



Running humans attain optimal elastic bounce in their teens

Mario A. Legramandi¹, Bénédicte Schepens² & Giovanni A. Cavagna¹

SUBJECT AREAS:
PHYSIOLOGY
AGEING
BIOENERGETICS
SKELETAL MUSCLE

¹Section of Human Physiology, Department of Pathophysiology and Transplantation (DePT), University of Milan, 20133 Milan, Italy, ²Institute of Neuroscience, Laboratoire de physiologie et biomécanique de la locomotion, Université catholique de Louvain, 1348 Louvain-la-Neuve, Belgium.

Received
16 November 2012
Accepted
4 February 2013
Published
19 February 2013

In an ideal elastic bounce of the body, the time during which mechanical energy is released during the push equals the time during which mechanical energy is absorbed during the brake, and the maximal upward velocity attained by the center of mass equals the maximal downward velocity. Deviations from this ideal model, prolonged push duration and lower upward velocity, have found to be greater in older than in younger adult humans. However it is not known how similarity to the elastic bounce changes during growth and whether an optimal elastic bounce is attained at some age. Here we show that similarity with the elastic bounce is minimal at 2 years and increases with age attaining a maximum at 13–16 years, concomitant with a mirror sixfold decrease of the impact deceleration peak following collision of the foot with the ground. These trends slowly reverse during the course of the lifespan.

Correspondence and requests for materials should be addressed to G.A.C. (giovanni.cavagna@unimi.it)

Indirect evidence that energy is partly conserved in human running thanks to an elastic bounce of the body is provided by an efficiency of positive work production twice that attained by a contracting muscle^{1,2}. The elasticity of the bounce can also be directly deduced by considering the mechanical energy changes of the center of mass of the body after landing and before takeoff^{3,4}. In bouncing gaits such as running, hopping and trotting mechanical energy is absorbed each step by muscle-tendon units when the body decelerates during the brake and restored when the body reaccelerates during the push. In this stretch-shorten cycle of muscle-tendon units, some energy is stored elastically during stretching and recovered during shortening. In adult running elastic energy storage and recovery is greater the greater the length change of tendon relative to that of muscle. This is because adult tendon has a very small elastic hysteresis^{5,6}, i.e. the force exerted during shortening is only slightly less than during stretching. Muscle's stretch-shorten cycle on the contrary exhibits a large hysteresis, i.e. a large energy loss, because it exerts a force during stretching F_{str} , which may largely exceed that during shortening F_{sho} . The relative role of muscle vs tendon involvement during the bounce can be deduced considering that during running on the level at a constant speed the momentum lost during the brake $F_{str} t_{brake}$ equals the momentum gained during the push $F_{sho} t_{push}$, and since $F_{str} > F_{sho}$ in contracting muscle then $t_{brake} < t_{push}$ when muscle instead of tendon lengthens and shortens. The ratio between time intervals during which negative and positive work are done t_{brake}/t_{push} would approach unity in an ideally elastic bounce sustained uniquely by tendon (where $F_{str} \sim F_{sho}$). The asymmetric response of muscle to lengthening and shortening also explains the difference between maximal downward velocity $V_{v,mx,down}$ (higher) and upward velocity $V_{v,mx,up}$ (lower) attained by the center of mass during the bounce. In fact, a higher $V_{v,mx,down}$ can be passively attained during the fall thanks to gravity relying, for the downward deceleration, on the greater force the muscle is able to afford when lengthening during the subsequent negative work phase (brake). On the contrary, a lower maximal upward velocity $V_{v,mx,up}$ is actively attained against gravity by muscular contraction during the positive work phase (push) when the muscle is shortening and is capable of a lower force. This explains why, when muscle operates instead of tendon, $V_{v,mx,up} < V_{v,mx,down}$. Therefore, t_{brake}/t_{push} and $V_{v,mx,up}/V_{v,mx,down}$ are greater the more the kinetics and the kinematics of the bounce approach those of an ideal elastic body. Both ratios increase with the active muscle contraction that prevents muscle lengthening and thus favors tendon lengthening. In fact: i) t_{brake}/t_{push} is lower at low running speed, when muscle activation is lower, whereas $t_{brake} \sim t_{push}$ at high speeds, when muscle activation is higher³; ii) t_{brake}/t_{push} is lower in old humans than in young adult humans associated with a lower force attained during the bounce by the elderly^{4,7}.

