

Atomic force microscopy fishing and mass spectrometry identification of gp120 on immobilized aptamers

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Abstract: Atomic force microscopy (AFM) was applied to carry out direct and label-free detection of gp120 human immunodeficiency virus type 1 envelope glycoprotein as a target protein. This approach was based on the AFM fishing of gp120 from the analyte solution using anti-gp120 aptamers immobilized on the AFM chip to count gp120/aptamer complexes that were formed on the chip surface. The comparison of image contrasts of fished gp120 against the background of immobilized aptamers and anti-gp120 antibodies on the AFM images was conducted. It was shown that an image contrast of the protein/aptamer complexes was two-fold higher than the contrast of the protein/antibody complexes. Mass spectrometry identification provided an additional confirmation of the target protein presence on the AFM chips after biospecific fishing to avoid any artifacts.

Keywords: gp120 HIV-1 envelope glycoprotein, aptamer, atomic force microscopy, mass spectrometry

Introduction

It is well established that 20%–80% of people worldwide who have human immunodeficiency virus (HIV) infection do not know their HIV status.¹ There are two types of tests in clinical practice to confirm HIV infection. Of them, HIV enzyme-linked immunosorbent assay (ELISA) and Western blot are designed to react in the presence of HIV antibodies in biomaterial (plasma/serum or saliva). A current list of HIV diagnostic tests approved by the US Food and Drug Administration includes 12 ELISA assays that detect antibodies to HIV types 1 and 2 (September 2013, <http://www.fda.gov/BiologicsBloodVaccines/BloodBloodProducts/ApprovedProducts/LicensedProductsBLAs/BloodDonorScreening/InfectiousDisease/UCM080466>).

Usually, measurable levels of HIV antibodies are developed within 30 days of infection, although sometimes this rise in level may take longer and lasts up to 3 months. Thus, during the first weeks after infection, there is a window period when antibody levels are too low to be detected reliably. During this time, an infected person can pass HIV to others, but he or she still has a negative result for the antibody test.²

ELISA tests have limitations besides inefficiency for early diagnosis due to false positive and negative results. Major causes of false positive HIV ELISA are provided by antibodies to human leukocyte antigens, multiple transfusions, recent influenza immunization, and improper specimen handling. False negative HIV ELISA results are caused by recent infection (window period), hypogammaglobulinemia, advanced HIV infection, and unusual HIV-1 serotype (group O).³ It is therefore important to develop biosensors for direct detection of infection to confirm the presence of HIV

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antigens in biomaterial to test recently infected people, who are unaware of their infection.

Accordingly, the development of lab-on-a-chip devices with a wide range of time-stable molecular probes for high-sensitivity analysis and early detection of the infection presents one of the major challenges in clinical proteomics and diagnostics.⁴ Analyzers in the recording part of these devices can be optical,⁵ electrical,^{6,7} or even nanomechanical, such as atomic force microscopy (AFM).⁸ To perform a biospecific direct detection of proteins in this case, it is necessary to use molecular probes (antibodies or aptamers) covalently immobilized on the chip surface. Implementation of these chips for detection of proteins in the analyte is restrained by a limited variety of commonly used molecular probes such as antibodies.

Deoxyribonucleic acid (DNA) aptamers offer an attractive alternative to antibodies as affinity reagents for protein detection. Aptamers are single-stranded DNA or ribonucleic acid structures generated via systematic evolution of ligands by exponential enrichment *in vitro* from a large library of randomized oligonucleotide sequences ($>10^{13}$).^{9,10} While aptamers are analogous to antibodies in their range of target recognition and variety of applications, they possess several key advantages over their protein counterparts.¹¹ Thus, they are self-refolding, single-chain, and redox insensitive; tolerate pH and heating levels that proteins do not; are easier and more economical to produce; are capable of having greater specificity and affinity than antibodies;¹² and are much more stable at ambient temperature than antibodies, yielding a much higher shelf-life. They can also tolerate transportation without any special requirements for cooling, eliminating the need for a continuous cold chain.¹³

Usability of aptamers as affinity reagents was demonstrated in recent papers^{14–18} where fluorescent^{14–16} and electrochemical analyses¹⁷ as well as surface plasmon resonance with interferometry¹⁸ were used, and data were obtained by measurement of properties of a molecular ensemble. In our study, AFM was used as a detector. It allows registration of single biomolecules on the AFM chip surface. Therefore, the sensitivity of analysis with an AFM-based molecular detector will not be limited by the sensitivity of the analyzer. AFM is broadly used due to its wide capabilities for determination of the interaction force between the tip-tethered aptamer and a protein immobilized on the substrate surface,^{19–21} and also for biospecific recognition of protein on the surface.^{22,23} The most popular object of aptamer-based applications in molecular research is detection of thrombin.^{24–27} The goal of our research was to highlight the advantages of aptamers as molecular probes for biospecific fishing of gp120 HIV

protein from the solution on the AFM chip surface. The aptamer-based approach is promising for development of high-sensitivity detection methods in proteomics and diagnostics. To demonstrate the potential of this approach, the following experiments were conducted: 1) aptamers were covalently immobilized on the AFM chip; 2) immobilized aptamers were visualized by AFM in a standard tapping mode and in a topography and recognition (TREC) mode; 3) AFM-biospecific fishing of the target protein was carried out using two types of AFM chips with different molecular probes, such as immobilized aptamers and immobilized antibodies; 4) the values of image contrast of protein/aptamer and protein/antibody complexes on the AFM images were estimated and compared; and 5) mass spectrometry (MS) identification of protein, fished out from the analyte solution onto the two types of immobilized molecular probes, was performed.

Anti-gp120 aptamers were used as molecular probes immobilized on the AFM chip. Gp120 was selected because it is the HIV-1 envelope protein and a biomarker in a medical diagnosis.²⁸ It was shown that AFM chips with immobilized anti-gp120 aptamers can be used to fish out gp120 from solution, and also to visualize and count its molecules, while a combination of AFM with MS allows identification of the protein fished out onto the AFM chip.

Materials and methods

Materials

Modified Dulbecco's phosphate buffer (PBS-D, 10 mM, pH 7.4), dithiobis-(succinimidyl propionate) (DSP) cross-linker, acetonitrile, trifluoroacetic acid (TFA), and ammonium bicarbonate were purchased from Pierce (USA). 3-aminopropyltriethoxysilane (APTES) and dimethyl sulfoxide were purchased from Sigma-Aldrich Co. (St Louis, MO, USA). α -Cyano-4-hydroxycinnamic acid (HCCA) and dihydroxybenzoic acid were purchased from Acros (USA). Ultrapure water was obtained using a Milli-Q system (Millipore, USA).

