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# Dual-targeted carbon-dot-drugs nanoassemblies for modulating Alzheimer's related amyloid- $\beta$ aggregation and inhibiting fungal infection

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# ABSTRACT

Amyloid aggregation and fungal infection, especially amyloid beta ( $A\beta$ ) peptide and *Candida albicans* are considered as two of the crucial pathogenic agents in Alzheimer's disease (AD). In this work, we propose an innovative treatment strategy for AD, targeting at not only  $A\beta$  aggregation but also *Candida albicans* infection. Here, a high-performance nanomaterial, namely gCDs-E, have been prepared by self-assembled of glycosylated carbon dots (gCDs) and epigallocatechin-3-gallate (EGCG). Surprisingly, gCDs-E can not only suppress the fibrillation of  $A\beta$  and disaggregate  $A\beta$  fibrils, but also effectively inhibit the activity of *Candida albicans*. More importantly, the prepared gCDs-E can effectively cut down the cytotoxicity of amyloid aggregations, and the cell viability reached to 99.2%. In addition, the capability of the gCDs-E for blood brain barrier (BBB) penetration was also observed using a normal mice model. Above all, the gCDs-E greatly cleaned  $A\beta$  deposition and improved memory impairment in APP/PS1 transgenic AD model mice, confirming its potential as therapeutic agent for AD treatment.

# 1. Introduction

Alzheimer's disease (AD), also namely dementia, is the most prevalent form of neurodegenerative disorder [1–3]. Although the pathogenesis of AD has not been clearly and thoroughly confirmed, its emphatic pathological traits have been verified, which is the extracellular deposits of amyloid aggregation from the amyloid- $\beta$  peptides (A $\beta$ ) [4–10]. The therapeutic and preventive methods of AD including inhibiting the aggregation of A $\beta$  into fibrils and oligomers is also effectual and widely accepted [11–17]. However, the recent failure of clinical trials suggests that further efforts on AD research is still demanding [12]. Interestingly, recent intense research indicates that some pathogenic microorganisms exist in the brain and postulated to be involved with A $\beta$  or even to AD [18–22]. For example, Pisa et al. [18] directly visualized fungal components inside neurons from AD patients. Wu et al.' [20] showed that *Candida albicans* can cross the BBB and cause a highly localized cerebritis. Moreover,  $A\beta$  accumulates within the activated microglial and astroglia cells, which are induced by *Candida albicans*. These evidences even indicated that  $A\beta$  peptides enhanced both phagocytic and antifungal activity from cells. According to Wu's research [20], *Candida albicans* can cause a highly localized cerebritis marked by the accumulation of activated microglial and astroglial cells around yeast aggregates, forming fungal-induced glial granulomas. In addition, they found that large amounts of  $A\beta$  peptides and insoluble  $A\beta$  aggregation accumulated around the yeast cells. This related research indicates that the more serious the fungal infection, the more obvious amyloid fibrillation.

Currently, most of  $A\beta$  inhibitors including biomolecules [23–26], functionalized nanomaterials and nanoparticles [16,17,27–31], have been shown to decelerate the aggregation of  $A\beta$  and suppress cellular toxicity of amyloid. For example, Sun et al. [32] reported a mesoporous

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**Scheme 1.** (a) The preparation process of gCDs and gCDs-E. (b) Schematic illustration of the mechanism of gCDs-E for crossing BBB, suppressing  $A\beta$  aggregation and inhibiting *Candida albicans*.

