

# Comparison of imaging-based gross tumor volume and pathological volume determined by whole-mount serial sections in primary cervical cancer

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**Objective:** To investigate the accuracy of imaging-based gross tumor volume (GTV) compared with pathological volume in cervical cancer.

**Methods:** Ten patients with International Federation of Gynecology and Obstetrics stage I–II cervical cancer were eligible for investigation and underwent surgery in this study. Magnetic resonance imaging (MRI) and fluorine-18 fluorodeoxyglucose positron emission tomography (<sup>18</sup>F-FDG PET)/computed tomography (CT) scans were taken the day before surgery. The GTVs under MRI and <sup>18</sup>F-FDG PET/CT (GTV-MRI, GTV-PET, GTV-CT) were calculated automatically by Eclipse treatment-planning systems. Specimens of excised uterine cervix and cervical cancer were consecutively sliced and divided into whole-mount serial sections. The tumor border of hematoxylin and eosin-stained sections was outlined under a microscope by an experienced pathologist. GTV through pathological image (GTV-path) was calculated with Adobe Photoshop.

**Results:** The GTVs (average  $\pm$  standard deviation) delineated and calculated under CT, MRI, PET, and histopathological sections were  $19.41 \pm 11.96$  cm<sup>3</sup>,  $12.66 \pm 10.53$  cm<sup>3</sup>,  $11.07 \pm 9.44$  cm<sup>3</sup>, and  $10.79 \pm 8.71$  cm<sup>3</sup>, respectively. The volume of GTV-CT or GTV-MR was bigger than GTV-path, and the difference was statistically significant ( $P < 0.05$ ). No significant difference was observed between GTV-PET and GTV-path ( $P > 0.05$ ). Spearman correlation analysis showed that GTV-CT, GTV-MRI, and GTV-PET were significantly correlated with GTV-path ( $P < 0.01$ ). There was no significant difference in the lesion coverage factor among the three modalities.

**Conclusion:** The present study showed that GTV defined under 40% of maximum standardized uptake value in PET images was very similar to the pathological volume of cervical cancer. This result should be replicated in a larger number of patients with cervical cancer in a future study of ours.

**Keywords:** MRI, <sup>18</sup>F-FDG PET/CT, pathological tumor volume, gross tumor volume, cervical cancer

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## Introduction

In modern radiation oncology, treatment techniques have been improved from a two-dimensional to a three-dimensional approach, which requires the use of various imaging modalities to adequately identify and delineate tumor structures. The gross tumor volume (GTV) is the target volume to be irradiated and covered by the radical dose level. Accurate delineation of target volumes is essential for optimal

radiation treatment to get high-dose coverage for the tumor and maintain an acceptable dose to adjacent organs at risk. Computed tomography (CT) and magnetic resonance imaging (MRI) are widely available and have become the reference imaging modality for treatment planning. They have the significant advantage of showing the anatomy in high resolution, also called anatomical imaging.

In recent years, biological imaging methods visualizing metabolic characteristics have been developed. Fluorine-18 fluorodeoxyglucose positron emission tomography ( $^{18}\text{F}$ -FDG PET) is one of the most used methods, especially combined with anatomic imaging, such as CT ( $^{18}\text{F}$ -FDG PET/CT), which gives information on molecular and morphologic characteristics, and potentially provides the most accurate information for staging of many malignancies.<sup>1</sup>  $^{18}\text{F}$ -FDG PET/CT has been widely used in tumor diagnosis, staging, showing lymph-node metastasis, and radiotherapy.<sup>2-4</sup> The accuracy of  $^{18}\text{F}$ -FDG PET/CT in the diagnosis of gynecologic cancer (including cervical cancer) is higher than conventional imaging.<sup>3</sup> Recently, PET/CT has also shown a positive value in the detection and radiotherapy of recurrent cancer. GTV delineation in 56% of cases was significantly changed when information from metabolic imaging was used in the treatment-planning process.<sup>5</sup>

GTV confirmed by histopathological specimen should be the basis by which to identify the target of radiotherapy in different imaging methods. There is not much evidence about the best image modality to delineate targets of radiotherapy. The aim of the present study was to test the value of the images in delineating GTV of cervical cancer through comparing GTV from CT, MRI, and FDG PET with GTV calculated by histopathological specimen.

