

## Research Article

# Role of Oxidation-Dependent CaMKII Activation in the Genesis of Abnormal Action Potentials in Atrial Cardiomyocytes: A Simulation Study

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Atrial fibrillation is a common cardiac arrhythmia with an increasing incidence rate. Particularly for the aging population, understanding the underlying mechanisms of atrial arrhythmia is important in designing clinical treatment. Recently, experiments have shown that atrial arrhythmia is associated with oxidative stress. In this study, an atrial cell model including oxidative-dependent  $\text{Ca}^{2+}$ /calmodulin- (CaM-) dependent protein kinase II (CaMKII) activation was developed to explore the intrinsic mechanisms of atrial arrhythmia induced by oxidative stress. The simulation results showed that oxidative stress caused early afterdepolarizations (EADs) of action potentials by altering the dynamics of transmembrane currents and intracellular calcium cycling. Oxidative stress gradually elevated the concentration of calcium ions in the cytoplasm by enhancing the L-type  $\text{Ca}^{2+}$  current and sarcoplasmic reticulum (SR) calcium release. Owing to increased intracellular calcium concentration, the inward  $\text{Na}^+/\text{Ca}^{2+}$  exchange current was elevated which slowed down the repolarization of the action potential. Thus, the action potential was prolonged and the L-type  $\text{Ca}^{2+}$  current was reactivated, resulting in the genesis of EAD. Furthermore, based on the atrial single-cell model, a two-dimensional (2D) ideal tissue model was developed to explore the effect of oxidative stress on the electrical excitation wave conduction in 2D tissue. Simulation results demonstrated that, under oxidative stress conditions, EAD hindered the conduction of electrical excitation and caused an unstable spiral wave, which could disrupt normal cardiac rhythm and cause atrial arrhythmia. This study showed the effects of excess reactive oxygen species on calcium cycling and action potential in atrial myocytes and provided insights regarding atrial arrhythmia induced by oxidative stress.

## 1. Introduction

Atrial fibrillation (AF) is the most common cardiac arrhythmia [1–3]. To design optimal treatment of AF, the mechanisms underlying AF need to be better understood. Both reactive oxygen species (ROS) and  $\text{Ca}^{2+}$ /calmodulin- (CaM-) dependent protein kinase II (CaMKII) have been shown to be associated with the development of cardiac arrhythmias [4, 5]. The kinase CaMKII is ubiquitously expressed in the cardiomyocytes [4, 6]. It is involved in numerous cellular signaling cascades, such as phosphorylation of L-type  $\text{Ca}^{2+}$  channels [7–9],  $\text{Na}^+$  channels [10, 11], ryanodine receptors

(RyRs) [12–18], and phospholamban (PLB) [12, 17, 19, 20]. Overexpression of CaMKII increases fractional sarcoplasmic reticulum (SR)  $\text{Ca}^{2+}$  release [13] and SR  $\text{Ca}^{2+}$  leakage [16], enhancing the activation of RyRs during both systole and diastole. As mentioned, it has been reported that CaMKII can also phosphorylate PLB [20]. In its unphosphorylated state, PLB acts as an endogenous inhibitor of sarco/endoplasmic reticulum  $\text{Ca}^{2+}$ -ATPase (SERCA). Therefore, phosphorylation of PLB by CaMKII will enhance SERCA activity [21]. In addition to SR  $\text{Ca}^{2+}$  dynamics, many ion channels show CaMKII-dependent phosphorylation. Phosphorylation of L-type  $\text{Ca}^{2+}$  channels induced by CaMKII is associated with

Ca<sup>2+</sup>-dependent Ca<sup>2+</sup> current facilitation [22, 23]; CaMKII-dependent phosphorylation of Na<sup>+</sup> channels may cause an increase in the late sodium current, which predisposes cardiomyocytes to arrhythmias [10, 11].

Conventionally, CaMKII is activated by Ca<sup>2+</sup>-bound calmodulin (Ca-CaM). Recently, a novel mechanism of CaMKII activation, which is ROS dependent, has been revealed [19, 24]. Previous studies have demonstrated that oxidative stress is closely associated with cardiac arrhythmias through alteration of the electrical activity and intracellular calcium dynamics of cardiac myocytes [25–27]. Oxidative stress is the main manifestation of cell metabolism disorders with excessive ROS. This oxidation-induced CaMKII activation is in relation to apoptosis [28], sinus node dysfunction [29], heart injury [30], and arrhythmias [31]. Although both ROS and CaMKII are associated with cardiac arrhythmias, the role of oxidative-dependent CaMKII activation in the development of atrial arrhythmias is not yet well understood.

In previous studies of cardiac arrhythmias, *in vivo* and *in vitro* experiments provide insights into mechanisms underlying arrhythmogenesis [5, 31]. However, these approaches have several limitations. For example, it is difficult to record the electrophysiological properties at different physical scales (from subcellular level to organ level) at the same time in one experiment. The electrophysiological properties recorded from different experiments, such as patch clamp and optical mapping, might be affected by gradual changes in cell or tissue properties. In addition to *in vivo* and *in vitro* experiments, a common method widely used in cardiac arrhythmia studies is *in silico* modeling. In this study, to simulate the effects of ROS-dependent CaMKII activation on regulations of intracellular Ca<sup>2+</sup> and ionic currents, we first developed a Markov chain model of CaMKII, including both the autophosphorylation and oxidation pathways. Then, the effect of CaMKII on related proteins and ion channels was integrated to establish a computational model of the atrial cell to simulate changes in the electrophysiology under oxidative stress conditions, including ion currents, ion concentrations, calcium cycling, and transmembrane potential. Finally, the two-dimensional (2D) spiral wave was induced and the electrical excitation propagation was analyzed under normal and oxidative stress conditions.

## 2. Methods

**2.1. CaMKII Model, including Both Autophosphorylation and Oxidation-Dependent Activation.** A six-state Markov chain model of CaMKII developed by our previous study of Zhang et al. [32] was incorporated into a human atrial model developed by Grandi et al. [33] to simulate autophosphorylation- and oxidation-dependent CaMKII activation.

The CaMKII monomer consists of three domains (an association domain, a regulatory domain, and a catalytic domain). When CaMca4 (one calmodulin bound with four Ca<sup>2+</sup>) binds to the regulatory domain, the catalytic domain will be exposed, leading to CaMKII activation. In this state, CaMKII can be further autophosphorylated or oxidized, producing a long-lasting activation, even if CaMca4 dissociates from CaMKII. Finally, CaMKII is fully deactivated by

dephosphorylation with protein phosphatases, or reduction with methionine sulfoxide reductases (MsrA). Based on the four-state model of CaMKII developed by Chiba et al. [34], two oxidized states, with and without CaMca4 binding with CaMKII, were added (see Figure S1 in the Supplementary Material for illustration), corresponding to the conformational change of oxidation-dependent CaMKII activation. Since there is no evidence to show that oxidation and autophosphorylation can occur at the same time, in this study, autophosphorylation and oxidation of CaMKII were treated as two independent processes [24]. The CaMKII autophosphorylation was based on the model developed by Chiba et al. [34]. The parameters of CaMKII oxidation were fitted to the experimental data recorded by Erickson et al. [24]. The detailed parameters of the CaMKII model are listed in Table S1 in the Supplementary Material.

