### **RESEARCH PAPER**



## Drug-induced shortening of the electromechanical window is an effective biomarker for in silico prediction of clinical risk of arrhythmias

Elisa Passini<sup>1</sup> | Cristian Trovato<sup>1</sup> | Pierre Morissette<sup>2</sup> | Frederick Sannajust<sup>2</sup> | Alfonso Bueno-Orovio<sup>1</sup> | Blanca Rodriguez<sup>1</sup>

<sup>1</sup>Department of Computer Science, University of Oxford, Oxford, UK

<sup>2</sup> SALAR, Safety and Exploratory Pharmacology Department, Merck Research Laboratories, Merck & Co., Inc., West Point, PA, USA

#### Correspondence

Elisa Passini, Department of Computer Science, University of Oxford, Wolfson Building, Parks Road, OX1 3QD Oxford, UK. Email: elisa.passini@cs.ox.ac.uk

#### Funding information

Oxford British Heart Foundation Centre ofResearch Excellencee, Grant/Award Numbers: RE/08/004/23915 and RE/13/1/30181; British Heart Foundation Intermediate Basic ScienceResearch, Grant/Award Number: FS/ 17/22/32644: DPhil Scolarship/html: EPSRC Impact Acceleration Awards, Grant/Award Number: EP/K503769/1; TransQST project, Grant/Award Number: 116030; CompBioMed project, Grant/Award Number: 675451; NC3Rs Infrastructure for Impact Award, Grant/Award Number: NC/P001076/1; Wellcome Trust Senior Research Fellowship in Basic Biomedical Sciences, Grant/Award Numbers: 214290/Z/18/Z and 100246/Z/12/Z

**Background and Purpose:** Early identification of drug-induced cardiac adverse events is key in drug development. Human-based computer models are emerging as an effective approach, complementary to in vitro and animal models. Drug-induced shortening of the electromechanical window has been associated with increased risk of arrhythmias. This study investigates the potential of a cellular surrogate for the electromechanical window (EMw) for prediction of pro-arrhythmic cardiotoxicity, and its underlying ionic mechanisms, using human-based computer models.

**Experimental Approach:** In silico drug trials for 40 reference compounds were performed, testing up to 100-fold the therapeutic concentrations (EFTPC<sub>max</sub>) and using a control population of human ventricular action potential (AP) models, optimised to capture pro-arrhythmic ionic profiles. EMw was calculated for each model in the population as the difference between AP and Ca<sup>2+</sup> transient durations at 90%. Drug-induced changes in the EMw and occurrence of repolarisation abnormalities (RA) were quantified.

**Key Results:** Drugs with clinical risk of Torsade de Pointes arrhythmias induced a concentration-dependent EMw shortening, while safe drugs lead to increase or small change in EMw. Risk predictions based on EMw shortening achieved 90% accuracy at  $10 \times \text{EFTPC}_{max}$ , whereas RA-based predictions required  $100 \times \text{EFTPC}_{max}$  to reach the same accuracy. As it is dependent on Ca<sup>2+</sup> transient, the EMw was also more sensitive than AP prolongation in distinguishing between pure hERG blockers and multichannel compounds also blocking the calcium current.

Abbreviations: EMw, electromechanical window change by drug action; AP, action potential; APD<sub>XX</sub>, action potential duration at XX% of repolarisation;  $CTD_{XX}$ ,  $Ca^{2+}$  transient duration at XX% of the initial base value; DA, depolarisation abnormalities;  $dV/dt_{MAX}$ , maximum upstroke velocity;  $EFTPC_{max}$ , maximal effective therapeutic free concentration; EMw, electromechanical window; FN, false negative(s); FP, false positive(s); G<sub>X</sub>, I<sub>X</sub> conductance; h, Hill coefficient; I<sub>CaL</sub>, L-type  $Ca^{2+}$  current; I<sub>K1</sub>, inward rectifier K<sup>+</sup> current; I<sub>Kn</sub>, rapid delayed rectifier K<sup>+</sup> current; I<sub>Ks</sub>, slow delayed rectifier K<sup>+</sup> current; I<sub>Nak</sub>, tast Na<sup>+</sup> current; I<sub>Nak</sub>, Na<sup>+</sup>-K<sup>+</sup> pump current; I<sub>NaL</sub>, late Na<sup>+</sup> current; I<sub>NCX</sub>, Na<sup>+</sup>-Ca<sup>2+</sup> exchanger current; I<sub>to</sub>, transient outward K<sup>+</sup> current; ORd, O'Hara-Rudy dynamic human ventricular model; RA, repolarisation abnormalities; RMP, resting membrane potential; TdP, Torsade de Pointes; TN, true negative(s); TP, true positive(s); Tri<sub>90-40</sub>, AP triangulation; V<sub>peak</sub>, peak voltage

This is an open access article under the terms of the Creative Commons Attribution License, which permits use, distribution and reproduction in any medium, provided the original work is properly cited.

© 2019 The Authors. British Journal of Pharmacology published by John Wiley & Sons Ltd on behalf of British Pharmacological Society.



**Conclusion and Implications:** The EMw is an effective biomarker for in silico predictions of drug-induced clinical pro-arrhythmic risk, particularly for compounds with multichannel blocking action.

## 1 | INTRODUCTION

Early prediction of drug-induced cardiotoxicity is key during drug development and still remains a major challenge (Laverty et al., 2011: Stevens & Baker, 2009). Animal models are widely used for preclinical in vitro, ex vivo, and in vivo studies, but safety findings do not always translate to humans (Berridge et al., 2013), and predictions of clinical risk of arrhythmias for large sets of compounds still show limited accuracy (Lawrence, Bridgland-Taylor, Pollard, Hammond, & Valentin, 2006; Valentin et al., 2009). The current ICH S7B/E14 guidelines (2005b, 2005a) focus on hERG channel block and QTc prolongation, as surrogate markers of pro-arrhythmia. Although this paradigm has been effective in preventing new pro-arrhythmic drugs from entering the market, it has important limitations and may have led to stopping the development of potentially valuable therapeutics (Sager, Gintant, Turner, Pettit, & Stockbridge, 2014). This suggests that new effective strategies and biomarkers, for a more comprehensive prediction of drug-induced cardiotoxicity in patients, are needed in the preclinical stages of drug development. In silico human-based methodologies are becoming increasingly established in pharmacology as a potential alternative to animal experiments in the early phases of drug development, using a variety of approaches (Abbasi, Small, Patel, Jamei, & Polak, 2017; Britton, Abi-Gerges, et al., 2017; Chang et al., 2017; Dutta et al., 2017; Krogh-Madsen, Jacobson, Ortega, & Christini, 2017; Lancaster & Sobie, 2016; Li et al., 2017, 2019; Paci, Passini, Severi, Hyttinen, & Rodriguez, 2017; Passini et al., 2017; Rodriguez et al., 2016). We recently demonstrated that human in silico drug trials can achieve high accuracy (close to 90%) in pro-arrhythmic cardiotoxicity prediction for more than 60 reference compounds (Passini et al., 2017). The occurrence of repolarisation abnormalities (RA), which are mechanistically linked with arrhythmias, was shown to be a sensitive biomarker to predict clinical drug-induced arrhythmic risk using populations of human ventricular in silico action potential (AP) models. However, the best prediction accuracy was achieved for drug concentrations up to 100-fold the maximal effective free therapeutic concentration (EFTPC<sub>max</sub>). While investigating the effect of potential overdoses is important in drug safety assessment, testing drug concentrations much larger than the EFTPC<sub>max</sub> might lead to false positives (Krogh-Madsen et al., 2017).

The electromechanical window (EMw), defined as the difference between the duration of electrical and mechanical systole, has been suggested as a promising biomarker to predict clinical risk of Torsade de Pointes (TdP) arrhythmia in several preclinical animal models (Guns, Johnson, Van Op den Bosch, Weltens, & Lissens, 2012; Guns, Johnson, Weltens, & Lissens, 2012; Morissette et al., 2016; van der Linde et al., 2010). However, for **dofetilide**, Stams et al. (2014) showed that, in the in vivo atrioventricular block canine model, the EMw solely

### What is already known

- Human in silico drug trials can predict clinical risk of druginduced arrhythmia with high accuracy
- Shortening of the electro-mechanical window in vivo is associated with pro-arrhythmia, but controversy exists

### What this study adds

- In silico, the electro-mechanical window increases predictive accuracy of drug-induced arrhythmias at clinically relevant doses
- The electro-mechanical window is more effective than alternative biomarkers as it reflects intracellular calcium changes.

### What is the clinical significance

- In silico drug trials can contribute to the development of safer and more efficient medicines
- Human-based computer models can identify subpopulations of patients vulnerable to drug-induced cardiac arrhythmias

reflects changes in QT prolongation and therefore lacks specificity for prediction of drug-induced TdP.