Recombinant protein HIV-1 gp120 (Mw \approx 115 kDa), produced in a Baculovirus expression system, and murine anti-gp120 HIV-1 monoclonal antibodies (mAb gp120, Mw \approx 150 kDa), which bind to the V3 loop of HIV-1 gp120, were purchased from Immuno Diagnostics, Inc. (USA). Protein Calibration Standard I was purchased from Bruker Daltonik GmbH (Germany), and trypsin was purchased from Promega (USA).

Anti-gp120 amino-modified biotinylated DNA aptamer (anti-gp120 aptamer, Mw \approx 23 kDa) was provided by Dr S P Radko (the Orekhovich Institute of Biomedical Chemistry of the Russian Academy of Medical Sciences, Moscow, Russia). Anti-gp120 amino-modified biotinylated DNA aptamer

(anti-gp120 aptamer, $M_w \approx 23$ kDa) used in our study was previously selected by Smith et al.²⁹ It was synthesized in house on an automated DNA synthesizer, ASM-800 (Biosset, Novosibirsk, Russia), according to manufacturer instructions, and purified by polyacrylamide gel electrophoresis. Its sequence is shown as follows, with X representing 5-bromo-2'-deoxyuridines (BrdUrds) and Y representing ten nucleotide spacers T: 5'-biotin-GGG AGG ACG ATG CCG AAX GCG CGA GCX XCC GAA AAG GAA AXX ACG CAG ACG ACG AGC GGG A-Y-NH₂-3'. Ten thymine nucleotides were added to facilitate both the aptamer immobilization on the chip surface and its interaction with the target protein.

AFM chip preparation

Amino-functionalization of mica substrate (SPI, Inc., USA), later used as an AFM chip, was carried out by a vapor deposition method using APTES.^{30,31} The APTES layer thus formed had a definite thickness (<0.7 nm).

There were two areas on the surface of an AFM chip: the area with immobilized molecular probes and the control zone without molecular probes. For covalent immobilization of molecular probes, an area of the silanized AFM chip was activated by 0.12 mM DSP solution in 10 mM PBS, pH 7.4, for 10 minutes and rinsed with solution (H₂O:C₂H₅OH=1:1, v/v) for 10 minutes, then dried in a nitrogen flow and immediately used for the immobilization. AFM chips with different molecular probes such as aptamers and antibodies were prepared.

Two microliters of 3 μ M anti-gp120 aptamer solution in 10 mM PBS, pH 7.4, was heated at 95°C for 5 minutes and cooled on ice for 3 minutes. After that, it was deposited onto the activated area of an AFM chip and left for 4 minutes. Then, the AFM chip was washed in ultrapure water for 25 minutes and dried in a nitrogen flow for the AFM visualization and further experiments.

One microliter of 1 μ M gp120 antibody solution in 10 mM PBS, pH 7.4, was deposited onto the activated area of an AFM chip and left for 30 minutes. Then, the AFM chip was washed in ultrapure water for 25 minutes and dried in a nitrogen flow for the AFM visualization and further experiments.

Biospecific fishing of gp120 on the AFM chip

To conduct biospecific fishing of gp120, the AFM chip with covalently immobilized antibodies or aptamers against gp120 was incubated in 1 mL of gp120 solution in 10 mM PBS in a shaker (850 ppm, Thermomixer comfort, Eppendorf) for 30 minutes at 25°C, washed with water three times for

30 minutes at 37°C, and dried in a nitrogen flow. Gp120 solutions 0.8×10^{-9} M and 0.8×10^{-11} M were used in the fishing experiments with aptamer as a molecular probe, and gp120 concentration in analyte solution was 1.0×10^{-8} M in the fishing experiments with antibody as a molecular probe.

The activated area of the AFM chip with immobilized molecular probes and the nonactivated control area without molecular probes were both visualized after biospecific fishing by AFM. Each experiment was repeated not less than three times.

AFM measurements in a tapping mode

AFM measurements were carried out in a tapping mode on the Agilent 5500 AFM (USA) and NTEGRA Prima AFM (NT-MDT, Russia) in air using standard probes PPP-NCH (Nanosensors, Switzerland) with the force constant about 42 Nm⁻¹ and the radius of curvature 10 nm. Scan rate was 1 Hz. At least ten frames of $1 \div 25 \mu\text{m}^2$ were obtained in each experiment.

Gp120 functionalized tip for AFM measurements in a PicoTREC mode

DNP-S10 cantilevers (the force constant was 0.32–0.58 Nm⁻¹, and the radius of curvature was 10–20 nm, Bruker) were used in PicoTREC experiments, and their tips were functionalized with gp120 in several steps. The cantilever was first treated in an ozonator for 60 minutes. After that, it was silanized and activated by DSP the same way as the AFM chip. For the gp120 immobilization, the activated tip was incubated in 10^{-10} M gp120 solution for 10 minutes at room temperature. After being rinsed with PBS for 20 minutes, a functionalized cantilever was placed in an AFM holder in a liquid cell to conduct AFM measurements in PicoTREC mode.

AFM measurements in a PicoTREC mode

TREC was also carried out using Agilent 5500 AFM (USA) in a PicoTREC mode that allows detection and mapping of molecular binding events while simultaneously generating topographic images.³² PicoTREC mode combines “topography” imaging of the surface and “recognition” imaging of the same part of the surface. Therefore, there will be a correlation between objects on the surface and events on the recognition image, which reflects their force interaction with a tip.

In our case, gp120 protein was attached to the AFM tip, and anti-gp120 aptamers were immobilized on the AFM chip. Then, aptamer/protein interaction was registered in a PicoTREC mode, and a molecular binding map was obtained. When AFM tip-tethered protein interacts with an aptamer

immobilized on the surface, there is a transient reduction in the oscillation amplitude of the tip. The imaging servo restores the signal amplitude, but with the peak signal shifted downward, and this peak shift provides the recognition signal for a specific aptamer/protein recognition event.^{32,33} So a molecular binding map is a “map” of the change in a peak signal where binding events appear as black spots.

