

POSTER PRESENTATION

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High-dose dobutamine stress SSFP cine MRI at 3 Tesla with patient adaptive local RF shimming using dual-source RF transmission

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Background

Image quality of cine imaging using steady state free precession (SSFP) sequences at 3T is insufficient due to increased RF-inhomogeneity (B1 field) and the high sensitivity of SSFP sequences to off-resonance artefacts. Recently, the introduction of a dual source RF transmission system with patient-adaptive local RF-shimming has led to a significant improvement of image quality of SSFP imaging at 3T.

The objective of this study was to prospectively evaluate the feasibility, image quality and diagnostic accuracy of high-dose dobutamine stress magnetic resonance imaging (DSMR) at 3T comparing dual-source versus single-source transmit technology.

Methods

DSMR was performed in 44 patients with each participant undergoing cine imaging at rest and during dobutamine infusion using both dual- and single-source transmit technology.

B1-maps and measurements of contrast to noise ratio (CNR) were evaluated to quantify the effect of RF calibration in both transmission modes.

Analysis of image quality (0=non diagnostic, 1=severe artifact, 2=slight artifact, 3=no artifact) and wall motion was performed at rest and at maximum stress comparing single- and dual-source technology.

CAD was defined on invasive coronary angiography as the presence of $\geq 70\%$ stenosis.

Results

The mean percentage of the intended flip angle within the heart increased from $88\% \pm 9.1$ with single-source to $103\% \pm 5.6$ with dual-source ($p < 0.001$). Deviation of the flip angle from the base to the apex along the pseudo-long axis decreased from $29.8\% \pm 12.9\%$ with single-source to $12.8\% \pm 7.2\%$ with dual-source.

CNR increased for dual-source vs. single-source especially pronounced at the apex (63.4 ± 24.2 vs. 36.5 ± 16.5 , $p < 0.001$) but also at the base (50.1 ± 14.8 vs. 39.3 ± 15.8 , $p < 0.001$).

Image quality of dual-source was higher than single-source both at rest (2.8 ± 0.5 vs. 2.6 ± 0.7 , $p < 0.001$) and stress (2.5 ± 0.7 vs. 2.0 ± 1.0 , $p < 0.001$). The number of segments with either severe artifacts or non-diagnostic image quality at stress was 27% using single-source compared to only 8% using dual-source (figure 1).

No significant differences between dual-source DSMR and single-source DSMR were seen regarding sensitivity (92% vs. 83%, $p = 0.38$) and specificity (88% vs. 50%, $p = 0.25$) due to the relatively small patient cohort. Diagnostic accuracy of dual-source DSMR (90%) was significantly higher than single-source DSMR (77%) ($p = 0.006$) (figure 2).

Conclusions

We demonstrated that using a dual-source transmit technology in a standard DSMR protocol is feasible in a 3T environment. Furthermore, the dual-source transmit technology provides better image quality and higher diagnostic accuracy compared to single-source transmit technology.

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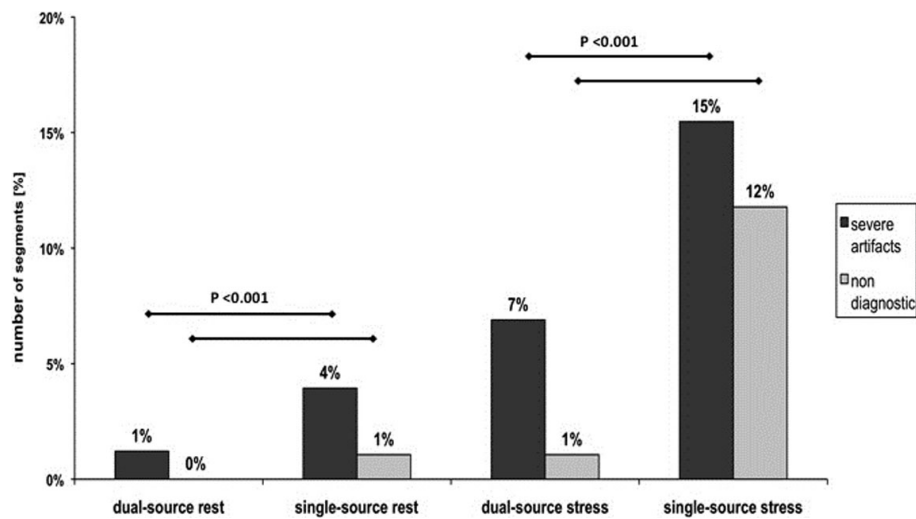