The aim of this study was to investigate the potential of a cellular surrogate for the EMw as a biomarker for predictions of clinical druginduced arrhythmic risk using human in silico trials for 40 reference compounds. We hypothesised that the EMw was a more sensitive biomarker of arrhythmic risk than AP prolongation and RA, particularly for multichannel block involving both potassium and calcium currents, given its dependency with calcium transient duration.

### 2 | METHODS

### 2.1 | Design of the control population of models

A control population of human ventricular AP models was constructed and optimised, blindly to the drug trials results. The population was constructed using the O'Hara-Rudy dynamic (ORd) model (O'Hara, Virág, Varró, & Rudy, 2011) as baseline and the experimentally calibrated population of models methodology (Britton et al., 2013; Muszkiewicz et al., 2016; Passini et al., 2017). The nine main ionic conductances were randomly varied: fast and late Na<sup>+</sup> (G<sub>Na</sub> and G<sub>NaL</sub> respectively), transient outward K<sup>+</sup> (G<sub>to</sub>), rapid and slow delayed rectifier K<sup>+</sup> (G<sub>Kr</sub> and G<sub>Ks</sub>), inward rectifier K<sup>+</sup> (G<sub>K1</sub>), Na<sup>+</sup>-Ca<sup>2+</sup> exchanger (G<sub>NCX</sub>), Na<sup>+</sup>-K<sup>+</sup> pump (G<sub>Nak</sub>), and the L-type Ca<sup>2+</sup> (G<sub>CaL</sub>). The ranges of variation of each conductance are shown in Table 1, and they were optimised based on results in Passini et al. (2017), to maximise the number of models accepted in the population while at the same time minimising the population size. In brief, models with severe G<sub>Na</sub>, G<sub>Kr</sub>, G<sub>Nak</sub>, or G<sub>K1</sub> down-expression often fail to produce physiological APs, while models with low repolarisation reserve (increased G<sub>CaL</sub>, G<sub>NaL</sub>, and G<sub>NCX</sub>, reduced G<sub>NaK</sub>, G<sub>Kr</sub>, and G<sub>Ks</sub>) are more prone to develop drug-induced RA. Using this process, an initial population of 150 models was produced.

This initial population was paced at 1 Hz for 500 beats (to allow the models to reach steady state), and the last AP trace for each model was used to compute a set of seven AP and two Ca<sup>2+</sup> transient biomarkers: AP duration at 40%, 50%, and 90% of repolarisation (APD\_{40,} APD\_{50}, and APD<sub>90</sub>); AP triangulation, defined as the difference between APD<sub>90</sub> and APD<sub>40</sub> (Tri<sub>90-40</sub>); maximum upstroke velocity (dV/dt<sub>MAX</sub>); peak voltage  $(V_{peak})$ ; resting membrane potential (RMP); and Ca<sup>2+</sup> transient duration at 50% and 90% of repolarisation (CTD<sub>50</sub> and CTD<sub>90</sub>). Both AP and Ca<sup>2+</sup> durations were computed starting from the instant of maximum dV/dt<sub>MAX</sub>.The population was then filtered based on experimental AP recordings (Britton, Bueno-Orovio, Virág, Varró, & Rodriguez, 2017; O'Hara et al., 2011), and Ca<sup>2+</sup> transient recordings (Coppini et al., 2013; Passini et al., 2016) from undiseased human hearts (N = 37 hearts, n = 62 cells for AP, N = 8 hearts, n = 25 cells for Ca<sup>2+</sup> transient). Out of the initial 150 AP models, 107 displayed biomarkers within the experimental ranges (Table 2) and were then used for the in silico drug trials. The refinement of ionic conductance ranges significantly enhanced model acceptance in the final population to >70% compared to ~40% in previous studies (Passini et al., 2017). It is worth noting that variability in the experimental data may be caused in part by experimental interventions, such as the isolation procedure, in addition to the original variability in ion channel density. However, with the population approach,

**TABLE 1** Variability ranges for each of the nine parameters in the control population, expressed as percentage of the baseline model values

Model parameter	Variability range
G <sub>Na</sub>	[30-200]%
G <sub>NaL</sub>	[100-200]%
G <sub>to</sub>	[0-200]%
G <sub>Kr</sub>	[45-100]%
G <sub>Ks</sub>	[0-100]%
G <sub>K1</sub>	[30-200]%
G <sub>NCX</sub>	[100-200]%
G <sub>NaK</sub>	[30-100]%
G <sub>CaL</sub>	[100-200]%

<sup>a</sup>Abbreviations:  $G_{Na}/G_{NaL}$ , fast/late Na<sup>+</sup> current conductance;  $G_{to}$ , transient outward K<sup>+</sup> current conductance;  $G_{Kr}/G_{Ks}$ , rapid/slow delayed rectifier K<sup>+</sup> current conductance;  $G_{K1}$ , inward rectifier K<sup>+</sup> current conductance;  $G_{NCX}$ , Na<sup>+</sup>-Ca<sup>2+</sup> exchanger;  $G_{NaK}$ , Na<sup>+</sup>-K<sup>+</sup>;  $G_{CaL}$ , L-type Ca<sup>2+</sup> current conductance.



**TABLE 2** Experimental AP (Britton, Bueno-Orovio, et al., 2017; O'Hara et al., 2011; Passini et al., 2017) and Ca<sup>2+</sup> transient (Coppini et al., 2013; Passini et al., 2016) biomarker ranges used to calibrate the control population of human ventricular AP in silico models

AP biomarker	Min value	Max value
APD <sub>40</sub>	85 ms	320 ms
APD <sub>50</sub>	110 ms	350 ms
APD <sub>90</sub>	180 ms	440 ms
Tri <sub>90-40</sub>	50 ms	150 ms
dV/dt <sub>MAX</sub>	100 V/s	1000 V/s
V <sub>peak</sub>	10 mV	55 mV
RMP	-95 mV	-80 mV
CTD <sub>50</sub>	120 ms	420 ms
CTD <sub>90</sub>	220 ms	785 ms

<sup>a</sup>Abbreviations: APD<sub>XX</sub>, AP duration at XX% of repolarisation; CTD<sub>XX</sub>, Ca<sup>2+</sup> transient duration at XX% of decay; dV/dt<sub>MAX</sub>, maximum upstroke velocity; RMP, resting membrane potential; Tri<sub>90-40</sub>, AP triangulation, defined as the difference between APD<sub>90</sub> and APD<sub>40</sub>; V<sub>peak</sub>, peak voltage.

we assume that different sources of variability can be globally modelled by varying ion channel conductances.

All the simulations presented in this study were conducted using Virtual Assay (v.2.4.800 © 2014 Oxford University Innovation Ltd. Oxford, UK), a user-friendly software package based on C++, and specifically designed for in silico drug assays in populations of computer models. The verification of Virtual Assay results against additional software packages has already been established (Passini et al., 2017). Further analysis of the results was performed in Matlab (Mathworks Inc. Natwick, MA, USA, RRID:SCR\_001622).

### 2.2 | Human in silico drug trials

In silico drug trials were performed in the population of 107 human AP models for 40 reference compounds. Drug effects were simulated using a simple pore-block model (Brennan, Fink, & Rodriguez, 2009), with IC<sub>50</sub> and Hill coefficient (h) acquired internally in whole-cell automated patch clamp configuration, for four ion channels: fast Na<sup>+</sup> current (I<sub>Na</sub>), rapid/slow delayed rectified K<sup>+</sup> current (I<sub>Kr</sub>/I<sub>Ks</sub>), and L-type Ca<sup>2+</sup> current (I<sub>CaL</sub>). Details on ion channel inhibition protocols are included in the Supporting Information. Additional data on drug/ion channel interactions have been integrated from publications for relevant compounds, as detailed in Supporting Information. Multiple concentrations were investigated for each compound, from 1 to 100-fold the maximal effective free therapeutic concentration (EFTPC<sub>max</sub>). The full list of reference compounds, together with IC<sub>50</sub>/h, EFTPC<sub>max</sub>, and the TdP risk category considered for this study, is included in Table S1.

Each drug was assigned to a TdP risk category, based on the classification by CredibleMeds® (Woosley & Romer, 1999), available on www.crediblemeds.org (Accessed November 30, 2018): 1 (known risk), drugs which prolong the QT interval and are clearly associated with a known risk of TdP, even when taken as recommended; 2 (possible risk), drugs which can cause QT prolongation but currently lack evidence for a risk of TdP risk when taken as recommended; 3 (conditional risk), drugs associated with TdP but only under certain circumstances of their use, for example, excessive dose, in patients with conditions such as hypokalaemia, or when taken with interacting drugs; NC (not classified), the drug was reviewed by CredibleMeds® but the evidence available did not result in a decision for it to be placed in any risk categories. Of the 40 considered compounds, 22 are categorised as known risk and eight as potential/conditional risk, for a total of 30 drugs associated with TdP risk. Verapamil, mexiletine, and diltiazem (categorised as NC) and the remaining seven compounds (not listed in CredibleMeds®) are considered as safe (no TdP risk) for the purpose of this study. The choice of reference compounds evaluated in this study was determined by the ion channel information available internally. Out of the 40 reference compounds, 22 were also investigated earlier by Passini et al., (2017), but using ion channel information from a different source.