nano-selenium release delivery system (MSe-Res/Fc- $\beta$ -CD/Bor), and this nano-selenium release delivery system could inhibit aggregation of  $A\beta$ and improve memory impairment in APP/PS1 mice. In addition, Yang et al. [13] devised a novel nanochaperone based on mixed-shell polymeric micelle, and applied nanochaperone to selectively capture  $A\beta$ peptides, inhibit A $\beta$  aggregation, and suppress A $\beta$ -mediated cytotoxicity. Epigallocatechin-3-gallate (EGCG), the major components of green tea extract, exhibits effects of anti-inflammation, antifungals and modulation of  $\beta$ -amyloid self-assembly [26,28,33–38]. For example, previous studies have shown that EGCG enable to inhibit the growth of Candida albicans, and bind with unfolded  $A\beta$  for inhibiting the formation of  $\beta$ -sheet structure amyloid [26,28,35,36]. Moreover, the related research reveal that EGCG have not obvious cytotoxicity to HEK 293 cells after 24 h at 160 µg/mL EGCG, and caused 90% growth inhibition of tested strains of C. albicans [36,39]. Nevertheless, BBB is the major obstacles in the treatment of AD [11,40-42], while it's difficult for EGCG to overcome it spontaneously [21]. Considering the hampering effect of the BBB, designed nanocarriers with the ability to anchor EGCG and overcome the BBB are required. Fortunately, carbon dots (CDs) have greatly attracted our attention due to their ability of crossing the BBB, unique optical property and low toxicity [43-47]. For example, Xiao and Wang et al. demonstrated that GQDs enable to cross the BBB, inhibit aggregation of A $\beta$  and rescue the cytotoxicity of A $\beta$  oligomers [27,48]. Liyanage et al. also reported the capability of carbon nitride dots to penetrate the BBB [49]. Moreover, Leblanc's group deeply explored the mechanism of overcoming the BBB with CDs and verified the ability of CDs for inhibiting the human amyloid precursor protein and A $\beta$  [50–53].

In this work, we propose a breakthrough strategy to consider these two possible pathogenic factors with unprecedented efficiency on inhibiting AD. A novel nanomaterial (gCDs-E) assembled from glycosylated carbon dots (gCDs) and EGCG (Scheme 1a) were fabricated, and its capability for treatment AD was explored. Different from traditional treatment strategies,  $A\beta$  aggregation and *Candida albicans* infection were both considered as possible pathogenic factors (Scheme 1b): Firstly, gCDs-E can effectively prevent misfolding of  $A\beta$  and inhibit its aggregation *in vitro*, and can remarkably reduce  $A\beta$ -mediated cytotoxicity. Next, gCDs-E can suppress the viability of *Candida albicans*, which preventing memory loss caused by fungal infection. Results from *in vitro* and *in vivo* experiments confirms the gCDs-E's high biocompatibility and ability of BBB penetration. Furthermore, gCDs-E can greatly clean  $A\beta$  deposition and improved memory impairment in APP/PS1 transgenic AD model mice.

