phase of the squat and jump: Between-athlete differences and sport-specific patterns. 2017;12(1).
- Harman EA, Rosenstein MT, Frykman PN, Rosenstein RM, Kraemer WJ. Estimation of human power output from vertical jump. J Strength Cond Res. 1991;5(3):116–20. https://doi.org/10.1519/00124278-199108000-00002
- Sayers SP, Harackiewicz DV, Harman EA, Frykman PN, Rosenstein MT. Cross-validation of three jump power equations. Med Sci Sports Exerc. 1999;31(4):572–7. https://doi.org/10.1097/00005768-199904000-00013 PMID:10211854
- Jenkins DG, Quintana-Ascencio PF. A solution to minimum sample size for regressions. PLoS One. 2020;15(2):e0229345. https://doi.org/10.1371/journal.pone.0229345 PMID:32084211
- **45.** Wang R, Hoffman JR, Sadres E, Bartolomei S, Muddle TWD, Fukuda DH, et al. Evaluating upper-body strength and power from a single test: the ballistic push-up. J Strength Cond Res. 2017;31(5):1338–45. https://doi.org/10.1519/JSC.0000000000001832 PMID:28166187
- 46. Strength N-N, Association C. Essentials of strength training and conditioning: Human Kinetics; 2021.
- 47. Bender B. Energy system development in the weight room: incorporating prescribed rest periods for NCAA men's basketball players. Strength Cond J. 2019;41(5):57–61. https://doi.org/10.1519/ssc.00000000000000487
- Sole CJ, Mizuguchi S, Sato K, Moir GL, Stone MH. Phase characteristics of the countermovement jump force-time curve: a comparison of athletes by jumping ability. J Strength Cond Res. 2018;32(4):1155–65. https://doi.org/10.1519/JSC.000000000001945 PMID:28644194
- McMahon JJ, Suchomel TJ, Lake JP, Comfort P. Understanding the key phases of the countermovement jump force-time curve. Strength Cond J. 2018;40(4):96–106. https://doi.org/10.1519/ssc.0000000000000375
- Chavda S, Bromley T, Jarvis P, Williams S, Bishop C, Turner AN, et al. Force-time characteristics of the countermovement jump: Analyzing the curve in Excel. Strength Cond J. 2018;40(2):67–77. https://doi.org/10.1519/ssc.000000000000000353
- Merrigan JJ, Strang A, Eckerle J, Mackowski N, Hierholzer K, Ray NT, et al. Countermovement jump force-time curve analyses: reliability and comparability across force plate systems. J Strength Cond Res. 2024;38(1):30–7. https://doi.org/10.1519/JSC.0000000000004586 PMID:37815253
- Hahn D. On the phase definitions of counter movement jumps. Scand J Med Sci Sports. 2023;33(3):359–60. https://doi.org/10.1111/sms.14288 PMID:36775878

- McBride JM, Kirby TJ, Haines TL, Skinner J. Relationship between relative net vertical impulse and jump height in jump squats performed to various squat depths and with various loads. Int J Sports Physiol Perform. 2010;5(4):484–96. https://doi.org/10.1123/ijspp.5.4.484 PMID:21266733
- Warr DM, Pablos C, Sánchez-Alarcos JV, Torres V, Izquierdo JM, Carlos Redondo J. Reliability of measurements during countermovement jump assessments: Analysis of performance across subphases. Cogent Soc Sci. 2020;6(1):1843835.