To conduct AFM measurements in a PicoTREC mode, an AFM chip with immobilized anti-gp120 aptamers was placed into a liquid cell of a microscope. AFM imaging was carried out by gp120 functionalized cantilever in a tapping mode with set-point amplitude $A \sim 5\text{--}8 \text{ nm} \sim 95\%\text{--}97\% A_0$. Scan rate was 1 Hz. In this experiment, at least five frames were obtained, whose sizes were $9 \mu\text{m}^2$. Each experiment was repeated not less than three times.

AFM measurements: control experiments

Control experiments were carried out by AFM imaging of the control area of the AFM chip in a tapping mode after immobilization of molecular probes and biospecific fishing of protein from solution. The size of the nonspecific objects on the AFM chip was $<0.7 \text{ nm}$ in these control experiments.

Analysis of AFM images

The heights of aptamers, antibodies, proteins, and their complexes on the AFM images were calculated in automatic mode using AFM-dtpr software (<http://ibmcsoft.ru>, IBMC RAMS, Russia).

As was previously shown,^{34–37} a standard AFM probe allows object height to be obtained with 0.1 nm resolution. In this case, the density of object distribution with height $\rho(h)$ was calculated as:

$$\rho(h) = \frac{N_h}{N} \times 100\% \quad (1)$$

where N_h is a number of visualized objects with height h , while N is the total number of visualized objects. This experimental distribution (1) was approximated by Gaussian function:

$$\rho(h) = \sum \rho_i(h) = \sum_i \frac{Ae^{-4 \ln(2)(h-h_{\max})^2/W^2}}{W \sqrt{\pi/4 \ln(2)}} \quad (2)$$

where A , h_{\max} , WA , h_{\max} , and W are approximation parameters; h_{\max} is a maximum height; W is a value of full width at half maximum; and a number of terms i was determined based on χ^2 criterion.^{36,37}

Image contrast of fished protein against the background of immobilized aptamers on the AFM image ($IC_{\text{protein/apt}}$) as well as image contrast of fished protein against the background of immobilized antibodies on the AFM image ($IC_{\text{protein/ab}}$) were estimated as:

$$IC_{\text{protein/apt}} = \frac{h_{\text{protein/apt}} - h_{\text{apt}}}{h_{\text{apt}}} \quad (3)$$

$$IC_{\text{protein/ab}} = \frac{h_{\text{protein/ab}} - h_{\text{ab}}}{h_{\text{ab}}} \quad (4)$$

where $h_{\text{protein/apt}}$ and $h_{\text{protein/ab}}$ are the height maximums of aptamer/protein and antibody/protein complexes on the AFM chips, respectively; h_{apt} and h_{ab} are the height maximums of aptamers and antibodies before protein fishing, respectively. Height maximums were obtained from Equation 2.

MS analysis of proteins on the AFM chip surface

Proteolysis on the AFM chip surface

Trypsinolysis of biospecifically fished proteins was done directly on the AFM chip according to the standard procedure at 42°C and at $\sim 100\%$ relative humidity.³⁰ Incubating solution for trypsinolysis contained 100 mM bicarbonate buffer (pH 7.4), 10% of acetonitrile, 1% of glycerol, and porcine trypsin (Promega Trypsin Gold, USA) in the ratio of 1:50 to target protein. After trypsinolysis, the tryptic mixture with peptide fragments was applied to the mass analyzer to carry out a protein identification.

Matrix-assisted laser desorption-ionization time-of-flight mass spectrometry (MALDI-TOF-MS) analysis

Protein identification was performed on a TOF-MS Autoflex III MALDI-TOF/TOF (Bruker, Germany) equipped with a nitrogen laser ($\lambda=337 \text{ nm}$). The MS calibration was performed with a peptide calibration standard for positive ions in a reflector mode (the reflector voltage was 5 kV), the range of detectable masses was 800–3,000 m/z, and the pulse delay time was 200 ns. The peptide calibration standard included the following peptides: bradykinin (monoisotopic ion mass was 757.3992 Da), angiotensin II (1,046.5420 Da), angiotensin I (1,296.6853 Da), peptide P (1,347.7361 Da), bombesin (1,619.8230 Da), renin (1,758.9326 Da), adrenocorticotrophic hormone (ACTH) fragment 1–17 (2,093.0868 Da), ACTH fragment 18–39 (2,465.1990 Da), and somatostatin (3,147.4714 Da). The peaks of matrix (HCCA in 50% acetonitrile and 0.7% TFA) and trypsin autolysis were

ignored in the spectral analysis. The mass spectrum was obtained in an automatic mode with the ion accumulation from 10,000 shots. To obtain the mass spectra of samples, the tryptic mixture was mixed in a ratio from 1:1,000 to 1:10,000 with an excess of matrix, and then this mixture was applied to MTP AnchorChip 384 target.

Mass spectra were analyzed with FlexAnalysis software 2.0 (Bruker, Germany). Protein identification was performed with Mascot software 2.2.04 (<http://www.matrixscience.com>) using the National Center for Biotechnology Information data library of protein sequences. The following search parameters were chosen: one missing hydrolysis site, monoisotopic mass determination accuracy was <100 ppm, and the oxidized methionine was mentioned as possible modification.

Results

AFM imaging of anti-gp120 aptamer in a tapping mode

Preparation of the AFM chip with the covalently immobilized aptamers against gp120 was described in the “Materials and methods” section.

Figure 1A represents an AFM image of anti-gp120 aptamers covalently immobilized on the AFM chip. This image was obtained by nonmodified cantilever in a standard tapping mode in air (see “Materials and methods”).