## Materials and methods

### Patients

From March 2010 to November 2010, ten patients with histologically proven cervical cancer at Xijing Hospital were enrolled in this study. All patients accepted preoperative imaging examination and underwent radical hysterectomy and pelvic lymphadenectomy. MRI and  $^{18}\text{F}$ -FDG PET/CT scans were done the day before surgery. The eligibility criteria were patients with International Federation of Gynecology and Obstetrics stage I–II, without diabetes, and no cancer-related treatment previously.

### Image acquisition

High-resolution MRI and  $^{18}\text{F}$ -FDG PET/CT examinations were performed the day before surgery in Xijing Hospital. All patients agreed to participate in this study. The protocol

was approved by the hospital's Protection of Human Subjects Committee (Xijing Hospital, Fourth Military Medical University, Clinical Ethics Committee).

### Magnetic resonance imaging

The MR images were acquired with a 3-T MR scanner (Tim Trio; Siemens, Erlangen, Germany). The patients were asked to empty their intestines before the MRI scan and were scanned in a supine position. The high-resolution anatomic MR images were acquired by using a 3-D fast field-echo sequence with the following parameters: matrix size of  $512 \times 512$ , field of view of  $20 \times 20 \text{ cm}^2$  and slice thickness of 4 mm, no gap between slices. The repetition time/echo time was 10,050 ms/95 ms for axial turbo spin-echo  $T_1$ -weighted and 6000 ms/102 ms for axial, coronal, sagittal turbo spin-echo  $T_2$ -weighted images.

### Fluorodeoxyglucose positron emission tomography/computed tomography

$^{18}\text{F}$ -FDG PET/CT scans were performed using a hybrid PET System (Biograph 40; Siemens, Malvern, PA, USA). All patients were asked to fast for at least 6 hours before the examination and normal blood glucose level was tested before tracer injection. After intravenous injection of 5.55–7.40 MBq/kg of  $^{18}\text{F}$ -FDG, emission images were acquired. High-quality CT images were provided, with a slice thickness of 3 mm, a 50 cm displayed field of view, and a rotational speed of 0.75 seconds per rotation. The patients were in a supine position and scanned from L3 to ischial tuberosity.

### Gross tumor volume

To avoid bias, two experienced radiation oncologists and one radiologist took part in the GTV delineation of all patients. Acquired images of MRI and PET/CT for each patient were transferred to Eclipse treatment-planning systems, version 8 (Varian Medical Systems, Palo Alto, CA, USA), and the GTVs were calculated automatically after the tumor border outlined on each floor of MR and PET/CT images. MRI-based GTV (GTV-MRI) was determined from  $T_2$ -weighted images, and  $T_1$ -weighted images were used as reference. The GTV on the PET images (GTV-PET) was shown by using an isointensity line based upon 40% of the maximum standardized uptake value, based on a previous study.<sup>6</sup> The GTV on CT image (GTV-CT) was outlined on 400 HU window width and 60 HU window level.

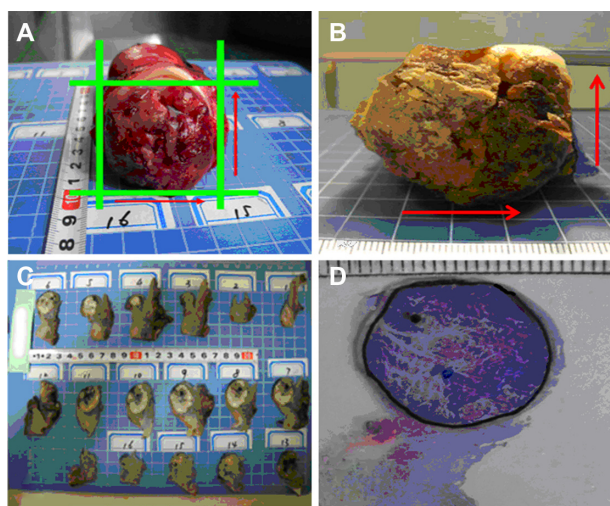
### Pathology procedure

All the patients underwent radical hysterectomy and pelvic lymphadenectomy the next day after MRI and PET/CT