For the human in silico drug trials, all 107 models in the experimentally calibrated control population were paced at 1 Hz for 150 beats, for each drug concentration. The last AP and Ca<sup>2+</sup> transient traces of each simulation were compared with the corresponding control (150 beats at 1 Hz without drug). All AP traces were automatically checked for repolarisation and depolarisation abnormalities (RA and DA respectively), as in Passini et al. (2017). Representative traces of these druginduced AP phenotypes are shown in Figure 1a,b. For models not displaying abnormalities,  $APD_{90}$  and  $CTD_{90}$  were computed as described above, together with the EMw, defined as the difference between  $CTD_{90}$  and  $APD_{90}$ , as shown in Figure 1c.

### 2.3 | TdP risk prediction and TdP score

In silico results were used to predict the TdP risk of each drug, based on two different criteria: (a) occurrence of drug-induced RA-a drug is classified as risky if it provokes RA in at least one model of the in silico population, as in Passini et al. (2017); (b) drug-induced changes in the EMw (EMw)-a drug is classified as risky if it shortens the EMw more than 10% (EMw < -10%; Morissette et al., 2016). To quantify EMw in the in silico population, the median of the drug-induced percentage changes of each model compared with the corresponding control was considered. The two above criteria will be hereafter referred to as "RA only" and "RA + EMw." It is worth noting that, following drug application, EMw distributions in the population vary up to four orders of magnitude: Therefore, EMw data are shown in a logarithmic scale. using the log-modulus transformation (L(x) = sign(x) \* log(|x| + 1)), which spreads out the smaller data while preserving their sign (John & Draper, 1980).

By comparing in silico results against the TdP risk categories, drugrisk predictions were divided into true positives (TP, drug with TdP risk



**FIGURE 1** Druginduced AP phenotypes and APD<sub>90</sub>, CTD<sub>90</sub> and EMw biomarkers. (a,b) Representative AP traces illustrating repolarisation abnormalities (a) and depolarisation abnormalities (b). (c) In silico EMw, defined here as the difference between CTD<sub>90</sub> and APD<sub>90</sub>



classified as risky); true negatives (TN, drug with no TdP risk classified as safe); FP (drug with no TdP risk, classified as risky); and false negatives (FN, drugs with TdP risk, classified as safe). Prediction performances were evaluated based on sensitivity = TP/(TP + FN); specificity = TN/(TN + FP); accuracy = (TN + TP)/(TN + TP + FN + FP); positive predictive value = TP/(TP + FP); and negative predictive value = TN/(TN + FN).

The scoring system based on RA occurrence proposed in Passini et al. (2017), in order to integrate the results obtained at different concentrations, was extended to include the information provided by the EMw, according to the following formulas:

new TdP score 
$$= \frac{\sum_{i} [w_i^* (nRA_i + nEMw_i)]}{n_{tot}^* \sum_{i} (w_i)}$$
original TdP score
$$= \frac{\sum_{i} (w_i^* nRA_i)}{n_{tot}^* \sum_{i} (w_i)}$$
from Passini et al.(2017),

where  $nRA_i$  is the number of models showing RA at the tested concentration *i* (*C<sub>i</sub>*),  $nEMw_i$  is the number of models for which  $EMw_i < -10\%$ ,  $w_i = EFTPC_{max}/C_i$  is the weigth inversely related to the tested concentration *C<sub>i</sub>*, and *n<sub>tot</sub>* is the total number of models in the population. For

each tested concentration  $C_i$ , the score considers the fraction of models showing drug-induced RA ( $nRA_i/n_{tot}$ ) or shortening of the EMw ( $nEMw_i/n_{tot}$ ) beyond threshold. All contributions are multiplied for a weight inversely related to their testing concentration (e.g., 1/30 for  $nRA_i$ + $nEMw_i$  observed at 30× EFTPC<sub>max</sub>) and added together for metric normalisation. Therefore, the final TdP score varies between 0 and 1, where 0 corresponds to a drug that does not provoke RA nor EMw shortening beyond threshold in any of the models in the population, while 1 corresponds to a drug that shows either RA or EMw shortening beyond threshold in 100% of the models, at all tested concentrations. By using the proposed score, RA and EMw shortening are naturally considered more severe when occurring at lower concentrations and/or affecting a higher fraction of the population of models.

### 2.4 | Ion channel block sensitivity analysis

To investigate the difference in drug-induced TdP risk predictions across different biomarkers (RA, EMw, and APD<sub>90</sub>), we performed a sensitivity analysis of multichannel drug blocks for the three ion channels which are known to play a major role in RA generation (Passini et al., 2016):  $I_{Kr}$ ,  $I_{CaL}$ , and  $I_{NaL}$ . Simulations were run for all the



**FIGURE 2** Optimised population of human ventricular models. (a) AP and  $Ca^{2+}$  transient traces of the 107 models in the calibrated population (blue and green respectively). (b) Ionic profile of the calibrated population, shown as scaling factors with respect to the baseline model. Central mark corresponds to median, box limits are the 25<sup>th</sup> and 75<sup>th</sup> percentiles, and whiskers extend to the most extreme data points. (c) AP and  $Ca^{2+}$  transient biomarker distributions for the calibrated population (blue histograms) and experimental ranges (black lines): AP duration at 40%, 50%, and 90% of repolarisation (APD<sub>40</sub>, APD<sub>50</sub>, and APD<sub>90</sub>); AP triangulation, as difference between APD<sub>90</sub> and APD<sub>40</sub> (Tri<sub>90-40</sub>);  $Ca^{2+}$  transient duration at 50% and 90% of decay (CTD<sub>50</sub> and CTD<sub>90</sub>)



combinations of five different current block percentages (0%, 25%, 50%, 75%, and 100%), for a total of  $5^3 = 125$  simulations. For each simulation, changes in the EMw and APD<sub>90</sub> compared to control were considered, as well as the fraction of models displaying either RA, EMw shortening beyond threshold (<-10%, as described above) or APD<sub>90</sub> prolongation beyond threshold (>6%, as defined in Passini et al., 2017). The data and statistical analysis comply with the recommendations of the British Journal of Pharmacology on experimental design and analysis in pharmacology.

### 2.5 | Nomenclature of targets and ligands

Key protein targets and ligands in this article are hyperlinked to corresponding entries in http://www.guidetopharmacology.org, the common portal for data from the IUPHAR/BPS Guide to PHARMA-COLOGY (Harding *et al.*, 2018), and are permanently archived in the Concise Guide to PHARMACOLOGY 2017/18 (Alexander, Kelly et al., 2017; Alexander, Striessnig et al., 2017).

## 3 | RESULTS

## An optimised human in silico control population of models

Figure 2 shows an illustrative summary of the human control population of 107 models, including AP and Ca<sup>2+</sup> transient traces (Figure 2a, blue and green respectively); ionic profile boxplots (Figure 2b), reflecting the ranges defined in Table 1; AP and Ca<sup>2+</sup> transient biomarker distributions (Figure 2c) and the corresponding human experimental ranges defined in Table 2 (black lines). All the 107 models show a healthy-looking AP phenotype, with all the AP and Ca<sup>2+</sup> transient biomarkers within the experimental ranges. They also have, by design, a weak repolarisation reserve (Varshneya, Devenyi, & Sobie, 2018), that is, the main repolarising currents are down-regulated, while the main inward currents are up-regulated. It is worth noting that, mainly due to I<sub>Kr</sub> down-regulation, the AP biomarkers more representative of the repolarisation phase (APD<sub>40</sub>, APD<sub>50</sub>, APD<sub>90</sub>, and Tri<sub>90-40</sub>) are distributed in the upper part of the experimental ranges.