**2.2. Effects of CaMKII on Ion Channels.** Previous studies showed that the ion channels influenced by CaMKII included the fast Na<sup>+</sup> current ( $I_{Na}$ ) and the L-type Ca<sup>2+</sup> current ( $I_{CaL}$ ) [7–11]. According to the method developed by O'Hara et al. [35], the current of each ion channel ( $I$ ) was divided into two parts:

$$I = (1 - \Phi)I_{base} + \Phi I_{CaMK}, \quad (1)$$

where  $I_{base}$  is the part of ion channel current not affected by CaMKII,  $I_{CaMK}$  is the part of ion channel current affected by CaMKII, and  $\Phi$  is the proportion affected by CaMKII using the following equations:

$$\Phi = \frac{CaMK_{active}}{CaMK_{active} + K_{CaMK}}, \quad (2)$$

where  $CaMK_{active}$  is the fraction of CaMKII activation and  $K_{CaMKII}$  is the Michaelis constant with the same value in O'Hara et al. [35]. For  $I_{Na}$ , the time constant of gate  $j$  was slowed down by 1.46-fold [32]. And for  $I_{CaL}$ , experimental data showed that CaMKII activation produced an increased amplitude and a slowed inactivation of  $I_{CaL}$  [36]. Therefore, in this study, the time constant of gate  $f$  was slowed down by 1.5-fold and the part of  $I_{CaL}$  affected by CaMKII was increased by  $\Delta I_{CaL,CaMK}$  shown in Equation (3).

$$\Delta I_{CaL,CaMK} = \frac{CaMKII_{active}^7}{CaMKII_{active}^7 + K_{CaMK}}. \quad (3)$$

**2.3. Effects of CaMKII on Ca<sup>2+</sup> Cycling.** Both RyR and PLB are primary regulatory proteins, controlling SR Ca<sup>2+</sup> release and uptake; these are crucial processes, maintaining the balance of intracellular Ca<sup>2+</sup>. CaMKII activation-induced RyR phosphorylation can increase RyR opening probability and SR Ca<sup>2+</sup> release. CaMKII activation-induced PLB phosphorylation can reduce SERCA inhibition, increasing SR Ca<sup>2+</sup> uptake during diastole. The RyR and PLB models developed by Soltis and Saucerman [37] were used to simulate the effects of CaMKII activation on intracellular Ca<sup>2+</sup> cycling. The rate constants controlling RyR opening ( $k_{oSRCa}$ ) and SR leakage

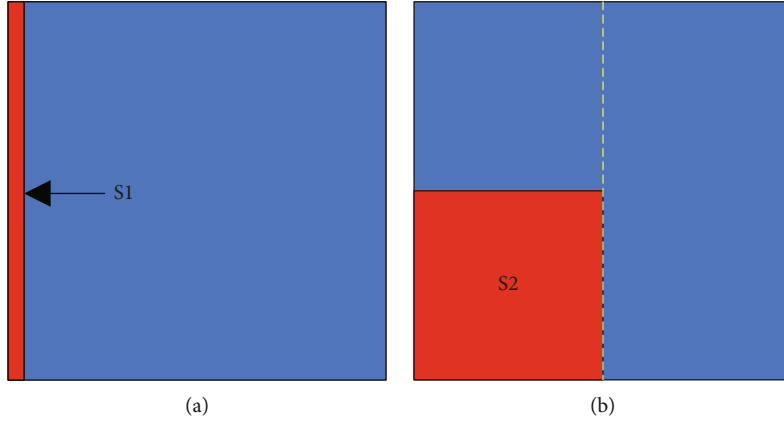


FIGURE 1: The S1–S2 protocol used in 2D simulations. The red bar in (a) and the red square in (b) represent the regions where S1 and S2 stimuli were applied.

( $k_{leak}$ ) were modified (Equations (4) and (5)) under CaMKII activation to increase RyR opening in both systolic and diastolic conditions. Meanwhile, the half maximal saturation constant of SERCA ( $K_{mf}$ ) was modified (Equation (6)) to mimic the phenomenon of increased SERCA pump calcium sensitivity, which is induced by Thr17 phosphorylation of PLB under CaMKII activation.

$$k_{oSRCa} = \left( \frac{[RyR_{2815p}]}{[RyR_{Tot}]} \frac{20}{3} - \frac{1}{3} \right) \frac{k_{oCa}}{k_{CaSR}}, \quad (4)$$

$$k_{leak} = 2.5 \frac{[RyR_{2815p}]}{[RyR_{Tot}]} + 0.5, \quad (5)$$

$$K_{mf} = K_{mf} \left( 1 - 0.5 \frac{[PLB_{T17p}]}{[PLB_{Tot}]} \right). \quad (6)$$

**2.4. Single Atrial Cell Model.** The cell membrane of an atrial myocyte was mimicked as an electrical circuit. The AP in a human atrial cell was calculated using the following ordinary differential equation [33]:

$$C_m \frac{dV_m}{dt} = -I_{ion} + I_{stim}, \quad (7)$$

where  $C_m$  is the cell capacitance,  $V_m$  is the transmembrane voltage,  $t$  is time,  $I_{ion}$  is the total transmembrane ionic current, and  $I_{stim}$  is the stimulus current.  $I_{ion}$  was calculated as

$$I_{ion} = I_{Na} + I_{Nabk} + I_{to} + I_{Kur} + I_{Kr} + I_{Ks} + I_{K1} + I_{NaK} + I_{CaL} + I_{Cabk} + I_{pCa} + I_{NCX} + I_{ClCa} + I_{Clbk}, \quad (8)$$

where  $I_{Na}$  is the fast  $Na^+$  current,  $I_{Nabk}$  is the background  $Na^+$  current,  $I_{to}$  is the transient outward  $K^+$  current,  $I_{Kur}$  is the ultrarapid delayed rectifier  $K^+$  current,  $I_{Kr}$  is the rapid activating  $K^+$  current,  $I_{Ks}$  is the slowly activating  $K^+$  current,  $I_{K1}$  is the inward rectifier  $K^+$  current,  $I_{NaK}$  is the  $Na^+/K^+$  pump current,  $I_{CaL}$  is the L-type  $Ca^{2+}$  current,  $I_{Cabk}$  is the

background  $Ca^{2+}$  current,  $I_{pCa}$  is the sarcolemmal  $Ca^{2+}$  pump current,  $I_{NCX}$  is the  $Na^+/Ca^{2+}$  exchange current,  $I_{ClCa}$  is the  $Ca^{2+}$ -activated  $Cl^-$  current, and  $I_{Clbk}$  is the background  $Cl^-$  current.

In this study, 0.5, 1, and 2 Hz stimulation frequencies were used to investigate the frequency dependency of CaMKII activation. Action potentials of atrial cells were produced by applying a stimulus current with an amplitude of  $-12.5$  pA/pF and a duration of 5 ms. The time step used in the simulation was 0.1 ms using the CVODE solver of the SUite of Nonlinear and Differential/ALgebraic equation Solvers (SUNDIALS) to solve initial value problems for ordinary differential equation systems. These simulation results were consistent with the ones using forward Euler with a time step of 0.005 ms. Under the control condition, the value of  $H_2O_2$  in the CaMKII model was  $0 \mu M$ , and the one was  $200 \mu M$  under the oxidative stress condition. To ensure that the model reached a quasistable steady state, the simulations were carried out for more than 50 s under the control condition and 150 s under the oxidative stress condition.

**2.5. Excitation Wave Conduction in 2D Tissue.** In this study, a monodomain model was used for 2D simulations in an ideal square tissue. The excitation wave propagation was simulated using the following equation:

$$\frac{\partial V_m}{\partial t} = -\frac{I_{ion}}{C_m} + \nabla \cdot (\mathbf{D} \nabla V_m), \quad (9)$$

where  $\mathbf{D}$  is the diffusion tensor describing the conductivity of the tissue and  $\nabla$  is the spatial gradient operator.