image examinations. Once the fresh specimen was collected after the operation, the maximum tumor diameters vertically and horizontally were documented by digital photography with a ruler (Figure 1A). The specimens were subsequently fixed in 10% formalin for at least 24 hours. The dimensions of the fixed tumor samples were also documented in the same way to determine the volume reduction due to fixation (Figure 1B). Then the fixed tumor specimens were sliced into consecutive tissue sections with intervals of 4 mm, so-called thick slices (Figure 1C). Each thick slice was numbered and photographed using a digital camera. After conventional pathological processing, the 4 mm-thick slices were embedded in paraffin and sliced into 4  $\mu$ m sections on a microtome (Microm HM 450; GMI, Ramsey, MN, USA) and stained with hematoxylin and eosin (Figure 1D). The tumor-containing area on the 4  $\mu$ m hematoxylin and eosin-stained section was outlined under light microscopy at 20 $\times$  magnification, reviewed and confirmed at 100 $\times$  magnification by an experienced pathologist. The outlined section was then photographed and saved. With Photoshop 7.01 (Adobe Systems, San Jose, CA, USA), the tumor-containing area ( $A_i$ ) for each slide was measured, and the GTV on pathology (GTV-path) for each specimen was calculated as  $GTV\text{-path} = \sum A_i/R$ , where R was defined as the ratio of the sample dimensions before and after fixation, respectively. The workflow of the processes to acquire all the imaging is briefly schematized in Figure 2.

## Volume analysis

Data of the different volumes – GTV-CT, GTV-MRI, GTV-PET, and GTV-path – were expressed as means  $\pm$  standard deviation.



**Figure 1 (A–D)** Pathology procedure. The specimens are collected from surgery (A) and fixed in 10% formalin (B). The fixed specimens are sliced in 4 mm-thick consecutive transverse slices (C). Each slice is embedded in paraffin, sectioned, and processed for hematoxylin and eosin staining (D).

The differences between GTV-CT, GTV-MRI, and GTV-PET with GTV-path were analyzed using paired *t*-test with SPSS software (version 15.0; IBM, Armonk, NY, USA). The correlation between different imaging volumes and pathological volume were also analyzed by the Spearman correlation test. A *P*-value of  $<0.05$  was considered statistically significant. The conformity index (CI) and lesion-coverage factor (LCF) were used to compare the correspondence among GTV-CT, GTV-MRI, and GTV-PET.<sup>7</sup> The CI means the relative concordance between the two different modalities, which was defined as  $GTV\text{-A}/GTV\text{-B}$ . The LCF means the percentage of overlap between the two different modalities, which was defined as overlap between GTV-A and GTV-B divided by GTV-A.

## Results

### Patient characteristics

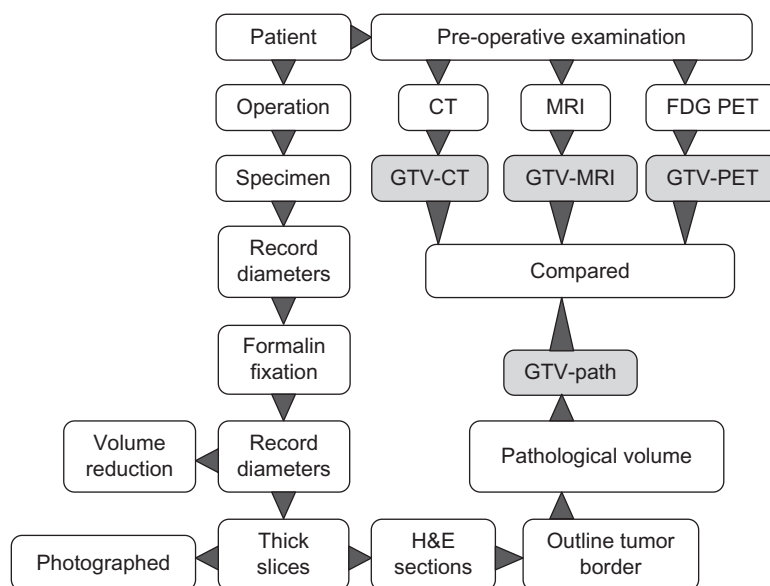
All ten patients were from northwest China, confirmed with squamous cell carcinoma after operation, and had no lymph-node metastasis or obviously parametrical violation. The median age of the patients was 40 years (range 32–55 years). Clinical stages (International Federation of Gynecology and Obstetrics) were two IB, three IIA, and five IIB. On FDG PET images, significantly abnormal radioactive uptake in tumor (standardized uptake value  $>2.5$ ) was found on all patients. No patient showed abnormal lymph nodes in the pelvic cavity.