**FIGURE 3** Drug-induced changes in EMw (EMw) in the in silico population for 40 compounds at 10× EFTPC<sub>max</sub>. Data are shown using the logmodulus transformation, as described in Section 2. EMw shortening threshold (–10%) is marked as a dashed red line. Colour scale (green to red) corresponds to TdP risk category: no TdP risk (green), conditional (yellow), possible (orange), and known (red) TdP risk. Drug-induced RA occurrence is marked by one or more asterisks, based on the fraction of models displaying RA: \* (>10%), \*\* (>30%), \*\*\* (>50%). Boxplots are not shown for drugs exhibiting more than 97% RA (three models or less for which to compute the EMw), and these are depicted on the dotted line at the bottom of the figure. Boxplots description as in Figure 2. Result obtained by using the single ORd model are shown as black dots, connected by a dashed black line

# 3.1 $\parallel\,$ Risky drugs induce shortening of the in silico EMw

Figure 3 shows the EMw distributions computed using the in human in silico model population for the 40 reference compounds, tested at 10× EFTPC<sub>max</sub>. Drugs inducing EMw shortening (EMw < -10%) are classified as risky (boxplots with median below the red dashed line), while drugs prolonging the EMw or inducing below-threshold EMw changes are considered safe (boxplots with median above the red dashed line). Many of the drugs shortening the EMw also induce RA in the population of models (marked with asterisks). All drugs with known TdP risk (red boxplots) are correctly predicted as risky using the in silico EMw. All safe drugs (green boxplots) are correctly classified as safe, except for Mexiletine. Only three drugs with possible/conditional TdP risk (orange/yellow boxplots) are categorised as safe: amitriptyline, ivabradine, nicardipine. Drug-induced EMw increase in magnitude with the tested concentrations (Figures S1-S2). For testing concentrations of 30× and 100×  $\mathsf{EFTPC}_{\mathsf{max}}$ , some compounds categorised as safe (i.e., ivabradine, metoprolol, and verapamil) can induce EMw shortening beyond threshold (Figure S2).

It is worth noting that, for all drugs, 75% of the models are either above or below the 10% EMw threshold, including the baseline ORd model (black dots, connected by a dashed black line in Figure 3). Even though predictions based on a single model would yield the same prediction accuracy as the population, for many drugs, such as ciprofloxacin, clarithromycin, clozapine, levofloxacin, ondansetron, pentamidine, and risperidone), the drug-induced EMw changes for the baseline model are very close to the threshold. In those cases, the population results provide additional evidence on the confidence and robustness of the simulations, thus reinforcing the results.

# 3.2 | Shortening of the EMw improves TdP risk prediction at low concentrations

Figure 4 shows a summary of the in silico predictions of clinical TdP risk for the 40 reference compounds at all tested concentrations, based on the two criteria described in Section 2: RA only (top line, in blue); RA + EMw (bottom line, in orange). The two different criteria reach the same maximum accuracy of 90% (highlighted with a rectangle), with 27/30 risky drugs classified as risky, 9/10 safe drugs classified as safe, and misclassified drugs as in Figure 3 (FN: amitriptyline, ivabradine, nicardipine; FP: mexiletine). However, the concentration at which the 90% accuracy is reached is substantially lower for predictions based on EMw shortening (10× vs. 100× EFTPC<sub>max</sub>). For both criteria, sensitivity always increases with the tested concentrations, whereas specificity decreases at very high drug concentrations for RA + EMw.

Figure 5 illustrates how the additional information provided by drug-induced EMw shortening in the TdP score improves the separation between safe and risky drugs in the TdP score plot, with respect

	up to		up to		<i>up to</i>		<i>up to</i>		<i>up to</i>	
	1× EFTPC <sub>m</sub>		3× EFTPC <sub>max</sub>		10× EFTPC <sub>max</sub>		30× EFTPC <sub>max</sub>		100× EFTPC <sub>max</sub>	
	true +	true –	true +	true –	true +	true –	true +	true –	true +	true –
	6	<b>10</b>	<b>13</b>	<b>10</b>	<b>18</b>	9	<b>22</b>	<b>9</b>	<b>27</b>	<b>9</b>
A only	FALSE +	false – 24	FALSE +	false – 17	FALSE + 1	false – 12	FALSE + 1	false – 8	FALSE + 1	false – 3
R	Accuracy: 40%		Accuracy: 58%		Accuracy: 68%		<u>Accuracy: 78%</u>		Accuracy: 90%	
	Sensitivity. 20%		Sensitivity. 43%		Sensitivity. 60%		Sensitivity. 73%		Sensitivity. 90% -	
	Specificity: 100%		Specificity: 100%		Specificity: 90%		Specificity: 90%		Specificity: 90%	
	PPV: 100% - NPV: 29%		PPV: 100% - NPV: 37%		PPV: 95% - NPV: 43%		PPV: 96% - NPV: 53%		PPV: 96% - NPV: 75%	
M	true +	true –	true +	true –	true +	true –	true +	true –	true +	true –
	<b>19</b>	<b>9</b>	<b>23</b>	9	<b>27</b>	<b>9</b>	<b>27</b>	<b>7</b>	<b>28</b>	<b>6</b>
+ AEM	FALSE +	false –	FALSE +	false –	false +	FALSE –	FALSE +	false –	FALSE +	false –
	1	11	1	7	1	3	3	3	4	2
RA	Accuracy: 70%		<u>Accuracy: 80%</u>		Accuracy: 90%		Accuracy: 85%		Accuracy: 85%	
	Sensitivity: 63%		Sensitivity: 77%		Sensitivity: 90%		Sensitivity: 90%		Sensitivity: 93%	
	Specificity: 90%		Specificity: 90%		Specificity: 90%		Specificity: 70%		Specificity: 60%	
	PPV: 95% - NPV: 45%		PPV: 96% - NPV: 56%		PPV: 96% - NPV: 75%		PPV: 90% - NPV: 70%		PPV: 88% - NPV: 75%	

**FIGURE 4** Clinical TdP risk predictions for 40 reference compounds, at five concentrations (multiples of EFTPC<sub>max</sub>) in the human in silico population of models, using RA occurrence only (top line, in blue), or using RA + EMw (bottom line, in orange). Predictions with accuracy >80% are shown in bold. Predictions with highest accuracy are highlighted with a rectangle



FIGURE 5 TdP scores, computed for the 40 reference compounds considering RA only (a) and RA + EMw (b). Compounds with a low TdP score are predicted to be safe, while compounds with a high TdP score are predicted to be risky. Drug TdP risk categories as in Figure 3, from green to red

to using RA only (Figure 5a vs. 5b). Results shown in Figure 5a are also depicted in Figure S3 with a logarithmic scale, required to appreciate separation for low TdP values. The four drugs that are misclassified according to the TdP score plot correspond to the FN/FP in Figure 3.

# 3.3 | The EMw is strongly correlated with $Ca^{2+}$ transient biomarkers but not to APD<sub>90</sub>

Figure 6 illustrates the relationship between EMw and APD<sub>90</sub> or  $CTD_{90}$  in panels 6a and 6b, and 6c and 6d respectively. All traces and dots are colour-coded based on the corresponding EMw magnitude. Figure 6a,b shows a weak correlation between EMw and APD<sub>90</sub>, whereas a strong correlation is observed between EMw and  $CTD_{90}$  (Figure 6c,d), with Pearson correlation coefficients equal to -0.55 and +0.90 for APD<sub>90</sub> and  $CTD_{90}$  respectively. Models in the population with the same APD<sub>90</sub> can have substantially different EMw, whereas a low Ca<sup>2+</sup> transient peak always translates into a long  $CTD_{90}$  (the 90% threshold of Ca<sup>2+</sup> transient decay is closer to 0), which in turn contributes to a large EMw.

This is particularly relevant when considering multichannel drug effects affecting ion channels with different block potencies. As an example, Figure S4 shows three different combinations of ion channel block, all inducing the same APD<sub>90</sub> prolongation (+44% with respect to control), but with very different outcomes in terms of CTD<sub>90</sub>, and in turn EMw:  $I_{Kr}$  block;  $I_{Kr} + I_{CaL}$  block; and  $I_{Kr} + I_{NaL}$  block. When blocking  $I_{Kr}$  only, or  $I_{Kr} + I_{NaL}$ , the APD<sub>90</sub> is prolonged, but there is almost no effect in CTD<sub>90</sub>, thus resulting in an overall shortening of the EMw. On the contrary, when  $I_{CaL}$  block is also present, the APD<sub>90</sub> prolongation is accompanied by a CTD<sub>90</sub> prolongation, and therefore, no change is observed in the EMw. It is worth noting that both  $I_{CaL}$  and  $I_{NaL}$  blocks counteract the APD<sub>90</sub> prolongation induced by  $I_{Kr}$  block: This is why a larger  $I_{Kr}$  block is needed to obtain the same APD<sub>90</sub> prolongation when also including a 50%  $I_{CaL}$  or  $I_{NaL}$  blocks.