In 2D simulations, the 2D ideal isotropic tissue was constructed as a sheet of  $1000 \times 1000$  nodes to investigate the stability of the spiral waves, as used in [38]. The time step  $\Delta t$  was set at 0.005 ms, and the space step  $\Delta x$  was 0.1 mm along both direction axes, as used in [39]. The S1–S2 stimulation protocol was used to produce spiral waves. An S1 stimulus was applied to the five column nodes on the left side to induce a plane wave (Figure 1(a)). After the nodes in the middle line (the dashed line in Figure 1(b)) reached the end point of

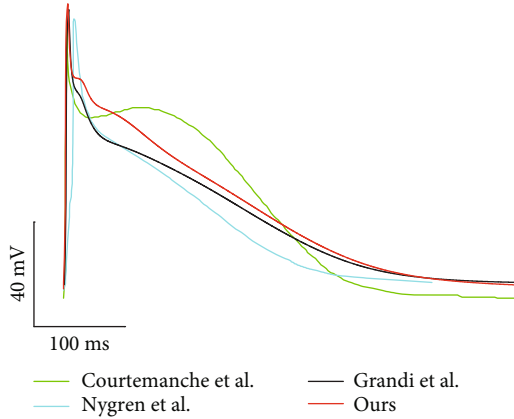


FIGURE 2: Action potential traces produced by our simulation and previous mathematical models and experiments at 1 Hz. Traces labeled “Courtemanche et al.,” “Nygren et al.,” and “Grandi et al.” were reproduced from mathematical models [33, 43, 44].

the refractory period, an S2 stimulus was applied in the left lower quadrant to induce a spiral wave (Figure 1(b)).

The conduction velocity (CV) was measured using the following equation:

$$CV = \frac{x_2 - x_1}{t_2 - t_1}, \quad (10)$$

where  $x_1$  and  $x_2$  are the positions and  $t_1$  and  $t_2$  are the times when the excitation reaches the two recording points. In 2D simulation, the tissue was isotropic and the diffusion tensor ( $D$ ) along both direction axes was set to  $0.029 \text{ mm}^2/\text{ms}$  to produce a CV of  $69 \text{ cm/s}$  in control conditions, which was consistent with the CV ( $70 \text{ cm/s}$ ) previously used for human atrial tissue simulation [40–42].

### 3. Results

**3.1. Electrophysiological Properties of a Single Atrial Cell under Control Conditions.** The action potential (AP) in a single-cell model was generated by applying a series of 1 Hz stimuli. The time trace of the simulated AP is presented in Figure 2, along with other AP traces from previous mathematical models [33, 43, 44]. The resting membrane potential (RMP), maximum upstroke velocity ( $dV/dt_{\max}$ ), action potential amplitude (APA), and action potential duration at 90% repolarization ( $APD_{90}$ ) were measured as  $-75.2 \text{ mV}$ ,  $160 \text{ mV/ms}$ ,  $110 \text{ mV}$ , and  $312 \text{ ms}$ , respectively. These parameters were consistent with previous models developed by Grandi et al. [33], Courtemanche et al. [43], and Nygren et al. [44], and  $APD_{90}$  was within the scope of previously reported experimental data [45–48], as listed in Table 1.

To further validate the model, the ionic currents and intracellular calcium cycling process were investigated and compared with those from the model of Grandi et al. [33] at 1 Hz, as shown in Figure 3. These results demonstrated an elevation in the repolarization phase of the AP and, therefore, a longer action potential duration (APD) in our model (Figure 3(a)). This was attributed to the change in  $I_{\text{CaL}}$ . In our model,  $I_{\text{CaL}}$  showed a larger amplitude and a slowed

TABLE 1: Comparison of action potential characteristics.

Model and experimental data	RMP (mV)	$dV/dt_{\max}$ (mV/ms)	APA (mV)	$APD_{90}$ (ms)
Courtemanche et al. [43]	-79.5	216	106	297
Nygren et al. [44]	-76.4	116	103.8	245
Grandi et al. [33]	-74.5	135	105	294
Our model	-75.2	160	110	312
Dawodu et al. [45]	—	—	—	$361 \pm 71$
Katoh et al. [46]	—	—	—	$255 \pm 39$
Bosch et al. [47]	—	—	—	$255 \pm 45$
Kim et al. [48]	—	—	—	$258 \pm 25$

inactivation (Figure 3(b)), which was consistent with the effect of CaMKII activation on  $I_{\text{CaL}}$  [36]. In addition to the AP, the variation in  $I_{\text{CaL}}$  altered intracellular calcium regulation, as  $I_{\text{CaL}}$  was the main influx of intracellular  $\text{Ca}^{2+}$ . The increase in  $I_{\text{CaL}}$  caused a larger  $\text{Ca}^{2+}$  influx, leading to a larger SR  $\text{Ca}^{2+}$  release (Figure 3(c)) and thus a larger intracellular  $\text{Ca}^{2+}$  concentration (Figure 3(d)). The accumulation of intracellular  $\text{Ca}^{2+}$  finally caused an elevation in the concentration of SR  $\text{Ca}^{2+}$  (Figure 3(e)). Interestingly, the peak inward  $I_{\text{NCX}}$  in our model declined even when the intracellular  $\text{Ca}^{2+}$  concentration increased (Figure 3(f)). This may be explained by the fact that the elevation of the membrane potential during the repolarization phase suppressed the inward  $\text{Na}^+$  flux and decreased  $I_{\text{NCX}}$ .

To justify the increase of intracellular  $\text{Ca}^{2+}$  concentration in our model, the  $\text{Ca}^{2+}$  concentration was compared with previous studies. The calcium transient amplitude in our model was  $\sim 0.53 \mu\text{M}$ , which was consistent with the studies of Courtemanche et al. and Colman et al. ( $0.45\text{--}0.55 \mu\text{M}$ ) [43, 49], although the  $\text{Ca}^{2+}$  transient amplitude in the study of Nygren et al. was reported to be even larger ( $\sim 1.2 \mu\text{M}$ ) [44].

The variations in  $I_{\text{CaL}}$  and intracellular calcium cycling were caused by adding the effect of CaMKII activation in our model. Previous studies demonstrated that CaMKII activation was significantly influenced by pacing frequencies. In our simulation, CaMKII activation and intracellular  $\text{Ca}^{2+}$  dynamics were investigated at 0.5, 1, and 2 Hz. Figure 4(a) shows that the fraction of CaMKII activation increased with increasing pacing rate. Meanwhile, the time required for CaMKII activation was also decreased, indicating a faster activation at a higher pacing rate (Figure 4(a)). The frequency-dependent activation of CaMKII was mainly due to the intracellular  $\text{Ca}^{2+}$  concentration. With increasing pacing rate, both RyR  $\text{Ca}^{2+}$  release and intracellular  $\text{Ca}^{2+}$  concentration increased (Figure 4(b)), causing an increase in CaMCA4 and, therefore, augmenting CaMKII activation.

**3.2. Electrophysiological Properties of a Single Atrial Cell under Oxidative Stress Conditions.** The simulation results showed that an EAD was induced in the AP under conditions of oxidative stress at a pacing rate of 1 Hz (Figure 5(a)). In this case, the elevated ROS concentration ( $0.2 \text{ mM}$ ) induced a significant increase in CaMKII activation (Figure 5(b)).

