Effect of tumour necrosis factor on the uptake of specific and control monoclonal antibodies in a human tumour xenograft model

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> Summary The investigations reported in this paper aim to exploit tumour necrosis factor (TNF)-induced vascular changes in an attempt to increase the tumour uptake of specific monoclonal antibody. The vascular permeability to monoclonal antibody of a human tumour xenograft increased 2.6-fold by ¹ h post injection of $2.5 \times 10³$ U of TNF, although this effect was lost by 3 h. The normal tissues also demonstrated increased vascular permeability to IgG, but to a lesser exent. Liver permeability increased 1.5-fold at ^I h but returned to the control value by 6 h. Lung permeability increased 1.4-fold at ¹ h post injection and returned to normal by 3 h. Muscle values were not significantly increased compared with controls. The blood activity was cleared more quickly in the TNF-treated mice $(t_{ij} = 101 \text{ h}$, compared with 121 h in control mice). This was probably due to the increased vascular permeability in normal organs of treated mice. At ^I day and ³ days post injection, the tumour uptake of the specific, but not the control, antibody was significantly increased by 25% and 29% respectively. This resulted in an increase in the area under the tumour activity curve, and therefore tumour radiation dose, of 25% in treated compared with control mice. In addition, ^a consequence of the faster blood clearance of the isotope in the TNF-treated mice was a reduction in the area under the blood activity curve of 12%, thereby reducing systemic toxicity. The increase in vascular permeability to IgG following TNF injection resulted in both specific and control antibodies having improved access to the tumour antigens, and a transient increase in uptake was observed. Only in the case of the specific antibody was the increase maintained, since this antibody binds to the available antigenic sites, whereas the control antibody was cleared from the tumour without binding. No evidence of tumour necrosis was observed at the TNF doses given, nor was there any toxicity to the mice.

Keywords: antibody; tumour necrosis factor; vascular permeability; xenograft

Vascular parameters such as blood flow, vascular permeability and vascular volume are serious obstacles limiting delivery of cytotoxic agents, including radiolabelled monoclonal antibodies, to tumours. Antibody access to tumour cells may be limited by the tumour vasculature, with its abnormal vessels and poor blood flow, and by regions of high interstitial pressure (Jain and Baxter, 1988; Jain, 1991).

Tumour vascular permeability and blood flow have been shown to correlate well with the uptake of monoclonal antibody in two different human tumour xenografts, the tumour having twice the vascular permeability, resulting in a 5-fold increase in antibody uptake (Sands et al., 1988). However, few attempts have been made to alter tumour vascular parameters. Bomber et al. (1986) showed that the β -blocker propranolol increases tumour perfusion and 67Ga uptake in a mouse sarcoma. Smyth et al. (1987) have shown, in a xenograft model, that both non-selective and cardioselective Padrenergic blocking agents increase the tumour-blood and tumour-liver uptake ratios of 125 I-labelled monoclonal antibody. Attard et al. (1991) used the corticosteroid dexamethasone to reduce tumour interstitial pressure and thereby increase the tumour-background ratios in patients being investigated by immunoscintigraphy. In one patient, two metastatic deposits which were not visible without dexamethasone administration became visible after dexamethasone. Tumour vessels differ from normal vessels, particularly in lacking sufficient smooth muscle to dilate or constrict in response to drugs which have these effects on normal blood vessels. By their selective action on normal blood vessels, vasoactive drugs can change the tumour-normal tissue perfusion ratio (Chan et al., 1984).