# 2. Results and discussion

#### 2.1. Characterization of gCDs and gCDs-E

Glycosylated carbon dots (gCDs) were firstly prepared using glucose as precursor by a solvothermal method. Following, gCDs-E was assembled from EGCG and gCDs through hydrogen bonding,  $\pi$ - $\pi$  stacking interaction and electrostatic binding [54]. The morphology and particle size of gCDs and gCDs-E were characterized by transmission electron microscopy (TEM) and atomic force microscopy (AFM). As shown in Fig. 1a, gCDs exhibit a uniform dispersion without any apparent aggregation, and the average size is about 4.25 nm. AFM image (Fig. S1) reveals that gCDs disperse nicely with a particle's height about 1.5 nm. The size distribution of both TEM and AFM indicate that gCDs are discoidal shape. The corresponding high-resolution TEM (HRTEM) image (Fig. 1b) shows the obvious lattices in carbon cores of gCDs, and the distribution of lattice spacing is about 0.21 nm. The lattice spacing value correspond to the (100) inter-planar spacing, demonstrating the almost defect-free graphene crystalline structure [55-57]. Raman spectrum of gCDs (Fig. S2) shows that the intensity ratio  $(I_D/I_G)$  of characteristic D and G bands is about 0.71, and are positioned at 1335 and 1583  $\text{cm}^{-1}$ , respectively. The ratio indicates that gCDs are consist of graphene structure (predominantly) and other disorder structure [57,58]. In the <sup>1</sup>H NMR spectra of gCDs, the peak at 9.53 ppm in Fig. S3 is the chemical shift of the carboxyl protons [56]. In addition, signals from the aromatic rings were detected at 8.37 ppm, which was attributed to graphitized cores' proton resonances [59]. Furthermore, the chemical shift values of aliphatic carbons are present in range from 1 to 5 ppm, which indicated the formation of glycosylated gCDs. As shown in Fig. 1c, it can be seen that the morphology of the prepared gCDs-E is circular or oval nanoparticle with a particles size about 25.5 nm. UV-Vis spectrum of gCDs is shown in Fig. 1d, the two obvious absorption peaks at 216 and 285 nm are attributed to the  $\pi = \pi^*$  transition of C=C bond, and the weak absorption band in the range of 300-380 nm belongs to n-p\* transition of the carboxylic C=O bond on the surface of gCDs [60,61]. The difference of UV-Vis spectrum (Fig. S4) for EGCG, gCDs and gCDs-E at 250-320 nm indicates that EGCG have been successfully anchored on the surface of gCDs. FL excitation and emission spectrum of gCDs (Fig. 1d) exhibits distinct and well-defined peaks at 362 and 445 nm. Fig. 1e and f represents the PL emission of the gCDs and gCDs-E solution under different excitation wavelengths. The gCDs (Fig. 1e) shows two stable emission centers at 445 and 545 nm. However, the as-prepared gCDs-E solution (Fig. 1f) exhibits distinctive excitation-dependent PL features, which can be attributed to the molecular interaction between EGCG and gCDs, and resulting in red shift of the emission [62]. In addition, after modification with EGCG, the formation of surface emissive traps as well as the varying size distribution of the gCDs caused by EGCG also lead to the wavelength-dependent fluorescence emission property [63,64]. The photoluminescence quantum yield (PLQY) of the gCDs and gCDs-E were calculated to be 12.7% and 9.8%, using the Quantaurus-QY equipment (Fig. S5). The full XPS spectrum presented in Fig. 1g and h shows two peaks at 284.8 and 532.2 eV, suggesting that the gCDs and gCDs-E consisted of C and O elements, and the calculated atomic ratios of gCDs and gCDs-E were 57.88%: 42.12% and 44.87%: 55.13%, respectively. In Fig. 1h and k, the high-resolution XPS spectrum of the C 1s band was separated into four peaks at 284.8, 285.8, 286.6, and 288.7 eV, which are assigned to C-C/C=C, C-O, C=O, and COOH, respectively. The O1s band (Fig. 1i and l) exhibits two peaks at 532.0 and 532.8 eV, respectively, which correspond to C=O and C-O groups. Then, Fourier



**Fig. 1.** (a) TEM image and the corresponding size distribution histogram of gCDs. (b) HR-TEM image of gCDs. (c) TEM image and the corresponding size distribution histogram of gCDs-E. (d) UV/Vis absorption spectrum of gCDs in water; the normalized FL emission and excitation spectra of gCDs in water. Fluorescence spectra of (e) gCDs and (f) gCDs-E solution at different excitation wavelengths. (g–i) XPS survey spectrum, high-resolution C 1s, and high-resolution O 1s spectrum of gCDs. (j–l) XPS survey spectrum, high-resolution C 1s, and high-resolution C 1s, and high-resolution O 1s spectrum of gCDs-E.

transform infrared (FT-IR) was constructed to characterize the functional groups of gCDs and gCDs-E (Fig. S6). In the curve of gCDs (red line) and gCDs-E (purple line), absorption bands at 1642 cm<sup>-1</sup>, 1108 cm<sup>-1</sup> are corresponding to the stretching vibration of C=O and C-O [47,61], respectively. Therefore, hydroxyl and carboxyl are the main functional groups on the surface of gCDs and gCDs-E.

### 2.2. Inhibition and disaggregation of $A\beta$ by gCDs and gCDs-E

Following, we investigated the potential role of the gCDs and gCDs-E in inhibiting  $A\beta$  fibrillization and disaggregating fibrils. TEM results are presented in Fig. 2a and Fig. S7. In the absence of gCDs or gCDs-E, mature  $A\beta_{42}$  and  $A\beta_{40}$  fibrils are obviously observed (Control group, Fig. 2a and Fig. S7a). The same assessments show that the gCDs-E (Fig. 2a and Fig. S7a) can predominantly disaggregate  $A\beta_{42}$  and  $A\beta_{40}$  fibrils into short fragments, with the average length of the fragments shortening from to 61 nm and 122 nm after gCDs-E treatment for 24 h, respectively. Corresponding DLS (Fig. S7b and Fig. S8) results also demonstrate the disaggregation ability of gCDs-E. In addition, the fibrillation process of  $A\beta_{42}$  monomers incubated with gCDs or gCDs-E is also effectively