It is not known how the running bounce differs from that of an ideal elastic body during growth. In this study we measured t_{brake} , t_{push} , $V_{v,mx,up}$, $V_{v,mx,down}$ and the vertical acceleration of the center of mass of the body a_v during running steps in nine age groups with mean ages ranging between 2.6 and 27.7 years.



Results

Indicative records obtained on two subjects 2.5 years and 15.8 years old, where the difference in results between ages is largest, are shown in Fig. 1. In the younger subject:

- 1) $t_{\text{brake}}/t_{\text{push}}$ is lower mainly due to a shorter duration of the brake consequent to a sharper decrease of the total mechanical energy of the center of mass E_{tot} following the aerial phase t_a .
- 2) The peak in kinetic energy of vertical motion $E_{\text{kv}} = 0.5 M_b V_v^2$ (where M_b is the mass of the body and V_v is the vertical velocity of the center of mass of the body) is lower during the lift than during the fall, indicating a lower ratio $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$.
- 3) The impact deceleration peak following landing $a_{v,\text{impact}}$ is much greater than in the older subject, whereas the subsequent 'active' peak, roughly simultaneous with the minimum of E_{tot} and E_p , is similar to that of the older subject⁸.

Average values of $t_{\text{brake}}/t_{\text{push}}$, $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$ and $a_{v,\text{impact}}$ measured in the nine age groups of the present study are given in Table 1 and plotted as a function of age in Fig. 2. The three last rows in Table 1 (indicated by asterisks) and the open symbols in Fig. 2 refer to $t_{\text{brake}}/t_{\text{push}}$ and $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$ data obtained in two previous studies^{3,4} in the same speed range. It can be seen that during growth both $t_{\text{brake}}/t_{\text{push}}$ and $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$ increase to a maximum at

13–16 years whereas $a_{v,\text{impact}}$ decreases to a minimum at about the same age. The maximal deceleration downward $a_{v,\text{impact}}$ following collision of the foot with the ground is, on average, ~ 6 times greater in the 2 years group than in the 16 years group (Table 1). Subsequently the ratios $t_{\text{brake}}/t_{\text{push}}$ and $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$, which would attain unity in an elastic bounce, decrease and $a_{v,\text{impact}}$ increases.

Discussion

The mirroring opposite trend of the $a_{v,\text{impact}}$ curve with the $t_{\text{brake}}/t_{\text{push}}$ and $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$ curves in Fig. 2 strongly suggests that the impact peak is a relevant factor impeding an elastic bounce. This is reasonable because some of the mechanical energy absorbed and released by the heel pad and other structures during the impact phase⁹ is lost prior the beginning of the push, thus decreasing the mechanical energy at disposal for the subsequent positive work phase. The fall in E_{tot} during t_{brake} represents the total amount of energy that can possibly be stored elastically. In the example of Fig. 1, the impact duration occupies $\sim 45\%$ of the total fall in E_{tot} in the 2.5 years old subject and $\sim 24\%$ in the 15.8 years old subject. It follows that relatively less mechanical energy is left after the impact phase to be stored in muscle-tendon units of the younger subject during the fall in E_{tot} . The mechanical energy lost during the impact phase must be replaced by muscular contraction during the following positive work phase resulting, as described above, in an increased duration of t_{push} and in a decrease of $V_{v,\text{mx,up}}$, i.e. in a less elastic bounce and a greater energy expenditure. In fact, measurements made in a previous study² show that the efficiency of positive work production during running below 11 km h^{-1} is lower in 4.5 years old children than in 21.6 years adults (0.405 ± 0.046 (s.d.), $N = 46$ vs. 0.426 ± 0.036 (s.d.), $N = 67$, $P = 0.014$).

This study draws attention to two points: i) the youngest subjects are more exposed to high-impact collisions, and ii) the impact peak and the similarity to an elastic bounce change during growth.

The first point has practical health implications. It is known that high-impact collision forces are likely to be associated with injuries of the muscular-skeleton system^{10–12}. The present finding, that the impact peak during running is elevated in the youngest subjects requires particular attention.