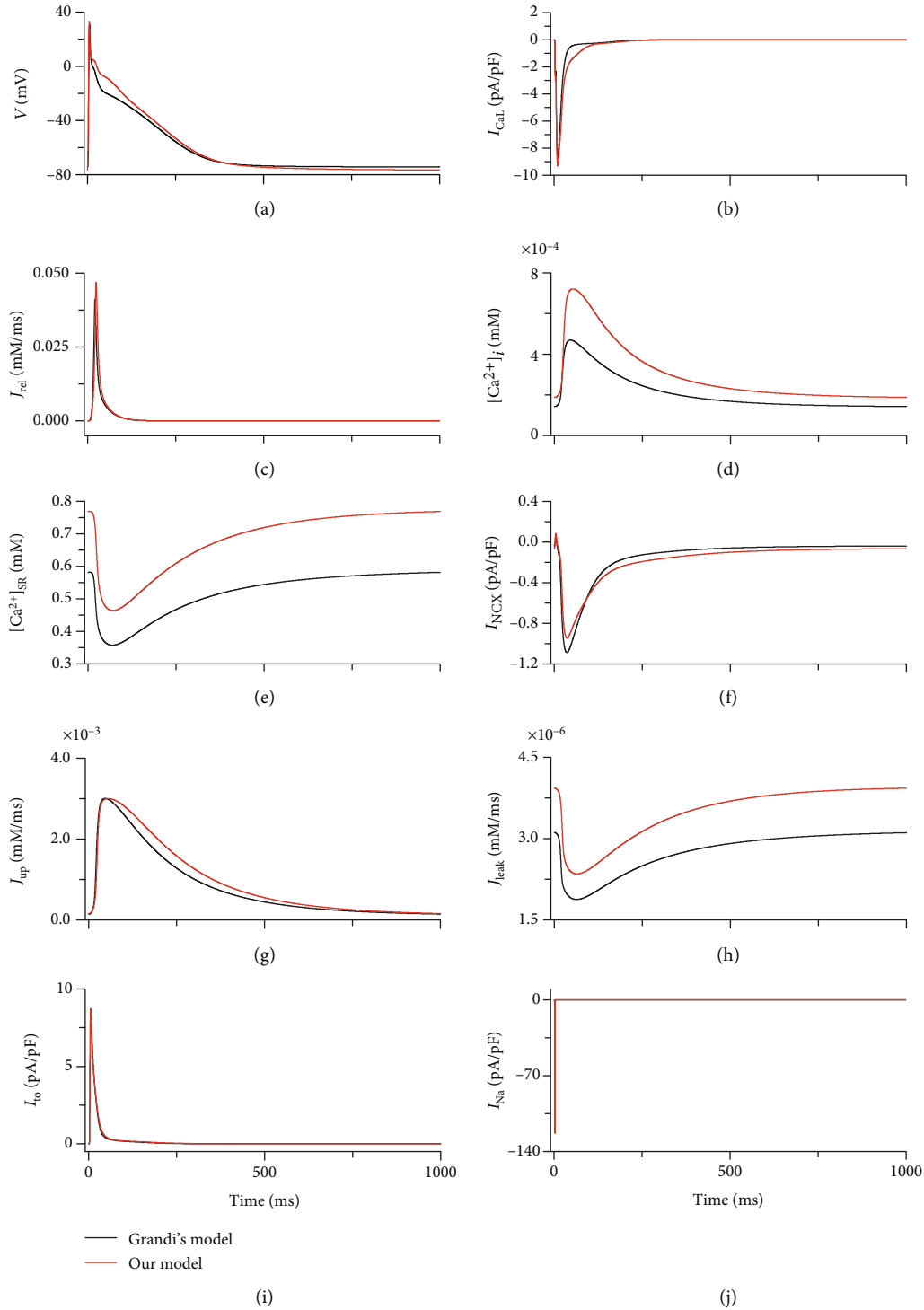


FIGURE 3: Traces of AP, ionic currents, and calcium cycling produced by our model (red) and the model of Grandi et al. [33] (black). (a) AP. (b)  $I_{CaL}$ . (c) SR  $Ca^{2+}$  release ( $J_{rel}$ ). (d) intracellular  $Ca^{2+}$  concentration ( $[Ca^{2+}]_i$ ). (e) SR  $Ca^{2+}$  concentration ( $[Ca^{2+}]_{SR}$ ). (f)  $I_{NCX}$ . (g) SR  $Ca^{2+}$  reuptake ( $J_{up}$ ). (h) SR  $Ca^{2+}$  leakage ( $J_{leak}$ ). (i)  $I_{to}$ . (j)  $I_{Na}$ .

ROS-enhanced CaMKII activation further enlarged  $I_{CaL}$ ,  $I_{NCX}$ , fraction of RyR phosphorylation, and fraction of PLB phosphorylation (Figures 5(c)–5(f)). Under oxidative stress conditions, the intracellular  $Ca^{2+}$  dynamics were remarkably changed. Enhanced RyR and PLB phosphorylation caused significant increases in  $J_{rel}$ ,  $J_{up}$ , and  $J_{leak}$  (Figures 5(g)–5(i)),

which further induced a dramatic increase in intracellular  $Ca^{2+}$  concentration (Figure 5(j)) and a decrease in minimum SR  $Ca^{2+}$  (Figure 5(k)). However, there was no obvious change in the intracellular  $Na^+$  concentration (Figure 5(l)).

As CaMKII activation showed frequency-dependent behavior, ROS-induced EADs are rate dependent as well.

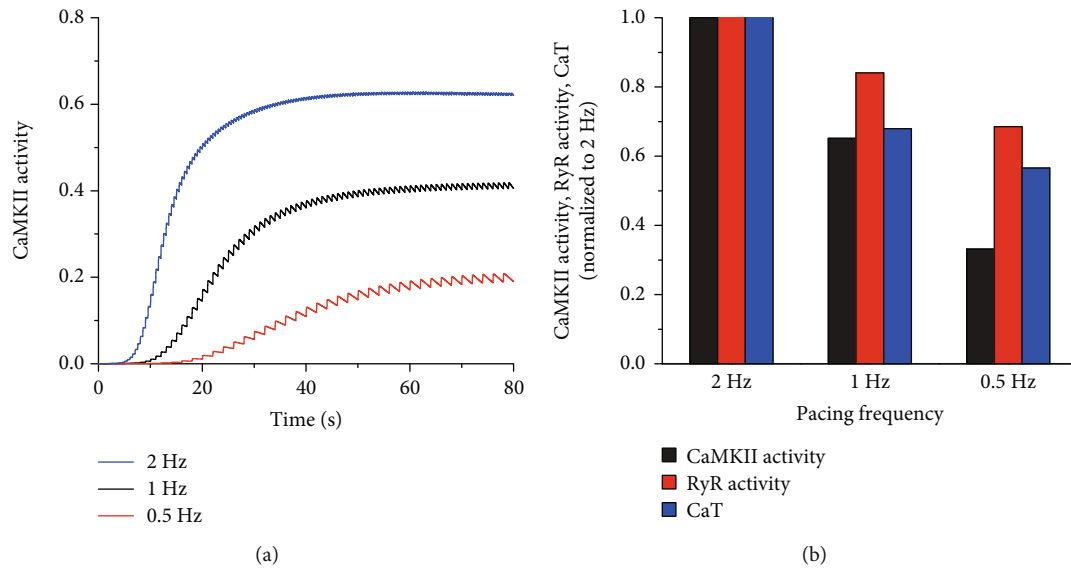


FIGURE 4: Frequency-dependent activation of CaMKII. (a) CaMKII activation curves at 0.5, 1, and 2 Hz in 80 s. (b) Normalized CaMKII activation, RyR calcium release (RyR Activity), and intracellular  $\text{Ca}^{2+}$  transient (CaT) to 2 Hz at 0.5, 1, and 2 Hz.

Under oxidative stress conditions, the occurrence of EADs in 50 s became more prominent with decreasing pacing rate, as shown in Figure 6. Under control conditions, the CaMKII activation (without ROS-induced activation) gradually decreased with decreasing pacing rate (Figure 4(b)). This meant that more CaMKII could be activated by ROS under oxidative conditions at low pacing rates. Consequently, the CaMKII activation induced by ROS gradually increased with decreasing pacing rate (green bars in Figure 6). Therefore, under oxidative stress conditions, more EADs were induced at low pacing rates.