### Gross tumor volume

GTV-path was indicated with a reduction to  $85\% \pm 10\%$  of the original tumor volumes (range 65%–97%) by comparing the tumor samples before (Figure 1A) and after (Figure 1B) formalin fixation (Table 1). There was no further volume shrinkage and changes in tissue shape during subsequent pathological procedures.

The tumor volumes of each case are shown in Table 1. The averages of GTV-CT, GTV-MRI, and GTV-PET were  $19.41 \pm 11.96 \text{ cm}^3$ ,  $12.66 \pm 10.53 \text{ cm}^3$ , and  $11.07 \pm 9.44 \text{ cm}^3$ , respectively. The actual pathological volume of tumors was  $10.79 \pm 8.71 \text{ cm}^3$  on average. One case example of CT, MRI, FDG PET imaging, and surgical pathological specimen is representatively shown in Figure 3.

Paired *t*-test results showed that the differences between GTV-CT, GTV-MRI, and GTV-path were statistically significant ( $P = 0.001$ ,  $P = 0.019$ ). GTV-CT and GTV-MRI were both bigger than GTV-path, but GTV-MRI was much closer to the actual pathologic volume. GTV-MRI was larger than GTV-path by approximately 17.3%, and GTV-CT was larger than GTV-path by close to two times.



**Figure 2** Workflow of image acquisition and pathological procedure.

**Abbreviations:** CT, computed tomography; MRI, magnetic resonance imaging; FDG-PET, fluorodeoxyglucose positron emission tomography; GTV-path, gross tumor volume through pathological image; H&E, hematoxylin and eosin.

There was no statistical difference between GTV-PET and GTV-path ( $P = 0.512$ ), even though the GTV-PET was bigger than the actual pathologic volume. Furthermore, comparing the GTV-MRI and GTV-PET, a significant difference ( $P = 0.048$ ) was observed. GTV-PET was much smaller than GTV-MR and closer to GTV-path.

## Spearman correlation analysis

Spearman correlation analysis showed that GTV-CT, GTV-MRI, and GTV-PET were significantly correlated with

GTV-path ( $r = 0.8545$ ,  $P = 0.0029$ ;  $r = 0.9879$ ,  $P < 0.0001$ ;  $r = 0.9879$ ,  $P < 0.0001$ ; Figure 4A–C).

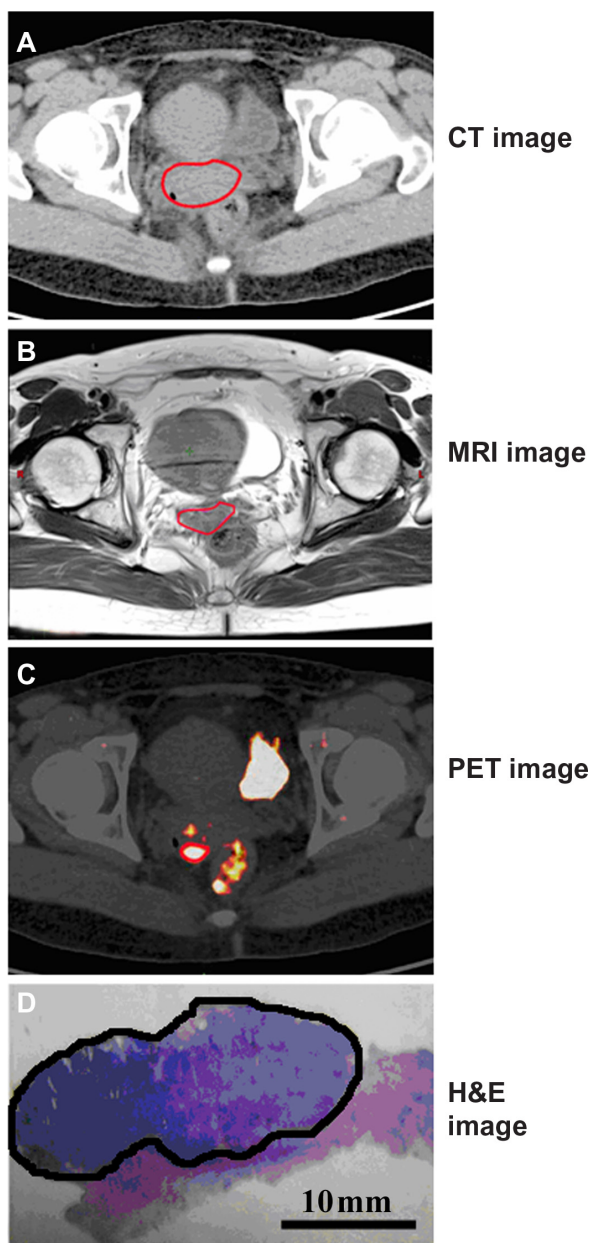
GTV-MRI was used as a reference in the CI and LCF volume relative concordance analysis, because GTV-MRI is most widely used in brachytherapy planning of cervical cancer. The CI and LCF for comparisons between GTV-CT, GTV-PET, and GTV-MRI are shown in Table 2. The average CI and LCF for GTV-CT versus GTV-MRI were  $2.18 \pm 1.25$  and  $0.63 \pm 0.20$ , and the average CI and LCF for GTV-PET versus GTV-MRI were  $0.86 \pm 0.12$  and  $0.75 \pm 0.09$ , respectively.