With regard to the second point it is relevant to consider that the mass-specific vertical stiffness of the running bounce k/M_b decreases during growth to a minimum in the 16 years group to increase again in the 28 years group⁸ with the same trend of the impact peak found in the present study. In other words, the step frequency is higher in the youngest, due to the lower dimensions of their body, requires a higher mass-specific vertical stiffness, to cope with the natural frequency of the bouncing system⁸, and this, in turn, causes a higher impact peak and a lower similarity to an elastic bounce. Interestingly, an inverse relationship between k/M_b and similarity to an elastic bounce was also found when comparing running, trotting and hopping animals of different size¹³. In adult humans, the height of the impact peak increases with the effective foot mass M_{eff} , i.e. with the proportion of the body mass M_b stopping abruptly at touch-down^{9,14}. We do not know studies describing changes of the ratio M_{eff}/M_b during growth: this requires further experiments. However, it is worth noting since now that the optimal similarity to an elastic bounce is attained in the 16 years group thanks to an increase in M_b not compensated by an increase in k (ref. 8), resulting in a more compliant system, and it is abandoned in the 28 years group because of an increase in k not compensated by the increase in M_b , resulting in a stiffer system. This suggests that the completion of neuro-muscular maturation¹⁵ associated with greater tendon compliance¹⁶ attains in the teens an ideal condition that is no longer tenable at an older age.

It remains to be explained why a stiffer system results in a less elastic bounce and if this condition is necessarily caused, in animals

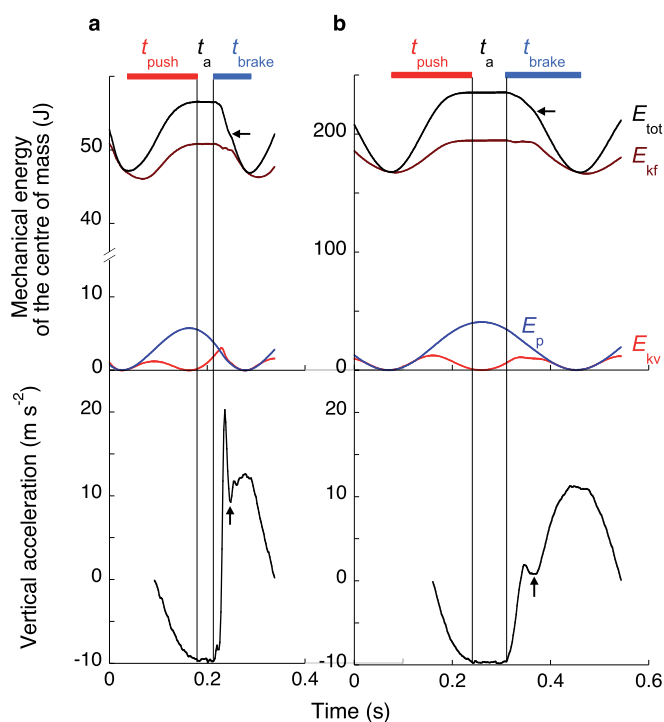


Figure 1 | Mechanical energy and vertical acceleration of the center of mass of the body in one running step of two subjects with lowest and highest similarity to an elastic bounce. (a), 2.5 years, 16.8 kg, 8.8 km h^{-1} ; (b), 15.8 years, 50.7 kg, 9.4 km h^{-1} . E_p is the gravitational potential energy, E_{kv} and E_{kf} are the kinetic energies of vertical and forward motion, respectively, and $E_{\text{tot}} = E_p + E_{\text{kv}} + E_{\text{kf}}$ is the total mechanical energy of the center of mass in a sagittal plane. Horizontal bars indicate push duration (t_{push} , time interval during which E_{tot} increases, red) and brake duration (t_{brake} , time interval during which E_{tot} decreases, blue) separated by the aerial phase t_a . After the aerial phase, E_{tot} decreases sharply in the younger subject resulting in a relatively shorter t_{brake} and higher peak of E_{kv} with a greater vertical deceleration following impact of the foot on the ground. Arrows show that the fraction of E_{tot} lost during the impact peak, and not available to be stored as elastic energy before the beginning of the push, is relatively greater in the younger subject.



Table 1 | Similarity to elastic bounce and impact peak at different ages are confronted with those at ~16 yr