**3.3. Mechanisms Underlying the Genesis of EAD under Oxidative Stress Conditions.** In the case of EAD,  $I_{\text{CaL}}$  and  $I_{\text{NCX}}$  were the main currents significantly influenced by oxidative stress. Blocking  $I_{\text{CaL}}$  at the point of  $I_{\text{CaL}}$  reactivation abolished EAD (data not shown), implying that  $I_{\text{CaL}}$  was a main factor contributing to the genesis of EAD. However, blocking  $I_{\text{NCX}}$  did not guarantee elimination of EAD. Figure 7 indicated the effects of blocking  $I_{\text{NCX}}$  at different times from the point of  $I_{\text{CaL}}$  reactivation (70 ms) to the time of the peak of EAD (350 ms). With the delay in blocking  $I_{\text{NCX}}$  (Figure 7(a)), the reactivation of  $I_{\text{CaL}}$  became more prominent (Figure 7(b)) and the APD gradually increased (Figure 7(c)). When blocking  $I_{\text{NCX}}$  in the interval 70–210 ms, the reactivation of  $I_{\text{CaL}}$  did not induce AP depolarization and therefore abolished EAD. On blocking  $I_{\text{NCX}}$  during the interval 210–280 ms, the enlarged reactivation of  $I_{\text{CaL}}$  started to transfer AP repolarization to depolarization. However, in this time interval, AP depolarization was not obvious and no EAD was induced. When blocking  $I_{\text{NCX}}$  during the interval 280–350 ms, the reactivation of  $I_{\text{CaL}}$  was able to induce AP depolarization. Consequently, in this time interval, blocking  $I_{\text{NCX}}$  could not eliminate EAD (Figure 7(c)). Therefore,  $I_{\text{NCX}}$  played an important role in  $I_{\text{CaL}}$  reactivation and thus in triggering EAD.

In our model,  $I_{\text{NCX}}$  was not directly regulated by ROS. As the main efflux of intracellular  $\text{Ca}^{2+}$ ,  $I_{\text{NCX}}$  was regulated by intracellular  $\text{Ca}^{2+}$  concentration;  $\text{Ca}^{2+}$  cycling was another important process affected by ROS-induced CaMKII activation. Three factors associated with intracellular cycling in our model were directly regulated by ROS-induced CaMKII activation, namely,  $I_{\text{CaL}}$ ,  $J_{\text{rel}}$ , and  $J_{\text{up}}$ . Under oxidative stress conditions, intracellular  $\text{Ca}^{2+}$  concentration significantly increased (Figure 5(j)). To investigate the role of  $[\text{Ca}^{2+}]_i$  regulation in the genesis of EAD, decreased  $I_{\text{CaL}}$ , reduced  $J_{\text{rel}}$ , and enhanced  $J_{\text{up}}$  were independently applied to reduce the  $[\text{Ca}^{2+}]_i$  under oxidative stress conditions, as shown in Figure 8. Figure 8(a) shows that decreasing  $I_{\text{CaL}}$  by 10% abolished EAD. This was due not only to  $[\text{Ca}^{2+}]_i$  decline but also to a decrease in  $I_{\text{CaL}}$  reactivation. Reducing SR  $\text{Ca}^{2+}$  release postponed the occurrence of EAD but did not successfully eliminate EAD (Figure 8(b)). Although a reduction in SR  $\text{Ca}^{2+}$  release temporarily reduced  $[\text{Ca}^{2+}]_i$ , it caused  $\text{Ca}^{2+}$  accumulation in SR, which finally induced  $[\text{Ca}^{2+}]_i$  elevation (data not shown) and EAD. Increasing SR  $\text{Ca}^{2+}$  uptake by 10% had a similar effect to that of reducing SR calcium release (Figure 8(c)). Nonetheless, further increasing  $J_{\text{up}}$  by 20%–30% abolished EAD. In these two cases, the SR  $\text{Ca}^{2+}$  uptake and release reached a new balance and maintained  $[\text{Ca}^{2+}]_i$  and  $[\text{Ca}^{2+}]_{\text{SR}}$  at a steady state (data not shown).

**3.4. Effect of Oxidative Stress on Excitation Wave Propagation in 2D Tissue.** The excitation wave propagation was investigated in 2D ideal tissue under control and oxidative stress conditions. Spiral waves were induced using the S1–S2 protocol. Under control conditions with the S1–S2 interval of 550 ms, a stationary spiral wave was produced, with its tip anchored in the central region of the square tissue, as shown in Figure 9. Under oxidative stress conditions, the ROS concentration was set to 0.2 mM for all nodes in the tissue. In this

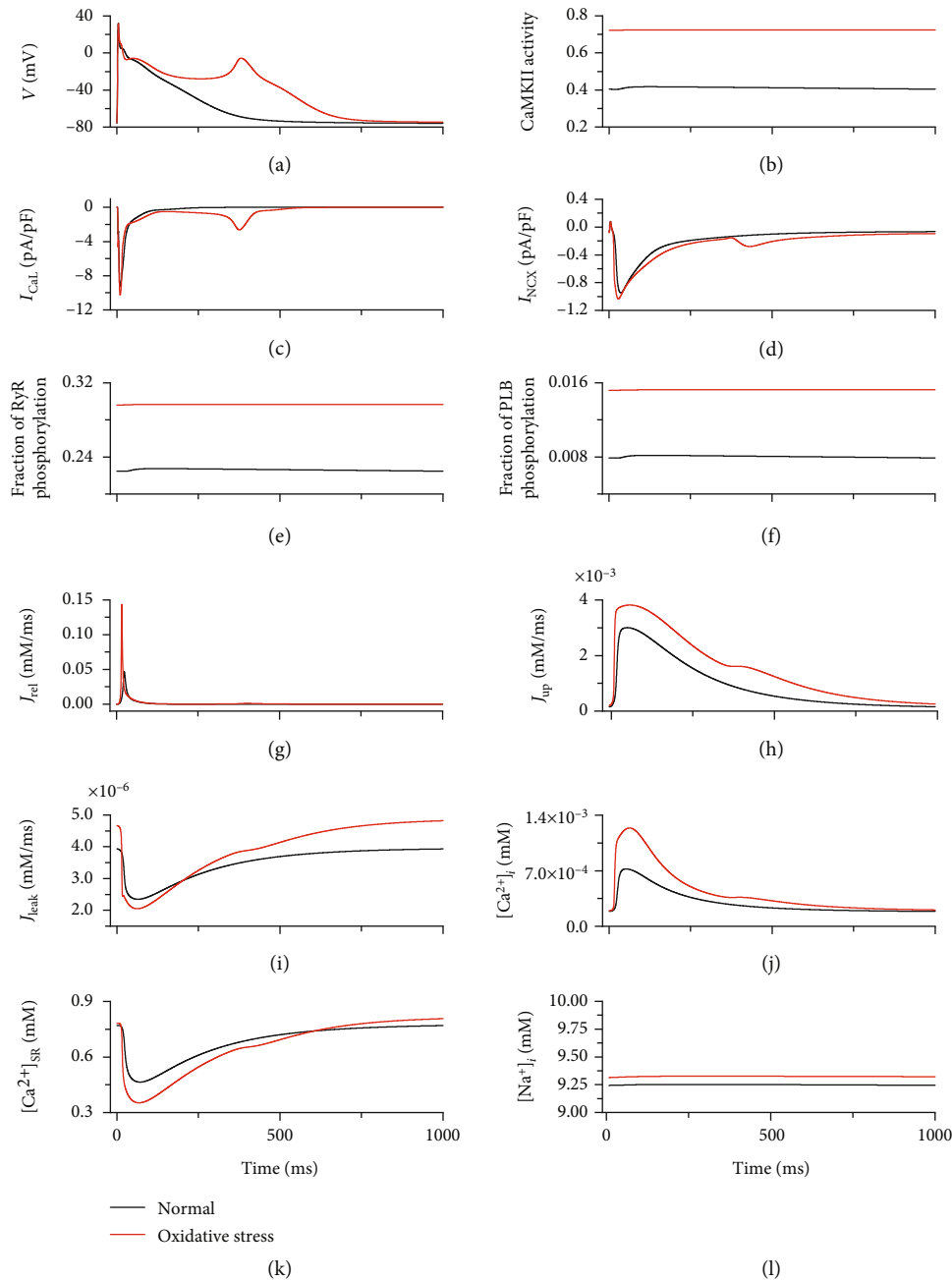


FIGURE 5: Traces of AP, ionic currents, and calcium cycling under normal (black) and oxidative stress (red) conditions. (a) AP. (b) CaMKII activity. (c)  $I_{CaL}$ . (d)  $I_{NCX}$ . (e) Fraction of RyR phosphorylation. (f) Fraction of PLB phosphorylation. (g)  $J_{rel}$ . (h)  $J_{up}$ . (i)  $J_{leak}$ . (j)  $[Ca^{2+}]_i$ . (k)  $[Ca^{2+}]_{SR}$ . (l) Intracellular  $Na^+$  concentration ( $[Na^+]_i$ ).