The cytokine interleukin 2 (IL-2) has been shown to increase vascular permeability in normal organs, either alone (Rosenstein et al., 1986) or in combination with lymphokineactivated killer cells (Ettinghausen et al., 1988). Tumour necrosis factor (TNF) is another cytokine which has been shown to increase endothelial permeability directly, as measured in endothelial cell monolayers (Royall et al., 1989). In vivo, TNF is known to be ^a mediator of the inflammatory response, and can lead to diffuse intravascular coagulation with consequent changes in vascular permeability. This damage to tumour vasculature induces ischaemia and haemorrhagic necrosis of the tumour within 24 h of administration, both in animal models (Palladino et al., 1987; van de Wiel et al., 1989) and in a patient (Robertson et al., 1989). This phenomenon was first exploited by Coley (1891), who treated sarcoma patients by injecting bacterial cultures containing Streptococcus erysipelatis, and noted tumour regressions, some complete, in many patients. The principal active constituent of Coley's toxins was undoubtedly lipopolysaccharide (LPS), which is a potent inducer of TNF. Endotoxic shock is associated with acute vascular endothelial injury resulting in oedema (Brunson et al., 1955). Administration of TNF to rats, in doses similar to those produced endogenously in response to endotoxin, produces many of the symptoms of LPS toxaemia, including hypotension, pulmonary inflammation and haemorrhage (Tracey et al., 1986). Pulmonary vascular leakage has also been induced in sheep by injection of TNF (Horvath et al., 1988). The barrier function of the endothelium has been shown to be altered directly by TNF (Sato et al., 1986). Aicher et al. (1990) have detected changes in capillary permeability to gadolinium-conjugated albumin in Meth A sarcomas in mice following TNF administration by means of contrast-enhanced magnetic resonance imaging. van de Wiel et al. (1989) suggested that the broad interference of tumour blood supply was the major cause of necrosis of Meth A sarcomas in mice, since TNF did not affect the Meth A cells in vitro. TNF has been shown to increase vascular permeability in vivo immediately after injection (Kallinowski et al., 1989), and to affect the functional and structural vascular volume in solid murine tumours (van

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de Wiel et al., 1990). Since poor vasculature is one of the factors limiting antibody uptake in tumours (Jain, 1991), if tumour vascular permeability could be increased by the administration of TNF, this would facilitate antibody access to tumour cell antigens. The investigations reported in this paper aim to exploit these vascular changes in an attempt to increase the tumour uptake of specific monoclonal antibody.

Materials and methods

Tumour model

The animals used in these studies were female nude mice of mixed genetic background. They were bred under specific pathogen-free conditions at the Imperial Cancer Research Fund Animal Breeding Unit, South Mimms, Herts, UK, and subsequently housed in sterile filter-top cages with sterile bedding, and maintained on irradiated diet and autoclaved, acidified water (pH 2.8).

The human tumour cell line HT29 was established in cell culture in 1964 from a primary tumour in a female patient with adenocarcinoma of the colon (Fogh and Trempe, 1975). Tumour cells were cultured in RPMI-1640 medium containing 100 U ml⁻¹ penicillin and $100 \mu g$ ml⁻¹ streptomycin, supplemented with 10% fetal calf serum (FCS) (Gibco, Paisley, UK) at 37°C in a humidified atmosphere of 5% carbon dioxide in air. Tumours were established in the right flanks of the mice by subcutaneous injection of 5×10^6 cells in 100 pl of tissue culture medium. Animals were used for experiment $3-4$ weeks later, when the tumours were $6-8$ mm in diameter.

Antibodies

AUAI Monoclonal antibody AUA1, of the IgGI subclass, was raised by immunising Balb/c mice with a human colon carcinoma cell line (Arklie, 1981). AUA1 recognises a M_r 35 000 cell-surface glycoprotein, which is coded for by a gene on chromosome 2, and which is only expressed in epithelial cells (Spurr et al., 1986). The antibody reacts with a wide range of tumours of epithelial origin such as breast, lung, ovarian and gastrointestinal cancers, as well as with proliferating epithelial cells in tissues such as normal colon, but not with any non-epithelial tissues or tumours (Arklie, 1981; Spurr et al., 1986). AUA1 was used as the specific antibody for HT29 tumours.