suppressed (Fig. 2b), and the average length of the fragments is shorted from 648 nm to 3.6 nm after gCDs-E treatment for 24 h (Fig. 2d). Obviously, more significant disaggregation and inhibition performance of gCDs-E is also exhibited compared with gCDs (Fig. 2c and d). Furthermore, circular dichroism (CD) spectra were used to analyze the change of the secondary structure of A $\beta$  peptides. The non-treated A $\beta_{42}$ monomers show random structures at 0 h and 30 min (Fig. 2e). However, the typical  $\beta$ -sheet structure of A $\beta_{42}$  occur from 6 h to 24 h in PBS solution (pH = 7.4), with positive and negative signals at 197 and 218 nm, respectively. Interestingly, the revealed  $\beta$ -sheet structure of A $\beta_{42}$  treated with the gCDs was significantly inhibited compared with control group (Fig. 2f). Moreover, gCDs-E treated A $\beta_{42}$  did not show  $\beta$ -sheet structures after 24 h, with only negative signals at 201 nm (Fig. 2f). Corresponding the fractional secondary structures were also analyzed using the algorithm CDNN (Fig. 2g). After treated with gCDs for 24 h, the  $\beta$ -sheet component of  $A\beta_{42}$  decrease from 55.7% to 45.6% and the random coil components increase from 19.3% to 32.3%. The gCDs-E treated A $\beta_{42}$ shows a drop of  $\beta$ -sheet component from 55.7% to 31.2% and an increase of the random coil components from 19.3% to 35.9%. Furthermore, gCDs and gCDs-E can reverse the secondary structure of A $\beta_{42}$  fibrils. As shown



**Fig. 2.** (a–b) TEM images of  $A\beta_{42}$  fibrils or  $A\beta_{42}$  monomers (25 µM) incubated in the absence and presence of nanomaterials (gCDs or gCDs-E) after 24 h. (c–d) The corresponding size distribution histogram of TEM results. (e) CD spectra for misfolding process of  $A\beta_{42}$  monomers. (f) CD spectra for  $A\beta_{42}$  incubated in the absence and presence of gCDs or gCDs-E after 24 h. (g) The corresponding Fractional secondary structure contents ratio of  $A\beta_{42}$ . (h) ThT fluorescence assay of  $A\beta_{42}$  (25 µM),  $A\beta_{42}$ / gCDs and  $A\beta_{42}$ /gCDs-E in 48 h. (i) The corresponding inhibition efficiency of gCDs or gCDs-E. (j) ThT fluorescence assay of preformed  $A\beta$  fibrillar samples that were incubated with or without nanomaterials. (k) The corresponding disaggregation efficiency of gCDs or gCDs-E. (l) AFM images of  $A\beta_{42}$  monomers incubated with or without nanomaterials at pH 7.4 after 24 h. (m) Particle height distributions determined from AFM images, displayed as violin plots.

in Figs. S9a and b, the most negative peaks of  $A\beta_{42}$  fibrils is typical  $\beta$ -sheet structure at 0 h. After adding gCDs and gCDs-E, the negative peaks of  $A\beta_{42}$  fibrils were significantly reduced and the gCDs-E treated group became more significant than that of gCDs (Fig. S9b). Fig. 2h displays a series of inhibition curves of  $A\beta_{42}$  aggregation *in vitro* by a thioflavin T (ThT) assay. The fluorescence intensity of non-treated  $A\beta_{42}$  is sharply changed and much strong at 24 h due to the larger amount of  $A\beta_{42}$  fibrillation formation. However, the fluorescence intensity of  $A\beta_{42}$  treated with gCDs significantly decrease and the inhibition efficiency is only 62.97% (Fig. 2i). gCDs-E treated group shows a weak fluorescence signal, indicating that  $A\beta_{42}$  fibrillation formation is completely

suppressed, and the inhibition efficiency of gCDs-E is higher than 90%. As shown in Fig. 2j, the ThT level of  $A\beta_{42}$  aggregate samples diminished distinctively in the presence of gCDs and gCDs-E during 24 h of incubation, and the disaggregation efficiency of gCDs and gCDs-E were 65% and 76%, respectively. We also used AFM to research  $A\beta_{42}$  treated with gCDs and gCDs-E. As shown in Figure 2l, non-treated  $A\beta_{42}$  is mainly long fibrils.  $A\beta_{42}$  treated with gCDs and gCDs-E were unable to form fibrils or other aggregation. In AFM, these  $A\beta_{42}$  fibrils or clusters have average heights of ~23.7 nm, compared to heights of ~3.1 and ~1.4 nm observed for  $A\beta_{42}$  treated with gCDs and gCDs-E (Figure 2m), respectively.