**Table 1** Summary on GTVs in patients with cervical cancer for each case

Case	Volume retraction (%)	GTV-path (cm <sup>3</sup> )	Actual GTV-path (cm <sup>3</sup> )*	GTV imaging (cm <sup>3</sup> )		
				CT	MRI	PET
1	88	1.04	1.18	5.76	1.5	1.34
2	95	1.76	1.85	10.94	2.7	2.01
3	78	3.64	4.67	18.13	4.95	3.92
4	97	4.34	4.47	15.92	5.72	3.98
5	65	4.89	7.52	7.64	7.81	7.89
6	72	6.80	9.44	12.35	9.28	9.59
7	86	12.13	14.10	18.47	16.4	14.25
8	87	13.42	15.43	27.89	18.84	15.39
9	90	20.84	23.15	42.04	29.32	22.46
10	92	24.04	26.13	34.99	30.03	29.88
Mean			10.79	19.41	12.66	11.07
SD			8.71	11.96	10.53	9.44
<i>P</i> value vs GTV-path				0.001	0.019	0.512

**Note:** \*Actual GTV-path calculated as GTV-path divided by the volume-retraction ratio.

**Abbreviations:** GTV-path, gross tumor volume through pathological image; CT, computed tomography; MRI, magnetic resonance imaging; PET, positron emission tomography; SD, standard deviation.



**Figure 3 (A–D)** One representative case (case 4) on CT image, MRI, PET image, and H&E image of surgical pathological specimen of cervical cancer. The tumor border is delineated by the red lines on CT (A), MRI (B), and PET (C), and by the black line on whole-mount section of tumor (D).

**Abbreviations:** CT, computed tomography; MRI, magnetic resonance imaging; PET, positron emission tomography; H&E, hematoxylin and eosin.

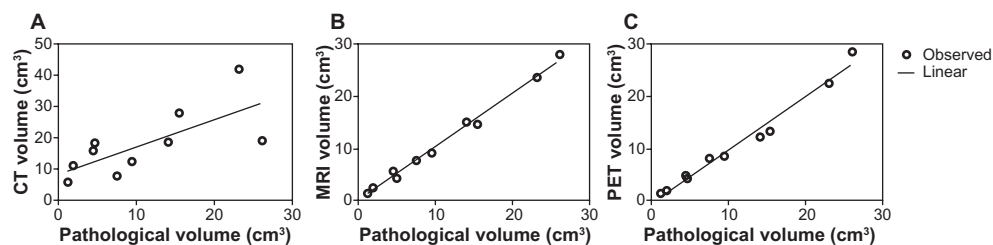
According to the differential prognosis described in previous research,<sup>8</sup> tumor size was divided into a  $<14\text{ cm}^3$  group and a  $>14\text{ cm}^3$  group based on MRI to be further analyzed. For GTV-CT and GTV-MRI, when the  $<14\text{ cm}^3$  group (average GTV-MRI  $5.33 \pm 2.95\text{ cm}^3$ ), the CI was  $2.77 \pm 1.33$  and LCF was  $0.68 \pm 0.15$ , while the CI fell to  $1.30 \pm 1.33$  and LCF to  $0.55 \pm 0.25$  in the  $>14\text{ cm}^3$  group. The result of *t*-tests showed a significant difference for CI ( $P=0.0027$ ); there was no significant difference for LCF ( $P=0.45$ ), between the two cohorts.