HMFGI This monoclonal antibody, also IgG1, was raised in Balb/c mice using delipidated human milk fat globule as immunogen (Taylor-Papadimitriou et al., 1981). The antibody is directed against a core protein determinant of a high molecular weight glycoprotein $(M_r > 400000)$ normally produced by the lactating human mammary epithelial cell (Burchell et al., 1987), but also found on some carcinomas, such as those of breast, ovary and lung, but not with tumours of mesenchymal tissue (Arklie et al., 1981). HMFG1 does not bind to HT29 cells and was used as the irrelevant control antibody.

Radiolabelling

Antibodies were labelled with '25I or '3'I (IMS 30 and IBS 30 respectively; Amersham International, Amersham, Bucks, UK) to a specific activity of approximately 2μ Ci μ g⁻¹ using the lodo-Gen method (Fraker and Speck, 1978).

Tumour necrosis factor

Recombinant human tumour necrosis factor (specific activity 2.27×10^6 U mg⁻¹) was supplied by Asahi Chemical Industry, Tokyo, Japan. Vials containing $10⁵$ U (44 μ g) in 1 ml of water were stored at -20° C until immediately before use.

Vascular studies

Vascular volume and vascular permeability to IgG were determined for groups of control and TNF-treated mice bearing s.c. HT29 xenografts. In the treated groups of mice, 2.5×10^3 U of TNF was injected i.v. at 1, 3, 6 and 24 h before injection of radioactivity. Vascular volume and vascular permeability were determined by the method of Song and Levitt (1970), as modified by Sands et al. (1985), who replaced ⁵¹Cr labelling of erythrocytes in vitro with radiolabelling in vivo using ^{99m}Tc (Pavel et al., 1977).

Groups of tumour-bearing mice were given i.v. injections of 1.2 μ g of stannous fluoride in 100 μ l of saline (Amerscan; Amersham International) via a lateral tail vein. This was followed after 30 min by an i.v. injection of a mixture of 25 μ Ci of [^{99m}Tc]technetium pertechnetate and 10 μ Ci (5 μ g) of '25I-labelled HMFG1 antibody. Exactly ¹ h post injection of radioactivity, mice were killed by cervical dislocation, and then tumour, liver, lung, muscle and a small sample of blood were removed, weighed and their ^{39II}TC activity counted in a y-counter. The low energy of the ¹²⁵I emission does not interfere with the detection of the ^{99m}Tc activity. After allowing sufficient time for the total decay of the $\frac{95 \text{ m}}{\text{TC}}$ ($t_1 = 6 \text{ h}$), the tissues were counted again to determine their ¹²⁵I content. The vascular volume (VV) in units of ml blood per g of tissue was calculated according to the formula:

$$
VV = \frac{\%m}{\%m}Tc \text{ activity } g^{-1} \text{ in tissue}
$$

$$
g^{-1} \text{ in blood}
$$

The vascular permeability (VP) to IgG was determined by calculating the amount of ^{125}I -labelled irrelevant antibody extravasated in 1 h, defined as the total plasma 125 I c.p.m. g^{-1} of tissue minus the intravascular plasma ^{125}I c.p.m. g^{-1} tissue. This was calculated in units of $mlh^{-1}g^{-1}$ tissue as:

 125 I c.p.m. g^{-1} in tissu $VP = \frac{^{125}}{^{125}} \frac{c.p.m. g^{-1}}{c.p.m. g^{-1}}$ in blood – VV (1 – haematocrit)

The haematocrit (the percentage red cell volume in the blood) was measured for several mice and found to agree with the published value for mice of 40% (Green, 1979), which was therefore used in all calculations. It has been found, however, that the haematocrit in tissues is less than that in the systemic circulation (O'Connor and Bale, 1984). Since, in the present study, vascular permeability is compared within the model in tumour and normal organs with and without TNF administration, then if the haematocrit were different from the systemic value this would result in a systematic error in both measurements, as it is unlikely that TNF administration alters the haematocrit.