AFM imaging showed that there were objects with height ~1 nm on the chip surface, which can be identified as aptamers, because there were no such objects in the control area of the AFM chip (Figure 1B). The respective

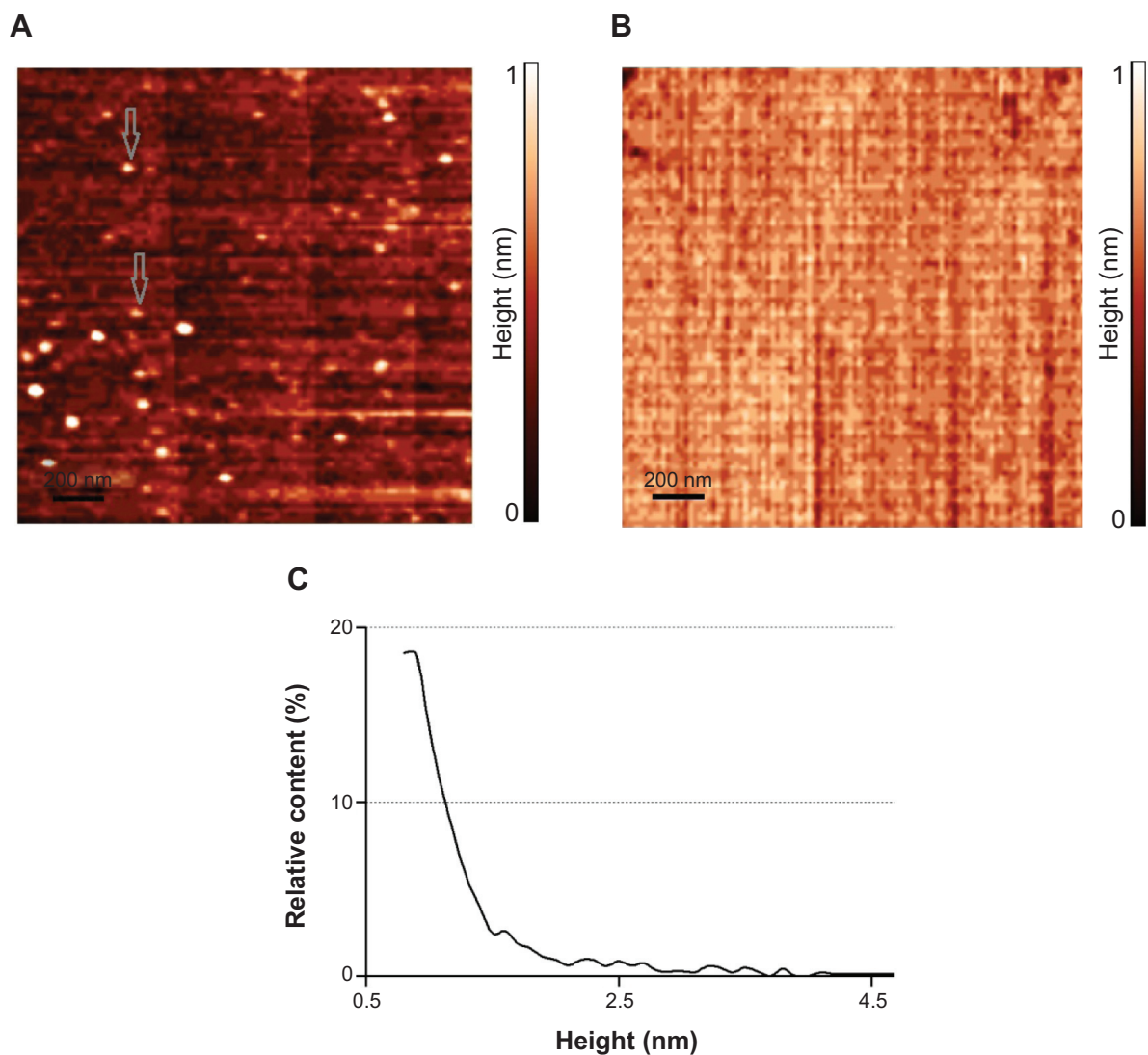


Figure 1 Atomic force microscopy (AFM) images of aptamer chip surface with immobilized aptamers (A) and image of the control area without aptamers before biospecific fishing of gp120. (B) Density of visualized object distribution with heights $\rho(h)$ over the area with immobilized anti-gp120 aptamers. (C) Density of visualized object distribution.

Notes: Experimental conditions were standard cantilever, tapping mode in air, relative humidity 60%, temperature of 22°C, scan size 2.0×2.0 μm^2 ; NTEGRA Prima AFM. Arrows point to several objects with height ~1 nm.

density of anti-gp120 aptamer distribution with heights $\rho(h)$ was obtained from AFM data processing (Figure 1C). Approximation of experimental density distribution of AFM visualized aptamers with heights $\rho(h)$ (1) was carried out using function (2). It was obtained from this approximation that visualized objects form a group of objects with the maximum height $h_{\max}(apt)=(0.9\pm 0.1)$ nm, and a full width at half maximum was $W=(0.5\pm 0.1)$ nm.

AFM imaging of anti-gp120 aptamer in a PicoTREC mode

In order to prove that visualized objects, which were described in the previous section, are anti-gp120 aptamers, AFM imaging of these objects was conducted in a PicoTREC mode. In this mode, a surface topography and a molecular binding map are obtained simultaneously. The principle of the TREC method is summarized in the literature³⁷ and briefly described in the “Materials and methods” section.

Figure 2 represents AFM images of the surface topography and molecular binding map, which were obtained by gp120 functionalized cantilever in a PicoTREC mode in buffer. Objects with heights up to 10 nm were visualized on the surface topography image (Figure 2A). These objects are higher than ones on the topography image obtained by standard cantilever in a tapping mode in air (see the previous section), because AFM visualization in a PicoTREC mode was conducted by a modified cantilever.

First, interaction of a tip-tethered protein with the surface and immobilized objects leads to distortion of the heights of visualized objects. Secondly, tip functionalization leads to significant enlargement of its radius of curvature, and visualized objects have distorted lateral dimensions as a result. Therefore, information obtained from AFM measurements of topography in a PicoTREC mode can be only qualitative, and density of objects distribution with heights will also be inaccurate.

Recognition events were visualized on the molecular binding map or recognition image (Figure 2B) as dark spots, due to reduction of the oscillation amplitude on binding anti-gp120 aptamer on the surface and tip-tethered gp120. Dark spots on the recognition image generally coincide with objects on the topography image (Figure 2A and B examples are indicated by circles).