case with the S1–S2 interval of 730 ms, a nonstationary spiral wave was induced. As the EAD was induced under this condition, the region to which the S2 stimulus was applied showed a prolonged depolarization (Figure 10, 1125 ms) and a second wavefront was induced at 1450 ms, as shown in Figure 10. When the wavefronts reached the region to which the S2 stimulus was applied (Figure 10, 1650 ms), the nodes were not fully repolarized, owing to the prolonged APD induced by EAD. Therefore, the excitation wave propagation was suppressed (Figure 10, 1650 ms). Finally, the tip of the spiral wave wandered across the tissue and pro-

duced a nonstationary spiral wave. When oxidative stress only occurred in the right third of the tissue, the spatial heterogeneity further aggravated the instability of the nonstationary spiral wave and gave rise to a breakup of the spiral wave (data not shown).

#### 4. Discussion

In this study, the effects of ROS-dependent CaMKII activation on regulations of intracellular  $Ca^{2+}$  and ionic currents were investigated *in silico* using the updated human atrial cell

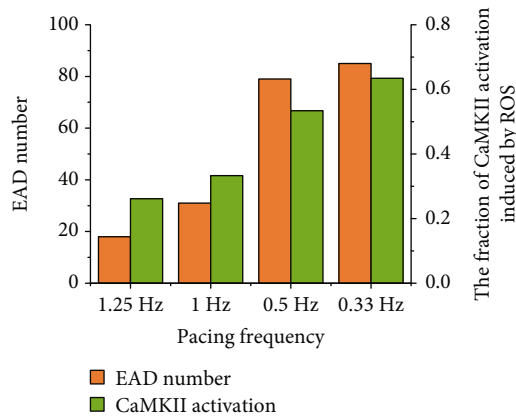


FIGURE 6: Number of EAD occurring in the same duration (orange) and the fraction of CaMKII activation induced by ROS (green) at different pacing rates under oxidative stress conditions.

model including the CaMKII model with autophosphorylation- and oxidation-dependent activation at the single-cell level and 2D tissue model. Our major findings follow: (i) A new Markov chain model of CaMKII, including both the autophosphorylation and oxidation pathways, was developed, and the effects of CaMKII on ion channels and  $\text{Ca}^{2+}$  cycling were incorporated into the computational model of the atrial myocyte. (ii) The mechanisms of oxidative stress-induced EADs in atrial cells were thoroughly examined which are helpful to further understand or investigate the mechanisms underlying oxidative stress-induced AF. The simulation results at the single-cell level illustrated that oxidative stress resulted in EADs of the AP at the normal pacing rate of 1 Hz. It was contributed by reactivation of  $I_{\text{CaL}}$  and intracellular  $\text{Ca}^{2+}$  elevation induced by CaMKII activation under oxidative stress conditions. (iii) The 2D simulations provide insights into reentry in atrial tissue under the oxidative stress condition, which plays significant roles in AF mechanisms. In 2D simulation, oxidative stress aggravated the instability of the excitation wave and gave rise to a non-stationary spiral wave, owing to the EAD induced by oxidative stress hindering the electrical conduction.

**4.1. Model Development of ROS-Dependent CaMKII Activation.** Previous experimental studies have revealed that both ROS and CaMKII are associated with the development of atrial arrhythmia [4, 5]. In addition, it has recently been reported that CaMKII can keep persistent activity by oxidation [24]. However, the role of ROS-dependent CaMKII activation in the genesis of atrial fibrillation is not yet well understood. In this study, we developed a computational model of human atrial cell including both ROS-dependent and autophosphorylation-dependent CaMKII activation to investigate effects of CaMKII activation on atrial electrophysiology under oxidative stress condition. In this CaMKII model, a pathway of ROS-dependent CaMKII activation was introduced which was different from previous CaMKII models only including the autophosphorylation-dependent CaMKII activation [34, 35, 50]. Christensen et al. [39] also developed a model of CaMKII activity including oxidation and autophosphorylation activation pathways. However, dif-

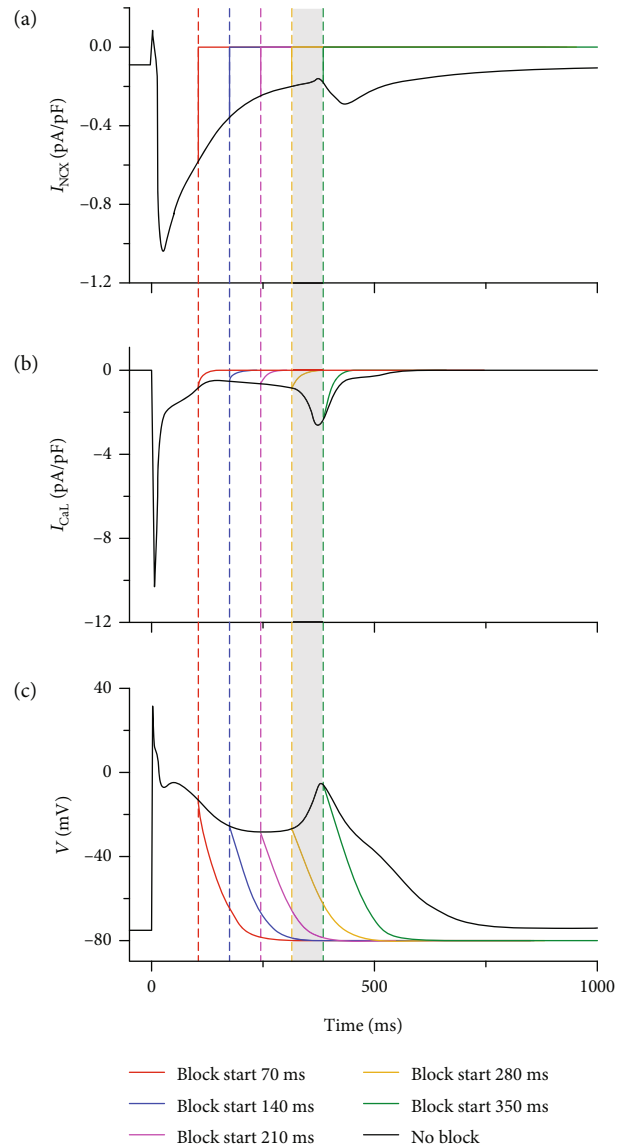


FIGURE 7: Effects of blocking  $I_{\text{NCX}}$  at different times on the genesis of EAD under oxidative stress condition: (a)  $I_{\text{NCX}}$ . (b)  $I_{\text{CaL}}$ . (c) AP. The gray box represents the time interval during which EAD can occur while blocking  $I_{\text{NCX}}$ .

ferent from their model, the oxidation and autophosphorylation activation pathways in our six-state CaMKII are mutual independence, implying that there is no such a state with both oxidation and autophosphorylation activation simultaneously. This fact is consistent with the experimental observations reported in [24].

The effect of CaMKII on  $I_{\text{Na}}$ ,  $I_{\text{CaL}}$ , RyR, and PLB was integrated into the human atrial myocyte model, producing action potential characteristics (such as RMP,  $dV/dt_{\text{max}}$ , APA,  $\text{APD}_{90}$ , and the calcium transient amplitude) consistent with previous models and experimental data of human atrial myocytes [33, 43–49] (Figure 2 and Table 1).