The efficiency of red cell labelling was estimated by injecting a group of mice with the same reagents at the same time intervals as the experimental animals, and killing them by exsanguination ¹ h post injection of radioisotopes. The blood was then centrifuged for 15 min at 2000 r.p.m. in a bench centrifuge to isolate the red cells, which were washed twice with phosphate-buffered saline (PBS). The ^{125}I and ^{99m}Tc activities in the erythrocytes and plasma were measured.

Biodistribution

Nude mice bearing s.c. HT29 tumours were given a mixture of 5 µg each of ¹³¹I-labelled AUA1 and ¹²⁵I-labelled HMFG1 antibodies i.v. In half the mice 2.5×10^3 U of TNF was combined with the injected antibody. Groups of four treated and control mice were dissected at times between 2 h and 6 days after antibody administration.

Statistical analysis

The statistical significance of the difference between means was determined using the Student's t-test. A P-value ≤ 0.05 was considered to be significant.

Results

Effect of TNF on tumour vascular parameters

The efficiency of red cell labelling in vivo was measured as described. The washed cells contained 98% of the ^{99m}Tc activity, while the plasma contained 99.5% of the ^{125}I activity, confirming the validity of the method. No evidence of tumour necrosis was observed at the TNF doses given, nor any toxicity to the mice.

Figures 1 and 2 show the effect of i.v. TNF $(2.5 \times 10^3 \text{ U})$ on the vascular volume and vascular permeability to IgG in treated and control mice bearing s.c. HT29 tumours. There was no significant difference in the vascular volume in any tissue at any time after i.v. TNF injection, except for liver at 1 and 3 h post injection. In contrast, the vascular permeability of tumour was increased 2.6-fold by 1 h post injection of TNF ($P \le 0.001$), although this effect was lost by 3 h. The normal tissues also demonstrated increased vascular permeability but to a lesser exent. Liver permeability increased 1.5-fold at 1 h $(P<0.02)$, but returned to the control value

Figure ¹ Vascular volume of HT29 tumour, lung, liver and muscle in control mice (C) and in mice given 2.5×10^3 U of TNF i.v. at 1 h, 3 h, 6 h and 24 h before injection of the $[^{99m}Tc]$ technetium pertechnetate and ¹²⁵I-labelled control antibody used to measure these parameters. Each bar represents the mean and s.d. of four mice.

Figure 2 Vascular permeability of HT29 tumour, lung, liver and muscle in control mice (C) and in mice given 2.5×10^3 U of TNF i.v. at 1 h, 3 h, 6 h and 24 h before injection of the $199m$ Tc]technetium pertechnetate and ¹²⁵I-labelled control antibody employed to measure these parameters. Each bar represents the mean and s.d. of four mice.

by 6 h. Lung permeability increased 1.4-fold at ¹ h post injection ($P \leq 0.02$) and returned to normal by 3 h. Muscle values did not increase significantly from controls.

Effect of TNF on antibody biodistribution

Tables ^I and II show the uptake of co-injected specific (AUAI) and control (HMFGl) antibodies, with or without the inclusion of 2.5×10^3 U of TNF, in mice bearing s.c. HT29 xenografts. The blood activity was cleared more quickly in the TNF-treated mice (for AUAl and HMFG1, respectively, $t_{18} = 101$ h and 101 h in TNF-treated mice compared with 121 h and 115 h in control mice). Although there are few time points used to calculate these values, since the same result is observed for both antibodies, it may be a genuine effect caused by increased vascular permeability in normal organs of treated mice. Two hours post injection, the tumour uptake of both antibodies was increased 2-fold, however this

Table ^I Percentage of administered dose of specific (AUAI) antibody per gram of tissue at the following times post injection. In half the mice, 2.5×10^3 U of TNF was included in the injectate. Each value represents the mean \pm s.d. of four mice