Biospecific fishing of gp120 on the AFM chip with immobilized aptamers

Figure 3A and B represents AFM images of the AFM chip surface with immobilized anti-gp120 aptamers after incubation in 0.8×10^{-9} M and 0.8×10^{-11} M gp120 solution in 10 mM PBS, respectively. As is seen from the figures, the objects with heights from 1 nm to 5 nm were visualized on the surface after incubation. Since there were no such objects with height $h>1$ nm in the control area of the AFM chip without immobilized molecular probes (Figures 3C), then visualized

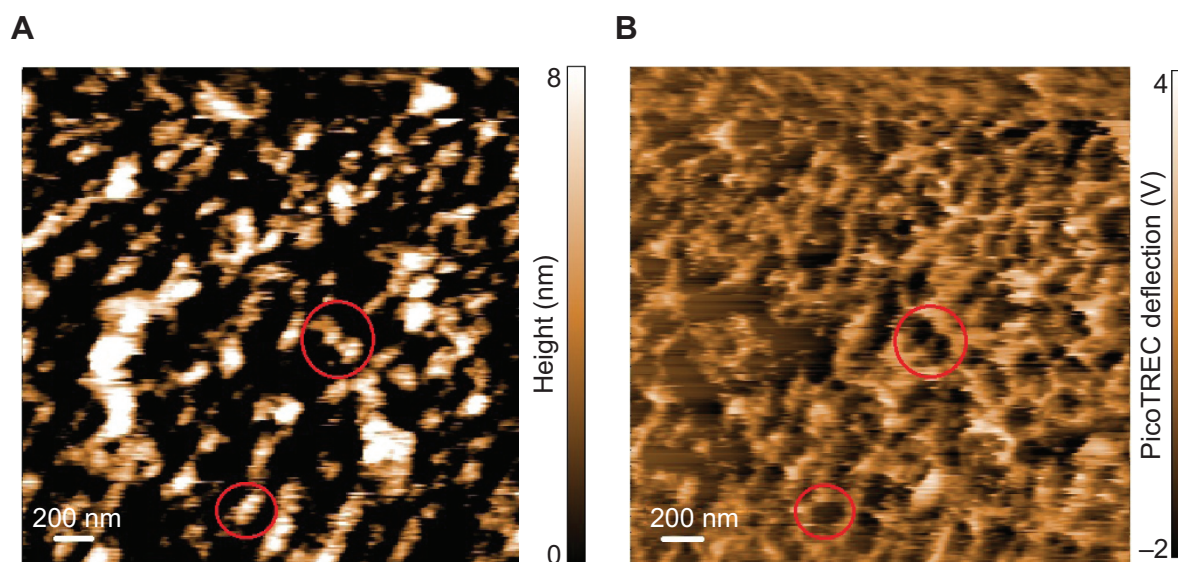


Figure 2 Atomic force microscopy (AFM) topography image (A) and recognition image (B) of the chip surface with immobilized anti-gp120 aptamers before biospecific fishing of gp120.

Notes: Experimental conditions were gp120-functionalized cantilever, PicoTREC mode in buffer, 10 mM Modified Dulbecco's phosphate buffer, pH 7.4, temperature of 22°C; scan size 3.0×3.0 μm^2 , Agilent 5500 AFM. Dark spots on the recognition image are recognition events on binding of aptamer on the surface and tip-tethered gp120. Some coincidences of objects and recognition events are indicated by circles as an example.

objects can be identified as the gp120/aptamer complexes that were formed during the fishing of gp120 on the AFM chip surface.

After AFM data processing, the respective densities of object distribution with heights were obtained (Figure 3D). Approximation of experimental density distribution of complexes with heights $\rho(h)$ (1) was carried out using function (2). As a result, maximum heights of the visualized complexes were 1) $h_{\max}(protein/apt)=(1.6\pm 0.1)$ nm after incubation in 0.8×10^{-9} M gp120 solution and 2) $h_{\max}(protein/apt)=(1.4\pm 0.1)$ nm after incubation in 0.8×10^{-11} M gp120 solution.

Using Equation 3, an image contrast of fished protein against the background of immobilized aptamers on the AFM image was estimated to be 0.8, where height of the immobilized aptamers was $h_{\text{apt}}=h_{\max}(apt)$ and height of the gp120/aptamer complexes was $h_{\text{gp120/apt}}=h_{\max}(protein/apt)$.

Biospecific fishing of gp120 on the AFM chip with immobilized antibodies

Figure 4A represents an AFM image of the AFM chip surface with immobilized gp120 antibodies before incubation in gp120 solution. Antibodies were visualized as the objects with heights from 1.2 nm to 2.5 nm. Maximum height from