For GTV-PET and GTV-MRI, a mean CI of  $0.86 \pm 0.14$  and LCF of  $0.74 \pm 0.09$  was found in the  $<14\text{ cm}^3$  group, while a mean CI of  $0.87 \pm 0.10$  and LCF of  $0.76 \pm 0.10$  was found in the  $>14\text{ cm}^3$  group. The CI and LCF differences between cohorts were not statistically significant ( $P=0.34$  and  $0.67$ , respectively).

## Discussion

Image-guided radiotherapy requires adequate knowledge of tumor extent so it can deliver a high and accurate radiation dose to the targets.<sup>9</sup> CT and MRI are widely used in GTV delineation for tumor radiation-therapy treatment planning to improve the accuracy of radiotherapy.

A number of publications from the American College of Radiology Imaging Network and the Gynecologic Oncology Group have demonstrated that traditional  $T_1/T_2$ -weighted MRI is superior to CT for tumor delineation in cervical cancer, due to its high soft-tissue contrast for the evaluation of local tumor extension.<sup>10</sup> In stage IIB cervical cancer, MRI had 91% diagnostic accuracy, 67% sensitivity, and 92% specificity in assessing infiltration of the vaginal fornices, and 89% diagnostic accuracy, 28% sensitivity, and 100% specificity in the assessment of the lymph nodes, with a cutoff value of 1 cm.<sup>11</sup> However, both CT and MRI cannot show the primary tumor's metabolic characteristics, while FDG PET can provide information concerning the metabolic activity of a tissue region. Clinical results show that FDG PET seems to be particularly valuable in target-volume definition and lymph-node status definition for lung, head-and-neck, genitourinary,



**Figure 4 (A–C)** Correlation of the different gross tumor volumes among imaging modalities and the surgical specimen. (A) CT; (B) MRI; (C) PET.

**Abbreviations:** CT, computed tomography; MRI, magnetic resonance imaging; PET, positron emission tomography.

**Table 2** Relative concordance among GTV-CT, -MRI, and -PET

Case	GTV-CT vs GTV-MRI		GTV-PET vs GTV-MRI	
	Conformity index	Lesion coverage factor	Conformity index	Lesion coverage factor
1	3.84	0.74	0.89	0.77
2	4.05	0.67	0.74	0.86
3	3.66	0.82	0.79	0.68
4	2.78	0.54	0.70	0.60
5	0.98	0.46	1.01	0.71
6	1.33	0.84	1.03	0.80
7	1.12	0.32	0.87	0.75
8	1.48	0.85	0.82	0.83
9	1.43	0.37	0.77	0.62
10	1.17	0.65	1.00	0.84

**Abbreviations:** GTV, gross tumor volume; CT, computed tomography; MRI, magnetic resonance imaging; PET, positron emission tomography.

and brain tumors and cervical cancer. Prior publications have highlighted the utility of FDG PET/CT simulation in defining nodal target areas and assessing posttreatment response.<sup>12</sup> It may become possible to improve tumor delineation further by depiction of the metabolic activity of the tumor.

However, neither CT and MRI can show the primary tumor's metabolic characteristics, while FDG PET can provide information concerning the metabolic activity of a tissue region. Clinical studies' results of the integration of PET in target-volume definition for lung, head-and-neck, genitourinary, and brain tumors were analyzed, and FDG PET seems to be particularly valuable in lymph-node status definition in cervical cancer. The authors proposed that PET showed advantages in terms of tumor delineation and the description of biological processes when doing treatment planning in radiotherapy.<sup>12</sup> It can be assumed that with depiction of the metabolic activity of the tumor, further improvement in tumor delineation may become possible. Prior publications have highlighted the utility of FDG PET/CT simulation in defining nodal target areas and assessing posttreatment response.<sup>12</sup>

It is generally accepted that the volume of surgical specimens is the gold standard for target-delineating studies. The whole-mount serial section technique was used in 3-D volumetric reconstruction in malignant tumors, including breast cancer, lung cancer, and laryngeal cancer.<sup>13-15</sup> Whole-mount serial section could offer advantages in correct documentation of tumor size, lesion distribution, disease extent, and surgical margins, and facilitate better understanding of the complex morphology of tumors. Large histopathology slides are optimal tools for confirming the correlations between radiology and pathology. In this study, we first used the whole-mount serial sections technique to reconstruct the cervical cancer pathological volume.