	2 h	l day	3 days	6 days
With 2.5×10^3 U TNF				
Blood	27.7 ± 3.2	15.8 ± 1.8	10.5 ± 0.7	6.9 ± 0.9
Tumour	8.1 ± 3.3	$7.3 \pm 0.5*$	$6.2 \pm 0.6*$	3.5 ± 0.8
Stomach	2.3 ± 0.4	2.1 ± 0.7	1.8 ± 0.9	0.9 ± 0.1
Intestine	3.9 ± 1.4	1.9 ± 0.3	1.2 ± 0.2	0.9 ± 0.1
Kidney	6.9 ± 0.6	3.8 ± 0.6	2.8 ± 0.6	1.5 ± 0.3
Spleen	5.4 ± 0.4	3.4 ± 0.7	1.9 ± 0.2	1.3 ± 0.1
Lung	7.6 ± 0.6	6.6 ± 1.2 **	3.6 ± 0.4 **	2.3 ± 0.5
Liver	8.9 ± 0.8	3.7 ± 0.7	2.3 ± 0.3	1.5 ± 0.2
Muscle	0.4 ± 0.1	0.7 ± 0.1	0.6 ± 0.1	0.4 ± 0.1
Without TNF				
Blood	28.4 ± 3.7	15.4 ± 0.6	13.7 ± 2.7	7.4 ± 1.5
Tumour	4.9 ± 1.9	5.8 ± 0.9	4.8 ± 0.3	3.6 ± 0.6
Stomach	2.0 ± 0.2	1.8 ± 0.2	1.7 ± 0.1	0.9 ± 0.2
Intestine	2.9 ± 0.2	1.6 ± 0.2	1.4 ± 0.1	0.9 ± 0.4
Kidney	6.4 ± 0.6	3.6 ± 0.2	2.9 ± 0.3	1.7 ± 0.5
Spleen	5.0 ± 0.5	2.9 ± 0.3	2.6 ± 0.5	1.3 ± 0.2
Lungs	7.9 ± 2.0	4.8 ± 0.1	5.3 ± 1.2	2.7 ± 0.5
Liver	7.4 ± 0.7	3.7 ± 0.2	3.4 ± 0.9	1.6 ± 0.4
Muscle	0.6 ± 0.1	0.8 ± 0.1	0.7 ± 0.1	0.4 ± 0.1

 $*P<0.05$, $*P<0.01$ compared with untreated mice.

Table II Percentage of administered dose of control (HMFGI) antibody per gram of tissue at the following times post injection. In half the mice, 2.5×10^3 U of TNF was included in the injectate. Each value represents the mean \pm s.d. of four mice

2 h	1 day	3 days	6 days	
With 2.5×10^3 U TNF				
25.3 ± 2.7	12.1 ± 1.1	8.1 ± 0.5	5.3 ± 0.6	
6.6 ± 2.9	3.9 ± 0.6	3.1 ± 0.3	1.8 ± 0.4	
3.7 ± 0.6 **	2.5 ± 1.4	1.4 ± 0.7	0.7 ± 0.0	
4.8 ± 2.1	1.8 ± 0.4	1.0 ± 0.2	0.7 ± 0.0	
6.7 ± 0.7	3.1 ± 0.4	2.2 ± 0.4	1.2 ± 0.2	
12.2 ± 4.9	3.1 ± 0.5	1.5 ± 0.2	1.0 ± 0.1	
7.4 ± 0.7	$5.3 \pm 1.1***$	2.7 ± 0.3 **	1.7 ± 0.4	
$11.5 \pm 0.9*$	3.3 ± 0.8	1.8 ± 0.2	1.1 ± 0.1	
0.4 ± 0.1	0.6 ± 0.1	0.5 ± 0.0	0.3 ± 0.0	
Without TNF				
25.7 ± 2.8	11.6 ± 0.6	10.5 ± 2.5	5.6 ± 0.6	
3.3 ± 0.8	3.5 ± 0.3	2.8 ± 0.2	1.9 ± 0.1	
2.7 ± 0.4	1.7 ± 0.2	1.3 ± 0.1	0.7 ± 0.1	
3.1 ± 0.2	1.4 ± 0.3	1.1 ± 0.1	0.7 ± 0.2	
5.9 ± 0.5	2.9 ± 0.2	2.3 ± 0.3	1.3 ± 0.2	
7.7 ± 1.1	2.7 ± 0.4	2.2 ± 0.6	1.0 ± 0.1	
7.5 ± 1.7	3.7 ± 0.2	3.9 ± 0.9	2.1 ± 0.2	
9.0 ± 0.8	3.1 ± 0.1	2.7 ± 0.9	1.2 ± 0.2	
0.5 ± 0.1	0.6 ± 0.1	0.6 ± 0.2	0.3 ± 0.0	