# 3.4 $\mid$ The EMw is more sensitive to Ca<sup>2+</sup> current block than APD<sub>90</sub>

Figure 7 illustrates the results of investigations into the factors determining differences in drug-induced TdP risk predictions for the



**FIGURE 6** Relationship between APD<sub>90</sub>, CTD<sub>90</sub>, and EMw, in the 107 human ventricular AP models in control. All data are colour coded (bar on the right) based on the magnitude of the corresponding EMw, from 0 ms (yellow) to 410 ms (dark pink). (a) AP traces for the control population. (b) EMw versus APD<sub>90</sub>, and their regression line. (c)  $Ca^{2+}$  transient traces for the control population. (d) EMw versus CTD<sub>90</sub>, and their regression line



**FIGURE 7** (a) Effect of multiple ion channel blocks ( $I_{Kr}$ ,  $I_{CaL}$ , and  $I_{NaL}$ ) on APD<sub>90</sub> (bottom row) and EMw (top row). Each column corresponds to a fixed percentage of  $I_{NaL}$  block (from 0% to 100%, left to right), and each single plot summarises the results for the 25 combinations of  $I_{Kr}$  and  $I_{CaL}$  blocks (y and x axis respectively). Values shown are the median changes in the 107 human models. "-" indicates that value could not be obtained due to occurrence of RA or lack of Ca<sup>2+</sup> transient (e.g., total  $I_{CaL}$  block). Opposite colour scales were used for EMw and APD<sub>90</sub>, from white to black for EMw and from black to white for APD<sub>90</sub>. Since drug-induced TdP risk is associated with EMw shortening and APD<sub>90</sub> prolongation, for both biomarkers, white is therefore associated with high risk. (b) Effect of multiple ion channel blocks on the fraction of models displaying RA occurrence (top row), EMw shortening beyond threshold (middle row), and APD<sub>90</sub> prolongation beyond threshold (bottom row). Numerical values are all in the range (0–100)%, coloured from black to white, and higher values correspond to block combinations predicted at higher risk for that specific biomarker

different biomarkers (RA, EMw, and APD\_{90}) for combinations of  $I_{Kr},$   $I_{CaL},$  and  $I_{NaL}$  blocks, from 0% to 100%.

Figure 7a shows the effect of the combinations of considered ion channel blocks on EMw (top row) and APD<sub>90</sub> (bottom row). Each column

corresponds to a fixed percentage of  $I_{NaL}$  block (from 0% to 100%, left to right), and each single plot summarises the results for the 25 combinations of  $I_{Kr}$  and  $I_{CaL}$  blocks (y and x axis respectively). The EMw shortens with the percentage of  $I_{Kr}$  block (from bottom to top, in each plot) and

increases with the percentage of  $I_{CaL}$  block (from left to right, in each plot). When combining both blocks at the same time, the two opposite effects compensate each other, with  $I_{CaL}$  block playing the major role (e.g., 50%  $I_{Kr}$  and  $I_{CaL}$  blocks induce a EMw = +17%). Shortening of the EMw is therefore observed only in the top-left corner of each plot. APD<sub>90</sub> increases with  $I_{Kr}$  block and decreases with  $I_{CaL}$  block. However, in this case,  $I_{Kr}$  has the predominant effect (e.g., 50%  $I_{Kr}$  and  $I_{CaL}$  blocks induce a APD<sub>90</sub> = +33%).  $I_{NaL}$  block has a positive effect on both biomarkers, contributing to counteract EMw shortening and APD<sub>90</sub> prolongation caused by  $I_{Kr}$  block.

Figure 7b quantifies risk predictions for each of the scenarios explored in the sensitivity analysis of Figure 7a, with numerical values indicating in this case the fraction of models displaying: RA occurrence (top row), EMw shortening beyond threshold (middle row), and APD<sub>90</sub> prolongation beyond threshold (bottom row). Numerical values are therefore all in the range (0–100)%, coloured from black to white, and higher values correspond to block combinations predicted at higher risk for those specific biomarkers. No RA occur when  $I_{Kr}$  is blocked less than 75%, in agreement with Britton, Bueno-Orovio, et al., (2017). However, the fractions of models displaying RA is overall higher in this study, for example, 25%  $I_{CaL}$  block, 75%  $I_{Kr}$  block: 49% versus 1% of models displaying RA. This is due to the novel design of the population, with ionic conductances defined to maximise the likelihood of RA.

RA and EMw show a similar pattern: The fraction of models displaying RA or EMw shortening beyond threshold increases with  $I_{\mathsf{Kr}}$  block and decreases with  $I_{\mathsf{CaL}}$  block. The block scenarios at higher risk are distributed in the top-left corner of each plot. However, changes in the EMw occur at lower percentage of IKr block, making it a more sensitive biomarker for low testing concentrations. On the contrary, APD<sub>20</sub> prolongation is less sensitive to I<sub>Cal</sub> block, compared to  $I_{Kr}$  block. Therefore, all the scenarios where  $I_{Kr}$  is blocked more than 25% would be considered as risky based on this biomarker only. This would lead to a misclassification of safe compounds which affect both  $I_{CaL}$  and  $I_{Kr}$ , for example, verapamil, which at 3× EFTPCmax blocks  $I_{Kr}$ ~25% and I<sub>CaL</sub> ~40% (based on IC<sub>50</sub>/h in Table S1). I<sub>NaL</sub> block contributes to decreasing the fraction of models involved for each scenario, by contrasting APD<sub>90</sub> prolongation. To better illustrate the effect of  $I_{NaL}$  block, Figure S5 shows the results of the sensitivity analysis with I<sub>CaL</sub> and I<sub>NaL</sub> block swapped.

### 4 | DISCUSSION AND CONCLUSIONS

Human in silico drug trials were conducted for 40 reference compounds with multichannel blocking actions, to evaluate how druginduced EMw shortening can potentially improve predictions of clinical pro-arrhythmic risk. A population of human ventricular AP models was optimised to capture pro-arrhythmic ionic profiles, blindly to the drug trials results.

The main findings of this simulation study are the following:

1. Predictions of clinical TdP risk based on in silico EMw shortening have a high accuracy (90% for 40 reference compounds) at low tested concentrations (up to  $10 \times \text{EFTPC}_{max}$ ). Predictions based on RA occurrence reach the same accuracy, but only when testing up to  $100 \times \text{EFTPC}_{max}$ . Reducing the maximum tested concentration is particularly important to minimise the risk of FP. It also reduces the simulation time required for each drug. The updated version of the TdP score, integrating information about both RA and EMw, also provides a better separation of safe/risky drugs compared to RA only (Figure 5).

- 2. EMw shortening is an effective biomarker for TdP risk prediction because it is more sensitive to  $I_{CaL}$  block compared to APD<sub>90</sub>. Indeed, taking into account drug-induced changes in the EMw allows discrimination between pure  $I_{Kr}$  blockers, prolonging APD<sub>90</sub> but with very little effect on Ca<sup>2+</sup> transient, and those exhibiting also  $I_{CaL}$  block, where cardiac adverse events are less likely to occur.
- 3. The novel design for population of models, where ionic current conductances are sampled to maximise the models accepted during calibration as well as drug-induced RA is successful for optimising populations for in silico drug trials. An accuracy comparable to our previous study (90% vs. 89% in Passini et al., 2017) was achieved by using about one tenth of the models, thus considerably reducing computing time (from 45 to 5 min for each compound at each concentration).

It is important to highlight that we correctly classified as risky all drugs with known TdP risk. When considering only drugs not listed in CredibleMeds (safe for the purpose of this study) and drugs with known TdP risk, our predictions show 100% accuracy, with 22 TP and eight TN. The results of this study are also fully consistent with previous in silico results, obtained with a similar methodology (Passini et al., 2017). Even if the two studies are based on different  $IC_{50}/h$  data sets, the classification for the 22 compounds in common is equivalent: 18 TP, three TN, and one FP.

Compounds misclassified as FN (nicardipine, ivabradine, and amitriptyline) all belong to potential/conditional risk categories, which are usually associated with overdoses or interactions with other drugs, and often controversial. Two of them (nicardipine and ivabradine) have actually been considered as negative controls in previous studies (Champéroux et al., 2005; Morissette et al., 2016). By considering these two drugs as safe, our prediction accuracy would reach 95% (Sensitivity 96%, Specificity 92%). The last FN, mitriptyline, affects both IKr and ICaL currents: The resulting safety profile is given by the balance between these two blocks, the former leading to QT prolongation and potentially TdP and the latter contributing to QT shortening and suppression of RA. Our input data could minimise amitriptyline risk by underestimating its effect on hERG trafficking (Dennis, Nassal, Deschenes, Thomas, & Ficker, 2011) and overestimating  $I_{\text{CaL}}\ IC_{50},$  for which controversial values have been reported (Crumb, Vicente, Johannesen, & Strauss, 2016; Lancaster & Sobie, 2016; Mirams et al., 2011; Zahradnı et al., 2008).

The only FP in this study is mexiletine, also misclassified in Passini et al. (2017). Mexiletine is a multichannel blocker, affecting mainly fast and late  $I_{Na}$ , as well as  $I_{Kr}$ . Based on a literature review, we can

speculate that the main reason for the misclassification relies in an overestimation of  $I_{Kr}$  block when using a simple pore drug block model. Mexiletine binds preferably to the open state of the hERG channel (Gualdani et al., 2015), and predictions could potentially improve by using a dynamic hERG channel drug block model, as the one recently proposed by the FDA (Dutta et al., 2017; Li et al., 2017). A more detailed discussion on the FN/FP drugs is included in the Supporting Information.