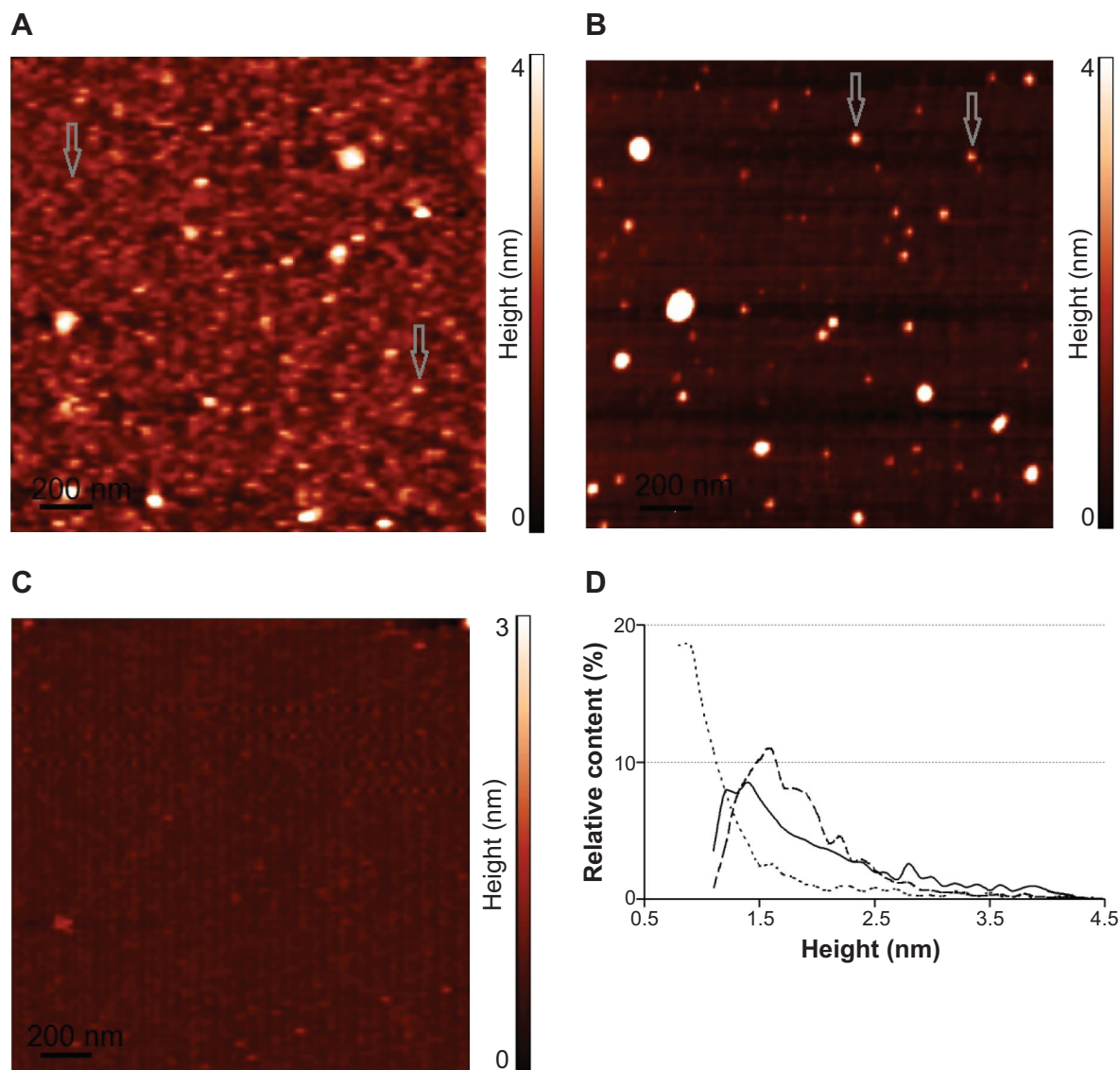


Figure 3 Atomic force microscopy (AFM) images of aptamer chip surface after biospecific fishing of gp120.

Notes: (A, B) AFM images of the area with immobilized aptamers, (C) AFM image of the control area without aptamers, and (D) density of visualized object distribution with heights $\rho(h)$ obtained over the area with immobilized aptamers after fishing of gp120 at different concentrations. Experimental conditions were concentrations of the analyte solutions (A, C) $C_{\text{gp120}}=0.8\times 10^{-9}$ M and (B) $C_{\text{gp120}}=0.8\times 10^{-11}$ M; standard cantilever, tapping mode in air, relative humidity 60%, temperature of 22°C, scan size 2.0×2.0 μm^2 ; NTEGRA Prima AFM. Arrows point to gp120/aptamer complexes. (D) $\rho(h)$ for $C_{\text{gp120}}=0.8\times 10^{-11}$ M (solid line), for $C_{\text{gp120}}=0.8\times 10^{-9}$ M (dashed line) and for $C_{\text{gp120}}=0$ (dotted line).

the density of distribution of antibodies with heights $\rho(h)$ (Figure 4C) was $h_{\max}(ab)=(1.8\pm 0.1)$ nm, which corresponds to the height of the immobilized antibodies of immunoglobulin G class.^{8,9,39,40}

Images of the chip surface with immobilized antibodies and without antibodies after incubation in 10^{-8} M gp120 solution are presented in Figure 4B and C. The objects with heights from 1.2 nm to 4 nm were visualized on the AFM chip surface with immobilized antibodies after incubation (Figure 4B). The respective densities of object distribution with heights $\rho(h)$ are on the Figure 4C. Approximation of experimental density distribution with heights $\rho(h)$ (1) was carried out using function (2) and lets visualized objects be divided into two groups with the following maximum heights: $h_{\max 1}=(1.8\pm 0.1)$ nm ($W_1=(0.8\pm 0.1)$ nm, share of

objects was 47%) and $h_{\max 2}=(2.5\pm 0.2)$ nm ($W_2=(1.3\pm 0.3)$ nm, share of objects was 53%).

Maximum height from the first group corresponds to the maximum height of the immobilized antibodies $h_{\max}(ab)$. Visualized objects from the second group are higher than immobilized antibodies, and also there were no similar objects in the control area of the AFM chip without immobilized molecular probes (Figure 4C). Therefore, the objects from the second group can be identified as the gp120/antibody complexes that were formed during the fishing of protein on the AFM chip surface.

To estimate the image contrast of fished protein against the background of immobilized antibodies on the AFM image, the following parameters were used: height of the immobilized antibodies $h_{ab}=h_{\max 1}$ and height of the gp120/antibody