 $*P< 0.05$, $*P< 0.01$ compared with untreated mice.

was not significant owing to the large errors on the data points. The tumour uptake of the control antibody (Table II) was within the range of the normal organs at all time points studied, while the tumour uptake of the specific antibody (Table I) was higher than all normal organs by 1 day post injection. At 1 day and 3 days post injection, the tumour uptake of the specific, but not the control, antibody was significantly increased by 25% and 29%, respectively, compared with that in untreated mice. This results in an increase in the area under the tumour activity curve, and therefore tumour radiation dose, of 25% in treated compared with control mice, as shown in Figure 3. In addition, a consequence of the faster blood clearance of the isotope in the TNF-treated mice is a reduction in the area under the blood activity curve of 12%, thereby reducing systemic toxicity.

Discussion

The increase in tumour vascular permeability following TNF injection (Figure 2) resulted in both specific and control antibodies having improved access to the tumour antigens, and a transient increase in uptake was observed. As seen in Tables I and II, only in the case of AUA1 was the increase maintained, since this antibody binds to the available antigenic sites, whereas HMFG1 is cleared from the tumour without binding. Liver and lung also showed a transient increase in vascular permeability after TNF treatment, but this did not result in increased antibody uptake, since the antibodies do not bind to normal organs.

In this paper, intravenous TNF has been shown to increase the vascular permeability of tumour and normal tissue, resulting in a sustained increase in uptake of specific, but not control, radiolabelled antibody in tumour bu tissue. Russell et al. (1990) found that murine TNF increased the level of antibody in a murine thymoma increased the cytotoxicity of an aminopterin-antibody conjugate in established tumours. Similarly, Melton et al. (1993) have shown that co-administration of human TNF increases uptake of an antibody-carboxypeptidase G_2 conjugate in a human tumour xenograft in nude mice. As in the present investigation, decreased blood activity was also observed in the latter study. No vascular parameters were measured in either of these studies. In contrast, Pimm et al. (1991) found that, 4 h after i.v. injection of human TNF, bl reduced in treated tumours compared with controls. In their study, TNF did not significantly alter the uptak in human osteosarcoma and gastric cancer xenografts, although the antibody and TNF were not administered simultaneously, and the number of mice was small. Changes

Figure 3 Tumour uptake of AUA1 antibody in mice receiving concurrent administration of 2.5×10^3 U of TNF (solid line) and in control mice (broken line). The increase in area under the curve in treated mice is proportional to the increase in radiation dose to the tumour.

in vascular permeability were not measured. The importance of tumour vascular permeability in relation to antibody uptake has been demonstrated by Sands et al. (1988), who showed that a renal cell carcinoma xenograft having twice the permeability of a breast tumour xenograft accumulated five times the amount of monoclonal antibody by 24 h post injection. In the present study, the TNF-induced elevation in tumour vascular permeability was short-lived, returning to the untreated value by 3 h (Figure 2), so that the concurrent administration of TNF and antibody is probably a major factor in the success of TNF in increasing the antibody uptake by tumour. Folli et al. (1993) have recently reported similar results using TNF and an anti-CEA antibody administered i.v. or intra-tumorally in four different human colon carcinoma xenografts. Clearly, intra-tumour injection of TNF would be suitable only for localised and not metastatic disease. However, we have previously shown that intratumour injection of radiolabelled monoclonal antibody alone results in very high levels of radioactivity in the tumour (Rowlinson-Busza et al., 1991).