Age (yr)	N (male/female)	Mass (kg)	N runs	$t_{\text{brake}}/t_{\text{push}}$	$t_{\text{brake}}/t_{\text{push}}$	$t_{\text{brake}}/t_{\text{push}}$ vs. 16 yr P	$V_{v,\text{max,up/down}}$	$V_{v,\text{max,up/down}}$ vs. 16 yr P	$\alpha_{v,\text{impact}}$ (m s^{-2})	$\alpha_{v,\text{impact}}$ (m s^{-2}) vs. 16 yr P
2.6 ± 0.3	6 (3/3)	13.9 ± 1.6	45	0.58 ± 0.10	0.58 ± 0.10	$5.27 \cdot 10^{-22}$	0.76 ± 0.08	$1.73 \cdot 10^{-20}$	16.09 ± 5.89	$5.34 \cdot 10^{-27}$
4.2 ± 0.4	7 (4/3)	17.6 ± 1.6	85	0.72 ± 0.12	0.72 ± 0.12	$8.81 \cdot 10^{-10}$	0.84 ± 0.10	$1.34 \cdot 10^{-13}$	9.30 ± 6.78	$1.20 \cdot 10^{-16}$
6.1 ± 0.3	6 (3/3)	20.7 ± 1.5	83	0.75 ± 0.09	0.75 ± 0.09	$5.16 \cdot 10^{-7}$	0.88 ± 0.07	$5.06 \cdot 10^{-9}$	6.76 ± 4.70	$3.95 \cdot 10^{-12}$
8.1 ± 0.7	6 (3/3)	26.3 ± 2.8	78	0.77 ± 0.08	0.77 ± 0.08	$3.24 \cdot 10^{-5}$	0.91 ± 0.07	0.001	5.49 ± 3.19	$6.57 \cdot 10^{-11}$
10.0 ± 0.5	6 (4/2)	30.2 ± 2.3	72	0.70 ± 0.10	0.70 ± 0.10	$2.31 \cdot 10^{-13}$	0.90 ± 0.08	$1.77 \cdot 10^{-4}$	6.85 ± 4.13	$5.02 \cdot 10^{-14}$
11.4 ± 0.2	6 (1/5)	35.7 ± 2.8	78	0.78 ± 0.07	0.78 ± 0.07	0.002	0.93 ± 0.06	0.087	5.70 ± 3.83	$2.81 \cdot 10^{-8}$
13.5 ± 0.3	6 (3/3)	48.2 ± 8.1	95	0.81 ± 0.11	0.81 ± 0.11	0.464	0.96 ± 0.08	0.257	3.69 ± 2.67	0.008
16.1 ± 0.4	6 (3/3)	57.3 ± 9.4	93	0.82 ± 0.10	0.82 ± 0.10	1	0.94 ± 0.07	1	2.70 ± 1.74	1
27.7 ± 2.5	6 (3/3)	63.8 ± 7.2	107	0.80 ± 0.07	0.80 ± 0.07	0.020	0.92 ± 0.04	0.003	3.81 ± 2.07	$4.41 \cdot 10^{-4}$
20.9 ± 1.4*	8 (6/2)	63.5 ± 8.5	120	0.84 ± 0.08	0.84 ± 0.08	0.343	0.92 ± 0.07	0.029	—	—
39.1 ± 4.7**	4 (3/1)	68.2 ± 9.7	61	0.80 ± 0.08	0.80 ± 0.08	0.160	0.89 ± 0.05	$1.76 \cdot 10^{-8}$	—	—
73.4 ± 5.3*	8 (8/0)	71.9 ± 8.6	75	0.80 ± 0.08	0.80 ± 0.08	0.072	0.87 ± 0.07	$3.02 \cdot 10^{-10}$	—	—

Data shown as mean ± s.d. t_{brake} and t_{push} are the durations of the negative and of the positive work done to decrease and increase the mechanical energy of the center of mass of the body during the running bounce. $t_{\text{brake}}/t_{\text{push}}$ attains unity in an elastic bounce. $V_{v,\text{mx,up}}$ and $V_{v,\text{mx,down}}$ are the maximal vertical velocities obtained by the center of mass in upward and downward directions. $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$ attains unity in an elastic bounce. $\alpha_{v,\text{impact}}$ is the vertical deceleration peak attained after collision of the foot with the ground. The values of P refer to a two-tailed F-test assuming unequal variances, alpha = 0.05 (Microsoft Excel for Mac version 11.6.6). *data from ref. 4; **data from ref. 3. Average speed of all the runs was $6.8 \pm 2.5 \text{ km h}^{-1}$ (n = 992).