Figure 1 Analysis of image quality of DSMR SSFP cine imaging at 3 Tesla. A significant difference existed between the number of segments with severe artifacts and no diagnostic segments comparing single-source and dual-source transmit technology both at rest and even more pronounced at maximum stress.

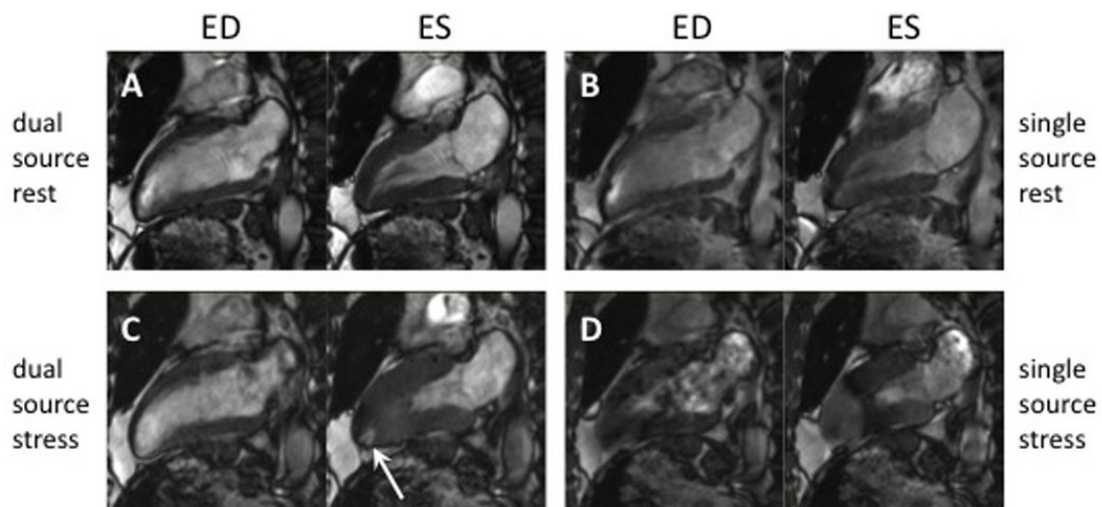


Figure 2. DSMR SSFP cine imaging at 3 Tesla using dual- vs. single source transmit technology. The single-source transmit technology is prone to banding artifacts especially at high heart rates leading to non diagnostic segments as seen on image D. A stress induced wall motion abnormality at the apex (white arrow) is visible during maximum stress using the dual source transmit technology (C). A high grade stenosis of the LAD (black arrow) is visualised by the corresponding patient's coronary angiogram (E).

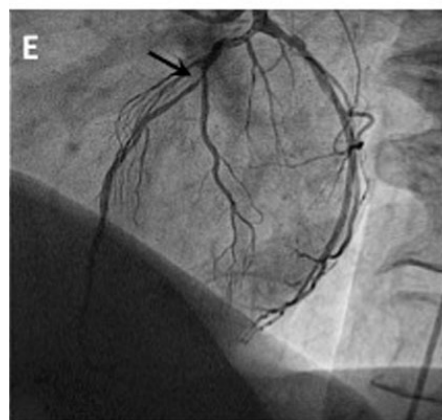


Figure 2

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