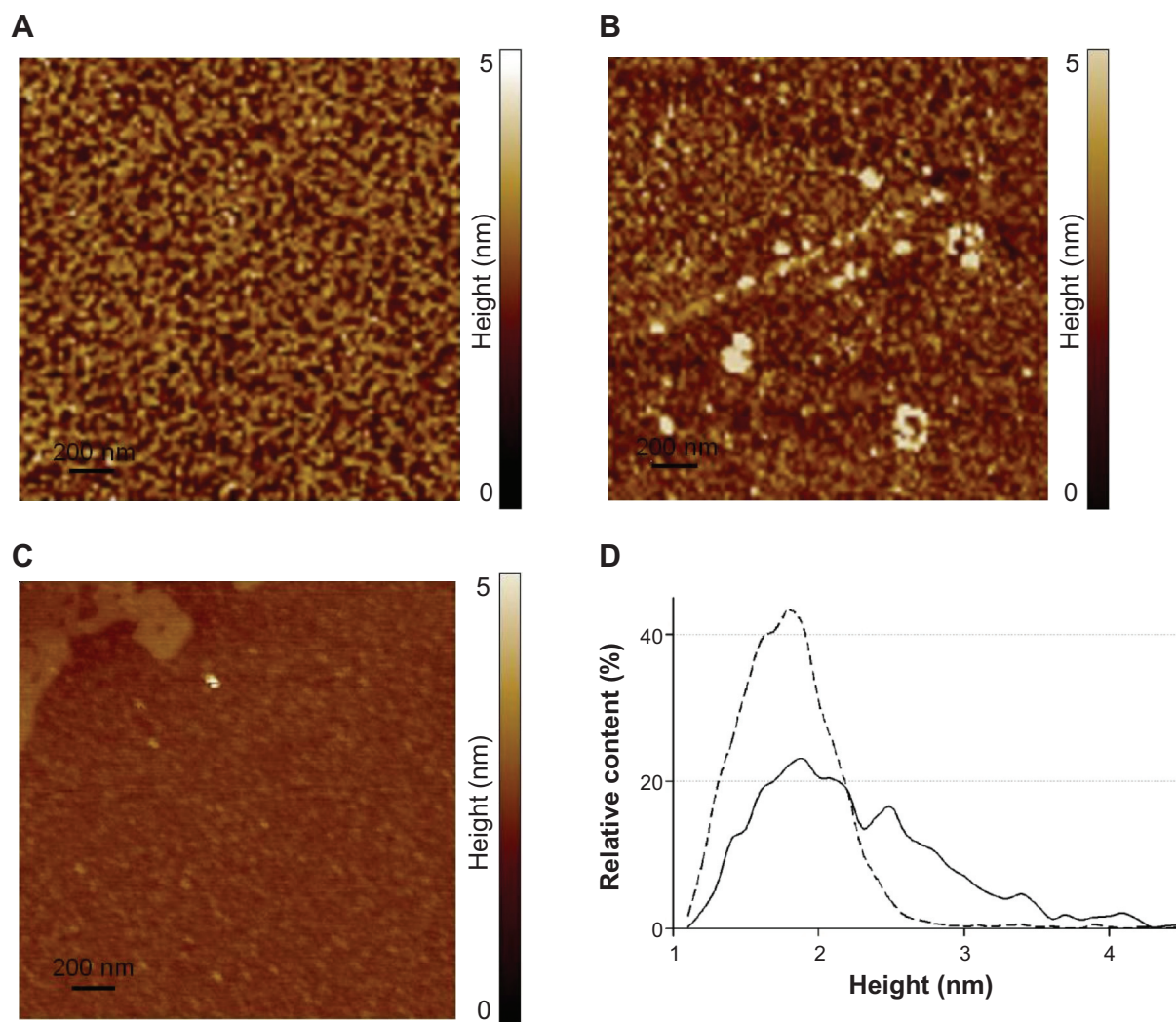


Figure 4 Atomic force microscopy (AFM) images of antibody chip surface after biospecific fishing of gp120.

Notes: (A) AFM image of the area with immobilized antibodies before biospecific fishing of gp120, (B) AFM image of the area with immobilized antibodies after biospecific fishing of gp120, (C) AFM image of the control area without antibodies, and (D) density of visualized objects distribution with heights $\rho(h)$ obtained over the area with immobilized antibodies. Experimental conditions were concentration of the analyte solution $C_{gp120}=10^{-8}$ M; standard cantilever, tapping mode in air, relative humidity 60%, temperature of 22°C, scan size 2.0×2.0 μm^2 ; NTEGRA Prima AFM. (D) $\rho(h)$ after fishing of gp120 (solid line) and before fishing of gp120 (dashed line).

complexes $h_{gp120/ab} = h_{max2}$. Using Equation 3, image contrast $IC_{gp120/ab}$ was calculated to be 0.4.

MS identification of gp120 after biospecific fishing on the AFM chip

Figure 5A and B illustrates the typical MALDI-TOF-MS control spectra of the samples obtained from AFM chips' surface before their incubation in a gp120 solution.

The spectrum obtained in the AFM experiments with aptamers as molecular probes (Figure 5A) contains a small amount of peaks in the peptide region, which correspond to autolysis peaks of trypsin with m/z values 842.509, 1,045.569, and 2,211.104. The control spectrum obtained in the AFM experiments with antibodies as molecular probes (Figure 5B) contains the peaks corresponding to anti-gp120 antibodies along with the trypsin autolysis peaks. Peptide