Compared to the classification shown in Passini et al. (2017), based on RA occurrence alone, the inclusion of the EMw has the main advantage of decreasing the need to test very high concentrations (Krogh-Madsen et al., 2017), while still considering a wide concentration range, which allows exploration of the drug effect induced by potential overdoses, as well as the EFTPCmax variability across patients. Testing EFTPCmax multiples is also the methodology proposed by within the Comprehensive in vitro Proarrhythmia Assay (CiPA) initiative (Li et al., 2019; Sager et al., 2014). Predictions based on EMw shortening achieved the same accuracy than those based on RA occurrence only, but at concentrations much closer to therapeutic doses (10× vs. 100× EFTPCmax). Reducing the range of tested concentrations also leads to a reduction of the simulation times required for each drug and, most importantly, limits the risk of inducing FP. While sensitivity increases with the tested concentration, specificity based on RA + EMw tends to decrease at high concentrations, when even safe compounds can cause a large EMw shortening (Figure S3). FBs at high concentrations are less likely to occur for RA: A small degree of I<sub>CaL</sub> block is sufficient to inhibit drug-induced RA, even without counteracting APD<sub>90</sub> prolongation and EMw shortening (Figure S6). The inclusion of the EMw also improves the separation between safe and risky drugs in the TdP score, originally presented in Passini et al. (2017). When considering the fraction of models displaying RA + EMw, the TdP score of risky drugs increases due to the EMw contribution, allowing for a clearer risk classification. It is worth noting that all models displaying RA at a specific concentration also show EMw shortening at a lower one (Figure S7).

Even if the shortening of the EMw has been presented as an effective biomarker of pro-arrhythmia in several experimental studies (Guns, Johnson, Van Op den Bosch, et al., 2012; Guns, Johnson, Weltens, & Lissens, 2012; Morissette et al., 2016; van der Linde et al., 2010), some controversy on its added value compared to APD<sub>90</sub> prolongation still exists (Stams et al., 2014). Our sensitivity analysis, exploring 125 multiple combinations of  $I_{Kr}$ ,  $I_{CaL}$ , and  $I_{NaL}$ blocks, showed how the EMw is more sensitive to drug-induced changes in Ca<sup>2+</sup> transient, and it is therefore able to distinguish between drugs which purely affect  $I_{Kr}$  and those with a multichannel action also modifying Ca<sup>2+</sup> dynamics. As shown in Figure 7, risk predictions based on APD<sub>90</sub> prolongation and EMw shortening are only in agreement when I<sub>CaL</sub> block is equal to 0%, showing progressive disagreement when I<sub>CaL</sub> block increases. Our results therefore explain why, in the in vivo canine atrioventricular block (CAVB) model under the effect of dofetilide "the EMw is solely reflecting changes in QT prolongation" (Stams et al., 2014): Dofetilide, well known to be a selective  $I_{Kr}$  blocker, exerts little or no effect on the Ca<sup>2+</sup> transient,

but it prolongs the APD<sub>90</sub>, thus causing, in turn, EMw shortening (Figure S4). However, our results suggest that the EMw is a better biomarker than APD<sub>90</sub> for drugs with a multichannel effect, as it also reflects changes in the Ca<sup>2+</sup> transient. It captures the balance between I<sub>Kr</sub> and I<sub>CaL</sub> blocks, which could result in a reduced likelihood of RA, while still causing APD<sub>90</sub> prolongation (Figure S6). In addition, it is known that in the CAVB model, there is compensated hypertrophy and increased contractility, and numerous modifications in ion channels and Ca<sup>2+</sup> handling have been reported, confirming a reduced repolarisation reserve (Bourgonje et al., 2013; Oros, Beekman, & Vos, 2008; Sipido et al., 2000; Volders et al., 1998). This could mask the effects of test article inhibition on inward currents (I<sub>CaL</sub> and I<sub>Na</sub>) which could lead to a greater effect of pure hERG blockers and to a reduced ability to assess multichannel block.

The results of this study are in overall agreement with experimental EMw measurements obtained in the in vivo guinea pig model for 26 compounds, and recently published by Morissette et al. (2016). In that paper, the authors classified compounds in four classes: proarrhythmic agents, rare cases of arrhythmias, negative controls, and positive inotropes. Compounds in the first two categories tend to induce EMw shortening, while compounds classified as negative controls show EMw increase or very little change following drug application. As mentioned above, this class also includes nicardipine and ivabradine. Results in the in vivo guinea pig are in qualitative agreement with our simulations, with the exception of the three positive inotropes: dobutamine, milrinone and levosimendan. These compounds are correctly classified as safe using our in silico trials, as they show a slight increase of the EMw following drug application. On the contrary, in the in vivo guinea pig model, they cause a substantial EMw shortening (>-10%), even though they have no effect on OTc interval and they are not classified as pro-arrhythmic agents. This is because the shortening of the EMw induced by these compounds is not driven by QT prolongation (Morissette et al., 2016), but rather by other mechanisms. Milrinone and dobutamine act by increasing cAMP which ultimately increases intracellular Ca<sup>2+</sup> and in turn contractility, while levosimendan acts by increasing the affinity of troponin C for Ca<sup>2+</sup>, thus suggesting that the EMw can also shorten following an increase in contractility not necessarily related to an increase in intracellular Ca<sup>2+</sup> concentration. We did not include those mechanisms in our in silico models, and therefore, they did not yielded the EMw shortening observed experimentally. The EMw considered in this study (CTD<sub>90</sub>-APD<sub>90</sub>) is a single cell surrogate measure for the in vivo EMw, defined as the difference between the end of the left ventricular pressure wave and the end of repolarisation (QT interval). In our study, we evaluate the effects of ion channel block on the EMw, as IC<sub>50</sub> values are routinely evaluated during the drug development process. Therefore, the EMw only captures drug-induced changes on ionic currents, in turn affecting Ca<sup>2+</sup> transient. Extensions to this approach, such as the consideration of drugs affecting the contractile machinery directly, and not via electrophysiology, could be simulated by integrating cardiac contraction models available in literature (Land et al., 2017; Negroni & Lascano, 2008) and conducting electromechanical simulations, typically requiring supercomputing power,

which would allow computation of biomarkers such as QT and left ventricular pressure. This would also improve EMw predictions for the positive inotropic compounds (i.e., dobutamine, milrinone, and levosimendan), bringing our simulation results closer to the experimental observations (Morissette et al., 2016). In addition, there are other Ca<sup>2+</sup> biomarkers described, which could provide similar or complementary information to the EMw, for example, the rate of Ca<sup>2+</sup> transient decay, shown to be slower in failing human ventricular myocytes (Piacentino et al., 2003). Finally, we considered drug effects on Na<sup>+</sup>, Ca<sup>2+</sup>, and K<sup>+</sup> ion channels as inputs, and the EMw proved to be an effective biomarker to predict arrhythmic risk based on those. However, some drugs could affect other mechanisms, for example, SERCA pump, Na<sup>+</sup>–K<sup>+</sup> pump, or Na<sup>+</sup>–Ca<sup>2+</sup> exchanger, and should this information become available, it could be easily incorporated into our simulations.

To conclude, this study demonstrates that in silico drug trials using the EMw constitute a powerful methodology to predict clinical risk of arrhythmias based on ion channel information. Such information is frequently available at the early stages of lead compound identification, and the integration of computer models in the existing pipelines for drug safety assessment could lead to a major replacement of animal experiments in the preclinical stages of drug development.

### ACKNOWLEDGEMENTS

E.P., C.T., A.B.O., and BR were respectively supported by an NC3Rs Infrastructure for Impact Award (NC/P001076/1), a DPhil scholarship funded by the Department of Computer Science (University of Oxford), a British Heart Foundation (BHF) Intermediate Basic Science Research Fellowship (FS/17/22/32644), and a Wellcome Trust Senior Research Fellowship in Basic Biomedical Sciences (100246/Z/12/Z and 214290/Z/18/Z). These authors also acknowledge additional support from EPSRC Impact Acceleration Awards (EP/K503769/1), the CompBioMed project (European Commission grant agreement 675451), the Oxford BHF Centre of Research Excellence (RE/08/ 004/23915 and RE/13/1/30181), and the TransQST project (Innovative Medicines Initiative 2 Joint Undertaking under grant agreement 116030, receiving support from the European Union's Horizon 2020 research and innovation programme and EFPIA).

### AUTHOR CONTRIBUTIONS

All the authors conceived and designed the study; E.P. designed the population of models for in silico drug assays, analysed the data, prepared the figures, and drafted the manuscript; E.P. and C.T. performed the simulations; P.M. and F.S. collected and provided the data for the reference compounds; E.P., A.B.O., and B.R. interpreted the results; all the authors edited and revised the manuscript and approved the final version.

### CONFLICT OF INTEREST

E.P., C.T., A.B.O., and B.R. declare no conflicts of interest. P.M. and F.S. are employees of Merck & Co., Inc.