- Sánchez-Sixto A, Harrison AJ, Floría P. Effects of plyometric vs. Combined plyometric training on vertical jump biomechanics in female basketball players. J Hum Kinet. 2021;77:25–35. https://doi.org/10.2478/hukin-2021-0009 PMID:34168689
- Oranchuk DJ, Robinson TL, Switaj ZJ, Drinkwater EJ. Comparison of the hang high pull and loaded jump squat for the development of vertical jump and isometric force-time characteristics. J Strength Cond Res. 2019;33(1):17–24. https://doi.org/10.1519/JSC.0000000000001941 PMID:28426514
- 57. Teo SY, Newton MJ, Newton RU, Dempsey AR, Fairchild TJ. Comparing the effectiveness of a short-term vertical jump vs. weightlifting program on athletic power development. J Strength Cond Res. 2016;30(10):2741–8. https://doi.org/10.1519/JSC.000000000001379 PMID:26890972
- Cooper CN, Dabbs NC, Davis J, Sauls NM. Effects of lower-body muscular fatigue on vertical jump and balance performance. J Strength Cond Res. 2020;34(10):2903–10. https://doi.org/10.1519/JSC.00000000000002882 PMID:30273290
- Koo TK, Li MY. A guideline of selecting and reporting intraclass correlation coefficients for reliability research. J Chiropr Med. 2016;15(2):155–63. https://doi.org/10.1016/j.jcm.2016.02.012
 PMID:27330520
- Collings TJ, Lima YL, Dutaillis B, Bourne MN. Concurrent validity and test–retest reliability of VALD ForceDecks' strength, balance, and movement assessment tests. J Sci Med Sport. 2024;27(8):572–80. https://doi.org/10.1016/j.jsams.2024.04.014
- 61. Lexell JE, Downham DY. How to assess the reliability of measurements in rehabilitation. Am J Phys Med Rehabil. 2005;84(9):719–23. https://doi.org/10.1097/01.phm.0000176452.17771.20 PMID:16141752
- 62. Hicks DS, Drummond C, Williams KJ. Measurement Agreement Between Samozino's Method and Force Plate Force-Velocity Profiles During Barbell and Hexbar Countermovement Jumps. J Strength Cond Res. 2022;36(12):3290–300. https://doi.org/10.1519/JSC.000000000004144 PMID:34657074
- Sullivan GM, Feinn R. Using effect size—or why the P value is not enough. J Grad Med Educ. 2012;4(3):279–82. https://doi.org/10.4300/JGME-D-12-00156.1 PMID:23997866
- 64. Cohen J. Statistical power analysis for the behavioral sciences: routledge; 2013.
- **65.** Souza AA, Bottaro M, Valdinar A ROCHA J, Lage V, Tufano JJ, Vieira A. Reliability and test-retest agreement of mechanical variables obtained during countermovement jump. Int J Exerc Sci. 2020;13(4):6.
- **66.** Xu J, Turner A, Comyns TM, Chavda S, Bishop C. The Countermovement Rebound Jump: Between-Session Reliability and a Comparison With the Countermovement and Drop Jump Tests. J Strength Cond Res. 2022;10:1519.
- 67. Bellicha A, Giroux C, Ciangura C, Menoux D, Thoumie P, Oppert J-M, et al. Vertical Jump on a Force Plate for Assessing Muscle Strength and Power in Women With Severe Obesity: Reliability, Validity, and Relations With Body Composition. J Strength Cond Res. 2022;36(1):75–81. https://doi.org/10.1519/JSC.00000000000003432 PMID:32218061
- Fahs CA, Rossow LM, Zourdos MC. Analysis of factors related to back squat concentric velocity. J Strength Cond Res. 2018;32(9):2435–41. https://doi.org/10.1519/JSC.000000000000002295
 PMID:30137028
- 69 Ferland P-M, Pollock A, Swope R, Ryan M, Reeder M, Heumann K, et al. The relationship between physical characteristics and maximal strength in men practicing the back squat, the bench press and the deadlift. Int J Exerc Sci. 2020;13(4):281–97. https://doi.org/10.70252/AJSZ9846 PMID:32148635
- 70. Edwards T, Weakley J, Woods CT, Breed R, Benson AC, Suchomel TJ, et al. Comparison of countermovement jump and squat jump performance between 627 state and non-state representative junior Australian football players. J Strength Cond Res. 2023;37(3):641–5. https://doi.org/10.1519/JSC.0000000000004299 PMID:35916875
- 71. Bartolomei S, Nigro F, Ruggeri S, Lanzoni IM, Ciacci S, Merni F, et al. Comparison between bench press throw and ballistic push-up tests to assess upper-body power in trained individuals. J Strength Cond Res. 2018;32(6):1503–10.

- 72. Thompson SW, Rogerson D, Ruddock A, Greig L, Dorrell HF, Barnes A. A novel approach to 1RM prediction using the load-velocity profile: A comparison of models. Sports (Basel, Switzerland). 2021;9(7):88. https://doi.org/10.3390/sports9070088 PMID:34206534
- 73. Banyard HG, Nosaka K, Haff GG. Reliability and validity of the load–velocity relationship to predict the 1RM back squat. J Strength Cond Res. 2017;31(7):1897–904. https://doi.org/10.1519/JSC.00000000000001657 PMID:27669192
- 74. Beck TW. The importance of a priori sample size estimation in strength and conditioning research. J Strength Cond Res. 2013;27(8):2323–37. https://doi.org/10.1519/JSC.0b013e318278eea0 PMID:23880657