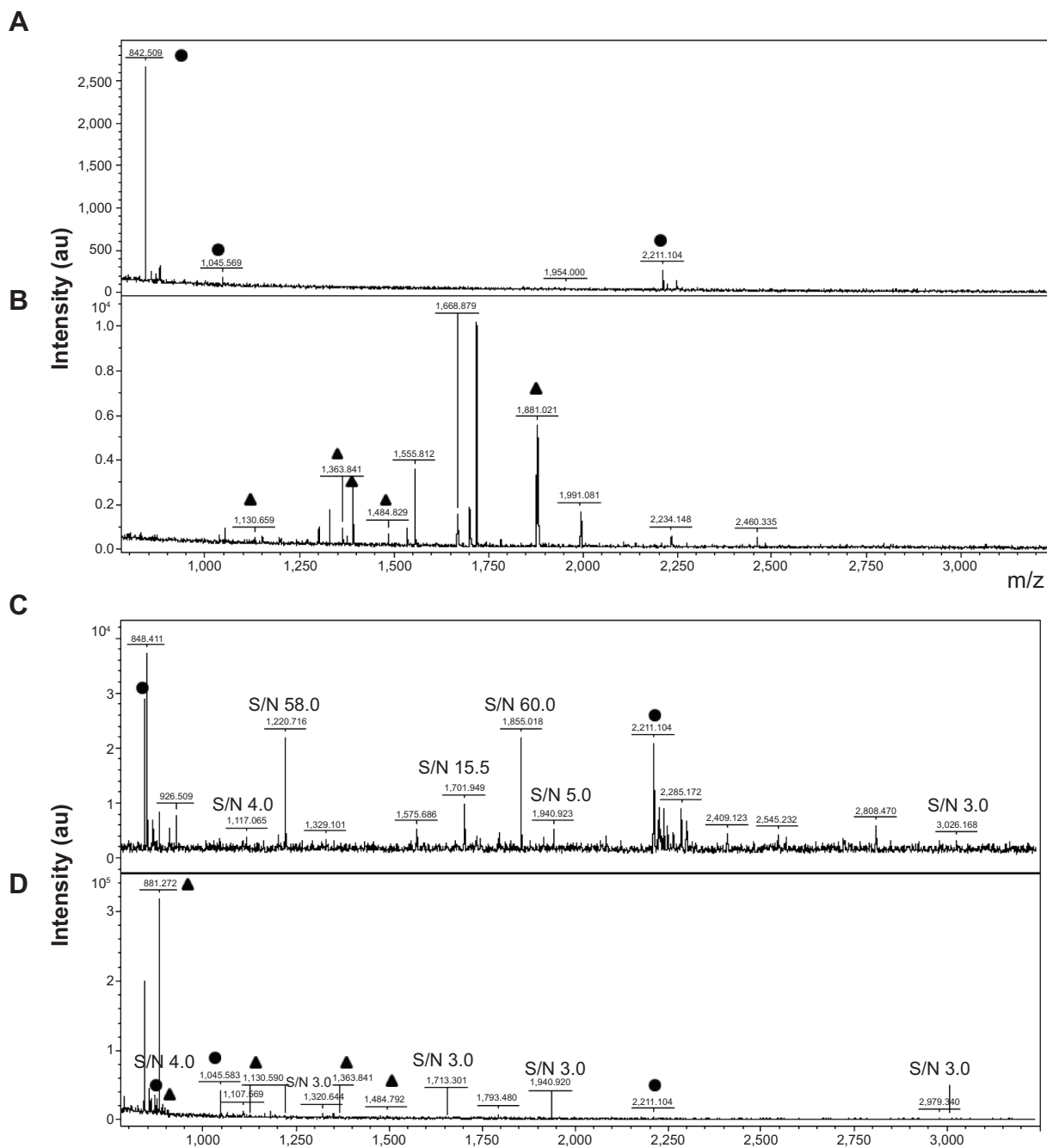


Figure 5 Mass spectra of objects on the atomic force microscopy (AFM) chips with molecular probes before and after biospecific fishing of gp120: before fishing on the AFM chip with immobilized aptamers (A) and antibodies (B); after fishing on the AFM chip with immobilized aptamers (C) and antibodies (D).

Notes: Experimental conditions were concentrations of the analyte solutions (C) $C_{gp120} = 0.8 \times 10^{-11}$ M and (D) $C_{gp120} = 10^{-8}$ M. Trypsin autolysis peaks are pointed by circles (●), peaks of antibodies are pointed by triangles (▲), gp120 peptides are marked as S/N with the corresponding values of the signal/noise ratio.

Abbreviation: au, arbitrary units.

fragments of gp120 were not observed in the control spectra (Figure 5A and B).

Figure 5C and D illustrates the typical MALDI-TOF-MS spectra of the samples obtained from AFM chip surface after biospecific fishing of gp120 on the AFM chips. The spectrum obtained from the AFM chips with immobilized aptamers (Figure 5C) contains two groups of peaks. One of them corresponds to autolysis peaks of trypsin and another one corresponds to the peptide fragments of gp120. The spectrum obtained from the AFM chips with immobilized antibodies (Figure 5D) contains the third group of the peaks: trypsin, gp120, and anti-gp120 antibodies.

Thus, an MS analysis provided an identification of gp120 as a target protein that was fished out on the AFM chip with immobilized molecular probes.

Discussion

In this study, AFM was used as a molecular detector to visualize and count gp120 protein that was fished out from the solution by the AFM chip with immobilized anti-gp120 aptamers. Aptamers immobilized on the AFM chip were visualized by AFM in a PicoTREC mode. As a result of TREC experiments, it was shown that immobilized aptamers retain their affinity and demonstrate their biospecific interaction with tip-tethered gp120.

It was shown that it is possible to use aptamers as immobilized molecular probes. Thus, gp120/aptamer complexes were formed on the AFM chip surface as a result of a biospecific fishing of gp120 from solution (gp120 concentrations were 0.8×10^{-9} M and 0.8×10^{-11} M) and were visualized by AFM (Figure 3A and B). Protein that was biospecifically fished out on this AFM chip was identified by MS analysis.

AFM measurements also showed that using aptamers as molecular probes allows obtaining a good image contrast of fished protein against the background of immobilized aptamers on the AFM image. This value was estimated from the experimental data to be $IC_{gp120/apt} = 0.8$, which is two-fold higher than the same value against the background of immobilized antibodies ($IC_{gp120/ab} \sim 0.4$).

Such an increase in the image contrast is expected and results from the fact that the molecular weight ratio of gp120 to aptamer is larger than molecular weight ratio of gp120 to antibody and image heights as a consequence. The value of AFM image contrast is affected by the height of immobilized probe molecules. If aptamers are used, the probe height is much smaller than in the case of antibodies. Thus, the height of an AFM image of an aptamer (~ 1 nm) is comparable with noise level, which is determined by silanized mica surface roughness. Therefore, the contrast

of an AFM image of a protein against a background of an aptamer is better.

Let us estimate the theoretically expected image contrast of fished protein against the background of immobilized aptamers and antibodies on AFM images. According to common knowledge, the height of the globular protein varies directly as $\sqrt[3]{M}$, where M is a molecular weight of globular protein in kDa.⁴¹ In the context of this assumption, Equations 3 and 4 simplify to:

$$IC_{\text{protein/apt}} = \frac{\sqrt[3]{M_{\text{protein/apt}}} - \sqrt[3]{M_{\text{apt}}}}{\sqrt[3]{M_{\text{apt}}}} \quad (5)$$

$$IC_{\text{protein/ab}} = \frac{\sqrt[3]{M_{\text{protein/ab}}} - \sqrt[3]{M_{\text{ab}}}}{\sqrt[3]{M_{\text{ab}}}} \quad (6)$$

where $M_{\text{protein/apt}}$ and $M_{\text{protein/ab}}$ are the weights of protein/ aptamer and protein/antibody complexes, respectively, and M_{apt} and M_{ab} are the weights of aptamer and antibody, respectively.

Since $M_{\text{apt}} = 23$ kDa, $M_{\text{ab}} \sim 150$ kDa, and $M_{\text{gp120}} = 115$ kDa, then the $IC_{gp120/apt}/IC_{gp120/ab}$ ratio will be equal to 4. Theoretically expected image contrast of fished protein against the background of immobilized aptamers has to be four-fold higher than the contrast against the background of immobilized antibodies on the AFM images.

One can see that the theoretical image contrast for protein/ aptamer complexes is several-fold higher than the contrast for protein/antibody complexes. This estimate corresponds with the experimental results.

Conclusion

Biospecific AFM fishing allows direct, label-free detection and counting of target proteins, and MS analysis provides an additional proof of the target protein presence to avoid any artifacts. It was shown that aptamers can be used as molecular probes on AFM chips for biospecific fishing of the proteins from analyte solution. In this case, the image contrast of fished protein against the background of immobilized aptamers is higher than against the background of immobilized antibodies on the AFM images. Another advantage of using aptamers on the AFM chip is an absence of contribution of the immobilized aptamers to the mass spectrum of protein peptide fragments (including gp120) in contrast to the possible contribution of antibody peptide fragments. In the case of gp120, it was shown that AFM in combination with an aptamer-based approach can be a follow-on technology for development of lab-on-a-chip diagnostics. Furthermore,

using a high-speed AFM with a scan rate more than ten-fold higher than conventional AFM could provide the background for future applications of point-of-care diagnostics.

Author contributions

The authors contributed equally to this paper.

Disclosure

The authors report no conflicts of interest in this work.

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