### DECLARATION OF TRANSPARENCY AND SCIENTIFIC RIGOUR

This Declaration acknowledges that this paper adheres to the principles for transparent reporting and scientific rigour of preclinical research as stated in the *BJP* guidelines for Design & Analysis, and as recommended by funding agencies, publishers and other organisations engaged with supporting research.

### ORCID

Elisa Passini D https://orcid.org/0000-0003-0116-6347

### REFERENCES

- Alexander, S. P. H., Kelly, E., Marrion, N. V., Peters, J. A., Faccenda, E., Harding, S. D., ... CGTP Collaborators (2017). THE CONCISE GUIDE TO PHARMACOLOGY 2017/18: Transporters. *British Journal of Pharmacology*, 174, S360–S446. https://doi.org/10.1111/bph.13883
- Alexander, S. P. H., Striessnig, J., Kelly, E., Marrion, N. V., Peters, J. A., Faccenda, E., ... CGTP Collaborators (2017). THE CONCISE GUIDE TO PHARMACOLOGY 2017/18: Voltage-gated ion channels. *British Journal* of Pharmacology, 174, S160–S194. https://doi.org/10.1111/bph.13884
- Abbasi, M., Small, B. G., Patel, N., Jamei, M., & Polak, S. (2017). Early assessment of proarrhythmic risk of drugs using the in vitro data and single-cell-based in silico models: Proof of concept. *Toxicology Mechanisms and Methods*, 27, 88–99. https://doi.org/10.1080/ 15376516.2016.1256460
- Berridge, B. R., Hoffmann, P., Turk, J. R., Sellke, F., Gintant, G., Hirkaler, G., ... Pettit, S. D. (2013). Integrated and translational nonclinical in vivo cardiovascular risk assessment: Gaps and opportunities. *Regulatory Toxicology and Pharmacology*, 65, 38–46. https://doi.org/10.1016/j. yrtph.2012.09.007
- Bourgonje, V. J. A., Vos, M. A., Ozdemir, S., Doisne, N., Acsai, K., Varró, A., ... Antoons, G. (2013). Combined Na+/Ca2+ exchanger and I-type calcium channel block as a potential strategy to suppress arrhythmias and maintain ventricular function. *Circulation. Arrhythmia and Electrophysiology*, 6, 371–379. https://doi.org/10.1161/CIRCEP.113.000322
- Brennan, T., Fink, M., & Rodriguez, B. (2009). Multiscale modelling of druginduced effects on cardiac electrophysiological activity. *European Journal of Pharmaceutical Sciences*, 36, 62–77. https://doi.org/10.1016/j. ejps.2008.09.013
- Britton, O. J., Abi-Gerges, N., Page, G., Ghetti, A., Miller, P. E., & Rodriguez, B. (2017). Quantitative comparison of effects of dofetilide, sotalol, quinidine and verapamil between human ex vivo trabeculae and in silico ventricular models incorporating inter-individual action potential variability. *Frontiers in Physiology*, *8*, 597. https://doi.org/10.3389/ fphys.2017.00597
- Britton, O. J., Bueno-Orovio, A., Van Ammel, K., Lu, H. R., Towart, R., Gallacher, D. J., & Rodriguez, B. (2013). Experimentally calibrated population of models predicts and explains intersubject variability in cardiac cellular electrophysiology. *Proceedings of the National Academy* of Sciences of the United States of America, 110, E2098–E2105. https://doi.org/10.1073/pnas.1304382110
- Britton, O. J., Bueno-Orovio, A., Virág, L., Varró, A., & Rodriguez, B. (2017). The electrogenic Na+/K+ pump is a key determinant of repolarization abnormality susceptibility in human ventricular cardiomyocytes: A population-based simulation study. *Frontiers in Physiology*, *8*, 278. https://doi.org/10.3389/fphys.2017.00278
- Champéroux, P., Viaud, K., El Amrani, A. I., Fowler, J. S. L., Martel, E., Le Guennec, J.-Y., & Richard, S. (2005). Prediction of the risk of Torsade de Pointes using the model of isolated canine Purkinje fibres. *British*

BRITISH PHARMACOLOGICAL 3832 BJP BRITISH PHARMACOLOGICA

Journal of Pharmacology, 144, 376–385. https://doi.org/10.1038/sj. bjp.0706070

- Chang, K. C., Dutta, S., Mirams, G. R., Beattie, K. A., Sheng, J., Tran, P. N., ... Li, Z. (2017). Uncertainty quantification reveals the importance of data variability and experimental design considerations for in silico proarrhythmia risk assessment. *Frontiers in Physiology*, *8*, 917. https:// doi.org/10.3389/fphys.2017.00917
- Coppini, R., Ferrantini, C., Yao, L., Fan, P., Del Lungo, M., Stillitano, F., ... Mugelli, A. (2013). Late sodium current inhibition reverses electromechanical dysfunction in human hypertrophic cardiomyopathy. *Circulation*, 127, 575–584. https://doi.org/10.1161/ CIRCULATIONAHA.112.134932
- Crumb, W. J., Vicente, J., Johannesen, L., & Strauss, D. G. (2016). An evaluation of 30 clinical drugs against the comprehensive in vitro proarrhythmia assay (CiPA) proposed ion channel panel. *Journal of Pharmacological and Toxicological Methods*, 81, 251–262. https://doi. org/10.1016/j.vascn.2016.03.009
- Dennis, A. T., Nassal, D., Deschenes, I., Thomas, D., & Ficker, E. (2011). Antidepressant-induced ubiquitination and degradation of the cardiac potassium channel hERG. *The Journal of Biological Chemistry*, 286, 34413–34425. https://doi.org/10.1074/jbc.M111.254367
- Dutta, S., Chang, K. C., Beattie, K. A., Sheng, J., Tran, P. N., Wu, W. W., ... Li, Z. (2017). Optimization of an in silico cardiac cell model for proarrhythmia risk assessment. *Frontiers in Physiology*, *8*, 616. https:// doi.org/10.3389/fphys.2017.00616
- Gualdani, R., Tadini-Buoninsegni, F., Roselli, M., Defrenza, I., Contino, M., Colabufo, N. A., Lentini, G. (2015). Inhibition of hERG potassium channel by the antiarrhythmic agent mexiletine andits metabolite mhydroxymexiletine. *Pharmacology Research and Perspectives*, 3, e00160. https://doi.org/10.1002/prp2.160
- Guns, P.-J., Johnson, D., Van Op den Bosch, J., Weltens, E., & Lissens, J. (2012). The electro-mechanical window in anaesthetized guinea pigs: A new marker in screening for Torsade de Pointes risk. *British Journal* of Pharmacology, 166, 689–701. https://doi.org/10.1111/j.1476-5381.2011.01795.x
- Guns, P.-J., Johnson, D. M., Weltens, E., & Lissens, J. (2012). Negative electro-mechanical windows are required for drug-induced Torsades de Pointes in the anesthetized guinea pig. *Journal of Pharmacological and Toxicological Methods*, *66*, 125–134. https://doi.org/10.1016/j. vascn.2012.03.007
- Harding, S. D., Sharman, J. L., Faccenda, E., Southan, C., Pawson, A. J., Ireland, S., ... NC-IUPHAR (2018). The IUPHAR/BPS guide to pharmacology in 2018: Updates and expansion to encompass the new guide to immunopharmacology. *Nucleic Acids Research*, 46, D1091–D1106. https://doi.org/10.1093/nar/gkx1121
- ICH (2005a). Harmonised Tripartite Guideline E14. Clinical evaluation of QT/QTc interval prolongation and proarrhythmic potential for nonantiarrhythmic drugs.
- ICH (2005b). Harmonised Tripartite Guideline S7B. Non-clinical evaluation of the potential for delayed ventricular repolarization (QT interval prolongation) by human pharmaceuticals.
- John, J. A. & Draper, N. R. (1980). An Alternative Family of Transformations. Applied Statistics, 29, 190–197. https://doi.org/10.2307/ 2986305
- Krogh-Madsen, T., Jacobson, A. F., Ortega, F. A., & Christini, D. J. (2017). Global optimization of ventricular myocyte model to multi-variable objective improves predictions of drug-induced Torsades de Pointes. *Frontiers in Physiology*, *8*, 1059. https://doi.org/10.3389/ fphys.2017.01059
- Lancaster, M. C., & Sobie, E. A. (2016). Improved prediction of druginduced Torsades de Pointes through simulations of dynamics and

machine learning algorithms. *Clinical Pharmacology and Therapeutics*, 100, 371–379. https://doi.org/10.1002/cpt.367