According to the previous reports, hydrophobic and electrostatic



Fig. 3. (a) and (b) The growth curves of *Candida albicans* after adding EGCG or gCDs-E with different concentrations. (c) The corresponding fungi survival rates after 48 h. (d) and (e) Antifungal activities of the EGCG or gCDs-E against *Candida albicans* evaluated by a standard plate count method.



Fig. 4. (a) The dose dependent cytotoxicity of gCDs and gCDs-E towards neuron cells (SK-N-SH) as determined by CCK-8. (b) Effects of EGCG, gCDs and gCDs-E on cell viability against  $A\beta$ -mediated cytotoxicity.

interactions play important roles in the process of interaction between the carbon materials and  $A\beta$  peptides [65–68]. Previous study showed that the negative charges of nanomaterials can effectively interact with positively charged His residues of  $A\beta$  peptides [65,66]. In this work, gCDs own a similar structure with graphene, and can interact with  $A\beta$  peptide by hydrophobic interactions. Zeta potential analysis showed that the surface of gCDs and gCDs-E were both negatively charged (Fig. S10). Therefore, hydrophobic interactions and electrostatic interactions are the two most important factors of inhibiting the  $A\beta$  peptide aggregation. More importantly, EGCG can directly bind with unfolded protein and react with free primary amine groups of  $A\beta$  peptide, forming a Schiff base, and inducing fibril remodeling [69]. These mechanisms have



**Fig. 5.** (a) The photographs of representative brains of mice after the treatments and fluorescence imaging of brains after different treatments (Control: PBS solution; gCDs solution; gCDs-E solution). (b) The corresponding average fluorescence intensity. (c) CLSM images of brain tissue slices of normal mice treated by gCDs and gCDs-E (Blue and Green signals are DAPI and FL-Dots, respectively). FL-Dots include gCDs and gCDs-E.

greatly promoted the efficiency of gCDs-E to inhibit A $\beta$  fibrillation.

#### 2.3. Evaluation of gCDs-E for inhibiting Candida albicans

Some research reveals that blood-borne infections with Candida albicans are implicated in diseases as diverse as AD [32]. Here, we verify the inhibition ability of gCDs-E for Candida albicans and further demonstrate a novel strategy of treating AD. Fig. 3a and b shows the growth curves of Candida albicans incubated with EGCG and gCDs-E, respectively. The OD<sub>600</sub> values of both EGCG and gCDs-E decreased sharply at 80  $\mu g \ m L^{-1}$  within 24 h. As expected, the antifungal efficiency remarkably increased with the increasing concentration of EGCG or gCDs-E, and the fungi survival rates of Candida albicans treated with EGCG and gCDs-E were only 13.9% and 11.5% at 480  $\mu$ g mL<sup>-1</sup> after 24 h (Fig. 3c), respectively. Then, morphology changes of the Candida albicans were investigated by scanning electron microscopy (SEM). The Candida albicans incubated with gCDs-E shows serious damage in the cell wall and leakage of cellular contents comparing with EGCG treated samples (Fig. S11). However, gCD have not the antifungal properties based on the growth curves of Candida albicans (Fig. S12). Next, the antifungal activities of EGCG and gCDs-E were evaluated by a standard plate count method using Candida albicans. Remarkably, EGCG and gCDs-E displayed a concentration-dependent antifungal activity against Candida albicans (Fig. 3d and e). Compared with EGCG (suppression effect: 23%), an obvious suppression effect on fungal viability (67.2%) was observed for gCDs-E at a low concentration of 80  $\mu$ g mL<sup>-1</sup>. These results indicated that EGCG assembled with gCDs demonstrate effective antifungal functions against Candida albicans.