Recently, different imaging modalities have been introduced to delineate and calculate GTV for cervical cancer. Dahele et al compared the discrepancies of tumor volume between FDG PET and MRI for cervical cancer. They found that MRI provided better visualization of larger tumors than smaller tumors in reference to FDG PET/CT. Also, FDG PET/CT visualized tumor volumes differently from  $T_2$ -weighted MRI, especially in tumors <14 cc.<sup>15</sup>

In the present study, we demonstrated the feasibility of pathology-validated target definition for cervical cancer. The results from the ten patients indicated that current target volumes based on CT, MRI, and PET data overestimate the real tumor volume. We found that GTV-CT and GTV-MRI overestimated GTV-PET volume in all ten patients, which is in agreement with the results from Dahele et al's study.<sup>15</sup>

A major difference between our outcomes and those of Dahele et al's study is that we were able to compare pathological volumes by 3-D reconstruction rather than areas or maximal tumor diameters. By comparing with GTV-path, we found that PET-based GTVs were the most accurate method in the three imaging modalities for radiation-treatment planning. The other difference was that there was no significant difference between FDG PET visualized tumor volumes from MRI in our study, whenever the tumor volume was <14 cm<sup>3</sup> or >14 cm<sup>3</sup>. Similar to Dahele et al's study, no significant difference in CI was observed in the two different tumor-volume subgroups. However, Dahele et al found that differences in LCF of tumor volume were statistically significant ( $P < 0001$ ) between FDG PET and MRI, especially for tumors <14 cm<sup>3</sup>, which meant that the tumor location was varying particularly for small tumor volumes. No significant difference in CI or LCF between FDG PET and MRI was shown in our research. A high level of LCF represented a high degree of overlap between the GTV-FDG PET and GTV-MRI despite the small tumor volume.

There are few studies on the comparison tumor volumes from different imaging modalities with those of surgical specimens. For oropharyngeal tumors, laryngeal, or hypopharyngeal tumors, Daisne et al found that the average GTVs delineated by CT or MRI showed no significant difference, whereas GTVs determined by FDG PET most accurately matched the pathologic volumes by 3-D reconstruction in pharyngolaryngeal squamous cell tumors. However, no approach could adequately depict superficial tumor extension, due to the lower spatial resolution when the surgical specimen was available.<sup>16,17</sup>

A major finding of our study is that the GTVs delineated by FDG PET were closest to the reference volume assessed from the surgical specimens, which could have tremendous implications for radiation-therapy treatment planning in

patients with cervical squamous cell carcinoma. In addition, compared to the actual volume of the tumor, the CT-derived tumor volumes had a bigger deviation than those from MRI or FDG PET. However, the delineated tumor volumes had a relatively good degree of overlap among the three modalities. The higher deviation of CT-derived tumors would be related to the CT scan without contrast. GTV-CT would include some normal tissue of the cervix.

To the best of our knowledge, the present study is the only research on comparing volume from different imaging modalities with that of the corresponding surgical specimens in cervical cancer. The limitations of the study were the small number of cases and singleness of pathological kind. In future, more patients with other histopathological types will be enrolled to verify the results of the study. Another limitation was the failure to overlap the volumes from imaging and pathology stereotactically, because of the lack of reliable markers in pathological sections. Although there were a few limitations, certain insights have been derived in the delineation of target volumes using PET/CT images for radiation therapy.

## Conclusion

In conclusion, the present study has demonstrated a potential role of FDG PET imaging for the delineation of GTV in squamous cell carcinoma of cervical cancer. Research in a larger number of patients with cervical cancer will need to be performed to prove the relationship between GTV-PET and GTV-path in the near future.

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## Disclosure

The authors report no conflicts of interest in this work.

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