- Land, S., Park-Holohan, S.-J., Smith, N. P., dos Remedios, C. G., Kentish, J. C., & Niederer, S. A. (2017). A model of cardiac contraction based on novel measurements of tension development in human cardiomyocytes. *Journal of Molecular and Cellular Cardiology*, 106, 68–83. https://doi.org/10.1016/j.yjmcc.2017.03.008
- Laverty, H. G., Benson, C., Cartwright, E. J., Cross, M. J., Garland, C., Hammond, T., ... Valentin, J. P. (2011). How can we improve our understanding of cardiovascular safety liabilities to develop safer medicines? *British Journal of Pharmacology*, 163, 675–693. https://doi.org/ 10.1111/j.1476-5381.2011.01255.x
- Lawrence, C. L., Bridgland-Taylor, M. H., Pollard, C. E., Hammond, T. G., & Valentin, J.-P. (2006). A rabbit Langendorff heart proarrhythmia model: Predictive value for clinical identification of Torsades de Pointes. *British Journal of Pharmacology*, 149, 845–860.
- Li, Z., Dutta, S., Sheng, J., Tran, P. N., Wu, W., Chang, K., ... Colatsky, T. (2017). Improving the in silico assessment of proarrhythmia risk by combining hERG (human ether-à-go-go-related gene) channel-drug binding kinetics and multichannel pharmacology. *Circulation. Arrhythmia and Electrophysiology*, 10, e004628.
- Li, Z., Ridder, B. J., Han, X., Wu, W. W., Sheng, J., Tran, P. N., ... Strauss, D. G. (2019). Assessment of an in silico mechanistic model for proarrhythmia risk prediction under the CiPA initiative. *Clinical Pharmacology and Therapeutics*, 105, 466–475.
- van der Linde, H. J., van Deuren, B., Somers, Y., Loenders, B., Towart, R., & Gallacher, D. J. D. (2010). The electro-mechanical window: A risk marker for Torsade de Pointes in a canine model of drug induced arrhythmias. *British Journal of Pharmacology*, 161, 1444–1454. https://doi.org/10.1111/j.1476-5381.2010.00934.x
- Mirams, G. R., Cui, Y., Sher, A., Fink, M., Cooper, J., Heath, B. M., ... Noble, D. (2011). Simulation of multiple ion channel block provides improved prediction of compounds' clinical torsadogenic risk. *Cardiovascular Research*, 91, 53–61. https://doi.org/10.1093/cvr/cvr044
- Morissette, P., Regan, C., Fitzgerald, K., Gerenser, P., Travis, J., Wang, S., ... Sannajust, F. (2016). Shortening of the electromechanical window in the ketamine/xylazine-anesthetized guinea pig model to assess proarrhythmic risk in early drug development. *Journal of Pharmacological and Toxicological Methods*, 81, 171–182. https://doi.org/10.1016/j. vascn.2016.06.003
- Muszkiewicz, A., Britton, O. J., Gemmell, P., Passini, E., Sanchez, C., Zhou, X., ... Rodriguez, B. (2016). Variability in cardiac electrophysiology: Using experimentally-calibrated populations of models to move beyond the single virtual physiological human paradigm. *Progress in Biophysics and Molecular Biology*, 120, 115–127. https://doi.org/10.1016/ j.pbiomolbio.2015.12.002
- Negroni, J. A., & Lascano, E. C. (2008). Simulation of steady state and transient cardiac muscle response experiments with a Huxley-based contraction model. *Journal of Molecular and Cellular Cardiology*, 45, 300–312. https://doi.org/10.1016/j.yjmcc.2008.04.012
- O'Hara, T., Virág, L., Varró, A., & Rudy, Y. (2011). Simulation of the undiseased human cardiac ventricular action potential: Model formulation and experimental validation. *PLoS Computational Biology*, 7, e1002061. https://doi.org/10.1371/journal.pcbi.1002061
- Oros, A., Beekman, J. D. M., & Vos, M. A. (2008). The canine model with chronic, complete atrio-ventricular block. *Pharmacology & Therapeutics*, 119, 168–178. https://doi.org/10.1016/j.pharmthera.2008.03.006
- Paci, M., Passini, E., Severi, S., Hyttinen, J., & Rodriguez, B. (2017). In silico modeling of human iPS cardiomyocytes: Effect of drugs and comparison to human adult cardiomyocytes. *Journal of Pharmacological and*

Toxicological Methods, 88, 240–241. https://doi.org/10.1016/j. vascn.2017.09.236

- Passini, E., Britton, O. J., Lu, H. R., Rohrbacher, J., Hermans, A. N., Gallacher, D. J., ... Rodriguez, B. (2017). Human in silico drug trials demonstrate higher accuracy than animal models in predicting clinical proarrhythmic cardiotoxicity. *Frontiers in Physiology*, 8, 1–15.
- Passini, E., Mincholé, A., Coppini, R., Cerbai, E., Rodriguez, B., Severi, S., & Bueno-Orovio, A. (2016). Mechanisms of pro-arrhythmic abnormalities in ventricular repolarisation and anti-arrhythmic therapies in human hypertrophic cardiomyopathy. *Journal of Molecular and Cellular Cardiol*ogy, 96, 72–81. https://doi.org/10.1016/j.yjmcc.2015.09.003
- Piacentino, V. 3rd, Weber, C. R., Chen, X., Weisser-Thomas, J., Margulies, K. B., Bers, D. M., & Houser, S. R. (2003). Cellular basis of abnormal calcium transients of failing human ventricular myocytes. *Circulation Research*, 92, 651–658. https://doi.org/10.1161/01.RES.0000062469.83985.9B
- Rodriguez, B., Carusi, A., Abi-Gerges, N., Ariga, R., Britton, O. J., Bub, G., ... Zhou, X. (2016). Human-based approaches to pharmacology and cardiology: An interdisciplinary and intersectorial workshop. *Europace*, 18, 1287–1298. https://doi.org/10.1093/europace/euv320
- Sager, P. T., Gintant, G., Turner, J. R., Pettit, S., & Stockbridge, N. (2014). Rechanneling the cardiac proarrhythmia safety paradigm: A meeting report from the Cardiac Safety Research Consortium. *American Heart Journal*, 167, 292–300. https://doi.org/10.1016/j.ahj.2013.11.004
- Sipido, K. R., Volders, P. G., de Groot, S. H., Verdonck, F., Van de Werf, F., Wellens, H. J., & Vos, M. A. (2000). Enhanced Ca(2+) release and Na/Ca exchange activity in hypertrophied canine ventricular myocytes: Potential link between contractile adaptation and arrhythmogenesis. *Circulation*, 102, 2137–2144. https://doi.org/10.1161/01.CIR.102.17.2137
- Stams, T. R. G., Bourgonje, V. J. A., Beekman, H. D. M., Schoenmakers, M., Van der Nagel, R., Oosterhoff, P., ... Vos, M. A. (2014). The electromechanical window is no better than QT prolongation to assess risk of Torsade de Pointes in the complete atrioventricular block model in dogs. *British Journal of Pharmacology*, 171, 714–722. https://doi.org/ 10.1111/bph.12483
- Stevens, J. L., & Baker, T. K. (2009). The future of drug safety testing: Expanding the view and narrowing the focus. *Drug Discovery Today*, 14, 162–167. https://doi.org/10.1016/j.drudis.2008.11.009

- Valentin, J. P., Bialecki, R., Ewart, L., Hammond, T., Leishmann, D., Lindgren, S., ... Wallis, R. (2009). A framework to assess the translation of safety pharmacology data to humans. *Journal of Pharmacological and Toxicological Methods*, 60, 152–158. https://doi.org/10.1016/j. vascn.2009.05.011
- Varshneya, M., Devenyi, R. A., & Sobie, E. A. (2018). Slow delayed rectifier current protects ventricular myocytes from arrhythmic dynamics across multiple species. *Circulation. Arrhythmia and electrophysiology*, 11, e006558.
- Volders, P. G. A., Sipido, K. R., Vos, M. A., Kulcsár, A., Verduyn, S. C., & Wellens, H. J. J. (1998). Cellular basis of biventricular hypertrophy and arrhythmogenesis in dogs with chronic complete atrioventricular block and acquired Torsade de Pointes. *Circulation*, 98, 1136–1147. https://doi.org/10.1161/01.CIR.98.11.1136
- Woosley, R., & Romer, K. (1999). www.Crediblemeds.org, QTdrugs List [Accessed 2018-11-30].
- Zahradni, I., Minarovic, I., Zahradni, A., Zahradnik, I., Minarovic, I., & Zahradniková, A. (2008). Inhibition of the cardiac L-type calcium channel current by antidepressant drugs. *Pharmacology and Experimental Therapeutics*, 324, 977–984.

### SUPPORTING INFORMATION

Additional supporting information may be found online in the Supporting Information section at the end of the article.

How to cite this article: Passini E, Trovato C, Morissette P, Sannajust F, Bueno-Orovio A, Rodriguez B. Drug-induced shortening of the electromechanical window is an effective biomarker for in silico prediction of clinical risk of arrhythmias. Br J Pharmacol. 2019;176:3819–3833. <u>https://doi.org/</u>10.1111/bph.14786