# 2.4. Anti-A $\beta$ toxicity evaluation

In order to evaluate the biological response of the prepared nanomaterials, we first explored its biocompatibility by measuring cytotoxicity in the human neuroblastoma cell line SK-N-SH. SK-N-SH Cells treated with gCDs or gCDs-E for 24 h were assessed by CCK-8 assay for detecting the cell viability [25,70]. Fig. 4a shows the cytotoxicity of various concentrations of the prepared nanomaterials from 1.8 to 160 µg mL<sup>-1</sup>, Cell viability is observed approximate 85% at a concentration of 160 µg mL<sup>-1</sup>, which suggests that gCDs-E are almost non-toxic to SK-N-SH cells and can be utilized for further in vitro experiments. To measure the anti-A $\beta$  toxicity of gCDs-E, gCDs and EGCG, we detected the cell viability of SK-N-SH cells treated with  $A\beta_{42}$  in the absence and presence of gCDs-E, gCDs and EGCG. As shown in Fig. 4b,  $A\beta_{42}$  alone exhibited obvious toxicity and cell viability was only 62%. However, gCDs-E, gCDs and EGCG were added to suppress the toxicity of  $A\beta_{42}$ . The gCDs-E treated groups showed remarkably higher cell viabilities than gCDs and EGCG treated groups. This difference in cell viabilities indicated that the combination of EGCG and gCDs resulted in a synergistic anti-A<sub>b</sub>-toxicity effect. In addition, gCDs-E, gCDs and EGCG alone exhibited high cell viability with approximate 100%. gCDs-E showed the highest cell viability (99.2%), close to that of the control group (100%) and was screened as the potential lead drugs for inhibiting A $\beta$ -induced toxicity and treating AD.

# 2.5. Brain penetration of the gCDs-E in vivo

Blood-brain barrier (BBB), is a widely considered in vivo experiment as a key factor in the treatment of AD. In order to evaluate the ability of gCDs and gCDs-E for overcoming BBB, we intravenously injected a dose of 1 mg mL<sup>-1</sup> samples into mice. The mice were sacrificed and the brains were harvested for fluorescence imaging. As shown in Fig. 5a, the higher fluorescence signal in gCDs indicated that this gCDs can reach to the brain compared with PBS treated group. In addition, the fluorescence signal of gCDs-E is also higher than PBS treated group, indicating that gCDs-E also can cross the BBB. The ability of gCDs and gCDs-E for overcoming BBB was further confirmed by immunohistochemical method. As shown in Fig. 5b, the distribution of the gCDs or gCDs-E in the hippocampus was further analyzed. The CLSM images displayed obvious dots of green signals (green fluorescence from gCDs; blue fluorescence from DAPI) in the gCDs and gCDs-E treated group. These results suggested that gCDs and gCDs-E could effectively overcome the BBB in vivo. According to previous report [11,71–73], the main method for nanomedicine to cross the BBB is to modify its surface with glucose. As outstanding candidate ligands for promoting BBB traversal, glucose, the main energy source in the brain, is notable because glucose transporter-1 (GLUT1) is expressed at a remarkably high level compared to many other receptors and transporters in brain capillary endothelial cells [74]. Based on current and previous work [75], the surface of gCDs carbonized by glucose own incompletely reacted glucose structure, which will promote the glucose-functionalized gCDs to cross the BBB through the dependence of glucose transporters.

#### 2.6. Improvement of memory deficits of APP/PS1 mice

As shown in Fig. 6a, the Morris Water Maze test was used to detect whether gCDs or gCDs-E could improve spatial learning ability in APP/ PS1 mice. As expected, non-treated APP/PS1 mice showed significant learning deficits. Fig. 6b shows that the learning ability of gCDs-E-treated mice were improved, such as a shorter escape latency after 5 days, longer residence time at the target platform position, and a greater possibility of



**Fig. 6.** (a) Time schedule of the experimental procedure for APP/PS1 mice. (b) Representative searching paths in Morris Water Maze (MWM) test. (c) Comparison of learning path delay time between different treatment groups. (d) The latency during the memory test in the MWM probe trial without a platform. (e) The percent (s) of time in the targeted quadrant where the platform had been located during the memory test in the MWM probe trial.

reaching the target platform quadrant (Fig. 6b, c and d). More importantly, gCDs-E exhibit significant performance improvement in APP/PS1 mice cognitive ability compared with that of gCDs.