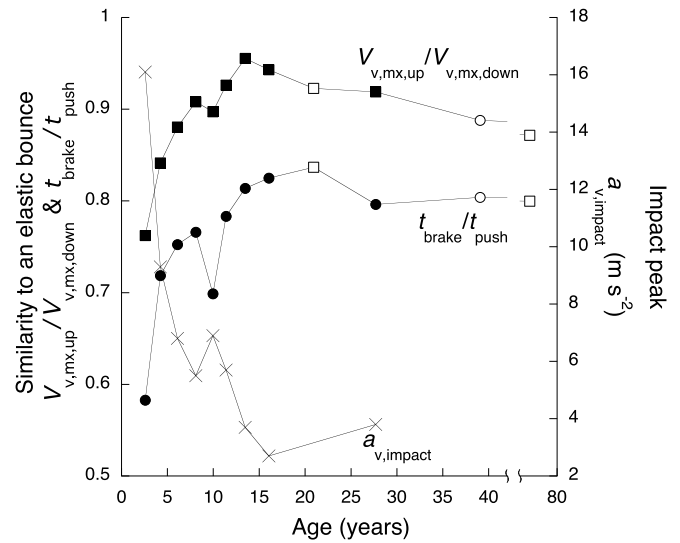


Figure 2 | Effect of age on the similarity to an elastic bounce and on the deceleration peak following impact of the foot on the ground. The similarity to an elastic bounce, which is greater the higher the ratios $t_{\text{brake}}/t_{\text{push}}$ and $V_{v,\text{mx,up}}/V_{v,\text{mx,down}}$, increases during growth, attains a maximum in the teens and subsequently decreases. This trend is mirrored by an opposite trend of the impact peak following collision of the foot on the ground after the aerial phase. Symbols are average values (Table 1) measured in the present study (filled squares, circles and crosses) and in two previous studies (open squares⁴ and circles³).

as in humans, by a greater impact peak following collision with the ground. In addition, do we really know that a greater kinematic and kinetic similarity of the bounce with that of an ideal elastic body translates into a more efficient run? Not necessarily, but experimental data show that in human running: i) the efficiency is greater at high speeds^{1,2} when $t_{\text{brake}} \sim t_{\text{push}}$ as in an elastic bounce³; ii) the greater deviation from the elastic model in the elderly⁴, i.e. a lower ratio $t_{\text{brake}}/t_{\text{push}}$, is associated with a greater energy expenditure¹⁷; iii) as mentioned above, both the efficiency² and the similarity to an elastic bounce (Fig. 2), increase from 4.5 to 21.6 years; and iv) in running turkeys and rhea, and hopping springhare and kangaroos, a lower efficiency in the smaller animal was found to be bound to a lower $t_{\text{brake}}/t_{\text{push}}$ ^{13,18}. The lower efficiency in smaller animals was ascribed in the literature to a less efficient elastic energy storage possibly due to their tendons being relatively thicker than those of larger animals^{19–22}.

Methods

Measurements were made starting from records of the force exerted by the foot on the ground in vertical and fore-aft directions obtained in a previous study⁸ by means of a force-platform. The method of analysis of the force records to obtain the mechanical energy of the center of mass of the body (Fig. 1) has been described in detail previously^{4,13}. Here we used only runs where: i) the ratio between positive and negative work done during the step to maintain the motion of the center of mass was between 0.75 and 1.25; ii) the curves of gravitational potential energy and of the kinetic energy of forward motion were in phase with an energy transfer between them $\leq 10\%$, warranting the mechanism of running rather than that of walking, and iii) the ratio between the average vertical force in the complete steps used for the analysis and the weight of the body was between 0.97 and 1.03. Analysis was restricted to running speeds less than 11 km h^{-1} because below this speed the mean vertical acceleration during the push is independent of body size and age⁸. Written informed consent of the subjects and/or their parents was obtained. Experiments involved no discomfort, were performed according to the Declaration of Helsinki and approved by the local ethics committee.

1. Cavagna, G. A., Saibene, F. P. & Margaria, R. Mechanical work in running. *J. Appl. Physiol.* **19**, 249–256 (1964).
2. Schepens, B., Willems, P. A., Cavagna, G. A. & Heglund, N. C. Mechanical power and efficiency in running children. *Pflugers Arch.* **442**, 107–116 (2001).