Other properties of tumour necrosis factor may make it a useful complement to radioimmunotherapy. The half-life of the radiolabelled antibody in the circulation was reduced in the TNF-treated mice, which would reduce the radiation dose to bone marrow, and therefore myelotoxicity. A different inflammatory cytokine, IL-1, has been shown to be a radioprotector (Neta et al., 1986). Old (1987) proposed that this may also be true of TNF, since TNF is one of the main mediators of endotoxin lipopolysaccharide action, and bacterial endotoxins have been shown to protect mice against lethal doses of X-rays (Smith et al., 1957). Neta et al. (1988) have also shown that human recombinant TNF protects lethally irradiated mice from death, but not as effectively as IL-1 on a dose per mouse basis. In addition, they demonstrated that administration of the two cytokines together resulted in additive radioprotection, implying that they each act through different radioprotective pathways. The same group has also shown that administration of anti-TNF antibodies reduces survival in irradiated mice, suggesting that natural levels of TNF contribute to radioresistance of normal mice (Neta et al., 1991). In addition, the radioprotective effect of systemically administered TNF could be blocked not only by anti-TNF antibody, but also by an antibody against the IL-1 receptor. Slørdal et al. (1989) have demonstrated TNF-dose-dependent enhancement of haematological recovery after irradiation in TNF-treated mice. A possible mechanism for this radioprotection is the induction by TNF of mRNA for manganous superoxide dismutase (MnSOD) (Wong and Goeddel, 1988). MnSOD is an enzyme which protects against oxidative damage by potentially toxic superoxide radicals, which can be produced by irradiation. Since the haematopoietic system is much more radiosensitive than the tumour cells, then this property of TNF and the more rapid blood clearance of radioactivity should selectively protect against myelosuppression during radioimmunotherapy, and allow a higher dose of radiation to be delivered to the tumour.

The mice in the studies presented in this paper tolerated 2.5×10^3 U (175 μ g m⁻²) of TNF well, although the T-cell deficiency of nude mice may have accounted for the lack of an inflammatory response. In addition, human TNF has been shown to react with the murine TNF receptor ¹ on tumour an inflammatory response. In addition, human TNF has been
shown to react with the murine TNF receptor 1 on tumour
and endothelial cells, but not with the murine TNF receptor
2 on thymocytes and cytotoxic lymphocytes (Tarta and endothelial cells, but not with the murine TNF receptor 1991). Phase ^I clinical trials have shown that the maximum tolerated single dose of TNF in humans is $350 \,\mu g$ m⁻²i.v. (Abbruzzese et al., 1989). Thus, it should be possible to increase the antibody uptake in tumours in patients with ⁶ cancer by the concurrent administration of a tolerable dose of TNF. The additional inflammatory response in patients, not observed in athymic mice, may also facilitate antibody access to tumour.

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ea under the The effect of TNF could be increased by targeting it directly to the tumour, resulting in an increased local concentration. Therefore, although TNF may be more toxic in

humans than in nude mice, targeting an antibody-TNF fusion protein to the tumour should allow lower doses to be given systemically to achieve the same tumour dose. Hoogenboom et al. (1991) have produced a hybridoma capable of secreting an antibody-TNF fusion protein which retains the biological activities of both constituent molecules in vitro. This type of fusion protein may be capable of specifically increasing tumour vascular permeability without the increase

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in normal tissue permeability observed in the studies reported in this paper. A recombinant fusion protein of ^a single-chain Fv region and IL-2 which retains the biological properties of each constituent protein has been produced (Savage et al., 1993). This method should also be suitable for TNF-sFv fusions, since the gene for human TNF has been cloned and expressed in Escherichia coli (Shirai et al., 1985).

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