**4.2. Mechanisms Underlying the Genesis of EAD under Oxidative Stress Conditions.** The generation of EADs



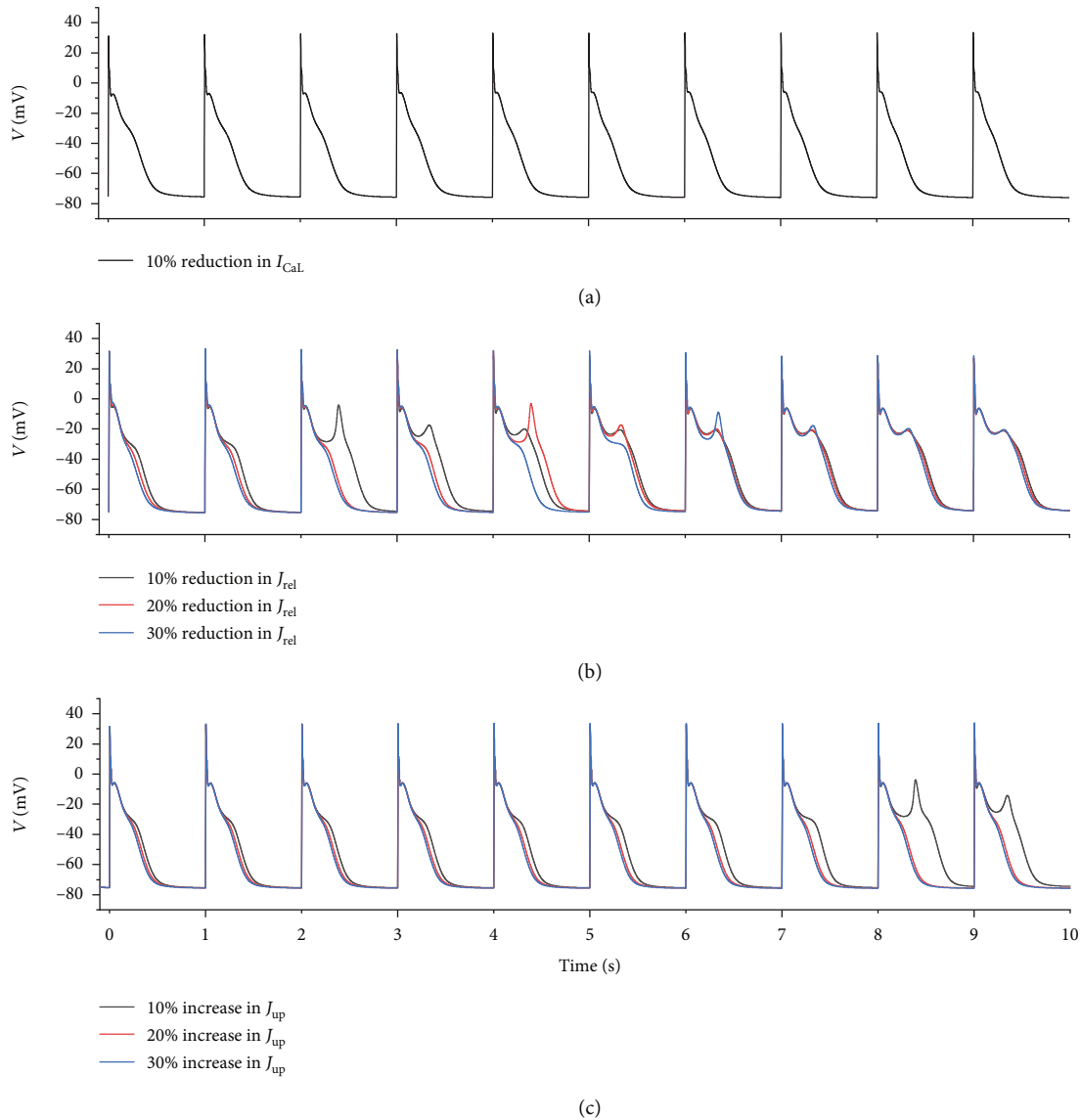


FIGURE 8: Effect of (a) reducing  $I_{CaL}$  by 10%, (b) reducing  $J_{rel}$  by 10%, 20%, and 30%, and (c) increasing  $J_{up}$  by 10%, 20%, and 30% on the genesis of EAD under oxidative stress conditions.

associated with ectopic (triggered) activity can be contributed by CaMKII activation [51–55]. Animal experiments have shown that oxidative stress can promote EADs in the ventricle of guinea pigs and rabbits [56]. Therefore, this study explored the intrinsic mechanisms of EADs associated with atrial arrhythmia induced by oxidative stress, using the developed CaMKII model.

First, simulation results demonstrated that the characteristics of AP and calcium cycling generated by our model were consistent with previous computational and experimental studies [43–49]. After model validation, the role of oxidation-dependent CaMKII activation on the AP was investigated in a single atrial cell model. The simulation results demonstrated that, under oxidative stress conditions, increasing ROS concentrations in the cytoplasm enhanced CaMKII activation and consequently augmented  $I_{CaL}$ , RyR phosphorylation, and PLB phosphorylation (Figures 5(c),

5(e), and (f)), inducing an enhanced  $Ca^{2+}$  influx, a larger SR  $Ca^{2+}$  release, and a promoted SR  $Ca^{2+}$  uptake (Figures 5(g) and 5(h)). These effects generated a remarkable elevation in intracellular  $Ca^{2+}$  concentration and therefore enlarged  $I_{NCX}$  via promoted  $Ca^{2+}$  extrusion (Figure 5(d)).  $I_{NCX}$  augmentation provided a depolarization component to counterbalance the repolarization reserve and prolong the APD. The elevated and prolonged AP in phase 3 gradually caused reactivation of  $I_{CaL}$  (Figure 5(c)), which ultimately induced action potential depolarization and produced EAD (Figure 5(a)), consistent with previous studies [57–59].

In this process, as  $I_{CaL}$  was the direct depolarization current inducing EAD, blocking  $I_{CaL}$  completely abolished EAD. However, blocking  $I_{NCX}$  at different time points had different effects on EAD. If  $I_{NCX}$  was blocked before  $I_{CaL}$  reactivation could induce AP depolarization, EAD was eliminated (Figure 7). This phenomenon suggested that  $I_{NCX}$

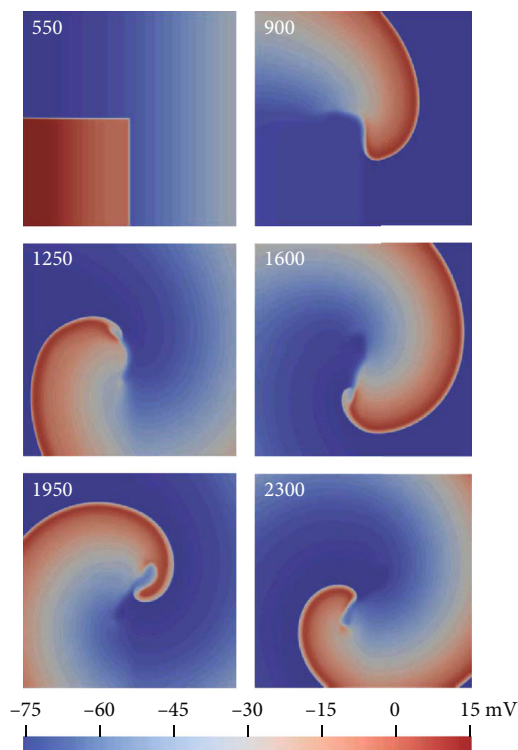


FIGURE 9: Spiral wave induced under control conditions using the S1–S2 protocol. The number in each panel represents the recording time.

augmentation acted as a trigger of  $I_{CaL}$  reactivation. EAD can be induced only when the trigger is large enough. Under oxidative stress condition, ROS elevation did not affect  $I_{NCX}$  directly and the increase of  $[Ca^{2+}]_i$  primarily accounted for  $I_{NCX}$  augmentation. Therefore, the effects of ROS-induced CaMKII activation on intracellular calcium cycling also played a crucial role in the genesis of EAD.