3. Cavagna, G. A. The landing-take-off asymmetry in human running. *J. Exp. Biol.* **209**, 4051–4060 (2006).
4. Cavagna, G. A., Legramandi, M. A. & Peyré-Tartaruga, L. A. The landing-take-off asymmetry of human running is enhanced in old age. *J. Exp. Biol.* **211**, 1571–1578 (2008).
5. Ker, R. F. Dynamic tensile properties of the plantaris tendon of sheep (*Ovis aries*). *J. Exp. Biol.* **93**, 283–302 (1981).
6. Alexander, R. M. Tendon elasticity and muscle function. *Comp. Biochem. Physiol.* **133A**, 1001–1011 (2002).
7. Cavagna, G. A., Legramandi, M. A. & Peyré-Tartaruga, L. A. Old men running: mechanical work and elastic bounce. *Proc. R. Soc. London Ser. B* **275**, 411–418 (2008).
8. Schepens, B., Willems, P. A. & Cavagna, G. A. The mechanics of running in children. *J. Physiol. (Lond)* **509**, 927–940 (1998).
9. Chi, K. J. & Schmitt, D. Mechanical energy and effective foot mass during impact loading of walking and running. *J. Biomech.* **38**, 1387–1395 (2005).
10. Gill, H. S. & O'Connor, J. J. Heelstrike and the pathomechanics of osteoarthritis: a pilot gait study. *J. Biomech.* **36**, 1625–1631 (2003).
11. Milner, C. E., Ferber, R., Pollard, C. D., Hamill, J. & Davis, I. S. Biomechanical factors associated with tibial stress fractures in female runners. *Med. Sci. Sports Exerc.* **38**, 323–328 (2006).
12. Pohl, M. B., Hamill, J. & Davis, I. S. Biomechanical and anatomical factors associated with a history of plantar fasciitis in female runners. *Clin. J. Sports Med.* **19**, 372–376 (2009).
13. Cavagna, G. A. & Legramandi, M. A. The bounce of the body in hopping, running and trotting: different machines with the same motor. *Proc. R. Soc. London Ser. B* **276**, 4279–4285 (2009).
14. Lieberman, D. E. *et al.* Foot strike patterns and collision forces in habitually barefoot versus shod runners. *Nature* **463**, 531–535 (2010).
15. Dotan, R., Cameron, M., Rotem, C., Klentrou, P., Gabriel, D. & Falk, B. Child-adult differences in muscle activation. A Review. *Pediatr. Exerc. Sci.* **24**, 2–21 (2012).
16. Kubo, K., Kanehisa, H., Kawakami, Y. & Fukunaga, T. Growth changes in the elastic properties of human tendon structures. *Int. J. Sports Med.* **22**, 138–143 (2001).
17. Evans, S. L., Davy, K. P., Stevenson, E. T. & Seals, D. R. Physiological determinants of 10-km performance in highly trained female runners of different ages. *J. Appl. Physiol.* **78**, 1931–1941 (1995).
18. Cavagna, G. A., Heglund, N. C. & Taylor, C. R. Mechanical work in terrestrial locomotion: two basic mechanisms for minimizing energy expenditure. *Am. J. Physiol.* **233**, R243–R261 (1977).
19. Biewener, A. A., Alexander, R. McN. & Heglund, N. C. Elastic energy storage in the hopping of kangaroo rats (*Dipodomys spectabilis*). *J. Zool.* **195**, 369–383 (1981).
20. Bennett, M. B. & Taylor, G. C. Scaling of elastic strain energy in kangaroos and the benefits of being big. *Nature* **378**, 56–59 (1995).
21. Alexander, R. McN., Jayes, A. S., Maloiy, G. M. O. & Wathuta, E. M. Allometry of the leg muscles of mammals. *J. Zool.* **194**, 539–552 (1981).
22. Pollock, C. M. & Shadwick, R. E. Allometry of muscle, tendon, and elastic energy storage capacity in mammals. *Am. J. Physiol.* **266**, R1022–R1031 (1994).

Acknowledgements

The authors wish to thank Andrea Cavagna for constructive discussions and suggestions on the manuscript preparation. This study was supported by the Fonds National de la Recherche Scientifique of Belgium and by the Italian Ministero dell'Istruzione, dell'Università e della Ricerca.

Author contributions

M.A.L. suggested to apply the landing-takeoff software^{3,4,13} to the force-platform records obtained in a previous study⁸, did most of the software arrangements and of the analysis of the data. B.S. provided the original force-platform records with instructions for their analysis and mechanical efficiency data, did most of the literature search and provided useful suggestions in the preparation of the manuscript. G.A.C. collaborated with software preparation, did some of the analysis of the data and wrote the paper.

Additional information

Competing financial interests: The authors declare no competing financial interests.

License: This work is licensed under a Creative Commons Attribution-NonCommercial-NoDerivs 3.0 Unported License. To view a copy of this license, visit <http://creativecommons.org/licenses/by-nc-nd/3.0/>

How to cite this article: Legramandi, M.A., Schepens, B. & Cavagna, G.A. Running humans attain optimal elastic bounce in their teens. *Sci. Rep.* **3**, 1310; DOI:10.1038/srep01310 (2013).