In addition, key factors of AD about A $\beta$  plaques and neuronal loss in the hippocampus were evaluated. Nissl staining analysis (Fig. 7a and c) results reveal that the non-treated and gCDs-treated APP/PS1 mice had few Nissl bodies compared to gCDs-E treated group. In other words, gCDs-E treatment added more neurons with restored integrity, and gCDs treatments is less effective than gCDs-E. An immunohistochemistry analysis was also performed on mouse brains (Fig. 7b and d). The A $\beta$ plaques in the gCDs-E-treated APP/PS1 mice decreased significantly compared with the control and gCDs-treated AD mice, indicating that gCDs-E reduces A $\beta$  plaques. These results indicated that gCDs-E had synergistic therapeutic effects on reducing amyloid plaque and inhibiting neuronal loss in APP/PS1 mice.

# 2.7. Biocompatibility evaluation of nanomaterials

The cytotoxicity is primary factor for application of nanomaterials in biomedicine. As shown in Fig. S13, the cell viability of the NRK cells remains higher than 90% when the concentration of gCDs and gCDs-E increases from 1.8 to 160  $\mu$ g mL<sup>-1</sup>. This result indicates that no significant toxicity was noted in either system at the tested exposure levels. Hemocompatibility is the first-level evaluation before the nanomaterials

was administered via tail vein injection [20]. As shown in Fig. S14, hemolysis degree of gCDs and gCDs-E is relatively low and the value of gCDs are 2.459% (80  $\mu$ g/mL) and 2.76% (160  $\mu$ g/mL), and the value of gCDs-E are 2.7% (80 µg/mL) and 3.93% (160 µg/mL), respectively. These results indicate that the gCDs and gCDs-E are safe for intravenous administration. The biocompatibility of gCDs and gCDs-E was analyzed in APP/PS1 mice, and the change in body weight after injecting the drug was measured (Fig. 7e). No significant difference in body weight was observed among gCDs or gCDs-E-treated APP/PS1 mice within 17 days. Further, normal mice were treated with different treatments (including PBS, gCDs, and gCDs-E treating), and no abnormal behavior was monitored and the main organs (Heart, Liver, Spleen, Lung, Kidney) of the mice were harvested for histopathological analysis. As shown in Fig. 7f, no obvious pathological abnormalities were detected, which indicated that gCDs and gCDs-E had a favorable biocompatibility, and could be used for further application of AD treatment.

# 3. Conclusions

In conclusion, we successfully fabricated dual-target nanoassemblies (namely gCDs-E) assembled with EGCG and glycosylated carbon dots, and have proposed an innovative multi-target therapeutic strategy for the treatment of AD. It is demonstrated that gCDs-E can effectively prevent misfolding of  $A\beta$  and inhibit its aggregation *in vitro*, and the inhibition



**Fig. 7.** (a) The Nissl staining of nerve cells in the brains of AD control mice, AD mice treated with gCDs, and AD mice treated with gCDs-E. (b) The immunohistochemical analysis of  $A\beta_{42}$  deposition in the brains of AD control mice, AD mice treated with gCDs, and AD mice treated with gCDs-E. (c) and (d) were the quantified results of (a, b), respectively. (e) Relative body weight of APP/PS1 mice after the treatment of PBS, gCDs, and gCDs-E in 17 days. (f) Hematoxylin and eosin (H&E) staining of the main organs (Heart, Liver, Spleen, Lung, Kidney) after PBS, gCDs, and gCDs-E injection.

efficiency is higher than 90%. CCK-8 experiments show that gCDs-E can remarkably reduce  $A\beta$ -mediated cytotoxicity. Importantly, gCDs-E also can suppress *Candida albicans* activity, which could prevent memory loss caused by fungal infection. *In vitro* and *in vivo* experiments confirm the gCDs-E's high-biocompatibility and ability of BBB penetration.

Furthermore, the gCDs-E can greatly clean  $A\beta$  deposition and improve memory impairment in APP/PS1 transgenic AD model mice. Therefore, gCDs-E nanomaterials can serve as a novel nanoplatform, exhibiting great potential therapeutic prospect in the treatment of AD.

# Credit author statement

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# Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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#### Appendix A. Supplementary data

Supplementary data to this article can be found online at https://doi.org/10.1016/j.mtbio.2021.100167.

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