To examine the role of ROS-induced  $[Ca^{2+}]_i$  elevation in the genesis of EAD,  $Ca^{2+}$  influx and SR  $Ca^{2+}$  release and uptake were modified to reduce ROS-induced  $[Ca^{2+}]_i$  elevation. First,  $I_{CaL}$  was reduced by 10% to inhibit  $Ca^{2+}$  influx, causing a decline of  $[Ca^{2+}]_i$ . Together with the decreased reactivation of  $I_{CaL}$ , the  $[Ca^{2+}]_i$  decline caused by reducing  $I_{CaL}$  abolished EAD (Figure 8(a)). Second, partial inhibition of SR  $Ca^{2+}$  release (by 10%–30%) temporarily reduced  $[Ca^{2+}]_i$ . However, inhibition of SR  $Ca^{2+}$  release gradually caused SR  $Ca^{2+}$  accumulation and ultimately gave rise to further  $[Ca^{2+}]_i$  elevation, which accounted for the fact that partial inhibition of SR  $Ca^{2+}$  release could only postpone the occurrence of EAD but could not abolish EAD (Figure 8(b)). Increasing SR  $Ca^{2+}$  uptake by 10% had a similar effect to partial inhibition of SR  $Ca^{2+}$  release. Interestingly, on further increasing SR  $Ca^{2+}$  uptake by 20% and 30%,  $[Ca^{2+}]_i$  declined and EAD was abolished. This phenomenon might be attributed to a new balance of increased SR  $Ca^{2+}$  uptake and ROS-induced  $[Ca^{2+}]_i$  release (Figure 8(c)). Therefore, the dynamic balance between SR  $Ca^{2+}$  release and uptake is the key factor in maintaining  $[Ca^{2+}]_i$  at a steady state.

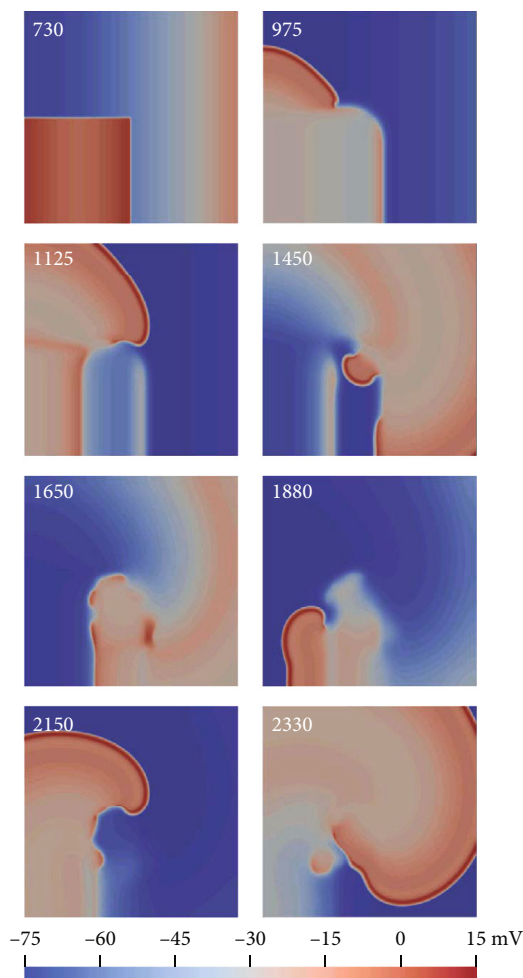


FIGURE 10: Spiral wave induced under oxidative stress conditions using the S1–S2 protocol. The number in each panel represents the recording time.

**4.3. Effect of Rate-Dependent CaMKII Activation on EAD under Oxidative Stress Conditions.** Under control conditions, CaMKII activation gradually decreased with a decrease in the pacing rate, as  $Ca^{2+}$  concentration gradually decreased at low pacing rates. However, under oxidative stress conditions, once CaMKII was activated, the high ROS concentration tended to maintain CaMKII activation. Therefore, under oxidative stress conditions, fractions of CaMKII activation at different pacing rates were similar and maintained at a high level (about 75%). This indicated that, at low pacing rates, ROS-induced CaMKII activation played a more important role. At low pacing rates, intracellular  $Ca^{2+}$  concentration could be dramatically increased by ROS-induced CaMKII activation and therefore could induce more EADs (Figure 6). Although the heart rate is not so slow such as 0.5 Hz and 0.33 Hz under normal conditions, it may be such slow under some pathological conditions, such as bradycardia [60]. The purpose of exploring up to such slow pacing frequencies is to investigate whether the occurrence of EAD is linear with the decrease of pacing frequency or not. The results showed that the occurrence of EAD was more

dependent on ROS-induced CaMKII activation rather than the pacing frequencies.

**4.4. Effect of Oxidative Stress on Excitation Wave Propagation in 2D Tissue.** The spiral wave is a well-known approach to understanding reentry in cardiac tissue, which plays significant roles in AF mechanisms [61]. This study investigated the stability of the spiral wave in 2D ideal tissue under control and oxidative stress conditions. In tissue with a uniform distribution of oxidative stress (Figure 10), the region to which the S2 stimulus was applied had a prolonged depolarization phase, owing to the ROS-induced EAD, forming a spiral wave barrier. In addition, the ROS-induced EAD produced a second excitation wavefront during wave propagation. These effects finally produced a nonstationary spiral wave. In the case of nonuniform distribution of oxidative stress, a breakup of the spiral wave was induced, which might disrupt normal cardiac rhythm and cause atrial arrhythmia [62–64].

**4.5. Model Limitations and Future Directions.** The present model was based on models of Grandi et al. [33] and O'Hara et al. [35] and thus inherited the same limitations of both models. The main limitation of the current model, which will be addressed in the future, is that the ROS concentration is constant. In future versions, pathways of ROS production and scavenging should be added. Another issue for model development is to expand the model into real 2D heart tissue and 3D organ models, to explore electrical wave propagation induced by abnormal action potentials, and electrocardiography in real heart geometry.

Although the S1–S2 interval in 2D simulation to produce the spiral wave was dependent on the tissue size, it is reasonable to investigate the difference in the stability of the spiral wave using the same tissue size under control and oxidative stress conditions. Further work is required to measure the range of S1–S2 intervals for producing the spiral wave (vulnerable window) varying from control to oxidative stress conditions to further determine the proarrhythmic effect of oxidative stress.

## 5. Conclusions

In this study, we have investigated the role of oxidation-dependent CaMKII activation in the genesis of abnormal action potentials in atria. It was shown that, at the atrial cell level, oxidation-dependent CaMKII activation-induced  $I_{CaL}$  reactivation and  $[Ca^{2+}]_i$  elevation contributed to EAD generation. Moreover, at the 2D tissue level, oxidative stress-induced EAD contributed to the instability of excitation waves, facilitating atrial arrhythmia. This study investigated the role of ROS-dependent CaMKII activation in the development of atrial arrhythmias, shedding light on the genesis of atrial arrhythmias under oxidative stress conditions.

## Data Availability

The data used to support the findings of this study are available from the corresponding author upon request.

## Conflicts of Interest

The authors declare that there is no conflict of interest regarding the publication of this paper.

## Authors' Contributions

Qince Li, Henggui Zhang, and Na Zhao conceived the study and designed the simulations. Na Zhao and Haibo Sui developed the model and conducted the simulations. The paper was written by Qince Li. Qince Li and Henggui Zhang analyzed the simulation results. Qince Li and Na Zhao contributed equally to this work. All the authors read and approved the final manuscript.

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## Supplementary Materials

Figure S1: The CaMKII model. B, CaMKII-CaMCA4 (bound state); BO, CaMKIIox-CaMCA4 (oxidized and bound state); BP, CaMKIIP-CaMCA4 (phosphorylated and bound state); I, CaMKII (inactive state); O, CaMKIIox (oxidized state); P, CaMKIIP (phosphorylated state). Table S1: Parameters of CaMKII model (*Supplementary Materials*)

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